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(54) **TOOL FOR SURGICAL OPERATION USING ULTRASONIC WAVES**

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Primary Examiner — Ryan J Severson

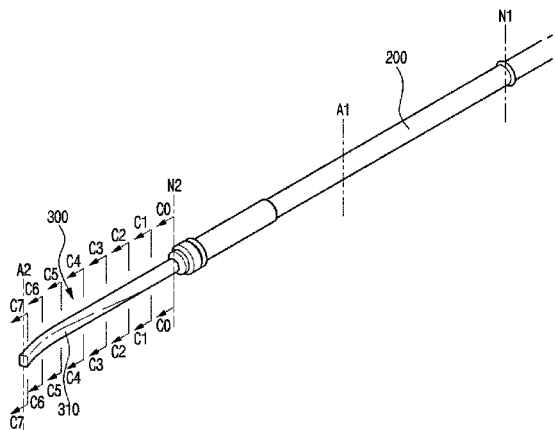
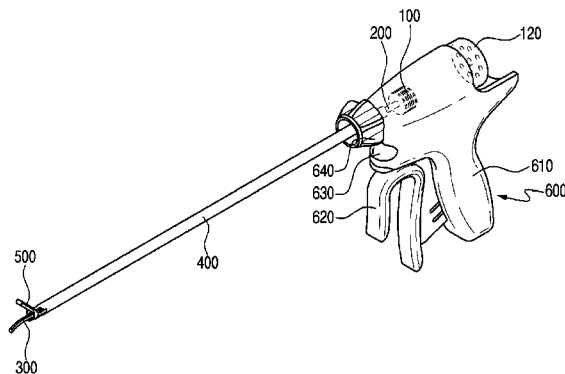
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(57) **ABSTRACT**

A tool for surgical operation using ultrasonic waves is provided. The tool includes a transducer generating ultrasonic waves, a cylindrical bar-shaped transmitting rod for transmitting the ultrasonic waves, an end effector for cutting a surgical site using the ultrasonic waves transmitted from the transmitting rod, extended from one end of the transmitting rod, in which a part of the circular cross-sectional area thereof is flatly formed from the point corresponding to a second vibration node so as to allow gain step to start at the second vibration node, a rod cover for encompassing the transmitting rod using, as connection points, a plurality of vibration nodes formed when ultrasonic waves are transmitted through the transmitting rod, and a jaw for holding the surgical site while engaged with the end effector, is combined to one end of the rod cover in a pivotable manner, and is positioned to face the end effector.

9 Claims, 9 Drawing Sheets



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A61B 2017/320089; A61B 2017/32009
See application file for complete search history.

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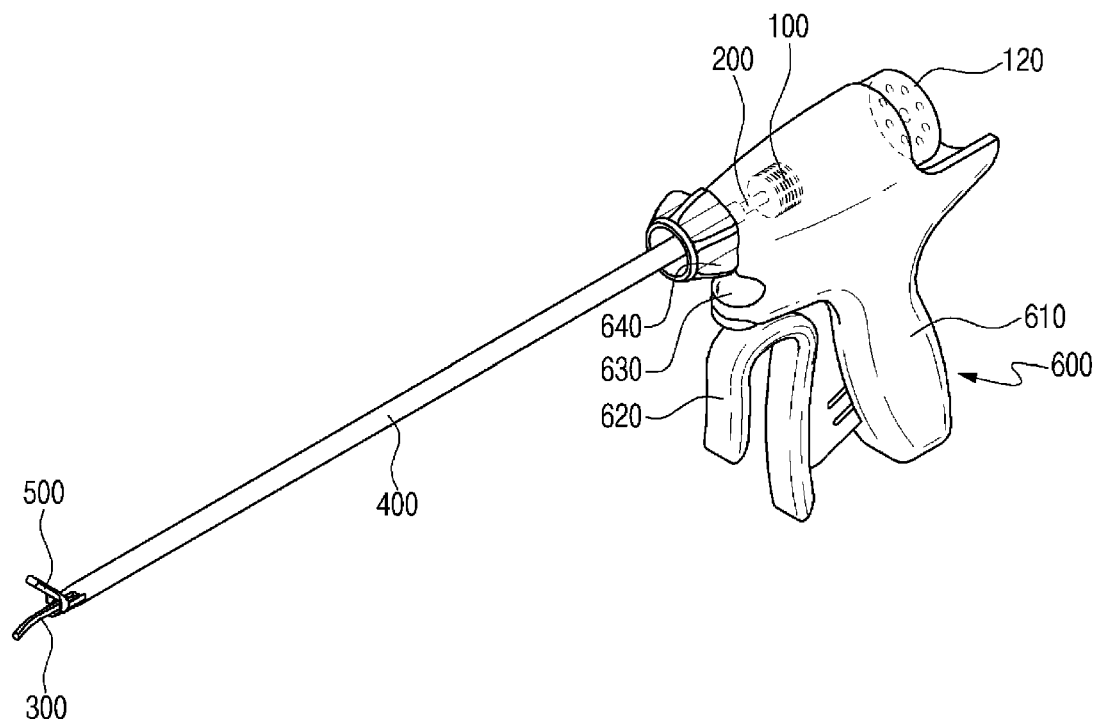
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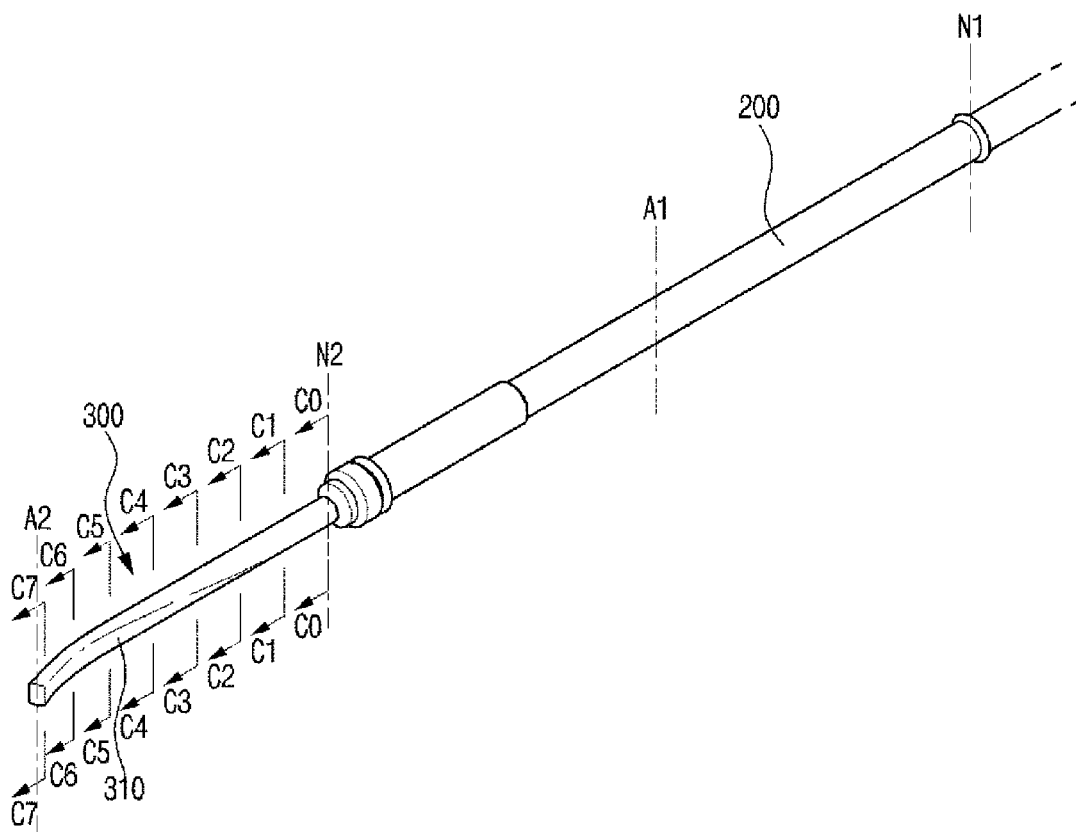
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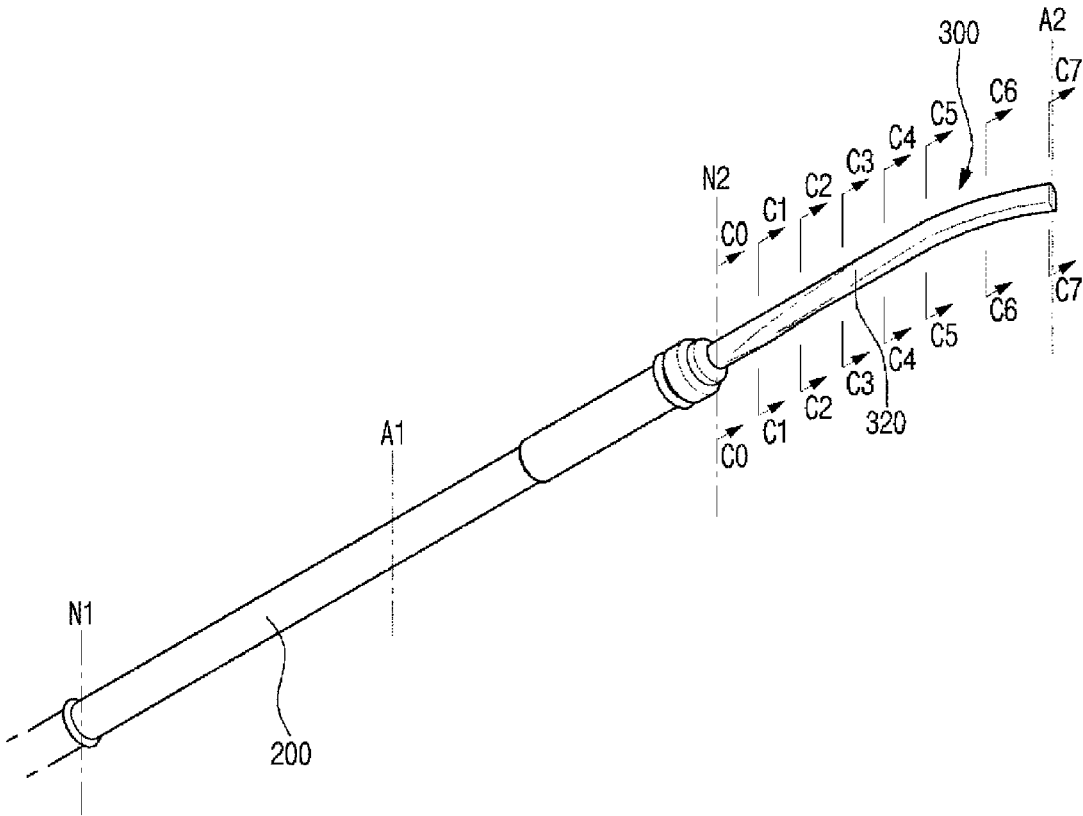
[Fig.1]



[Fig.2]

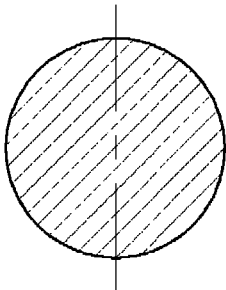


[Fig.3]



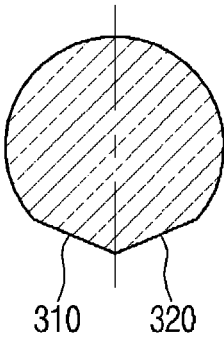
[Fig.4]

300



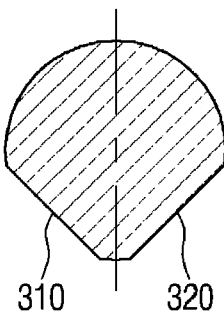
[Fig.5]

300

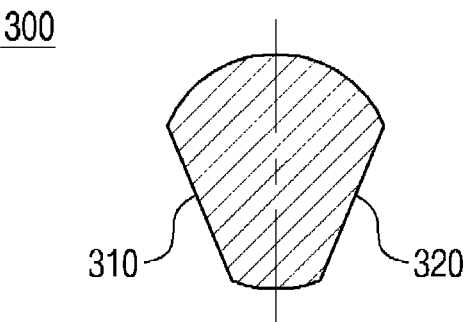


[Fig.6]

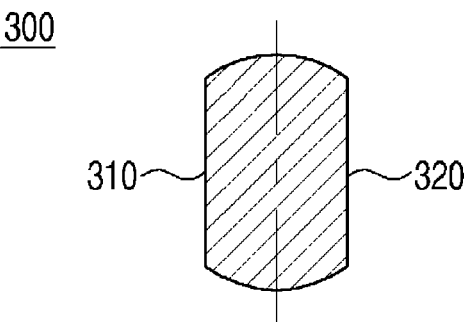
300



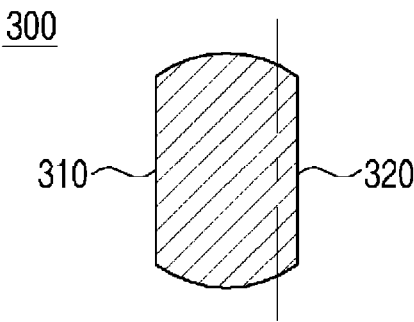
[Fig.7]



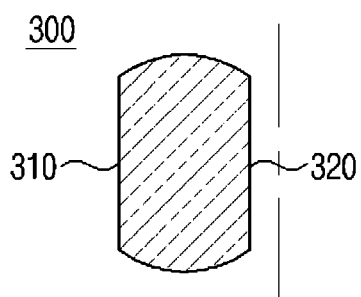
[Fig.8]



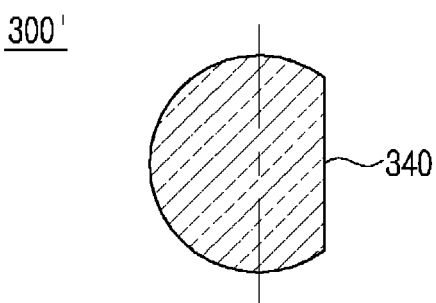
[Fig.9]



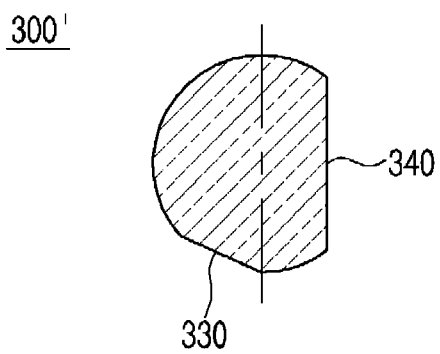
[Fig.10]



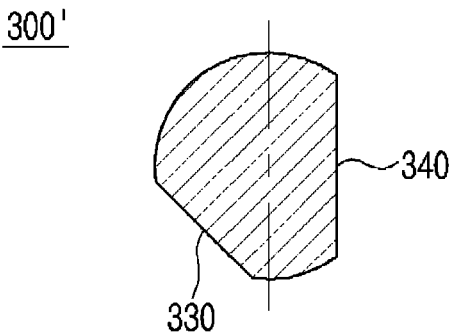
[Fig.11]



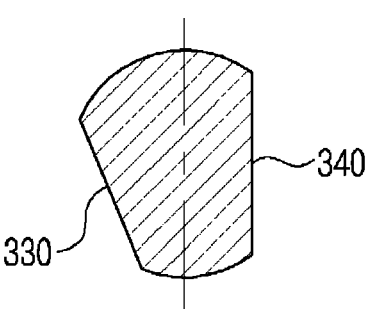
[Fig.12]



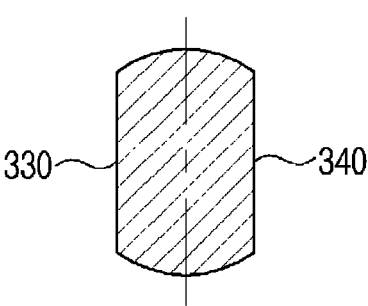
[Fig.13]



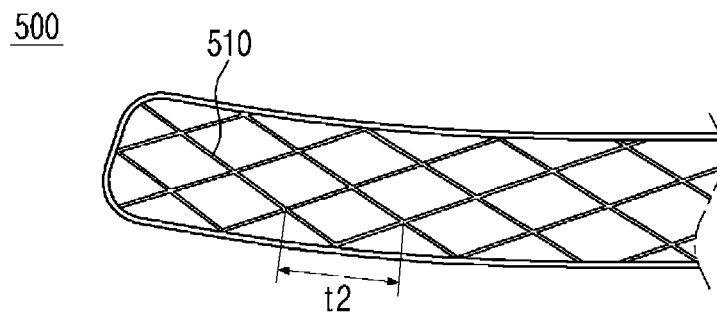
[Fig.14]



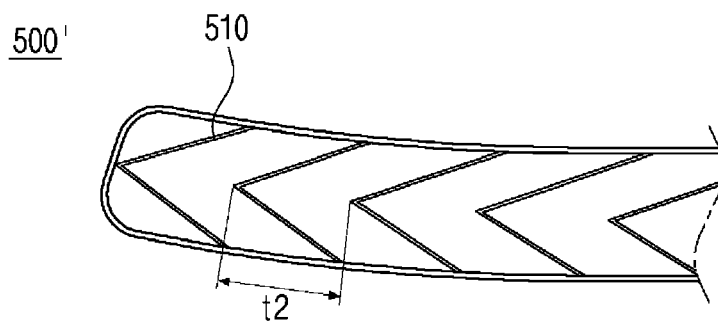
[Fig.15]



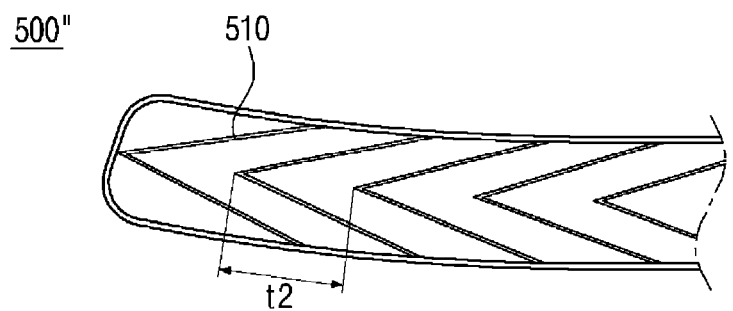
[Fig.16]



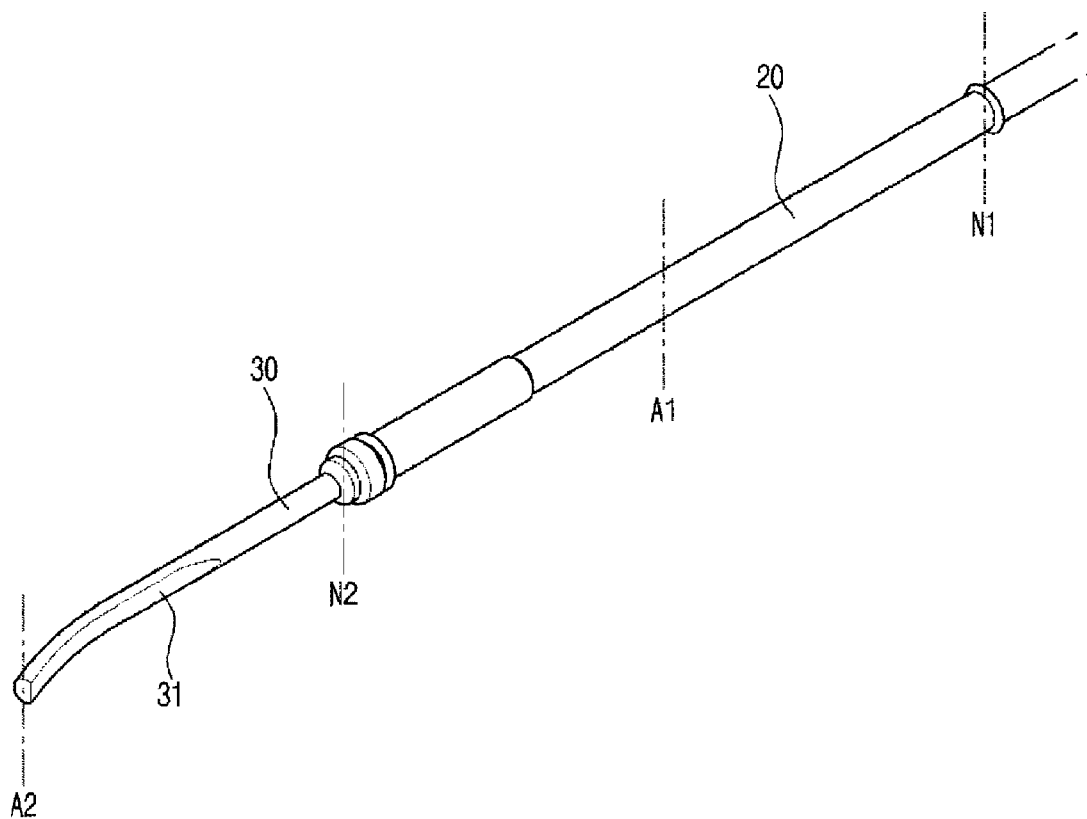
[Fig.17]



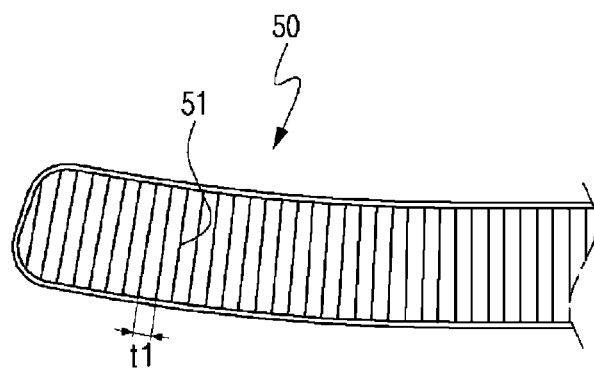
[Fig.18]



[Fig.19]



[Fig.20]



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TOOL FOR SURGICAL OPERATION USING ULTRASONIC WAVES

INCORPORATION BY REFERENCE TO ANY PRIORITY APPLICATIONS

This application is the U.S. National Phase of International Application No. PCT/KR2012/001183, filed Feb. 16, 2012, designating the U.S. and published in Korean as WO 2013/122274 on Aug. 22, 2013, which is hereby incorporated by reference in its entirety.

SUMMARY

The present invention relates to a tool for a surgical operation using ultrasonic waves, and more particularly, to a tool for surgical operation using ultrasonic waves, which can more rapidly and effectively perform cutting and hemostasis by ensuring a maximum active length while maximizing ultrasonic wave strength by ensuring a maximum value of a gain step.

BACKGROUND ART

These days, instruments that perform a surgical operation by using ultrasonic waves have been gradually developed. A representative tool for surgical operation used in laparoscopic surgery among them is Harmonic Scalpel disclosed in Japanese Patent No. 4307890.

However, in the case of the Harmonic Scalpel in the related art, which is disclosed in Japanese Patent No. 4307890, a maximum value which a gain step can have in order to ensure a maximum active length cannot be ensured, and as a result, ultrasonic wave strength cannot be maximized.

That is, in the tool for surgical operation using the ultrasonic waves, such as the Harmonic Scalpel in the related art, the active length and the gain step are determined as contrary components, and as a result, only an instrument performing the surgical operation, which can perform cutting and hemostasis by selecting only any one of both components according to a surgical site has been developed.

DISCLOSURE

Detailed Description of Certain Embodiments

A technical object of the present invention is to provide a tool for surgical operation using ultrasonic waves, which can more rapidly and effectively perform cutting and hemostasis by ensuring a maximum active length while maximizing ultrasonic wave strength by ensuring a maximum value which a gain step can have.

Technical objects to be solved by the present invention are not limited to the aforementioned technical object and other unmentioned technical objects will be clearly understood by those skilled in the art from the following description.

Technical Solution

An exemplary embodiment of the present invention provides a tool for surgical operation using ultrasonic waves, the tool including: a transducer generating ultrasonic waves; a transmitting rod having a cylindrical bar shape and transmitting the ultrasonic waves generated by the transducer to one end portion from the other end portion connected with the transducer; an end effector that extends from one end

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portion of the transmitting rod and cuts a surgical site by using the ultrasonic waves received from the transmitting rod in which a part of a circular cross-section area is formed to be flat from a point corresponding to the second vibration node so that a gain step is started at the second vibration node most adjacent from one end portion of the transmitting rod; a rod cover covering the transmitting rod by using a plurality of vibration nodes formed when the ultrasonic waves are transmitted through the transmitting rod as connection points; and a jaw for holding the surgical site while engaged with the end effector, which is combined to one end portion of the rod cover in a pivotable manner and is positioned to face the end effector.

In this case, an interval corresponding to the gain step may be a distance up to a second vibration anti-node positioned at a position spaced apart by a distance which is $\frac{1}{4}$ larger than the length of a wavelength for one cycle of the ultrasonic waves generated from the transducer in a direction opposite to a direction in which the transducer is connected from the second vibration node.

Here, when a frequency of the ultrasonic waves generated from the transducer is set to 55.5 kHz and the transmitting rod is made of cylindrical titanium, the gain step may become 20 mm and an active length which is cut while contacting the surgical site may become 15 mm.

Meanwhile, a part of the cross-sectional area of the end effector which is flat may be divided into a first surface and a second surface around the center of the other surface of the end effector and both the first surface and the second surface may be provided on the other surface opposite to one surface of the end effector contacting the jaw.

In this case, the first surface and the second surface may be tilted toward both sides between one surface and the other surface of the end effector at the center of the other surface of the end effector in opposite directions to each other.

Further, the first and second surfaces may be consecutively formed in a longitudinal direction which extends from the second vibration node to the second vibration anti-node, and tilts of the first and second surfaces may increase toward the second vibration anti-node.

Further, the first surface and the second surface may be symmetric to each other to have the same area and the same tilt.

Meanwhile, a part of the cross-sectional area of the end effector which is flat may be divided into a third surface and a fourth surface around the center of the other surface of the end effector and the third surface may be provided on the other surface opposite to one surface of the end effector contacting the jaw and the fourth surface may be provided on one side between one surface and the other surface of the end effector.

In this case, the third surface may be tilted toward the other side between one surface and the other surface of the end effector opposite to one side of the end effector where the fourth surface is provided at the center of the other surface of the end effector.

Further, the third surface may be consecutively formed in a longitudinal direction which extends from the second vibration node to the second vibration anti-node, and a tilt of the third surface may increase toward the second vibration anti-node.

Further, the fourth surface may have the same cross-sectional length vertically to the other surface of the end effector and may be consecutively formed in a longitudinal direction that extends from the second vibration node to the second vibration anti-node.

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Meanwhile, the jaw may include a tissue contacting surface and the tissue contacting surface has grooves formed on the tissue contacting surface forming one surface of the end effector at a predetermined interval in order to prevent the surgical site held while engaged with the end effector from being deviated, and the grooves may be angled in a longitudinal direction of the jaw based on a direction vertical to the longitudinal direction of the jaw.

Here, the grooves may be angled at 10° to 80° in the longitudinal direction of the jaw when an angle in the direction vertical to the longitudinal direction of the jaw is 0°.

Furthermore, the grooves may be provided on the inner surface of the jaw in a lattice shape or provided in a symmetric bent shape toward both sides from the center of the inner surface of the jaw.

Meanwhile, the tool may further include an actuating unit controlling the ultrasonic waves generated from the transducer and controlling motions of the rod cover and the jaw, in which the actuating unit may be included in a part of a control unit constituting a computer-integrated robotic surgery system and the motions of the rod cover and the jaw may be complexly automatically controlled together with other tools for surgical operation included in the computer-integrated robotic surgery system.

Advantageous Effects

According to a tool for surgical operation using ultrasonic waves in accordance with the present invention, cutting and hemostasis can be more rapidly and effectively performed by ensuring a maximum active length while maximizing ultrasonic wave strength by ensuring a maximum value which a gain step can have.

DESCRIPTION OF DRAWINGS

FIG. 1 is a perspective view illustrating an exemplary embodiment of a tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 2 is an enlarged perspective view illustrating one end of a transmitting rod and an end effector in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 3 is an enlarged perspective view illustrating one end of the transmitting rod and the end effector in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention in another direction.

FIG. 4 is a cross-sectional view taken along line C0 in FIGS. 2 and 3.

FIG. 5 is a cross-sectional view taken along line C1 in FIGS. 2 and 3.

FIG. 6 is a cross-sectional view taken along line C2 in FIGS. 2 and 3.

FIG. 7 is a cross-sectional view taken along line C3 in FIGS. 2 and 3.

FIG. 8 is a cross-sectional view taken along line C4 in FIGS. 2 and 3.

FIG. 9 is a cross-sectional view taken along line C5 in FIGS. 2 and 3.

FIG. 10 is a cross-sectional view taken along line C6 in FIGS. 2 and 3.

FIG. 11 is a cross-sectional view illustrated to correspond to FIG. 4, when one end of the transmitting rod and the end

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effector are modified in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 12 is a cross-sectional view illustrated to correspond to FIG. 5, when one end of the transmitting rod and the end effector are modified in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 13 is a cross-sectional view illustrated to correspond to FIG. 6, when one end of the transmitting rod and the end effector are modified in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 14 is a cross-sectional view illustrated to correspond to FIG. 7, when one end of the transmitting rod and the end effector are modified in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 15 is a cross-sectional view illustrated to correspond to FIG. 8, when one end of the transmitting rod and the end effector are modified in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 16 is a plan view illustrating an example of one surface of a jaw contacting the end effector in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 17 is a plan view illustrating a modified example of one surface of the jaw contacting the end effector in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 18 is a plan view illustrating another modified example of one surface of the jaw contacting the end effector in the exemplary embodiment of the tool for surgical operation using ultrasonic waves according to the present invention.

FIG. 19 is an enlarged perspective view illustrating one end of a transmitting rod and an end effector in a tool for surgical operation using ultrasonic waves in the related art.

FIG. 20 is a plan view illustrating one surface of a jaw contacting the end effector in the tool for surgical operation using ultrasonic waves in the related art.

Hereinafter, exemplary embodiments of the present invention will be described in detail with reference to the accompanying drawings. However, in describing the present invention, a detailed description of already known functions or configurations will be omitted so as to make the subject matter of the present invention clear.

An exemplary embodiment of a tool for surgical operation using ultrasonic waves according to the present invention is configured to include a transducer 100, a transmitting rod 200, an end effector 300, a rod cover 400, and a jaw 500, as illustrated in FIGS. 1 to 18.

Herein, the transducer 100 is a component generating ultrasonic waves by receiving an electric signal capable of generating the ultrasonic waves from an input terminal 120 (however, in FIGS. 1 to 18, circuits, electric wires, and the like for transmitting a signal between the transducer 100 and the input terminal 120 are not illustrated).

A frequency of the ultrasonic waves generated by the transducer 100 varies depending on conditions of the transmitting rod 200 and the end effector 300 to be described below. That is, the transducer 100 generates optimal ultrasonic waves according to a shape and a material of the transmitting rod 200 or designs of a gain step and an active length which may be generated in the end effector 300.

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For example, if it is designed that the transmitting rod **200** is made of cylindrical titanium, the gain step which may be generated in the end effector **300** is set to approximately 20 mm, and the active length is set approximately 15 mm, the transducer **100** is set to generate ultrasonic waves having a frequency of approximately 55.5 kHz.

Further, the strength (amplitude and displacement) of the ultrasonic waves generated by the transducer **100** may be controlled through a second switch **630** to be described below by considering a surgical site to be cut.

For example, in the case where the surgical site is a portion which is formed by a thick tissue or through which blood vessels pass, the strength of the ultrasonic waves is controlled to increase and in other portions, the strength of the ultrasonic waves is controlled to decrease so as to prevent the operation from being disturbed by a by-product generated upon cutting.

Meanwhile, the transmitting rod **200** serves to transmit the ultrasonic waves generated by the transducer **100** to the end effector **300** by connecting the transducer **100** and the end effector **300**.

The transmitting rod **200** may have a cylindrical bar shape which is thin and long so that the end effector **300** is inserted into a hole formed in a trocar used in laparoscopic surgery to reach the surgical site.

In this case, the length of the transmitting rod **200** may be a length suitable for a user to perform the laparoscopic surgery, but may be a length which is as large as a vibration node (means a point where the strength of the ultrasonic waves is substantially 0) of the ultrasonic waves generated by the transducer **100** and a vibration anti-node (means a point where the strength of the ultrasonic waves is substantially maximum as a concept contrary to the vibration node) may be repeated multiple times. Further, it is apparent that a fact that an interval corresponding to the gain step of the end effector **300** according to the present invention may become a distance corresponding to a cycle which is $\frac{1}{4}$ as long as the ultrasonic waves should be considered as described below.

In addition, the transmitting rod **200** may be made of various materials, but as illustrated above, the transmitting rod **200** may be advantageously made of a titanium material in order to effectively transmit the frequency of 55.5 kHz generated by the transducer **100**.

Meanwhile, the end effector **300** is configured to perform cutting or hemostasis of the surgical site by using the ultrasonic waves and the end effector **300** is provided at one end portion of the transmitting rod **200** to perform cutting or hemostasis of a surgical site by receiving the ultrasonic waves generated by the transducer **100**.

Since the end effector **300** uses the ultrasonic waves, the end effector **300** need not be unconditionally sharp unlike general cutting tools. That is, the end effector **300** is formed to perform cutting or hemostasis of the surgical site by using vibration energy and thermal energy generated by the ultrasonic waves, and as a result, the end effector **300** is effective in cutting or performing hemostasis of the surgical site through which the blood vessels pass.

For example, the end effector **300** may be formed to extend from one end portion of the transmitting rod **200** as illustrated in FIGS. 1 to 18 and the end effector **300** may cut the surgical site with the vibration energy and the thermal energy by compressing the surgical site together with a jaw **500** to be described below, which is provided at an opposite thereto.

Since the end effector **300** should be able to cut the surgical site by using the ultrasonic waves received from the

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transmitting rod **200**, the end effector **300** should have the gain step (means that amplification rate is substantially 1 or more).

In this case, the shape and the structure of the end effector **300** may be diversified as a method for the end effector **300** to have the gain step, and in the present invention, a dimension of a transverse cross-sectional area of the end effector **300** is smaller than that in the vibration node to amplify energy of the ultrasonic waves according to a transverse cross-sectional area ratio. Accordingly, when the end effector **300** is formed to extend from the transmitting rod **200**, a cross-sectional area is decreased by flattening a part of a circular cross-sectional area to form the gain step.

Meanwhile, in forming the end effector **300**, it is important as much as the end effector **300** is formed to have the gain step is how large active length the end effector **300** has. That is, in the end effector **300**, although the gain step is formed to amplify the energy of the ultrasonic waves, if the active length is small, in other words, if the ultrasonic waves may not have strength to substantially cut the surgical site, the end effector **300** is meaningless to the user who intends to cut the surgical site.

In order to ensure the active length having the important meaning, a point where the gain step is started and the vibration node are configured to be spaced apart from each other by 5% or more so as to maximally ensure the active length as illustrated in FIG. 19 in the related art. (In this case, a description of the tool for surgical operation using the ultrasonic waves in the related art is not contents mentioned in Japanese Patent No. 4307890 mentioned in Background Art, but the description is contents which can be apparently verified from a product widely used by doctors who actually perform the surgical operation.)

That is, in the tool for surgical operation using the ultrasonic waves in the related art, the cross-sectional area of even the end effector **30** is decreased by flattening a part of the circular cross-sectional area to form the gain step, but the point where the gain step is started and the vibration node is configured to be spaced apart from each other by a distance therebetween of 5% or more.

Accordingly, in the tool for surgical operation using the ultrasonic waves in the related art, in the end effector **300**, a point where the gain step is ended may not be formed up to a point which a maximum amplitude (displacement) of the ultrasonic waves shown in the vibration anti-node reaches and this represents that a maximum value of the gain step is abandoned in order to ensure the maximum active length.

However, in the exemplary embodiment of the tool for surgical operation using the ultrasonic waves according to the present invention, the end effector **300** is configured so that the maximum active length may be ensured while ensuring the maximum value of the gain step by making the point where the gain step is started coincide with the vibration node.

That is, in the exemplary embodiment of the tool for surgical operation using the ultrasonic waves according to the present invention, if the end effector **300** is configured as described below, an interval corresponding to the gain step and a length corresponding to the maximum active length may similarly be a distance up to a second vibration anti-node **A2** positioned at a position spaced apart by a distance which is $\frac{1}{4}$ larger than the length of a wavelength for one cycle of the ultrasonic waves generated from the transducer **100** in a direction opposite to a direction in which the transducer **100** is connected from a second vibration node **N2**.

First, when one example of the end effector **300** illustrated in FIGS. **2** to **10** is described, a part of a flat cross-sectional area of the end effector **300** may be configured to be divided into a first surface **310** and a second surface **320** around the center of the other surface (an opposite surface to one surface of the end effector **300** contacting the jaw **500**) of the end effector **300**.

Herein, both the first surface **310** and the second surface **320** may be provided on the other surface of the end effector **300** and the first and second surfaces **310** and **320** may be tilted toward both sides between one surface and the other surface of the end effector **300** at the center of the other surface of the end effector **300** in opposite directions to each other, similarly as a shape of the bottom of a ship.

In this case, the first and second surfaces **310** and **320** may be consecutively formed in a longitudinal direction which extends from the second vibration node **N2** to the second vibration anti-node **A2**, and may be configured in such a manner that a slope increases toward the second vibration anti-node **A2**.

In more detail, the first and second surfaces **310** and **320** are constituted as one same surface at the center of the other surface of the end effector **300** as illustrated in FIG. **4** in the second vibration node **N2**, but the first and second surfaces **310** and **320** are configured to be gradually largely tilted toward both sides at the center of the other surface of the end effector **300** as illustrated in FIGS. **5** to **7** toward the second vibration anti-node **A2**.

The first and second surfaces **310** and **320** configured as above may be configured in parallel to each other as illustrated in FIGS. **8** to **10** when the first and second surfaces **310** and **320** are adjacent to the second vibration anti-node **A2** and although a part of the end effector **300** adjacent to the vibration anti-node **A2** is curved for convenience of the surgery, the first and second surfaces **310** and **320** may maintain the same shape without a change in configuration thereof.

Further, the first surface **310** and the second surface **320** may be symmetric to each other so as to have the same area and the same tilt. In this case, although the first surface **310** and the second surface **320** are configured to be asymmetric to each other, the first surface **310** and the second surface **320**, of course, do not depart from the scope of the present invention and in the case where the first surface **310** and the second surface **320** are configured to be symmetric to each other, the ultrasonic waves will better proceed to one surface of the end effector **300** contacting the jaw **500**.

Subsequently, when a modified example of the end effector **300** illustrated in FIGS. **11** to **15** is described, a part of the flat cross-sectional area of the end effector **300** may be configured to be divided into a third surface **330** and a fourth surface **340** around the center of the other surface (an opposite surface to one surface of the end effector **300** contacting the jaw **500**) of the end effector **300**.

Herein, the third surface **330** is a surface provided on the other surface of the end effector **300** contacting the jaw **500** and the fourth surface **340** is a surface provided on one side between one surface and the other surface of the end effector **300**.

In more detail, the third surface **330** is a surface that is tilted toward the side of the end effector **300** at the center of the other surface of the end effector **300** similarly as the first surface **310** of one example of the end effector **300** illustrated in FIGS. **2** to **10** as described above and is consecutively formed with the tilt increased toward the second vibration anti-node **A2** from the second vibration node **N2**.

However, the fourth surface **340** is a surface that has the same cross-sectional length vertically to the other surface of the end effector **300** unlike one example of the end effector **300** illustrated in FIGS. **2** to **10** as described above and is consecutively formed without a change in tilt up to the second vibration anti-node **A2** from the second vibration node **N2**.

That is, as verified from FIGS. **11** to **15**, the modified example of the end effector **300** is configured to be consecutively formed from the second vibration node **N2** to the second vibration anti-node **A2** with the change in slope on only one side between both sides between one surface and the other surface of the end effector **300**.

In this case, one side whose tilt is changed, that is, the third surface **330** may be one side in a direction corresponding to a direction in which a part of the end effector **300** adjacent to the second vibration anti-node **A2** bent for the convenience of the surgery, but the present invention is not limited thereto.

When the modified example of the end effector **300** is configured as above, the modified example is just different from one example of the end effector **300** illustrated in FIGS. **2** to **10** as described above in regarding whether the ultrasonic waves better proceeding to one surface of the end effector **300** contacting the jaw **500** and both examples are not different from each other in providing the tool for surgical operation using the ultrasonic waves, which can more rapidly and effectively perform cutting and hemostasis by ensuring the maximum active length while maximizing the strength of the ultrasonic waves by ensuring the maximum value of the gain step which is the technical object to be solved by the present invention.

Meanwhile, the rod cover **400** is configured to cover the transmitting rod **200** in order to protect transmitting of the ultrasonic waves through the transmitting rod **200**.

It is preferable that the rod cover **400** does not contact the transmitting rod **200**, but the rod cover **400** needs to be connected while contacting the transmitting rod **200** in the case where the transmitting rod **200** is long. In this case, any point is not used as a connection point, but it is preferable that a plurality of vibration nodes (for example, the second vibration node **N2** and the first vibration node **N1**) where the ultrasonic waves are formed through the transmit node **200** is used as the connection point.

The reason is that in terms of a non-vibration node, since the intensity is not 0 (zero), and in terms of the non-vibration node, when the transmitting rod **200** and the rod cover **400** are connected to each other, a small amount of ultrasonic waves transmitted through the transmitting rod **200** is transmitted to the rod cover **400** to be lost.

Meanwhile, the jaw **500** is disposed at the position facing the end effector **300** to serve to hold the surgical site while engaged with the end effector **300**.

If there is no jaw **500**, there is no component supported when the end effector **300** is pushed in order to cut the surgical site, and as a result, the surgical site is pushed out and may not be cut well. That is, the jaw **500** is a configuration to cut the surgical site by assisting the end effector **300**.

The jaw **500** playing the role may be configured to be coupled with the transmitting rod **200**, but since the transmission of the ultrasonic waves to the end effector **300** may be interrupted, the jaw **500** is advantages to be configured to be coupled with one end of the rod cover **400**.

Further, in order to easily hold or release the surgical site, the jaw **500** may be configured to be pivotably coupled with

the rod cover **400**, and may be configured to be interlocked with the first switch **620** so as to be easily controlled by the user.

In addition, the jaw **500** may have grooves **510** formed on the inner surface facing one surface of the end effector **300** at predetermined intervals, so as to prevent the surgical site held while engaged with the end effector **300** from being deviated.

In this case, the grooves **510** may be configured to be angled in a longitudinal direction of the jaw **500** based on a vertical direction to the longitudinal direction of the jaw **500**.

That is, in the jaw **500**, when a parallel direction with the direction in which the second vibration node **N2** and the second vibration anti-node **A2** are connected to each other is referred to as the longitudinal direction, if a slope in the vertical direction to the longitudinal direction is 0° , the grooves **510** may be formed to be angled at a predetermined angle in the longitudinal direction of the jaw **500**.

In other words, when the predetermined angle is small, the grooves **510** may be formed in the vertical direction to the longitudinal direction of the jaw **500**, and when the predetermined angle is large, the grooves **510** may be formed in the longitudinal direction of the jaw **500**.

In this case, since the shape of the inner surface of the jaw **500** is close to a rectangle, the range of the predetermined angle may be 0° to 90° . However, as illustrated in FIG. **20** described below, in order to verify the difference on the effect from the grooves **51** formed on the inner surface of the jaw **500** of the tool for surgical operation using the ultrasonic waves in the related art, the angle needs to be 10° or more, and in order that the held surgical site is not slid in a holding direction, the angle is advantageously 80° or smaller.

As such, when the grooves **510** are angled at the predetermined angle, the grooves **510** may not be limited to the shapes thereof. However, for example, referring to the drawing for more detailed description, the grooves **510** may have a grid shape on the inner surface of the jaw **500** as illustrated in FIG. **16**.

The end effector **300** and the jaw **500** have an advantage of increasing the holding force when holding the surgical site, but grooves **510** having the shape has a difficulty to manufacture, and may have a shape of a modified example illustrated in FIG. **17** or FIG. **18**. That is, as illustrated in FIG. **17** or FIG. **18**, grooves **510'** and **510''** may have a symmetric bent shape toward both sides from the center of the inner surface of the jaw **500**.

When the jaw **500** is configured as described above, it is possible to solve a problem that may be generated when the surgical site is held by the jaw **500** of the tool for surgical operation using the ultrasonic waves in the related art having the grooves **51** as illustrated in FIG. **20**.

That is, when the surgical site is held by the jaw **500** of the tool for surgical operation using the ultrasonic waves in the related art having the grooves **51** as illustrated in FIG. **20**, the held surgical site may be aggregated in a holding direction to interrupt the end effector **300** cutting and cauterizing the surgical site.

However, when the surgical site is held by the jaw **500** of the tool for surgical operation using the ultrasonic waves according to the present invention, the held surgical site may be aggregated in a both side direction of the jaw **500**, not the holding direction not to interrupt the end effector **300** cutting and cauterizing the surgical site, and as a result, the surgical site may be more rapidly and effectively cut and cauterized.

In addition, since the tool for surgical operation using the ultrasonic waves in the related art does not ensure a maximum value of a gain step in order to ensure a maximum

operation length, only when the holding force of the surgical site between the end effector **300** and the jaw **500** is large, the cutting and cauterizing may be performed. As a result, as illustrated in FIG. **20**, the holding force needs to be increased by making an interval **t1** of the grooves **51** dense.

However, while ensuring the maximum operation length, the tool for surgical operation using the ultrasonic waves according to the present invention ensures the maximum value of the gain step, and as a result, the holding force may be small as compared with the tool for surgical operation using the ultrasonic waves in the related art, thereby increasing an interval **t2** of the grooves **510**.

As such, when the interval **t2** of the grooves **510** is increased, it is natural to require smaller efforts and costs when manufacturing the inner surface of the jaw **500**.

Meanwhile, an actuating unit **600** is a component to control the transducer **100** and adjust the motion of the rod cover **400** and the jaw **500**, and may be variously configured according to convenience of the user.

For example, in the exemplary embodiment of the tool for surgical operation using the ultrasonic waves according to the present invention, the actuating unit **600** may be configured by a handle **610**, a first switch **620**, a second switch **630**, and a third switch **640**.

Here, the handle **610** may be configured to be similar to a grip of a handgun so as the user to easily perform the operation by holding the tool for surgical operation using the ultrasonic waves according to the present invention with one hand and bringing the end effector **300** at the surgical site.

Further, the first switch **620** may be configured to turn on/off the transducer **100** to generate the ultrasonic waves and move the jaw **500** to hold and cut the surgical site together with the end effector **300**.

Further, the second switch **630** may be configured to control the intensity of the ultrasonic waves generated from the transducer **100**, and the third switch **640** may be configured to rotate the rod cover **400** for an index finger of the user to rotate the end effector **300** or/and the jaw **500**.

Meanwhile, the tool for surgical operation using the ultrasonic waves according to the present invention is directly used by hand power when the user operates, but the present invention is not limited thereto, and it is natural that the present invention may be extended and used in an automatic robot in which the tool for surgical operation is installed.

In more detail, for example, the actuating unit **600** may be considered to be included in a part of a control unit (not illustrated) constituting a computer-integrated robotic surgery system, and as such, in the case of constituting the actuating unit **600**, the actuating unit **600** needs not to be configured by the handle **610**, the first switch **620**, the second switch **630**, and the third switch **640**.

That is, when the actuating unit **600** is included in the part of the control unit (not illustrated) constituting the computer-integrated robotic surgery system, the motion of the rod cover **400** and the jaw **500** may be complexly automatically controlled together with other tools for surgical operation included in the computer-integrated robotic surgery system.

Although the specific exemplary embodiments have been described and illustrated as above, the present invention is not limited to the exemplary embodiments described herein, and it would be apparent to those skilled in the art that various changes and modifications might be made to these exemplary embodiments without departing from the spirit and the scope of the invention. Accordingly, the changed example and modified examples should not be individually

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appreciated from the technical spirit or the viewpoint of the present invention and it should be appreciated that modified exemplary embodiments will be included in the appended claims of the present invention.

What is claimed is:

1. A tool for surgical operation using ultrasonic waves, the tool comprising:

a transducer generating ultrasonic waves;
a transmitting rod having a cylindrical bar shape and transmitting the ultrasonic waves generated by the transducer to a distal end portion from a proximal end portion connected with the transducer;

an end effector that extends from the distal end portion of the transmitting rod configured to perform cutting or hemostasis of a surgical site by using the ultrasonic waves received from the transmitting rod, wherein:

a cross-sectional area of the end effector is substantially circular at a proximal portion adjacent the distal end of the transmitting rod;

two symmetrical, non-parallel flat indentations extend longitudinally along the end effector from a point corresponding to a second vibration node to a point corresponding to a second vibration anti-node; and

an angle between the symmetrical, non-parallel flat indentations decreases as the flat indentations extend longitudinally from the second vibration node to the second vibration anti-node until the flat indentations are parallel and disposed on opposite sides of the end effector at the second vibration anti-node, such that the cross-sectional area of the end effector decreases from the second vibration node to the second vibration anti-node;

a rod cover covering the transmitting rod; and

a jaw for holding the surgical site while engaged with the end effector, which is combined to one end portion of the rod cover in a pivotable manner and is positioned to face the end effector.

2. The tool of claim 1, wherein when a frequency of the ultrasonic waves generated from the transducer is set to 55.5 kHz and the transmitting rod is made of titanium, a gain step is 20 mm and an active length which will cut while contacting the surgical site is 15 mm.

3. The tool of claim 1, wherein the symmetrical, non-parallel flat indentations are provided on a surface opposite to a surface facing the jaw at the second vibration node and gradually rotate longitudinally to surfaces to sides of the surface facing the jaw at the second vibration anti-node.

4. The tool of claim 1, wherein the jaw includes a tissue contacting surface comprising grooves formed on the tissue contacting surface forming one surface of the end effector at a predetermined interval in order to prevent the surgical site held while engaged with the end effector from being deviated and the grooves are angled in a longitudinal direction of the jaw based on a direction vertical to the longitudinal direction of the jaw.

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5. The tool of claim 4, wherein the grooves are angled at 10° to 80° in the longitudinal direction of the jaw when an angle in the direction vertical to the longitudinal direction of the jaw is 0°.

6. The tool of claim 5, wherein the grooves are provided on the inner surface of the jaw in a lattice shape or provided in a symmetric bent shape toward both sides from the center of the inner surface of the jaw.

7. The tool of claim 1, further comprising:

an actuating unit controlling the ultrasonic waves generated from the transducer and controlling motions of the rod cover and the jaw.

8. A tool for surgical operation using ultrasonic waves, the tool comprising:

a transducer generating ultrasonic waves;

a transmitting rod having a cylindrical bar shape and transmitting the ultrasonic waves generated by the transducer to a distal end portion from a proximal end portion connected with the transducer;

an end effector that extends from the distal end portion of the transmitting rod configured to perform cutting or hemostasis of a surgical site by using the ultrasonic waves received from the transmitting rod, wherein:

a cross-sectional area of the end effector is substantially circular at a proximal portion adjacent the distal end of the transmitting rod;

two asymmetrical, non-parallel flat indentations extend longitudinally along the end effector from a point corresponding to a second vibration node to a point corresponding to a second vibration anti-node;

the non-parallel, asymmetrical flat indentations include a first surface opposite to a surface facing a jaw and a second surface on a side disposed between the first surface and the surface facing the jaw;

an angle of the first surface with respect to the second surface decreases as the first surface extends longitudinally from the second vibration node to the second vibration anti-node; and

an angle of the second surface is unchanged from the second vibration node to the second vibration anti-node;

a rod cover covering the transmitting rod; and

wherein the jaw is for holding the surgical site while engaged with the end effector, which is combined to one end portion of the rod cover in a pivotable manner and is positioned to face the end effector.

9. The tool of claim 8, wherein the first surface gradually rotates longitudinally from the surface opposite the surface facing the jaw at the second vibration node to a surface on a side opposing the second surface at the second vibration anti-node.

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