

(19)



(11)

**EP 2 848 214 A1**

(12)

**EUROPEAN PATENT APPLICATION**

(43) Date of publication:  
**18.03.2015 Bulletin 2015/12**

(51) Int Cl.:  
**A61B 17/32** <sup>(2006.01)</sup> **A61B 17/16** <sup>(2006.01)</sup>  
**A61B 17/14** <sup>(2006.01)</sup>

(21) Application number: **14176285.6**

(22) Date of filing: **02.12.2005**

(84) Designated Contracting States:  
**AT BE BG CH CY CZ DE DK EE ES FI FR GB GR  
HU IE IS IT LI LT LU LV MC NL PL PT RO SE SI  
SK TR**

(30) Priority: **02.12.2004 GB 0426503**

(62) Document number(s) of the earlier application(s) in  
accordance with Art. 76 EPC:  
**05814086.4 / 1 876 978**

(71) Applicant: **ORTHOSONICS LIMITED**  
**Ashburton,**  
**South Devon TQ13 7JX (GB)**

(72) Inventor: **Young, Michael**  
**Devon, TQ13 7JX (GB)**

(74) Representative: **Dauncey, Mark Peter**  
**Marks & Clerk LLP**  
**1 New York Street**  
**Manchester, M1 4HD (GB)**

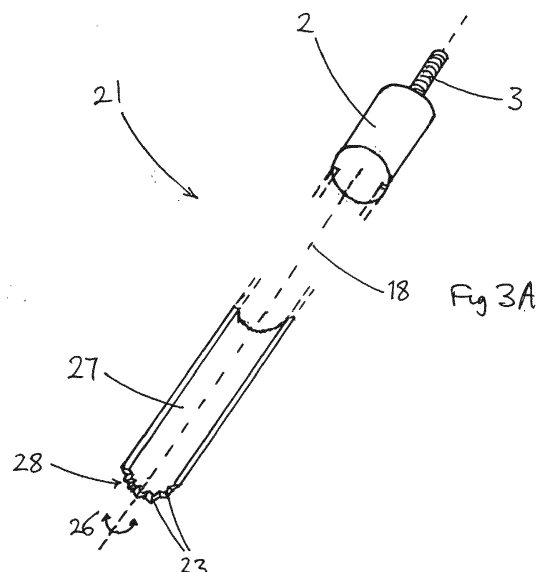
Remarks:

This application was filed on 09-07-2014 as a  
divisional application to the application mentioned  
under INID code 62.

(54) **Improved osteotome**

(57) A tool (1, 31) for cutting bone comprises an elongate blade (7, 37) connectable to a generator of longitudinal-mode ultrasonic vibrations. The blade (7, 37) has two lateral cutting edges (9, 10) linked by a rounded distal tip (8). A series of triangular teeth (13) extends along each cutting edge (9, 10) and the distal tip (8). The blade (37) may taper towards each cutting edge (9, 10) and the distal tip (8). A variant of the tool (21) comprises an elongate

gate part-cylindrical blade (27) connectable to a generator of torsional-mode ultrasonic vibrations. The blade (27) has a cutting edge at its distal tip (28) provided with a plurality of triangular teeth (23). All forms of the tool (1, 21, 31) are particularly suitable for cutting cancellous bone around an implant to be removed during revision of a joint arthroplasty.



**EP 2 848 214 A1**

## Description

**[0001]** The present invention relates to a tool for cutting into or through bone, for example during orthopaedic surgery. More particularly, but not exclusively, it relates to a tool for cutting through cortical or cancellous bone, for example to separate a joint prosthesis from surrounding bone as part of a revision procedure.

**[0002]** A frequently required procedure in orthopaedic surgery is revision of a joint arthroplasty, for example revision of a hip joint replacement, should an implanted prosthesis break or wear unacceptably over its articulating surface. The invention will be described in relation to its use in hip joint revision, but is equally applicable to other joints and the terms "hip", "pelvis" and "femur" may be replaced as necessary. In many cases, an implanted prosthesis is secured in a cavity within a bone, such as a femur, using polymeric organic cement such as polymethylmethacrylate. Tools have been devised to soften and remove this cement and to allow convenient removal of a worn or damaged prosthesis, followed by implantation of a replacement.

**[0003]** However, there has been a recent increase in the use of press-fit prostheses. No cement is used to hold these in place within the femur, pelvis, etc. Instead, the implanted portions of the prostheses have porous surfaces or surfaces coated with hydroxy-apatite, which encourage ingrowth of bone, leading to stable, well-anchored implants. This formation of cancellous bone may also occasionally occur with cement-anchored implants. While not as strong as the structural bone of the wall of the femur, the pelvis or other bone, cancellous bone is not easily susceptible to cutting using the tools devised for revising cement-anchored implants, and it has become necessary to attack cancellous bone mechanically in order to revise such implants.

**[0004]** Furthermore, in order to remove a prosthesis, it may be necessary to remove portions of cortical bone, which cannot be achieved without using mechanical means.

**[0005]** A manual osteotome is effectively a specialised form of chisel, which is forced longitudinally through the bone between a prosthesis and surrounding structural bone. The force required can be so great as to compromise the directional accuracy of the technique, and may thereby damage surrounding structural bone, especially if it is weakened by osteoporosis or the like.

**[0006]** Another approach is to use powered burrs to drill out the bone. These may also be difficult to guide accurately, and flexure in their elongate rotating drive shafts may lead to unacceptable collateral damage in surrounding structural bone. This approach also produces inconveniently large quantities of bone swarf, which must be removed to allow clear visualisation of the point at which the burr is cutting. Furthermore, high-speed burrs lead to significant localised frictional heating, which may also harm adjacent bone, tissue or marrow.

**[0007]** Manual sawing through bone is a slow, tiring

process, also leading to localised heating and copious bone swarf. In any case, conventional bone saws could not easily be inserted or operated between a hip or other joint prosthesis shaft and an inner wall of a femur, or between a part-spherical acetabular shell and a pelvic bone, for example.

**[0008]** It is hence an object of the present invention to provide a tool for cutting bone, particularly bone adjacent an arthroplasty implant, that obviates the above disadvantages and allows accurate, rapid and convenient removal of such implants as part of a revision procedure.

**[0009]** According to a first aspect of the present invention, there is provided a tool for cutting bone comprising a means of generating ultrasonic vibrations, elongate blade means operatively connectable thereto and having at least one cutting edge provided with a plurality of serrations each having a first cutting facet substantially transverse to the direction of said ultrasonic vibrations.

**[0010]** In a first embodiment, the tool is adapted to be vibrated by longitudinal mode ultrasonic vibrations, for example directed substantially parallelly to a longitudinal axis of the blade means.

**[0011]** Preferably, the blade means then comprises an elongate substantially planar member having two substantially oppositely-facing lateral edges.

**[0012]** Advantageously, said lateral edges each extend substantially parallelly to the longitudinal axis of the blade means.

**[0013]** The elongate member may further comprise a rounded distal tip.

**[0014]** Said distal tip may extend between a distal end of a first said lateral edge and a distal end of a second said lateral edge.

**[0015]** Preferably, the cutting edge extends along at least part of a respective one of said lateral edges.

**[0016]** Advantageously, the cutting edge extends along at least part of each said lateral edge.

**[0017]** The cutting edge may extend around all or part of the rounded distal tip.

**[0018]** A continuous cutting edge may extend around at least a distal portion of each lateral edge and the distal tip extending therebetween.

**[0019]** Preferably, at least part of the blade means has a cross-sectional profile tapering towards one or each lateral edge.

**[0020]** Advantageously, the blade means has a cross-sectional profile adjacent its distal tip tapering towards said tip.

**[0021]** Said tapering profile may comprise at least one angled surface located on each opposite face of the blade means.

**[0022]** A single angled surface may extend adjacent each lateral edge and the distal tip on each said face.

**[0023]** Said angled surfaces may be connected at their respective outer peripheries by an edge surface extending transversely to the general plane of the blade member.

**[0024]** Said edge surface may be substantially narrow-

er than an overall thickness of the blade means.

[0025] Preferably, said tapering profile is at least co-extensive with the cutting edge of the blade means.

[0026] Preferably, each serration of the or each cutting edge is generally triangular.

[0027] Each serration may have the first, cutting facet extending generally orthogonally to a local alignment of the cutting edge.

[0028] Each serration may then have a second, angled facet extending obliquely to said local alignment.

[0029] Each pair of neighbouring serrations may be so relatively aligned that a first facet of one serration of said pair is adjacent a second facet of the next serration of said pair.

[0030] Each first facet of a first lateral cutting edge may face towards a distal tip of the blade means and each first facet of a second opposite lateral cutting edge may then face towards a proximal root of the blade means.

[0031] Preferably, each serration extends outwardly from the cutting edge, substantially in the plane of the elongate member.

[0032] In a second embodiment, the tool is adapted to be vibrated by torsional mode ultrasonic vibrations.

[0033] The blade means then preferably comprises an elongate member having a curved cross-section, optionally substantially comprising an arc of a circle.

[0034] Advantageously, said cross-section is substantially constant along a whole of the elongate member.

[0035] The tool may be so adapted as to be torsionally vibratable about an longitudinal axis extending through the centre of said circle.

[0036] Preferably, a distal tip of the elongate member comprises the cutting edge of the tool.

[0037] The serrations of the cutting edge may be generally triangular.

[0038] The serrations may extend distally from the tip of the member.

[0039] A portion of the elongate member adjacent its tip may taper longitudinally towards said tip.

[0040] The tapered portion may comprise an angled surface located on a concave face of a curved elongate member.

[0041] In each embodiment, the generator means is advantageously adapted to generate ultrasonic vibrations at a frequency within the range of twenty to seventy-five kilohertz.

[0042] According to a second aspect of the present invention, there is provided a method of cutting bony material comprising the steps of providing a tool as described in the first aspect above, applying a cutting edge of the tool to a surface of bony material to be cut, causing the tool to vibrate at an ultrasonic frequency and drawing the cutting edge of the tool across said surface.

[0043] Preferably, the cutting edge is drawn reciprocally across said surface.

[0044] Advantageously, the bony material comprises cancellous and/or cortical bone holding an orthopaedic implant to a bone of a living body, and the method com-

prises the step of cutting the bone as described above until the implant is separable therefrom.

[0045] Embodiments of the present invention will now be more particularly described by way of example and with reference to the accompanying drawings in which:

**Figure 1** is a perspective view of a first tool embodying the present invention;

**Figure 2A** is a plan view of a distal portion of the tool shown in Figure 1;

**Figure 2B** is a schematic plan view of an intermediate part of the distal portion shown in Figure 2A;

**Figure 3A** is a partial perspective view of a second tool embodying the present invention;

**Figure 3B** is an elevation of a distal end of the tool shown in Figure 3A;

**Figure 4** is a perspective view of a third tool embodying the present invention;

**Figure 5** is a cross-sectional elevation of a blade of the tool shown in Figure 4, taken along the line V - V; and

**Figure 6** is a cross-sectional elevation of a blade of the tool shown in Figure 4, taken along the line VI - VI.

[0046] Referring now to the Figures and to Figure 1 in particular, a first osteotomy tool 1 comprises a cylindrical connecting body 2 provided at a proximal end with a threaded spigot 3, by which the tool 1 may detachably be connected to a generator of ultrasonic vibrations (not shown). An elongate blade portion 4 of the tool 1 extends from a distal end of the connecting body 2, and is aligned generally coaxially therewith.

[0047] The blade portion 4 comprises a proximal blade root 5 having a substantially rectangular cross-section and linked by a tapered portion 6 to a thin, flat elongate blade 7 with a generally rounded distal tip 8. A distal portion of the blade 7 has two oppositely-facing lateral cutting edges 9, 10. Each of the lateral cutting edges 9, 10 and the tip 8 is provided with a plurality of teeth 13, as shown in more detail in Figures 2A and 2B. A proximal portion of the blade 7 is toothless, although the relative lengths of the toothed and toothless portions may vary from that shown.

[0048] The cylindrical connecting body 2 is provided with spanner flats 11 to allow application of tightening torque sufficient to bring the tool 1 into secure contact with the ultrasound generator, allowing effective vibrational coupling through a contact surface 12 of the body 2. The tool 1 is preferably made of titanium or stainless steel.

[0049] As Figures 2A and 2B illustrate, the teeth 13 of the blade 7 are preferably shaped generally as conventional saw teeth, having a first edge 14 substantially orthogonal to a longitudinal axis of the blade 7 and a second edge 15 at a relatively shallow angle thereto. In a conventional saw, the first edge 14 would be sharpened, and the saw would cut when pulled (or sometimes pushed) in a longitudinal direction in which the first edge 14 is a

leading edge of the tooth 13. In the present invention, it is believed to be unnecessary to sharpen the teeth 13.

**[0050]** In the tool 1 shown, the teeth 13 extend in a continuous array along a first cutting edge 9, around the tip 8 and along a second cutting edge 10, without the relative dispositions of the first and second edges 14, 15 of the teeth 13 changing. Thus, the first cutting edge 9 is adapted to cut on a longitudinal pull stroke as indicated by arrow 16 and the second cutting edge 10 is adapted to cut on a longitudinal push stroke as indicated by arrow 17.

**[0051]** Were the tool 1 a conventional mechanical saw, this arrangement would not be particularly effective, a push cut being particularly difficult to control in direction or force. Manual sawing at bone, even cancellous bone, produces significant frictional heating and requires considerable effort on the part of the user.

**[0052]** However, when the blade 7 is subjected to longitudinal mode ultrasonic vibrations, directed parallelly to the longitudinal axis 18 of the tool 1, the effectiveness of both the pull stroke 16 and the push stroke 17 is greatly improved. The velocity amplitude of the first edge 14 of each tooth 13 as it contacts the bone is much greater than the speed of the stroke 16, 17 alone. This leads to much more rapid cutting through the bone, with much less friction, and hence much less heating. The user does not need to force the tool 1 through the bone, allowing much greater accuracy and control in the cut, for both the push and pull strokes 16, 17. The tip 8 may be sunk longitudinally into the bone with only small lateral movements of the tool 1.

**[0053]** The tool 1 is connected to an ultrasound generator operating in the frequency range 20-75kHz.

**[0054]** Thus, for a replacement hip joint prosthesis held in a cavity within a femur by friction or by interaction with cancellous bone, and requiring revision, it is relatively straightforward to sink the tool 1 between the stem of the prosthesis and the femur itself, tip first and extending generally parallelly to the stem. The tool 1 can then be moved laterally around the stem, with a gentle sawing motion, cutting through the bone and freeing the prosthesis.

**[0055]** Compared to the alternative approach of using powered burrs, the ultrasonically-vibrated tool 1 is significantly more accurate, and does not flex when it meets increased resistance, which might cause unacceptable collateral bone damage. Frictional heating is lower with the tool 1 shown than with powered burrs, and the amount of bone swarf produced is significantly lower.

**[0056]** Manual (chisel-like) osteotomes require considerable force to drive between the prosthesis and the femur, which could damage a weakened femur wall and frequently compromises the directional accuracy of the technique.

**[0057]** The tool 1 may also be of use in other surgical procedures where rapid and accurate bone cutting is required, such as bone grafting or amputations.

**[0058]** A second osteotomy tool 21 is shown in Figure

3A. As for the first 1, it comprises a cylindrical body 2 with a proximally-mounted threaded spigot 3 by which it is connectable to a generator of ultrasonic vibrations. However, in this case, the generator produces torsional mode ultrasonic vibrations. As for the longitudinally-vibrated first tool 1, vibrations in the frequency range 20-75kHz are preferred.

**[0059]** The second tool 21 is provided with a generally hemicylindrical blade 27, aligned coaxially with the connecting body 2 along a longitudinal axis 18 of the tool 21. A distal tip 28 of the hemicylindrical blade 27 is provided with a plurality of teeth 23. The teeth 23 are shown as symmetrical, although they may be asymmetrical as for the teeth 13 of the first tool 1, set in either sense or even set in alternating senses. The tip 28 thus comprises a generally semicircular cutting edge, as shown in Figure 3B.

**[0060]** The torsional mode ultrasonic vibrations transmitted through the connecting body 2 to the blade 27 thus vibrate the tip 28 as shown by arrows 26. The user rotates the second tool 21 manually about the axis 18, without needing to exert significant longitudinal force, and the ultrasonic vibrations cause the tool 21 to cut rapidly and accurately into the bone to which it is applied.

**[0061]** As well as being useful for cutting between a prosthesis and a concave inner wall of a long bone, the second tool 21 may also be usable to cut circular bone samples, or in cranial surgery. Although a generally hemicylindrical blade 27 is probably optimal for arthroplasty revision work, blades comprising greater or lesser proportions of a hollow cylinder may be appropriate in other applications.

**[0062]** A third osteotomy tool 31, shown in Figure 4, is a preferred variant of the first tool 1, shown in Figure 1.

As for the first tool 1, the third tool 31 comprises a connecting body 2 having a threaded spigot 3, by which the tool 31 may detachably be connected to a generator of ultrasonic vibrations. An elongate blade portion 4 extends from a distal end of the connecting body 2, generally coaxially aligned therewith.

**[0063]** The blade portion 4 comprises a proximal blade root 5 of generally rectangular cross-section, linked by a tapered portion 6 to a thin, elongate blade 37 with a generally rounded distal tip 8. As for the blade 7 of the first tool 1, this comprises a distal portion having two oppositely-facing lateral cutting edges 9, 10. A plurality of teeth 13 extend along each cutting edge 9, 10 and the rounded tip 8 that joins them.

**[0064]** The blade 37 of the third tool 31 differs in cross-sectional profile from that of the first tool 1. Whereas the blade 7 has a rectangular cross-section, the blade 37 has a substantial bevelled region 32 extending longitudinally of the blade 37 adjacent each edge 33 thereof and around its distal tip 8. (A corresponding bevelled region 32 is provided on a reverse face of the blade 37 to that visible in Figure 4).

**[0065]** Thus, as shown more clearly in Figure 5, the blade 37 has an octagonal cross-section. Respective

bevelled regions 32 on each face of the blade 37 define a narrow edge 33 extending between them. It is preferable that the edge 33 is not actually sharpened, to reduce the likelihood of it cutting anything accidentally while the tool 31 is not ultrasonically activated.

**[0066]** As shown in Figure 6, the indentations between the teeth 13 of the blade 37 extend only partially across the bevelled regions 32. They are thus both triangular in plan view (see Figures 2 and 3) and generally triangular in profile.

**[0067]** The teeth 13 of the blade 7 of the first tool 1 have a substantially rectangular cross-section, and it is believed that the outer corners thereof may be prone to damage. It is probable that an activated tool 1 would at some point come into contact with a prosthesis being removed and the corners of the teeth 13 would tend to impact thereon. There would be a significant chance of these corners being knocked off, notched or chipped as a result. It is important to balance an ultrasonically-vibratable blade, and significant loss of material from the teeth 13 might require the whole blade 7 to be rebalanced or even disposed of. Also, if damage occurs at a region of the blade 7 that is under raised stress, fatigue fractures of the blade 7 might quickly follow, originating from the damage.

**[0068]** The blade 37 with bevelled regions 32 avoids such problems to a great extent. While a face of the blade 37 might contact the prosthesis in use, its teeth 13 (and particularly the narrow edge 33 forming the tips of the teeth 13) are set back from the face and less likely contact the prosthesis. Even if they did, the profile created means that such contacts would be more glancing and less liable to cause damage. Nevertheless, the tooth 13 profile of the blade 37 of the third tool 31 is just as effective as that of the first tool in cutting through cancellous bone.

**[0069]** A similar tapered profile may also be created around the cutting distal tip 28 of the second tool 21.

## Claims

### 1. A tool adapted to cut bone comprising:

means for generating ultrasonic vibrations, and an elongate blade operatively connectable thereto, the blade having at least one cutting edge provided with a plurality of serrations each having a first cutting facet substantially traverse to the direction of said ultrasonic vibrations, wherein the means for generating ultrasonic vibrations produces torsional mode ultrasonic vibrations.

### 2. A tool as claimed in claim 1, wherein the serrations are generally triangular.

### 3. A tool as claimed in claim 1 or 2, wherein the blade comprises an elongate member having a curved

cross-section substantially comprising an arc of a circle.

### 4. A tool as claimed in claim 3, wherein said tool is adapted to be torsionally vibratable about a longitudinal axis extending through the centre of said circle.

### 5. A tool as claimed in claim 3 or 4, wherein a distal tip of the elongate member comprises the at least one cutting edge.

### 6. A tool as claimed in claim 5, wherein the serrations extend distally from the tip of the elongate member.

### 7. A tool as claimed in claim 5, wherein a portion of the elongate member adjacent its tip tapers longitudinally towards said tip.

### 8. A tool as claimed in claim 7, wherein the tapered portion comprises an angled surface located on a concave face of a curved elongate member.

### 9. A tool as claimed in any preceding claim, wherein the ultrasonic generator is adapted to generate ultrasonic vibrations at a frequency within the range of 20-75 kHz.

### 10. A method of cutting bony material comprising the steps of:

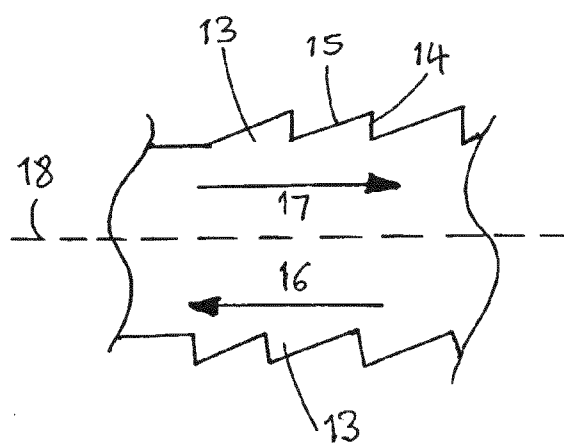
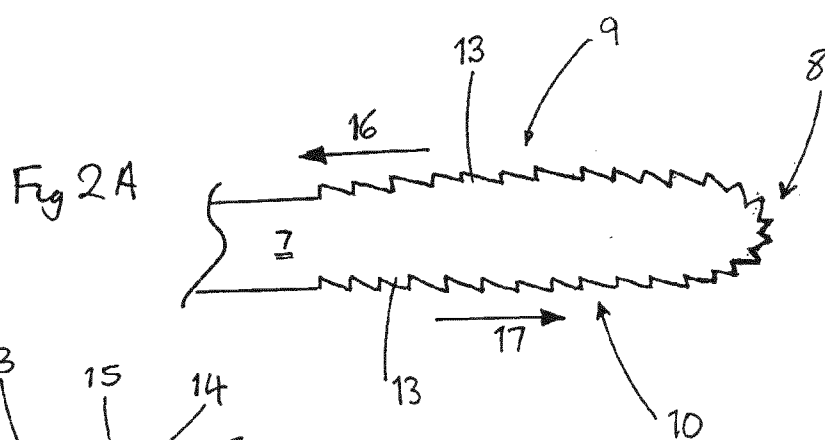
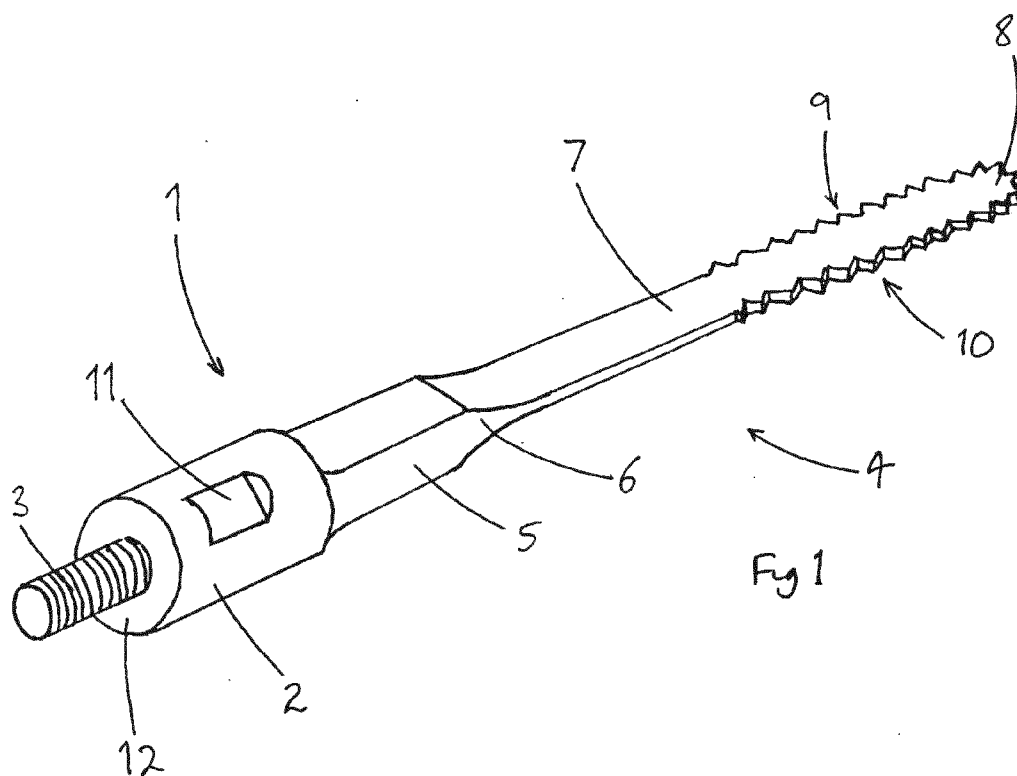
providing a tool adapted to cut bone comprising:

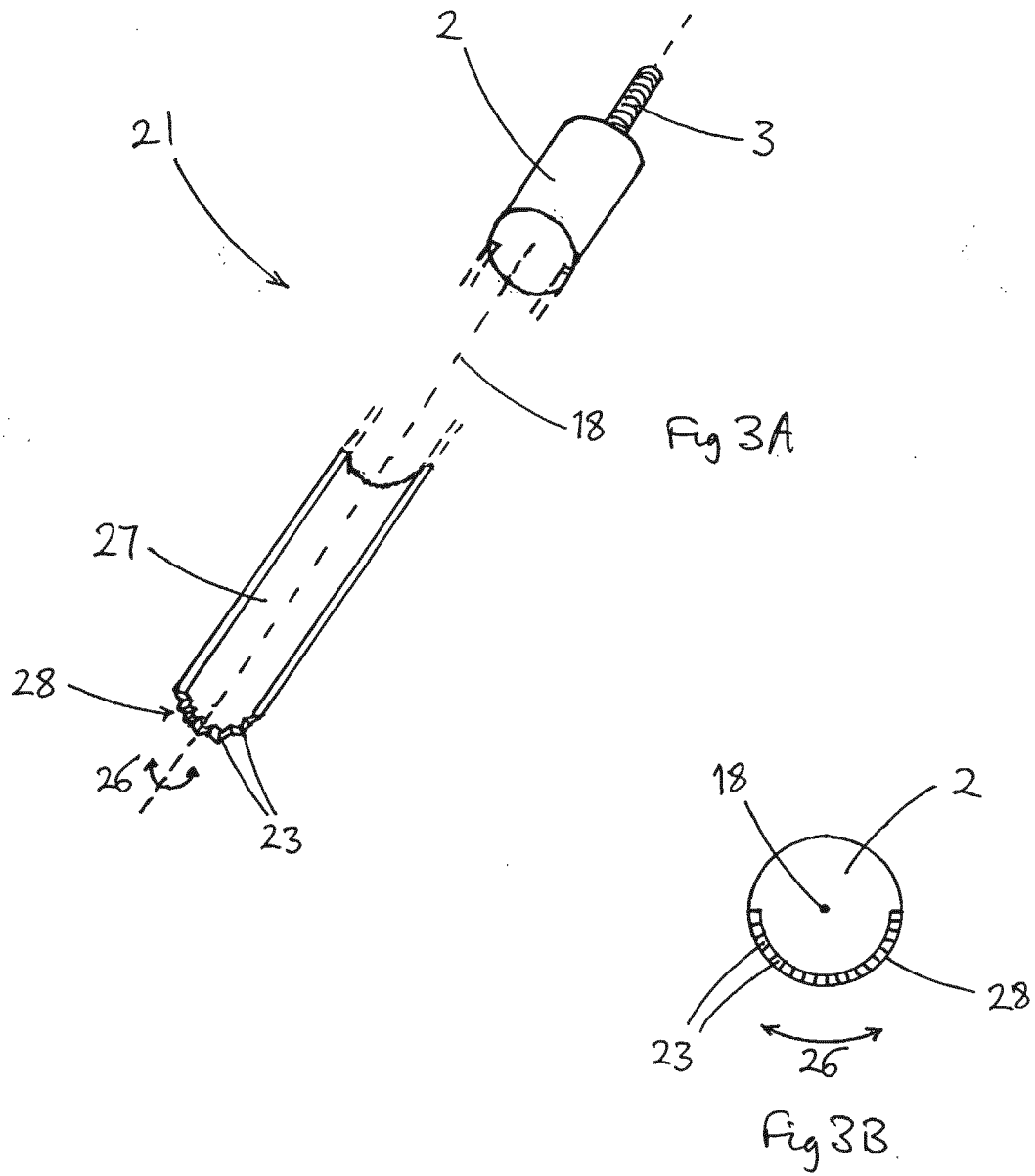
an ultrasonic generator, and  
an elongate blade operatively connectable thereto, the blade having at least one cutting edge provided with a plurality of serrations each having a first cutting facet substantially traverse to the direction of said ultrasonic vibrations, wherein the ultrasonic generator produces torsional mode ultrasonic vibrations;

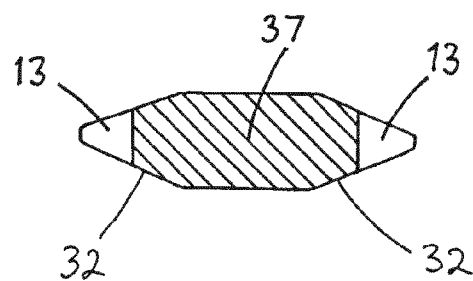
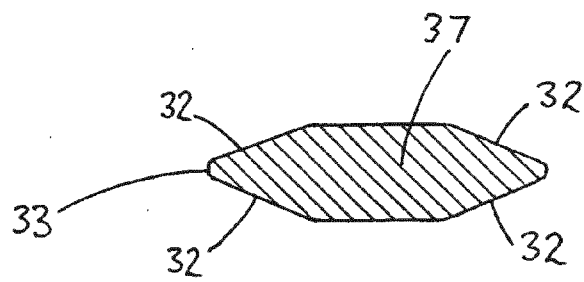
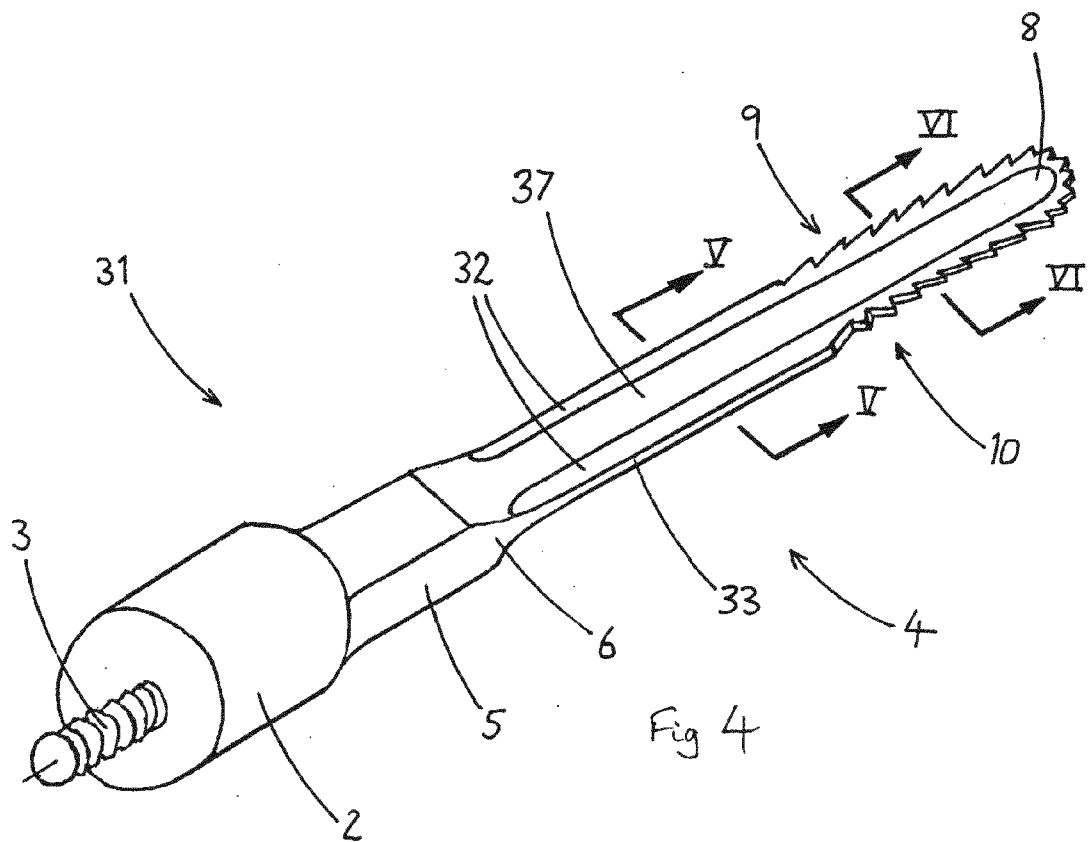
applying said at least one cutting edge of the tool to a surface of bony material to be cut;  
causing the tool to vibrate at an ultrasonic frequency by actuating the ultrasonic generator;  
and  
drawing the cutting edge of the tool across said surface.

### 11. The method of claim 10, wherein the bony material comprises cancellous and/or cortical bone holding an orthopaedic implant to a bone of a living body.

### 12. The method of claim 11 wherein the method further comprises cutting the bone until the implant is separable therefrom.











## EUROPEAN SEARCH REPORT

Application Number  
EP 14 17 6285

5

10

15

20

25

30

35

40

45

50

55

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 2002/099400 A1 (WOLF JOHN R ET AL) 25 July 2002 (2002-07-25) * paragraphs [0020], [0050]; figures 4,5,10,11 *	1-9	INV. A61B17/32 A61B17/16 A61B17/14
X,P	WO 2005/076951 A2 (EASLEY JAMES C [US]) 25 August 2005 (2005-08-25) * pages 1,6; figure 1 *	1-3,5, 7-9	
E	WO 2006/012797 A1 (SHI WENYONG [CN]; ZHOU ZHAOYING [CN]; ZHANG YULI [CN]; LUO XIAONING [C]) 9 February 2006 (2006-02-09) * paragraphs [0010], [0014], [0015], [0025], [0033] - [0035], [0042], [0047]; figures 6,7,8 * & US 2006/030797 A1 (ZHOU ZHAOYING [CN] ET AL) 9 February 2006 (2006-02-09)	1-9	
A	WO 92/22259 A2 (ADVANCED OSSEOUS TECH [US]) 23 December 1992 (1992-12-23) * pages 13,14; figures 28,40 *	1	TECHNICAL FIELDS SEARCHED (IPC)
A	US 4 188 952 A (LOSCHILOV, VLADIMIR I ET AL) 19 February 1980 (1980-02-19) * column 5, lines 39-44; figures 2-4,6 *	1	A61B A61F
A	US 5 935 143 A (HOOD ET AL) 10 August 1999 (1999-08-10) * columns 1,2,3; figures 1-3,4a,5 *	1	
A	US 5 897 570 A (PALLEVA ET AL) 27 April 1999 (1999-04-27) * figures 4,21a,22b,24a *	1	
A	EP 1 380 265 A (OLYMPUS CORPORATION) 14 January 2004 (2004-01-14) * figure 4g *	1	
		-/--	
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 28 November 2014	Examiner Assion, Jean-Charles
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

EPO FORM 1503 03.02 (P04C01)



## EUROPEAN SEARCH REPORT

Application Number  
EP 14 17 6285

5

10

15

20

25

30

35

40

45

50

55

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
A	US 5 676 680 A (LIM ET AL) 14 October 1997 (1997-10-14) * figure 9 *	1	
A	WO 93/01751 A (HALLAMSHIRE SURGICAL SAWS LIMITED) 4 February 1993 (1993-02-04) * abstract; figures 2-3 *	1	
			TECHNICAL FIELDS SEARCHED (IPC)
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 28 November 2014	Examiner Assion, Jean-Charles
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

EPO FORM 1503 03.82 (P04C01)

**ANNEX TO THE EUROPEAN SEARCH REPORT  
ON EUROPEAN PATENT APPLICATION NO.**

EP 14 17 6285

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.  
The members are as contained in the European Patent Office EDP file on  
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

28-11-2014

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2002099400 A1	25-07-2002	NONE	
WO 2005076951 A2	25-08-2005	EP 1718226 A2 JP 2007521880 A US 2005177184 A1 WO 2005076951 A2	08-11-2006 09-08-2007 11-08-2005 25-08-2005
WO 2006012797 A1	09-02-2006	CN 1732861 A DE 112005001878 T5 JP 2008508065 A US 2006030797 A1 WO 2006012797 A1	15-02-2006 28-06-2007 21-03-2008 09-02-2006 09-02-2006
WO 9222259 A2	23-12-1992	US 5318570 A WO 9222259 A2	07-06-1994 23-12-1992
US 4188952 A	19-02-1980	NONE	
US 5935143 A	10-08-1999	US 5695510 A US 5935142 A US 5935143 A	09-12-1997 10-08-1999 10-08-1999
US 5897570 A	27-04-1999	US 5728118 A US 5843110 A US 5897570 A US 6106535 A	17-03-1998 01-12-1998 27-04-1999 22-08-2000
EP 1380265 A	14-01-2004	EP 1380265 A1 US 2004010267 A1	14-01-2004 15-01-2004
US 5676680 A	14-10-1997	US 5658304 A US 5676680 A	19-08-1997 14-10-1997
WO 9301751 A	04-02-1993	NONE	

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

专利名称(译)	改良骨凿		
公开(公告)号	<a href="#">EP2848214A1</a>	公开(公告)日	2015-03-18
申请号	EP2014176285	申请日	2005-12-02
[标]申请(专利权)人(译)	ORTHOSONICS		
申请(专利权)人(译)	ORTHOSONICS有限公司		
当前申请(专利权)人(译)	ORTHOSONICS有限公司		
[标]发明人	YOUNG MICHAEL		
发明人	YOUNG, MICHAEL		
IPC分类号	A61B17/32 A61B17/16 A61B17/14		
CPC分类号	A61B17/16 A61B17/142 A61B17/144 A61B17/1628 A61B17/1637 A61B17/1642 A61B17/1664 A61B2017/320077		
优先权	2004026503 2004-12-02 GB PCT/GB2005/004618 2005-12-02 WO		
其他公开文献	EP2848214B1		
外部链接	<a href="#">Espacenet</a>		

#### 摘要(译)

一种用于切割骨的工具 ( 1,31 ) , 包括可连接到纵向超声波振动发生器的细长刀片 ( 7,37 ) 。刀片 ( 7,37 ) 具有由圆形远侧末端 ( 8 ) 连接的两个侧切削刃 ( 9,10 ) 。一系列三角形齿 ( 13 ) 沿着每个切削刃 ( 9,10 ) 和远侧末端 ( 8 ) 延伸。刀片 ( 37 ) 可朝向每个切削刃 ( 9,10 ) 和远侧末端 ( 8 ) 渐缩。工具 ( 21 ) 的变型包括可连接到扭转模式超声波振动发生器的细长部分圆柱形刀片 ( 27 ) 。刀片 ( 27 ) 在其远侧末端 ( 28 ) 处具有设有多个三角形齿 ( 23 ) 的切削刃。所有形式的工具 ( 1,21,31 ) 特别适合于在关节置换术的修正期间在要移除的植入物周围切割松质骨。

