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(54) **VACUUM POWERED SALINE INJECTION SYSTEM**

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A61M 3/02 (2006.01)
A61B 18/14 (2006.01)

(52) **U.S. Cl.**

CPC **A61M 1/0064** (2013.01); **A61B 18/1482** (2013.01); **A61B 2018/1422** (2013.01); **A61B 2018/1475** (2013.01); **A61B 2218/002** (2013.01); **A61B 2218/007** (2013.01); **A61M 1/00** (2013.01); **A61M 1/0056** (2013.01); **A61M 1/0068** (2014.02); **A61M 3/02** (2013.01); **A61M 3/0233** (2013.01); **A61M 3/0254** (2013.01); **A61M 3/0279** (2013.01); **A61M 3/0283** (2013.01); **A61M 2205/7545** (2013.01); **A61M 2205/7554** (2013.01)

(58) **Field of Classification Search**

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See application file for complete search history.

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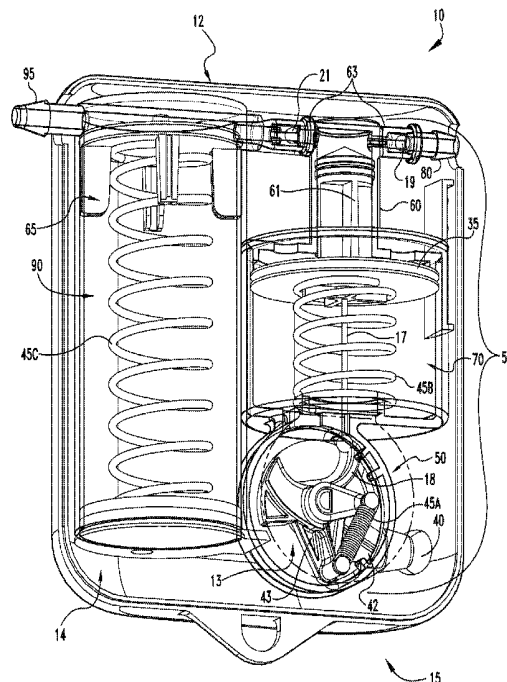
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(57) **ABSTRACT**

A method and apparatus for injecting saline into an open cavity of a patient's body, and, alternatively, vacuuming fluids from said cavity, during laparoscopic surgery that provides constant feed and amplified pressure to provide a steady fluid output, in a disposable, single use handheld surgical device.

3 Claims, 7 Drawing Sheets



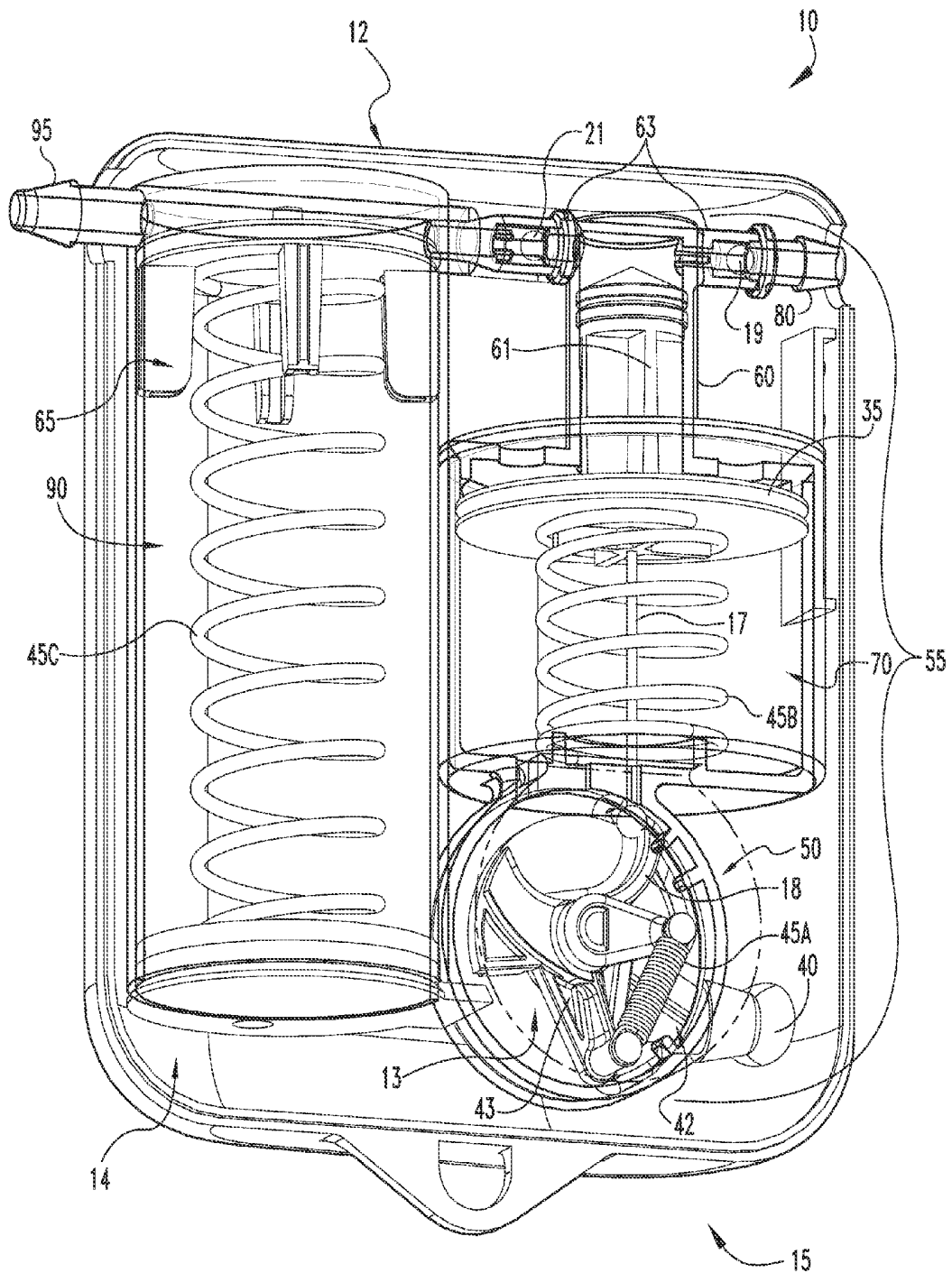


Fig. 1

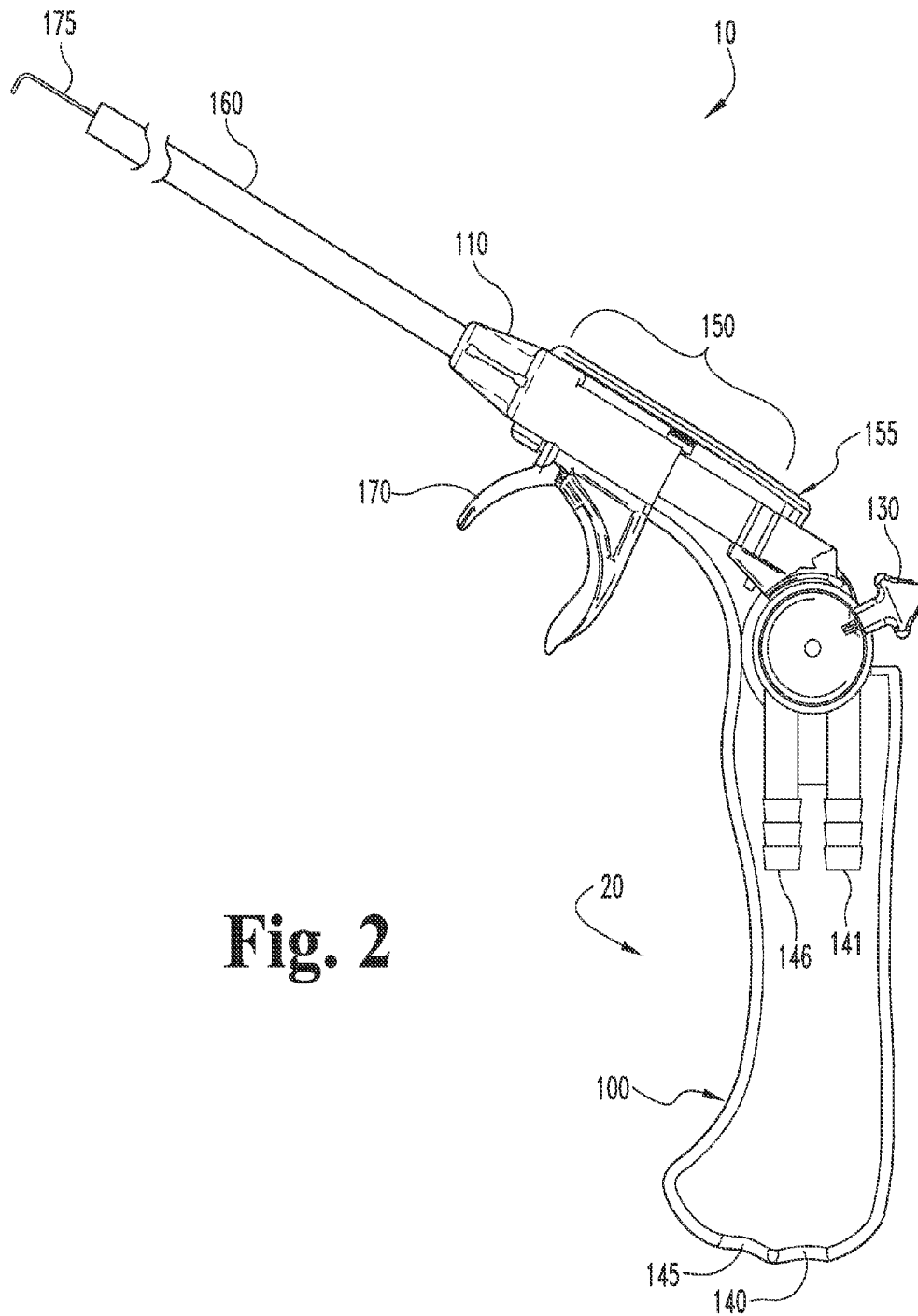
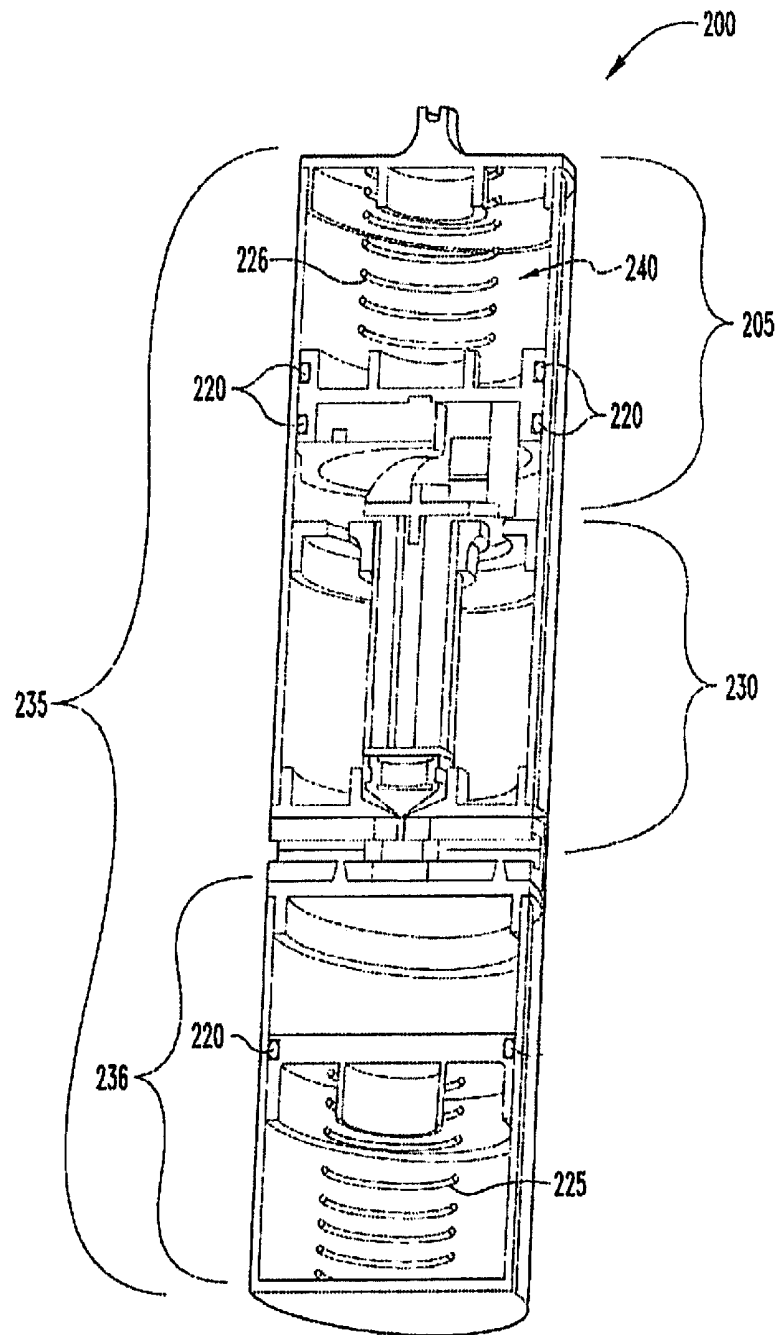
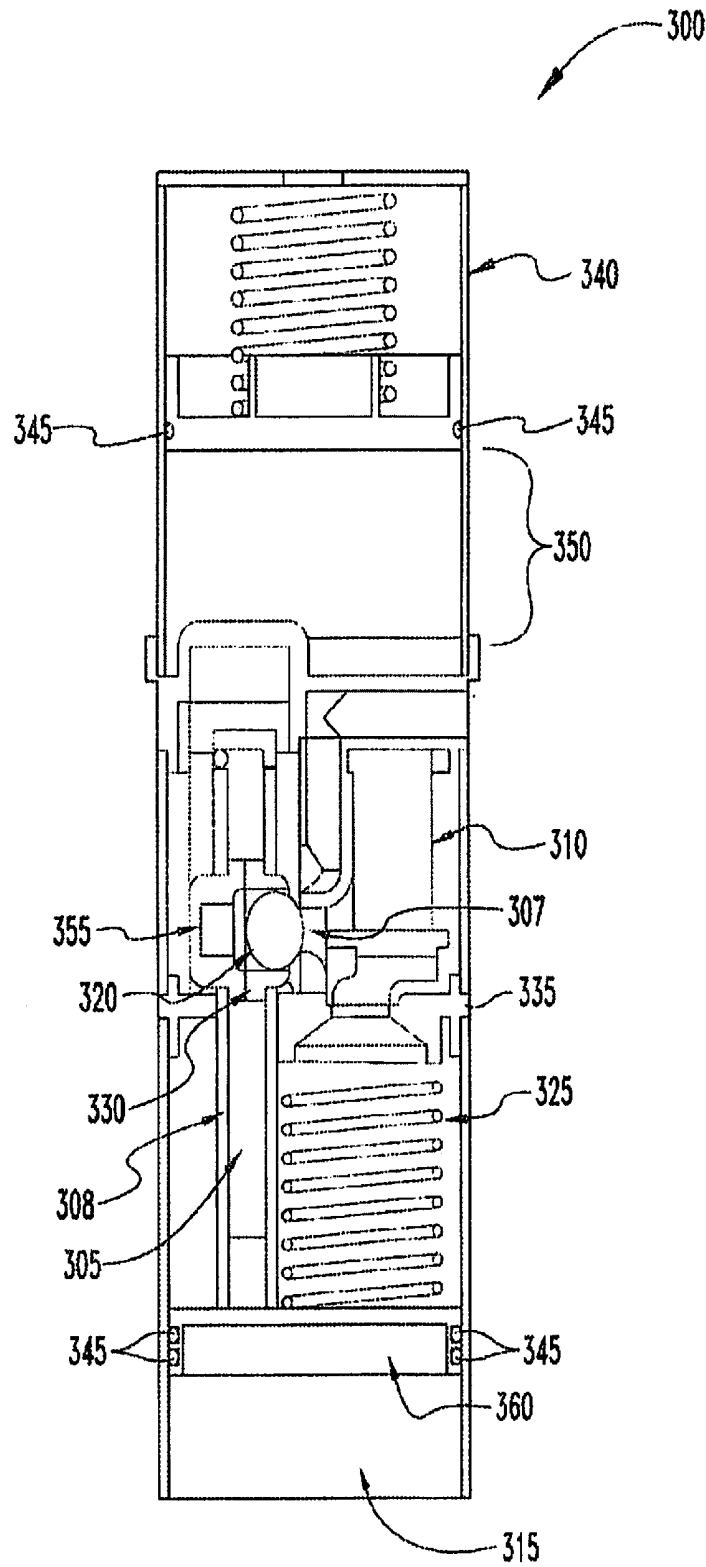
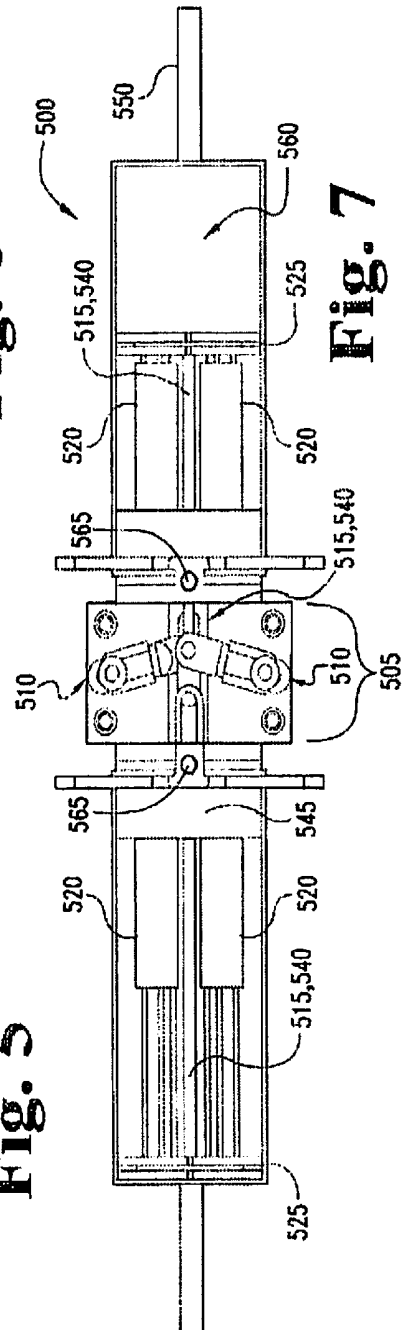
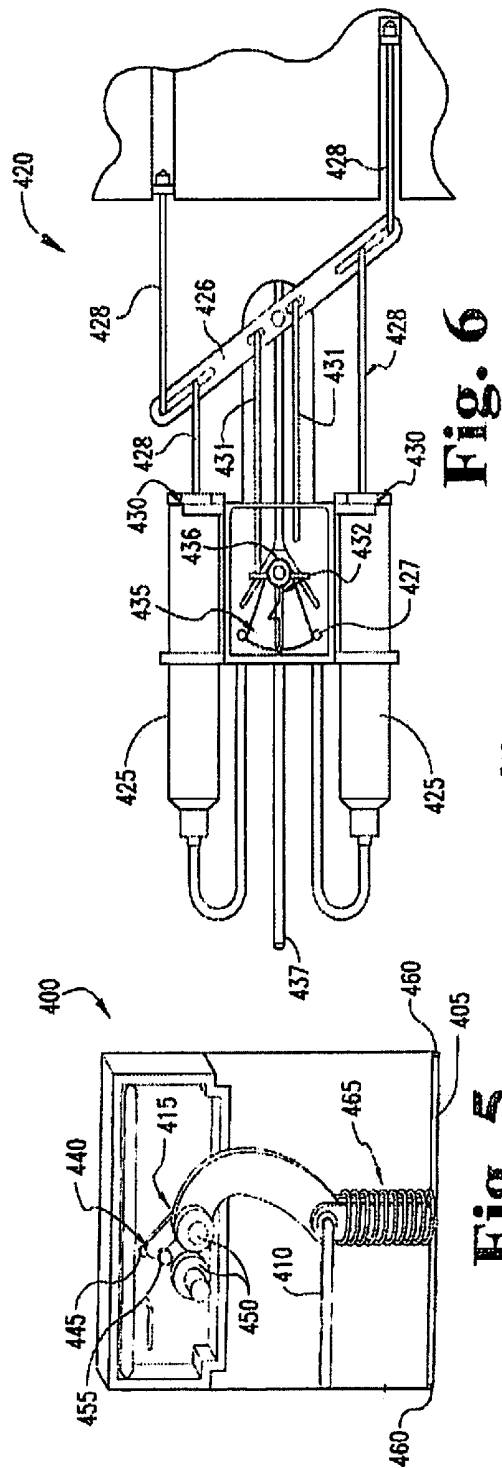
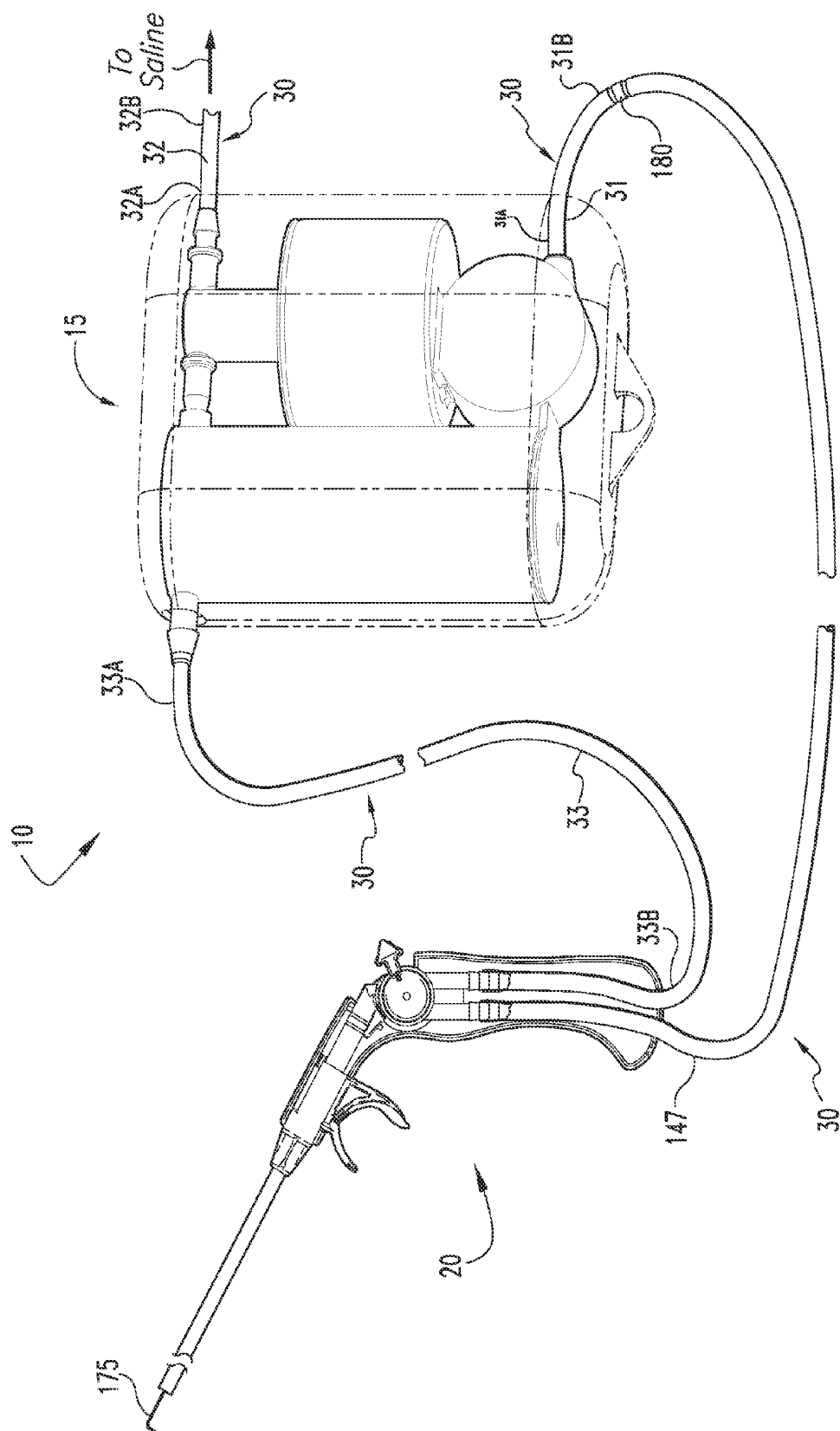


Fig. 2

**Fig. 3**

**Fig. 4**





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b
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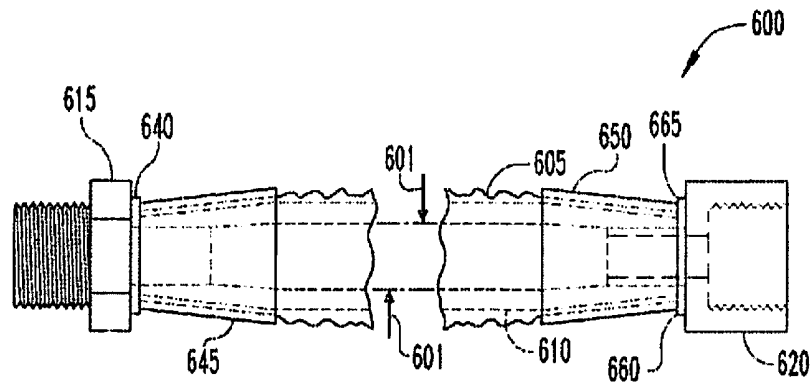


Fig. 9

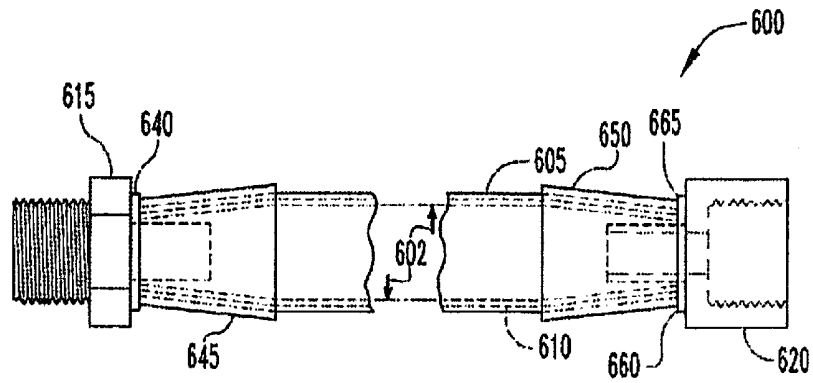


Fig. 10

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VACUUM POWERED SALINE INJECTION SYSTEM

TECHNICAL FIELD

The present novel technology relates to the field of medical device technology, and more particularly, a method and apparatus used during laparoscopic surgery for injecting saline into an open cavity of the patient's body, and, alternatively, vacuuming fluids from said cavity.

BACKGROUND

Laparoscopic surgery has continuously gained momentum and popularity since it was first introduced in the United States around 1988. Laparoscopic surgery, a minimally invasive surgical technique in which surgeons operate through multiple, small incisions in the abdomen, reduces standard risks, patient discomfort, scarring, and recovery time compared to previously utilized open surgical techniques.

Due to the intricate process of utilizing specialized instrumentation and a laparoscope camera to perform the operation while watching detailed images on a monitor, a clear surgical field is important. Without a clear surgical field, the surgeon is essentially operating "blind". Irrigation and aspiration are essential procedures during laparoscopic surgery, especially for maintaining a clear visual field and maintained hemostasis. Therefore, it is crucial that the device used for irrigation and aspiration provide enough hydraulic pressure to clear away debris, blood, blood clots, char, or any other material that may obstruct the surgeon's vision throughout the procedure, without delay.

Typically, disposable, single-use battery-powered laparoscopic devices are utilized for irrigation and aspiration. These mechanical pumping systems typically utilize standard alkaline batteries to power a motor, which in turn, activates a pump to drive irrigation fluid through the system for delivery to the operative site. Although these devices provide portable handheld systems with a built-in pump motor and generally adequate fluid pressure, there is currently a need for an aspiration and irrigation device that solves several issues unaddressed by the devices currently in the marketplace. The current solution is expensive and requires multiple disposal methods for proper disposal of the various components, such as metal, chemical, and surgical waste. In addition, an improved method of operating a pump, utilizing standard operating room resources, would be more transferable, efficient, inexpensive, and reliable. The present novel technology addresses this need.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a front plan view of a vacuum powered saline injection system according to a first embodiment of the present novel technology.

FIG. 2 is a side plan view of a first embodiment illustrating the gun portion of the vacuum powered saline injection system.

FIG. 3 is a front perspective view of a second embodiment vacuum powered saline injection system.

FIG. 4 is a front perspective view of a third embodiment vacuum powered saline injection system.

FIG. 5 is a front perspective view of a forth embodiment vacuum powered saline injection system.

FIG. 6 is a front perspective view of a fifth embodiment vacuum powered saline injection system.

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FIG. 7 is a front perspective view of a front perspective view of a sixth embodiment vacuum powered saline injection system.

FIG. 8 is a front plan view of the first embodiment vacuum powered saline injection system illustrating both the pump portion and the gun portion.

FIG. 9 is a side plan view of a seventh embodiment illustrating the accumulator portion of a vacuum powered saline injection system in its contracted state.

FIG. 10 is a side plan view of the seventh embodiment illustrating the accumulator portion of a vacuum powered saline injection system in its expanded state.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

For the purposes of promoting an understanding of the principles of the novel technology and presenting its currently understood best mode of operation, reference will now be made to the embodiments illustrated in the drawings and specific language will be used to describe the same. It will nevertheless be understood that no limitation of the scope of the novel technology is thereby intended, with such alterations and further modifications in the illustrated device and such further applications of the principles of the novel technology as illustrated therein being contemplated as would normally occur to one skilled in the art to which the novel technology relates.

FIGS. 1-2 and FIG. 8 illustrate a first embodiment of the present novel technology, a disposable, single-use handheld surgical vacuum powered saline injection system 10 for aspiration, and alternatively, irrigation during surgical procedures such as laparoscopic procedures. The vacuum powered saline injection system 10 generally includes a pump portion 15 and a wand or gun portion 20, and typically, a plurality of tubing portions 30, one of which operationally connects the pump 15 and gun portions 20 of the vacuum powered saline injection system 10.

The pump portion 15 generally includes a housing 12, which is customarily defined by a base portion 14 and an engageable cover portion (not illustrated in the drawings). Housing 12 is typically made of hard plastic or the like, although any convenient material may be selected. The housing 12 encases a pump motor 55, which typically includes a spring-biased valve 50 having a pivotable pump 13 connected in fluidic communication with a vacuum inlet 40, a generally cylindrical lower fluid storage chamber 70 (typically made of plastic or other polymeric material or the like) operationally connected to the spring-biased valve 50 and pivotable pump 13, a rod 17 extending vertically through the lower chamber 70 and down into the spring-biased valve 50 and pivotable pump 13, a generally cylindrical upper chamber 60 (typically made of plastic or other polymeric material or the like) in pneumatic communication with the lower chamber 70, a saline inlet 80 connected to the upper chamber 60, a generally cylindrical spring-biased accumulator or storage tank 90 (typically made of plastic or other polymeric material or the like) connected in fluidic communication to the upper chamber 60, and an outlet 95 for connecting the pump portion 15 and the gun portion 20 of the system 10 by way of a tubing component 33, in fluidic communication with the upper chamber 60 and flexible plastic tubing 30.

A vacuum source is connected in fluidic communication with inlet 40. The vacuum source is likewise connected to the lower chamber 70 through pivotable pump 13, such that when a partial vacuum is introduced, air pressure differen-

tials are generated and air pressure urges disk member 35 against spring 45B, moving disk 35 toward pump 13, likewise pushing rod 17 into receptacle 18 and urging pivotable pump disk 13 to pivot in a first direction. Pivoting pump disk 13 generates a biasing force in spring 45A, which urges pivoting of disk 13 in a second, opposite direction. Disk 13 pivots in the first direction until port 43 is opened to atmosphere, allowing air into fluidic communication with vacuum source and disk member 35, reducing the pressure differential and enabling spring 45A to urge pivoting of disk 13 in the second, opposite direction and spring 45B to urge disk 35 away from disk 13. As disk 13 pivots in the second direction, port 43 is closed to atmosphere, air pressure in disk area 13 and around spring 45B under disk 35 decreases, and the pump cycle repeats.

The side of disk 35 opposite spring 45B is connected to plunger 61 which is disposed inside upper cylinder 60. Movement of disk 35 towards disk 13 draws plunger 61 away from cylinder 60, generating a partial vacuum in cylinder 60 and urging fluid from saline source connected to inlet 80 through check valve 19 and into cylinder 60. As plunger 61 travels back into cylinder 60, saline therein is urged through check valve 21 into chamber/storage tank 90, urging disk 65 to move against spring 45C, compressing spring 45C and storing biasing energy therein. When outlet 95 is open, saline is urged from the tank 90. The vacuum pump motor 55 thus operates to fill tank 90 by urging saline therein with a first urging force. Once the tank is full, spring 45C and the incompressibility of saline generate a second, opposite force urging saline from outlet 95 when outlet is open and an unblocked fluid flow path exists; otherwise, the balance of forces prevent disk 35 from moving and the pump 55 automatically pauses.

The pump portion 15, gun portion 20, and plurality of tubing components 30, are powered by connection to a standard operating room medical vacuum system, allowing the vacuum powered saline injection system 10 to be utilized in most surgical and/or operating rooms. A first tubing component 31, has a proximal end 31A operationally connected to a fluid inlet port within the spring-biased valve 50 and pivotable pump 13, and a distal end 31B having a generally elastic, hydrocarbon polymer connector 180 operatively designed to engage a standard operating room medical vacuum system. In other embodiments, the connector 180 is sized and configured to engage non-standard vacuum sources, such as stand-alone vacuum pumps.

In operation, a flushing agent, such as isotonic saline, may be drawn from the distal end of a second tubing component 32, having a proximal end 32A operatively designed to engage a flushing agent from an outside source, and a distal end 32B in fluidic communication with the upper chamber 60 through a fluid inlet port 80. A generally T-shaped connector 63 made out of hard plastic, although any convenient material may be selected, is oriented within a first major axis, perpendicular to a generally small upper chamber 60 and in fluidic communication with both the upper chamber 60 and the spring-biased storage chamber 90, contains a plurality of typically round check valves, a first check valve 19 and a second check valve 21, to channel the incoming flushing agent between the upper chamber 60 and the spring-biased storage chamber 90. As the flushing agent enters the system 10 through the fluid inlet port 80, a first check valve 19 allows the flushing agent to enter the system 10 while a second check valve 21 blocks the flushing agent from passing through the generally T-shaped connector 63 to the spring-biased storage chamber 90. As the flushing agent enters the system 10, the spring-biased valve 50 and pivot-

able pump 13 operationally connected to a vacuum source, continuously cycle, urging a rod 17, generally connected to a first spring biased disk member 35 and typically extending vertically through the lower chamber 70 down into the spring-biased valve 50, to engage the spring 45C located within the spring-biased valve 50 to close a first port 43 operationally connected to an atmospheric opening. While a second port 42 operationally connected to a vacuum source is open, the first spring-biased disk member 35 is forced to draw against the biasing force and away from the upper chamber 60, producing a partial vacuum in the upper chamber 60, drawing the flushing agent into the upper chamber 60 and down into the lower chamber 70 as the spring-biased disk member 35 is compressed. As the pivotable pump 13 cycles, the spring-biased valve 50 forces a second port 42 operationally connected to a vacuum source to close, opening the first port 43 operationally connected to atmospheric air. The atmospheric air entering the system 10 negates the vacuum force entering the system, allowing the spring-bias 45 to urge a first spring-biased disk 35 positioned in the lower chamber 70, back towards the upper chamber 60, drawing the flushing agent back into the upper chamber 60. As the flushing agent is drawn back into the upper chamber 60 from the lower chamber 70, the first check valve 19 located within the generally T-shaped connector 63 moves towards the saline port 80 to block fluid from entering the vacuum powered saline injection system 10 from an outside source, forcing the flushing agent from the upper chamber 60 into the spring-biased storage chamber 90, containing a second spring-biased disk member 65. The method of forcing a flushing agent from the lower chamber 70 into a generally smaller upper chamber 60, while also forcing the flushing agent into the spring-biased storage tank 90 as the system 10 cycles, enables the system 10 to provide constant feed with amplified pressure, and thus, provide a constant, steady fluid output stream through a third tubing component, 33, having a proximal end 33A removably connected to the gun portion 20 of the system, and a distal end 33B in fluidic communication with the spring-biased storage chamber 90 through an inlet 95. The fluid output of the system 10 is controlled by the user through a multi-position valve 130 located on the gun portion 20 of the system, discussed in more detail herein. The vacuum powered pump further comprises an automatic shutoff feature when the spring-biased storage chamber 90 back pressure is equal to pump pressure forcing the fluid flow to cease through the system, the pivotable spring-biased pump 13 to stop pivoting, and the pump to idly wait until fluid is extracted from the storage chamber 90.

FIG. 2 generally illustrates the gun portion 20 of the vacuum powered saline injection system 10. The gun portion 20 (typically made of hard, electrically non-conducting plastic or the like, although any convenient material may be selected) is generally "L"-shaped, and is more typically ergonomically contoured for comfort and ease of use. The gun portion 20 typically contains a first inlet 140 for receiving a tubing component 33 to place the pump portion 15 in fluidic communication with the gun portion 20 through a tubing inlet 141 located within the pistol-shaped handle 100, and a second inlet 145 for receiving a vacuum tubing component 147, located on the underside of the pistol-shaped handle 100, through a second tubing inlet 146 located within the pistol-shaped handle 100, in fluidic communication to the storage chamber 90, as well as the operating room vacuum source. Additionally, a fluid nozzle 110 located on the barrel portion of the gun 150 places the handle 100 and barrel portions of the gun 150, including the

vacuum tubing inlet **146**, as well as the saline tubing inlet **141**, in fluidic communication with the cannula **160**. A multi-position valve **130**, located on the top of the handle between the handle **100** and the barrel **150**, permits a surgeon to quickly and easily manipulate whether the vacuum powered saline injection system **10** is in irrigation, aspiration, or off mode by simply rotating the typically circularly rounded valve **130** to the forward position, center, or back position. The multi-position valve **130** also permits a surgeon to control the flow and rate of a flushing agent, such as isotonic saline solution, or the rate and pressure of the vacuum. Thus, the gun portion's **20** functionality permits a surgeon to control aspiration or irrigation, as well as utilize a diathermy hook **175** located inside of a generally elongated cannula **160**, without having to use additional tools, reach away from the operating table, and/or physically move to control the function of the system.

The generally hollow, cylinder-shaped cannula **160** houses a typically L-shaped spring-biased diathermy hook **175** that may be extended from the cannula **160** through an opening located on the distal end of the conduit **160**. The diathermy hook **175** is typically made of surgical stainless steel or metal, although any convenient material may be selected, and is operationally connected to the moveable trigger **170** located on the barrel portion **150** of the gun handle **100**. Actuation of the trigger **170** extends the hook from within the distal end of the cannula **160** in relative relation to the location of the trigger **170**, to aid in clearing unwanted tissue beside linear structures during surgery.

Additional embodiments follow, wherein the vacuum powered saline injection system **10** operates as described above, however, the valve systems of the vacuum motor and the pump location differ. More specifically, the spring-biased valve **50** and the lower chamber **70** illustrated in FIG. **1** are replaced by alternative embodiments.

In an alternate embodiment, as illustrated in FIG. **3**, a magnetically triggered valve system **200** cycles the saline pump assembly **235** by opening the vacuum chamber **240** to atmosphere when activated. Magnets (not shown), located on both the sliding valve gate (not shown) and the wall of the vacuum chamber **240**, provide attractive and repulsive forces that allow the valve gate (not shown), located on the syringe pump **230**, to move between alternating open and closed positions. In operation, the sliding gate valve (not shown) is initially in closed position sealing the vacuum chamber **240**. As a vacuum is created within the vacuum motor **205**, the atmospheric pressure pushes the syringe pump **230**, compressing the spring bias **226** within the vacuum chamber **240** and the spring bias **225** within the accumulator **236**, drawing a flushing agent such as saline into the attached spring bias syringe pump **230**. As the syringe pump **230** passes the magnet (not shown) affixed to the vacuum chamber wall, the magnet embedded in the sliding valve gate (not shown) is repelled, allowing atmosphere to equalize in the vacuum chamber **240**. The energy stored in the vacuum chamber **240** spring bias **226** pushes the syringe pump **230**, discharging the saline. As the syringe pump **230** returns to the home position with the sliding valve gate (not shown) in closed position, the magnet in the sliding valve gate is attracted to the chamber mounted wall magnet, sealing the vacuum chamber **240** and concluding the stroke cycle.

In another alternate embodiment, as illustrated in FIG. **4**, a roller ball valve system **300** contains a lifter **305** that is operationally attached to the motor plunger **360** within the vacuum chamber **315** that actuates a spring-loaded roller ball **320** that opens and closes the atmospheric inlet **307**

allowing atmosphere into the vacuum chamber **315**. While engaging a vacuum source, vacuum is applied to the vacuum chamber **315** and atmosphere pushes the motor plunger (not shown) and check valve **310** which drives the lifter **305** and compresses the motor spring **325**. The spring-loaded roller ball **320**, located in a slotted track **308** of the lifter **305** containing an independent spring-loaded push-rod **330**, compresses forcing the roller ball valve **355** to open the vacuum chamber **315** to atmosphere and close the vacuum supply port **335**. Thereafter, the motor spring **325** releases, pushing the motor plunger (not shown) and attached saline chamber accumulator **350** to discharge saline through the attached syringe pump **340** and return to home position wherein the slot on the lifter **[13081]** **305** returns the roller ball assembly **320** to home position, sealing the vacuum chamber **315** and opening the vacuum supply port **335**. A plurality of O-Rings **345** located between the vacuum chamber **315** and vacuum motor plunger **360**, as well as between the saline chamber accumulator **350** and the pump **340**, provides a fluid-tight seal when required.

In another embodiment, as illustrated in FIG. **5**, the vacuum powered saline injection system **10** valve contains an over-the-center toggle system **400** wherein the pump is driven by the linear motion of the motor plunger **405**, wherein O-rings **460** are located thereon. A motor plunger **405** directly attached to a push-rod lifter **410** located within the vacuum chamber alternatively forces the atmospheric port **445** or the vacuum port **455** to open, and alternately close when the over-the-center spring **450** loaded toggle **415** assembly strikes a valve or gate valve **440** that is spring **465** driven.

In an additional embodiment, as illustrated in FIG. **6**, an alternate over-the-center toggle valve system **400** contains an adjacent vacuum redirect valve system **420** wherein the vacuum, entering the system **10** through a vacuum supply line **437** into vacuum ports **427** is redirected to alternating vacuum chambers **425**. Each chamber **425** has a plunger **430** operationally connected to a connecting lever **426** via a plunger push-rod **428** extending from both sides of the connecting lever **426** to the saline pump. The connecting lever **426** drives a second set of push-rods **431** for the over-the-center toggle **432** via a spring bias **436**, to redirect vacuum flow and the pump.

In an additional embodiment, as illustrated in FIG. **7**, the vacuum powered saline injection system **10** contains a vacuum connection **550** to an inline vacuum redirect valve **500** wherein the over-the-center toggle valve system **505** is comprised of spring loaded levers **510** driven by a central slotted push-rod **515/540** connected to two vacuum chambers **560**. Atmosphere alternately pushes the motor plungers **525** through the use of check valves **565** located between the over-the-center toggle valve center and the saline pump **545** and saline pump syringes **520**, driving the central push-rod **515/540** and pumps. As the slotted central push-rod **515/540** moves the redirect valve that is held in place by spring loaded levers **510**, the vacuum is applied to each vacuum chamber **560** sequentially. The saline pump syringes **520** are positioned in line with the shown vacuum chambers **560** and are attached to the spring loaded levers **510** by push-rods **540**.

In an alternative embodiment, as illustrated in FIGS. **9** and **10**, the system **10** functions as described above regarding the first embodiment **10**, with the exception being that the accumulator **90** has been replaced by an expanding length of hose/tubing **600**. The tubing **600** is typically self-expanding **602** upon application of fluid pressure and increased fluid volume causing a restricting force within the

hose 600 and, more typically, self-contracting 601 upon release of the fluid pressure and fluid volume from within the hose 600. The hose 600 is typically composed of two separate and distinct tubes—an inner tube 605 and an outer tube 610, both at least partially encased within an expansion restrictor sleeves 645, 650. The inner tube 605 is typically formed from a material that is elastic and has the ability to expand from its relaxed or unexpanded length when a pressurized fluid is introduced into the elastic inner tube 605 and expands radially outwardly or laterally, with respect to its length; the radial expansion of the inner tube 605 is constrained by the maximum diameter of the non-elastic outer tube 610. The outer tube 610 is typically formed from a relatively non-elastic, relatively soft, bendable, tubular webbing or like material that is typically strong enough to withstand internal pressures of up to 250 pounds per square inch, (psi).

The hose 600, in its contracted form 601 as illustrated in FIG. 9, results from a lack of force being applied to the inner tube 605, allowing a flushing agent to enter the storage tank or accumulator 90. The fluid pressure within the hose 600 is generated by introducing fluid under pressure into one end of the hose 600 and restricting the flow of the fluid out of the other end of the hose 600, typically controlling fluid passage through the use of washers 660 located on a male coupler 615 and a female coupler 620, positioned on opposite ends of the flexible tubing 600. As a pressurized fluid is introduced into the elastic inner tube 605 in its contracted and relaxed state 601, the elastic inner tube 605 begins to expand laterally and longitudinally and the outer tube 610 begins to unfold and uncompress around the circumference of the elastic inner tube 605. Consequently, when the inner tube 605 expands to a predetermined degree, the outer tube 610 unfolds, and uncompresses along the entire length of the inner tube 605 until it reaches the same length as the inner tube 605 in the expanded condition 602. Also, because the inner tube 605 expands both longitudinally and laterally and its expansion is constrained by the non-elastic outer tube 610, the inner tube 605 fills all of the available space inside the non-elastic outer tube 610 and thus the surface of the unfolded, uncompressed outer tube 601 becomes smooth in the expanded condition 602 (as depicted in FIG. 10), generating an urging force upon the stored fluid within the accumulator 90 for discharge of saline from the system 10, when the valve 50 is open.

While the novel technology has been illustrated and described in detail in the drawings and foregoing description, the same is to be considered as illustrative and not restrictive in character. It is understood that the embodiments have been shown and described in the foregoing specification in satisfaction of the best mode and enablement requirements. It is understood that one of ordinary skill in the art could readily make a nigh-infinite number of insubstantial changes and modifications to the above-described embodiments and that it would be impractical to attempt to describe all such embodiment variations in the present specification. Accordingly, it is understood that all changes

and modifications that come within the spirit of the novel technology are desired to be protected.

What is claimed is:

1. A system for injecting and removing fluids during electro surgery:

comprising:

a pump portion;
a fluid storage chamber operationally connected to the pump portion; and

a wand portion connected in fluidic communication with the pump portion;

wherein when the pump portion is fluidically connected to a vacuum source and fluidically connected to a fluid reservoir, a vacuum pump operable to urge fluid from the reservoir and into the fluid storage chamber with a first urging force;

wherein fluid filling the storage chamber works against an energy storage member to generate an opposite biasing force;

wherein the pump portion further comprises: a vacuum powered pump motor;

a vent port in communication with an atmospheric pressure;

a hose operationally connected to the vacuum powered pump motor for connection to the vacuum source;

a spring-biased valve operationally connected to the hose; an operationally connected cylindrical vacuum chamber; a spring-biased disk positioned within the cylindrical vacuum chamber and operationally connected to the spring-biased valve;

a fluid pumping chamber; a fluid pumping plunger operationally connected to the spring-biased disk; a fluidic inlet port operationally connected to the fluid pumping chamber and connectable in fluidic communication with the fluid reservoir;

a fluidic outlet port operationally connected to the fluid storage chamber; a first check valve operationally connected between the inlet port and the pumping chamber; and

a second check valve operationally connected between the outlet port and the fluid storage chamber;

wherein when the pump portion is connected to the vacuum source and to the fluid reservoir, the spring-biased disk moves with the atmospheric pressure creating a reciprocating action alternately rotating the spring-biased valve to open and close the vent port; and

wherein when the spring-biased disk connected to the fluid pumping plunger moves with the atmospheric pressure, a biasing force is generated to urge the fluid from the fluid reservoir to the fluid storage chamber.

2. The system of claim 1 wherein the wand portion further comprises a hook extending through a cannula and a trigger operationally connected to the hook, wherein actuation of the trigger extends the hook from within the cannula.

3. The system of claim 1 wherein the fluid storage chamber is an at least partially elastic flexible hose.

* * * * *

专利名称(译)	真空动力盐水注射系统		
公开(公告)号	US9468710	公开(公告)日	2016-10-18
申请号	US14/086434	申请日	2013-11-21
[标]申请(专利权)人(译)	托马斯P 林顿的石头 WEBER DAVID		
申请(专利权)人(译)	CLEMENT , THOMAS P. 林顿S. STONE WEBER , DAVID		
当前申请(专利权)人(译)	CLEMENT , THOMAS P. 林顿S. STONE		
[标]发明人	CLEMENT THOMAS P LINTON S STONE		
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其他公开文献	US20150141907A1		
外部链接	Espacenet USPTO		

摘要(译)

一种用于在腹腔镜手术期间将盐水注射到患者身体的开放腔中并且可替代地从所述腔中抽吸流体的方法和装置，所述腹腔镜手术提供恒定的进给和放大的压力以提供稳定的流体输出，手术装置。

