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(54) **MAIN OPTICAL SYSTEM FOR ENDOSCOPE**

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(57) **ABSTRACT**

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This invention relates to a main optical system for an endoscope, in particular, to a main optical system for an endoscope that is focally imaging in the visible and near-infrared lights, which belongs to the technical field of minimally invasive surgery. The used approach is: the objective lens set has a positive off-focus and positive field curvature. The steering set has the negative off-focus and negative field curvature. Moreover, a field lens set is added between the objective lens set and the steering set. The field lens set is located near the focus of the objective lens set. After the field lens is combined with the objective lens set, it will have the positive off-focus and positive field curvature that match to the steering set so that the 850 m defocus amount is less than 0.05 mm and the edge field curvature is less than 0.1 mm in the main endoscope optical system. The system is good in imaging. The invention controls the defocus amount and field curvature in the infrared and visible light bands by offsetting the negative and positive defocus amount and field curvature of the objective lens set, field lens set and steering set; it ensures the imaging quality of the main endoscope optical system and effectively addresses the shortcoming that it is difficult to realize the image difference correction within the broad spectral range for the objective lens set and steering sets independently; it has the advantages, such as more simpler processing, better control precision and lower cost, etc comparing the structure of used steering set and the traditional HOPKINS steering system; and it is especially applicable to the minimally invasive surgery under the infrared fluorescent lights, thus addressing the problems of repeated refocusing in traditional endoscope used for such operation.

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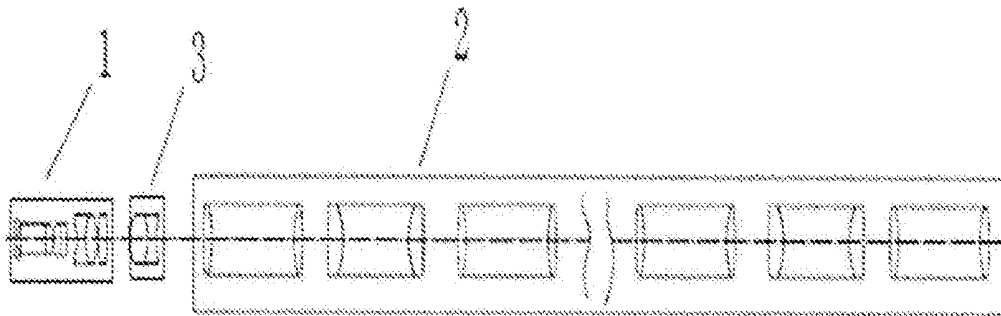
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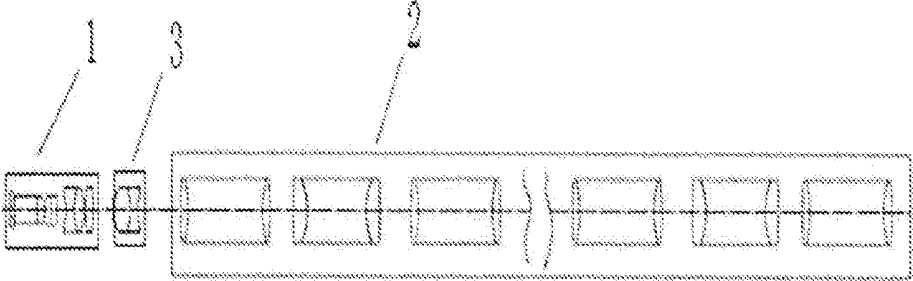


Fig. 1

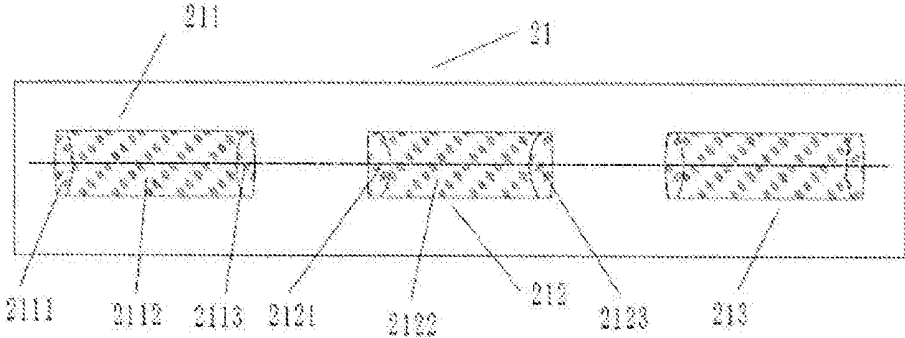


Fig. 2

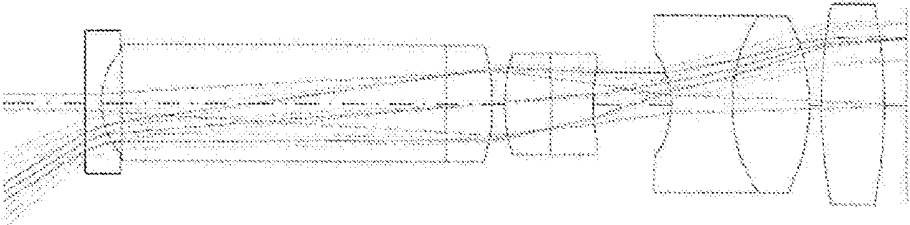


Fig. 3

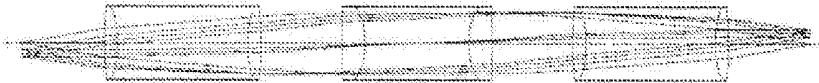


Fig. 4

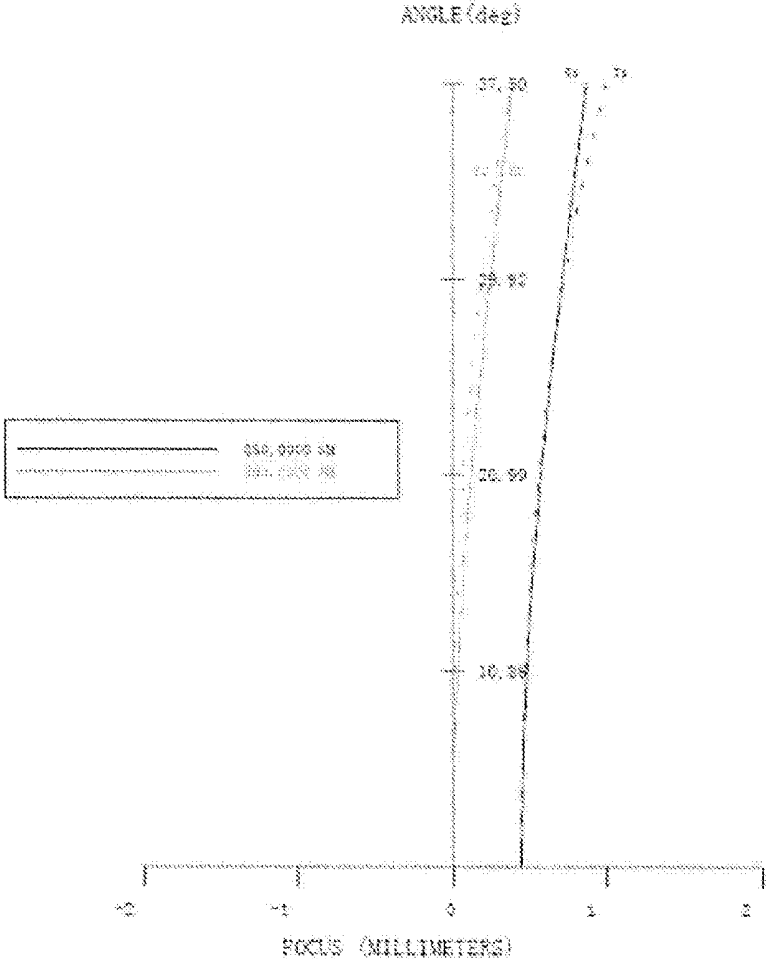


Fig. 5

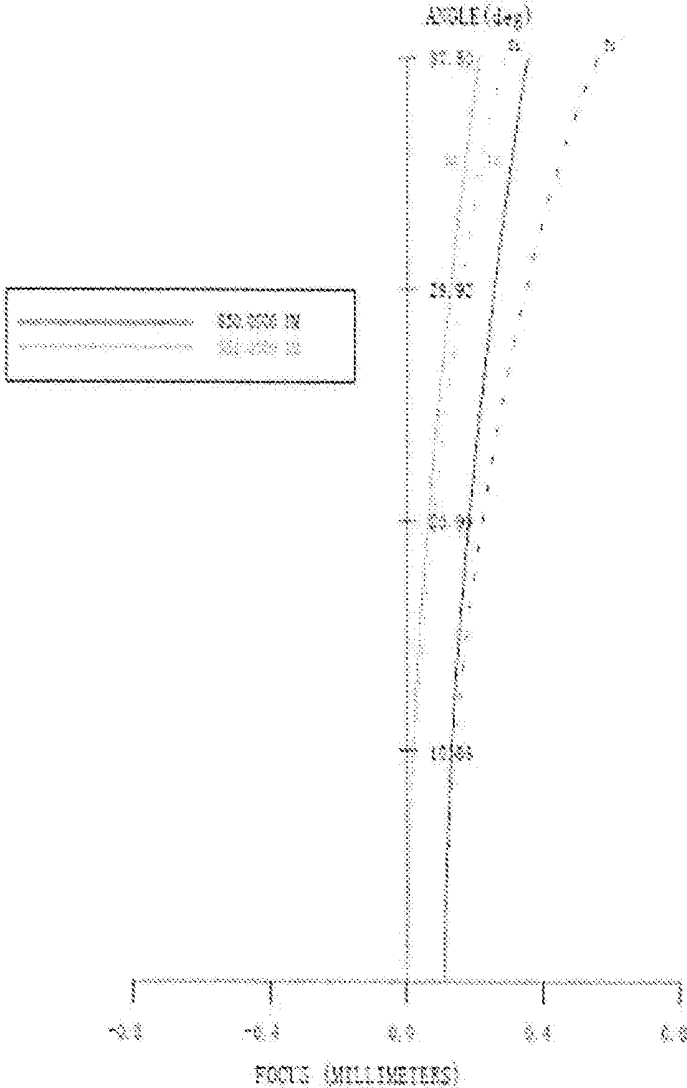


Fig. 6

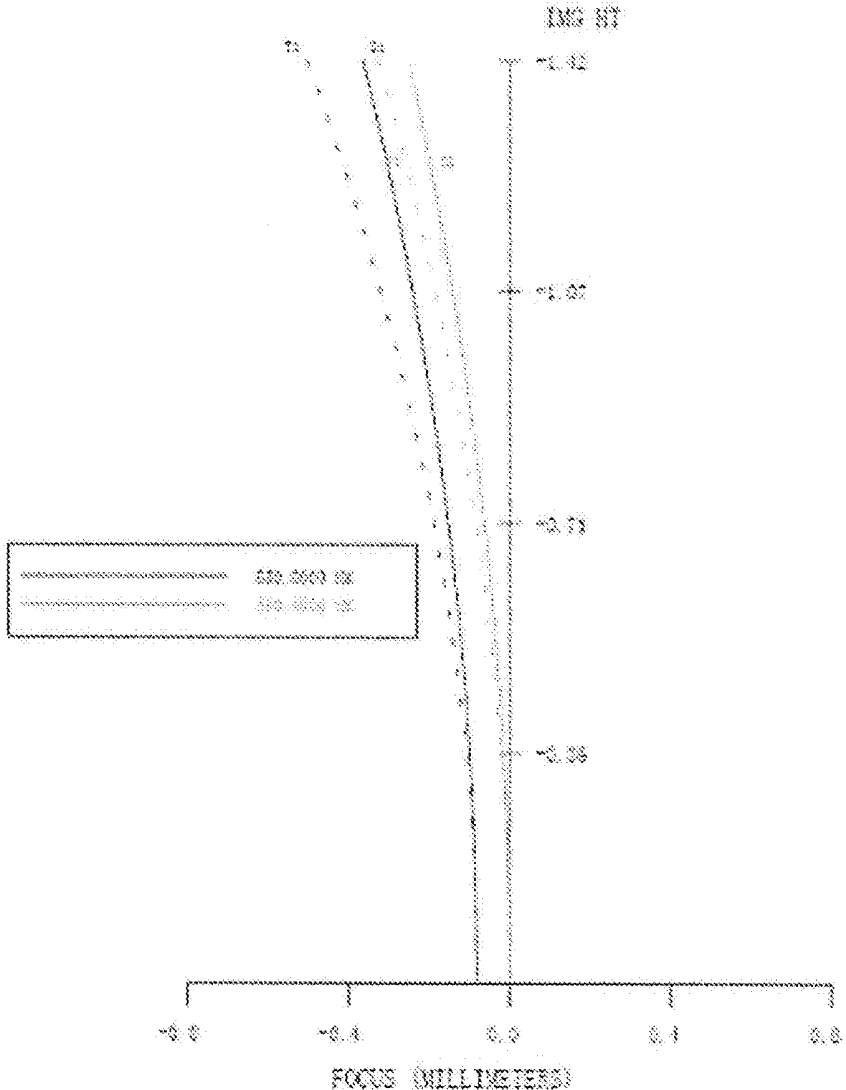


Fig. 7

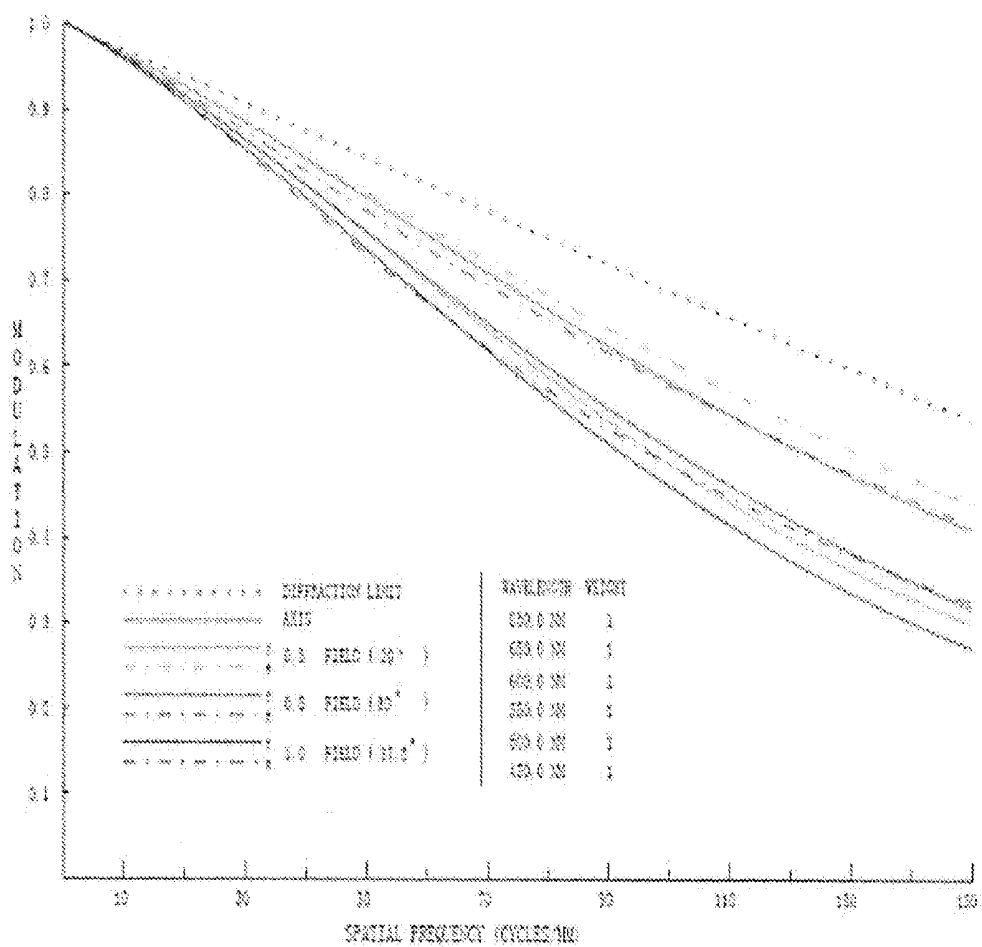


Fig. 9

MAIN OPTICAL SYSTEM FOR ENDOSCOPE

TECHNICAL FIELD

[0001] This invention relates to a main optical system for an endoscope, in particular, to a main optical system for an endoscope that is focally imaging in the visible and near-infrared lights, which belongs to the technical field of minimally invasive surgery.

BACKGROUND TECHNIQUE

[0002] The medical endoscope has been used more and more widely as an important part of minimally invasive surgery. With the gradual development of minimally invasive surgery technology, a higher technical requirement has been put forward, for instance, a more promising application is currently to add the near-infrared fluorescence analysis technology in the minimally invasive procedure. This requires that the endoscope system must be equipped with a wide spectral imaging ability, must yield imaging simultaneously in the visible (400 nm-700 nm) and near-infrared (700 nm-900 nm) lights and must ensure the focal imaging in the visible and near-infrared lights. At present, the traditional endoscope system can yield imaging in the visible and near infrared lights, however, there is an off-focal distance 0.3 mm-0.5 mm between the near infrared imaging location and the visible light imaging location, which results in refocusing at the observation of the infrared fluorescence image. Refocusing will affect the doctor's operational efficiency each time as the doctor must repeatedly switch the visible light images and near-infrared fluorescent images during the surgery procedure. Therefore, there must be an endoscope system that yields the visible and near infrared images to meet the operational requirements for doctors during surgery procedures.

[0003] The endoscopic imaging system consists essentially of an endoscope optical system, a camera adapter optical system and an image sensor. The endoscope optical system consists of a main endoscope optical system and an eyepiece optical system. The main endoscope optical system is composed by an objective lens set and a steering set. The imaging quality of the endoscope is determined by the imaging quality of the main optical system. The objective lens set images the operational field into the focal plane of the objective lens set. The steering set is composed by a HOPKINS rod lens system with an odd array of amplification rate by -1 time. The steering set is designed to transfer the images yielded by the objective lens set to the final image plane of the steering set in 1:1 to ensure the adequate working length of the endoscope. The images yielded in the operational field by the main endoscope optical system becomes the virtual images after the eyepiece optical system. The camera adapter optical system projects the virtual images onto the image sensors. The images in the operational fields are sent to the monitor via circuits and software for doctor's observation.

[0004] To achieve parfocality, the entire endoscope imaging system must focus in various components under the visible and near-infrared lights. Specifically, the main endoscope optical system, the eyepiece optical system and the camera adapter optical system must be parfocal. The parfocality is judged by the defocus amount. Pertinent to this application, the defocus amount in the near infrared and visible lights can be defined as: the axial distance between the imaging location of central view field at near Infrared 850 nm

wavelength and the imaging location of the central view field at the visible light 550 nm wavelength is an 850 nm defocus amount of the central view field. To simplify the description, the after-said defocus amount refers to the defocus amount of the central view field between the near infrared 850 nm and visible light 550 nm. The analysis finds that the eyepiece optical system and the camera adapter optical system have the defocus amount less than 0.02 mm when the main endoscope optical system achieves the defocus amount less than 0.05 mm and the edge view field curvature less than 0.1 mm; and the entire endoscope system can achieve the parfocal imaging when the main endoscope optical system achieves the defocus amount less than 0.02 mm and the edge view field curvature less than 0.02 mm.

[0005] It is easy to achieve the defocus amount less than 0.02 mm and edge view field curvature less than 0.02 mm in the eyepiece optical system and the camera adapter optical system, however, it is very difficult to achieve is to achieve the defocus amount less than 0.05 mm and edge view field curvature less than 0.1 mm in the main endoscope optical system. Concurrently, no literature has reported to meet the requirements.

CONTENTS OF THE INVENTION

[0006] The technical problem to be solved by the invention is to provide a main endoscope optical system that yields focal imaging in the visible light (400 nm-700 nm) and near infrared light (700 nm-900 nm). The used approach is: the objective lens set has a positive off-focus and positive view field curvature. The steering set has the negative off-focus and negative view field curvature. A field lens set is added between the objective lens set and the steering sets. The field lens set is located near the focus of the objective lens set. After the field lens is combined with the objective lens set, it will have the positive off-focus and positive field curvature that match to the steering set so that the 850 m defocus amount is less than 0.05 mm and the edge field curvature is less than 0.1 mm in the main endoscope optical system. The system is good in imaging.

[0007] The technical scheme of the invention to be detailed in combination of drawings

[0008] A main endoscope optical system structure that yields images in the visible (400 nm-700 nm) and near infrared (700 nm-900 nm) includes an objective lens group **1**, a steering set **2**, a field lens set **3**, which is characterized in that the objective lens set **1** is an optical lens set. The wavelength 850 nm has a positive field curvature and a positive defocus and the defocus amount is less than 0.5 mm in the imaging plane of the objective lens set **1**. The field lens set **3** is placed between the objective lens set **1** and the steering set **2**, and located near the imaging place of the objective lens set **1** to form the telecentric virtual images of the objective lens set **1**. In the virtual image location, the wavelength 850 nm has a positive defocus amount less than the objective lens set **1**, the edge view field has a curvature less than the objective lens set **1**, and the steering set **2** is a focus-free system and composed by 3 or 5 sets of identically-structured rod lens steering system **21** by -1 time. The rod lens steering system **21** by -1 time consists of 3 glued lenses, including a front rod lens set **211**, a middle rod lens set **212**, and a rear lens set **213**. The middle rod lens set **212** consists of a positive lens **2121**, a negative rod lens **2122** and a positive lens **2123** in a gluing way. The positive lens **2121** and the positive lens **2123** are positive biconvex lens. The positive lens **2121** and the positive lenses

2123 are made from the same material in the same structure and size. The negative rod lens **2122** is negative biconcave lens, which are equal in the spherical curvature radius and has the same curvature radius as the glued planes of the positive lens **2121** and the positive lens **2123**. The rear rod lens **213** has the same material, structure and size as the front rod lens **211** and arranged symmetrically against the middle rod lens **212**. The front rod lens **211**, the middle rod lens **212** and the rear rod lens **213** are arranged in coaxial manner. The distance between front rod lens **211** and the middle rod lens **212** is equal to that between the middle rod lens **212** and the rear rod lens **213**. The objective distance and image distance of the rod lens steering system **21** by -1 time are equal. The steering system **21** composed by 3 or 5 sets of rod lens by -1 time is arranged in such a way that the objective plane and image plane are superposed in two adjacent sets of rod lens steering systems **21** by -1 time to form the steering set **2**. The steering set **2** has the negative defocus amount and negative field curvature. The defocus amount value is larger than 0.1 mm and the field curvature value is larger than the objective lens set **1**. The main endoscope optical system composed by the field lens set **3** and the steering set **2** has the smallest defocus amount and less edge view field curvature. The def-focus amount is less than 0.05 mm and the field curvature is less than 0.1 mm. The transfer function MTF value of the central view field is larger than 0.3 at 150 alignment/mm and the transfer function MTF value of the edge view field is larger than 0.2 at 150 alignment/mm.

[0009] The further technology in the technical scheme of the invention is characterized in that the said field lens set **3** is a double-glued crescent lens.

[0010] The further technology in the technical scheme of the invention is characterized in that the said front rod lens **211** of the rod lens steering system **21** by -1 time contains a positive lens **211**, a negative lens **2122** and a positive lens **2113**. The positive lens **211** is a positive biconvex lens and the negative rod lens **2112** is a negative biconcave lens. The positive lens **2113** and the positive lens **2111** have the same material, structure and size fully. The negative lens **2112** has the same curvature radius in both spherical surface and has the same curvature radius as the gluing surfaces of the positive lens **2111** and **2113**.

[0011] The advantages of the invention are: 1. To control the defocus amount and field curvature in the infrared and visible light bands by offsetting the negative and positive defocus amount and field curvature of the objective lens set, field lens set and steering set; to ensure the imaging quality of the main endoscope optical system and effectively address the shortcoming that it is difficult to realize the image difference correction within the broad spectral range for the objective lens set and steering sets independently; 2) Comparing the structure of used steering set and the traditional HOPKINS steering system, it has the advantages, such as more simpler processing, better control precision and lower cost, etc.

DESCRIPTION OF DRAWINGS

[0012] Drawing 1: The structural schematic drawing for the main endoscope optical system in the invention

[0013] Drawing 2: The structural schematic drawing for the rod lens steering system **21** by -1 time

[0014] Drawing 3: The schematic drawing for objective lens structure and imaging principles in the embodiment

[0015] Drawing 4: The structural schematic drawing for the rod lens steering system **21** by -1 time in the embodiment

[0016] Drawing 5: The schematic drawing for defocus amount and field curvature of objective lens **1** in the embodiment

[0017] Drawing 6: The schematic drawing for defocus amount and field curvature after the objective lens **1** and field lens **3** are combined

[0018] Drawing 7: The schematic drawing for defocus amount and field curvature of steering set **2** in the embodiment

[0019] Drawing 8: The schematic drawing for defocus amount and field curvature of the main endoscope optical system in the embodiment

[0020] Drawing 9: The imaging transfer function for the main endoscope optical system in the embodiment

SPECIFIC EMBODIMENT

[0021] In the embodiment, a 10 mm main laparoscope optical system with a field angle 75 degrees and the numerical aperture 0.12 in the image side is made as an example to clarify the technical scheme and working principle of the invention. The key data is listed to avoid repetition as the device in the embodiment has the same structure as the said structures in the invention fully.

[0022] The objective lens set **1** is structurally illustrated in Drawing 3, including 5 sets of lens. The field lens set **3** is a double-glued crescent lens. The image-transferring set **2** consists of 3 sets of rod lens steering system by -1 time. The rod lens steering system **21** by -1 time is showed schematically in Drawing 4. The front rod lens set **211** contains the positive lens **2111**, negative rod lens **2112** and the positive lens **2113**. The positive lens **2111** is a biconvex lens. The negative rod lens **2112** is a biconcave lens. The positive lens **2113** has the same material, structure and size as the positive lens **2111**. The negative lens **2112** has the same curvature radius in the spherical surface, has the same curvature radius of the glued surface of the positive lens **2111** and **2113**. The defocus amount and field curvature curve are illustrated in Drawing 5. The defocus amount and field curvature curve are illustrated in Drawing for the objective lens set **1** and the field lens set **2**. The defocus amount and field curvature curve are illustrated in Drawing 7 for the steering set **3**. The defocus amount and field curvature curve are illustrated in Drawing 8 for the main endoscope optical system. The transfer function of the main endoscope optical system is illustrated in Drawing 9.

[0023] The working principle is: the objective lens set project the images yielded in the operational field onto the rear focal plane of the objective lens set. The image has the positive defocus amount and positive field curvature. The field lens set projects the telecentric images to the objective plane of the image-transferring set. The location of the virtual image is superposed with the steering set whilst the defocus amount and field curvature diminishes. The imaging principle for the rod lens steering system by -1 time is illustrated in drawings. After 3 sets of rod lens steering system by -1 time, the operational field projects the images onto imaging plane of the final set of rod lens steering system by -1 time finally. The rod lens steering system has a negative defocus amount and negative field curvature. The image difference in the same direction will superpose and the image difference in the reverse direction will offset as the optical system combines. Therefore, the system composed by the objective lens set, the field lens set and image-transferring set is combined, the

defocus amount and field curvature will offset mutually and the main endoscope optical system has the smallest defocus amount and field curvature. As viewed from the defocus amount and field curvature as well as transfer function drawing of the main endoscope optical system, the device in the embodiment has the smallest defocus amount <0.04 mm and field curvature >0.08 mm. As viewed from the transfer function curve, the system has met the imaging requirements for the HD endoscope system.

[0024] The technical scheme of the invention is especially applicable to the minimally invasive surgery under the infrared fluorescent lights, thus addressing the problems of repeated refocusing in traditional endoscope used for such operation.

1. A main endoscope optical system structure that yields parfocal images in the visible (400 nm-700 nm) and near infrared (700 nm-900 nm), including an objective lens group (1), a steering set (2), a field lens set (3), which is characterized in that the objective lens set (1) is an optical lens set. The wavelength 850 nm has a positive field curvature and a positive defocus and the defocus amount is less than 0.5 mm in the imaging plane of the objective lens set (1). The field lens set (3) is placed between the objective lens set (1) and the steering set (2), and located near the imaging place of the objective lens set (1) to form the telecentric virtual images of the objective lens set (1). In the virtual image location, the wavelength 850 nm has a positive defocus amount less than the objective lens set (1), the edge view field has a curvature less than the objective lens set (1), and the steering set (2) is a focus-free system and composed by 3 or 5 sets of identically-structured rod lens steering system (21) by -1 time. The rod lens steering system (21) by -1 time consists of 3 glued lenses, including a front rod lens set (211), a middle rod lens set (212), and a rear rod lens set (213). The middle rod lens set (212) consists of a positive lens (2121), a negative rod lens (2122) and a positive lens (2123) in a gluing way. The positive lens (2121) and the positive lens (2123) are positive biconvex lens. The positive lens (2121) and the positive lenses (2123) are made from the same material in the same structure and size. The negative rod lens (2122) is negative biconcave lens, which are equal in the spherical curvature radius and has the same curvature radius as the glued planes of the positive lens (2121) and the positive lens (2123). The rear rod lens (213) has the same material, structure and size as the front rod lens (211) and arranged symmetrically against the middle rod lens (212). The front rod lens (211), the middle rod lens (212) and the rear rod lens (213) are arranged in coaxial manner. The distance between front rod lens (211) and the middle rod lens (212) is equal to that between the middle rod lens (212) and the rear rod lens (213). The objective distance and image distance of the rod lens steering system (21) by -1 time are equal. The steering system (21) composed by 3 or 5 sets of rod lens by -1 time is arranged in such a way that the objective plane and image plane are superposed in two adjacent sets of rod lens steering systems (21) by -1 time to form the steering set (2). The steering set (2) has the negative defocus amount and negative

field curvature. The defocus amount value is larger than 0.1 mm. The main endoscope optical system composed by the objective lens set (1), the field lens set (3) and the steering set (2) has the smallest defocus amount and less edge view field curvature. The def-focus amount is less than 0.05 mm and the field curvature is less than 0.1 mm. The transfer function MTF value of the central view field is larger than 0.3 at 150 alignment/mm and the transfer function MTF value of the edge view field is larger than 0.2 at 150 alignment/mm.

2. According to claim 1, the said main endoscope optical system structure that yields parfocal images in the visible (400 nm-700 nm) and near infrared (700 nm-900 nm), characterized in that the said field lens set (3) is a double-glued crescent lens.

3. According to claim 1, the said main endoscope optical system structure that yields parfocal images in the visible (400 nm-700 nm) and near infrared (700 nm-900 nm), characterized in that the said front rod lens (211) of the rod lens steering system (21) by -1 time contains a positive lens (2111), a negative lens (2112) and a positive lens (2113). The positive lens (2111) is a positive biconvex lens and the negative rod lens (2112) is a negative biconcave lens. The positive lens (2113) and the positive lens (2111) have the same material, structure and size fully. The negative lens (2112) has the same curvature radius in both spherical surface and has the same curvature radius as the gluing surfaces of the positive lens (2111) and (2113).

4. According to claims 1, 2 and 3, the said main endoscope optical system structure that yields parfocal images in the visible (400 nm-700 nm) and near infrared (700 nm-900 nm), characterized in that a 10 mm main laparoscope optical system with a field angle 75 degrees and the numerical aperture 0.12 in the image side. The objective lens set (1) is structurally illustrated in Drawing 3, including 5 sets of lens. The field lens set (3) is a double-glued crescent lens. The image-transferring set (2) consists of 3 sets of rod lens steering system by -1 time (21). The rod lens steering system by -1 time (21) is showed schematically in Drawing 4. The front rod lens set (211) contains the positive lens (2111), negative rod lens (2112) and the positive lens (2113). The positive lens (2111) is a biconvex lens. The negative rod lens (2112) is a biconcave lens. The positive lens (2113) has the same material, structure and size as the positive lens (2111). The negative lens (2112) has the same curvature radius in the spherical surface, has the same curvature radius of the glued surface of the positive lens (2111) and (2113). The defocus amount and field curvature curve are illustrated in Drawing 5. The defocus amount and field curvature curve are illustrated in Drawing for the objective lens set (1) and the field lens set (2). The defocus amount and field curvature curve are illustrated in Drawing 7 for the steering set (3). The defocus amount and field curvature curve are illustrated in Drawing 8 for the main endoscope optical system. The transfer function of the main endoscope optical system is illustrated in Drawing 9.

* * * * *

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[标]申请(专利权)人(译)	青岛奥美克医疗科技有限公司		
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摘要(译)

内窥镜主光学系统技术领域本发明涉及一种内窥镜主光学系统，尤其涉及一种在可见光和近红外光下进行局部成像的内窥镜主光学系统，属于微创手术技术领域。使用的方法是：物镜组具有正离焦和正场曲率。转向装置具有负离焦和负的场曲率。此外，在物镜组和转向装置之间增加了一个场镜组。场镜组位于物镜组焦点附近。在将场镜与物镜组合后，它将具有与转向装置匹配的正离焦和正场曲率，使得850米散焦量小于0.05mm并且边缘场曲率小于主内窥镜光学系统为0.1 mm。该系统具有良好的成像能力。本发明控制红外线中的散焦量和场曲率通过偏移物镜组，场镜组和转向装置的负和正离焦量和场曲率，可见光带；它确保了主内窥镜光学系统的成像质量，有效地解决了难以在物镜组和转向装置的宽光谱范围内实现图像差异校正的缺点；与传统的HOPKINS转向系统结构相比，它具有加工更简单，控制精度更高，成本更低等优点；特别适用于红外荧光灯下的微创手术，解决了传统内窥镜重复使用的问题。

