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(54) **LAPAROSCOPIC SURGICAL SCAFFOLD**

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A61B 90/50 (2016.01)
A61B 17/00 (2006.01)

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5/0084 (2013.01); **A61B 17/0281** (2013.01); **A61B 90/30** (2016.02); **A61B 90/50** (2016.02); **A61B 2017/00283** (2013.01); **A61B 2017/00477** (2013.01)

(58) **Field of Classification Search**

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USPC **600/222**, **229**, **233**, **234**
See application file for complete search history.

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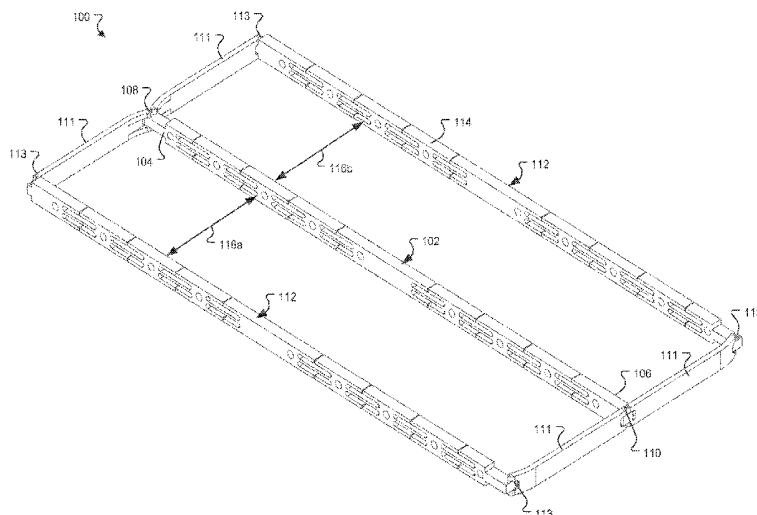
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(57) **ABSTRACT**

A collapsible scaffolding can collapse for deployment to a laparoscopic surgical site through a trocar or the like, and can expand to provide a surface for organ retraction within a body cavity. In the expanded state, the scaffolding may assist a surgical procedure in a variety of ways, such as by providing a rigid structure upon which to secure retracted organs or surgical tools such as lights, cameras, and so forth.

21 Claims, 8 Drawing Sheets



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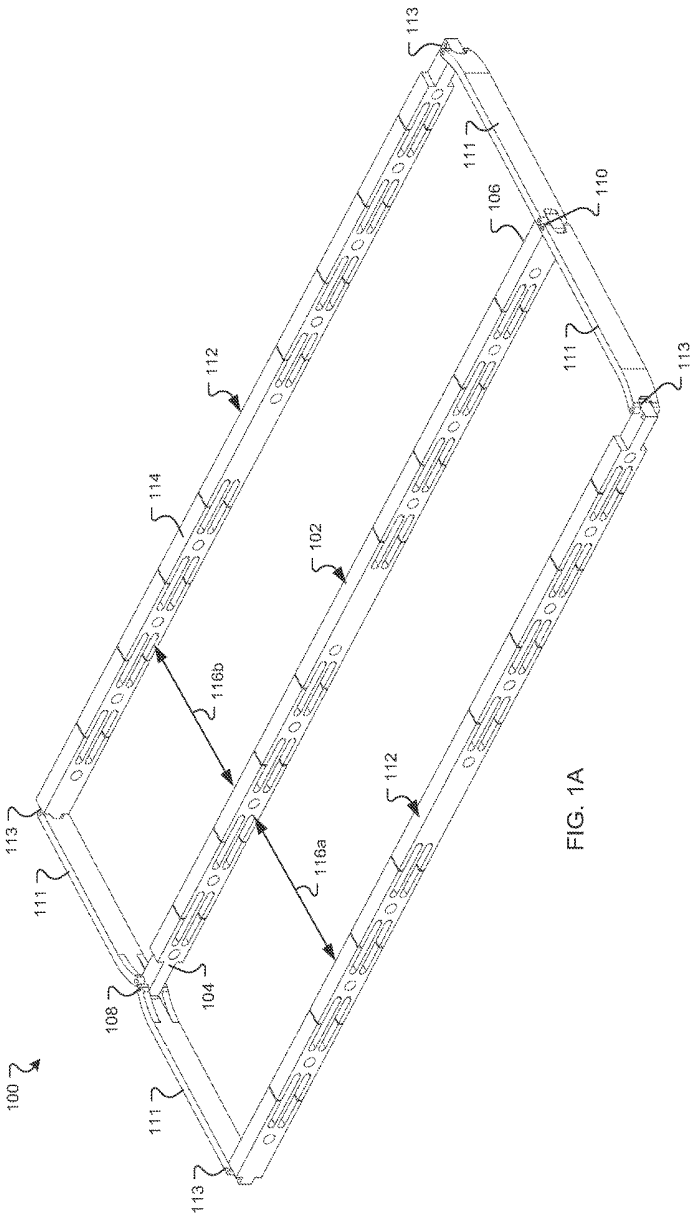
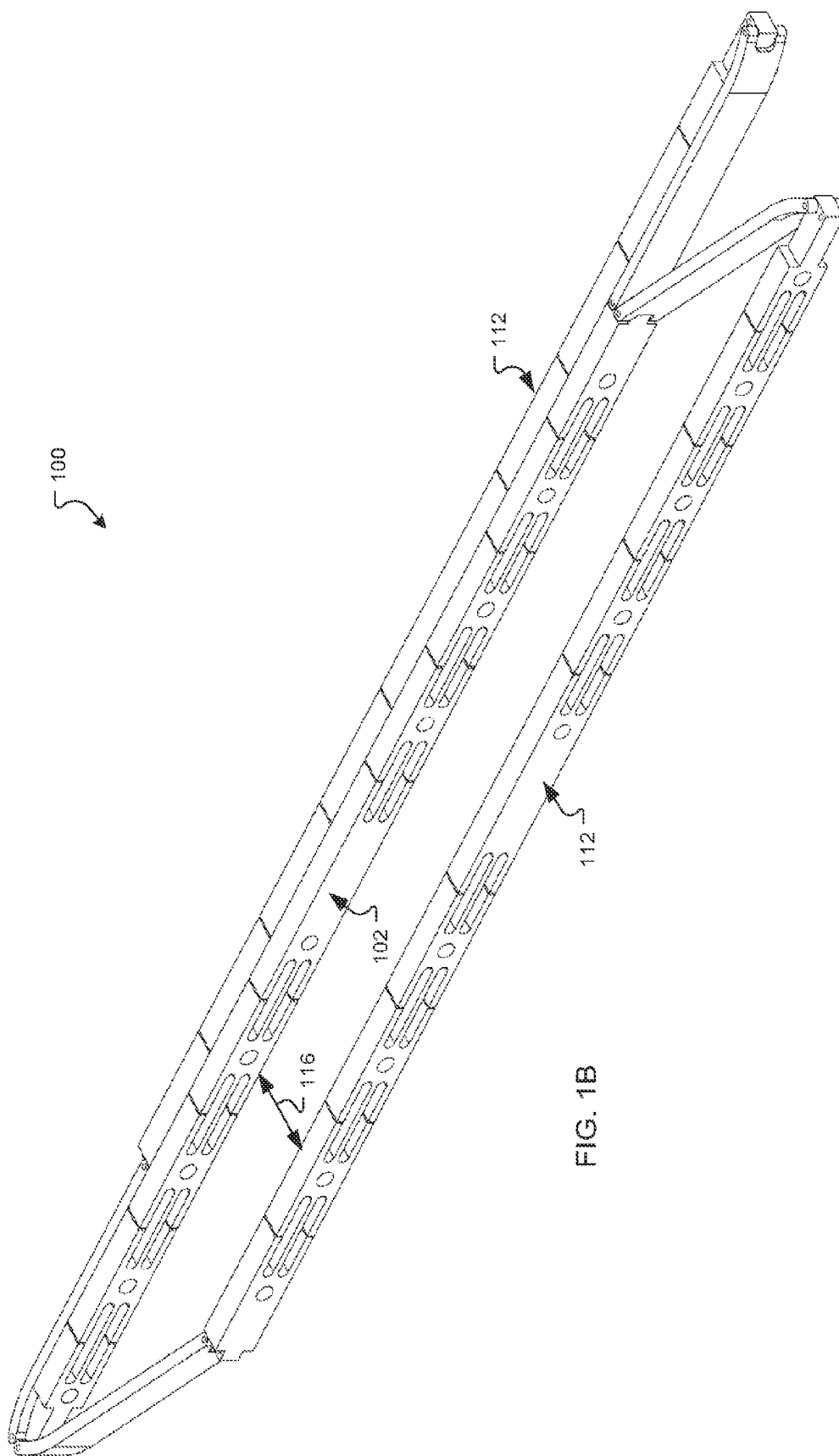


FIG. 1A



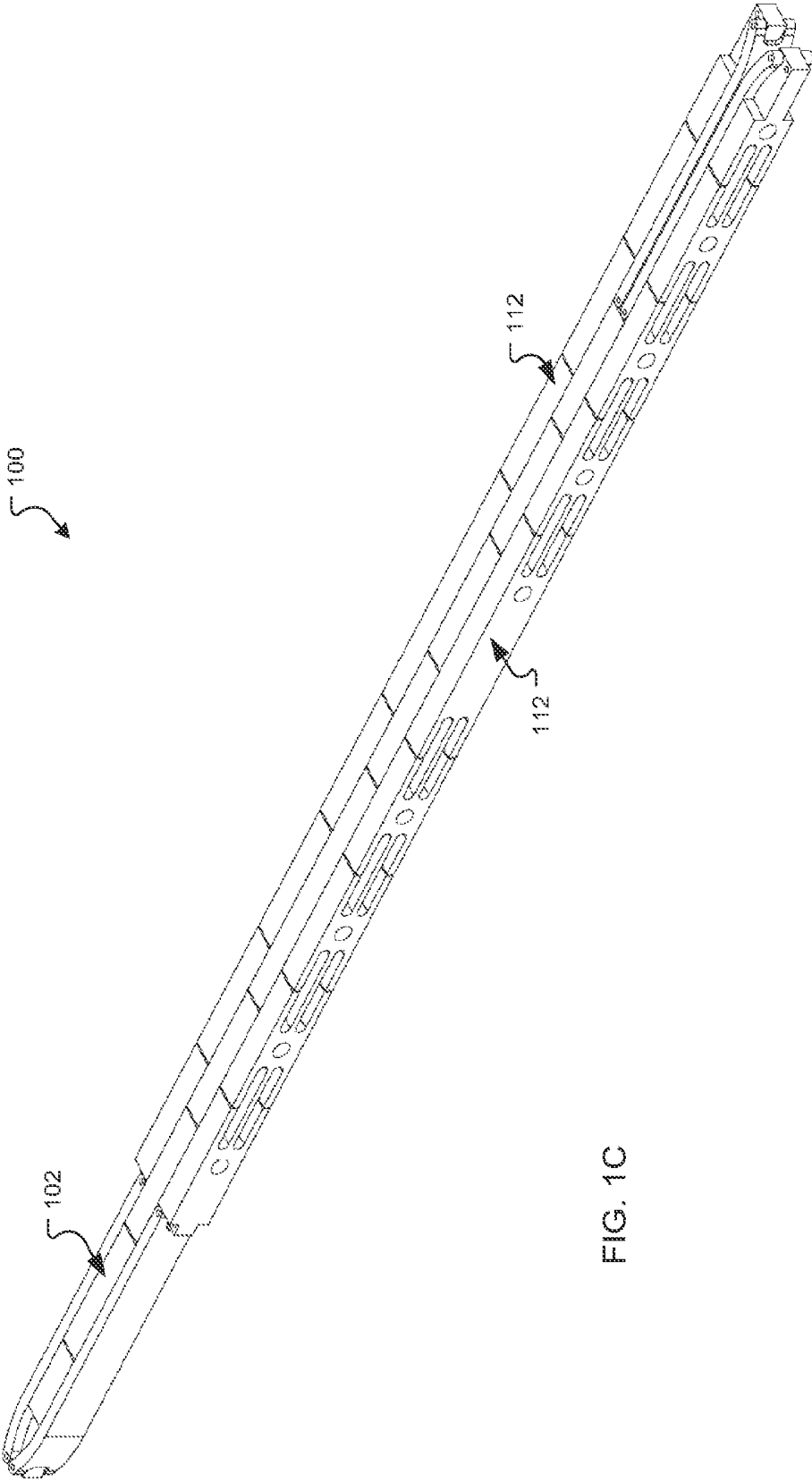


FIG. 1C

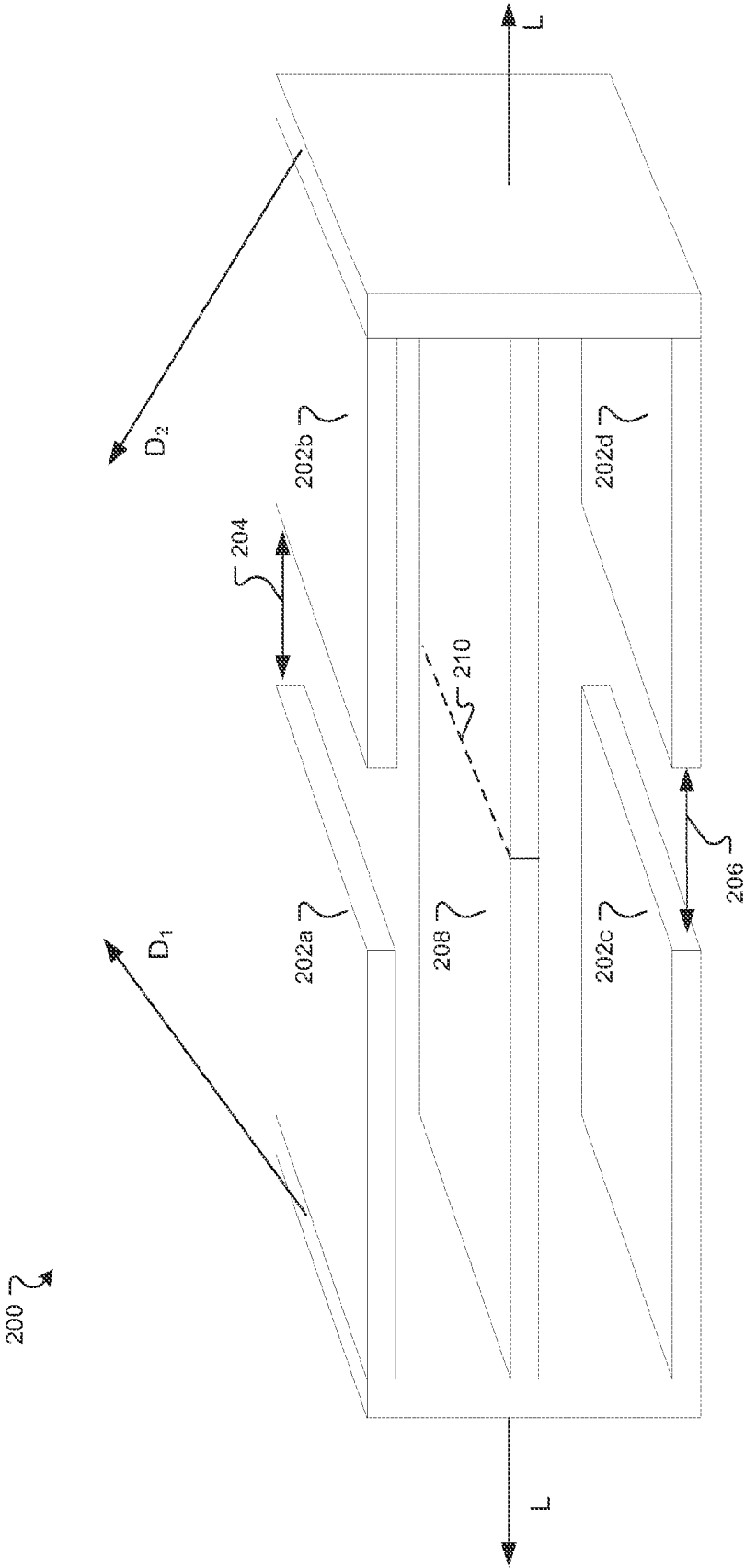
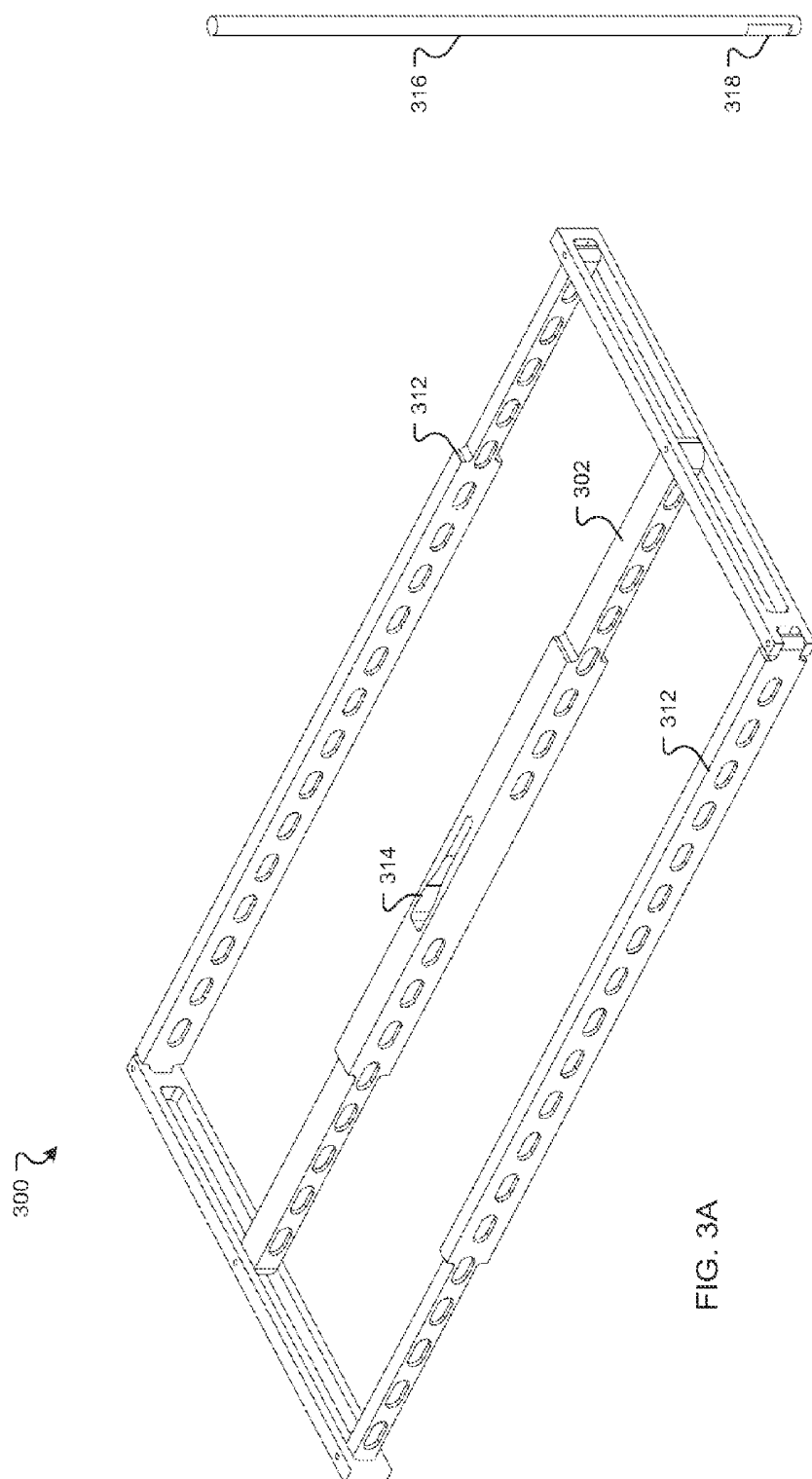
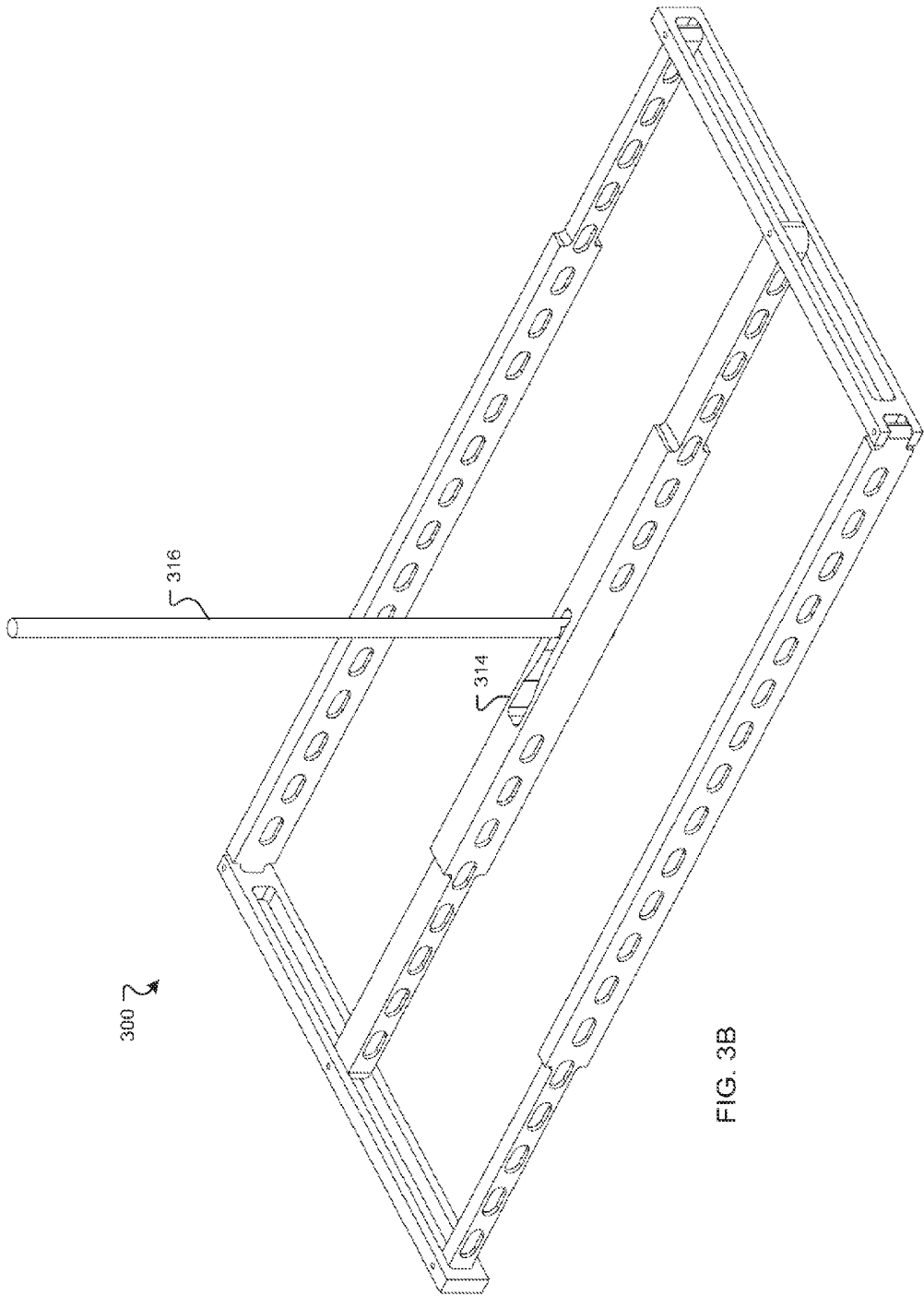


FIG. 2





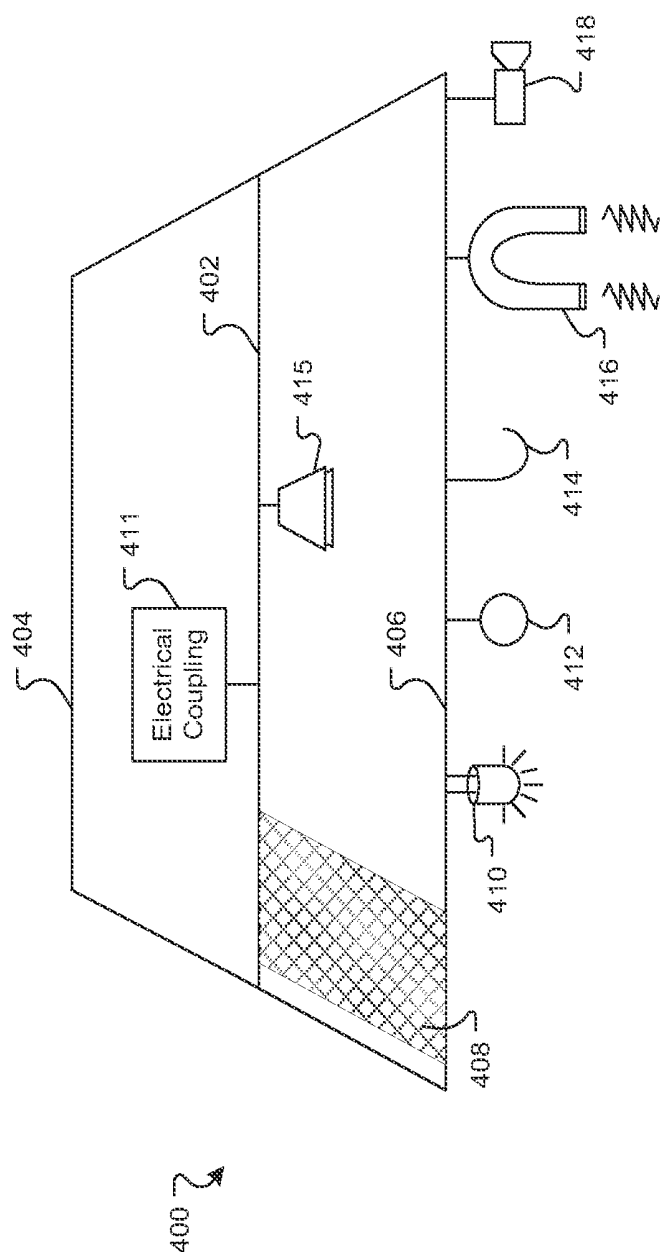


FIG. 4

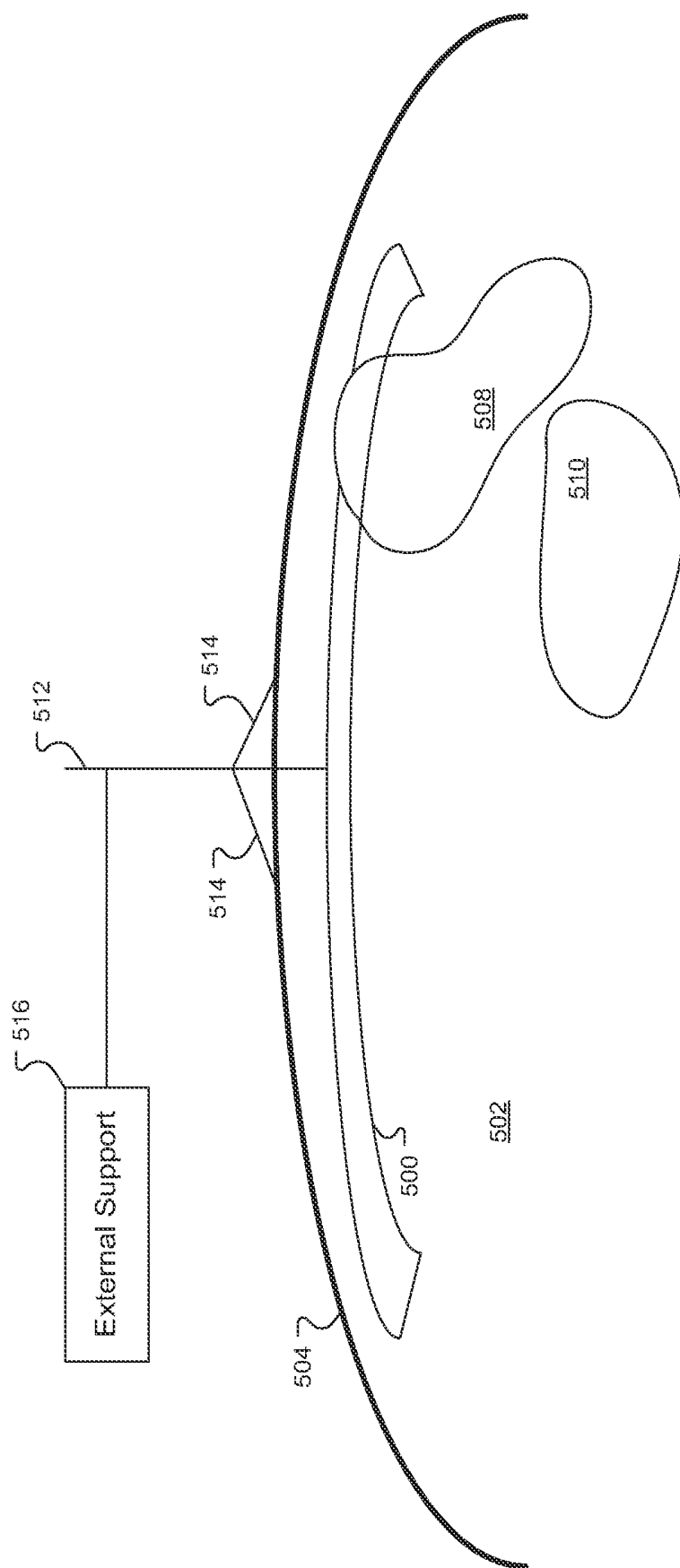


FIG. 5

LAPAROSCOPIC SURGICAL SCAFFOLD

CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims the benefit of U.S. Provisional App. 61/671,140, filed Jul. 13, 2012, the entirety of which is incorporated herein by reference.

BACKGROUND

Laparoscopic surgery involves creating one or more relatively small incisions in a subject that provide a surgeon's tools with access to a surgical site. Laparoscopic surgery enjoys certain advantages over more invasive procedures because the small surgical incisions often require less time to heal, are less painful, and leave smaller scars. On the other hand, in these minimally invasive techniques a surgeon generally operates in a highly constrained space within a patient's body such as the abdominal cavity.

Moreover, inside the abdominal cavity, organs and other tissue may obstruct access to a surgical site. For example, with a patient lying supine on an operating table, the patient's liver typically covers the gallbladder. Thus, laparoscopic procedures on a gallbladder often involve a precursor step of moving and securing the patient's liver away from the surgical site. This typically requires an additional person to manipulate the liver during the procedure and perform related tasks such as manipulating a light or camera, which can further limit the surgeon's working space inside and outside the abdominal cavity.

There remains a need for improved surgical tools to simplify laparoscopic surgical procedures.

SUMMARY

A collapsible scaffolding can collapse for deployment to a laparoscopic surgical site through a trocar or the like, and can expand to provide a surface for organ retraction within a body cavity. In the expanded state, the scaffolding may assist a surgical procedure in a variety of ways, such as by providing a surface to manually expand the cavity, or by providing a rigid structure upon which to secure retracted organs or surgical tools such as lights, cameras, and so forth.

BRIEF DESCRIPTION OF THE FIGURES

The invention and the following detailed description of certain embodiments thereof may be understood by reference to the following figures:

FIG. 1A is a perspective view of a surgical scaffold in a deployed state.

FIG. 1B is a perspective view of a surgical scaffold in a partially deployed state.

FIG. 1C is a perspective view of a surgical scaffold in an undeployed state.

FIG. 2 is a schematic view of a flexural structure.

FIGS. 3A and 3B are a perspective view of a surgical scaffold with a retaining member.

FIG. 4 is a schematic view of a surgical scaffold with additional elements.

FIG. 5 is a schematic view of a surgical scaffold deployed during a surgical procedure.

DETAILED DESCRIPTION

In the following description, references to items in the singular should be understood to include items in the plural,

and vice versa, unless explicitly stated otherwise or clear from the context. Grammatical conjunctions are intended to express any and all disjunctive and conjunctive combinations of conjoined clauses, sentences, words, and the like, unless otherwise stated or clear from the context. Thus the term "or" should generally be understood to mean "and/or" and so forth.

Terms of degree, such as "about" or "substantially" are intended to contemplate a range of values within the ordinary variability expected by one of ordinary skill in the art and suitable for the uses contemplated herein.

Among other things, disclosed herein are various embodiments of a surgical scaffold device that can be deployed in a laparoscopic procedure. Among other advantages, the scaffold helps mitigate some of the difficulties associated with certain laparoscopic procedures discussed above.

FIG. 1A is a perspective view of a surgical scaffold in a deployed state. The scaffold 100 may include a primary member 102 having a front end 104 and a back end 106. As used herein, the terms "front" and "back" are arbitrary terms employed for convenience only. These terms are not intended to convey any preferred orientation, function, or structure, or to suggest any intrinsic difference or similarity between the ends of the scaffold, or any other components referred to herein as "front" and "back" components. While certain differences may be noted below, these are provided only by way of exemplary embodiments and are not intended to limit the meaning of the terms "front" and "back" as described above. Similarly, terms such as "top" and "bottom" are provided for convenience only, and are not intended to convey any specific orientation, function, or structure unless explicitly noted to the contrary or otherwise clear from the context.

The primary member 102 may be coupled to lateral support members 111 by one or more front hinges 108 and back hinges 110. The hinges 108, 110 may, for example, be barrel hinges, pivot hinges, mortise hinges, flexural hinges, or any other type(s) of hinges suitable for use in a surgical device. The hinges 108, 110 may be integrally formed into the material of the primary member 102 and lateral support members 111 where these members meet, or the hinges 108, 110 may be separate mechanical components attached as appropriate to these members. In order for the scaffold 100 to deploy into a resilient working surface, the hinges 108, 110 may collectively articulate in a plane of articulation that contains the scaffold 100 (if the scaffold is not flexed, as described below). That is, the hinges 108, 110 may constrain motion of the connected elements so that they remain within a plane formed by the deployed scaffold 100, or stated alternatively, the hinges 108, 110 may rotate about an axis perpendicular to the plane formed by the deployed scaffold 100.

A lateral support member 111 may be rotatably coupled to the primary member 102 at each hinge 108, 110. Ancillary members 112 may be rotatably coupled to the lateral support member 111 by hinges 113. Although FIG. 1A shows two ancillary members 112, in principle any number of ancillary members may be employed. The terms "primary" and "ancillary" are terms of convenience only; there need not be any structural differences (or similarities) between primary and ancillary members, except in certain embodiments as noted below. The term "axial member" is used to collectively refer to either the primary or any ancillary member.

The primary member 102 and ancillary members 112 may include one or more flexural structures 114. The flexural structures 114 may be any structure(s) that allow a member to flex in a direction outside the plane of the scaffold. The

flexural structures **114** may be advantageously constructed, e.g., as shown below, to facilitate planar deflection of the scaffold **100** while inhibiting in-plane movement (e.g., lateral displacement) of the individual axial members. Any suitable flexural structure **114** may be used, including but not limited to hinges, springs, or the like. Further details of some flexural elements suitable for use as the flexural structures **114** of the scaffold **100** are provided below.

The “deployed” state is characterized by the distances **116a, b** between the primary member **102** and the ancillary members **112** being maximized, or more generally greater than a partially deployed or undeployed state.

FIG. 1B is a perspective view of the surgical scaffold in a partially deployed state. In general, the hinges described above facilitate a range of in-plane movements of the axial members of the scaffold **100** relative to one another between an undeployed state and a deployed state. A “partially deployed” state may be any relative position of the axial members characterized by at least one inter-member distance **116** between an ancillary member **112** and the primary member **102** being greater than in the undeployed state and less than in the deployed state. More specifically as depicted, one ancillary member **112** is fully collapsed and in contact with the primary member **102**, while a second ancillary member **112** is partially collapsed

FIG. 1C is a perspective view of the surgical scaffold in an undeployed state characterized by a minimized distance between the primary member **102** and the ancillary members **112**. Although FIG. 1C shows an undeployed state with a minimized distance of zero—i.e., the members are in contact—in general this contact need not occur in an undeployed state.

In some uses, the scaffold **100** may be inserted into a patient’s body through a trocar. Thus, in the undeployed state, the maximum cross-sectional distance across the scaffold **100** in a plane perpendicular to the axes of the members **102, 112** may be small enough to fit through such a trocar. Trocars in common use today may have inner diameters of approximately 10-15 mm, and the undeployed scaffold **100** may correspondingly have a cross section (perpendicular to the axis of the primary member **102**) with a diameter of about 10-15 mm. In one aspect, the cross-sectional form of the ancillary members may be rounded or otherwise shaped to fit within a trocar barrel.

In some implementations, the length of scaffold **100** in the undeployed state may be long enough to fulfill the functions described herein, but not so long as to pose a safety risk to the patient during insertion through the trocar. In some implementations, the length of the scaffold **100** in its deployed state may be about eight inches, or between about seven inches and about ten inches. The ancillary members may be any suitable length, such as between about one inch and about two inches.

The scaffold **100** may be constructed of any material or combination of materials suitable for insertion into a living patient. This may include, for example, alloys such as surgical stainless steel, shape memory alloys, polymers, plastics, or the like. In one aspect, the scaffold **100** may be formed of relatively inexpensive materials such as a biocompatible polymer for use as a disposable surgical tool. In another aspect, the scaffold **100** may be formed of a surgical stainless steel or other autoclavable material suitable for repeated use.

FIG. 2 is a schematic view of an exemplary flexural structure. The flexural structure **200** is shown relative to an axis **L** of the axial member that incorporates the flexural structure **200**.

The flexural structure **200** may include axial protrusions **202a, b, c, d** that extend axially toward one another without contacting one another when the flexural structure **200** is unflexed. The axial protrusions **202a, 202b** may form a top layer that defines a top gap **204**. Similarly, the axial protrusions **202c, 202d** may form a bottom layer that defines a bottom gap **206**. In general, the dimensions of the protrusions **202a, 202b, 202c, 202d** (and therefore, the dimensions of the top and bottom gaps) need not be identical.

The flexural structure **200** may also include a middle layer **208**. The middle layer may include a flexible region **210**. Although shown schematically as a line in FIG. 2, the flexible region **210** may extend throughout the entire middle layer **208**, or any subset thereof. The middle layer **208**, and more generally, the flexible structure **200**, may be formed from any resilient material suitable for insertion into a living patient, including the materials described above. In some implementations, the middle layer and/or flexible region may be relatively narrow, thereby providing sufficiently low stiffness to allow a desired degree of flexure. Similarly, the thickness of the middle layer **208** may depend upon the desired stiffness of the flexural structure **200**, the material from which the flexural structure **200** and/or middle layer **208** are formed, and any other appropriate design constraints. For example, for a particular, predetermined stiffness, a substantially thicker middle layer **208** may be required if the middle layer **208** is formed from a medical grade polyurethane rather than surgical stainless steel.

When flexure-inducing forces are applied to the flexural structure **200**, for example in the directions **D₁** and **D₂** shown in FIG. 2, the ends of the structure **200** will deflect, and the middle layer will flex, e.g. at the flexible region **210**. As the flexural structure **200** continues to flex, one of the gaps **204** and **206** may shrink. For example, when the ends of the structure **200** move in the directions **D₁** and **D₂**, the top gap **204** tends to close. If enough flex-inducing force is applied, then eventually an opposing pair of the protrusions **202a-d** may come in contact, and the gap they define may disappear. In this state, the contact between the protrusions tends to inhibit any further flexure of the flexural structure **200**. Thus, upward or downward flexural limits may be individually implemented at various points along the axial members by choosing the size of the top or bottom gaps **204, 206** at those points.

In some implementations, it may be desirable for the scaffold **100** to conform to the curved wall of a typical human’s abdomen. As such, the flexural structures **200** may be shaped and sized to accommodate a corresponding deflection in the axial members of a scaffold. In some implementations, the axial members may be configured using the flexural structures **200** to permit an end-to-end deflection of some predetermined angle, such as five degrees or less, but to inhibit end-to-end deflection greater than the predetermined angle. It is within the ordinary skill in the art to determine shapes and sizes of the protrusions and gaps in each flexural structure **200** to accommodate this predetermined flexing behavior, and the variations and details are omitted here. In some implementations, an axial member may include flexural structures **200** and gaps/protrusions at predetermined intervals (e.g., at a pitch of one inch) or of a predetermined number to create a desired flexing behavior of the axial member(s).

FIG. 3A is a perspective view of a surgical scaffold with a retaining member. The scaffold **300** may include a primary member **302** and ancillary members **312** as described above. The scaffold **300** may also include a coupling **314** such as a through-hole with one or more coupling or registration

features to removably and replaceably receive a retaining member **316** in a manner that facilitates manipulation of the scaffold **300** with the retaining member **316**. Although the coupling **314** is shown in the primary member **302**, in principle the coupling **314** can be located anywhere on the scaffold **300**.

A separate retaining member **316** may also be provided. As described below, the retaining member **316** may be operable to help keep the scaffold **300** in place while the scaffold is deployed within a patient. The retaining member **316** may include a coupling **318** at its distal end that is configured to mate with the coupling **314** on the scaffold **300**. FIG. 3B shows the retaining member **316** coupled to the scaffold **300** via the couplings **314** and **318** (not shown).

When the retaining member **316** is coupled to the scaffold **300**, the couplings **314**, **318** may be configured to allow the retaining member **316** to provide the scaffold with torque, a normal force, and an in-plane force in at least some directions. In this context, “normal” connotes the direction perpendicular to the plane of the scaffold, and “in-plane” connotes a direction parallel to the plane of the scaffold. In some implementations, applying force in certain in-plane directions is operable to disengage the retaining member **316** from the coupling **314**, but force in other in-plane directions is operable to transfer such force to the scaffold **300**. In some implementations, through a combination of applied normal and in-plane forces, the retaining member **316** may transfer a retaining force to the scaffold. “Retaining force” connotes force in a direction that is counter to the load on the scaffold **300** by an organ retained thereon. Thus, by application of a retaining force, the retaining member **316**, may permit a surgeon to lift or otherwise retract an organ from a surgical site within an abdominal cavity.

The retaining member **316** may be inserted through the patient’s abdominal cavity to engage the scaffold **300** once the scaffold has been deployed within the cavity. In some implementations, the retaining member **316** has a cross-sectional area small enough to minimize scarring in the resultant puncture. In some implementations, the retaining member **316** may have maximum cross sectional distance less than two millimeters.

In some implementations, the couplings **314**, **316** may also include an electrical coupling. The electrical coupling may be operable to provide power or control signals from an external source to additional elements on the scaffold **300**, as described more fully below. In some implementations, one or more electrical couplings can be located elsewhere on the scaffold **300**. In some implementations, the electrical couplings can receive power or control signals through one or more wires fed through the insertion trocar.

FIG. 4 is a schematic view of a surgical scaffold with additional elements. The additional elements described below may be useful during some laparoscopic procedures.

The scaffold **400** may have a short ancillary member **404** and a long ancillary member **406** so that the scaffold deploys in the shape of a trapezoid. This may be advantageous when an anticipated use of the scaffold **400** involves positioning it with one end (e.g., the short end) in a relatively small space, such as abutting the patient’s diaphragm. More generally, the scaffold **400** can include ancillary members having different dimensions that result in any other perimeter geometry that conforms to an anticipated deployment site.

The scaffold **400** may include a mesh **408** deployed between two members. The mesh **408** may advantageously help retain some of the patient’s anatomical structures in a safe location during the surgical procedure. The mesh **408** may be constructed from any suitable biocompatible mate-

rial, including polymer threads such as nylon or polyester, natural threads such as silk, or the like. Although the mesh **408** is shown in only a portion between the members **402** and **406**, in principal the mesh **408** can extend throughout the entire space between any two members, or any portion thereof.

The scaffold **400** may include one or more light sources **410**, including but not limited to light emitting diodes (LEDs). The light source **410** may provide illumination to the surgical site. Moreover, using more than one light source **410** may mitigate the effect of shadows and reduce the chances of obstructing illumination with the movement of surgical instruments. As such, the scaffold **400** may include two light sources, three light sources, or any other number of light sources suitable for illuminating surfaces of interest in a surgical procedure. In some implementations, the light sources **410** may be provided with power and/or control signals from an external source via the retaining member through an electrical coupling **411**.

The scaffold **400** may include one or more loops **412**. The loops **412** may advantageously serve as tie points that can be used to anchor organs or other surgical tools to the scaffold **400** using surgical thread, clamps, or the like. Similarly, the scaffold **400** may include one or more hooks **414** or clamps **415** that may be similarly employed to secure tissue or surgical instruments as appropriate.

The scaffold **400** may include a high-friction surface (e.g., the top side or a portion thereof), such as a textured or knurled surface, that may help promote organ retention. The top side of the scaffold **400** may also or instead include one or more regions having a relatively soft or pliable coating to mitigate irritation to the patient’s abdominal wall or diaphragm from the scaffold **400**. The pliable coating may include any soft surgical material, such as rubber, silicone, other elastomers, or the like.

The scaffold **400** may include one or more magnets **416**. The magnets **416** may include permanent magnets or electromagnets. In embodiments involving electromagnets, the electromagnets **416** may receive power and/or control signals from an external source via the retaining member through an electrical coupling **411**. The magnets **416** may advantageously provide locations to easily and securely place magnetic surgical tools or other magnetic materials.

The scaffold **400** may include one or more video cameras **418**. The video camera(s) **418** may receive power and/or control signals from an external source via the retaining member through an electrical coupling **411**. The video camera(s) **418** may also send a video signal to an outside receiver through the electrical coupling, or the video camera(s) **418** may transmit video wirelessly using, e.g., radio frequency communications. The video camera(s) **418** may be movably connected to the scaffold **400**, such as by removably and replaceably coupling a video camera **418** to the scaffold **400**, or by including a universal joint or the like in a mechanical coupling from the video camera **418** to the scaffold **400**. In this manner, the field of view of one of the video cameras **418** may be adjusted during the surgical procedure. In some implementations, two or more cameras **418** may be mounted on the scaffold **400** such that every camera has a field of view that overlaps with the field of view of at least one other camera.

FIG. 5 is an exemplary schematic cross-sectional view of a surgical scaffold deployed in a human patient during a surgical procedure. In this example, the scaffold **500** is deployed within the abdominal cavity **502** defined in part by the patient’s abdominal wall **504**. An obstructing organ **508** (e.g., the liver) is secured to the platform **500** by any of the

techniques described above, thus exposing the surgical target **510** (e.g., the gallbladder). Thus, a surgeon may access the surgical target **510**. Moreover, the overhead clearance of the surgical target **510** is relatively well utilized, inasmuch as the scaffold **500** substantially conforms to the patient's abdominal wall **504**. Although FIG. 5 shows a gap between the scaffold **500** and the abdominal wall **504**, this has been shown for clarity. The scaffold **500** may contact the abdominal wall **504** to a substantial degree, such as where the scaffold **500** is also used to lift the abdominal wall **504** away from the surgical site.

The scaffold **500** is held in place by a retaining member **512**. In some implementations, the retaining member **512** may be further stabilized with support structures **514** that mechanically couple the retaining member to the patient. In some implementations, the retaining member **512** may be further stabilized via a mechanical coupling to an external support **516**. The external support **516** may include any manner of structures—e.g., clamps, graspers, vices, magnets, actuators, etc.—that may be collectively operable to hold the retaining member **512** in a fixed or otherwise controllable position.

While the invention has been disclosed in connection with the preferred embodiments shown and described in detail, various modifications and improvements thereon will become readily apparent to those skilled in the art. Accordingly, the spirit and scope of the present invention is not to be limited by the foregoing examples, but is to be understood in the broadest sense allowable by law.

What is claimed is:

1. A device comprising:
 - a primary member having:
 - a front end and a back end;
 - a front hinge and a back hinge, that collectively articulate in a plane of articulation;
 - an ancillary member movably connected to the primary member via the front hinge and the back hinge; wherein the primary member and ancillary member are:
 - constructed from a surgical material; and
 - individually flexible in a direction perpendicular to the plane of articulation to a degree substantially conforming to a human abdomen; and further wherein the device is configured to transition between a first state and a second state by articulating the hinges, in which the first state is characterized by minimizing a distance between the primary member and the ancillary member and the second state is characterized by maximizing the distance between the primary member and the ancillary member, in which a maximum device cross section in the first state is suitable for insertion through a trocar in a laparoscopic procedure on a human; and
 - a number of independent flexural structures in each of the primary member and ancillary member to facilitate flexure in the direction perpendicular to the plane of articulation, each independent flexural structure including an opposing pair of axial protrusions extending toward one another across a gap within the plane of articulation when the flexural structure is unflexed, wherein the opposing pair of axial protrusions impose a flexural limit at a point where a deflection of a corresponding one of the independent flexural structures causes the opposing pair of axial protrusions to come in contact across the gap.
2. The device of claim 1, wherein each one of the flexural structures includes a top layer, a flexible middle layer, and a bottom layer, in which the top and bottom layers each include a plurality of gaps that facilitate a deflection of the

flexible middle layer and inhibit the deflection beyond an upward and a downward flexural limit according to a size of one or more corresponding top or bottom ones of the plurality of gaps.

3. The device of claim 1, further including an electrical coupling site.

4. The device of claim 3, further comprising a light source electrically coupled to the electrical coupling.

5. The device of claim 4, wherein the light source is movably coupled to at least one of the primary member and the ancillary member.

6. The device of claim 3, further comprising a camera electrically coupled to the electrical coupling site.

7. The device of claim 6, wherein the camera is movably coupled to at least one of the primary member and the ancillary member.

8. The device of claim 6, further comprising a plurality of cameras, each camera having a corresponding field of view, wherein the field of view of any camera in the plurality overlaps with at least one other field of view of at least one other camera in the plurality.

9. The device of claim 1, further comprising an attachment point for anchoring an organ.

10. The device of claim 9, wherein the attachment point is selected from the group consisting of: a textured surface, a hook, a clamp, a loop, and a magnet.

11. The device of claim 10, wherein a perimeter of the device bears a trapezoidal geometry when the device is in the second state.

12. The device of claim 1, further comprising a pliable mesh between the primary and ancillary members.

13. The device of claim 1, wherein the articulating hinges include a shape memory alloy.

14. The device of claim 1, wherein a top side of the device is constructed from a soft material.

15. The device of claim 1, further comprising a second ancillary member coupled to the primary member.

16. The device of claim 1, wherein the primary member further has a first coupling configured to mechanically couple to a retaining member not in the plane of articulation.

17. The device of claim 16, wherein the first coupling is dimensioned to mechanically couple to a retaining member of cross sectional area less than four square millimeters.

18. The device of claim 16, wherein the first coupling is configured to transfer torque, normal force, and in-plane force in at least one direction from the retaining member to the device.

19. A device comprising:

- a primary member having:
 - a front end and a back end;
 - a front hinge, a back hinge, that collectively articulate in a plane of articulation;

- an ancillary member movably connected to the primary member via the front hinge and the back hinge; wherein the primary member and ancillary member are:

- constructed from a surgical material; and
- individually flexible in a direction perpendicular to the plane of articulation and configured to inhibit deflection greater than five degrees; and further wherein

the device is configured to transition between a first state and a second state by articulating the hinges, in which the first state is characterized by minimizing a distance between the primary member and the ancillary member and the second state is characterized by maximizing the distance between the primary member and the ancillary members, in which a maximum device cross section in

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the first state is suitable for insertion through a trocar in a laparoscopic procedure on a human; and
 a number of independent flexural structures in each of the primary member and ancillary member to facilitate flexure in the direction perpendicular to the plane of articulation, each independent flexural structure including an opposing pair of axial protrusions extending toward one another across a gap within the plane of articulation when the flexural structure is unflexed, wherein the opposing pair of axial protrusions impose a flexural limit at a point where a deflection of a corresponding one of the independent flexural structures causes the opposing pair of axial protrusions to come in contact across the gap.

20. The device of claim 19, wherein the device further includes a first coupling configured to mechanically couple to a retaining member not in the plane of articulation.

21. An expandable structure having an expanded state forming a plane shaped and sized to support an organ during a minimally-invasive surgical procedure and a collapsed state shaped and sized to fit through a trocar for delivery to a surgical site for the minimally-invasive surgical procedure, the expandable structure comprising:

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two or more axial members, each individually flexible in a direction perpendicular to the plane to conform to an abdominal cavity;

two or more lateral support members;

a number of hinges coupling the two or more lateral support members to the two or more axial members to facilitate a movement of the axial members and lateral support members within the plane between the expanded state and the collapsed state; and

a number of independent flexural structures in each of the two or more axial members to facilitate flexure in the direction perpendicular to the plane, each independent flexural structure including an opposing pair of axial protrusions extending toward one another across a gap within the plane when the flexural structure is unflexed, wherein the opposing pair of axial protrusions impose a flexural limit at a point where a deflection of a corresponding one of the independent flexural structures causes the opposing pair of axial protrusions to come in contact across the gap.

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摘要(译)

可折叠的脚手架可以通过套管针等塌缩以便部署到腹腔镜手术部位，并且可以扩张以提供用于体腔内器官收缩的表面。在扩张状态下，脚手架可以以各种方式辅助外科手术，例如通过提供刚性结构，在该刚性结构上固定缩回的器官或手术工具，例如灯，照相机等。

