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(12) **United States Patent**
Kuslich et al.

(10) **Patent No.:** **US 7,135,026 B2**
 (45) **Date of Patent:** ***Nov. 14, 2006**

(54) **LAPAROSCOPIC SPINAL STABILIZATION
 SURGICAL METHOD**

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 (US)

(73) Assignee: **Zimmer Spine, Inc.**, Minneapolis, MN
 (US)

(*) Notice: Subject to any disclaimer, the term of this
 patent is extended or adjusted under 35
 U.S.C. 154(b) by 0 days.

This patent is subject to a terminal dis-
 claimer.

(21) Appl. No.: **10/627,589**

(22) Filed: **Jul. 25, 2003**

(65) **Prior Publication Data**

US 2004/0082957 A1 Apr. 29, 2004

Related U.S. Application Data

(60) Continuation of application No. 09/369,614, filed on
 Aug. 6, 1999, now Pat. No. 6,599,320, which is a
 continuation of application No. 08/902,746, filed on
 Jul. 29, 1997, now abandoned, which is a division of
 application No. 08/752,818, filed on Nov. 21, 1996,
 now Pat. No. 5,947,971, which is a continuation of
 application No. 08/482,025, filed on Jun. 7, 1995,
 now Pat. No. 5,720,748, which is a division of
 application No. 08/299,807, filed on Sep. 1, 1994,
 now Pat. No. 5,489,307, which is a continuation of
 application No. 08/015,863, filed on Feb. 10, 1993,
 now abandoned.

(51) **Int. Cl.**
A61B 17/17 (2006.01)
A61B 17/90 (2006.01)

(52) **U.S. Cl.** 606/90; 606/96

(58) **Field of Classification Search** 606/80,
 606/90, 96

See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

669,764 A	3/1901	Potter
3,848,601 A	11/1974	Ma et al.
3,875,595 A	4/1975	Froning
4,349,921 A	9/1982	Kuntz
4,545,374 A	10/1985	Jacobson
4,596,243 A	6/1986	Bray
4,686,972 A	8/1987	Kurland
4,743,256 A	5/1988	Brantigan
4,772,287 A	9/1988	Ray et al.
4,834,757 A	5/1989	Brantigan
4,878,915 A	11/1989	Brantigan
4,904,260 A	2/1990	Ray et al.
4,961,740 A	10/1990	Ray et al.
5,015,247 A	5/1991	Michelson

(Continued)

FOREIGN PATENT DOCUMENTS

DE 3505567 A1 6/1986

(Continued)

OTHER PUBLICATIONS

Declaration of Douglas Kohrs, filed in patent U.S. Appl. Ser. No.
 08/752,818, the original was filed in related U.S. Appl. Ser. No.
 08/015,863.

(Continued)

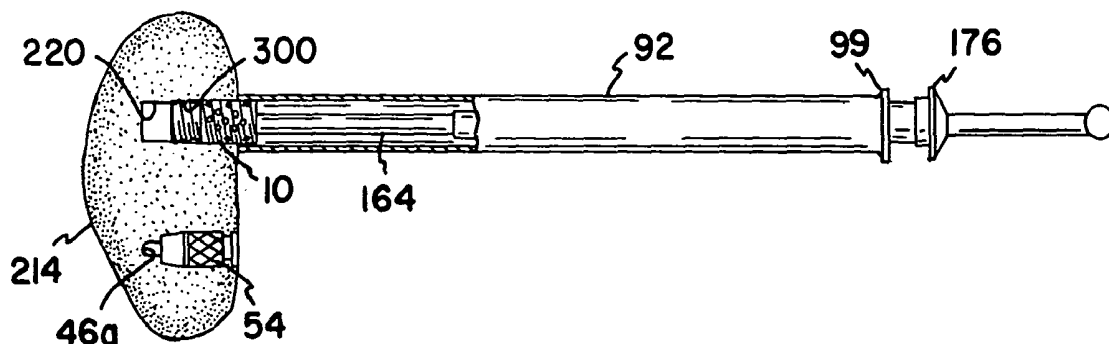
Primary Examiner—David H. Willse

(74) *Attorney, Agent, or Firm*—Wood, Herron & Evans,
 LLP

(57) **ABSTRACT**

Spinal fusion implants are laparoscopically placed in a disk
 space separating two vertebrae. Implant tools, including
 distraction spacers, boring tools and implants, are passed
 through a cannula toward the disk space.

13 Claims, 19 Drawing Sheets



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U.S. PATENT DOCUMENTS

5,026,373 A	6/1991	Ray et al.
5,484,437 A	1/1996	Michelson
5,489,307 A	2/1996	Kuslich et al.
5,505,732 A	4/1996	Michelson
5,609,636 A	3/1997	Kohrs et al.
5,776,196 A	7/1998	Matsuzaki et al.
5,797,909 A	8/1998	Michelson

FOREIGN PATENT DOCUMENTS

DE	3800482	7/1989
EP	0 077 159 A1	4/1983

EP	0260044	3/1988
EP	0 307 241 A2	3/1989
WO	WO 91/06261	5/1991
WO	WO 94/28824	12/1994

OTHER PUBLICATIONS

Declaration of George W. Bagby, M.D., 5 pages.

Posterior Lumbar Interbody Fusion by Paul Lin (© 1982), pp. 114-125.

Spine: State of the Art Review, vol. 6, No. 1, Jan. 1992, pp. 175-200.

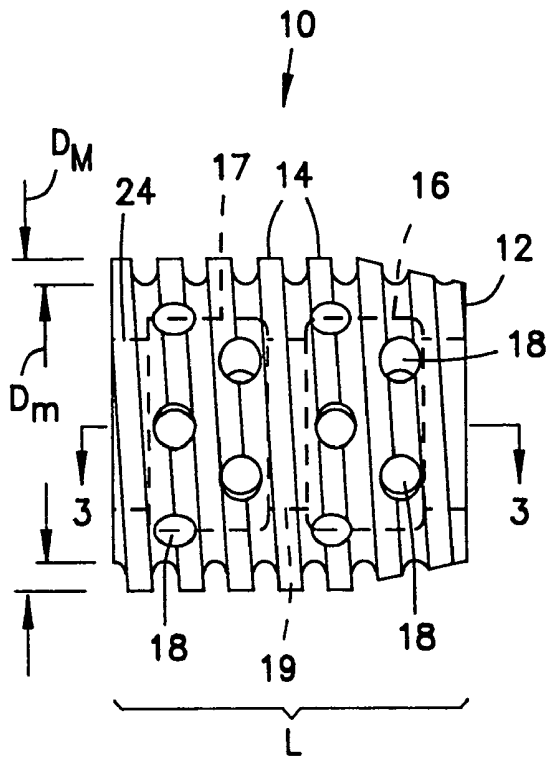


FIG. 1

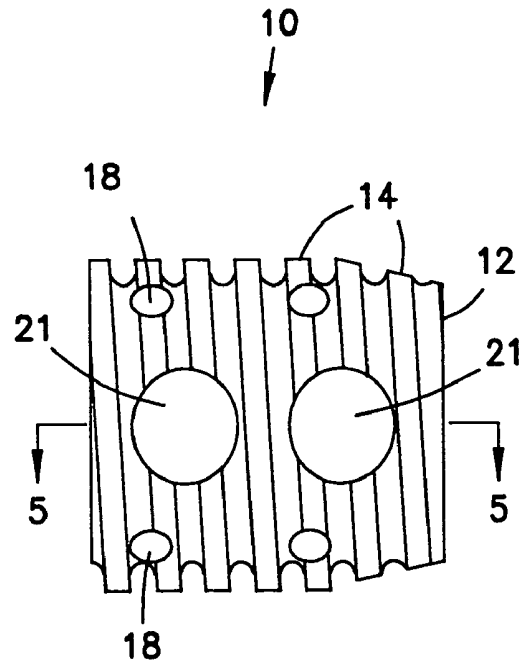


FIG. 2

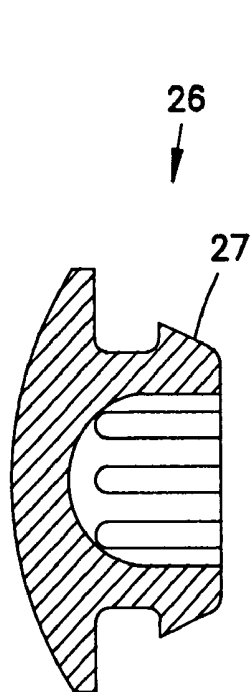


FIG. 7

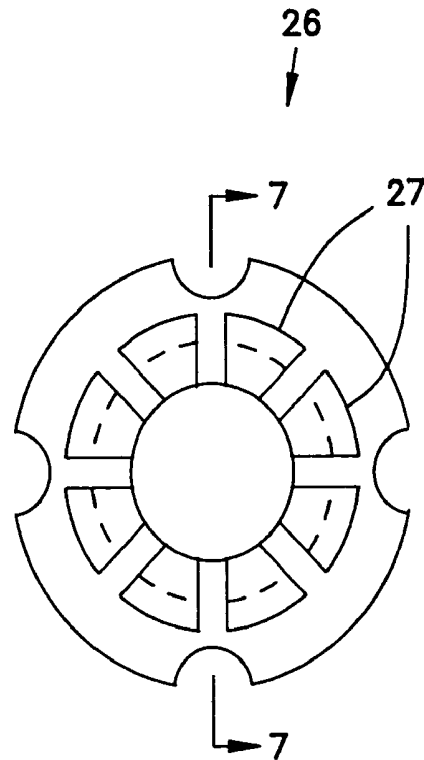


FIG. 8

FIG. 3

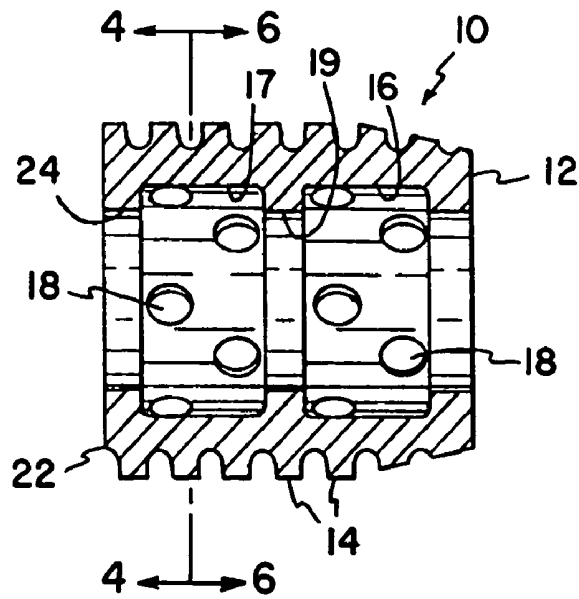


FIG. 4

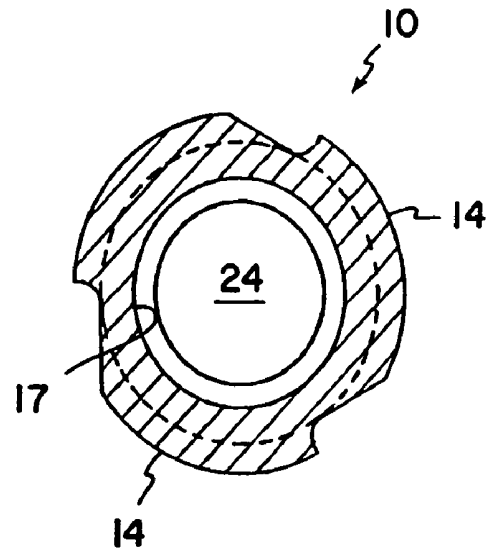


FIG. 5

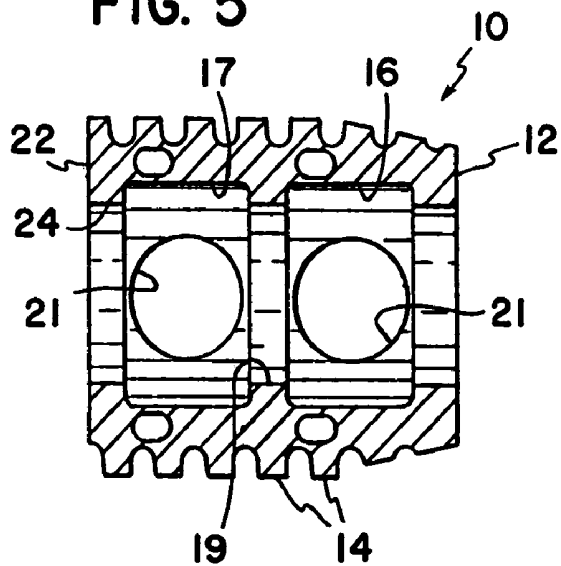
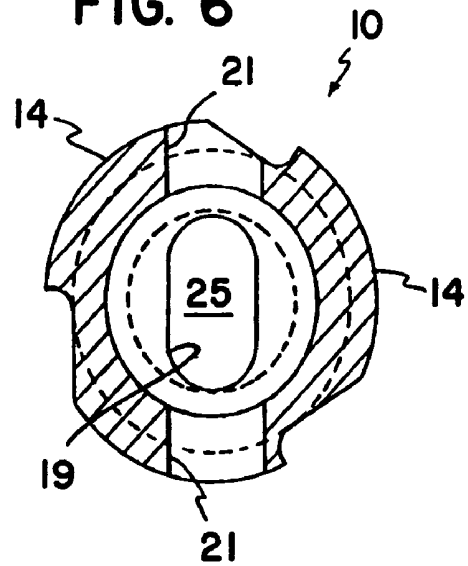


FIG. 6



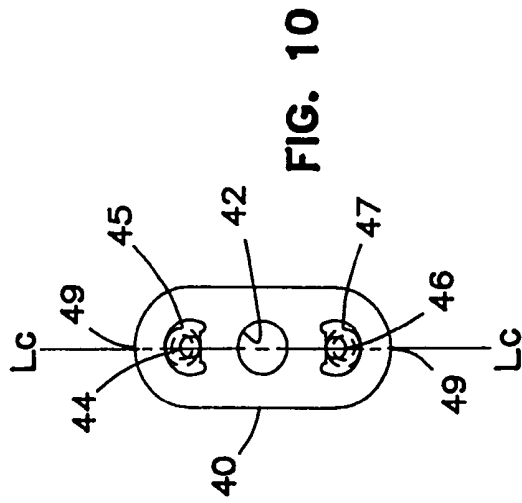


FIG. 9

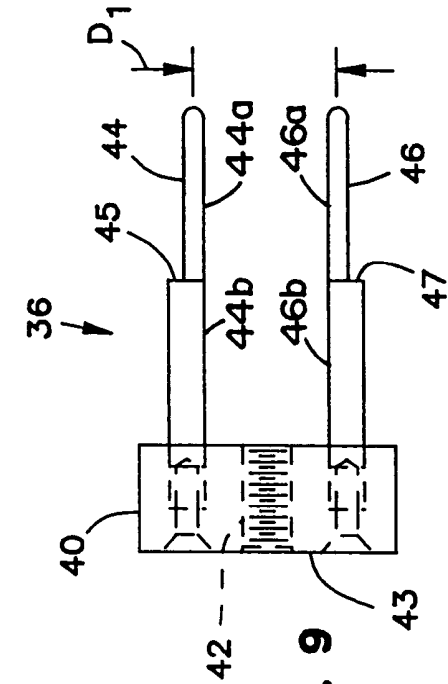


FIG. 10

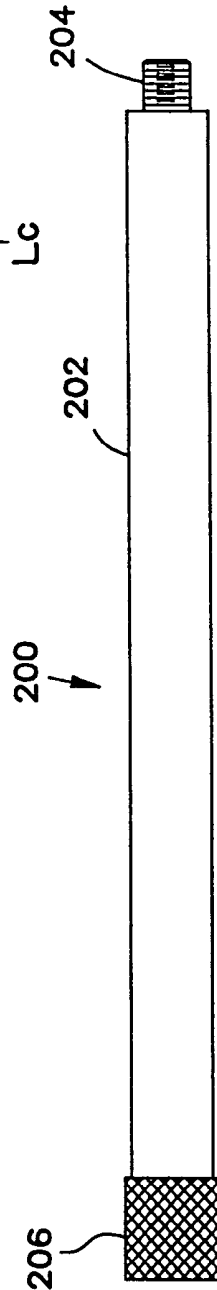


FIG. 11

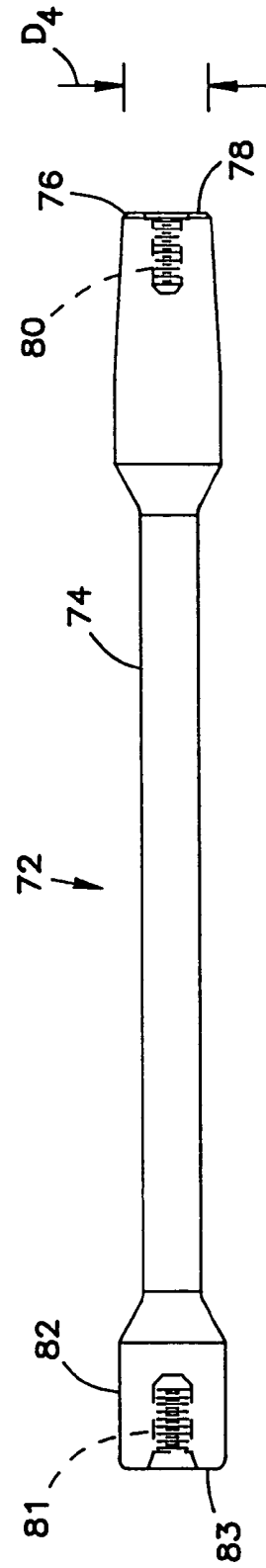


FIG. 12

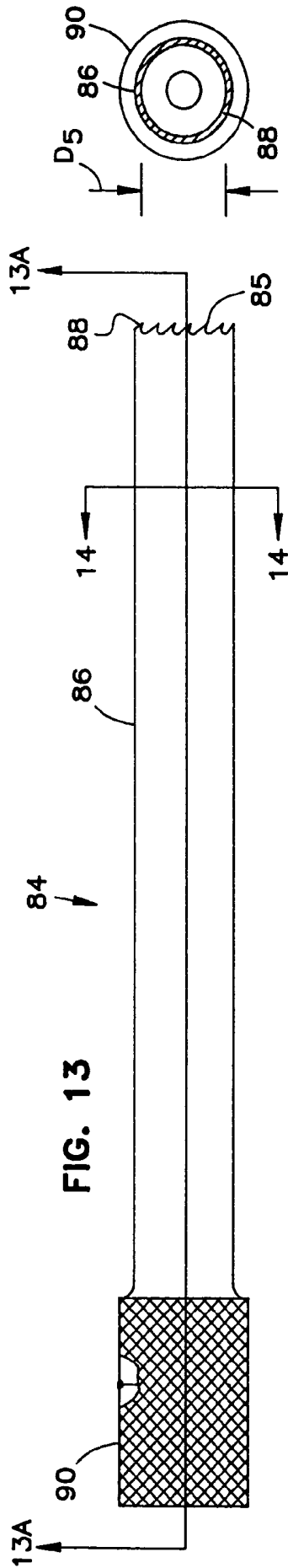


FIG. 14

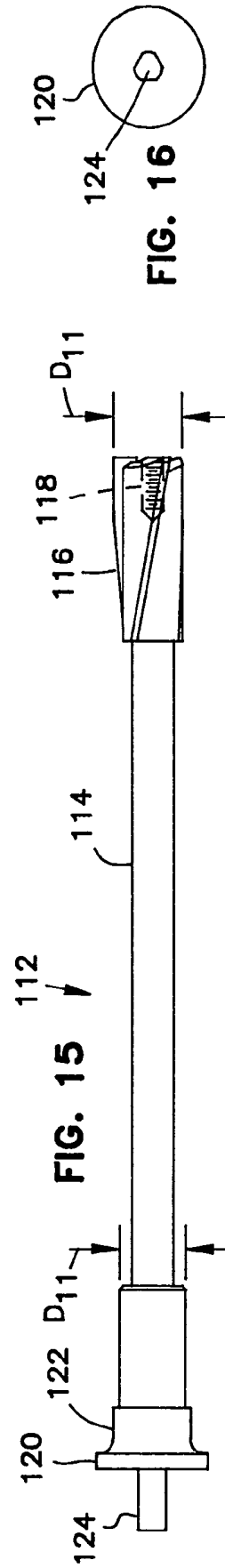
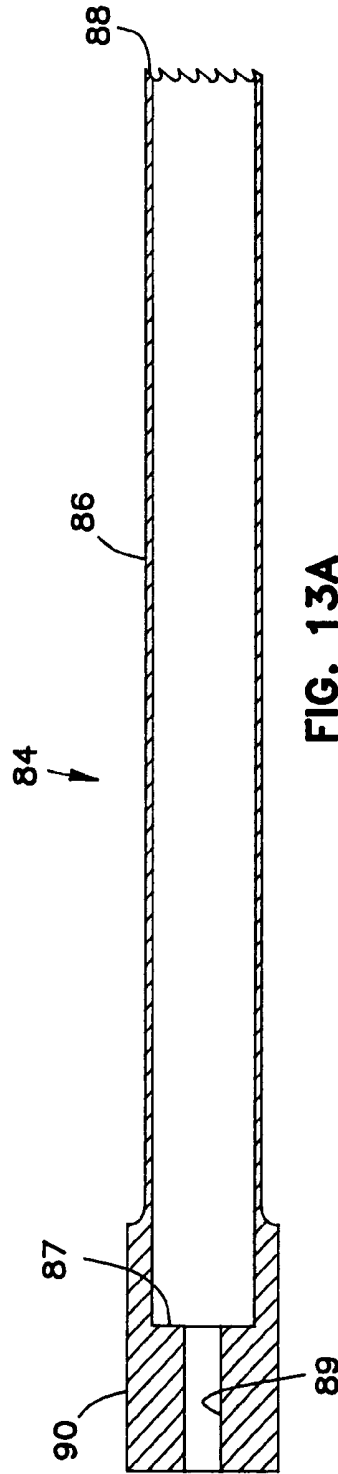
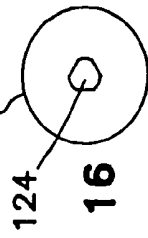


FIG. 16



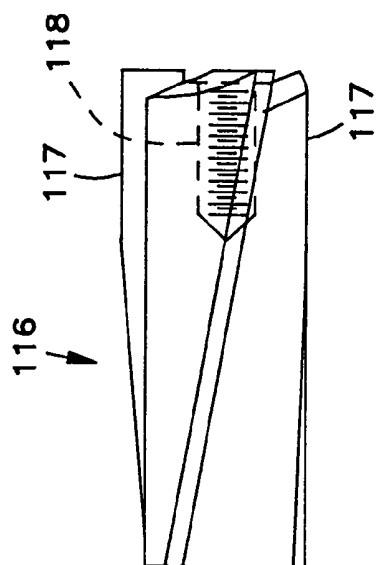


FIG. 17

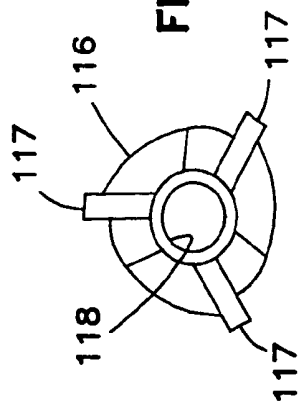


FIG. 18

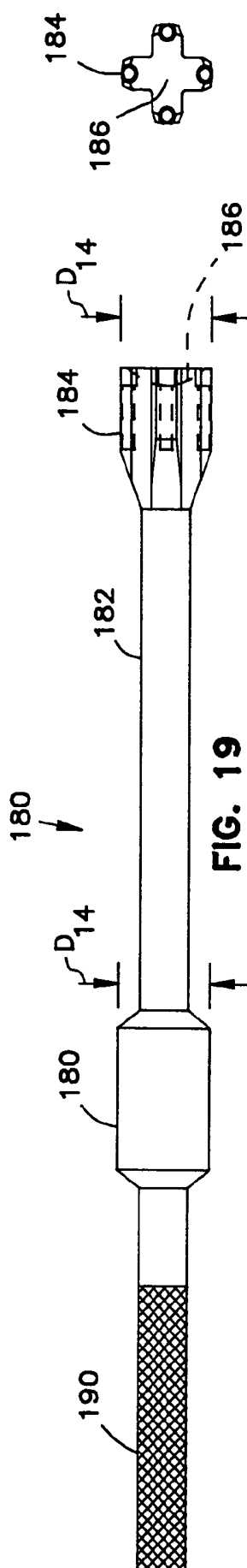


FIG. 19

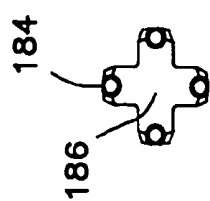


FIG. 20

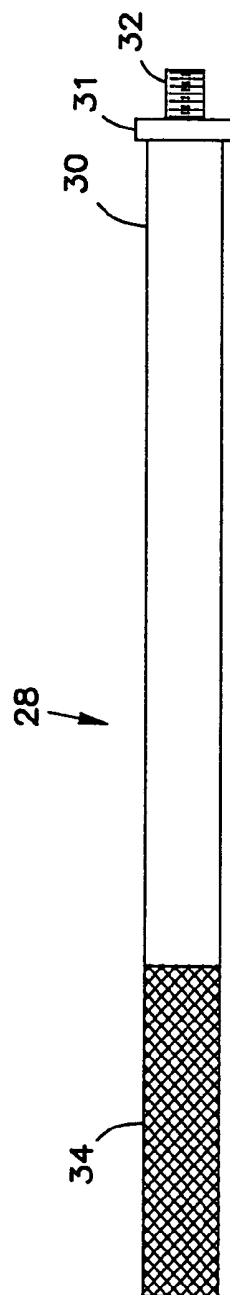


FIG. 21

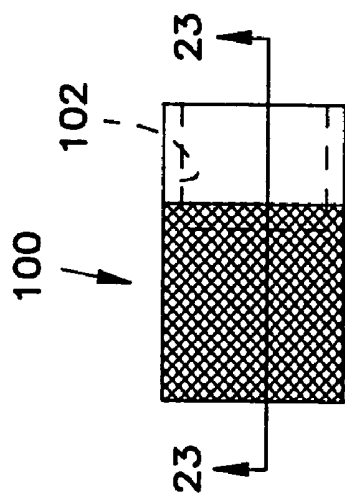


FIG. 22

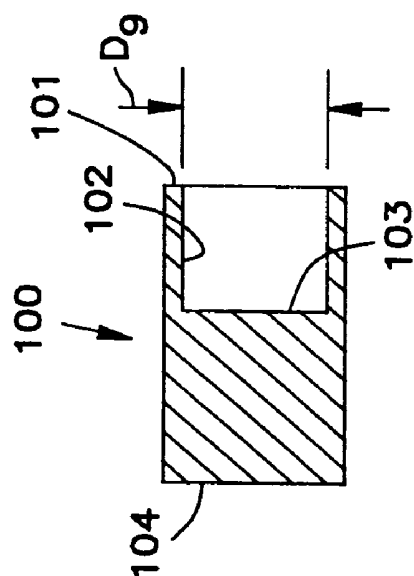


FIG. 23

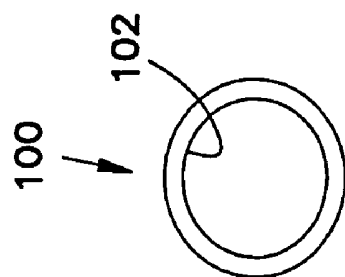


FIG. 24

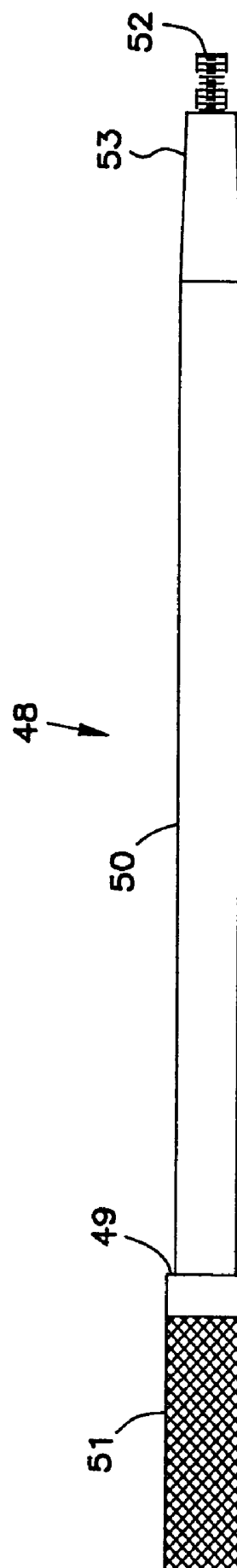


FIG. 25

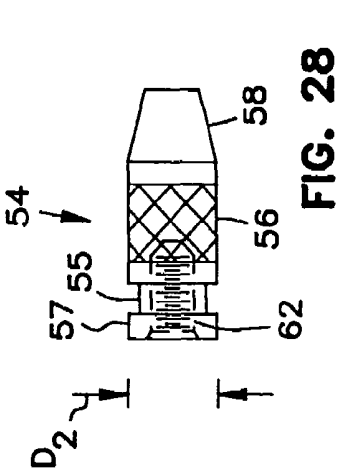


FIG. 26

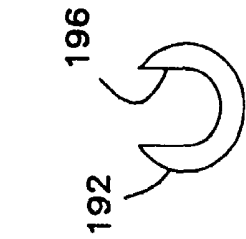


FIG. 27

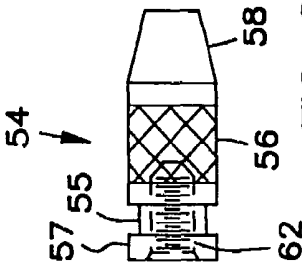


FIG. 28

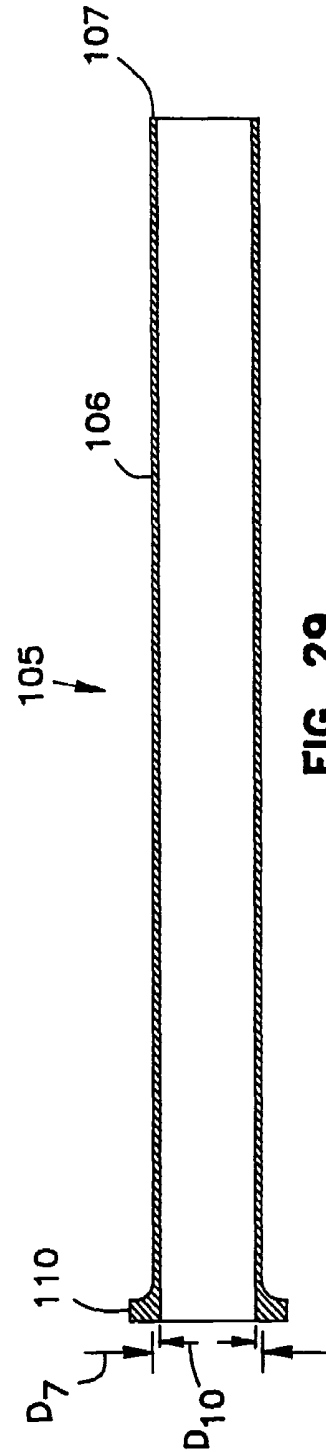


FIG. 29

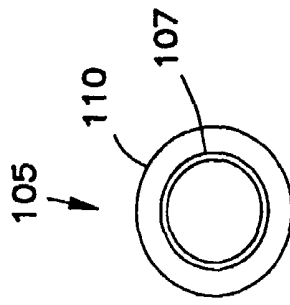


FIG. 30

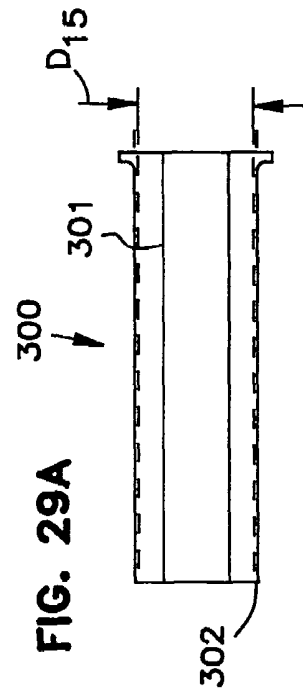


FIG. 29A

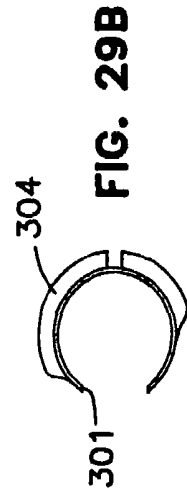
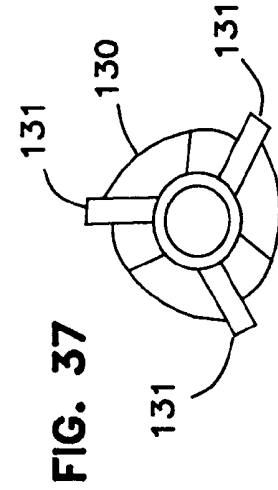
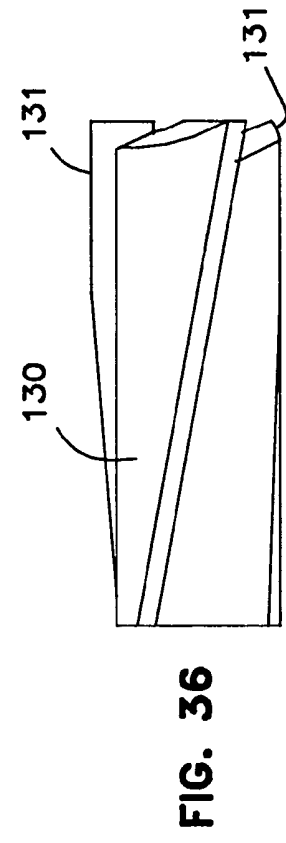
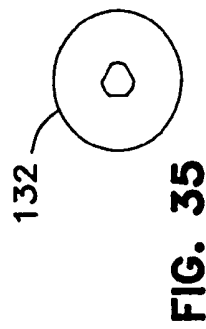
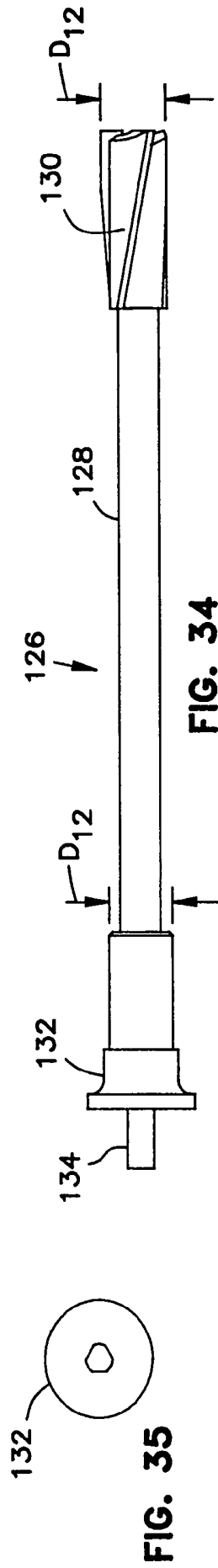
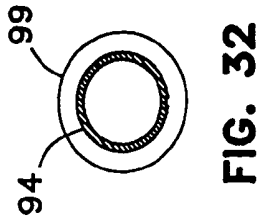
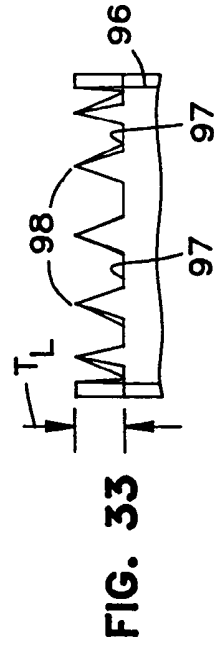
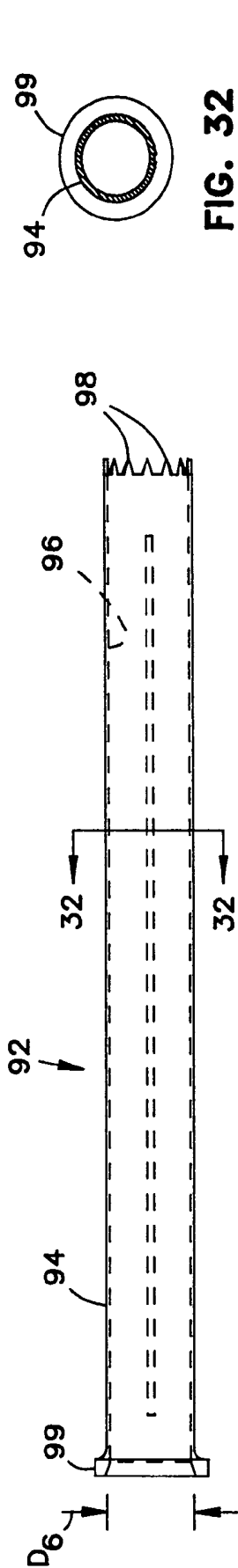
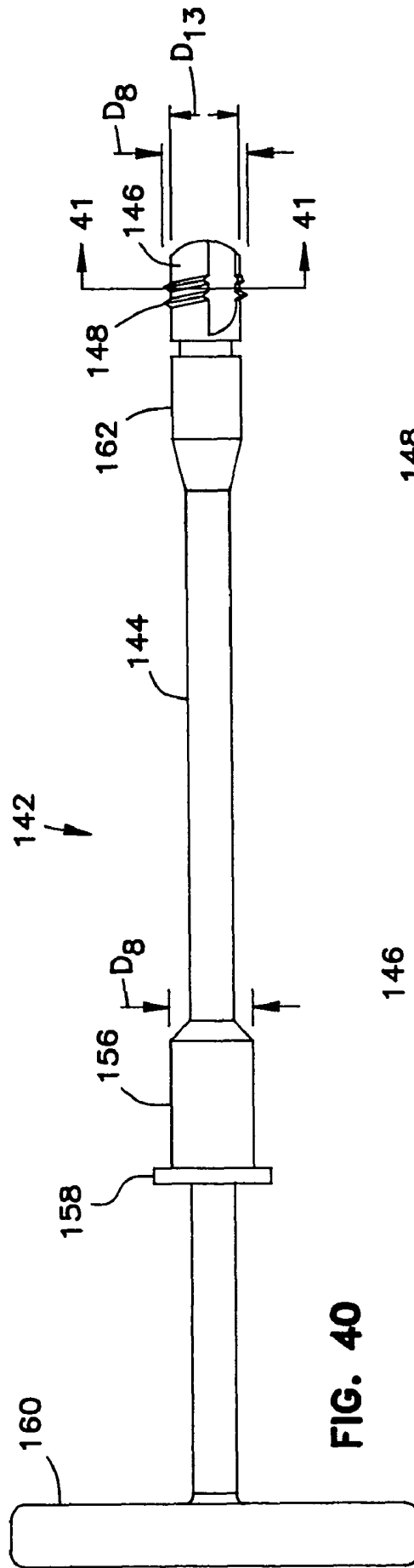
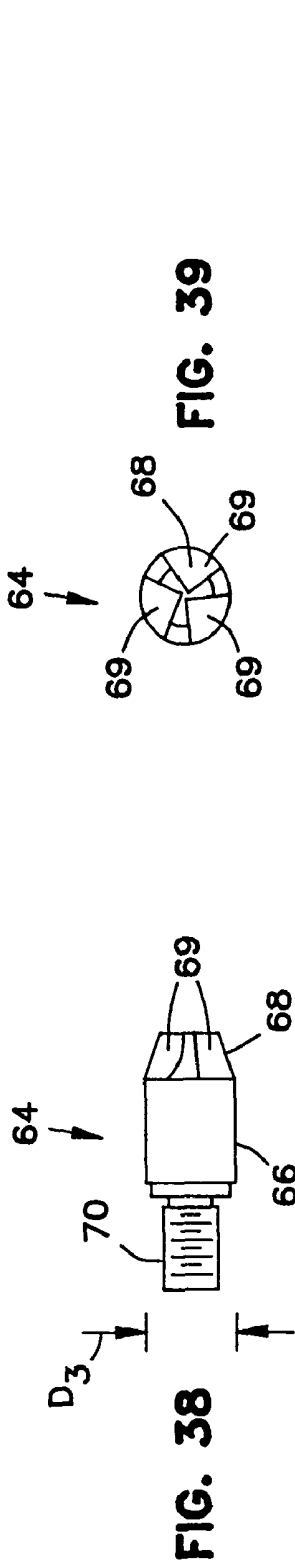
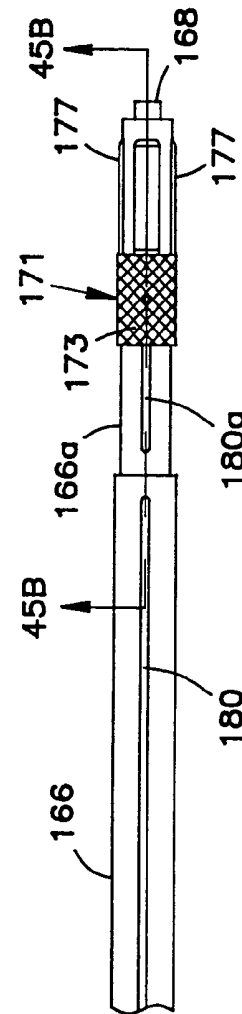
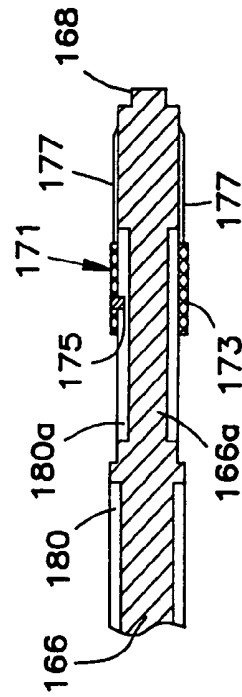
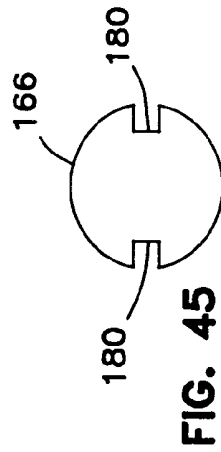
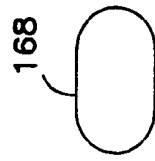
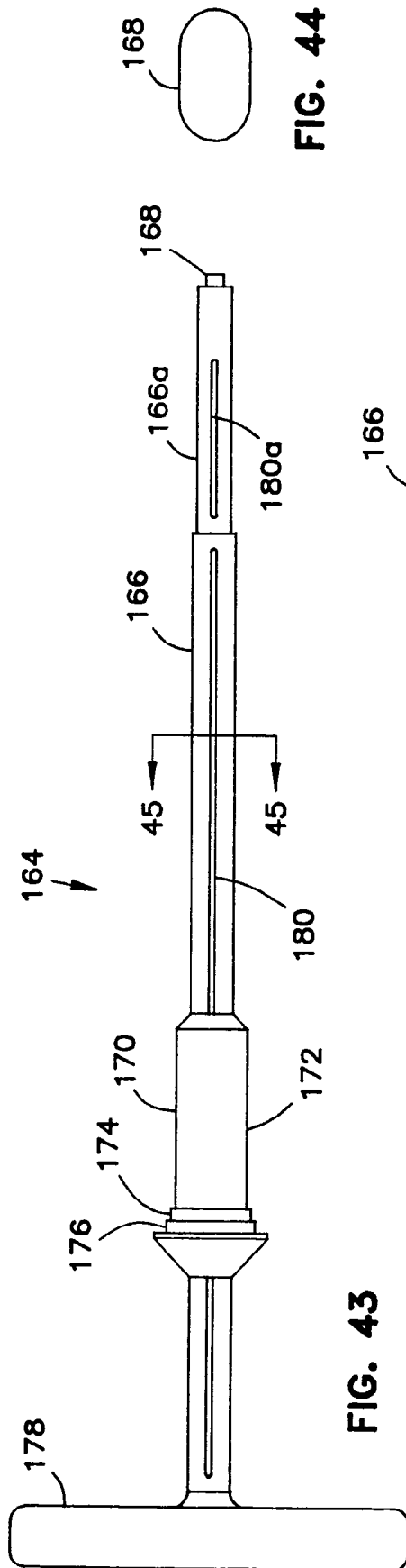


FIG. 29B







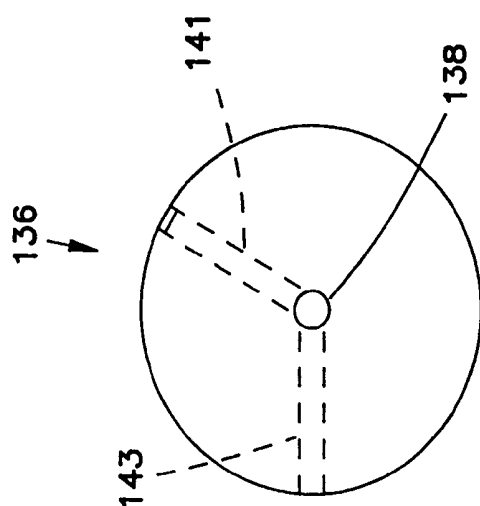


FIG. 47

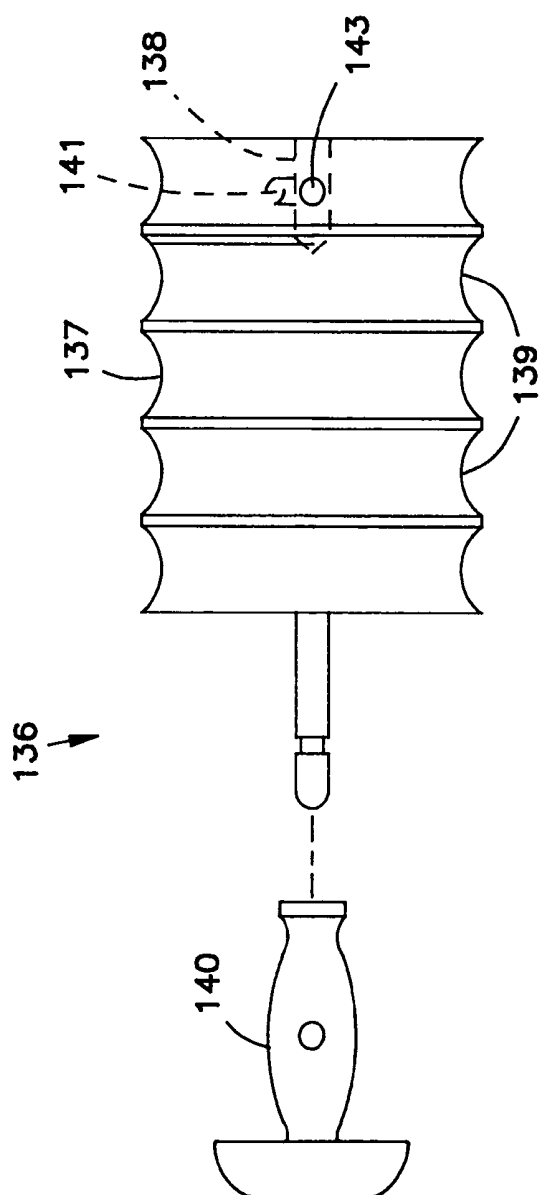


FIG. 46

FIG. 48

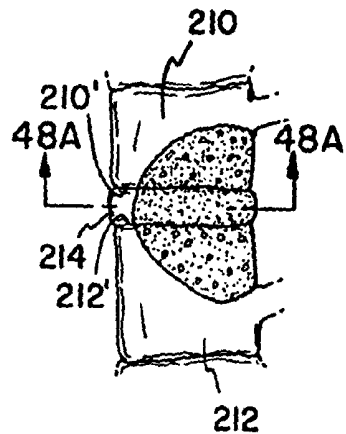


FIG. 48A

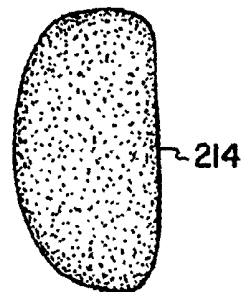


FIG. 49

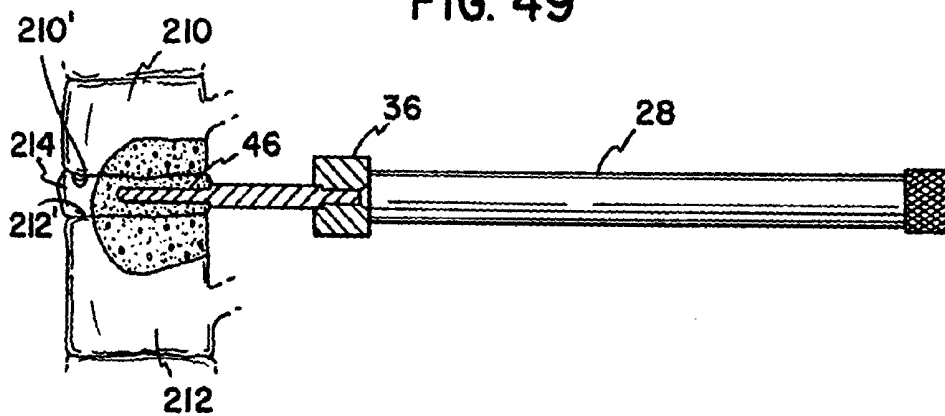


FIG. 49A

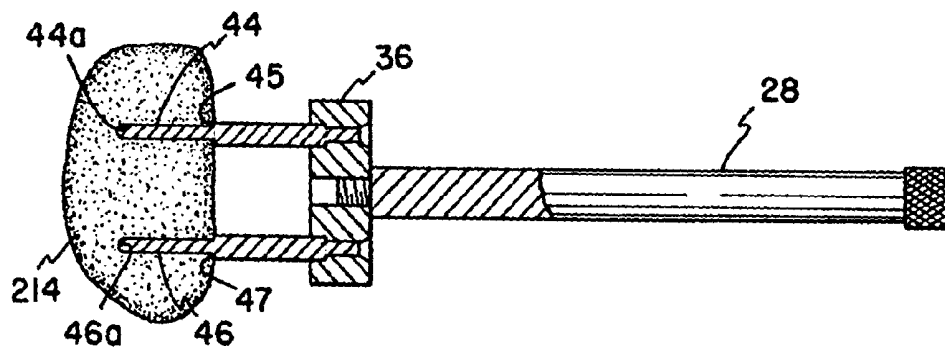
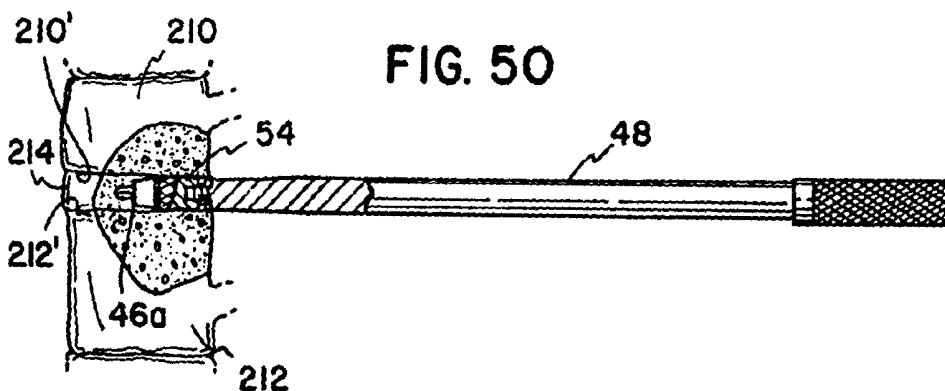
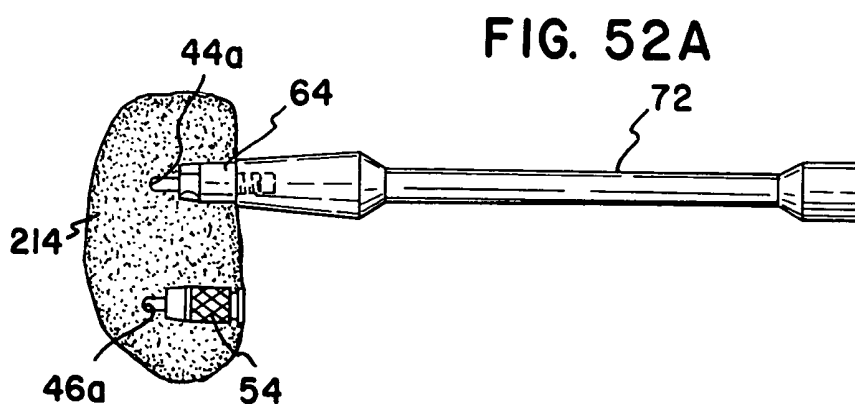
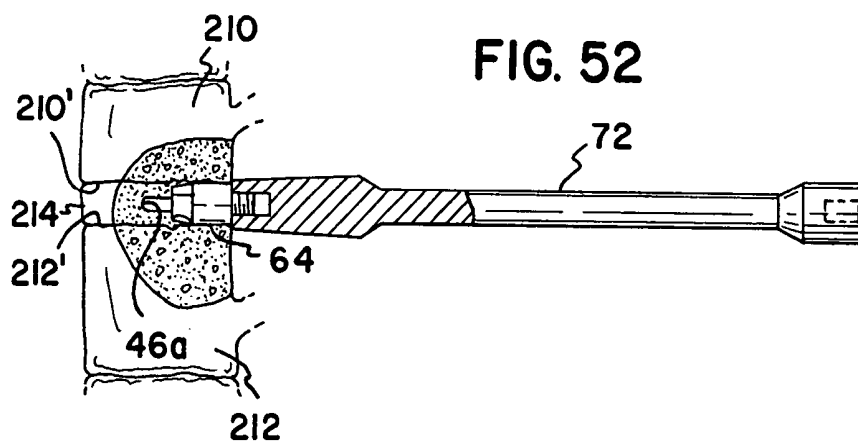
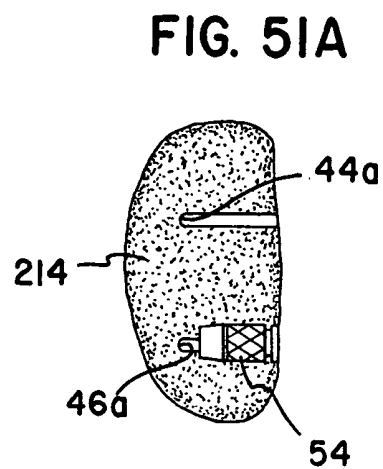
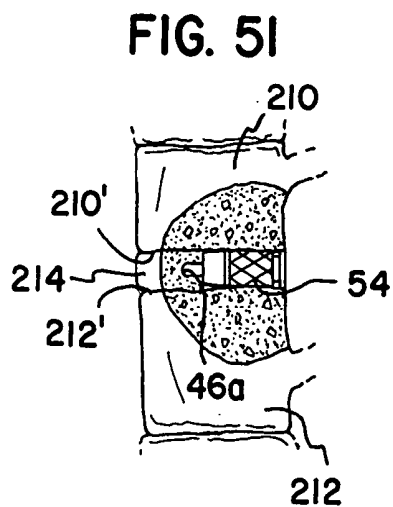
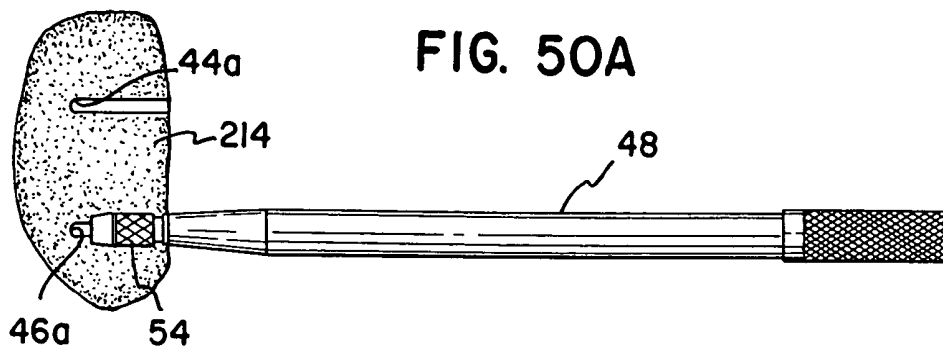


FIG. 50





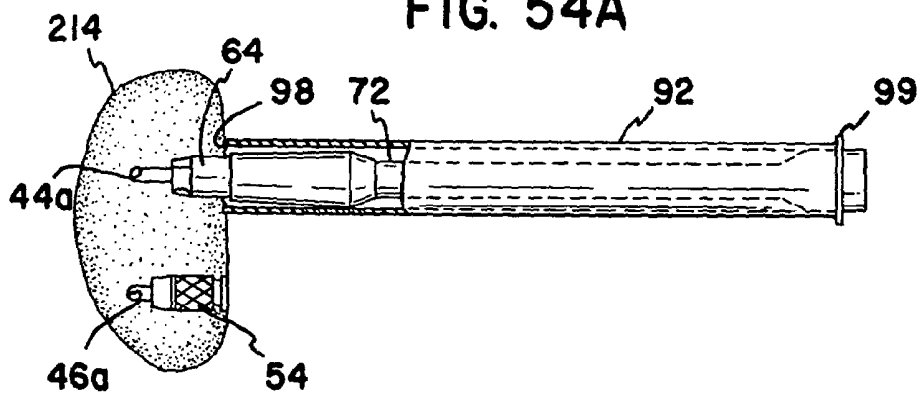


FIG. 55

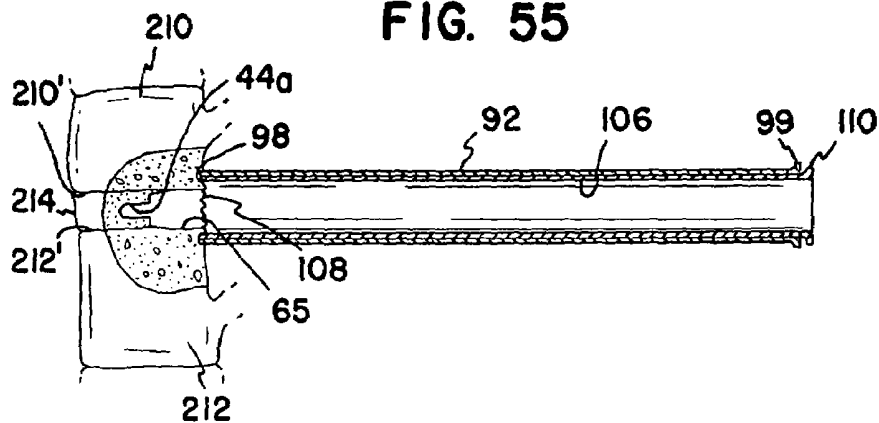


FIG. 55A

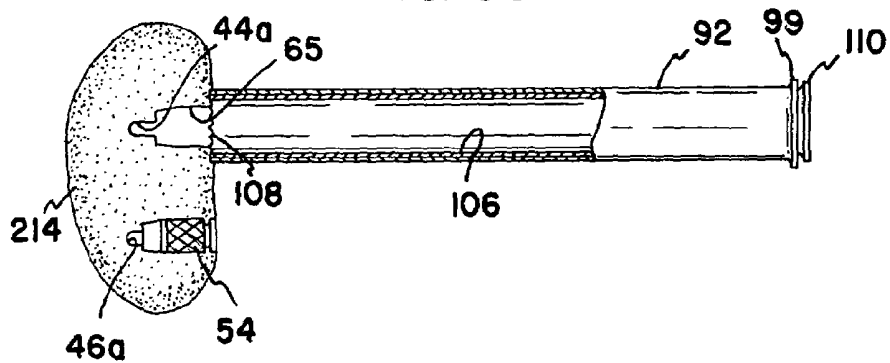


FIG. 56

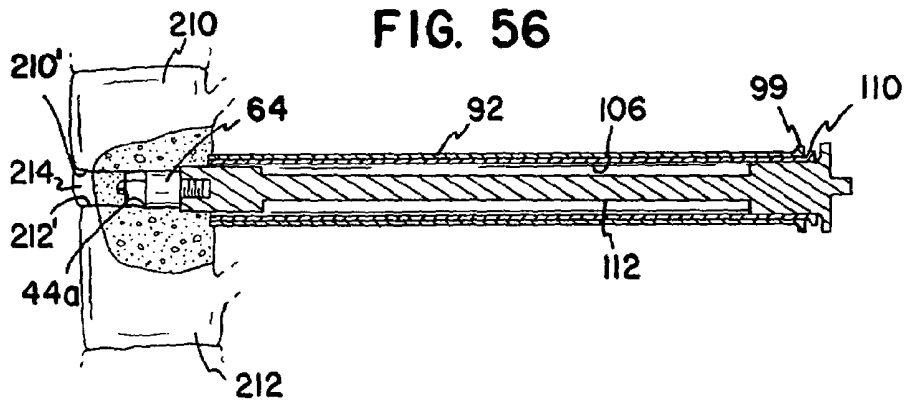


FIG. 56A

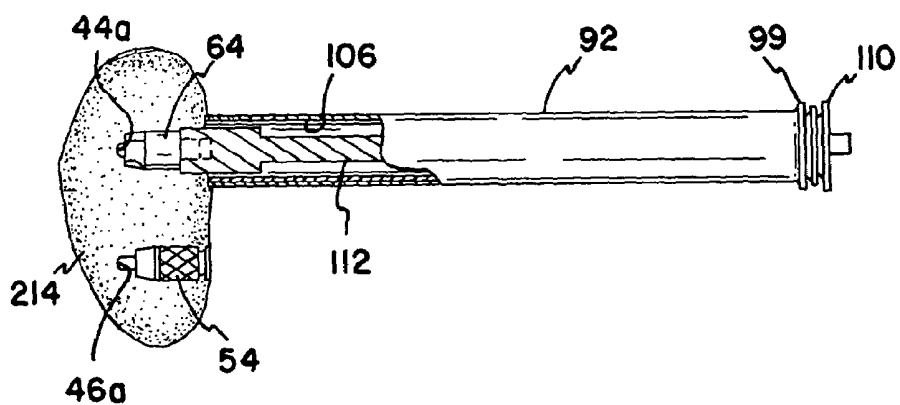


FIG. 57

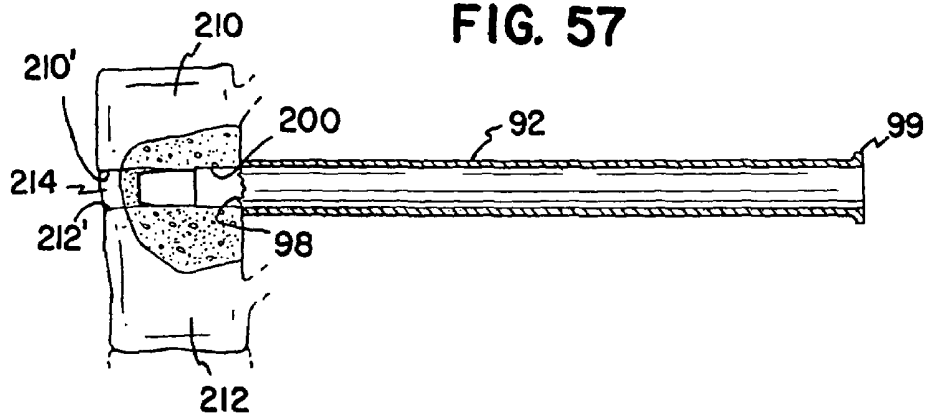


FIG. 57A

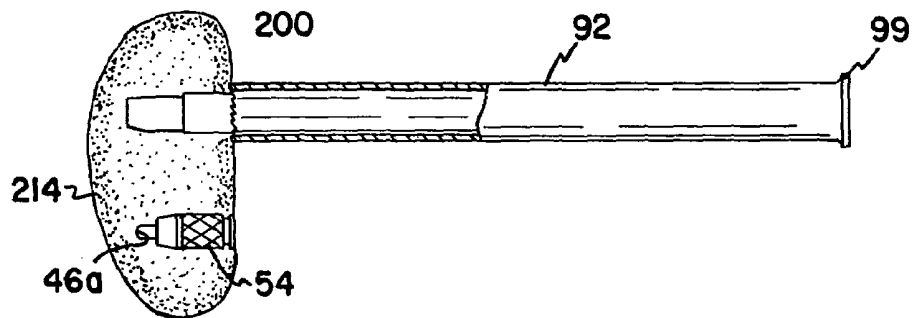


FIG. 58

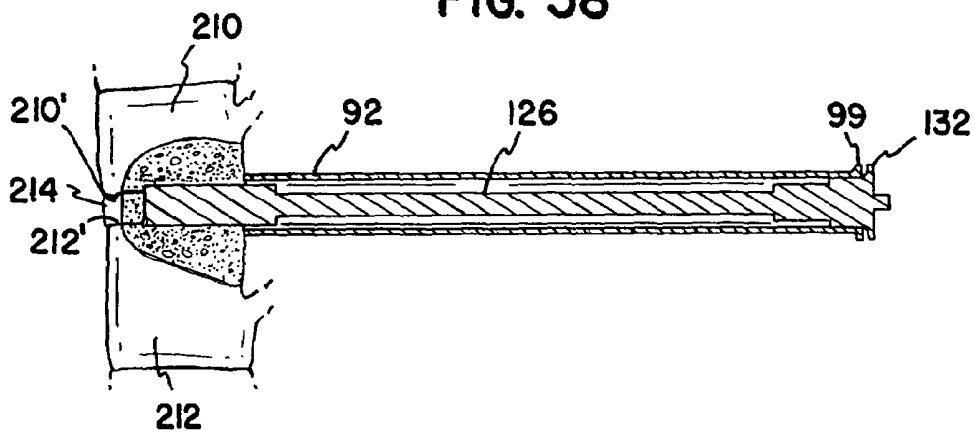
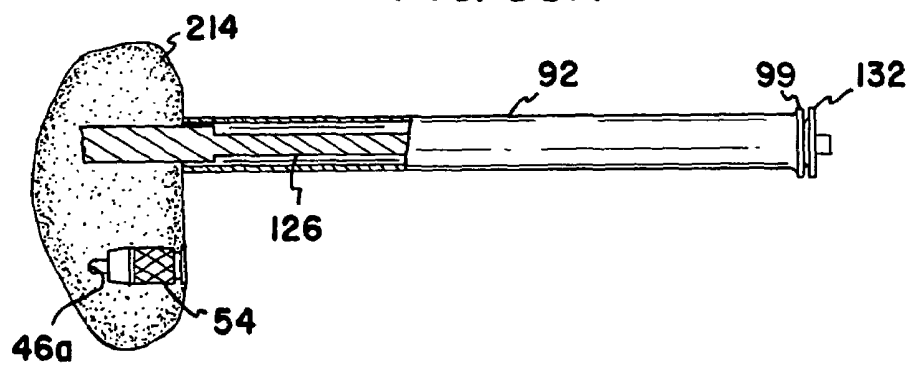


FIG. 58A



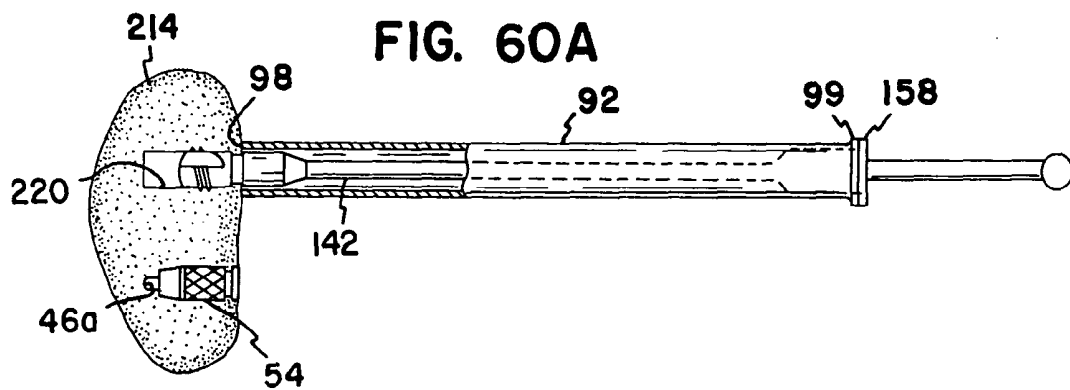
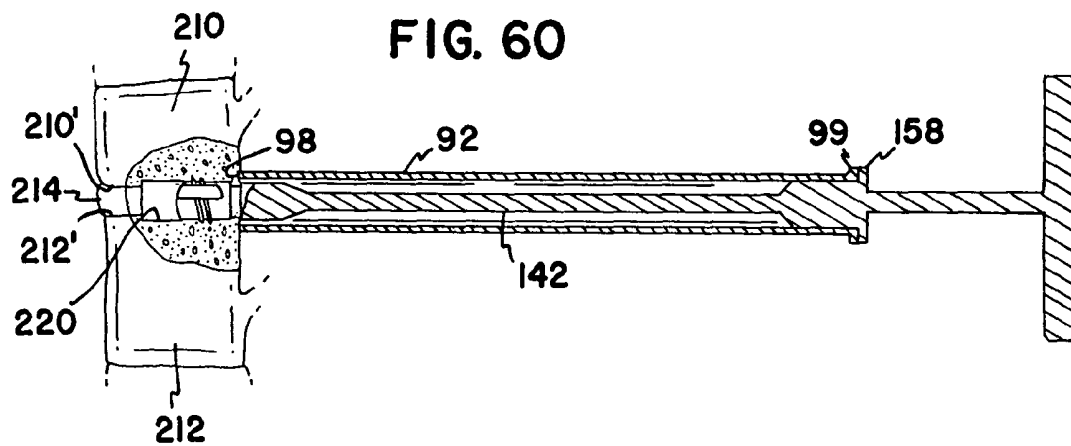
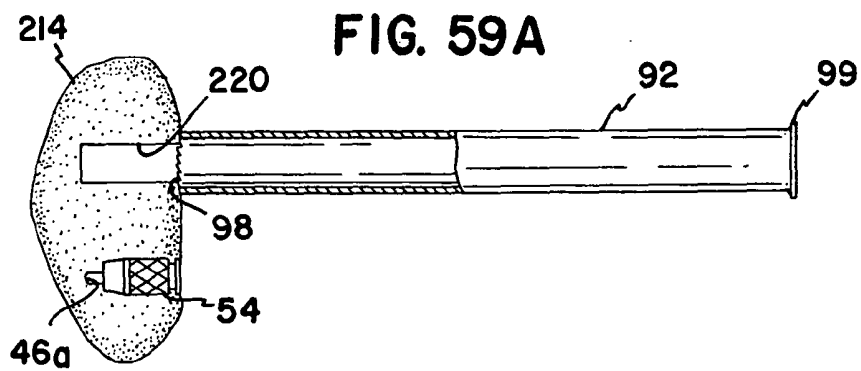
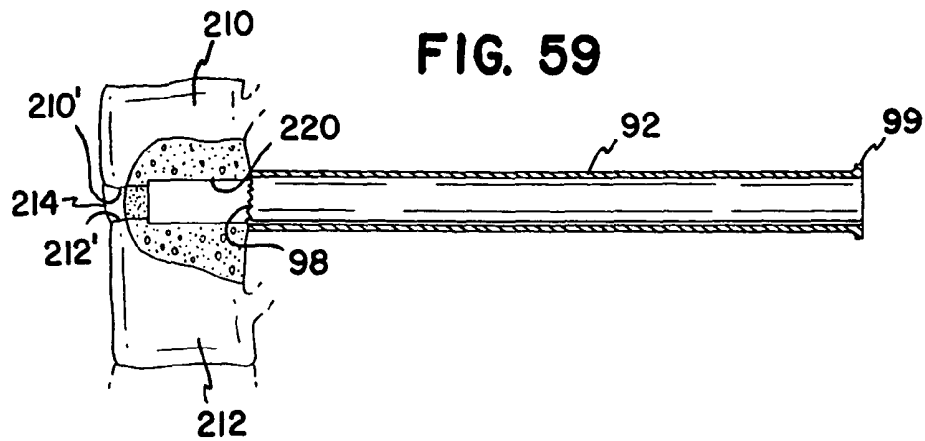


FIG. 61

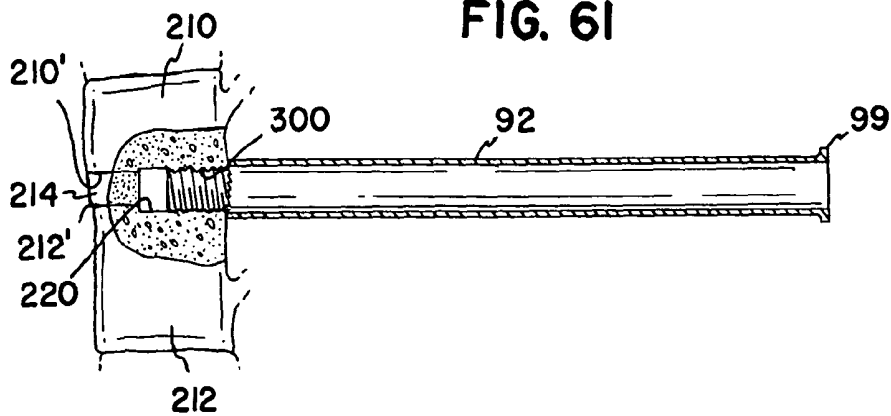


FIG. 61A

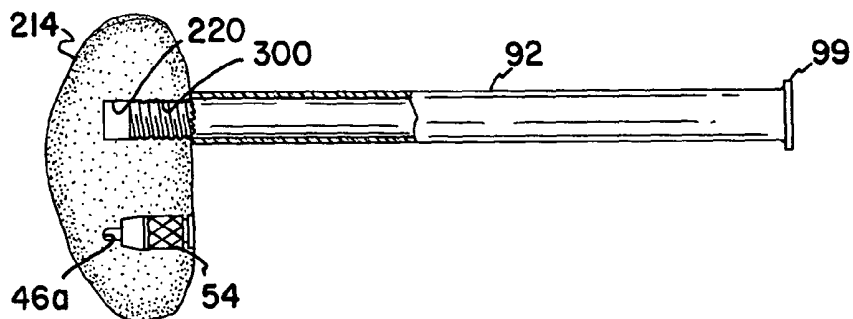


FIG. 62

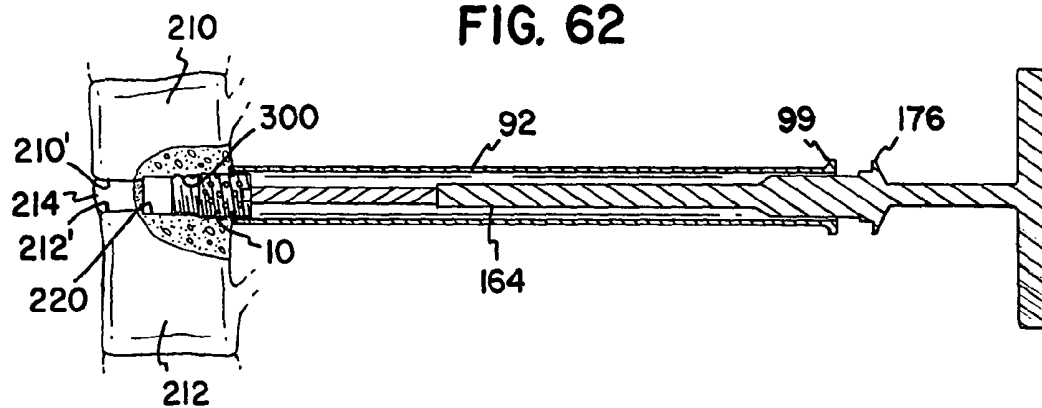
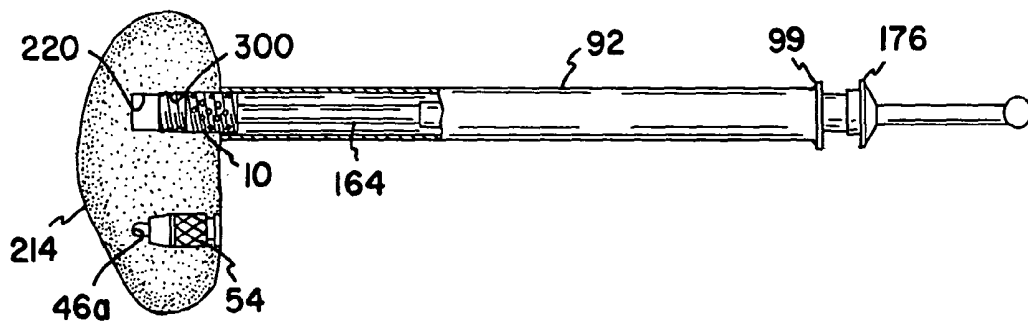
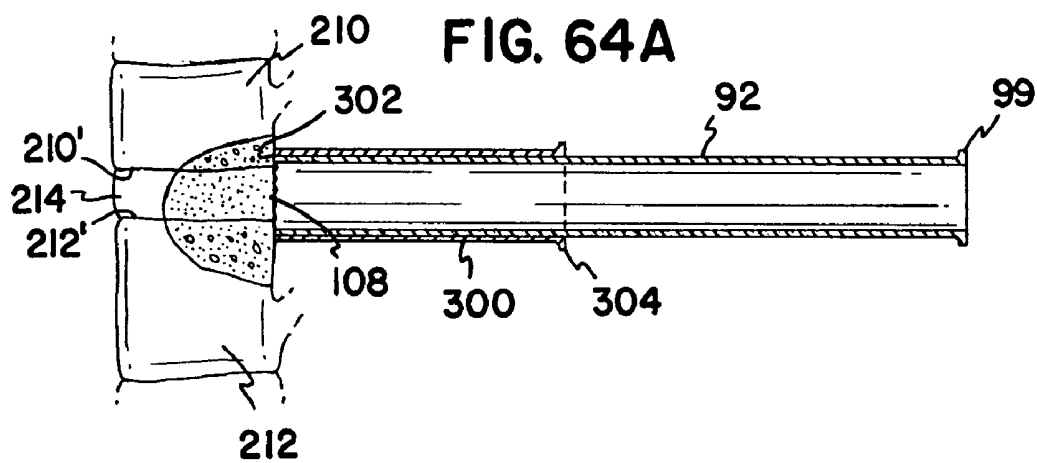
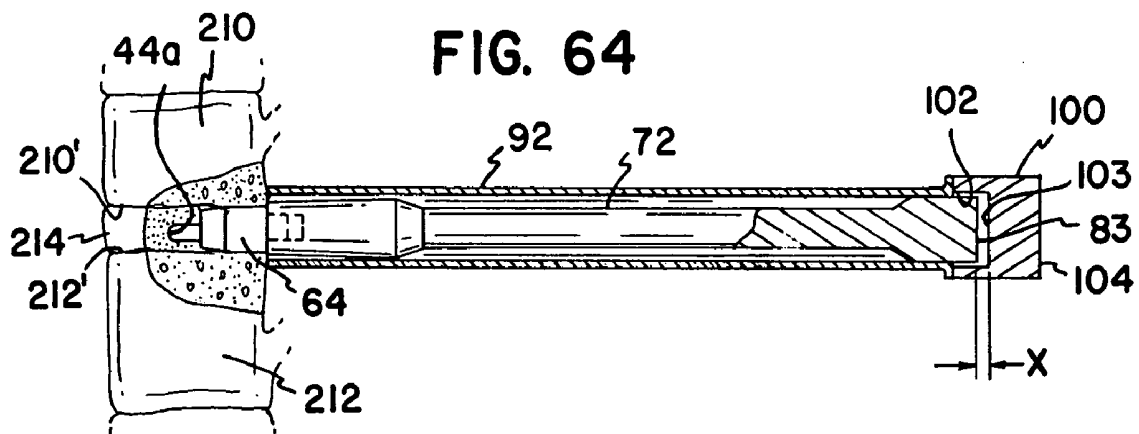
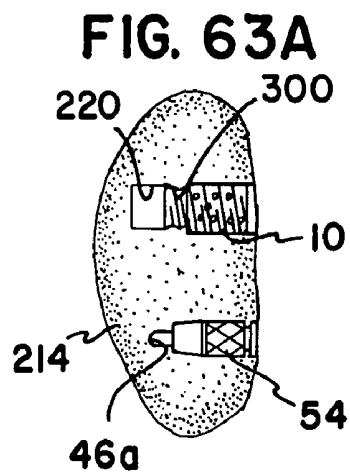
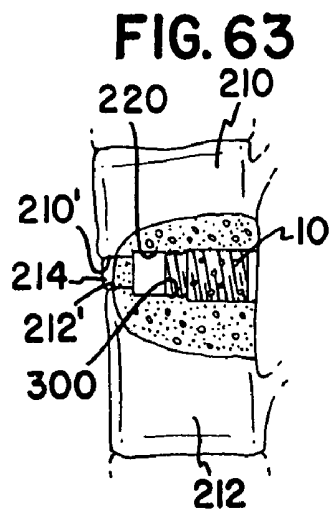


FIG. 62A





LAPAROSCOPIC SPINAL STABILIZATION SURGICAL METHOD

This application is a continuation of U.S. application Ser. No. 09/369,614, filed Aug. 6, 1999, now U.S. Pat. No. 6,599,320, which is a continuation of U.S. application Ser. No. 08/902,746, filed Jul. 29, 1997, now abandoned, which is a divisional of U.S. application Ser. No. 08/752,818, filed Nov. 21, 1996, now U.S. Pat. No. 5,947,971, which is a continuation of U.S. application Ser. No. 08/482,025, filed Jun. 7, 1995, now U.S. Pat. No. 5,720,748, which is a divisional of U.S. application Ser. No. 08/299,807, filed Sep. 1, 1994, now U.S. Pat. No. 5,489,307, which is a continuation of U.S. application Ser. No. 08/015,863, filed Feb. 10, 1993, now abandoned, which applications are incorporated herein by reference.

I. BACKGROUND OF THE INVENTION

1. Field of the Invention

This invention pertains to a spinal stabilization surgical procedure. More particularly, this invention pertains to a method for implanting a fusion spinal implant between two vertebrae.

2. Description of the Prior Art

Chronic back problems cause pain and disability for a large segment of the population. In many cases, the chronic back problems are attributed to relative movement between vertebrae in the spine.

Orthopaedic surgery includes procedures to stabilize vertebrae. Common stabilization techniques include fusing the vertebrae together.

Fusion techniques include removing disc material which separates the vertebrae and impacting bone into the disc area. The impacted bone fuses with the bone material of the vertebrae to thereby fuse the two vertebrae together.

As in any surgical technique, it is desirable in back surgery to provide a procedure which permits rapid post-operative recovery. To this end and to increase the probability of a successful fusion, spinal implants have been developed. An example of such a spinal implant is shown in commonly assigned and co-pending U.S. patent application Ser. No. 07/702,351 filed May 15, 1991 (claiming priority to Jul. 6, 1989). That patent application teaches a threaded spinal implant which includes a hollow cylinder into which bone chips or bone slurry may be placed. The cylinder has holes extending radially therethrough. The bone material grows through the holes to fuse with the bone material of the vertebrae.

A threaded spinal implant is also shown in U.S. Pat. No. 5,015,247, dated May 14, 1991. In addition to teaching a threaded spinal implant, U.S. Pat. No. 5,015,247 shows a method of implantation including certain tools to form a bore into which the implant is threaded.

A threaded fusion cage and a method of inserting such a cage is also shown in U.S. Pat. No. 4,961,740 to Ray et al. dated Oct. 9, 1990 as well as U.S. Pat. No. 5,026,373 to Ray et al. dated Jun. 25, 1991. The latter patent teaches preparing a bore for the implant by drilling over a pilot rod. In addition to the above, spinal implants are shown in U.S. Pat. No. 4,875,915 to Brantigan dated Nov. 7, 1989, German Patent 3505567A1 dated Jun. 5, 1986 to Vich, U.S. Pat. No. 4,834,757 to Brantigan dated May 30, 1989 and U.S. Pat. No. 4,507,269 to Bagby dated Feb. 27, 1985. The latter is not a threaded implant but uses a cage or basket which is impacted into a bore formed between bone to be fused.

When performing back surgery (such as placing implants in a spine) it is desirable that the surgical procedure be performed as quickly and as accurately as possible. Accordingly it is an object of the present invention to provide a surgical procedure for placing an implant in a spine in a procedure which can be done quickly and accurately.

In addition to the foregoing, it is known to be desirable to place two implants between opposing vertebrae (although a single implant procedure may be advisable in some circumstances). In a two implant procedure, bores are formed on opposite sides of the vertebrae to receive each of the implants. I have found that in such a procedure, the forming of the bores can cause misalignment of the vertebrae which is undesirable. Also, prior art techniques (e.g., drilling over a guide rod) can result in a bore which does not cut equally into both vertebrae. Accordingly, it is a further object of the present invention to provide a surgical implant procedure which assures accurate alignment of the vertebrae throughout the procedure.

Furthermore, it is an object of the present invention to provide a surgical procedure that can be performed posteriorly, anteriorly or as a laparoscopic procedure.

II. SUMMARY OF THE INVENTION

A surgical method for implanting at least two spinal fusion implants into a disc space of a disc material which separates two vertebrae is disclosed. The surgical method includes the steps of distracting one side of the disc space with a spacer and forming an implant receiving bore in an opposite of the disc space. After implanting the implant into the opposite side, the spacer is removed and a bore receiving implant is formed to receive a second implant.

III. BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a side elevation view of an implant for use with the method of the present invention;

FIG. 2 is the view of the implant of FIG. 1 with the implant rotated 90° about its axis;

FIG. 3 is a view taken along line 3—3 of FIG. 1;

FIG. 4 is a view taken along lines 4—4 of FIG. 3;

FIG. 5 is a view taken along lines 5—5 of FIG. 2;

FIG. 6 is a view taken along lines 6—6 of FIG. 3;

FIG. 7 is a cross-sectional side view of an end cap for use with the implant of FIG. 1;

FIG. 8 is a plan view of the implant of FIG. 7;

FIG. 9 is a top plan view of an alignment guide assembly;

FIG. 10 is an end plan view of the guide assembly of FIG. 9;

FIG. 11 is a side elevation view of a drill tube guide removal handle;

FIG. 12 is a side elevation view of a drill tube guide;

FIG. 13 is a side elevation view of a drill tube planar according to the present invention;

FIG. 13A is a cross-sectional side view of the planar of FIG. 13;

FIG. 14 is a view taken along line 14—14 of FIG. 13;

FIG. 15 is a side elevation view of a starter vertebral reamer according to the present invention;

FIG. 16 is a proximal end view of the reamer of FIG. 15;

FIG. 17 is an enlarged side elevation view of a reamer head of the starter reamer of FIG. 15;

FIG. 18 is a distal end elevation view of the reamer head of FIG. 17;

FIG. 19 is a side elevation view of an end cap inserter according to the present invention;

FIG. 20 is a distal end view of the inserter of FIG. 19;
FIG. 21 is a side elevation view of a starter alignment guide handle;

FIG. 22 is a side elevation view of a drill tube inserter cap;
FIG. 23 is a view taken along lines 23—23 of FIG. 22;
FIG. 24 is a distal end view of the inserter cap of FIG. 22;
FIG. 25 is a side elevation view of a distraction plug inserter;

FIG. 26 is a side elevation view of a slap hammer;
FIG. 27 is a distal end elevation view of the slap hammer of FIG. 26;

FIG. 28 is a side elevation view of a distraction plug for use with the present invention;

FIG. 29 is a side sectional view of a drill tube sleeve according to the present invention;

FIG. 29A is a side elevation view of a sheath for use with the present invention;

FIG. 29B is a distal end elevation view of the sheath of FIG. 29A;

FIG. 30 is a distal end elevation view of the drill tube sleeve of FIG. 29;

FIG. 31 is a side elevation view of a drill tube for use with the present invention;

FIG. 32 is a view taken along line 32—32 of FIG. 31;

FIG. 33 is an enlarged side elevation view of a distal end of the drill tube of FIG. 31;

FIG. 34 is a side elevation view of a final vertebral reamer;

FIG. 35 is an elevation view of a proximal end of the final reamer of FIG. 34;

FIG. 36 is an enlarged view of a reamer head of the reamer of FIG. 34;

FIG. 37 is an end elevation view of a distal end of the reamer head of FIG. 36;

FIG. 38 is a side elevation view of a vertebral reamer guide pin;

FIG. 39 is a plan end view of the guide pin of FIG. 38;

FIG. 40 is a side elevation view of a starter tap;

FIG. 41 is a view taken along line 41—41 of FIG. 40;

FIG. 42 is an enlarged sectional view of thread cutting teeth of the tool of FIG. 40;

FIG. 43 is a side elevation view of an implant driver for use with the present invention;

FIG. 44 is an end view of a hub on a distal end of the tool of FIG. 43;

FIG. 45 is a view taken along line 45—45 of FIG. 43;

FIG. 45A is a side elevation view of a shaft of the tool of FIG. 43 showing an attached collet;

FIG. 45B is a cross sectional view of FIG. 45A taken along lines 45B—45B;

FIG. 46 is a side elevation exploded view of a vertebral reamer hand driver;

FIG. 47 is an end elevation view of the tool of FIG. 46;

FIG. 48 is a side elevation view of two vertebrae separated by a disk;

FIG. 48A is a view taken along lines 48A—48A of FIG. 48;

FIGS. 49 and 49A are views similar to FIGS. 48, 48A showing insertion of a starter alignment guide assembly;

FIGS. 50 and 50A are views similar to FIGS. 48 and 48A showing placement of a distraction plug by use of an inserter;

FIGS. 51 and 51A are views showing the distraction plug in place;

FIGS. 52, 52A are views similar to the preceding views showing placement of a vertebral reamer guide pin;

FIGS. 53, 53A are views similar to the foregoing views showing placement and use of a drill tube planar;

FIGS. 54, 54A are views similar to the foregoing views showing placement of a drill tube;

FIGS. 55, 55A are views similar to the foregoing showing placement of a drill tube sleeve;

FIGS. 56, 56A are views similar to the foregoing showing preboring of an implant bore;

FIGS. 57, 57A are views similar to the foregoing views showing a partially formed bore following the preboring of FIGS. 56, 56A;

FIGS. 58, 58A are views similar to the foregoing views showing final boring of an implant bore;

FIGS. 59, 59A are views similar to the foregoing showing formation of a completed bore after removal of the final boring tool of FIGS. 58, 58A;

FIGS. 60, 60A are views similar to the foregoing showing tapping of the bore formed in FIGS. 59, 59A;

FIGS. 61, 61A are views similar to the foregoing showing the tapped bore;

FIGS. 62, 62A are views similar to the foregoing showing placement of an implant within a threaded bore;

FIGS. 63, 63A are views showing completed placement of an implant within the bore;

FIG. 64 is a view showing placement of a drill tube using an end cap inserter; and

FIG. 64A is a view showing use of a sheath on a drill tube.

IV. DESCRIPTION OF THE PREFERRED EMBODIMENT

1. Generally

Referring now to the several drawing figures in which identical elements are numbered identically throughout, a description of the preferred embodiment will now be provided. For purposes of illustrating a preferred embodiment, a description of the surgical procedure will be given with respect to an implant 10 such as that shown and described in commonly assigned and co-pending U.S. patent application Ser. No. 07/702,351. It will be appreciated that the present surgical procedure can apply to a wide variety of implants including threaded implants such as those shown in the aforementioned U.S. Pat. Nos. 5,015,247 and 4,961,740 as well as non-threaded implants such as shown in U.S. Pat. No. 4,507,269 or other implants. The term "implant" as used herein may also include bone implants (e.g., autograft, allograft or artificial bone).

The implant 10 (FIGS. 1–6) is a hollow cylinder 12 having male threads 14 exposed on the exterior cylindrical surface of cylinder 12. The cylinder includes a forward interior chamber 16 and a rear interior chamber 17 separated by a reinforcing rib 19, a bone slurry or bone chips may be compacted into chambers 16, 17 as will be described.

A first plurality of holes 18 extend radially through the cylinder wall and communicate with the chambers 16, 17. A second (and enlarged) plurality of holes 21 are disposed on diametrically opposed sides of the implant 10.

A rear end 22 of the implant has a slot 24 which communicates with the chamber 17. The slot 24 allows the bone slurry or bone chips to be impacted into the implant 10. A slot 25 is defined by rib 19. The slot 25 is sized to receive the distal end of a tool (as will be more fully described) to place the implant within a bore formed between opposing vertebrae.

An endcap 26 (FIGS. 7, 8) is provided to snap fit onto the rear end 12 by means of snap tabs 27. In a preferred

embodiment, the endcap **26** is polyethylene or some other radiolucent material to permit post-operative x-ray inspection and determine the adequacy of the fusion after the implant surgery has been performed.

2. Tools

A. Generally

In a preferred embodiment the technique of the present invention will be performed with a prescribed kit of tools. For the purpose of illustrating the preferred embodiment, the tools of the kit will now be described. It will be appreciated that the method of the surgery can be practiced using a wide variety of tools of different size and shapes.

Each of the tools of a kit necessary to perform the surgery as described in this application will be separately described. The use of the tools will become apparent with the description of the method of the invention in Section IV.3 of this application. Unless otherwise specified, all tools are formed of stainless steel.

Since vertebrae size and disc space size vary from patient-to-patient (and since such sizes vary along the length of the spine of any given patient), several sizes of implants **10** are anticipated. Presently, implants **10** having minor outside diameters (D_m) of 3 mm, 5 mm, 7 mm, 9 mm, 11 mm, 13 mm, 15 mm, 17 mm, 19 mm and 21 mm with lengths (L) of 10 mm, 12 mm, 14 mm, 16 mm, 18 mm, 20 mm, 24 mm, 28 mm, 28 mm and 30 mm, respectively, are anticipated to accommodate various spine locations and sizes. The major outside diameters (D_M) of the implants **10** are 2.5 mm larger than the minor outside diameters D_m .

Several of the tools to be described (e.g., reaming tool **126**) are sized for particular sizes of implants. Namely, the reaming tool **121** must form a bore sized to receive the implant. Since ten sizes of implants are anticipated, ten sizes of boring tools **126** are anticipated as will become apparent to one of ordinary skill in the art.

B. Starter Alignment Guide Handle

The kit of the present invention includes a starter alignment guide handle **28** (see FIG. **21**). The handle includes a distal end **30** having an impact flange **31** and an axially extending threaded stud **32**. A proximal end **34** of the handle is knurled to permit a surgeon to firmly grip the handle **28**.

C. Starter Alignment Guide Assembly

The starter alignment guide assembly **36** (FIGS. **9** and **10**) includes a main body **40** having a threaded bore **42** sized to receive the threaded end **32** of handle **28**. Extending from the body **40** are parallel pins **44**, **46**. The pins are spaced apart by a distance D_1 as will be more fully described. The pins **44**, **46** have stop surface **45**, **47**.

As mentioned, since human anatomy varies significantly from one patient to another (and since the sizing of vertebrae varies depending on the location within the spine), it is anticipated that the kit will require various sizes of tools. With respect to starter alignment guide assembly **36**, it is anticipated that at least ten tools will be provided having pin spacings D_1 selected to identify a desired spacing of two implants each of diameters of 3, 5, 7, 9, 11, 13, 15, 17, 19, and 21 mm, respectively. However, such a kit will only require one guide handle **28** which can be inserted and attached to each of the starter alignment guide assemblies **36**.

The main body **40** is nylon to be X-ray transparent. Also, the body **40** has curved edges **49** with a radius of curvature to match a radius of a corresponding drill tube **92**. For example, for placing two 13 mm (D_m) implants **10**, a drill tube **92** with an inside diameter of 16.0 mm (for a D_M of 15.5) is required (the 0.5 mm difference providing clear-

ance). The edges **49** match the contour of the drill tube **92** and are spaced apart equal to a spacing of the drill tube when operating on either the right or left side. As a result, the back surface **43** of main body **40** may be placed against the spine to outline an area which must be cleared for the procedure. This aids the surgeon in determining the proper laminectomy size or required amount of vessel retraction.

D. Distraction Plug Inserter

A distraction plug inserter **48** (FIG. **25**) is provided and includes a shaft **50** and a handle end **51** which is knurled to provide a secure grip. A distal end **53** has a threaded shaft **52** extending axially therefrom. End **51** has a larger diameter than shaft **50** to provide a surface **49** against which slap hammer **192** (FIG. **26**) may strike as will become apparent.

E. Distraction Plug

A distraction plug **54** (FIG. **28**) is provided having a generally cylindrical body **56** with a tapered forward end **58**. The rear end has a reduced diameter portion **55** terminating at a flange **57** having a diameter the same as the body **56**. A threaded bore **62** is formed through the rear end to receive the threaded shaft **52** of the distraction plug inserter **48**. The body **56** is knurled to prevent undesired axial movement of the plug **54** after it is inserted.

As will be more fully described, the distraction plug **54** is used to initially distract opposing vertebrae. The amount of desired distraction will vary from patient to patient and from spine location to spine location. Accordingly, it is anticipated that distraction plugs having diameters D_2 ranging from 3 to 14 mm (by one millimeter increments) shall be included within the kit. Each of the distraction plugs fits on the inserter **48** such that only one inserter **48** is required for the kit.

F. Vertical Reamer Guide Pin

A vertebral reamer guide pin **64** (FIGS. **38** and **39**) is provided including a generally cylindrical body **66** having a tapered forward end **68** and a reduced diameter threaded rear end **70**. The tapered forward end **68** has three flats **69** that grind away disc material when the pin **64** is secured to a starter reamer **112** (FIG. **15**) as will be described.

As with the distraction plug **54**, a wide variety of sizes of guide pins **64** are anticipated to be required in the kit having diameters D_3 ranging from 3 through 14 mm (increasing by one millimeter increments). For reasons that will become apparent, it is desired that all of the guide pins **64** have a threaded stud **70** of identical size.

G. Drill Tube Guide

A drill tube guide **72** (FIG. **12**) is provided including a cylindrical shaft **74** and a distal end **76**. The distal end **76** has a predetermined maximum outside diameter D_4 . Provided on the axial face **78** of distal end is a bore **80** which is threaded and sized to receive stud **70** of the guide pin **64**. A proximal end **82** (of diameter D_4) of the drill tube guide has a threaded bore **81** for purposes that will be described. End **82** terminates at a flat axial face **83**.

In application, various sizes of implants **10** will be required depending on the anatomical sizing of the vertebrae to be fused. It is anticipated that implants **10** of ten different major outside diameters D_M will be required to accommodate a wide variety of applications. Accordingly, the kit of the present invention will include ten drill tube guides having outside diameters D_4 to finally prepare bores to receive the three sizes of implants as will be described. The outside diameters D_4 are equal to D_M for each matching pair of implant **10** and drill tube guide **72**.

H. Drill Tube Planar

In some applications, it may be desirable to plane a surface of a vertebrae. For example, tissue may covet the

surface of the vertebrae to be bored. The various tools of the present invention should abut vertebrae bone to insure that an implant 10 is inserted to a proper depth. A drill tube planar 84 removes the tissue and provides a flat surface on the vertebrae bone against which to place tools.

The drill tube planar 84 (FIGS. 13 and 14) includes a hollow tube 86 having an inside diameter D_5 . The distal end 88 of the drill tube planar 84 includes a toothed rasp surface 85 to rasp away bone material as the distal end 88 is placed against bone and the planar 84 is rotated about its axis. The proximal end 90 of the planar 84 includes a knurled handle to permit a surgeon to securely grasp the planar during the planing operation.

As will be more fully described, in the anticipated method of the present invention, the planar 84 will slip over the drill tube guide 72 with the diameter D_4 selected in close tolerance to D_5 (i.e., D_5 is 0.5 mm larger than D_4). As a result, ten planars 84 are required to fit on the ten sizes of drill tube guides 72.

The planar 84 includes an internal stop 87 positioned to oppose surface 83 of guide 72 when the planar 84 is placed over guide 72. A clean out hole 89 is provided to clean out planar 84.

I. Drill Tube

A drill tube 92 (FIGS. 31, 32, and 33) is provided in the form of a hollow cylindrical tube 94. The distal end 96 of the tube 94 is provided axially projecting teeth 98. The proximal end 99 of the tube 94 is flared outwardly for purposes that will become apparent. As will be apparent, ten sizes of tube 92 are required with inside diameters D_6 to slip in close tolerance over ten sizes of drill tube guide 72 (i.e., D_6 is 0.5 mm larger than D_4).

The teeth 98 each have a length, T_L , of preferably 3 mm. The valleys 97 are flat to provide stop surfaces to hit bone as teeth 98 are forced into vertebrae. This helps prevent the drill tube 92 from being forced too far into bone.

J. Drill Tube Insert Cap

As will be more fully described, the drill tube 92 is secured to vertebrae by forcing the teeth 98 into the vertebrae bone material. This is done by impacting the proximal end 99 of the drill tube 92. An inserter cap 100 (FIGS. 22, 23 and 24) is provided in the form of a solid cylinder having an axial bore 102 with an inside diameter D_9 terminating at a flat annular face 101. Diameter D_9 is slightly larger than outside diameter D_4 of drill tube guide 72 (FIG. 12) so that cap 100 can slip over end 82 of guide 72 with a stop surface 103 opposing end 83 and with surface 101 opposing flared end 99 of drill tube 92. The cap 100 has an opposite flat end 104 against which a surgeon may impact. This impacts the drill tube 92 to force the teeth 98 into the bone of a vertebrae.

K. Drill Tube Sleeve

A drill tube sleeve 105 (FIGS. 29 and 30) is provided in the form of a hollow tube having a flat distal end and an outwardly flared proximal end 110. Ten sizes of sleeves 105 are required in the kit having outside diameters D_7 sized to slip within, in close tolerance, the ten sizes of drill tubes 92. The inside diameter D_{10} is selected to be slightly greater (e.g., 0.5 mm larger) than the minor outside diameter D_m of the implants 10.

L. Starter Vertebral Reamer

To start a bore between opposing vertebrae, a starter vertebral reamer 112 is provided (FIGS. 15 through 18). The starter reamer 112 has a shaft 114. A reamer head 116 is secured to the distal end of the shaft 114. An axial face of the reamer 116 has a threaded bore 118 sized to receive the threaded shaft 70 of the vertebral reamer guide pin 64. A proximal end 120 has an outwardly flared hub 122 to act as

a positive stop against flare 110 of the drill tube sleeve 106 as will be more fully described. A shaft 124 extends from the distal end. The reamer 116 includes cutting blades 117 that provide both end cutting and side cutting into bone as the starter reamer 112 is rotated about its axis.

To accommodate ten sizes of implants, ten sizes of vertebral reamers 112 are included in the kit. The reamers 112 have outside diameters D_{11} equal to the minor outside diameters D_m of the implants 10.

M. Final Vertebral Reamer

A final vertebral reamer 126 (FIGS. 34 through 37), is provided for completing a bore started by the starter vertebral reamer 112. The final reamer 126 includes a shaft 128. A distal end of the shaft is provided with a reamer end 130 having side and end cutting blades 131. A proximal end of the shaft is provided with an outwardly flared hub 132. Extending from hub 132 is an axial shaft 134. For reasons given with respect to starter reamer 112, ten sizes of final reamers 126 are required with the kit. The outside diameter D_{12} of final reamer 126 equals the minor outside diameter D_m of implants 10.

N. Vertebral Reamer Hand Driver

To operate reamers 112 and 126, a hand driver 136 (FIGS. 46 and 47) is provided. The hand driver includes an axial bore 138 to receive either of shafts 124 or 134. The hand driver 136 also includes a manually engageable handle 140 to be actuated by a surgeon performing the surgery of the present invention.

The handle has an enlarged barrel portion 137 with radial grooves 139. With one hand, a surgeon puts axial pressure on handle 140 and with the other hand the surgeon rotates barrel 137 with fingers in grooves 139. Thus, the surgeon can securely turn a reamer secured to the driver 136.

Radial bores 141, 143 extend through barrel 137 to receive set screws to fix a shaft 124 or 134 received within bore 138.

O. Bone Tap

In the event a threaded implant is utilized (as is the case in the preferred embodiment of the present invention), the bores for the implant are partially prethreaded. To prethread, a bone tap 142 (FIGS. 40 through 42) is provided, having a shaft 144. At the distal end of the shaft 144 is a tapping head 146 having tapping threads 148. Near the proximal end of the shaft 144 is an enlarged diameter portion 156 having an outwardly flared flange 158. A handle 160 is secured to the enlarged portion 156. The shaft 144 is also enlarged at portion 162 adjacent tapping head 146. The enlarged portion 156 is sized with diameter D_8 to be received, in close tolerance, within the drill tube 92 such that the tube 92 will guide the tap 142 as will be more fully described.

Since ten sizes of implants 10 are intended to be utilized, ten sizes of bone taps 142 are required. Diameter D_6 is equal to the major outside diameter D_M of implant 10. The head 146 has a minor outside diameter D_{13} (i.e., the diameter without threads 148) equal to the minor outside diameter D_m of the implants 10.

P. Implant Driver

To place implant 10, an implant driver 164 (FIGS. 43 through 45) is provided. The driver 164 includes a shaft 166 having a reduced diameter distal portion 166a. A distal end of the shaft 166 is provided with a hub 168 sized to be received within slot 24 of the implant 10 to urge the implant 10 to rotate as the implant driver 164 is rotated. The implant driver 164 includes a stepped enlarged portion 170 including a first diameter portion 172, a second diameter portion 174 and a third diameter portion 176 to accommodate the different diameters of drill tubes 92. A handle 178 is secured to the shaft 164. Grooves 180, 180a are formed on the shafts

166, 166a and extend along their axial lengths. The grooves 180 provide a means for a surgeon to sight the alignment of the implant.

FIGS. 45A and 45B show the implant driver 164 with a collet 171. The collet 171 has a cylindrical, knurled body 173 slidably carried on shaft 166a. A pin 175 extending from body 173 into groove 180a permits collet 171 to slide on shaft 166 but not rotate. Four prongs 177 extend axially from body 173 toward hub 168.

In use, shaft 166 is passed through end opening 24 of implant 10. Hub 168 is receiving within slot 25. The prongs 177 are forced by a surgeon pushing on body 171 for the prongs 177 to be urged between opposing surfaces of the implant 10 and shaft 166a to thereby securely capture the implant 10 on driver 164. As a result, the implant 10 cannot inadvertently fall off. (For ease of illustration, the Figures showing the method of the invention, FIGS. 48–63A, do not show use of collet 171).

Q. Endcap Inserter

Once an implant is placed between two vertebrae an endcap must be secured to the implant according to the preferred embodiment. To this end, an endcap inserter 180 (FIGS. 19 and 20) is provided. The inserter 180 includes a shaft 182. At the distal end of the shaft, a head 184 is provided having a cupped surface 186 to receive and temporarily hold an endcap 26 before it is secured in place. An enlarged portion 180 of the shaft is sized to be received, in close tolerance, within drill tube 92 to be guided by the tube 92. Since ten sizes of drill tubes are required for ten sizes of implants, ten sizes of endcap inserters are also required. The inserter 180 has an outside diameter D_{14} just smaller than (e.g., 0.5 mm smaller) than the inside diameter D_6 of the drill tube 92. A knurled handle 190 is provided on the proximal end of the shaft 182.

R. Slap Hammer

To remove the distraction plug 54 or drill tube guide 72, a slap hammer 192 (FIGS. 26 and 27) is provided. The slap hammer is a cylindrical body having a knurled surface to permit a surgeon to securely grip the body. The hammer has an axial slot 196. The hammer is placed on the shafts 202, 50 of handle 200 or inserter 48, respectively, with the tool shaft received within slot 196. By pulling back on hammer 192 and impacting it against a stop surface (e.g., surface 49 of tool 48), a tool can be removed.

S. Drill Tube Guide Removal Handle

A handle 200 (FIG. 11) is provided to remove the drill tube guide 72. The handle 200 includes a shaft 202. At the distal end, a threaded stub 204 is provided sized to be threadably received within the threaded bore 84 of the drill tube guide 72. A proximal end of the handle 200 is provided with an enlarged diameter knurled handle 206 to permit a surgeon to securely grasp the handle 200 and to stop the travel of slap hammer 192.

T. Drill Tube Sheath

As will become apparent, drill tube 92 or planar 84 are passed through a patient's body to an implant site. To avoid risk of teeth 85 or 98 damaging vessels, nerves or organs, a drill tube sheath 300 is provided (FIGS. 29A, 29B). The sheath 300 is a hollow tube with inside diameter D_{15} slightly smaller than the outside diameter of drill tubes 92 or planars 84 (accordingly ten sizes of sheath 300 are required). The sheath 300 has an axial slit 301 extending its entire length. The sheath 300 has a blunt distal end 302 and a flared proximal end 304.

The sheath is slipped onto the drill tube 92 or planar 84 with end 302 extending beyond the teeth 85 or 98 (see FIG. 64A illustrating use of sheath 300 with drill tube 92). As the

planar 84 or drill tube 92 are passed to an implant site the blunt end 302 covers the teeth and prevents the unwanted cutting of vessels, nerves or organs. When pressed against vertebrae, the end 302 abuts the vertebrae. With continued advancement of the tube 92 or planar 84 toward the vertebrae, the sheath 300 slides on the planar 84 or tube 92 until teeth 85,98 abut the vertebrae.

In the method of the invention, sheath 300 remains in place whenever planar 84 or drill tube 92 are used. However, for ease of illustration, sheath 300 is not shown in FIGS. 46–63A.

3. Posterior Technique

A. Surgical Approach

The present invention will first be described with reference to use in a posterior approach. In a posterior approach, a surgeon seeks access to the spine through the back of the patient. An alternative approach is an anterior approach where the surgeon seeks access to the spine through the abdomen of a patient. The anterior approach can be done through open surgery or through laparoscopic surgery.

While a posterior approach will be described in detail, it will be appreciated that the present invention can be used in an anterior approach for both laparoscopic or non-laparoscopic procedures.

Once a surgeon has identified two vertebrae which are to be fused together, the surgeon identifies an implant of desired size and the surgeon determines the desired amount of distraction to be required between the vertebrae before placement of the implant. In selecting the implant size, the surgeon should ensure that the device will remain within the lateral borders of the intervertebral disc while also penetrating at least 3 mm into the vertebral bodies cephalad and caudal to the disc.

In the posterior technique, a patient is placed on the operating table in either a prone or kneeling-sitting position. At the discretion of the surgeon, the spine is flexed slightly. Anesthesia is administered.

Exposure of the intervertebral disc is obtained through any suitable technique well-known in the art. The facet of the vertebrae is removed in as limited amount as possible to permit insertion of the instruments and the implants. Preferably, bone dissected from the lamina, facets and spinous process are preserved for later use as bone graft.

Referring to FIG. 48, two vertebrae 210, 212 are separated by a disc 214. The disc 214 is shown in plan view in FIG. 48A. As shown in the figures, no procedure has yet been performed on the disc such that the disc 214 is in a relaxed, undistracted state.

B. Identifying Desired Implant Locations

After having selected the implant size, the surgeon selects the starter alignment guide assembly 36 and secures the handle 28 to the assembly 36 by threading shaft 32 into bore 42. The prongs 44, 46 of the guide 36 are placed on either side of the cauda equina such that they are at mid-disc height and equidistant from the mid-sagittal plane. The guide is pressed ventrally to make two points 44a, 46a on the disc for implant insertion as shown in FIGS. 49, 49A. The two points 44a, 46a mark right and left side desired implant location points. For the purposes of this discussion, right and left will mean with respect to the view of the back of the spine as viewed by the surgeon performing the surgery through the posterior approach.

After the starter alignment guide 36 is urged into position as shown in FIGS. 49, 49A, the handle 28 is unscrewed and removed from the guide 36. Lateral and anterior-posterior x-rays or C-arm fluoroscopy are taken the alignment guide

36 to verify its orientation within the disc space. If the alignment guide 36 is determined to be correctly positioned, it is removed from the disc space by reattaching handle 28 and pulling the guide 36 out. A limited discectomy is performed through the two openings 44a, 46a in the disc to permit insertion of a distraction plug 54.

C. Left Side Distraction

Once the left and right side desired implant locations are identified by placement of the starter alignment guide 36, and after the guide 36 is removed, the surgeon selects a side (i.e., left or right) in which to initiate the distraction procedure. Beginning with the left side for purposes of example, the distraction plug inserter 48 is secured to a distraction plug 54 by threading end 52 into bore 62. The distraction plug 54 is forced into the disc space at the indent 46a made at the left side of the vertebrae by the prong 46 (see FIGS. 50 and 50A). The size of distraction plug 54 is selected to distract the annulus fibrosus without causing damage to the surrounding vertebral bone, annular fibers or spinal nerves. Accordingly, it is recommended the surgeon initially insert a relatively small plug 54 (for example, 8 mm) followed by successively larger plugs until the annulus is distracted to the surgeon's satisfaction. Once the correct maximum size distraction plug 54 has been chosen, it is left in place and the handle 48 removed as shown in FIGS. 51 and 51A. The disc 214 has now been stretched so that a parallel distraction of the opposing end plates 210', 212' of the vertebrae 210, 212 has occurred on both the left and right sides. The distraction plug 54 is fully inserted such that it is either flush or slightly recessed within the disc space.

In performing the procedures of the present method, the surgeon takes care to retract the cauda equina and nerve roots from the area being prepared for the drill tube 92 as will be described. To this end, the distraction plug 54 is placed recessed. As a result, the cauda can be moved over into the region of the distractor plug 54 without the distractor plug 54 damaging the cauda equina.

D. Right Side Alignment

Once the distraction plug 54 is inserted as shown in FIGS. 51, 51A, the surgeon proceeds to the right side location 44a. The vertebral reamer guide pin 64 is secured to the drill tube guide 72 by threading the shaft 70 within the bore 80. The guide pin 64 selected is preferably the same diameter as the final distraction plug 54 left in place within the disc space on the left side. As a result, upon insertion of the guide pin 64 as shown in FIGS. 52, 52A, the guide pin 64 abuts the opposing end plates 210', 212' of the vertebrae 210, 212 as does plug 54. The axis of pin 64 is equidistant from the end plates 210', 212'.

E. Planing Vertebral Surface

The surface of the vertebrae 210, 212 against which tools are to be placed should be smooth with the surface of the two vertebrae 210, 212 aligned. Frequently, this condition will not naturally exist. Therefore, the vertebrae 210, 212 must be pre-planed to a flat surface.

If planing is deemed necessary by the surgeon, the drill tube planar 84 is passed over the drill tube guide 72 with the rasp end 88 abutting the disc material 214 and vertebrae 210, 212 or tissue (not shown) on the vertebrae as shown in FIGS. 53, 53A. The interior diameter of the planar 84 is selected to have a close tolerance with the exterior diameter of the drill tube guide 72. As a result, the planar 84 can rotate on the drill tube guide 72 and move axially relative thereto but cannot move laterally relative to the tube guide 72. The surgeon rotates the planar 84 to rasp a planed flat surface on the vertebrae. The rasping will provide a smooth surface for

placing of the drill tube as will be described. For purposes of illustration, the rasp end 88 is shown deeply received with the vertebrae after rasping.

The drill tube guide 72 prevents planar 84 from excessive axially movement. Namely, when planar 84 is fully advanced, surface 87 abuts surface 83 signalling completion of the rasping operation.

F. Fixing Right Side Alignment

After the surface of the vertebrae has been planed smooth, the planar 84 is removed and the appropriately sized drill tube 92 is passed over the drill tube guide 72 (see FIGS. 54, 54A). The teeth 98 of the drill tube 92 are secured to the posterior vertebral bodies using the drill tube inserter cap 100 to pound the teeth 98 into the vertebral bodies 210, 212. The drill tube guide 72 and the vertebral reamer guide plug 64 are then removed from the drill tube 92 leaving the drill tube 92 in place and with the teeth 98 thereby retaining the vertebral bodies in the distracted state. To remove the guide 72, handle 18 is attached to guide 72 by threading stud 204 into bore 84. The surgeon uses the slap hammer 192 to remove the guide and handle assembly.

FIG. 64 illustrates use of the cap 100 to advance teeth 98 into the vertebrae 210, 212. As shown, the drill tube guide 72 is longer than drill tube 92. With teeth 98 aligned with end 78, end 83 protrudes beyond flange 99. The cap 100 is positioned as shown in FIG. 22A. The cap is sized for the distance, X, between surfaces 83, 103 to be about 3 mm when teeth 98 are flush with end 78. Pounding on surface 104, teeth 98 are driven in 3 mm until surface 103 stops against surface 83. The flats 97 of the teeth 98 prevent further advancement of the drill tube 92 into the bone.

The drill tube 92 has an inside diameter approximate to the outside diameter of the drill tube guide 72. Accordingly, the drill tube guide 72 accurately places the drill tube 92 in proper alignment. In this alignment, the tube 92 has its axis equidistant from the end plates 210', 212' of vertebrae 210, 212. Since all insertion tools and tubes of the kit have lengths sized off of the drill tube guide 72, the guide 72 insures that a final desired depth of implant penetration is attained.

G. Placement of Drill Tube Sleeve

With the drill tube guide 72 and the vertebral reamer guide plug 64 removed from the drill tube 92, a drill tube sleeve 106 is placed in the drill tube with the top end 110 abutting the top end 99 of the drill tube 98. As shown in FIGS. 55, 55A, when the sleeve is fully inserted, its flared end 110 abuts the flared end of the drill tube.

H. Pre-Boring of Implant Bore

The vertebral reamer guide pin 64 is then threaded on to the starter vertebral reamer 112. The guide pin 64 used is the same pin 64 previously used on the drill tube guide 72. The cavity 65 (FIG. 55) left after removal of the pin 64 (described in step G, above) receives the pin 64/reamer 112 assembly to guide the reamer 112 such that the reamer 112 cuts equal amounts of bone from both vertebrae 210, 212.

The starter vertebral reamer 112 is inserted into the drill tube sleeve 106 and then a bore is partially reamed until a shoulder 122 on the reamer 112 abuts the drill tube sleeve 106 as shown in FIGS. 56, 56A. The hand driver 136 (FIG. 46) is used to turn reamer 112. However, for ease of illustration, the driver 136 is not shown in FIGS. 56, 56A. The reamer 112 and the drill tube sleeve 106 are then removed from the drill tube 92 (see FIGS. 57, 57A) exposing a pre-drilled bore 200 with a diameter equal to the minor outside diameter D_m of implant 10.

I. Final Reaming

The preparation of the implant bore is then completed by inserting the final vertebral reamer **126** into the drill tube **92** (FIGS. **58**, **58A**). The reamer **126** is rotated with driver **136** (not shown in FIG. **46**) until the shoulder **132** on the reamer **126** meets the flared end of the drill tube **92** to thereby provide a positive stop.

Since bore **200** is pre-drilled, a drill sleeve **106** is not required for final drilling since the bore **200** initially guides final reamer **126**. This provides greater clearance and ease of operation of final reamer **126**. The final reamer **126** is removed leaving a fully drilled implant receiving bore **220** with a diameter equal to the minor outside diameter D_m of implant **10** (see FIGS. **59** and **59A**).

In the foregoing, the reader will note that the lengths of the various drill tubes, drill tube sleeves and reamers are selected such that the flared ends provide accurate depth of reaming between the vertebral bodies. Also, the reader will note that both vertebrae **210**, **212** are equally drilled. Additionally, the reader will not the pre-boring of step H, above, ensures the final bore **220** is cut parallel to end plates **210'**, **212'** and equally cut into both vertebrae **210**, **212**.

J. Bone Tap

In the event a threaded implant is used (as is the case in the preferred embodiment), a bone tap **142** is passed through the drill tube **92** and rotated to partially pre-tap the bore **210**. The tap is introduced until the stop **158** on the handle abuts the top of the drill tube **92** as shown in FIGS. **60**, **60A**.

The tap is then removed to expose a partially tapped, fully bored implant bore **300** with the drill tube **92** remaining in place (see FIGS. **61** and **61A**).

K. Placing Implant

The front chamber **16** of the implant **10** is packed with bone graft. The graft may be autograft obtained previously from the iliac crest or some other graft material (e.g., allograft or artificial bone). The implant **10** is attached to the implant driver **164** by placing the hub **188** within the slot **24** and securing the implant with collet **171** (not shown in FIGS. **62**, **62A**). The implant **10** is then passed into the drill tube **92** (FIGS. **62**, **62A**). The implant **10** is threaded into the bore **300** with implant driver **168** by the surgeon rotating the driver **168** and advancing it into the tube **92** until the driver stop **176** contacts the top of the drill tube **92**.

It is desirable that the large holes **211** of the implant are oriented in a superior-inferior direction (i.e., the large holes are facing the vertebrae). This orientation is guaranteed by orienting the slots **180** in the implant driver **168** to be vertical.

After the implant **10** is fully in place (recessed into bore **300**), the implant driver **168** and the drill tube **92** are removed from the right-side hole (see FIGS. **63** and **63A**). Simply pulling on driver **164** releases the implant **10** from the collet **171**.

At this point in the procedure, it is recommended that the surgeon obtain a lateral radiograph or C-arm fluoroscopy to verify the positioning of the implant **10** within the intervertebral space. If proper positioning has been obtained, the back chamber **17** of the implant **10** is packed with bone graft. Alternative to the above, the drill tube **92** may be left in place with the graft inserted to chamber **17** through tube **92**. If removed, tube **92** is repositioned after chamber **17** is filled. The polyethylene endcap **26** is attached to the end of the implant **10** with the endcap inserter **180** by passing the endcap through the drill tube **92**.

At this stage in the procedure, the right side implant is fully inserted.

The reader will note in placing the implant **10**, the movement of driver **164** is limited by stop **176**. If a smaller implant **10** is used (and hence a smaller diameter drill tube **92**), the movement is stopped by surface **174** or **176** (see FIG. **43**).

L. Left Implant and Closure

The surgeon returns to the left side and removes the distraction plug **54** by threading the handle **48** into the distraction plug **54** and pulling it out using slap hammer **192**. If, for any reason, the threaded stud **52** on handle **48** were to break, the reduced diameter portion **55** of plug **54** permits a surgeon to pull on flange **57** to remove plug **54**.

The left side is now prepared for receiving an implant in a manner identical to that described above for the right disc space with the procedures identified in FIGS. **52** through **63A**.

After the right and left implant are fully inserted, it is recommended that a lateral radiograph be taken of the implants. Assuming proper positioning, bone graft is impacted between and surrounding the implants to better facilitate fusion. The wound is closed.

4. Other Surgical Procedures

The foregoing procedure illustrates the method of the present invention with respect to a posterior approach. However, the identical procedure can be used with an anterior approach. Also, those skilled in the art will note that the present procedure is readily adaptable to a laparoscopic approach. Through placement of a cannula (not shown) in a laparoscopic approach, all the procedures can be performed through the cannula with the various tubes and sleeves described above passed through the cannula and accurately placed.

All of the foregoing tools of the kit of the invention can be passed through a cannula except for alignment guide assembly **36**. Instead of using assembly **36** in a laparoscopic approach, the implant sites can be marked through any other suitable technique or a collapsible alignment guide assembly can be provided to pass through a cannula.

In addition to the above, the method and tools of the invention can be used with a single implant (either a threaded implant **10**, a non-threaded implant or a bone or any other implant). In this method, the plug **54** is inserted at a desired site. The plug **54** is then removed and the pin **64** inserted into the same site using the guide **72**. All procedures described above are then used to form an implant receiving bore.

From the foregoing detailed description of the present invention, it has been shown how the objects of the invention have been obtained in the preferred manner. However, modifications and equivalents of the disclosed concepts such as those which would occur to one of ordinary skill in the art, are intended to be included within the scope of the present invention.

What is claimed is:

1. A surgical method for laparoscopically implanting at least two spinal fusion implants into a disk space separating a first vertebra and a second vertebra for stabilization of the spine, said method comprising:

- (a) placing a cannula for accessing the spine and passing implantation tools through the cannula in alignment with a first location at said disk space;
- (b) selecting a distraction spacer having a rigid body with diametrically opposite surfaces separated by a distance corresponding to a desired distraction of said vertebrae;
- (c) passing said distraction spacer through said cannula to said first location;

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- (d) distracting said disk space by urging said distraction spacer completely into said disk space at said first location from said cannula;
- (e) placing said cannula in alignment with a second location at said disk space after steps (a) through (d);
- (f) passing a first of said implants through said cannula to said second location;
- (g) inserting said first implant into said second location;
- (h) placing said cannula at said first location after steps (e) through (g);
- (i) removing said spacer through said cannula;
- (j) passing a second of said implants through said cannula to said first location; and
- (k) inserting said second implant into said first location.

2. A method according to claim 1 further comprising selecting a hollow tube having an open first end and an open second end and with said first end having a plurality of exposed teeth around said open first end to bite into both of said vertebrae, said exposed teeth extending permanently and axially away from said open first end and surrounding a perimeter of said open end.

3. A method according to claim 2 further comprising placing a sleeve around an external surface of said tube with said sleeve having a blunt distal end and with said sleeve slidably placed on said tube with said blunt end surrounding said perimeter and covering said exposed teeth, said sleeve slidable on said tube to a recessed position with said blunt end recessed for said teeth to extend beyond said blunt end.

4. A method according to claim 3 further comprising laparoscopically advancing said first end of said tube and said distal end of said sleeve toward a desired implant location of said disk space with said blunt end contacting said vertebrae at said location.

5. A method according to claim 4 further comprising continuing advancement of said first end of said tube toward said location with said blunt end maintained in contact with said vertebrae at said location and with said sleeve sliding relative to said tube to said recessed position during said continuing advancement and urging said teeth into said vertebrae to fix said tube first end at said location, whereby said blunt end covers said teeth throughout advancement of said tube first end to prevent injury from said teeth as said first end of said tube is advanced.

6. The method of claim 1, further comprising marking said first and second locations at said disk space before step (a).

7. The method of claim 1, further comprising: after step (e):

- (e1) passing a guide tube through said cannula to said second location with an axis of said guide tube centrally positioned between end plates of said first and second vertebrae;
- (e2) passing a boring tool through said guide tube to said second location and with said boring tool and guide tube having cooperating surfaces to prevent lateral movement of said boring tube relative to said guide tube as said boring tool is moved axially relative to said guide tube;

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- (e3) boring a bore with said boring tool at said second location into said disk space and at least partially into each of said first vertebra and said second vertebra;
- (e4) removing said boring tool through said cannula; and after step (i) and before step (j):
- (i1) passing a boring tool through said cannula to said first location;
- (i2) boring a bore with said boring tool at said first location into said disk space and at least partially into each of said first vertebra and said second vertebra;
- (i3) removing said boring tool through said cannula.

8. The method of claim 7, wherein step (g) comprises inserting said first implant into the bore bored at said second location, and step (k) comprises inserting said second implant into the bore bored at said first location.

9. A surgical method for laparoscopically implanting a spinal fusion implant into a disk space separating a first and second vertebra for stabilization of the spine, said method comprising:

placing a cannula for accessing the spine and passing implantation tools through the cannula;

laparoscopically placing through said cannula a hollow tube having an open first end and an open second end with said tube placed with said first end positioned against said disk space at a desired implant location; and

selecting a boring tool having a guide pin on a distal end thereof and a cutting portion proximal to the guide pin, said guide pin having a radial dimension sized to approximate a desired distraction of said disk space and smaller than a radial dimension of the cutting portion of said tool at said distal end, said guide pin attached to said boring tool for movement therewith and prevented from movement independent from said boring tool, and said guide pin having at least one flat capable of grinding away disk material.

10. A method according to claim 9 further comprising simultaneously inserting said distal end and said attached guide pin into said second end of said tube and passing said distal end and said attached guide pin through said tube to said desired implant location.

11. A method according to claim 10 further comprising advancing said guide pin into said disk space with said pin urging against opposing surfaces of said first vertebra and said second vertebra.

12. A method according to claim 11 further comprising rotating a proximal end of said boring tool external of said tube to cause rotation of said cutting portion with said cutting portion boring into said opposing surfaces.

13. A method according to claim 12 further comprising advancing said distal end into said disk space while continuing said rotation and with said guide pin guiding said distal end by advancing into said disk space simultaneous with an advancement of said cutting portion to maintain an axis of said distal end in parallel and equidistant spacing between said opposing surfaces.

* * * * *

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摘要(译)

脊柱融合植入物通过腹腔镜放置在分隔两个椎骨的椎间盘中。植入工具，包括撑开间隔器，钻孔工具和植入物，通过套管朝向磁盘空间。

