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(54) **STEREO LAPAROSCOPE WITH DISCRETE WORKING DISTANCE**

(52) **U.S. Cl.** 600/111; 600/173

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(57) **ABSTRACT**

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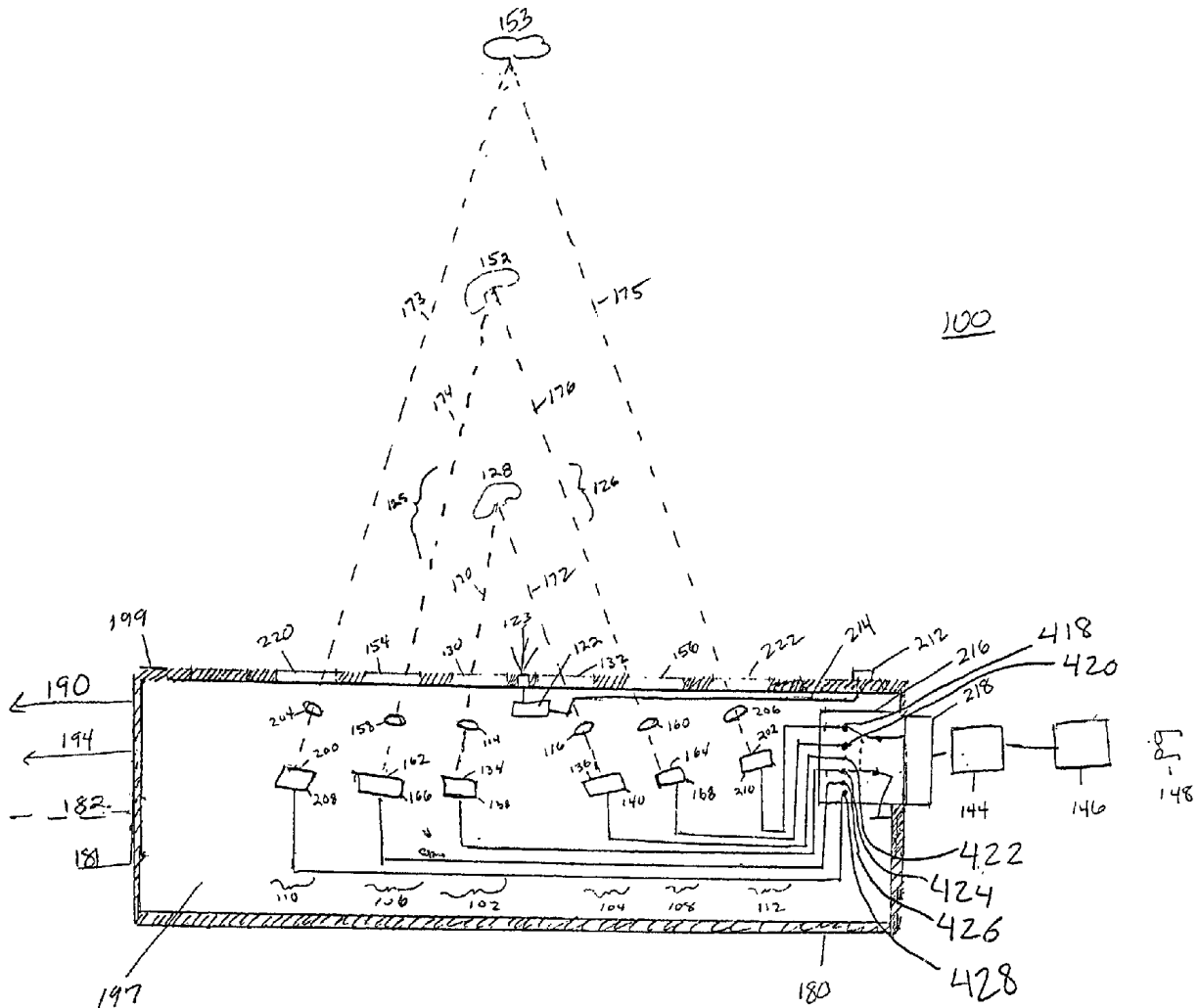
A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region to be viewed through a small incision. The stereo laparoscope included multiple imaging assemblies disposed in a direction non-parallel to the axis of the laparoscope. The imaging assemblies are disposed in a fixed orientation relative. Selection and processing means are included for enabling the user to select a left imaging assembly and a right imaging assembly from three or more imaging assemblies. The left and right views provide three dimensional or stereoscopic viewing, and the distance between at least two assemblies can be greater than the diameter of the laparoscope.

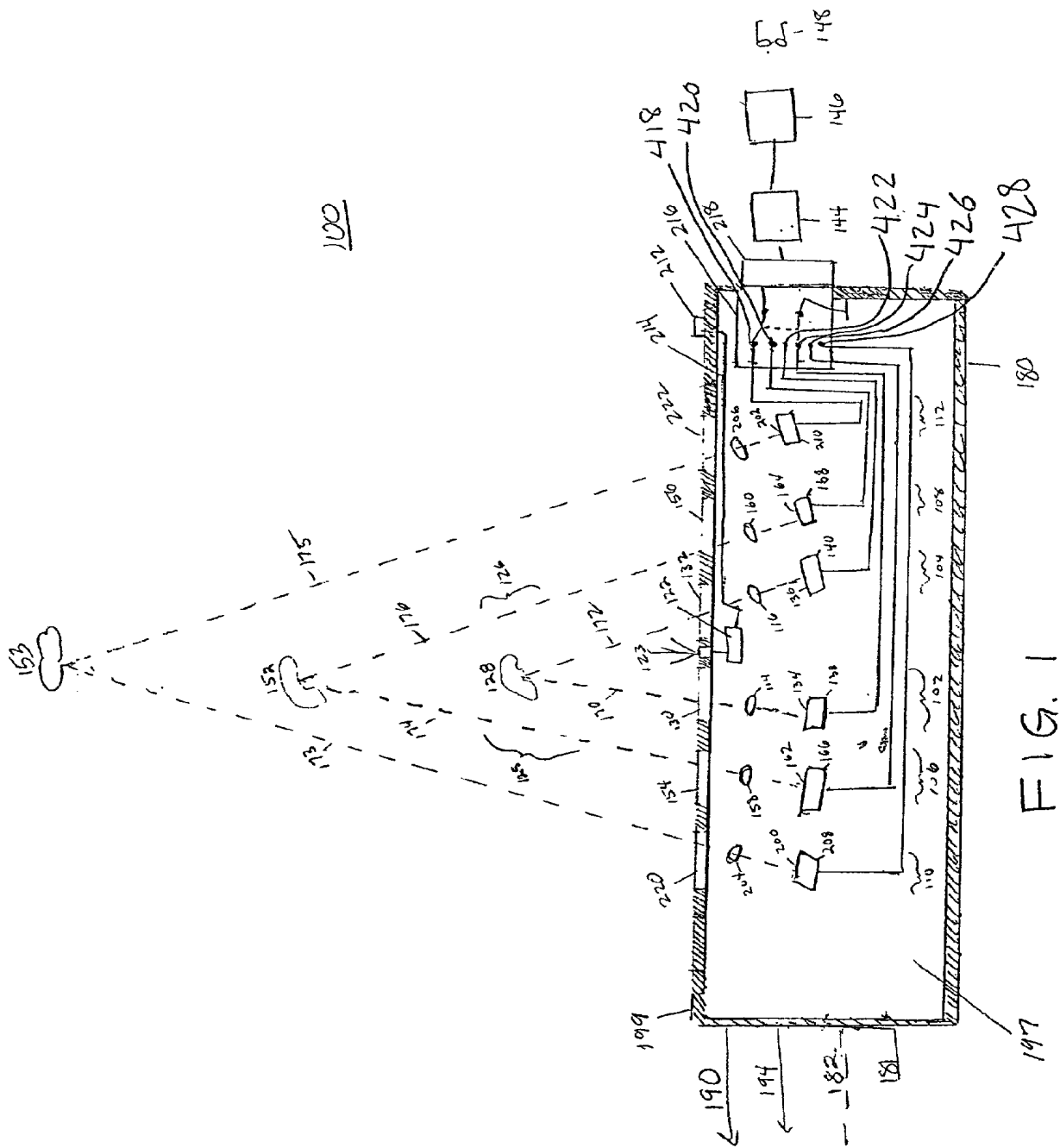
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(51) **Int. Cl.⁷** **A61B 1/04**





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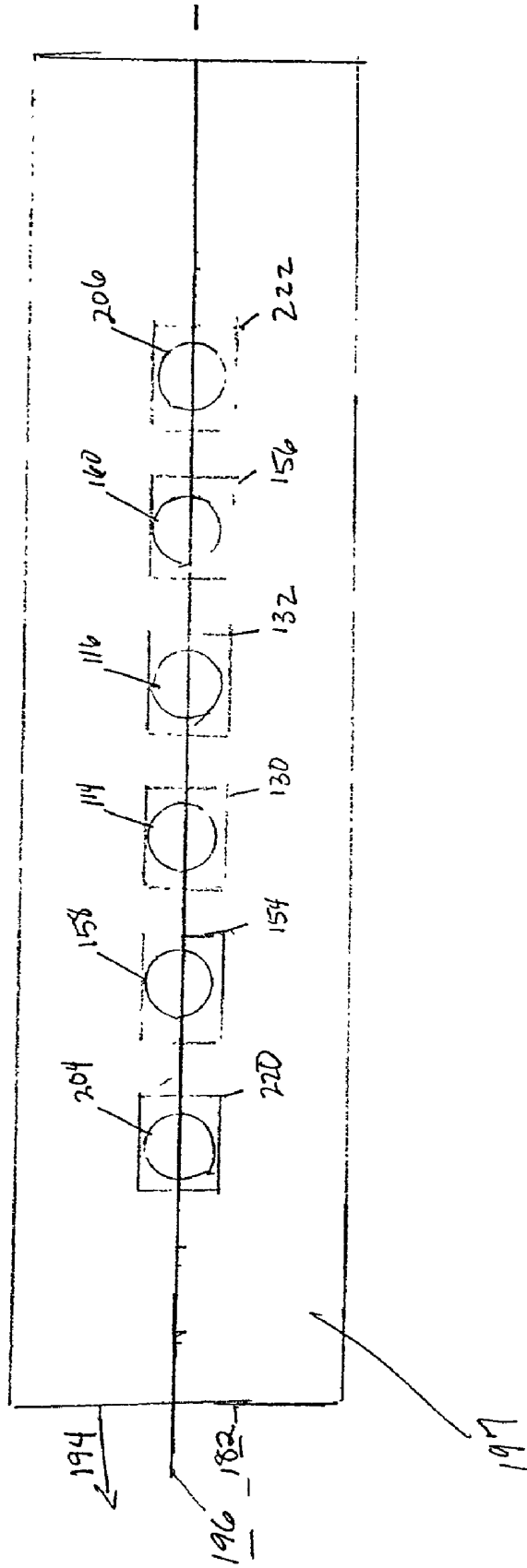
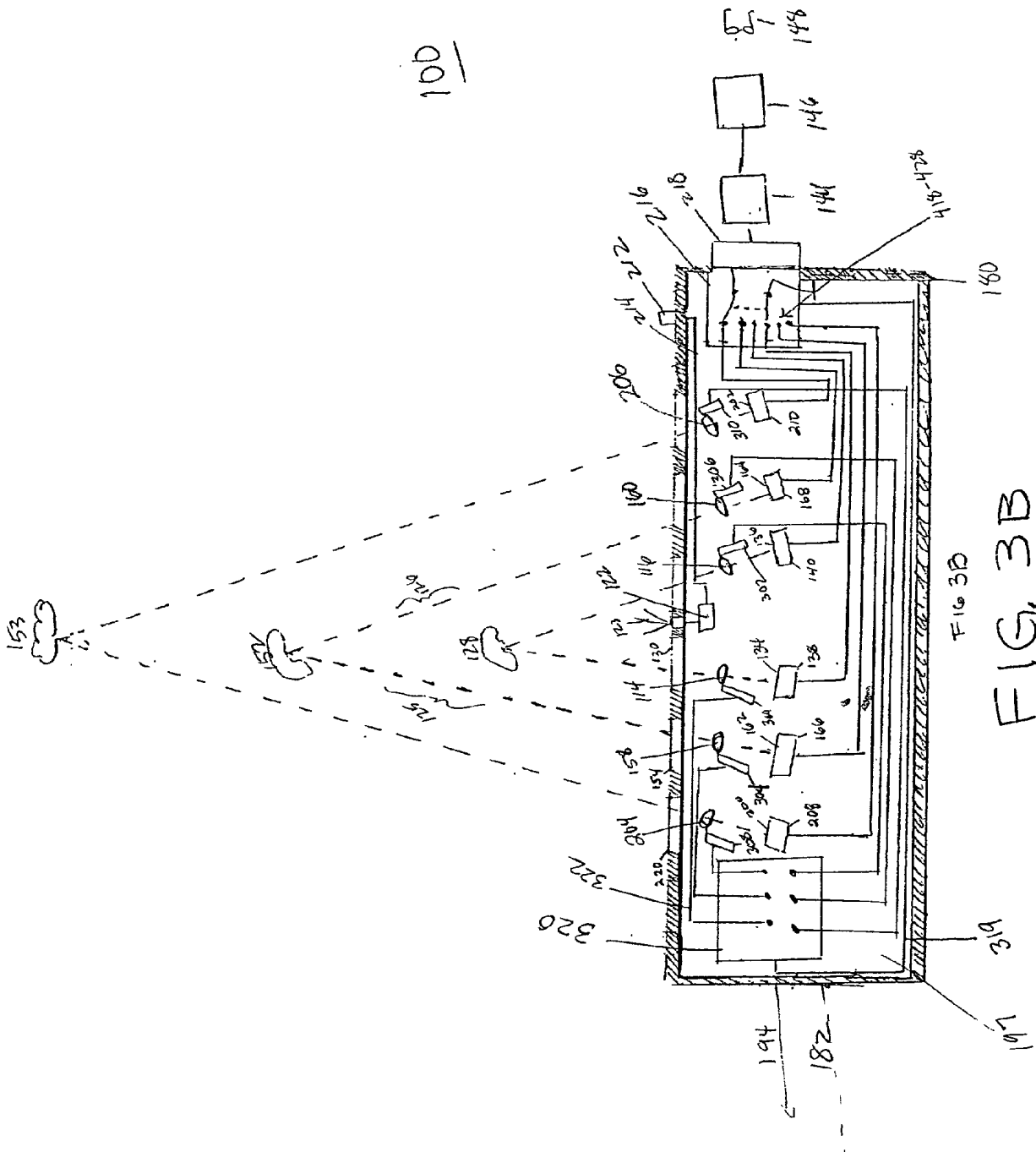


FIG. 2



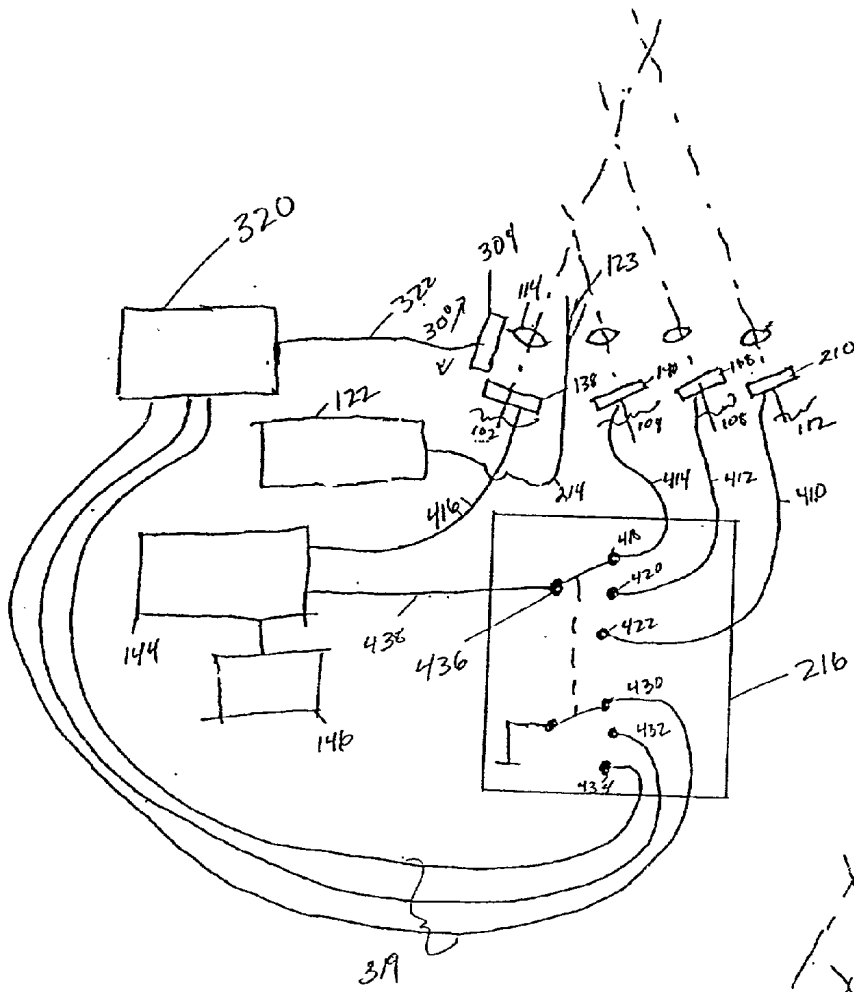


FIG 4

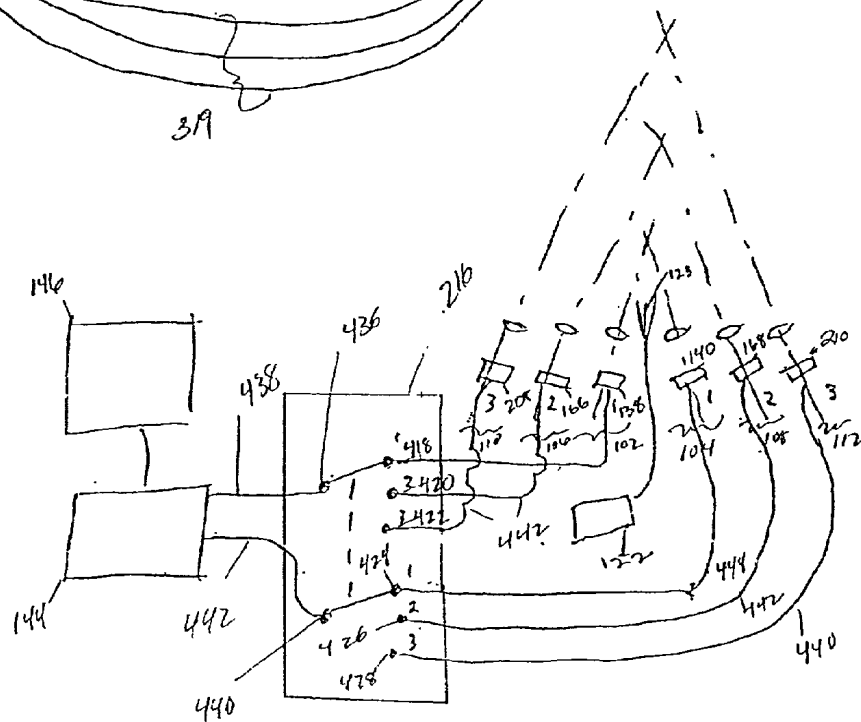


FIG 5

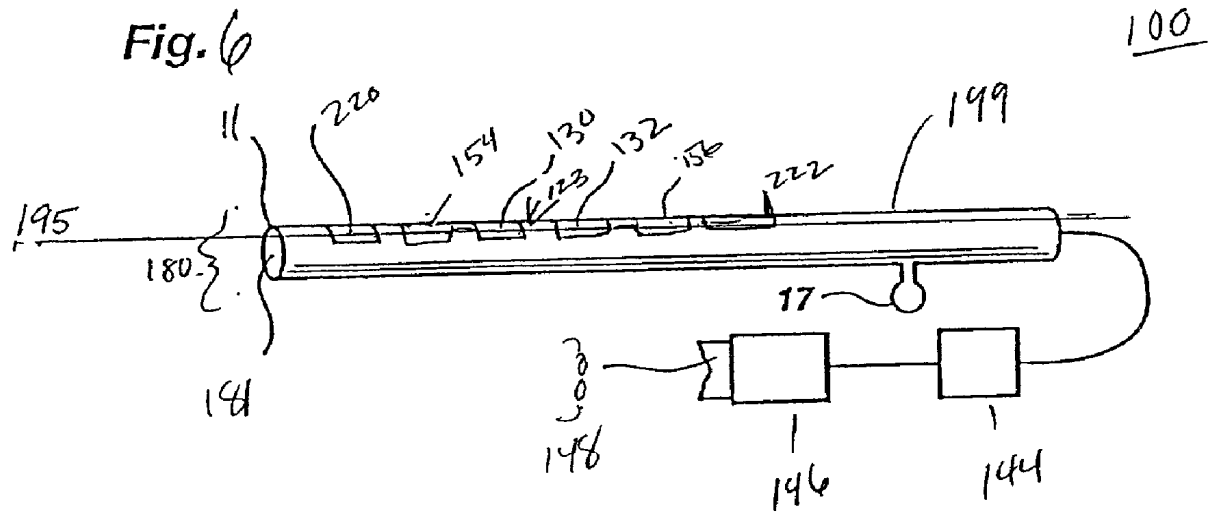
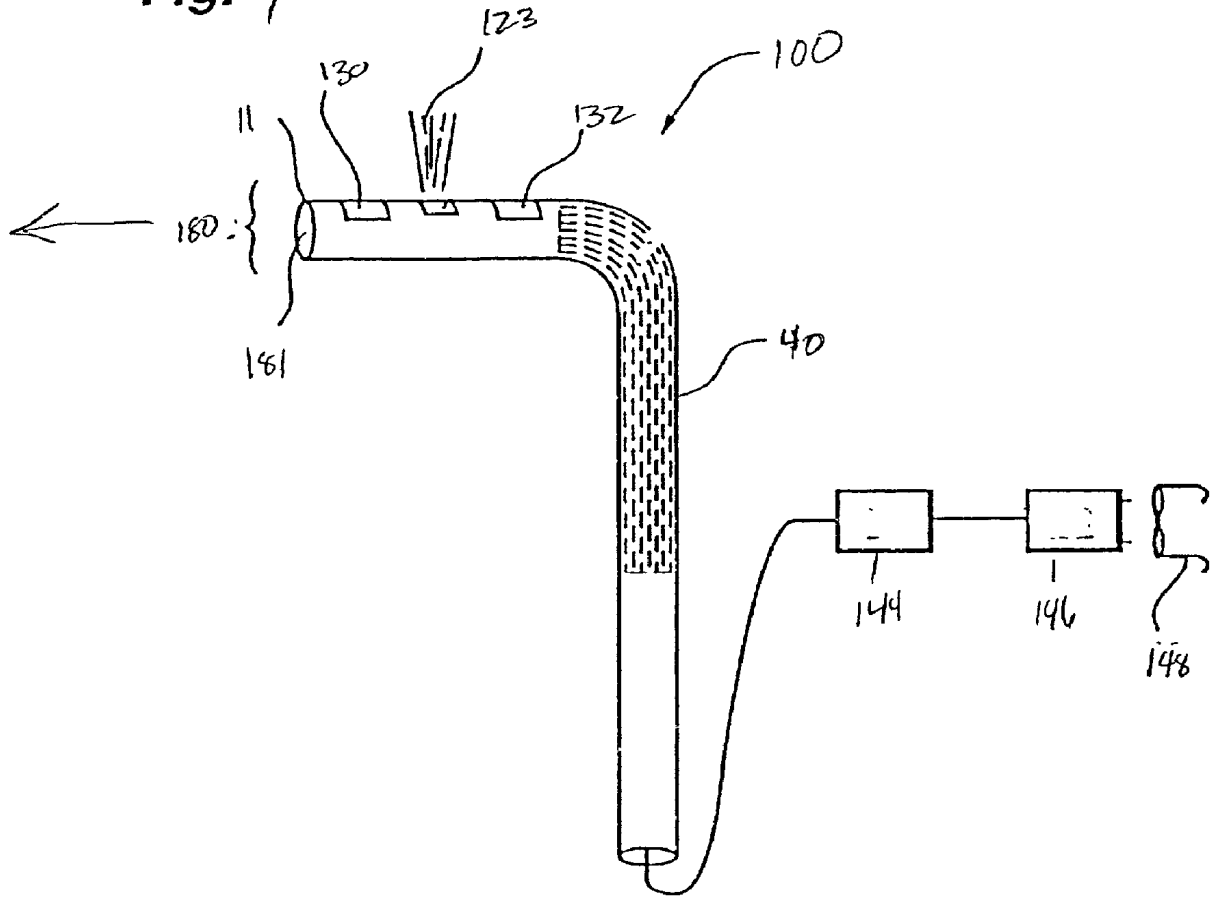


Fig. 7



STEREO LAPAROSCOPE WITH DISCRETE WORKING DISTANCE

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This application is a continuation-in-part of co-pending international application Serial No. PCT/US99/22864, with an international filing date of Oct. 4, 1999, published in english under PCT Article 21(2), entitled "STEREO LAPAROSCOPE WITH SYNCHRONIZED OPTICS."

[0002] This application is a continuation-in-part of co-pending international application Serial No. PCT/US99/22864, with an international filing date of Oct. 4, 1999, published in english under PCT Article 21(2), entitled "STEREO LAPAROSCOPE WITH SYNCHRONIZED OPTICS," of which the following selected portions are hereby incorporated by reference in this application:

- [0003] page 1, lines 11-15 ending at the word "imaging;"
- [0004] page 1, line 21 through page 2, line 27 ending at "images;"
- [0005] page 2, line 32 through page 3, line 27;
- [0006] page 3, line 31 through page 5, line 1 ending "image;"
- [0007] page 5, lines 6-23;
- [0008] page 7, line 19 beginning at "the" through page 7, line 25 ending at "112;"
- [0009] page 7, line 29 through page 8, line 17 ending at "100;"
- [0010] page 8, lines 24-29;
- [0011] page 9, line 8-12;
- [0012] page 9, line 21 through line 24, ending at "art;"
- [0013] page 10, lines 7-20;
- [0014] page 11, line 6 beginning at "Preferably," through line 10;
- [0015] page 12, lines 1-27;
- [0016] page 12, line 31 through page 22, line 14 ending at "lenses;"
- [0017] page 22, line 28 through page 23, line 33 ending at "viewing,"
- [0018] page 24, line 4 beginning at "an" through page 25, line 4

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

[0019] Not Applicable.

BACKGROUND OF THE INVENTION

[0020] 1. The Field of the Invention

[0021] The present invention relates generally to apparatus for producing a stereoscopic optical image, and more particularly, but not necessarily entirely, to a laparoscope

utilizing three or more selectable optical imaging assemblies to provide a stereoscopic view of the internal regions of the human body in a direction non-parallel to the axis of the laparoscope.

[0022] 2. Description of Related Art

[0023] Modern surgeons seek to perform necessary surgical procedures on a patient while minimizing the disturbance and destruction to intervening tissues and organs. To this end, medical endoscopes have been developed as an aid to diagnostic, surgical and other medical procedures. Medical endoscopes enable visual examination of body channels, cavities, spaces and internal organs through a natural opening or small incision, and thus without conventional surgery.

[0024] Medical endoscopes are also useful for visual observation during surgery. Specific endoscopes have been developed for access to various body lumens and cavities. For example, laparoscopes, bronchoscopes, sigmoidoscopes, gastroscopes, and so forth, are all available. The main difference between these devices is the size of the instrument. However, the general configuration and method of use of such scopes are quite similar. Many of the body cavities and hollow conduits (e.g. peritoneal, abdominal, bronchial, lung, esophagal, etc.) can thus be accessed through endoscopic means, without surgical incisions and the resulting trauma to the patient.

[0025] Endoscopes typically include a long, thin tubular casing optically connected to a viewing mechanism. The tubular casing is narrow enough to insert through a small natural or surgical opening in the body. When the endoscope is inserted and positioned for use, an image of the object being viewed is formed at an inserted end thereof by an objective lens. The image is passed through a series of relay lenses down the cylinder to an eye lens or video camera at a viewing end of the endoscope. A major drawback to using an endoscope as a surgical aid is that it gives a monocular view and therefore no depth perception. Surgical procedures such as suction, irrigation, biopsy, incisions, suturing and cutting must be learned without the benefit of three dimensional visualization.

[0026] Endoscopes have recently been developed that produce the illusion of three dimensions or depth by combining two dimensional images. The stereoscopic effect is created by producing two optical images of the desired region, each image having a different point of view, such as a left image and a right image. It is known to incorporate two separate optical fiber bundles in parallel inside a single casing to add the advantages of fiberoptics to stereoscopic viewing. The two images are carried by the two optical fiber bundles, respectively, to left and right image sensors, which may comprise charge-coupled device (CCD) cameras or other image sensing devices. The sensing devices convert the left and right optical images into left and right video images, respectively. The video images are then presented as alternating left-right images on a viewing monitor to the user to thereby create a stereoscopic or three-dimensional optical view.

[0027] Although endoscopes known in the prior art have succeeded in producing a stereoscopic or three dimensional effect, they are characterized by a number of disadvantages. Many of the devices known in the prior art only provide two non-moveable optical imaging assemblies. Two non-move-

able assemblies do not allow the user to adjust for viewing objects at different distances. If an object is too close, a cross-eye feeling is experienced by the user, and if the object is too far distant, the three dimensional perception diminishes to an irrelevant value.

[0028] In an attempt to provide variable depth perception views, U.S. Pat. No. 6,306,082 (granted Oct. 23, 2001 to Takahashi et al.) discloses an endoscope that allows the user to view multiple selectable images, but this device has limited usefulness for viewing areas with a narrow portal entry space. The design of this device is less effective because the distance between optical image systems cannot be greater than the diameter of the endoscope. Furthermore, the prior art requires a relay system between the objective lens and the image receiving means, which adds to the cost and complexity of the device.

[0029] Other devices known in the art attempt to provide variable depth perception with two optical imaging assemblies that are moveable in relation to the other. These devices requires complex electronic control circuitry to provide movement and synchronization. These devices are expensive to manufacture and complex in operation.

[0030] It is noteworthy that none of the prior art known to applicant provides a stereo laparoscope capable of providing multiple, selectable depth perception views where the distance between the optical assemblies is not limited by the diameter of the endoscopic instrument and where a relay system between the objective lens and the image receiving means is not necessary. There is a long felt need, illustrated by the disadvantageous endoscope devices currently known, for an endoscope that is inexpensive to make, simple in operation and which provides multiple, selectable depth perception views without a relay system of areas where the portal entry space is limited.

[0031] The prior art is thus characterized by several disadvantages that are addressed by the present invention. The present invention minimizes, and in some aspects eliminates, the above-mentioned failures, and other problems, by utilizing the methods and structural features described herein.

[0032] The features and advantages of the invention will be set forth in the description which follows, and in part will be apparent from the description, or may be learned by the practice of the invention without undue experimentation. The features and advantages of the invention may be realized and obtained by means of the instruments and combinations particularly pointed out in the appended claims.

BRIEF DESCRIPTION OF THE DRAWINGS

[0033] The features and advantages of the invention will become apparent from a consideration of the subsequent detailed description presented in connection with the accompanying drawings in which:

[0034] **FIG. 1** is a side, cross sectional view of an embodiment of a stereo laparoscope, made in accordance with the principles of the present invention;

[0035] **FIG. 2** is a top view of the **FIG. 1**.

[0036] **FIG. 3A** is a side, cross sectional view of a further embodiment of a stereo laparoscope, made in accordance with the principles of the present invention.

[0037] **FIG. 3B** is a side, cross sectional view of a further embodiment of a stereo laparoscope, made in accordance with the principles of the present invention.

[0038] **FIG. 4** is schematic drawing of the selection means and focusing means of the embodiment in **FIG. 3A**.

[0039] **FIG. 5** is a schematic drawing of the selection means and focusing means of the embodiment in **FIG. 1**.

[0040] **FIG. 6** is a perspective view of a stereo laparoscope made in accordance with the principles of the present invention.

[0041] **FIG. 7** is a perspective view of another alternative embodiment of the stereo laparoscope of **FIG. 1** with an optical fiber bundle shown in phantom;

DETAILED DESCRIPTION OF THE INVENTION

[0042] For the purposes of promoting an understanding of the principles in accordance with the invention, reference will now be made to the embodiments illustrated in the drawings and specific language will be used to describe the same. It will nevertheless be understood that no limitation of the scope of the invention is thereby intended. Any alterations and further modifications of the inventive features illustrated herein, and any additional applications of the principles of the invention as illustrated herein, which would normally occur to one skilled in the relevant art and having possession of this disclosure, are to be considered within the scope of the invention claimed.

[0043] It must be noted that, as used in this specification and the appended claims, the singular forms "a," "an," and "the" include plural referents unless the context clearly dictates otherwise.

[0044] Referring now to **FIG. 1**, the imaging assemblies, **102, 104, 106, 108, 110** and **112** are disposed in the support body **180** of the laparoscope. The position of the imaging assemblies **102, 104, 106, 108, 110** and **112** with respect to the support body may comprise any suitable disposition; for example, the imaging assemblies may be inside the support body, attached to the support body, connected with the support body, resting on the support body, or supported by the support body of the laparoscope.

[0045] The support body of the laparoscope **180** may comprise any suitable structure, including a rigid or flexible casing, a hollow container, a clear receptacle or any other support body configured for the disposition of imaging assemblies. The support body **180** comprises an elongate body having a sidewall **199** circumscribing an interior space **197** and defining an axial direction **182**.

[0046] Six imaging assemblies are pictured in **FIG. 1**, but the present invention encompasses a plurality of imaging assemblies not limited by the number pictured in this embodiment. The imaging assemblies, **102, 104, 106, 108, 110** and **112**, are aligned in a single-file sequence in a first lateral direction **190** as is best shown in **FIG. 2**, which is a top view of the embodiment of **FIG. 1**. Because the imaging assemblies are aligned in a single-file sequence in a first lateral direction, the distance between the imaging assemblies can be greater than the diameter of the laparoscope. The lenses are also aligned in a single-file sequence in a first lateral direction, so the distance between the lenses can be

greater than the diameter of the laparoscope. The first lateral direction is indicated by an arrow **190**. The lenses are aligned such that an imaginary plane **196** intersects every imaging assembly. This plane runs generally in the longitudinal direction of the support body without varying more than twenty degrees with respect to the longitudinal axis **182** of the support body.

[**0047**] The laparoscope **100** is inserted, such as through a surgical incision, along the axis of insertion, indicated by the arrow **194** in both **FIGS. 1 and 2**. Referring again to **FIG. 1**, as the laparoscope is inserted, a light means **122** is used to illuminate an intracorporeal region **128**. The light means is connected by optical connecting means **214** to the light switch **212**. Light **123** reflected from the intracorporeal region **128** is received through first left opening **130** and first right opening **132**, and is processed by the objective lenses **114** and **116** into left and right optical images, respectively. The left and right optical images are then received at image planes **134** and **136**, respectively, of the image receiving means **138** and **140**, respectively. One feature of the invention is the absence of a relay means between an objective lens of the optical imaging assembly **114** and an image receiving means **138** of the optical imaging assembly. Other laparoscopes known in the art utilize mirrors or other reflective means or image-conveying means to the image from the objective lens to the image receiving means, but this is not necessary in the present invention.

[**0048**] Imaging assemblies **102, 104, 106, 108, 110** and **112** include image planes **134, 136, 162, 164, 200** and **202**, respectively, and objective lenses **114, 116, 158, 160, 204** and **206**, respectively, each objective lens having a focal length. Each objective lens and corresponding image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

[**0049**] wherein

[**0050**] f_1 =the focal length of the objective lenses,

[**0051**] 1_1 =working distance, defined as a distance between the objective lenses and the intracorporeal region, and

[**0052**] 1_2 =image distance, defined as a distance between an objective lens and an image plane.

[**0053**] The image receiving means **138, 140, 166, 168, 200, 210**, which might illustratively comprises CCD camera chips as known in the art, then convey the images to the switches, **418, 420, 422, 424, 426, 428** of the optical selection switch housing **216**, which is connected with the optical connecting structure **218**, which is connected to a camera apparatus **144**, which also may be called the image processor **144**. The camera apparatus **144** is connected to a monitor **146** and glasses **148**. Alternatively, the image receiving means **138, 140, 166, 168, 200, 210** may be replaced with any suitable photo-sensitive image capturing chips such as a single optical fiber bundle which receives both left and right optical images in an alternating manner, with the aid of suitably placed reflective means and optical switching technology, as well as any related optical necessities such as magnification means, as this alternative design is understood by those having ordinary skill in the art.

[**0054**] The means for alternating the left and right optical images may also comprise apparatus such as observation windows with a liquid crystal display (LCD), shutter-type windows designed to alternately block and receive light, or other windows which can be shown to block and receive light at a predetermined rate.

[**0055**] The camera apparatus **144** then passes the images to any suitable displaying means for displaying the images as a stereoscopic image, such as monitor **146** and viewing glasses **148**. The glasses **148** may comprise CrystalEyes™ glasses. The first left and first right openings **132** and **136** preferably comprise windows formed in sidewall **199** of a support body **180** of the laparoscope **100**. As can be seen in **FIG. 6**, the observation windows are aligned single-file, meaning that a second imaginary plane **195** intersects every observation window. This plane runs generally in the longitudinal direction of the support body without varying more than twenty degrees with respect to the longitudinal axis of the support body, which axis may be considered to be co-axial with the longitudinal direction **182**. Accordingly, reference numeral **182** shall refer to both the longitudinal axis of the support body and the longitudinal direction.

[**0056**] “Working distance” is the distance from an objective lens to the intracorporeal region. The phrase “depth perception” as used herein refers to the ratio of the separation distance between the objective lenses and to the working distance.

[**0057**] It is useful if distances of the working distances of the left and right objective lenses is substantially the same. **FIG. 1** shows the first left working distance **125** and the first right working distance **126** as substantially the same. It is also useful if the ratio of the working distance to the separation distance is equal to 5, but it can also be another number. If the value of this ratio is too high, then the three-dimensional appearance of the intracorporeal space is lost. However, if the value of this ratio is too small, then the user experiences a “cross-eyed” view, straining the eyes and sometimes causing headaches. In the first embodiment pictured in **FIG. 1**, the distances between the left and right objective lenses are pre-set; thus, the separation distance between the left imaging assemblies and the right imaging assemblies is a pre-set constant. The user adjusts to see intracorporeal regions of different distances by selecting from among the plurality of imaging assemblies, a left and a right imaging assembly. The user cannot move the imaging assemblies, but can accomplish various separation distances by choosing a separation distance through selection of a left and right imaging assembly.

[**0058**] If the second left and second right assemblies are selected by the selection means (described in detail in **FIG. 4** and **FIG. 5**), the process is similar to that described for the first left and first right imaging assemblies. Light reflected from the intracorporeal region **152** is received through second left opening **154** and second right opening **156** and is processed by the objective lenses **158** and **160** into left and right optical images, respectively. The left and right optical images are then received at image planes **162** and **164**, respectively, of the image receiving means **166** and **168**, respectively. The image receiving means **166** and **168**, which might illustratively comprises CCD camera chips as known in the art, then convey the images to switches, **418, 420, 422, 424, 426, 428** of the optical selection switch

housing 216, which is connected with the optical connecting structure 218, which is connected to a camera apparatus 144. The camera apparatus 144 then passes the images to any suitable displaying means for displaying the images as a stereoscopic image, such as monitor 146 and viewing glasses 148. The glasses 148 may comprise CrystalEyes.TM glasses.

[0059] The glasses 148 are simply two optical valves or shutters that transmit the images one at a time alternately to the left eye and the right eye in tandem at a predetermined rate. The predetermined rate of alternation is preferably controlled by a scan signal from monitor 146, which controls the optical valves in the glasses 148 with conventional video circuitry. This arrangement ensures that the camera, monitor and optical valves operate in tandem and at the same rate. Thus, the left eye sees only images from one of the left imaging assemblies, 102, 106, and 110, of the endoscope and the right eye sees only images from one of the right imaging assemblies 104, 108, and 112, creating a stereoscopic view. The rate of alternation is faster than the flicker-sensing limit of the human eye, resulting in flicker free viewing.

[0060] It is to be understood that each objective lens 114, 116, 158 and 160 has a focal length, as that optical parameter is understood by those having ordinary skill in the relevant art. This focal length can be pre-set as in FIG. 1 or variable, as in the second embodiment of the present invention, shown in FIG. 3A. The objective lenses 114 and 116 can be positioned and arranged such that their optical axes 170 and 172 coincide substantially at the intracorporeal region 128 to thereby define an acute angle as shown in FIG. 1. Objective lenses 158 and 160 can also be positioned and arranged such that their optical axes 174 and 176 coincide substantially at the intracorporeal region 152 to thereby define an acute angle as shown in FIG. 1. Objective lenses 158 and 160 can also be positioned and arranged such that their optical axes 173 and 175 coincide substantially at the intracorporeal region 15 to thereby define an acute angle as shown in FIG. 1.

[0061] The support body 180 comprises an elongate support body having sidewall defining an axial direction 182. At least the first left observation opening 130 and first right observation opening 132 are formed in said sidewall. Observation openings 154, 156, 220 and 222 are also shown in FIG. 1. The first left objective lens 114 defines a first left optical axis 170, and the first right objective lens 116 defines a first right optical axis 172. The first left and first right objective lenses 114 and 116 are disposed to face the first right and first left observation openings 130 and 132, respectively, such that the first right and first left optical axes 170 and 172 extend transversely with respect to the axial direction 182 of the casing 180. It is useful for the optical axes to lie in the same planes, but multiple planes are possible as well.

[0062] The first left image receiving means 138 is disposed in alignment with the first left objective lens 114 and the first right image receiving means 140 is disposed in alignment with the first right objective lens 116.

[0063] Similarly, the second left observation opening 154 and the second right observation opening 156 are formed in said sidewall. The second left objective lens 158 defines a second left optical axis 174, and the second right objective lens 160 defines a second right optical axis 176. The second

left and second right objective lenses, 158 and 160, are disposed to face the second right and second left observation openings 154 and 156, respectively, such that the second right and second left optical axes 174 and 176 extend transversely with respect to the axial direction 182 of the casing 180. The second left image receiving means 166 is disposed in alignment with the second left objective lens 158 and the second right image receiving means 168 is disposed in alignment with the second right objective lens 160.

[0064] The intracorporeal region is lit by one light means 122 or a plurality of lighting means, 121 and 122. A fiberoptic light source comprising an arc lamp connected to light-emitting fibers for introducing light is one example of a light means. The light means 122 may alternatively comprise a halogen lamp or any other light source suitable for introducing light into fiberoptic filaments. When the light switch 212 is actuated, light is introduced into the lighting means 122 which may alternatively comprise fibers which carry the light. The light 123 is thereby projected into the intracorporeal region, or may alternatively be so conveyed in any manner known to those skilled in the art. The light 123 then illuminates an object or region (not shown) external to the laparoscope 100 to thereby cause said external object to reflect light.

[0065] Referring to FIG. 3A, there is shown a second embodiment of the present invention, wherein the focus of the first left assembly 102 is an adjustable focus. Fixed focus optics are suitable for many applications of stereoscopic imaging. However, adjustable focus is a useful feature for many of the demands of surgery and other medical procedures. It will be appreciated by those skilled in the art that if the components of the first and second embodiments are the same size, then the separation distance between the left and third right assembly, 102 and 112, is smaller than the separation distance between the third left 110 and the third right 112 imaging assemblies of the first embodiment in FIG. 1. This result occurs simply because in FIG. 1, four imaging assemblies fit between the third left and the third right imaging assemblies, but in FIG. 3A, only two assemblies fit between the left and third right assembly. The embodiment of FIG. 3A, therefore, can offer settings with a smaller working distance than the embodiment of FIG. 1, if the imaging assembly components for both embodiments are the same size.

[0066] Adjustable focus may be provided for the embodiments of FIG. 3A and FIG. 3B, by designing the focusing objective lens to be moveable using mechanical or electrical remote control as is known in the art. In FIG. 3A the focus is adjusted by the focusing means 304 for moving the objective lens 114 in a substantially transverse direction 300 relative to the axial direction 182 of the casing 180. The focusing means 304 may comprise automated control means for varying the focus of the left optical image responsive to selection of the right imaging assembly. It will be appreciated that the focusing means may be attached to one or more right objective lenses or to one or more left objective lenses or to both right and left objective lenses. FIG. 3B illustrates an embodiment wherein focusing means, 300, 302, 304, 306, 308, 310 are attached to all of the objective lenses 114, 116, 158, 160, 204, 206, respectively.

[0067] Referring to FIG. 4, there is shown the focusing and selection means of the embodiment shown in FIG. 3A

in greater detail. The focusing means **204** of the first left lens **114** of the first left imaging assembly **102** allows movement of the objective lens in along a direction indicated by arrow **300**, so that the focus is adjustable. The focusing means may comprise a stepper motor, Piezo actuator, cervo actuator, or any other type of linear actuator or any other suitable focusing means. The focusing means **304** can be controlled by any suitable motion controller **320**, and is connected to the controller with suitable connecting means **322**.

[0068] Referring to **3B**, the focusing means, **300**, **302**, **304**, **306**, **308**, **310** are controlled by a motion controller **320** and attached to the motion controller **320** with connecting means **322**. The motion controller **320** attaches to the selection switch housing **216** with a suitable connecting means **319**. Referring to **FIG. 4**, the focusing means **304** is controlled by a motion controller **320** and attached to the motion controller **320** with connecting means **322**. The motion controller **320** attaches to selection switches **430**, **432**, and **434** in the selection switch housing **216** with a suitable connecting means.

[0069] The imaging assemblies are selected using suitable selection means. In **FIG. 4**, this selection means comprises circuit means, **410**, **412**, and **414** that run from the image receiving means **210**, **168**, and **140** of imaging assemblies **112**, **108** and **104**, respectively to a selection switches **422**, **420** and **418**. A double pole switch is useful, but the selection switch may comprise any selection switch deemed appropriate by one of ordinary skill in the art. The circuit means, **410**, **412**, and **414** connect to the main selection switch **436**, which is connected by suitable connecting means **438** to the camera apparatus **144**, which is also known as an image processor **144**. The first left image receiving means **138** is connected by suitable connecting means **416** to the camera apparatus **144**.

[0070] **FIG. 5** shows the focusing means and selection means of the embodiment pictured in **FIG. 1**. In **FIG. 5**, the image receiving means **210**, **168** and **140** of imaging assemblies **104**, **108**, and **112** are connected with connecting means **440**, **442**, and **444** to selection switches **428**, **426** and **424** of the selection switch housing **216**. The imaging receiving means **138**, **166** and **208** of imaging assemblies **102**, **106**, and **110** are connected to switches **418**, **420** and **422** by suitable connecting means **442**. These switches are controlled by main switch **436**, which is connected by connecting means **438** to the image processor **144**, which is connected to the monitor **146**.

[0071] Referring to **FIG. 6**, there is shown a perspective view of a stereolaparoscope made in accordance with the principles of the present invention. The stereo laparoscope is generally designated at **100**, and is inserted into the abdominal cavity through a small incision. The stereo laparoscope **100** comprises a hollow, elongate casing designated by bracket **180** having a cylindrical side walls **199**. An illuminating window light **123** from the illuminating means (not shown) is pictured. Observation windows **222**, **154**, **130**, **132**, **156** and **122** are disposed in the side wall **199**, preferably near distal extremity **11**. A side mounted handle grip **17** for gripping by the user provides a natural feel.

[0072] A unique aspect of the present invention can be observed in **FIG. 6**, in that the observation windows **222**, **154**, **130**, **132**, **156** and **122** are disposed in the side wall **199** of the casing **180** instead of in the front-end face **181**. This

window arrangement advantageously allows a user to position the side wall **199** adjacent to a desired intracorporeal viewing region for a transverse view, instead of requiring the front-end face **181** to face the viewing region. The transverse viewing arrangement also allows for a larger separation of distance between the windows, **222**, **154**, **130**, **132**, **156** and **122**, and associated objective lenses, **206**, **160**, **116**, **114**, **158**, and **204** (not shown) while maintaining a smaller diameter of the support body **180**. The window arrangement of the present invention thereby makes it easier for the user to view relatively remote intracorporeal regions, with a minimum of disturbance to surrounding tissue and organs. It will be appreciated from the above that a direction of view of each imaging assembly **102**, **104**, **106**, **108**, **110** and **112** (shown in **FIG. 1**) is non-parallel to longitudinal axis of the support body, which axis may be considered to be co-axial with the longitudinal direction **182**. Accordingly, reference numeral **182** shall refer to both the longitudinal axis of the support body and the longitudinal direction. The longitudinal axis **182** of the laparoscope **100**, and forms an acute angle relative to said axis **195**.

[0073] The embodiment presented in **FIG. 6** illustrates the simplest embodiment, namely, a stereo laparoscope **100** comprising a rigid or semi-rigid straight casing **180** allowing observations from a plurality of imaging assemblies (not shown) through a plurality of observation windows at the right angle. However, the laparoscope may alternatively comprise a rigid or semi-rigid casing **180** bent at a **90** degree angle as shown in **FIG. 7**. At least the portion of the casing between the front-end face **181** and the fiber bundle **40** must be rigid in order to maintain precise positioning of the imaging optics therein. The embodiment of **FIG. 7** allows for a straight forward observation while utilizing the fiberoptic advantage of transmitting an image around curves by using a curved fiber bundle, illustrated in phantom at **40** in **FIG. 7**. It is also within the scope of the present invention to use a flexible casing with a flexible fiber bundle to allow the physician to selectively flex the laparoscope in order to achieve a desired point of view.

[0074] Referring again to **FIG. 6**, The observation windows **222**, **154**, **130**, **132**, **156** and **122** are arranged in a single file sequence in a first lateral direction **190** along the hollow casing **180**, but may alternatively be arranged in some other configuration.

[0075] Instead of using objective lenses (not shown in **FIG. 6**) to process the light into left and right optical images, optical imaging properties may be incorporated into the observation windows, **222**, **154**, **130**, **132**, **156** and **122**. In this configuration, said windows **222**, **154**, **130**, **132**, **156** and **122** would serve the dual purpose of receiving the light reflected from an external object to be viewed, and processing the light received into left and right optical images. The objective lenses have been presented as single element components. However, the scope of the invention includes multi-element objective lenses as are known in the art for improving the image quality and otherwise optimizing the performance of the system.

[0076] It is known in the art to rotate optical images electronically. The optical images produced in accordance with the present invention could be electronically rotated by **180** degrees, thereby allowing insertion of the laparoscope **100** from either side of a region to be viewed.

[0077] In accordance with the disclosure described above, a useful method of producing a stereoscopic optical image of an intracorporeal region comprises the steps of:

[0078] (a) selecting left and right imaging assemblies

[0079] (b) inserting a casement into a body cavity and illuminating the intracorporeal region to thereby cause said region to reflect light;

[0080] (c) processing light reflected from the intracorporeal region into left and right optical images and transmitting said optical images within the casement to an image receiving means disposed within said casement; and

[0081] (d) transmitting said optical images to an output display to thereby produce a stereoscopic optical image of the intracorporeal region on said output display.

[0082] The embodiment of the invention as a surgical instrument is merely illustrative, and does not limit the scope of the present invention. For example, the invention may be applied to extend optical vision to any context or space where it is desired that human contact therewith be avoided, such as in radioactive environments, in space or in deep sea applications. Any suitable size or configuration of the invention may be employed, and the optical imaging assemblies may in some applications be spaced six feet apart, for example.

[0083] It is to be understood that the above-described arrangements are only illustrative of the application of the principles of the present invention. Numerous modifications and alternative arrangements may be devised by those skilled in the art without departing from the spirit and scope of the present invention and the appended claims are intended to cover such modifications and arrangements.

[0084] It is a feature of the present invention to provide a laparoscope device which is simple in design and manufacture. Another feature of the present invention is to provide an improved stereo endoscope for producing a stereoscopic optical image of an intracorporeal region. It is a further feature of the present invention, in accordance with one aspect thereof, to provide a stereoscopic device which provides variable depth perception views by allowing the user to selection images from three or more imaging assemblies. It is a further feature of the present invention, in accordance with one aspect thereof, to provide a stereoscopic device wherein the distance between at least two optical imaging assemblies is greater than the diameter of the device. It is a further feature of the present invention, in accordance with one aspect thereof, to provide a stereoscopic device wherein the axis of view is non-parallel to the elongated axis of the stereoscopic device and wherein a relay means between the objective lens and image receiving means is not necessary.

[0085] It is to be understood that the above-described arrangements are only illustrative of the application of the principles of the present invention. Numerous modifications and alternative arrangements may be devised by those skilled in the art without departing from the spirit and scope of the present invention and the appended claims are intended to cover such modifications and arrangements. Thus, while the present invention has been shown in the

drawings and described above with particularity and detail, it will be apparent to those of ordinary skill in the art that numerous modifications, including, but not limited to, variations in size, materials, shape, form, function and manner of operation, assembly and use may be made without departing from the principles and concepts set forth herein.

What is claimed is:

1. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

a plurality of imaging assemblies configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a left imaging assembly and at least a first right imaging assembly and a second right imaging assembly, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly;

selection and processing means for enabling a user to select a combination of a left imaging assembly and a right imaging assembly from among the plurality of imaging assemblies, and causing left and right images to be processed from said left and right imaging assemblies, respectively, in accordance with a selection made by said user;

wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies; and

means for causing the left and right images to be viewable by an observer.

2. The stereo laparoscope as in claim 1, wherein each right imaging assembly further comprises an objective lens and an image receiving means, wherein the objective lens is disposed in a fixed orientation relative to the image receiving means at a pre-determined distance from said image receiving means to thereby provide a fixed-focus image.

3. The stereo laparoscope as in claim 1, wherein at least one of said imaging assemblies comprises a focus means and wherein the focus means of at least one imaging assembly comprises an adjustable focus means.

4. A stereo laparoscope as in claim 1, wherein said laparoscope comprises a casing containing the imaging assemblies.

5. A stereo laparoscope as in claim 4, wherein said casing comprises two elongate sidewalls.

6. A stereo laparoscope as in claim 4, wherein a plurality of observation windows are disposed in the sidewalls of the casing.

7. A stereo laparoscope as in claim 6, wherein said observation windows are positioned in a single-file sequence in a first lateral direction, such that each observation window

is intersected by an imaginary plane that extends along a field of view of at least one of said observation windows.

8. A stereo laparoscope as in claim 1, wherein said laparoscope comprises light means for illuminating said intracorporeal region.

9. A stereo laparoscope as in claim 8, wherein said laparoscope comprises a plurality of said light means.

10. A stereo laparoscope as in claim 8, wherein said laparoscope comprises an elongate casing comprising two sidewalls and wherein said plurality of light means are disposed in said casing.

11. A stereo laparoscope as in claim 1, wherein the laparoscope comprises selection means for selecting selectable depth perception views and wherein said selectable depth perception views are selectable prior to insertion of the laparoscope.

12. A stereo laparoscope as in claim 1, wherein at least one imaging assembly comprises a lens and an image receiving means.

13. A stereo laparoscope as in claim 12, wherein said image receiving means comprises CCD camera chips.

14. A stereo laparoscope as in claim 12, wherein said image receiving means comprises a single optical fiber bundle disposed within a casing and having a first end, and a second end, and fibers for receiving optical images at the first end.

15. A stereo laparoscope as in claim 12, wherein said imaging assemblies are disposed in a casing and wherein a distance between at least two lenses of the imaging assemblies is greater than a diameter of the casing.

16. A stereo laparoscope as in claim 12, wherein said lenses of the imaging assemblies comprise at least a first left lens and a first right lens, said first left lens having a first left optical axis and said first right lens having a first right optical axis, wherein the lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle.

17. A stereo laparoscope as in claim 16, wherein the image receiving means comprises a first left image receiving means and a first right image receiving means disposed within the casing, said first left and first right image receiving means respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially nonparallel to said first left and first right optical axes.

18. A stereo laparoscope as in claim 1, wherein the laparoscope comprises a casing, and wherein each imaging assembly is intersected by a first imaginary plane that runs generally in the longitudinal direction of the casing without varying more than least twenty degrees from a longitudinal axis of said casing.

19. A stereo laparoscope as in claim 1, wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed.

20. A stereo laparoscope as in claim 19, wherein the desired ratio is equal to 5.

21. A stereo laparoscope as in claim 1, wherein each imaging assembly further comprises an image plane and an

objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

wherein

f_1 =the focal length of the lenses,

1_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

1_2 =image distance, defined as a distance between a lens and an image plane.

22. A stereo laparoscope as in claim 1, wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis.

23. A stereo laparoscope as in claim 1, wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means.

24. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

a plurality of imaging assemblies configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a right imaging assembly and at least a first left imaging assembly and a second left imaging assembly, wherein the first and second left imaging assemblies are each disposed in a fixed orientation relative to the right imaging assembly to thereby maintain a substantially constant separation distance between the right imaging assembly and the left imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the right imaging assembly and the first left imaging assembly, and a pre-set second selectable depth perception view involving the right imaging assembly and the second left imaging assembly;

selection and processing means for enabling a user to select a combination of a left imaging assembly and a right imaging assembly from among the plurality of imaging assemblies, and causing left and right images to be processed from said left and right imaging assemblies, respectively, in accordance with a selection made by said user;

wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies;

means for causing the left and right images to be viewable by an observer.

25. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope comprising:

at least three imaging assemblies that produce images;

wherein each imaging assembly comprises an objective lens;

wherein a distance between at least two of the objective lenses is greater than a diameter of the laparoscope; and

means for causing the images to be viewable by an observer.

26. The stereo laparoscope as in claim 25, wherein each right imaging assembly further comprises an objective lens and an image receiving means, wherein the objective lens is disposed in a fixed orientation relative to the image receiving means at a pre-determined distance from said image receiving means to thereby provide a fixed-focus image.

27. A stereo laparoscope as in claim 25, wherein said laparoscope comprises an elongate casing comprising a sidewall.

28. A stereo laparoscope as in claim 27, wherein a plurality of observation windows are disposed in the sidewall of the casing.

29. A stereo laparoscope as in claim 28, wherein said observation windows are positioned in a single file sequence in a first lateral direction along the casing in an axial direction.

30. A stereo laparoscope as in claim 25, wherein the imaging assemblies are positioned in a single file sequence in a first lateral direction along the casing in an axial direction.

31. A stereo laparoscope as in claim 25, wherein at least one of said imaging assemblies comprises adjustable focusing means.

32. A stereo laparoscope as in claim 25, wherein said imaging assemblies comprise image receiving means.

33. A stereo laparoscope as in claim 32, wherein a distance between at least two of the image receiving means is greater than the diameter of the support body of the laparoscope.

34. A stereo laparoscope as in claim 32, wherein said image receiving means comprises CCD camera chips.

35. A stereo laparoscope as in claim 32, wherein said image receiving means comprises a single optical fiber bundle disposed within a casing and having a first end, and a second end, and fibers for receiving optical images at the first end.

36. A stereo laparoscope as in claim 25, wherein said laparoscope comprises a casing containing the imaging assemblies.

37. A stereo laparoscope as in claim 25, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly.

38. A stereo laparoscope as in claim 37, wherein the laparoscope comprises selection means for selecting selectable depth perception views and wherein said selectable depth perception views are selectable prior to insertion of the laparoscope.

39. A stereo laparoscope as in claim 25, wherein said imaging assemblies are disposed in a casing and wherein a

distance between at least two lenses of the imaging assemblies is greater than a diameter of the casing.

40. A stereo laparoscope as in claim 25, wherein said lenses of the imaging assemblies comprise at least a first left lens and a first right lens, said first left lens having a first left optical axis and said first right lens having a first right optical axis, wherein the lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle.

41. A stereo laparoscope as in claim 40, wherein the image receiving means comprises a first left image receiving means and a first right image receiving means disposed within the casing, said first left and first right image receiving means respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially nonparallel to said first left and first right optical axes.

42. A stereo laparoscope as in claim 25, wherein the laparoscope comprises a casing, and wherein each imaging assembly is intersected by a first imaginary plane that runs generally in the longitudinal direction of the casing without varying more than least twenty degrees from a longitudinal axis of said casing.

43. A stereo laparoscope as in claim 37, wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed.

44. A stereo laparoscope as in claim 43, wherein the desired ratio is equal to 5.

45. A stereo laparoscope as in claim 25, wherein each imaging assembly further comprises an image plane and an objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

wherein

f_1 =the focal length of the lenses,

1_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

1_2 =image distance, defined as a distance between a lens and an image plane.

46. A stereo laparoscope as in claim 25, wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis.

47. A stereo laparoscope as in claim 25, wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means.

48. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and

arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies further comprising a left imaging assembly and at least a first right imaging assembly and a second right imaging assembly;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to said axis; and

means for causing the images to be viewable by an observer.

49. A stereo laparoscope as in claim 48, wherein the plurality of imaging assemblies includes first and second right imaging assemblies that are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly.

50. A stereo laparoscope as in claim 48, wherein said laparoscope comprises a casing comprising a sidewall.

51. A stereo laparoscope as in claim 50, wherein a plurality of observation windows are disposed in the sidewall of the casing.

52. A stereo laparoscope as in claim 51, wherein said observation windows are positioned in a single file sequence along the casing in an axial direction with respect to said casing.

53. A stereo laparoscope as in claim 48, wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies.

54. A stereo laparoscope as in claim 48, wherein at least one of said imaging assemblies comprises an adjustable focusing means.

55. A stereo laparoscope as in claim 48, wherein said imaging assemblies further comprise image receiving means.

56. A stereo laparoscope as in claim 48, wherein each imaging assembly comprises an objective lens, wherein a distance between at least two of the objective lenses is greater than a diameter of the laparoscope.

57. A stereo laparoscope as in claim 55, wherein the image receiving means comprises CCD camera chips.

58. A stereo laparoscope as in claim 55, wherein the image receiving means comprises a single optical fiber bundle disposed within a casing and having a first end, and a second end, and fibers for receiving optical images at the first end.

59. A stereo laparoscope as in claim 48, wherein said laparoscope comprises light means for illuminating said intracorporeal region.

60. A stereo laparoscope as in claim 59, wherein said light means comprises a plurality of light means.

61. A stereo laparoscope as in claim 59, wherein said laparoscope comprises a casing and wherein said plurality of light means are disposed in said casing.

62. A stereo laparoscope as in claim 48, wherein each imaging assembly contains an objective lens and image receiving means, such that a first left imaging assembly contains a first left objective lens and a first right imaging assembly contains a first right objective lens.

63. A stereo laparoscope as in claim 48, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly.

64. A stereo laparoscope as in claim 48, wherein said lenses of the imaging assemblies comprise at least a first left lens and a first right lens, said first left lens having a first left optical axis and said first right lens having a first right optical axis, wherein the lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle.

65. A stereo laparoscope as in claim 64, wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within the casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially nonparallel to said first left and first right optical axes.

66. A stereo laparoscope as in claim 48, wherein the laparoscope comprises a casing, and wherein each imaging assembly is intersected by a first imaginary plane that runs generally in the longitudinal direction of the casing without varying more than least twenty degrees from a longitudinal axis of said casing.

67. A stereo laparoscope as in claim 63, wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed.

68. A stereo laparoscope as in claim 67, wherein the desired ratio is equal to 5.

69. A stereo laparoscope as in claim 48, wherein each imaging assembly further comprises an image plane and an objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/l_1+1/l_2,$$

wherein

f_1 =the focal length of the lenses,

l_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

l_2 =image distance, defined as a distance between a lens and an image plane.

70. A stereo laparoscope as in claim 48, wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis.

71. A stereo laparoscope as in claim 48, wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means.

72. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies disposed on the support body, said imaging assemblies being further comprising a right imaging assembly and at least a first left imaging assembly and a second left imaging assembly;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

73. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies disposed on the support body, said imaging assemblies being further comprising a left imaging assembly and a first right imaging assembly and a second right imaging assembly;

wherein the first and second right imaging assemblies are disposed in a fixed orientation relative to each other to thereby pre-set first and second depth perception views;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

74. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies further comprising a right imaging assembly and a first left imaging assembly and a second right left assembly;

wherein the first and second left imaging assemblies are disposed in a fixed orientation relative to each other to thereby pre-set first and second depth perception views;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

75. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies further comprising a left imaging assembly and a first right imaging assembly and a second right imaging assembly and a third right imaging assembly;

wherein the first and second and third right imaging assemblies are disposed in a fixed orientation relative to each other;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

76. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies disposed on the support body, said imaging assemblies being further comprising a right imaging assembly and a first left imaging assembly and a second right left assembly and a third right left assembly;

wherein the first, second, and third left imaging assemblies are disposed in a fixed orientation relative to each other;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

77. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and

arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies further comprising a first left imaging assembly and a second left imaging assembly and a first right imaging assembly and a second right imaging assembly;

wherein the plurality of imaging assemblies are disposed in a fixed orientation relative to each other;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

78. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images;

said plurality of imaging assemblies further comprising a first left imaging assembly and a second left imaging assembly and a third left imaging assembly and a first right imaging assembly and a second right imaging assembly and a third right imaging assembly;

wherein the plurality of imaging assemblies are disposed in a fixed orientation relative to each other;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope, and forms an acute angle relative to the laparoscope; and

means for causing the images to be viewable by an observer.

79. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

a plurality of imaging assemblies configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a left imaging assembly and at least a first right imaging assembly and a second right imaging assembly, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly;

selection and processing means for enabling the user to select a combination of a right imaging assembly and a left imaging assembly from among the plurality of

imaging assemblies, and causing right and left images to be processed from said right and left imaging assemblies, respectively in accordance with a selection made by said user;

wherein each imaging assembly comprises an objective lens and an image receiving means, said each imaging assembly being characterized by an absence of a relay means between the objective lens and the image receiving means;

means for causing the images to be viewable by an observer.

80. A stereo laparoscope as in claim 79, wherein the laparoscope comprises an elongate casing comprising a sidewall.

81. A stereo laparoscope as in claim 79, wherein a plurality of observation windows are disposed in the sidewall of the casing.

82. A stereo laparoscope as in claim 81, wherein said observation windows are positioned in a single file sequence along the casing in an axial direction with respect to said casing.

83. A stereo laparoscope as in claim 79, wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies.

84. A stereo laparoscope as in claim 79, wherein said laparoscope comprises light means for illuminating said intracorporeal region.

85. A stereo laparoscope as in claim 84, wherein said laparoscope comprises a plurality of said light means.

86. A stereo laparoscope as in claim 85, wherein said laparoscope comprises a casing and wherein said light means is disposed within said casing.

87. A stereo laparoscope as in claim 79, wherein the laparoscope comprises selection means for selecting selectable depth perception views and wherein said selectable depth perception views are selectable prior to insertion of the laparoscope.

88. A stereo laparoscope as in claim 79, wherein at least one imaging assembly comprises an objective lens and an image receiving means.

89. A stereo laparoscope as in claim 88, wherein said image receiving means comprises CCD camera chips.

90. A stereo laparoscope as in claim 88, wherein said image receiving means comprises a single optical fiber bundle disposed within a casing and having a first end, and a second end, and fibers for receiving optical images at the first end.

91. A stereo laparoscope as in claim 88, wherein each imaging assembly comprises an objective lens, wherein a distance between at least two of the objective lenses is greater than a diameter of the laparoscope.

92. A stereo laparoscope as in claim 79, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and

a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly.

93. A stereo laparoscope as in claim 79, wherein said lenses of the imaging assemblies comprise at least a first left lens and a first right lens, said first left lens having a first left optical axis and said first right lens having a first right optical axis, wherein the lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle.

94. A stereo laparoscope as in claim 93, wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within the casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially nonparallel to said first left and first right optical axes.

95. A stereo laparoscope as in claim 79, wherein the laparoscope comprises a casing, and wherein each imaging assembly is intersected by a first imaginary plane that runs generally in the longitudinal direction of the casing without varying more than least twenty degrees from a longitudinal axis of said casing.

96. A stereo laparoscope as in claim 92, wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed.

97. A stereo laparoscope as in claim 96, wherein the desired ratio is equal to 5.

98. A stereo laparoscope as in claim 79, wherein each imaging assembly further comprises an image plane and an objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

wherein

f_1 =the focal length of the lenses,

1_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

1_2 =image distance, defined as a distance between a lens and an image plane.

99. A stereo laparoscope as in claim 79, wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis.

100. A stereo laparoscope as in claim 79, wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means.

101. A stereo laparoscope as in claim 79, wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within the casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in

alignment with the first left and first right optical axes, and are substantially non-parallel to said first left and first right optical axes.

102. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

a plurality of imaging assemblies configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a right imaging assembly and at least a first left imaging assembly and a second left imaging assembly, wherein the first and second left imaging assemblies are each disposed in a fixed orientation relative to the right imaging assembly to thereby maintain a substantially constant separation distance between the right imaging assembly and the left imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the right imaging assembly and the first left imaging assembly, and a pre-set second selectable depth perception view involving the right imaging assembly and the second left imaging assembly;

selection and processing means for enabling the user to select a combination of a right imaging assembly and a left imaging assembly from among the plurality of imaging assemblies, and causing right and left images to be processed from said right and left imaging assemblies, respectively in accordance with a selection made by said user;

wherein each imaging assembly comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means;

means for causing the images to be viewable by an observer.

103. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images,

said plurality of imaging assemblies further comprising a left imaging assembly and at least a first right imaging assembly and a second right imaging assembly,

wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies; and

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope; and

means for causing the images to be viewable by an observer.

104. A stereo laparoscope as in claim 103, wherein the first and second right imaging assemblies are each disposed

in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly.

105. A stereo laparoscope as in claim 104, further comprising selection and processing means for enabling a user to select a combination of a left imaging assembly and a right imaging assembly from among the plurality of imaging assemblies, and causing left and right images to be processed from said left and right imaging assemblies, respectively, in accordance with a selection made by said user.

106. The stereo laparoscope as in claim 103, wherein each right imaging assembly further comprises an objective lens and an image receiving means, wherein the objective lens is disposed in a fixed orientation relative to the image receiving means at a pre-determined distance from said image receiving means to thereby provide a fixed-focus image.

107. The stereo laparoscope as in claim 103, wherein each right imaging assembly further comprises an objective lens and an image receiving means, wherein the objective lens is disposed in a fixed orientation relative to the image receiving means at a pre-determined distance from said image receiving means to thereby provide a fixed-focus image.

108. The stereo laparoscope as in claim 103, wherein at least one of said imaging assemblies comprises a focus means and wherein the focus means of at least one imaging assembly comprises an adjustable focus means.

109. A stereo laparoscope as in claim 103, wherein said laparoscope comprises a casing containing the imaging assemblies.

110. A stereo laparoscope as in claim 109, wherein said casing comprises two elongate sidewalls.

111. A stereo laparoscope as in claim 109, wherein a plurality of observation windows are disposed in the sidewalls of the casing.

112. A stereo laparoscope as in claim 111, wherein said observation windows are positioned in a single-file sequence in a first lateral direction, such that each observation window is intersected by an imaginary plane that extends along a field of view of at least one of said observation windows.

113. A stereo laparoscope as in claim 103, wherein said laparoscope comprises light means for illuminating said intracorporeal region.

114. A stereo laparoscope as in claim 113, wherein said laparoscope comprises a plurality of said light means.

115. A stereo laparoscope as in claim 113, wherein said laparoscope comprises an elongate casing comprising two sidewalls and wherein said plurality of light means are disposed in said casing.

116. A stereo laparoscope as in claim 103, wherein the laparoscope comprises selection means for selecting selectable depth perception views and wherein said selectable depth perception views are selectable prior to insertion of the laparoscope.

117. A stereo laparoscope as in claim 103, wherein at least one imaging assembly comprises a lens and an image receiving means.

118. A stereo laparoscope as in claim 117, wherein said image receiving means comprises CCD camera chips.

119. A stereo laparoscope as in claim 117, wherein said image receiving means comprises a single optical fiber bundle disposed within a casing and having a first end, and a second end, and fibers for receiving optical images at the first end.

120. A stereo laparoscope as in claim 117, wherein said imaging assemblies are disposed in a casing and wherein a distance between at least two lenses of the imaging assemblies is greater than a diameter of the casing.

121. A stereo laparoscope as in claim 117, wherein said lenses of the imaging assemblies comprise at least a first left lens and a first right lens, said first left lens having a first left optical axis and said first right lens having a first right optical axis, wherein the lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle.

122. A stereo laparoscope as in claim 121, wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within the casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially nonparallel to said first left and first right optical axes.

123. A stereo laparoscope as in claim 103, wherein the laparoscope comprises a casing, and wherein each imaging assembly is intersected by a first imaginary plane that runs generally in the longitudinal direction of the casing without varying more than least twenty degrees from a longitudinal axis of said casing.

124. A stereo laparoscope as in claim 103, wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed.

125. A stereo laparoscope as in claim 124, wherein the desired ratio is equal to 5.

126. A stereo laparoscope as in claim 103, wherein each imaging assembly further comprises an image plane and an objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

wherein

f_1 =the focal length of the lenses,

1_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

1_2 =image distance, defined as a distance between a lens and an image plane.

127. A stereo laparoscope as in claim 103, wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis.

128. A stereo laparoscope as in claim 103, wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being

characterized by an absence of a relay means between the objective lens and the image receiving means.

129. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a right imaging assembly and at least a first left imaging assembly and a second left imaging assembly, wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies;

wherein a direction of view of each imaging assembly is non-parallel to the axis of the laparoscope; and

means for causing the images to be viewable by an observer.

130. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images, said plurality of imaging assemblies further comprising a left imaging assembly and at least a first right imaging assembly and a second right imaging assembly, wherein the first and second right imaging assemblies are each disposed in a fixed orientation relative to the left imaging assembly to thereby maintain a substantially constant separation distance between the left imaging assembly and the right imaging assemblies, respectively, to thereby accomplish a pre-set first selectable depth perception view involving the left imaging assembly and the first right imaging assembly, and a pre-set second selectable depth perception view involving the left imaging assembly and the second right imaging assembly;

selection and processing means for enabling a user to select a combination of a left imaging assembly and a right imaging assembly from among the plurality of imaging assemblies, and causing left and right images to be processed from said left and right imaging assemblies, respectively, in accordance with a selection made by said user;

wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies;

wherein a direction of view of each imaging assembly is non-parallel to a longitudinal axis of the laparoscope;

wherein each imaging assembly further comprises an objective lens and an image receiving means, said each

image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means;

wherein the assemblies are contained in a casing;

wherein the laparoscope further comprises one or more observation windows disposed on casing;

wherein the laparoscope comprises light means for illuminating said intracorporeal region;

wherein said image receiving means comprises a CCD camera chip;

wherein the imaging assemblies comprise at least a first left objective lens and a first right objective lens, said first left objective lens having a first left optical axis and said first right objective lens having a first right optical axis, wherein the objective lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle;

wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within said casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially non-parallel to said first left and first right optical axes;

wherein said laparoscope comprises a direction of insertion and wherein the direction of view of said imaging assembly is non-parallel to the direction of insertion of said laparoscope; and

means for causing the left and right images to be viewable by an observer;

wherein each selectable combination of a left imaging means and a right imaging means comprises a separation distance between objective lenses of said left imaging means and right imaging means that is fixed in accordance with a desired ratio of working distance to separation distance, wherein the phrase "working distance" means a distance between an objective lens and the intracorporeal region to be viewed, the desired ratio being equal to 5;

wherein each imaging assembly further comprises an image plane and an objective lens having a focal length, wherein the lens and the image plane are configured and positioned in accordance with a desired working distance, to thereby maintain a mathematical relationship as follows:

$$1/f_1=1/1_1+1/1_2,$$

wherein

f_1 =the focal length of the lenses,

1_1 =working distance, defined as a distance between the lenses and the intracorporeal region, and

1_2 =image distance, defined as a distance between a lens and an image plane.

wherein a direction of view of each imaging assembly is non-parallel to an axis of the laparoscope, and forms an acute angle relative to said axis;

wherein each imaging assembly further comprises an objective lens and an image receiving means, said each image assembly being characterized by an absence of a relay means between the objective lens and the image receiving means.

131. A stereo laparoscope for producing a stereoscopic optical image of an intracorporeal region external to the laparoscope, said laparoscope comprising:

an elongate support body having an elongate axis;

a plurality of imaging assemblies disposed on the support body, said imaging assemblies being configured and arranged for receiving light reflected from an intracorporeal region and processing said light into images,

said plurality of imaging assemblies further comprising a right imaging assembly and at least a first left imaging assembly and a second left imaging assembly,

wherein the first and second right imaging assemblies are disposed in a fixed orientation relative to each other to thereby pre-set first and second selectable depth perception views, respectively, when used in conjunction with the right imaging assembly;

selection and processing means for enabling a user to select a combination of a left imaging assembly and a right imaging assembly from among the plurality of imaging assemblies, and causing left and right images to be processed from said left and right imaging assemblies, respectively, in accordance with a selection made by said user;

wherein the imaging assemblies are aligned in a single-file sequence in a first lateral direction, such that each imaging assembly is intersected by a first imaginary plane that extends along a field of view of at least one of said imaging assemblies;

wherein a direction of view of said imaging assembly is non-parallel to the axis of the laparoscope;

wherein each imaging assembly comprises an objective lens and an image receiving means; said each imaging

assembly being characterized by an absence of a relay means between the objective lens and the image receiving means;

wherein the assemblies are contained in a casing;

wherein one or more observation windows comprise said casing;

wherein the laparoscope comprises light means for illuminating said intracorporeal region;

wherein each said imaging assembly comprises an objective lens and an image receiving means;

wherein said image receiving means comprises a CCD camera chip;

wherein said objective lenses of the imaging assemblies comprise at least a first left objective lens and a first right objective lens, said first left objective lens having a first left optical axis and said first right objective lens having a first right optical axis, wherein the objective lenses are positioned and arranged such that the first left and first right optical axes coincide substantially at the intracorporeal region to thereby define an acute angle;

wherein the image receiving means comprises a first left image receiver and a first right image receiver disposed within said casing, said first left and first right image receivers respectively defining first left and first right image planes that reside in alignment with the first left and first right optical axes, and are substantially non-parallel to said first left and first right optical axes;

wherein said laparoscope comprises a direction of insertion and wherein the direction of view of said imaging assembly is non-parallel to the direction of insertion of said laparoscope; and

means for causing the left and right images to be viewable by an observer.

* * * * *

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摘要(译)

一种立体腹腔镜，用于产生通过小切口观察的体内区域的立体光学图像。立体腹腔镜包括沿与腹腔镜的轴线不平行的方向设置的多个成像组件。成像组件相对于固定方向设置。包括选择和处理装置，以使用户能够从三个或更多个成像组件中选择左成像组件和右成像组件。左视图和右视图提供三维或立体观察，并且至少两个组件之间的距离可以大于腹腔镜的直径。

