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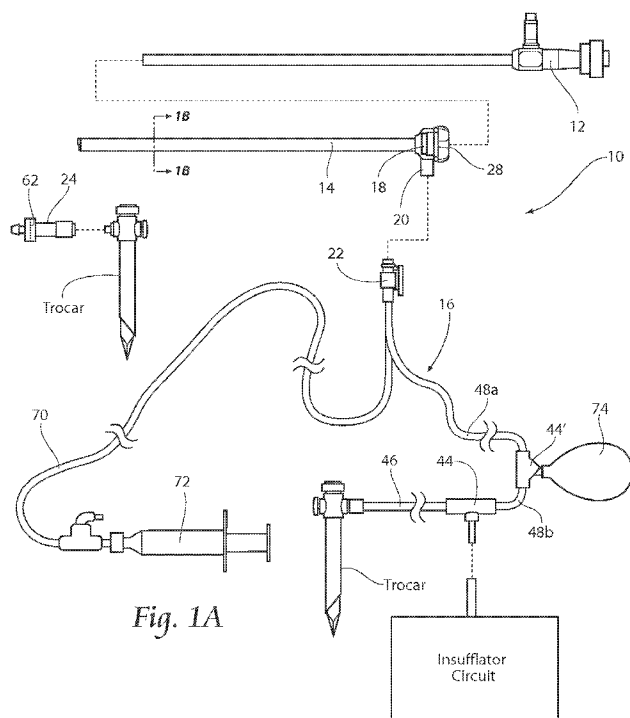
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(54) Title: SYSTEMS AND METHODS FOR OPTIMIZING AND MAINTAINING VISUALIZATION OF A SURGICAL FIELD DURING THE USE OF SURGICAL SCOPES



(57) Abstract: A view optimizing assembly, method and kit for use in combination with a laparoscope having a lens located on the shaft tip of the laparoscope, and a source of insufflation CO₂. The invention includes a multi-lumen sheath assembly, a deflector assembly in fluid communication with the lumens of the sheath assembly, wherein the flow of CO₂ through the lumens forms a vortex when coming into contact with the deflector assembly, thereby preventing fogging of the laparoscope lens.



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- 1 -

**SYSTEMS AND METHODS FOR OPTIMIZING AND MAINTAINING
VISUALIZATION OF A SURGICAL FIELD DURING
THE USE OF SURGICAL SCOPES**

Related Application

5 This application claims priority to United States
Provisional Patent Application Serial No. 61/400,900,
filed August 4, 2010, entitled "Systems and Methods for
Optimizing and Maintaining Visualization of a Surgical
Field During the Use of Surgical Scopes." and United
10 States Provisional Patent Application Serial No.
61/452,982, filed March 15, 2011, entitled "Systems and
Methods for Optimizing and Maintaining Visualization of a
Surgical Field During the Use of Surgical Scopes." This
application is also a continuation-in-part of co-pending
15 United States Patent Application Serial No. 12/653,148,
filed December 9, 2009, entitled "Systems and Methods for
Optimizing and Maintaining Visualization of a Surgical
Field During the Use of Surgical Scopes," which claims
the benefit of U.S. Provisional Patent Application Serial
20 No. 61/121,514 filed 10 December 2008, and entitled
"Device for Maintaining Visualization with Surgical
Scopes," which is incorporated herein by reference, and
which also claims the benefit of U.S. Provisional Patent
Application Serial No. 61/170,864 filed 20 April 2009,
25 and entitled "Surgical Scope Stabilizer for Use with

- 2 -

Device for Maintaining Visualization with Surgical
Scopes" which is also incorporated herein by reference,
and which is also a continuation-in-part of U.S. Utility
Application Serial No. 11/765,340, filed 19 June 2007,
5 which corresponds to PCT Application Serial No.
PCT/US2008/067426, filed 19 June 2008, the entirety of
which applications are incorporated herein by reference.

Field of the Invention

The invention generally relates to surgical scopes,
10 and, more particularly, for optimizing and maintaining
visualization of a surgical field when using a surgical
scope, such as, e.g., a laparoscope.

Background of the Invention

Minimally invasive surgical procedures utilizing
15 surgical scopes are desirable because they often provide
one or more of the following advantages: reduced blood
loss; reduced post-operative patient discomfort;
shortened recovery and hospitalization time; smaller
incisions; and reduced exposure of internal organs to
20 possible contaminants.

Generally, minimally invasive surgeries utilize
scopes, such as laparoscopes, that permit remote
visualization of a surgical site within a patient's body
while the surgical procedure is being performed. During a
25 laparoscopic procedure, the patient's abdominal or pelvic
cavity is accessed through two or more relatively small
incisions rather than through a single large incision
that is typical in a conventional surgery. Surgical
scopes, such as laparoscopes, usually consist in part of
30 a rigid or relatively rigid rod or shaft having an
objective lens at one end and an eyepiece and/or
integrated visual display at the other. The scope may
also be connected to a remote visual display device or a
video camera to record surgical procedures.

35 In laparoscopic surgeries, the abdomen is typically

- 3 -

inflated with a gas through the use of an insufflator, to distend the abdominal space by elevating the abdominal wall above the internal organs and thereby create a sufficient working and viewing space for the surgeon.

5 Carbon dioxide is usually used for insufflation, though other suitable gases may also be used. Conventional insufflators are adapted to cycle on and off to maintain a preset and suitable pressure within the patient's body cavity.

10 The local environment within a patient's abdominal space is generally rather warm and humid, and the use of devices such as harmonic scalpels and other cutting and coagulating devices generate mist, smoke, and other debris that is released into the surgical field and often
15 becomes suspended throughout the expanded abdominal space. Additionally, blood, bodily fluids, pieces of tissue, fat or other bodily material may come in contact with or even attach to the lens. As a result of these conditions, visualization through the scope can be
20 significantly diminished. Typically, the only solution to fogging and debris collection on the lens is removal of the scope from the body cavity and defogging or cleaning the lens by wiping it with a cloth, warming the scope tip, or utilizing another defogging method. The need to
25 remove the scope to defog and remove debris from the lens is inconvenient for the scope operator and the surgeon and can interrupt and undesirably prolong surgical procedures.

Summary of the Invention

30 One aspect of the invention provides a view optimizing assembly having a deflector assembly that makes possible intra-operative defogging, surgical debris deflection, and cleaning of a laparoscope lens during minimally invasive surgery, while also maintaining
35 visualization of the surgical site. In use, the view

- 4 -

optimizing assembly makes possible the practice of a surgical method for maintaining clear visualization of the surgical site without removing the laparoscope 12 from the abdominal cavity for the purpose of cleaning or
5 de-fogging its lens.

Brief Description of the Drawings

Fig. 1A is a somewhat schematic, exploded view of a view optimizing assembly for use with a laparoscope having a 0° shaft tip.

10 Fig. 1B is a section view of the sheath, showing internal fluid flow lumens, taken generally along line 1B-1B in Fig. 1A.

Fig. 2A is a somewhat schematic, exploded view of a view optimizing assembly for use with a laparoscope
15 having an angled shaft tip.

Fig. 2B is a section view of the sheath, showing internal fluid flow lumens, taken generally along line 2B -- 2B in Fig. 2A.

Fig. 3A is perspective view of a T-connector for
20 connecting a squeeze pump to the tubing set of the present invention, with squeeze pump capable of providing a burst of CO₂ to the system.

Fig. 3B is a cross-sectional view of the connector of Fig. 3A taken along line 3B -- 3B of Fig. 3A, showing
25 the normal flow of CO₂ from an insufflator through the T-connector.

Fig. 3C is cross-sectional view of the connector of Fig. 3A, taken along line 3C - 3C of Fig. 3A, showing the squeeze pump being activated and providing a burst of CO₂
30 to the system.

Fig. 4A is a perspective view of a pressure valve used in connection with a sterile fluid source used with the present invention.

Fig. 4B is a cross-sectional view of the pressure
35 valve of Fig. 4A taken along the line 4B -- 4B of Fig.

- 5 -

4A, with the pressure valve being shown in a normal operating position.

Fig. 4C is a cross-sectional view of the pressure valve of Fig. 4A taken along line 4C -- 4C of Fig. 4A, showing sterile fluid being introduced into the tubing set of the present invention.

Fig. 5 is a somewhat schematic view of the optimizing assembly, demonstrating normal operation of the assembly with the delivery of CO₂ to the assembly.

Fig. 6 is a perspective view of the lens of a laparoscope during normal operation procedure, with the lens having surgical debris on the lens.

Fig. 7 is a somewhat schematic view of the optimizing assembly, demonstrating the delivery of a cleaning fluid to the assembly.

Fig. 8 is a perspective view of the lens of Fig. 6, with the cleaning fluid removing the surgical debris from the lens.

Fig. 9 is a perspective view of the lens of Fig. 8, demonstrating the formation of bubbles being formed on the lens during use of the optimizing assembly.

Fig. 10 is a somewhat schematic view of the optimizing assembly, demonstrating the delivery of a burst of CO₂.

Fig. 11 is another somewhat schematic view of the optimizing assembly demonstrating the delivery of a burst of CO₂.

Fig. 12 is a perspective view of the lens of Fig. 9, showing the removal of bubbles from the lens after the application of a burst of CO₂.

Fig. 13 is a somewhat schematic view of the optimizing assembly demonstrating the removal of bubbles from the optimizing assembly.

Fig. 14 shows a cleared laparoscope lens after a

- 6 -

burst of air has been sent to the laparoscope lens.

Fig. 15A is an enlarged perspective view of a manifold that the view optimizing assembly shown in Fig. 1A or Fig. 2A incorporates, including a quick exchange coupling, and a quick exchange coupler that the tubing set shown in Fig. 1A or Fig. 2A incorporates, the coupling and the coupler being disconnected.

Fig. 15B is a sectional view taken generally along line 15B -- 15B in Fig. 15A, showing a one way check valve that is normally closed.

Fig. 16A is an enlarged perspective view of the manifold including a quick exchange coupling and the quick exchange coupler of the tubing set, as shown in Fig. 15A, but now connected.

Fig. 16B is a sectional view taken generally along line 16B--16B in Fig. 16A, showing the one way check valve that is opened by the connection of the quick exchange coupling and connectors.

Figs. 17 and 18 are different perspective views of the manifold showing how passages in the manifold communicate with a manifold junction within the manifold.

Fig. 19 is a perspective view of the manifold, showing in exploded view the keyed fitting of the sheath within the manifold junction.

Fig. 20 is a section view of the sheath taken generally alone line 20--20 in Fig. 19, showing the orientation of the lumens of the sheath provided by the keyed fitting of the sheath to the manifold junction.

Fig. 21A is a side section view of the manifold showing details of the locking collar.

Fig. 21B is a side section view of an alternative arrangement of the manifold employing an alternative locking collar.

Figs. 22A and 22B are views of the locking collar when unlocked (Fig. 22A) and locked (Fig. 22B).

- 7 -

Figs. 22C and 22D are views of an alternative embodiment of the locking collar comprising a collet mechanism when opened (Fig. 22C) and closed (Fig. 22D),

Fig. 23 is an enlarged, exploded view of the
5 deflector assembly for use with a laparoscope having a 0° shaft tip.

Fig. 24 is a perspective view of the deflector assembly shown in Fig. 16 when viewed from the inside of the sheath.

10 Fig. 25A is a perspective, diagrammatic view of the deflector assembly shown in Fig. 23, assembled to the sheath, depicting a rolling vortex that is created by the deflector assembly that extends across and beyond the laparoscopic lens.

15 Fig. 25B is a photograph showing the effects of the rolling vortex depicted in Fig. 25A in creating a clear zone across and beyond the laparoscopic lens.

Fig. 26 is an enlarged, exploded view of the deflector assembly for use with a laparoscope having an
20 angled shaft tip.

Fig. 27 is a perspective view of the deflector assembly shown in Fig. 26 when viewed from the inside of the sheath.

25 Fig. 28A is a perspective, diagrammatic view of the deflector assembly shown in Fig. 26, assembled to the sheath, depicting a rolling vortex that is created by the deflector assembly that extends across and beyond the laparoscopic lens.

30 Fig. 28B is a photograph showing the effects of the rolling vortex depicted in Fig. 28A in creating a clear zone across and beyond the laparoscopic lens.

Fig. 29 is a schematic view of the critical physical, pneumatic, and optical characteristics of the deflector assembly shown in Fig. 23.

35 Fig. 30 is an enlarged, exploded view of another

- 8 -

embodiment of a deflector assembly for use with a laparoscope having a 0° shaft tip.

Fig. 31 is a perspective view of the deflector assembly shown in Fig. 30 when viewed from the inside of the sheath.

Fig. 32 is a perspective, diagrammatic view of the deflector assembly shown in Fig. 30, assembled to the sheath, depicting a rolling vortex or a pattern of rolling vortices that can be created by the deflector assembly and that extend across and beyond the laparoscopic lens, creating a clear zone across and beyond the laparoscopic lens.

Fig. 33 is an enlarged, exploded view of another embodiment of a deflector assembly for use with a laparoscope having an angled shaft tip.

Fig. 34 is a perspective view of the deflector assembly shown in Fig. 33 when viewed from the inside of the sheath.

Fig. 35 is a perspective, diagrammatic view of the deflector assembly shown in Fig. 33, assembled to the sheath, depicting a rolling vortex or a pattern of rolling vortices that can be created by the deflector assembly and that extend across and beyond the laparoscopic lens, creating a clear zone across and beyond the laparoscopic lens.

Fig. 36A is a proximal end view looking distally of the sheath like that shown in Fig. 19, sized and configured for use with a conventional 5 mm laparoscope, including dimensions and identifying Lumens 1, 2, 3, and 4 as points of future reference.

Fig. 36B is a perspective side view of the proximal end of the sheath shown in Fig. 36A, trimmed to form a plenum.

Fig. 36C is a perspective side view of the proximal end of the sheath shown in Fig. 36B, showing the

- 9 -

direction and deflection of pressurized CO₂ introduced in the plenum, for entry into the Lumens 1, 2, 3, and 4.

Fig. 37A is a proximal end view looking distally of the sheath like that shown in Fig. 36A, but sized and configured for use with a conventional 10 mm laparoscope, including dimensions and identifying Lumens 1, 2, 3, and 4 as points of future reference.

Fig. 37B is a perspective side view of the proximal end of the sheath shown in Fig. 37A, trimmed to form a plenum that corresponds with Device 1 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 38A is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 2 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 38B is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 3 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 38C is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 4 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 38D is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 5 in Table 1 of Example 2, and annotated to show the relative air

- 10 -

speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 39 is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 6 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 40A is a perspective side view of the proximal end of an alternative embodiment of a sheath, trimmed to form a plenum that corresponds with Device 7 in Table 1 of Example 2, and annotated to show the relative air speeds of pressurized CO₂ that is directed and deflected within the plenum into the Lumens 1, 2, 3, and 4.

Fig. 40B is a perspective side view of the proximal end of the sheath shown in Fig. 33A, showing the direction and deflection of pressurized CO₂ introduced in the plenum, for entry into the Lumens 1, 2, 3, and 4.

Description of the Preferred Embodiments

Although the disclosure hereof is detailed and exact to enable those skilled in the art to practice the invention, the physical embodiments herein disclosed merely exemplify the invention, which may be embodied in other specific structure. While the preferred embodiment has been described, the details may be changed without departing from the invention, which is defined by the claims.

I. View Optimizing Assembly

A. Overview

Figs. 1A/1B and Fig. 2A/2B show embodiments of a view optimizing assembly 10 for use in association with a state of the art laparoscope 12. In Figs. 1A/1B, the laparoscope 12 possesses at 0° (blunt) shaft tip. In Figs. 2A/2B, the laparoscope possess an angle shaft tip (e.g., a 30° shaft tip or 45° shaft tip). The components of

- 11 -

the view optimizing assembly 10 may be made from plastic materials (extruded and/or molded), but other suitable materials, such as metal or a composite material, or combinations thereof could be used.

5 As will be described in greater detail, the view optimizing assembly 10 facilitates intra-operative defogging, surgical debris deflection, and cleaning of a laparoscope lens during minimally invasive surgery, while also maintaining visualization of the surgical site. The
10 view optimizing assembly 10 is intended to be a single-use, disposable laparoscopic accessory. The view optimizing assembly 10 is desirably a sterile accessory for immediate set up and use on a sterile operating field.

15 As shown in Figs. 1A and 2A, the view optimizing assembly 10 comprises a multi-lumen sheath assembly 14, which mounts over the shaft of the laparoscope 12. In the illustrated embodiment, there are five lumens 34; 36; 38; 40; and 42 in the sheath 14, as shown in section views
20 Figs. 1B and 2B. The end of the sheath 14 is sized and configured to match the size and configuration of the corresponding laparoscope 12, having a blunt tip in Fig. 1A and an angled tip in Fig. 2A.

 The assembly 10 includes a tubing set 16 to connect
25 the sheath 14 to an existing carbon dioxide (CO₂) insufflation circuit and to a source of a flushing liquid 72. Further details of the flushing liquid will be described later. A manifold 18 on the proximal end of the sheath 14 includes a quick exchange coupling 20 that
30 mates with a quick exchange coupler 22 on the tubing set 16, to quickly couple the tubing set 16 in fluid communication with the interior lumens 34; 36; 38; 40; and 42 of the sheath 14. Further details of the quick exchange coupling 20 and the quick exchange coupler 22
35 are shown in Figs. 3A/38 and 4A/4B, and will be described

- 12 -

later.

In use, the view optimizing assembly 10 makes possible the practice of a surgical method for maintaining clear visualization of the surgical site without removing the laparoscope 12 from the abdominal cavity for the purpose of cleaning or de-fogging its lens. Furthermore, the view optimizing assembly 10 also makes possible a surgical method for maintaining clear visualization that includes the ability to make a quick exchange of laparoscopes having different operating characteristics (e.g., laparoscopes with different tip angles, lengths, or diameters) entirely on the sterile operating field and without interference with the preexisting surgical set-up on the sterile operating field. The view optimizing assembly 10 integrates with the existing suite of minimally invasive instrumentation. It does not interfere with the surgical set-up, and it requires minimal change in the process or practice of a surgical operating room (OR) team.

The view optimization assembly 10 desirably comes packaged for use in sterile peel away pouches. The pouches contain the components of the view optimization assembly 10 as shown in Figs. 1A and 2A, including the sheath 14, the manifold 18 that is assembled to the sheath 14 and that includes a quick exchange coupling 20; the tubing set 16 which includes a quick exchange coupler 22 that mates with the quick exchange coupling 20 on the manifold 18; and (optionally) a vent device 24. The vent device 24 (see Figs. 1A and 2A) comprises a tube with an inline membrane 62 that restricts air flow through the tube. A proximal end of the tube is sized and configured to couple to a stopcock valve of a conventional trocar. In use, the vent device 24 provides a controlled leak of CO₂ from the operating cavity.

B. The Sheath

- 13 -

As shown in Figs. 1A and 2A, the sheath 14 is sized and configured to receive a laparoscope 12 having a prescribed tip angle, length, and diameter. The distal end of the sheath 14 includes a stop 26 (best shown in Figs. 12 and 15). The stop 26 prevents advancement of the laparoscope 12 beyond the distal end of the sheath 14. The stop 26 assures that the lens at the distal end of the laparoscope 12 rests in a desired, generally coterminous alignment with the distal end of the sheath 14.

The sheath 14 also includes a locking collar 28 at its proximal end, to frictionally engage the laparoscope 12 and resist axial withdrawal of the laparoscope 12 from the sheath 14. Further details of the locking collar 28 are shown in Figs. 14 and 15A/15B and will be described later.

In use, it is expected that the laparoscope 12 will be inserted into the sheath 14 by a scrub nurse during set-up for the operation. The assembled laparoscopic and sheath 14 will then be handed as a unit to personnel at the operating room (OR) table at the desired time. The laparoscope 12 is then connected in a conventional way by personnel at the OR table in conventional fashion to a light cable (which directs light to illuminate the operative field) and the camera cable (which takes the image from the scope and displays it on monitors in the OR). The sheath 14 is sized and configured not to interfere with this normal set-up of the laparoscope 12.

In use, the assembled laparoscopic and sheath 14 are placed as a unit through a trocar into the body cavity (e.g., the abdominal cavity), for viewing the surgical procedure as it is performed.

C. The Manifold

The manifold 18 at the proximal end of the sheath 14 communicates with the multiple lumens 34; 36; 38; 40; and

- 14 -

42 formed within the wall of the sheath 14. As shown in Figs. 3A and 3B, the manifold 18 includes the quick exchange coupling 20 with inlet passages 30 and 32 opening into a manifold junction 104. Fig. 5 shows inlet passage 30 opening into the manifold junction 104. Fig. 6 shows inlet passage 32 opening into the manifold junction 104 generally across from the inlet passage 30. In use, the inlet passage 30 is intended to convey a sterile flushing liquid to the manifold junction 104. In use, the inlet passage 32 is intended to convey pressurized CO₂ to the manifold junction 104.

As Figs. 5 and 7 show, the manifold junction 104 and the proximal end of the sheath 14 are keyed to fit the proximal end of the sheath 14 in a prescribed rotational orientation within the manifold junction 104. Manifold key K1 in Fig. 5 receives sheath key K2 in Fig. 7. The proximal ends of the lumens 34; 36; 38; 40; and 42 are configured to register with the inlet passages 30 and 32 in a specific way when the proximal end of the sheath 14 is key-fitted in the manifold junction 104 in the prescribed rotational orientation. The specific registration couples the inlet passage 30 in flow communication only with the interior lumen 38 of the sheath, and thereby dedicates the interior lumen 38 to the conveyance of sterile flushing liquid to the distal end of the sheath 14 (see Fig. 8). The specific registration couples the inlet passage 32 in concurrent flow communication with all the remaining interior lumens 34; 36; 40; and 42, and thereby dedicates the interior lumens 34; 36; 40; and 42 to the conveyance of pressurized CO₂ to the distal end of the sheath (see Fig. 8).

D. The Tubing Set

As previously described, the tubing set 16 includes a quick exchange coupler 22 that mates with the quick

- 15 -

exchange coupling 20 on the manifold 18 (see Figs. 8A/8B and 9A/9B). The tubing set 16 includes lengths of flexible medical grade tubing with individual end couplers (best shown in Figs. 1A and 2A) that connect to
5 an existing CO₂ insufflation circuit and, if desired, a source 72 of sterile flushing liquid (e.g. a saline or sterile water, preferably with a "surface active agent") on the sterile operating field (e.g., a bag or a syringe). The tubing set 16 includes a T-connector 44 for
10 coupling the insufflation CO₂ circuit directly to the trocar. A first branch of tubing 46 (see Fig. 2A) may be used to connect the T-connector 44 to the trocar. The T-connector also provides for the CO₂ output of the insufflation circuit to a second branch 48 coupled to the
15 quick exchange coupler 22. Either arrangement shown in Fig. 1A or 2A may be used to connect the insufflation circuit to the trocar. A second T-connector 44' that is in-line with the second branch 48 provides connection to a squeeze-pump 74 that will allow the delivery of a burst
20 of air into the tubing set 16, as discussed below. As with the trocar, the squeeze pump 74 may be directly connected to the T-connector 44' (Fig. 1A) or connected with the use of tubing (Fig. 2A).

The second branch 48 diverts a small portion of the
25 CO₂ output (e.g., 20% or less) to a male coupler 80 on the quick exchange coupler 22 that is sized and configured to mate within the inlet passage 32 of the quick exchange coupling 20.

The T-connector 44' is shown in more detail in Figs.
30 3A-3C. The T-connector 44' forms a valve 128 that has a first end 120 to be connected to the first portion 48a of the second branch 48 and a second end 122 for connecting to a second portion 48b of the second branch 48 of the tubing 16 (see Fig. 1A). The bottom 124 of the T-
35 connector 44' provides a fitting 126 for connection to

- 16 -

the squeeze-pump 74, as shown in Figs. 1A and 2A.

As is demonstrated in Fig. 3B, when the insufflator is in normal use, CO₂ will flow through the T-connector 44'. A ball 130 is located within the valve 128, with the pressure of the flowing CO₂ maintaining the ball 130 within the bottom section of the valve 128.

As is discussed further below, Figure 3C demonstrates the use of the squeeze-pump 74 to deliver a burst of CO₂ to the lens of the laparoscope. Pressure is applied to the squeeze pump 74, thereby moving the ball 130 up into the second end 122 of the T-connector 44', thereby momentarily stopping the flow of CO₂ from the insufflator circuit and providing the burst of CO₂.

Figs. 4A-4C show a pressure release valve 140 (also shown in Figs. 1A/2A) that works in connection with the source of sterile fluid 72 (see Figs. 1A/2A). The pressure release valve has a first end 142 that allows connection to the sterile fluid source 72 and a second end 144 for connection to the tubing 70 (see Figs. 1A/2A). A pressure exit 146 is located on the pressure release valve 140, which allows venting of excess gas when the assembly is in use. The pressure exit 146 is shown as being an attached drain structure, but it is understood that such a structure is not necessary for the exit 146 to work properly as part of the release valve 140.

As shown in Fig. 4B, a flapper valve 148 is located within the pressure release valve 140 and is normally positioned in a manner that closes the first end 142 of the valve 140, thereby preventing back flow of gas into the sterile fluid source 72. As will be discussed further below, gas will be allowed to move outwardly through the valve 140 and exit through the pressure exit 146.

When it is desired to inject fluid into the tubing set 16, the sterile fluid source, i.e. the syringe, 72

- 17 -

will be pushed forward to dispel fluid, as shown in Fig. 4C. The pressure being applied will move the flapper valve 148 from the position in Fig. 4B to the position in Fig. 4C. The fluid from the syringe 72 will be delivered
5 to the optimizing assembly, while the pressure exit 146 will momentarily be closed off. The flapper valve 148 also acts as a seal in the valve. It has been determined that the flapper valve 148 must be flexible enough so that it will be able to move from the position in Fig. 4B
10 to the position in Fig. 4C, while maintaining a positive seal when in the position shown in Fig. 4C. That is, the pressure normally used during a laparoscopic procedure, e.g. 15 mm Hg, will provide a force that will maintain the flapper valve 148 in the position in 4B, and the
15 flapper valve 148 should be manufactured from a material that will allow such a positive seal. An example of a preferred material is a silicone rubber, having a durometer = 20 shore A.

Use of the squeeze pump 74 and the pressure release
20 valve 140 contribute to the ability of the present optimizing assembly 10 to be operated without the necessity of the laparoscope 12 being removed during a procedure. Such a process was not realized with prior art assemblies, as the interaction between the use of air and
25 cleaning fluids and their interaction was not properly appreciated with the prior art. Figs. 5-14 demonstrate the procedure carried out according to the present invention.

Fig. 5 shows the optimizing assembly of the present
30 invention during normal operating procedure during a laparoscopic procedure. The insufflator circuit delivers CO₂ to the system, with the T-connector 44' being in the position shown in Fig. 3B and the pressure release valve 140 being in the position shown in Figure 4B. Eventually,
35 sheeting of surgical debris will build up on the lens 11

- 18 -

of the laparoscope, as shown in Fig. 6.

To clear the debris off of the lens 11, sterile fluid is delivered to the lens, as shown in Fig. 7. The T-connector 44' remains in position as shown in Fig. 3B, while the pressure release valve is in the position shown in Fig. 4C. As demonstrated in Fig. 8, the release of sterile fluid removes the surgical debris from the lens 11

As shown in Fig. 9, during normal operating procedures, the flow of CO₂ may eventually cause the formation of bubbles on the surface of the laparoscope lens, which can inhibit the view through the lens. Figs. 10 and 11 shows the squeeze pump 74 being compressed, thereby moving the T-connector 44' to the position shown in Fig. 3C. The compression squeeze pump 74 allows a burst of air to travel towards the laparoscope and across the lens.

As is depicted in Fig. 12, the lens of Fig. 9 has been cleared of the bubbles, thereby allowing a procedure to continue without having to remove and clean the lens. The cleared bubbles will exit out of the system, through the pressure release valve 140, as shown in Fig. 13. The result is a lens 11, free of both debris and bubbles as shown in Fig. 14.

The above described process was not previously realized in the prior art. Particularly it was not realized that the use of the CO₂ burst in combination with a cleansing liquid was used to provide a clear lens as shown in Fig. 14 without necessitating removal of the laparoscope during a procedure.

Referring now to Figs. 15A and 15B, the male coupler 80 of the quick exchange coupler 22 includes a one way check valve 50 that communicates with the second branch 48 of the tubing set 16. In the illustrated embodiment, the check valve 50 comprises a ball valve. Insufflation

- 19 -

pressure normally presses the ball valve 50 against a ball valve seat 52 (as shown in Fig. 15B). A projection 54 in the inlet passage 32 of the manifold 18 displaces the ball valve 50 from the valve seat 52 when the male
5 coupler 80 of the quick exchange coupler 22 mates within inlet passage 32 of the quick exchange coupling 20 on the manifold 18 (as shown in Fig. 16B). Unseating the ball valve 50 opens flow communication through the check valve 50 of the CO₂ into the inlet passage 32 and thus via the
10 manifold junction 104 into all the lumens 34; 36; 40; and 42 of the sheath 14. In the absence of coupling the male coupler 80 of the quick exchange coupler 22 to the inlet passage 32 on the manifold 18, the check valve 50 remains closed, normally blocking flow of CO₂ through the second
15 branch 48.

Thus, the tubing set 16 accommodates the set-up of the supply of the entire CO₂ output to an insufflation trocar through the tubing set 16, separate and independent of the connection of the tubing set 16 to the
20 manifold 18 of the sheath 14.

The tubing set 16 also includes, connected to the quick exchange coupler 22, a length of tubing 70 sized and configured for connection to a source 72 of sterile liquid, such as saline or sterile water (as shown in
25 Figs. 1A and 2A).

As shown in Figs. 1A/2A, the sterile liquid tubing 70 desirably includes an in-line pumping device 72. The in-line pumping device 72 is sized and configured to be operated on demand by a person at the OR table to convey
30 bursts of sterile liquid through the tubing 70. The in-line pumping device 72 and source can be integrated and comprise, e.g., a 20cc syringe filled with sterile liquid and connected by a tubing luer-lock on the saline tubing. Alternatively, the in-line pumping device 72 and source
35 can be separate and comprise, e.g., a bag of sterile

- 20 -

liquid, a spike connection on the saline tubing of the tubing set 16 to open communication with the bag in conventional fashion.

Preferably, the sterile liquid includes in solution
5 a "surface-active agent" that stabilizes mixtures of oil and water (e.g., fat) by reducing the surface tension at the interface between the oil and water molecules.

As Figs. 15A/15B and 16A/16B show, the tubing 70 conveys the sterile liquid to a male coupler 82 on the
10 quick exchange coupler 22 that is sized and configured to mate within the inlet passage 30 of the quick exchange coupling 20. Mating the male coupler 82 and inlet passage 30 establishes flow communication for the sterile liquid into the inlet passage 30 and thus via the manifold
15 junction 104 into the lumens 38 of the sheath 14.

As Figs. 15A and 16A further show, a latch 56 carried on a spring-biased button 58 on the quick exchange coupler 22 "clicks" into a detent 60 on the quick exchange coupling 20 on the manifold 18 to reliably
20 lock the coupler 22 and coupling 20 together for use, opening the check valve to flow CO₂ through the second branch 48 and establishing flow communication for the sterile liquid through the tubing 70 (shown in Figs. 9A/9B). Depressing the button 58 allows the quick
25 exchange coupler 22 and coupling 20 to be separated, and the check valve 50 will close in response to insufflation pressure in the second branch 48 (as shown in Figs. 15A/15B).

Connection of the quick exchange coupling 20 on the
30 manifold 18 to the quick exchange coupler 22 on the tubing set 16 is intended to occur at the OR table in the normal course, after the laparoscope 12 is connected to the light cable and the camera cable. Upon coupling, the one way check valve 50 is opened, and the manifold 18
35 directs the small portion of CO₂ from the CO₂ insufflation

- 21 -

circuit. Upon coupling, the manifold 18 also establishes flow communication for the sterile liquid. Disconnection of the of the quick exchange coupling 20 on the manifold 18 to the quick exchange coupler 22 on the tubing set 16 is also intended to occur at the OR table in the normal course, after a removal and/or exchange of a laparoscope 12.

E. The Locking Collar

The laparoscope 12 can be inserted down into the sheath 14. The sheath 14 is sized and configured so that the laparoscope 12 will slide smoothly through the sheath 14. Insertion continues until the lens and distal rim of the laparoscope 12 seat against the stop 26 at the distal end of the sheath 14. The laparoscope 12 will "bottom out" inside the sheath 14 against the stop 26, assuring correct axial alignment of the lens with a deflector assembly 64 located at the distal end of the sheath 14, as will be described in greater detail later.

If the laparoscope 12 is angled (as shown in Fig. 2A), the corresponding angled sheath assembly will also include an alignment fork guide 78. The alignment fork guide is also shown in Figs. 8A and 8A. The light post of the scope seats within the alignment fork guide 78, therefore assuring correct rotational alignment between the angled lens and the deflector assembly 64.

Once the laparoscope 12 is fully inserted into and aligned with the sheath 14, a member of the OR set-up team can rotate the locking collar 28 on the manifold 18 in the desired direction, e.g., clockwise (see Figs. 21 and 17B), until a firm stop is felt tactilely (e.g., after approximately one-third (1/3) of a turn). Registration of an alignment mark on the locking collar 28 and an alignment mark on the manifold 18 can additionally serve to visually confirm that the laparoscope 12 is secured against axial movement relative

- 22 -

to the sheath 14.

In the illustrated embodiment (see Fig. 21A), the locking collar 28 comprises a grip handle 84 mounted for rotation by a collet interacting with tabs 86 engaging an annular flange 88 on the manifold 18. An eccentric aperture 90 is formed in the grip handle 84. In a first rotational position (shown in Fig. 22A), the axis of the aperture 90 aligns with the axis of the sheath 14, allowing free passage of the laparoscope 12 through the aperture 90 into the sheath 14. In a second rotational position (shown in Fig. 22B), the axis of the eccentric aperture 90 shifts out of alignment with the axis of the sheath 14, and an interior edge of the aperture 90 frictionally contacts an exterior wall of the laparoscope 12. A pattern of cut-outs 92 formed about the periphery of the eccentric aperture 90 provide a spring resilience to the frictional contact. The frictional contact secures the laparoscope 12 against axial movement relative to the sheath 14.

In an alternative arrangement shown in Fig. 21B, the locking collar 28 on the manifold 18 can comprise a conventional collet mechanism 87. The collet mechanism 87 includes an inner sleeve 89 that, in response to rotation of the grip handle 84, radially closes to form a collar around the shaft of the laparoscope 12, to exert a clamping force that secures the laparoscope 12 against axial movement relative to the sheath 14. A seal 91 is also used to insure proper fluid flow through the assembly.

As shown in Figs. 22D and 22C, rotating the grip handle 84 of Fig. 21B in one direction (see Fig. 22D) closes the collar to squeeze the sleeve against the laparoscope 14, resulting in high static friction. Rotating the grip handle 84 in an opposite direction (see Fig. 22C) opens the collar, to release the laparoscope

- 23 -

14.

F. The Deflector Assembly

1. CO₂

The sheath 14 includes at its distal end a deflector
5 assembly 64 (see Figs. 23 and 24 for a blunt shaft tip
and Figs. 19 and 20 for an angled shaft tip). The
deflector assembly 64 projects a predetermined distance
beyond the distal end of the sheath 14, and thus also a
predetermined distance beyond the lens at the distal end
10 of the laparoscope 12 (see also Fig. 29).

In the embodiments shown in Figs. 23/24 and 26/27,
the deflector assembly 64 is secured to the distal end of
the sheath 14 by mounting tabs 94 that insert into the
lumens 40 and 42, thereby blocking CO₂ flow through these
15 lumens 40 and 42 at the distal end of the sheath. The
deflector assembly 64 also includes smaller mounting tabs
96 that fit into and partially occupy the lumens 34 and
36, so that the deflector assembly 64 communicates with
the lumens 34 and 36 in the sheath 14.

20 The deflector assembly 64 is sized and configured to
direct the portion of the CO₂ that is conveyed by the
sheath 14 through the lumens 34 and 36 in a prescribed
flow path and flow velocity across the laparoscopic lens,
as will be described in greater detail later. The flow
25 path and flow velocity of the CO₂ across the laparoscopic
lens prevents fogging and also desirably serves to
prevent entrainment or deposition of particles (moisture
and particulate matter) onto the lens, as well as deflect
smoke and surgical debris away from the laparoscopic lens
30 during surgery, preventing entrainment.

2. Physical, Pneumatic, and Optical

Characteristics of the Deflector Assembly

The size and configuration of the deflector assembly
64 are defined and constrained by several, sometime
35 overlapping considerations including (i) prescribed

- 24 -

physical characteristics, which are imposed due to the need to access the operating environment in as minimally invasive of a manner as possible and to be compatible with state of the art laparoscopes and other laparoscopic surgical instruments and techniques; (ii) prescribed pneumatic characteristics, which are imposed due to the need to create a particular flow path and flow velocity of CO₂ across the laparoscopic lens; and (iii) prescribed optical characteristics, which are imposed due to the need to prevent interference with the field of view and the visualization of the operating field by the laparoscope 12.

3. Physical Characteristics

The size and configuration requirements for minimally invasive access compatible with state of the art laparoscopic instrumentation and techniques are paramount. These requirements impose constraints upon the minimum inside diameter of the sheath 14 as well as the maximum outside diameter of the sheath 14. Because state of the art laparoscopes are provided with different shaft diameters, lengths, and lens configurations, the sheath dimensions and configuration change for compatibility with them. The view optimizing assembly 10 actually includes a family of sheath 14 / manifold 18 assemblies differently sized and configured to accommodate different classes of laparoscopes, to make possible compatibility with the families of state of the art laparoscopes that are in use.

For example, state of the art laparoscopes include 10 mm laparoscopes, 5 mm laparoscopes, and, within these sizes, 0° shaft tips, 30° shaft tips, and 45° shaft tips. Further, within these classes of laparoscopes, manufacturing tolerances typically vary from scope to scope, as well as from manufacturer to manufacturer. A given sheath 14 / manifold 18 assembly for a given

- 25 -

laparoscope class (e.g., 10 mm or 5 mm) desirably takes these typical manufacturing and manufacturer variances into account, and is desirably sized and configured to fit the largest scope variance encountered within a given
5 laparoscope class.

To maximize the fluid flow lumen area within the sheath 14, the minimum inside diameter of a given sheath 14 must closely conform to the maximum outside diameter of the shaft of the particular state of the art
10 laparoscope 12 selected for use, which the sheath 14 must accommodate in a smooth, sliding fit. Further, a gap between the outside diameter of the laparoscope shaft and the inside diameter of the sheath 14 must be minimized to avoid the transport and leakage of blood and fluids from
15 the operating field. Still further, minimizing the gap also assures that the laparoscope 12 self-centers in the sheath 14, thereby assuring faithful and accurate visualization through the laparoscope lens.

For example, for a typical laparoscope 12 in the 10
20 mm class, which measures 0.392 inch, the inside diameter of the sheath 14 is manufactured to .405 inch, providing a gap thickness of 0.0064 inch. For a 5 mm laparoscope 12 in the 5 mm class, which measures 0.196 inch, the inside diameter of the sheath 14 is manufactured to 0.218 inch,
25 providing gap thickness of 0.011 inch.

The maximum outside diameter of the sheath 14 for minimally invasive access must take into account the minimum inside diameter of the trocar, which the maximum outside diameter cannot exceed. That is, the outside
30 diameter of the sheath 14 is constrained by the inside diameter of the trocar. For example, in one embodiment a 5mm sheath 14 is used in combination with a trocar having a 7mm inside diameter and a 10mm sheath 14 is used in combination with a trocar having a 12mm diameter.

35 For example, for a typical 10 mm trocar that

- 26 -

measures 0.509 inch, the outside diameter of the sheath 14 is manufactured to 0.486 inch, providing a gap thickness of 0.0115 inch. For a typical 5 mm trocar that measures 0.324 inch, the outside diameter of the sheath 5 14 is manufactured to 0.300 inch, providing a gap thickness of 0.012 inch.

It is desirable, given the particular size and configuration constraints of the laparoscopic instrumentation and techniques used, to maximize the 10 outside diameter to the extent possible. This is because, together, the inside and outside diameters of the sheath 14 define the wall thickness for the sheath S_w , as Fig. 22 shows. The wall thickness S_w , together with the length of the sheath 14, in turn, defines the maximum area 15 available for the transport of the CO_2 and fluids by the sheath 14. The area of the fluid flow lumen or lumens dedicated to the supply of CO_2 , in turn, defines the maximum flow rate of the CO_2 directed by the deflector assembly 64. The flow rate should be sufficient at a 20 minimum, given the output of the insufflator selected for use, to supply CO_2 across the lens of the laparoscope 12 sufficient to prevent fogging.

Also affecting the effectiveness of the CO_2 to defog the lens is the water content of the CO_2 . Given the same 25 flow rate, the less water that is present in the CO_2 , the greater is the defogging capacity of the assembly. Further, the flow rate desirable should also be sufficient to deflect smoke and surgical debris away from the viewing field of the laparoscopic lens during 30 surgery, so that the CO_2 directed by the deflector assembly 64 both defogs and deflects debris.

Medical grade CO_2 for use with conventional insufflators is typically 99% pure, that is, no more than 1% of the gas is other than CO_2 , and such medical grade 35 CO_2 generally has a maximum moisture content of 25 parts

- 27 -

per million by volume. Typically, a state of the art insufflator circuit delivers CO₂ at a max flow rate of about 20 liters per minute. Typically, the insufflator circuit will sense pressure in the circuit and cycle off
5 when the sensed pressure is at or above 15 mmHg and cycle on when the sensed pressure is below 15 mmHg. Generally during procedures, the flow rate ranges between 3LPM - 7LPM for approximately 50% of a procedure, with the remainder of the time of the procedure having the flow
10 rate adjusted up or down, as determined by measuring the peritoneal pressure.

Given the above sheath dimensions, and given the supply of typical medical grade CO₂, a flow rate of at least about 1.0 liters per minute is critical to
15 achieving this objective. Given the above dimensions, and the supply of typical medical grade CO₂, a flow rate less than 0.8 liters per minute is not sufficient to prevent significant accumulation of moisture on the laparoscope lens.

20 In a representative embodiment, for a sheath 14 having an inside diameter of .405 inch and an outside diameter of .486 inch, and a length of 11.25 inch (which accommodates passage of a typical 10 mm laparoscope and its own passage through a conventional trocar) (i.e., S_w
25 = .081 inch), the total area available in the sheath wall is 0.056 square inches. Based upon required structural support within the wall (inside, outside, and radial) the total available area for lumens to transport fluids is 0.027 square inch.

30 In a representative embodiment, the total lumen area is occupied by five lumens 34 to 42. The area of each lumen can be maximized by selection of lumen geometry. In a representative embodiment, lumen geometry is generally triangular or pie shaped with rounded corners. The radial
35 walls that separate the lumens within the sheath 14 are

- 28 -

sized to minimize the spacing between the lumens.

In a representative embodiment, CO₂ transport is accomplished by the two lumens 34 and 36 that extend about 175 degrees about the outer circumference of the sheath 14 and comprising a flow area of 0.013 square inches. Sterile liquid transport is accomplished by one lumen 38 comprising a flow area of 0.003 square inches.

4. Pneumatic Characteristics.

As diagrammatically shown in Fig. 29, the deflector assembly 64 overhangs the laparoscopic lens by a prescribed transverse distance, defining a deflection width X, sufficient to change the direction of CO₂ flowing axially through lumens 34 and 36 of the sheath 14 (i.e., along the axis of the laparoscope shaft) into a non-axially, transverse path across the laparoscopic lens. The distance of the deflection width X should not extend to the point that is obstructs the field of the view of the laparoscopic lens. This is an example where a pneumatic characteristic of the deflector assembly 64 overlaps with an optical characteristic. Further optical characteristics will be described in greater detail below.

As also shown in Fig. 22, the deflector assembly 64 must also project axially beyond the distal terminus of the sheath 14 by a prescribed axial distance, defining an air channel distance Y, sufficient to maintain the CO₂ flowing along the path bounded by the deflection width X at a distance sufficiently close (proximal) to the laparoscopic lens.

Together, the deflection width X and the channel distance Y define the pneumatic characteristics of the deflection assembly 64. At the desired minimum flow rate, the pneumatic characteristics create a flow path that diverts CO₂ from the lumens 34 and 36 at the desired flow velocity across the laparoscopic lens toward the facing

- 29 -

side of the deflection assembly 64 (see Figs. 17 and 19). In the illustrated embodiment (see Fig. 22), the facing side of the deflection assembly 64 comprises a dead end, because the lumens 40 and 42 are blocked. The CO₂ from lumens 34 and 36 that is diverted across the laparoscopic lens encounters another air flow diversion at the facing side of the deflection assembly 64 (i.e., by blocked lumens 40 and 42), which is defined by a deflection width X and a channel distance Y at that end of the flow path. As Fig. 29 shows, reencountering an airflow diversion at this end of the flow path can serve to redirect the CO₂ back across the laparoscopic lens. A rolling vortex can be created that extends across and beyond the laparoscopic lens. The rolling vortex creates an air curtain across the lens sufficient to defog the lens. The rolling vortex is positioned beyond the lens with a sufficient air velocity to attract the particles away from the lens and thereby avoid entrainment or deposition of particles on the lens. To avoid entrainment, it is desirable that the vortex attracts particles away from the lens in a direction (when looking down the scope in a distal direction) toward a 3 O'clock (090) or Right Side or in a direction (also when looking down the scope in a distal direction) toward a 9 O'clock (270) or Left Side. As Fig. 29 generally shows, the rolling vortex appears to spiral about an axis that is generally transverse the axis of the sheath. CO₂ eventually exits the rolling vortex in a flow path that extends generally parallel to the axis of the sheath 14, carrying the particles with it.

EXAMPLE 1

A plume of water vapor (mist) is created by an ultrasonic transducer and channel through a tube. The distal end of sheath 14 (with a deflection assembly 64) is positioned over the plume, and CO₂ is conveyed through

- 30 -

the deflection assembly 64 in the manner described. Fig. 25B is a photograph demonstrating the presence of a "vortex shearing" effect across and beyond the laparoscopic lens for a deflection assembly 64 on a blunt sheath 14. Fig. 26B is a photograph demonstrating the presence of a "vortex shearing" effect across and beyond the laparoscopic lens for a deflection assembly 64 on a 30° angled sheath 14. In both instances, the deflected airflow is shown, with the accompanying shear and the resulting clear zone across and beyond the laparoscopic lens.

The rolling vortex for a blunt end sheath 14 is depicted in Fig. 25A (with a corresponding photograph shown in Fig. 25B), and the rolling vortex for an angled sheath is depicted in Fig. 28A (with a corresponding photograph shown in Fig. 28B). The rolling vortex is observed to create a "vortex shearing" effect across and beyond the laparoscopic lens, disrupting the ambient atmosphere at or near the tip of the sheath 14 to create a clear zone that extends across and beyond (by approximately 0.25 inch or more) the plane of the lens. The clear zone created by the vortex shearing effect prevents fogging, as well as deflects smoke and surgical debris away from the viewing field of the laparoscopic lens during surgery.

5. Optical Characteristics

The optical characteristics of the deflector assembly 64 are selected (i) to not block or reduce the illuminated image of the operating field provided by the laparoscope 12; (ii) not decrease the intensity of the illumination provided by the laparoscope 12 on the operating field; and (iii) prevent reflection of illumination light at the lens of the laparoscope 12.

As discussed above, the maximum deflection width X takes into account one of the desirable optical

- 31 -

characteristics; namely, the deflection width X should not obstruct the field of the view of the laparoscopic lens.

To prevent the decrease of the illumination, the deflector assembly 64 is desirably made from a material having high light transmission properties (i.e., transparency), to not interfere with the passage of light through the light cable 30 onto the operating field as well as the passage of the reflected image conveyed to the camera cable 32 of the laparoscope 12.

Furthermore, the material and surface finish of the deflector assembly 64 must pose minimal reflectivity to light. In a representative embodiment, the deflector assembly 64 is made from Bayer Makrolen Rx1805 with a surface finish defined as SPI/SPE A-3.

6. Orientation

As before described, CO₂ transport is accomplished by two lumens 34 and 36 that extend about 175 degrees about the outer circumference of the sheath 14. For a 0° shaft tip (see Fig. 16), the orientation of the deflector assembly 64 relative to the laparoscopic lens is not believed to be critical. However, for angled shafts (e.g., 30° shaft tips and 45° shaft tips) (see Fig. 26), the orientation of the deflector assembly 64 having this pneumatic characteristic relative to the laparoscopic lens is believed to be critical.

As Fig. 26 shows, the angled tip of a typical laparoscope 12 has a high end 66 and a low end 68. The lens slopes at the prescribed angle between the high end 66 and the low end 68. In a laparoscope 12 having a angled tip, the illumination cable (transmitting light onto the operating field) is located at the high end 66 of the angled tip, and the camera cable (transmitting reflected light back to the camera) is located at the low end 68 of the angled tip. To provide the desired vortex

- 32 -

shear effect on an angled tip having a pneumatic characteristic just described, it is believed to be critical that the deflector assembly 64 be oriented relative to the sloped laparoscopic lens such that the flow CO₂ is directed across the sloped plane of the lens from the low end 68 of the tip (from lumens 34 and 36) toward the high end 66 of the tip (toward the dead end lumens 40 and 42). In this arrangement, the defogging and debris deflection flow path originates proximal to the camera cable, which effectively comprises the eyes of the OR team. In this arrangement, the "vortex shearing" effect is across and beyond the sloped plane of the laparoscopic lens to achieve optimal defogging and debris deflection.

G. Sterile Liquid Flush

As previously explained, if desired, the tubing set 16 can also include, connected to the quick exchange coupler 22, a length of tubing 70 sized and configured for connection to a source 72 of sterile liquid, such as saline or sterile water (as shown in Figs. 1A and 2A). As shown in Figs. 1A/2A, the sterile liquid tubing 70 desirably includes an in-line pumping device 72, which in the illustrated embodiment comprises a 20cc syringe filled with sterile liquid fluid and connected by a tubing luer-lock on the saline tubing.

Preferably, the sterile liquid includes in solution a "surface-active agent" (surfactant) that stabilizes mixtures of oil and water (e.g., fat) by reducing the surface tension at the interface between the oil and water molecules.

In one preferred form of the sterile liquid solution, the solution comprises a dioctyl sulfosuccinate salt, such as dioctyl sodium sulfosuccinate (DSS) (also referred to as docusate sodium), docusate calcium, or docusate potassium. A buffer may be used to provide a

- 33 -

neutral and stabilized pH between 6.5-7.5. The remainder of the solution may comprise water for injection (WFI) quality water.

5 The higher the percentage of DSS shortens the time for cleaning the lens, but increases the tendency for the formation of bubbles on the lens. Conversely, a lower percentage of DSS in the solution has a lower tendency for the formation of bubbles, but also has a longer time for cleaning the lens. The present invention provides a
10 solution that balances these considerations. For example, a preferred formula may comprise DSS between 0.05%-0.25% w/v of the solution, with a more preferred range of the DSS being between 0.1%-0.2% w/v of the solution.

15 One preferred solution comprises 1.5 g DSS/1000ml WFI water, 2ml phosphate buffer/1000ml WFI water, with the remaining amount of the solution being WFI water. The solution comprises 0.15% w/v DSS, 0.002% w/v buffer, with the buffer concentration being 0.2M.

20 When the quick exchange coupler 22 and the quick exchange coupling 20 are connected, operation of the in-line pumping device 72 directs bursts of the sterile liquid through the lumen 38 in the sheath 14 to the deflector assembly 64 at the distal end of the sheath 14.

25 In this arrangement, the deflector assembly 64 is also sized and configured to direct the burst of sterile liquid in a desired path across the laparoscopic lens. The bursts of sterile liquid serve to flush debris off the end of the lens that may eventually accumulate, thereby cleaning the lens. Thereafter, bursts of air
30 supplied by the lumens 34 and 36 to the deflector assembly 64 by a squeeze pump 74 in the tubing set 16 (see Figs. 1A/2A) serve to clear residual fluid droplets off the lens to maintain an acceptable view.

35 In an illustrative embodiment (see Figs. 24 and 27), the deflector assembly 64 directs the bursts of sterile

- 34 -

liquid along a plurality of individual diverging channels 76 (three are shown). The diverging channels 76 distribute the bursts of sterile liquid in a fanning pattern across the lens of the laparoscope 12. In the illustrative embodiment, the diverging channels 76 discharge the bursts of sterile liquid in a path that is generally ninety-degrees to the path of CO₂. This orientation of the sterile liquid path relative to the CO₂ path across the lens, optimal for effective lens cleaning, applies to both 0° shaft tips and angled tips (e.g., 30° shaft tips and 45° shaft tips).

II. Illustrative Alternative Embodiments

Figs. 30 to 32 and 33 to 35 show another embodiment of view optimizing assembly 10' for use in association with a state of the art laparoscope (not shown). In Figs. 30 to 32, the view optimizing assembly 10' includes a shaft 14' for a laparoscope possessing at 0° (blunt) shaft tip. In Figs. 33 to 35, the view optimizing assembly 10' includes a shaft 14' for a laparoscope possessing an angle shaft tip (e.g., a 30° shaft tip or 45° shaft tip). An angled shaft tip is measured as angled from a blunt shaft tip, i.e. a shaft tip that is perpendicular to the central axis of the laparoscope. Thus, a 30° shaft tip would be angled 30° from a plane that is perpendicular of the central axis of the laparoscope.

In many respects, the fit, form, and function of the view optimizing assembly 10 shown in Figs 30 to 32 and 33 to 35 are at least equivalent to those previously described. As previously described, the sheath 14' comprises multiple interior lumens 34'; 26'; 38'; 40'; and 42', and the multi-lumen sheath 14 is sized and configured to mount over the shaft of the laparoscope. As also previously described, the shaft 14' is intended to be coupled via a manifold to a tubing set in the manner previously described (shown in Figs. 15A / 16A),

- 35 -

to connect the lumens of the sheath 14' to an existing carbon dioxide (CO₂) insufflation circuit, as well as to a source of flushing liquid, in the manner shown in Figs. 1A / 2A.

5 In the embodiment shown in Figs. 30 to 32 and 33 to 35, the sheath 14' includes at its distal end a deflector assembly 98. As the deflector assembly 64 previously described, the deflector assembly 98 projects a predetermined distance beyond the distal end of the
10 sheath 14, and thus also a predetermined distance beyond the lens at the distal end of the laparoscope 12' (see Figs. 32 and 35). In the embodiment illustrated in Figs. 30 to 32 and 33 to 35, the deflector assembly 98 comprises an injected molded part (see Figs. 30 and 33)
15 that is sized and configured to be glued onto the distal tip of the sheath 14', without need of any mounting tabs that project into any one of the lumens. Therefore, mounting the deflector assembly 98 onto the sheath 14' does not sacrifice any CO₂ flow capacity. In this
20 arrangement, there are also no dead ends to any CO₂ flow path. CO₂ can be conveyed to the deflector assembly 98 by all four lumens 34'; 36'; 40'; and 42' in the sheath 14.

As shown in Figs. 31 and 34, in this arrangement, CO₂ is circumferentially diverted from four diversion
25 regions 100 formed on the deflector assembly 98, each defining a deflection width X and a channel distance Y. Thus, CO₂ is diverted by the four circumferentially spaced regions 100 across the laparoscopic lens, lying along an arc of about 350°. The remaining lumen 38 conveys sterile
30 flushing liquid, as already described.

In the illustrated embodiment (see Fig. 30 and 33), the aperture 102 defined in the middle of the deflector assembly 98, into which the CO₂ is diverted across the laparoscopic lens, is smaller in diameter than the
35 aperture in the center region of the previously described

- 36 -

deflector assembly 64 (compare, e.g., Figs. 23 and 26). The smaller ("tighter") center region 102 in the deflector assembly 98 further centralizes the air flow region across the laparoscopic lens.

5 As Figs. 31 and 34 show, the four diversion regions 100 formed on the deflector assembly 64 each define a deflection width X and a channel distance Y to change the direction of CO₂ flowing axially through the four supply lumens 34'; 36'; 40'; and 42' of the sheath 14'. The CO₂
10 flows in four paths along an enlarged arc of about 350° transversely across the laparoscopic lens toward the facing sides of the deflection assembly 64. The CO₂ in each of the four paths will encounter a deflection width X and channel distant Y at their respective facing side
15 of the deflection assembly 64. Encountering a deflection width X and channel distant Y at these ends of the flow paths can redirect the CO₂ back across the laparoscopic lens, adding to the flow that enters at these ends (see Figs. 27 and 31). This rebounding flow pattern can form
20 one or more rolling vortices, or a pattern of multiple rolling vortices, that extend across and beyond the laparoscopic lens, disrupting the ambient atmosphere at or near the tip of the sheath 14 to create a clear zone extending across and beyond the laparoscopic lens, as
25 previously described. As Figs. 25 and 29 generally show, each rolling vortex appears to spiral about an axis that is generally transverse the axis of the sheath 14'. The array of rolling vortices may intersect one another, forming "butterfly wing" patterns, as Figs. 32 and 35
30 show. CO₂ eventually exits the rolling vortices in a flow path that extends generally parallel to the axis of the sheath 14, as before described with the previously described vortex embodiments.

 The rolling vortex pattern for a blunt end sheath 14
35 is depicted in Fig. 32, and the rolling vortex pattern

- 37 -

for an angled sheath is depicted in Fig. 35. The rolling vortex pattern creates a "vortex shearing" effect across and beyond the laparoscopic lens, disrupting the ambient atmosphere at or near the tip of the sheath 14 to create a clear zone that extends across and beyond the plane of the lens. As before, the clear zone created by the vortex shearing effect prevents fogging, as well as deflects smoke and surgical debris away from the viewing field of the laparoscopic lens during surgery.

10 **III. Optimizing the Rolling Vortex Pattern**

The creation of a vortex pattern at the distal end of the sheath is the outcome of properly establishing desirable physical and pneumatic conditions at the proximal end of the sheath. The vortex pattern assures that particles are moved away from the lens, and not toward the lens (a condition called deposition or entrainment). The vortex pattern also establish a gas curtain across the lens sufficient to defog the lens.

A. Exemplary Sheath for a 5 mm Laparoscope

20 Fig. 36A shows a proximal end view of a representative embodiment of a sheath, looking distally. In this embodiment, the sheath includes a center passage sized and configured to receive a typical 5 mm laparoscope. In a representative embodiment, the maximum outer wall diameter of the sheath (at the distal end) is .300 inch.

The orientation of the lumens 34, 36, 40, and 42 for conveying pressured CO₂ to the deflection assembly 64 in this size configuration are shown. For the purpose of description, the lumens 40, 42, 36, and 34 are numbered 1, 2, 3, and 4, respectively, counterclockwise from the saline lumen 38.

As Fig. 36A shows, the radial dimension of the lumens 1, 2, 3, and 4, measured between the inner and outer walls of the lumens are equal (in a representative

- 38 -

embodiment, 0.020 inch). However, the dimensions, expressed in degrees of arc, of lumens 1, 2, 3 and 4 differ. More particularly, the lumens 3 and 4 extend in degrees along a greater arc than lumens 1 and 2. In a
5 representative embodiment, the lumens 3 and 4 each extend 83° (tangentially 0.176 inch), whereas the lumens 1 and 2 extend 71° (tangentially .152 inch). The lumens 3 and 4 are therefore in volume larger than lumens 1 and 2.

In use with an angled tip sheath (see Fig. 36), the
10 larger lumens 3 and 4 (i.e., lumens 36 and 34) are positioned at the low end 68 of the tip in a desired registration with the deflector assembly 64, such that the flow CO_2 from the lumens 3 and 4 is directed across the sloped plane of the lens from the low end 68 of the
15 tip toward the high end 66 of the tip. In this arrangement, the defogging and debris deflection flow path originates proximal to the camera cable, which effectively comprises the eyes of the OR team. In this arrangement, the "vortex shearing" effect (see Fig. 28A)
20 is across and beyond the sloped plane of the laparoscopic lens to achieve optimal defogging and debris deflection.

As shown in Fig. 36B, the outer wall of the proximal end of the sheath, which is sized and configured to be fitted into the manifold junction 104 (see Fig. 19), is
25 reduced or trimmed in diameter to define, when fitted into the manifold junction 104, a plenum between the interior of the manifold junction 104 and the trimmed outer wall of the sheath. The plenum communicates with the lumens 1, 2, 3, and 4. Pressurized CO_2 enters the
30 plenum through the inlet passage 32 (see Fig. 36A, as is also shown in Fig. 18), which is located 180° opposite to the inlet passage 30 for saline (see Fig. 29A, as is also shown in Fig. 10).

In a representative embodiment, 0.117 inch of the
35 outer wall is removed for an axial distance of .140 inch

- 39 -

measured from the proximal terminus of the sheath (which will also be called the "trim distance) to form the plenum.

As Fig. 36C shows, in this representative
5 embodiment, pressurized CO₂ enters the plenum through the inlet port 32 at a velocity of 2 mm/sec. The inlet port 32 directs the pressurized CO₂ airflow simultaneously into lumens 2 and 3 in a counterclockwise direction. As can be
10 seen in Fig. 36A, a greater extent of lumen 3 overlaps the inlet port 32 than lumen 2, because the combined angular reach of lumens 3 and 4 is greater than the combined angular reach of lumens 1 and 2.

The pressurized CO₂ enters lumen 3 in a
counterclockwise flow direction toward lumen 4. A smaller
15 proportion of the pressurized CO₂ enters lumen 2. To reach lumen 1, there must be a sufficient clockwise backflow to direct the CO₂ toward lumen 1. Given the size and configuration of the plenum and lumens 1, 2, 3, and 4
shown in Figs. 36A, 36B, the proportional distribution of
20 CO₂ in the plenum among lumens 1, 2, 3, and 4, as shown in Fig. 29C, occurs.

As shown in Fig. 36C, the plenum directs a proximal
CO₂ airflow, at an entrance velocity of 2 mm/sec, into the
lumens 1, 2, 3, and 4 and through the deflector assembly
25 64 at the distal end of the sheath. The deflector assembly 64 includes a channel or gap distance Y of .005 inch (see Fig. 29.) The deflector assembly 64 directs the CO₂ at an increased exit velocity across the 5 mm lens,
creating a desired rolling vortex and "vortex shearing"
30 effect, which is shown in Figs. 25B and 28B, and as described in Example 1 (which tested a 5 mm sheath). The vortex pattern moves particles away from the lens, avoiding deposition or entrainment. The vortex pattern also establish a gas curtain across the lens sufficient
35 to defog the lens.

- 40 -

B. Exemplary Sheath for a 10 mm Laparoscope

Fig. 25A shows a proximal end view of a representative embodiment of another, larger sheath, looking distally. In this embodiment, the sheath includes
5 a center passage that is sized and configured to receive a typical 10 mm laparoscope. In a representative embodiment, the maximum outer wall diameter of the sheath (at the distal end) is .486 inch.

The orientation of the lumens 34, 36, 40, and 42 for
10 conveying pressured CO₂ to the deflection assembly 64 in Fig. 37A are shown to be generally the same as in Fig. 36A. As in Fig. 36A, for the purpose of description, the lumens 40, 42, 36, and 34 are numbered 1, 2, 3, and 4, respectively, counterclockwise from the saline lumen 38.

15 As Fig. 37A shows, the radial dimension of the lumens 1, 2, 3, and 4, measured between the inner and outer walls of the lumens are equal (in a representative embodiment, 0.020 inch). However, as in the embodiment shown in Fig. 29A, the dimensions of lumens 1, 2, 3 and
20 4, expressed in degrees of arc, differ. As in Fig. 36A, each lumen 3 and 4 individually extends 83°, and each lumen 1 and 2 individually extends 71°. Because of the overall larger diameter of the sheath in Fig. 37A, the same degrees of arc translate into larger tangential
25 dimensions in Fig. 30A: the lumens 3 and 4 extend tangentially 0.301 inch, and the lumens 1 and 2 extend tangentially 0.261 inch. As in Fig. 36A, the lumens 3 and 4 in Fig. 37A are in volume larger than lumens 1 and 2 in Fig. 37A, for the reasons stated with respect to the Fig.
30 36A embodiment.

As shown in Fig. 37B, the outer wall of the proximal end of the sheath, which is sized and configured to be fitted into the manifold junction 104 (in the manner shown in Fig. 19), is (as in Fig. 36B) reduced or trimmed
35 in diameter. The trimmed diameter defines, when fitted

- 41 -

into the respective manifold junction 104, a plenum between the interior of the manifold junction 104 and the sheath. The plenum communicates with the lumens 1, 2, 3, and 4.

5 In the representative embodiment shown in Fig. 37B, .140 inch of the outer wall is removed for an axial distance of .140 inch measured from the proximal terminus of the sheath (which will also be called the "trim distance") to form the plenum.

10 As generally explained with regard to Fig. 36C, pressurized CO₂ enters the plenum shown in Fig. 37B through the inlet port 32 at an entrance velocity of 2 mm/sec. The inlet port 32 directs the pressurized CO₂ airflow simultaneously into lumens 2 and 3 in a counterclockwise direction. As can be seen in Figs. 37A and 37B, because the combined angular reach of lumens 3 and 4 is greater than the combined angular reach of lumens 1 and 2, a greater volume of lumen 3 overlaps with the inlet port 32 than does lumen 2.

20 As previously explained, within the plenum, the pressurized CO₂ enters lumen 3 in a counterclockwise flow rotation toward lumen 4. A smaller proportion of the pressurized CO₂ enters lumen 2. To reach lumen 1, there must be a sufficient clockwise backflow to direct the CO₂ toward lumen 1. However, as the next Example 2 demonstrates, given the larger proportions of the plenum and lumens 1, 2, 3, and 4 in Figs. 37A and 37B, the direction and deflection of CO₂ by the plenum is not uniform in terms of variance of among the air speeds in the lumens, as well as in terms of the differential between the maximum and minimum air speeds: the air speeds fluctuate from 0.1 m/sec (at lumen 1) to 0.7 m/sec (at lumen 4) and 0.9 and 1.0 m/sec (at lumens 2 and 3), and the maximum air speed of CO₂ measured (in lumen 2) is 35 8.5 times the minimum air speed measured (in lumen 1).

- 42 -

Despite experiencing an increased exit velocity through the deflection assembly 64 at the distal end of the sheath (due to a reduced channel or gap distance Y of .005 inch), the direction and deflection and distribution of CO₂ within the entire proximal plenum is not uniform at the lumens 1, 2, 3, and 4. An insufficiently uniform direction and deflection and distribution of CO₂ within the entire plenum results in two undesired outcomes: (i) no rolling vortex is created; and/or (ii) an area of low pressure is created drawing the debris towards the lens, causing deposition or entrainment.

EXAMPLE 2

Various sheaths (identified as Devices 1 to 7) were constructed with distal plenums having differing sizes and configurations. These are described in the following Table 1:

Table 1: Sheaths Constructed

Device Designations	Proximal Plenum Configuration	Proximal Distances	Trim
1	As Shown in Fig. 37B	All lumens	0.140 inch
2	As Shown in Fig. 38A	Lumens 1 and 4 = 0.140 inch Lumens 2 and 3 = 0.70 inch	
3	As Shown in Fig. 38B	All Lumens	0.330 inch
4	As Shown in Fig. 38C	Lumens 1, 2, and 4 = 0.140 inch Lumen 3 = 0.70	
5	As Shown in Fig. 38D	Lumens 1 and 2 = 0.140 inch Lumens 3 and 4 = 0.0 inch	

- 43 -

Device Designations	Proximal Plenum Configuration	Proximal Distances	Trim
6	As shown in Fig. 39A	Lumens 1 and 4 = 0.140 inch Lumens 2 and 3 = 0.70 inch Divider Between 1 and 2 at 0.140 inch	
7	As Shown in Fig. 40A	All Lumens 0.140 inch Divider Between 2 and 3 at 0.140 inch	

Pressurized CO₂ was conveyed into the plenum of each Device 1 to 7, at an entrance pressure of 15mmHg and a flow rate of 14 L/min. Air speeds (m/sec) were measured coming out of each individual lumen (with no defection assembly attached at the distal end of the sheath) using a hot wire anemometer.

The air speeds measured are listed in the following Table 2:

10 **Table 2: Sheath Performance (Lumen Air Speeds: No Tip)**

Device Designations	Air Speed Lumen 1 Without Deflection Tip (m/sec)	Air Speed Lumen 2 Without Deflection Tip (m/sec)	Air Speed Lumen 3 Without Deflection Tip (m/sec)	Air Speed Lumen 4 Without Deflection Tip (m/sec)
1	0.2	1.7	0.7	0.6
2	0.1	1.1	1.3	0.8
3	0.1	1.0	0.9	0.7
4	0.2	1.1	1.2	0.7
5	0.4	1.5	0.4	0.1
6	0.1	0.9	1.0	0.5
7	0.4	0.9	1.0	0.7

Next, deflection assemblies 64 were attached to the distal end of the Devices 1 to 7. The deflector

- 44 -

assemblies 64 including a reduced channel or gap distance Y of .005 inch (see Fig. 29.) The Devices 1 to 7 with deflection assemblies were mated with conventional 10 mm laparoscopes with different tip configurations, i.e., blunt tips (0°) and angled tips (30° and 45°). CO₂ was conveyed through the deflection assemblies 64 at an entry pressure of 15 mm Hg and an entry flow rate of 14 L/min. For each Device 1 to 7, the flow rate (L/min) of the CO₂ exiting the deflection assembly was measured using digital flow meters measured in conjunction with an Omega DAQ system, as was the air speed (m/sec) using a hot wire anemometer.

As described in Example 1, a plume of water vapor (mist) was created by an ultrasonic transducer and channel through a tube. The distal ends of Devices 1 to 7 (with deflection assemblies 64) were positioned over the plume as CO₂ is conveyed through the deflection assembly 64. The plume of water vapor was observed for the presence or absence of a rolling vortex. The presence of a rolling vortex for a 5 mm sheath is shown in Figs. 25B and 28B.

The results are described in the following Table 3:

Table 3: Sheath Performance: Flow Rates/Plume
Performance with Deflection Assemblies (.005 Gap)

Device Designations↓	Flow Rate L/min			Air Speed m/sec			Plume
Distal Tip Angle →	0°	30°	45°	0°	30°	45°	
1	8.10	7.31	5.8	1.8	2.1	2.0	No Distinct Vortex Entrainment (Lumen 1)
2	7.40	6.51	7.6	2.0	1.7	2.1	Small Air Curtain Entrainment (Lumen 1)
3	6.80	6.35	6.71	1.5	1.5	1.8	No Distinct Vortex Entrainment (Lumens 2)

- 45 -

							and 3)
4	6.10	5.85	6.63	1.5	1.9	1.9	Dual Vortex Entrainment (Lumen 4)
5	6.60	6.65	6.40	1.8	1.7	2.0	Entrainment (Lumens 3 and 4)
6	7.10	6.3	6.25	1.8	1.4	1.5	Dual Vortex But Very Turbulent Entrainment (Lumen 2)
7	8.00	7.59	6.70	3.3	2.2	2.1	Distinct Vortex Large Air Curtain No Entrainment

As demonstrated in Table 2, CO₂ distribution within the plenum of the Devices 1 to 4 (Figs. 37B; 38A; 38B; 38C, respectively) was comparable. In all Devices 1 to 4, Lumens 2 and 3 received most of the CO₂, and the other two Lumens 1 and 4 received less. Lumen 1 always had the lowest air speed. The direction and deflection and distribution of CO₂ within the plenum was not uniform. The maximum air speed measured at the other lumens ranged between 6 to 13 times the minimum air speed measured at Lumen 1.

In these configurations, the CO₂ travels within the plenum from the manifold to the sheath in a counter-clockwise rotation, away from Lumen 1. In order for the CO₂ to travel into and through Lumen 1, it has to travel the opposite clockwise direction i.e. against the flow. The proportions of the 5 mm plenum shown in Figs. 29B and 29C directed and deflected and distributed the counterclockwise and clockwise flows within the plenum sufficiently to support a rolling vortex. However, as demonstrated in Table 3, the larger size proportions of the 10 mm plenum shown in Figs. 37B; 38A; 38B; 38C did not direct and deflect and distribute the

- 46 -

counterclockwise and clockwise flows within the plenum in a sufficiently uniform manner to support a rolling vortex. Further, entrainment occurred.

5 In Device 5 (Fig. 38D), Lumens 1 and 2 had a trim distance of 0.140, as in Device 1 (Fig. 37), but, unlike Device 1, Lumens 3 and 4 in Device 5 included no trim distance.

10 In the results observed for Device 5 in Table 2, like Device 1, Lumens 2 and 3 received most of the CO₂, and the other two Lumens 1 and 4 received less. However, in Device 5, Lumen 4 had the lowest air speed (the reverse of Device 1). As also observed in Devices 1 to 4, the direction and deflection and distribution of CO₂ within the plenum was not uniform. In Device 5, the
15 maximum air speed at the other lumens was 15 times the minimum airspeed at Lumen 4 (for comparison, in Device 1, the maximum air speed at the other lumens was 8.5 times the minimum air speed at Lumen 1; in Devices 1 to 4, the difference ranged upward to 13 times).

20 Device 5 does demonstrate that the absence of any trim distance in the plenum can lead to a significant deterioration of air speed in the affected lumens. This demonstrates that the presence of a plenum is beneficial.

25 In Device 5, as in Devices 1 to 4, the size and configuration of the 10 mm plenum, as shown in Fig. 38D, did not direct and deflect and distribute the counterclockwise and clockwise flows within the plenum in a sufficiently uniform manner to support a rolling vortex. Still further, entrainment occurred.

30 In Device 6 (Fig. 32), the plenum was enlarged at Lumens 2 and 3, and an air divider was placed in the plenum between Lumens 1 and 2. Compared to Device 1 (Fig. 37B), the maximum air flow speed measured in Device 6 (1.0 m/sec at Lumen 3) deteriorated and changed lumens
35 (in Device 1, the maximum air flow speed was 1.7 m/sec in

- 47 -

Lumen 2). Compared to Devices 1 to 4, there was not an appreciable improvement in the minimum air flow speed (0.1 m/sec at Lumen 1), and the difference between maximum and minimum air speeds was great (10 times). The presence of the air divider in the 10 mm plenum shown in Fig. 27 did change the direction and deflection of CO₂ flow within the plenum, as a vortex developed. However, the vortex was not beneficial -- there were dual vortices and turbulence. Further, entrainment persisted.

In Device 7 (Fig. 40A), an air divider was placed in the plenum between Lumens 2 and 3, and the plenum was equalized at a trim distance 0.140 inch at all lumens. Thus, Device 7 comprises Device 1 (Fig. 37B), with the addition of the air divider between Lumens 2 and 3. The presence of the air divider in Device 7 promoted counterclockwise CO₂ flow in the plenum sufficient to supply Lumens 3 and 4 with improved and more equalized air speeds, compared to Device 1. The presence of the air divider in Device 7 also intensified the clockwise CO₂ counter flow of CO₂ in the plenum sufficient to supply Lumens 1 and 2 with more equalized air speeds, compared to Device 1). The improved uniformity among the air speed was also noticed with respect to the difference between the maximum and minimum air speeds. The maximum air speed (in Lumen 3) in Device 7 was only 2.5 times the minimum air speed (in Lumen 1), compared to a difference of 8.5 times in Device 1.

Looking at the data of Table 3, which lists exit velocities measured at the distal end of Devices 1 to 7, it is difficult to determine why desirable results were achieved in Device 7, but undesirable results were achieved in Devices 1 to 6.

The data of Table 2, which lists air speeds of CO₂ directed, deflected, and distributed at the proximal plenum of Devices 1 to 7, it can be appreciated that it

- 48 -

is a uniformity of deflection and direction and distribution of CO₂ at the proximal end of the sheath that provides the expectation that a desired vortex effect will be achieved at the distal end of the sheath. It was the proximal configuration of Device 7 that promoted, in a 10 mm sheath, improved counterclockwise CO₂ flow in the plenum sufficient to supply Lumens 3 and 4 with improved and more equalized air speeds (1.0 and 0.7, respectively). It was the proximal configuration of Device 7 that promoted intensified clockwise CO₂ counter flow of CO₂ in the plenum sufficient to supply Lumens 1 and 2 with more equalized air speeds (0.9 and 0.4 respectively). The improved uniformity among the air speed in Device 7 was also present with respect to the difference between the maximum and minimum air speeds. The maximum air speed (in Lumen 3) in Device 7 was only 2.5 times the minimum air speed (in Lumen 1), compared to a difference of 8.5 times in Device 1. The equalized air speeds in Lumens 2 and 3 in Device 7 also correlate with a desired positioning of the vortex at the 9 O'clock (090) Left Hand position, because it is at this position that CO₂ transported by the Lumens 2 and 3 exits the deflection assembly.

The foregoing Example 2 demonstrates that the creation of a desirable vortex pattern at the distal end of the sheath is the outcome of properly establishing desirable physical and pneumatic conditions at the proximal end of the sheath. The desirable vortex pattern that is created in this manner assures that particles are moved away from the lens, and not deposited or entrained on the lens. The desirable vortex pattern that is created also establishes a gas curtain across the lens sufficient to defog the lens.

IV. Conclusion

The view optimizing assembly as described herein

- 49 -

prevents condensation from forming on the end of the
laparoscope during surgery. It further reduces or
eliminates the tendency for aerosolized debris from
cautery or other energy sources from settling on the lens
5 which can reduce visual acuity and waste time. The view
optimizing assembly as described herein gives a surgeon
an uninterrupted view of a laparoscopic operating field
by defogging and deflecting debris from the lens of the
laparoscope without having to remove the scope from the
10 abdominal cavity for cleaning.

- 50 -

Claims

1. A view optimizing assembly for use in combination with a laparoscope having a lens located on the shaft tip of the laparoscope, and a source of
5 insufflation CO₂, the assembly comprising:

a multi-lumen sheath assembly having a proximal end and a distal end capable of being mounted over the shaft of the laparoscope;

a deflector assembly located at the distal end of
10 the sheath assembly and in fluid communication with the lumens of the sheath assembly,

a tubing set connecting the lumens of the sheath assembly to the source of insufflation CO₂

wherein the flow of CO₂ through the lumens forms a
15 vortex when coming into contact with the deflector assembly, thereby preventing fogging of the laparoscope lens.

2. The optimizing assembly according to claim 1 further comprising:

20 a manifold located on the proximal end of the sheath assembly for coupling the tubing set to the sheath assembly.

3. The optimizing assembly of claim 2, wherein the manifold includes a quick exchange
25 coupling for connecting the tubing set to the sheath assembly.

4. The optimizing assembly of claim 3, wherein the manifold further comprises a plurality of inlets arranged to interact with the lumens of
30 said sheath assembly.

5. The optimizing assembly of claim 1 wherein the sheath comprises a stop at said distal end for limiting the distance the sheath may be inserted into laparoscope.

- 51 -

6. The optimizing assembly of claim 1 further comprising a locking collar located at said proximal end of said sheath assembly to frictionally engage the laparoscope and resist axial withdrawal of the
5 laparoscope from the sheath assembly.

7. The optimizing assembly of claim 1 wherein the distal end of the sheath assembly and the deflector assembly being substantially parallel to the surface of the laparoscope shaft tip.

10 8. The optimizing assembly of claim 8 wherein the surface of the laparoscope shaft tip is angled at a non-perpendicular angle with respect to the central axis of the laparoscope, the shaft tip has a low end and a high end.

15 9. The optimizing assembly of claim 8 wherein the angle of the shaft tip is 30° from perpendicular with respect to the central axis of the laparoscope.

10 10. The optimizing assembly of claim 8 wherein the angle of the shaft tip is 45° from perpendicular with respect to the central axis of the laparoscope.

11. The optimizing assembly of claim 8 wherein the vortex by the deflector assembly is formed by blowing CO₂ across the shaft tip from the low end of the shaft tip to the high end of the shaft tip.

25 12. The optimizing assembly of claim 1 further comprising an in-line pumping device located in said tubing set, said pumping device capable of delivering cleaning fluid to said deflector assembly.

30 13. The optimizing assembly of claim 1 further comprising means for providing an air burst across the lens of the laparoscope.

- 52 -

14. A method of preventing fogging of the lens of a laparoscope during a laparoscopic procedure comprising The steps of:

- providing a source of insufflation CO₂
- 5 providing a view optimizing assembly comprising
 - a multi-lumen sheath assembly having a proximal end and a distal end capable of being mounted over the shaft of the laparoscope;
 - a deflector assembly located at the distal end of
 - 10 the sheath assembly and in fluid communication with the lumens of the sheath assembly,
 - a tubing set connecting the lumens of the sheath assembly to the source of insufflation CO₂
 - flowing CO₂ from the source of insufflation CO₂ to
 - 15 the deflector assembly, and
 - blowing CO₂ across the lens of the laparoscope by forming a vortex of the CO₂ with the deflector assembly, thereby defogging the laparoscope lens.

15. The method of claim 14 wherein the lens of the
20 laparoscope is angled at a non-perpendicular angle with respect to the central axis of the laparoscope, the lens having a low end and a high end.

16. The method of claim 15 wherein the step of blowing CO₂ across the lens of the laparoscope further
25 comprises blowing CO₂ across the lens from the low end of the shaft tip to the high end of the shaft tip.

17. The method of claim 14 further comprising the step of

30 pumping a cleaning fluid across the surface of the lens of the laparoscope.

18. The method of claim 17 further comprising the step of

pumping an air burst across the lens of the laparoscope.

35 19. A kit comprising the view optimizing assembly

- 53 -

of claim 1.

20. A method for clearing the lens of laparoscope during a laparoscopic procedure comprising the steps of:

providing a source of sterile fluid;

5 flowing sterile solution over said lens to remove surgical debris formed during said laparoscopic procedure;

providing a source of insufflation CO₂;

blowing insufflation CO₂ over said lens; and

10 providing a burst of insufflation CO₂ to remove bubbles from the laparoscopic lens formed during the laparoscopic procedure.

21. The method of claim 20 further comprising the step of

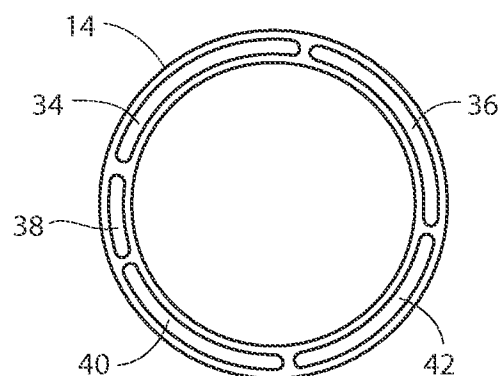
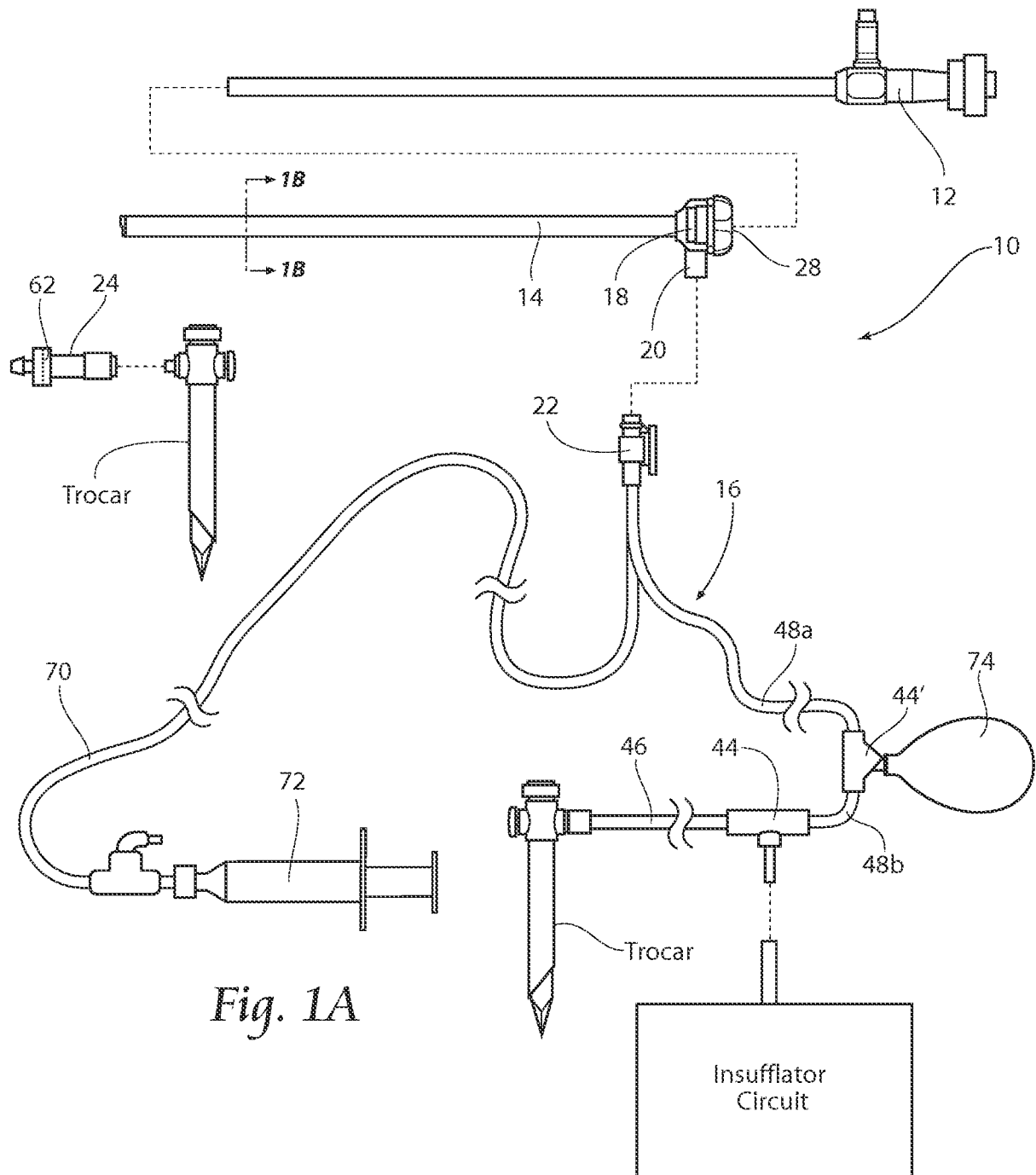
15 providing a release vent for said formed bubbles.

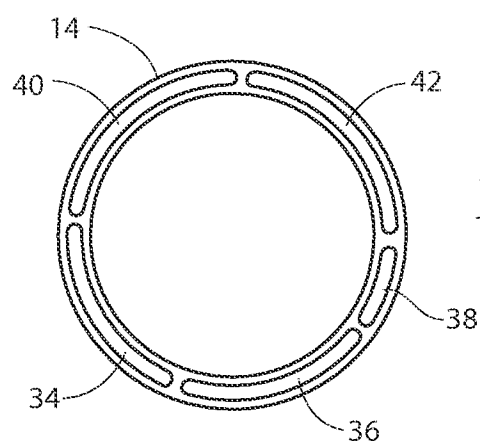
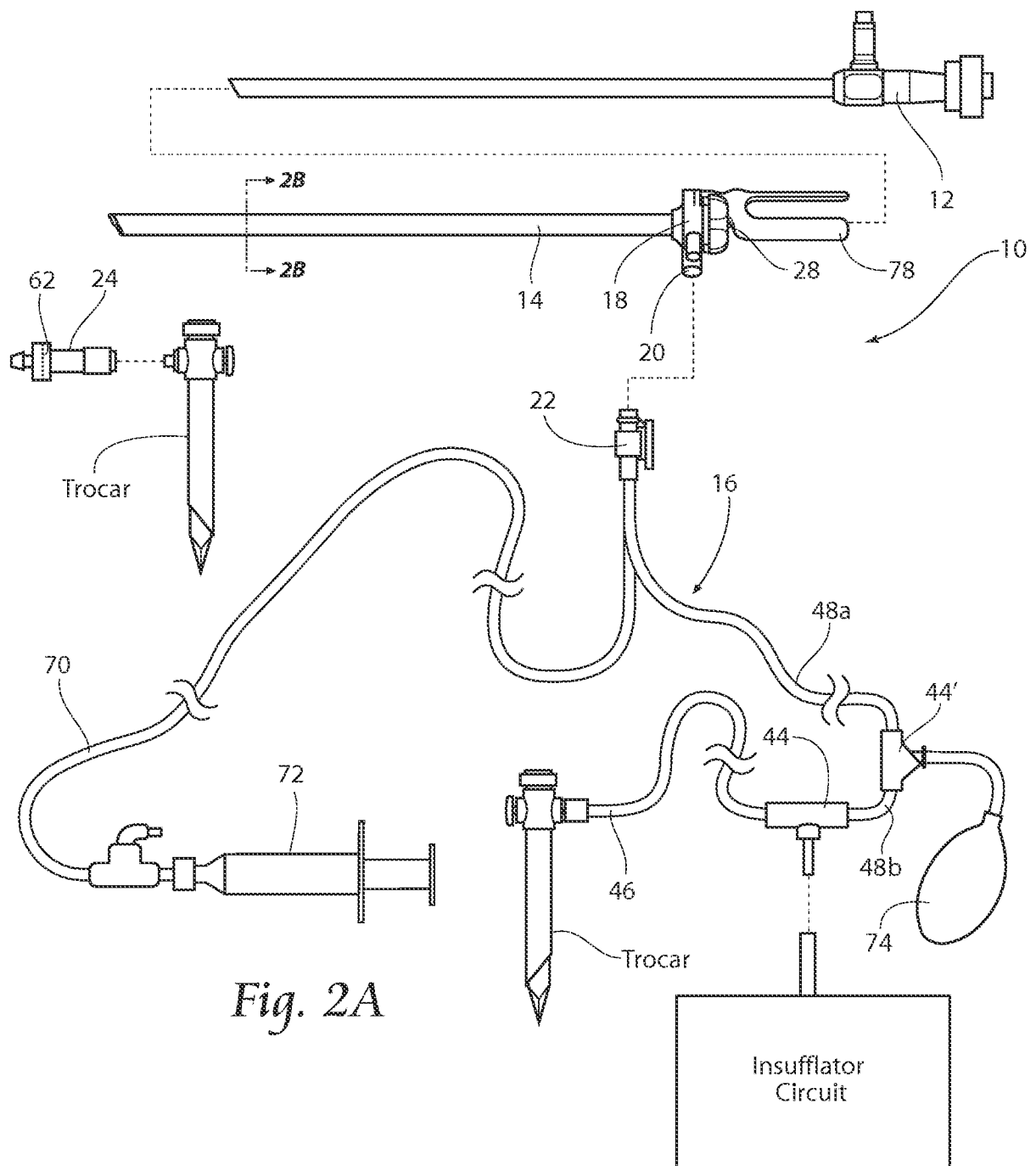
22. The method of claim 20 wherein the sterile fluid comprises a dioctyl sulfosuccinate salt.

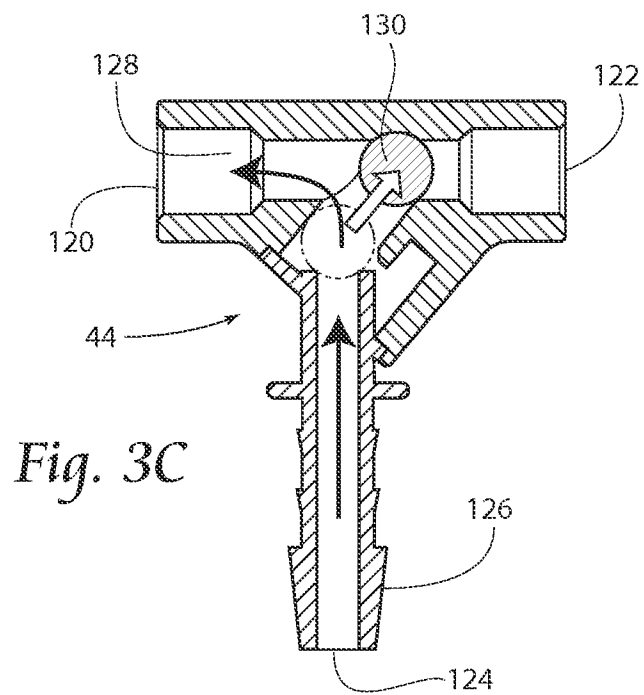
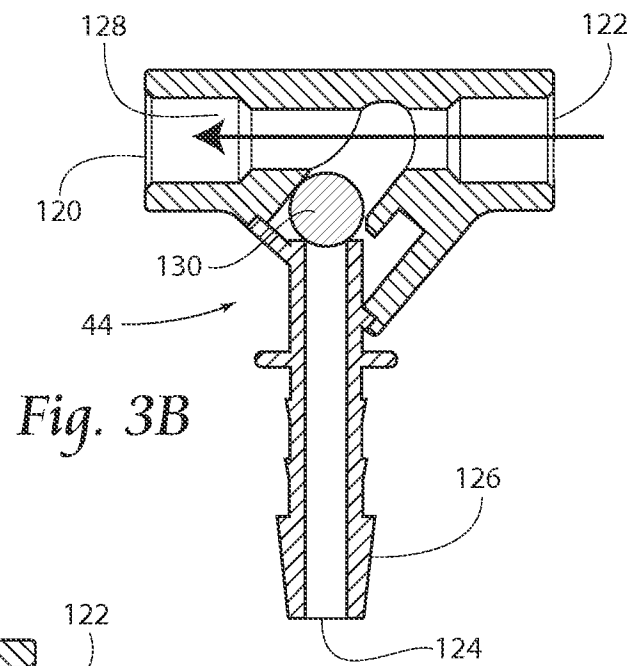
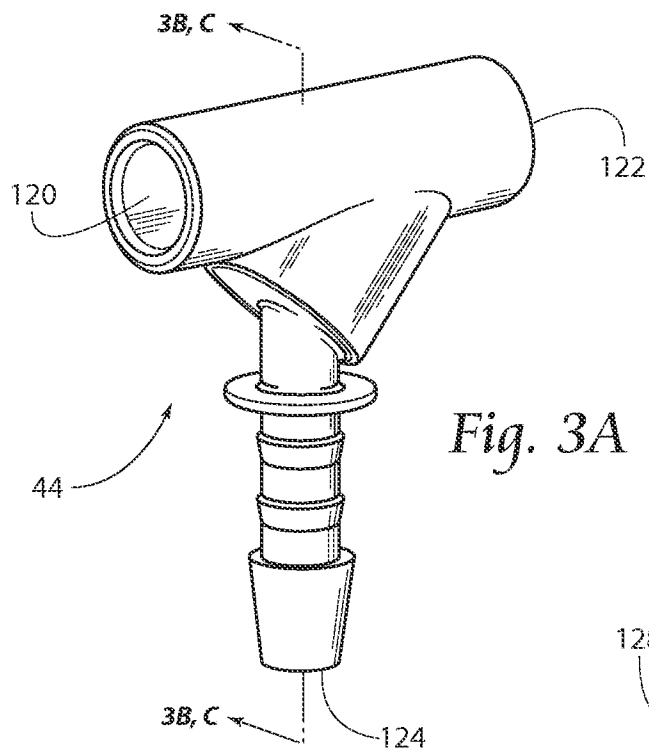
23. The method of claim 22 wherein the sterile fluid further comprises dioctyl sodium sulfosuccinate.

20 24. The method of claim 23 wherein the dioctyl sodium sulfosuccinate comprises between about 0.05%-0.25% w/v of the sterile solution.

25 25. The method of claim 24 wherein the sterile solution has a pH between about 6.5-7.5.







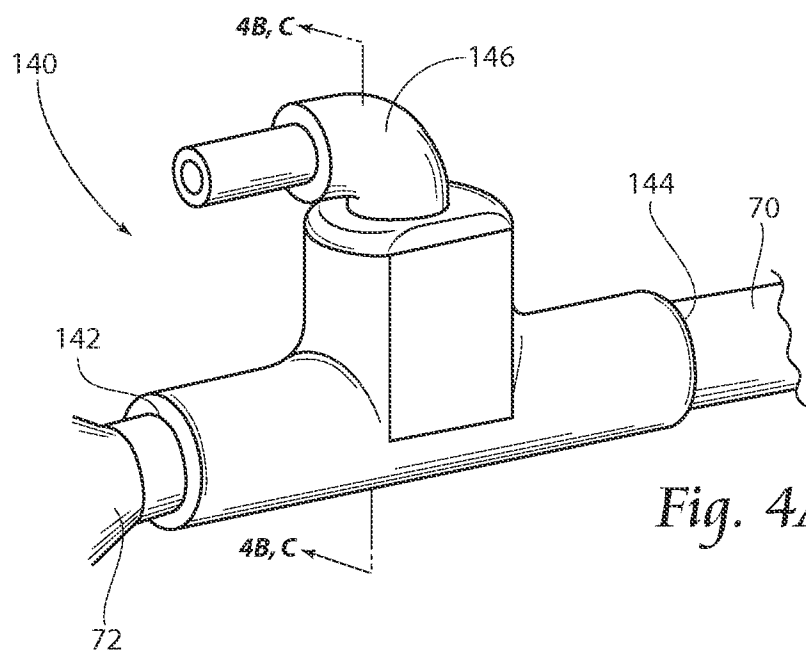


Fig. 4A

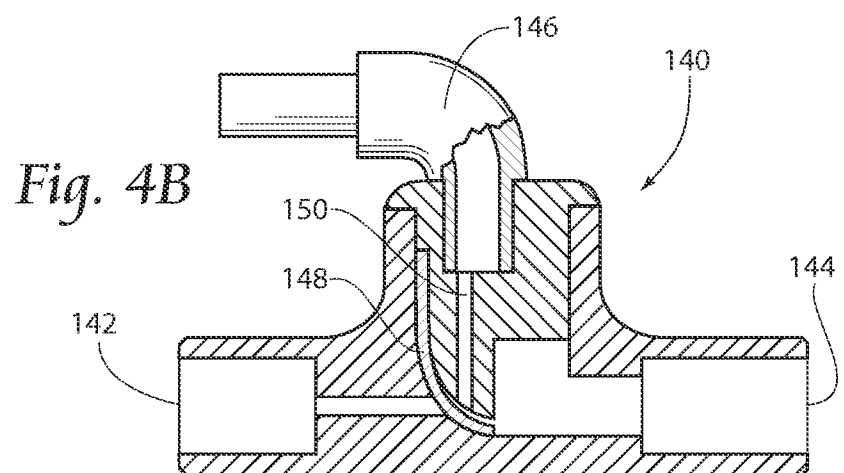


Fig. 4B

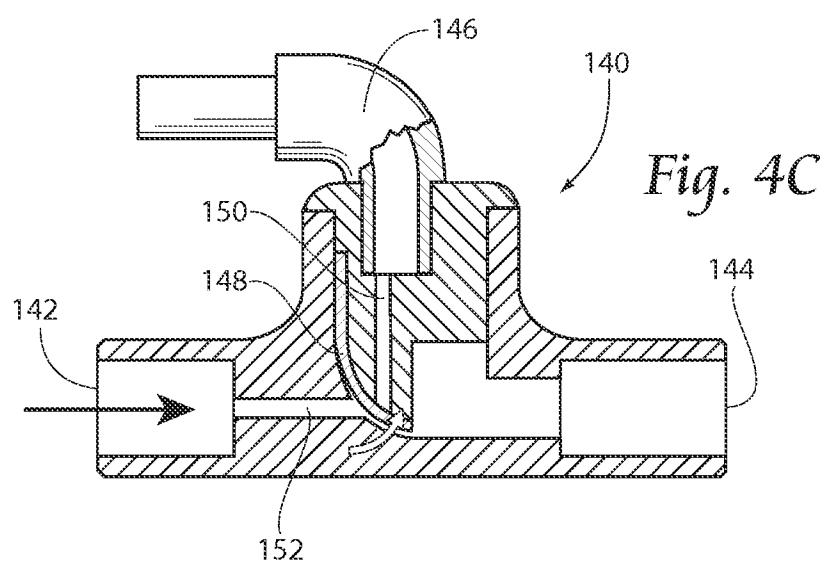


Fig. 4C

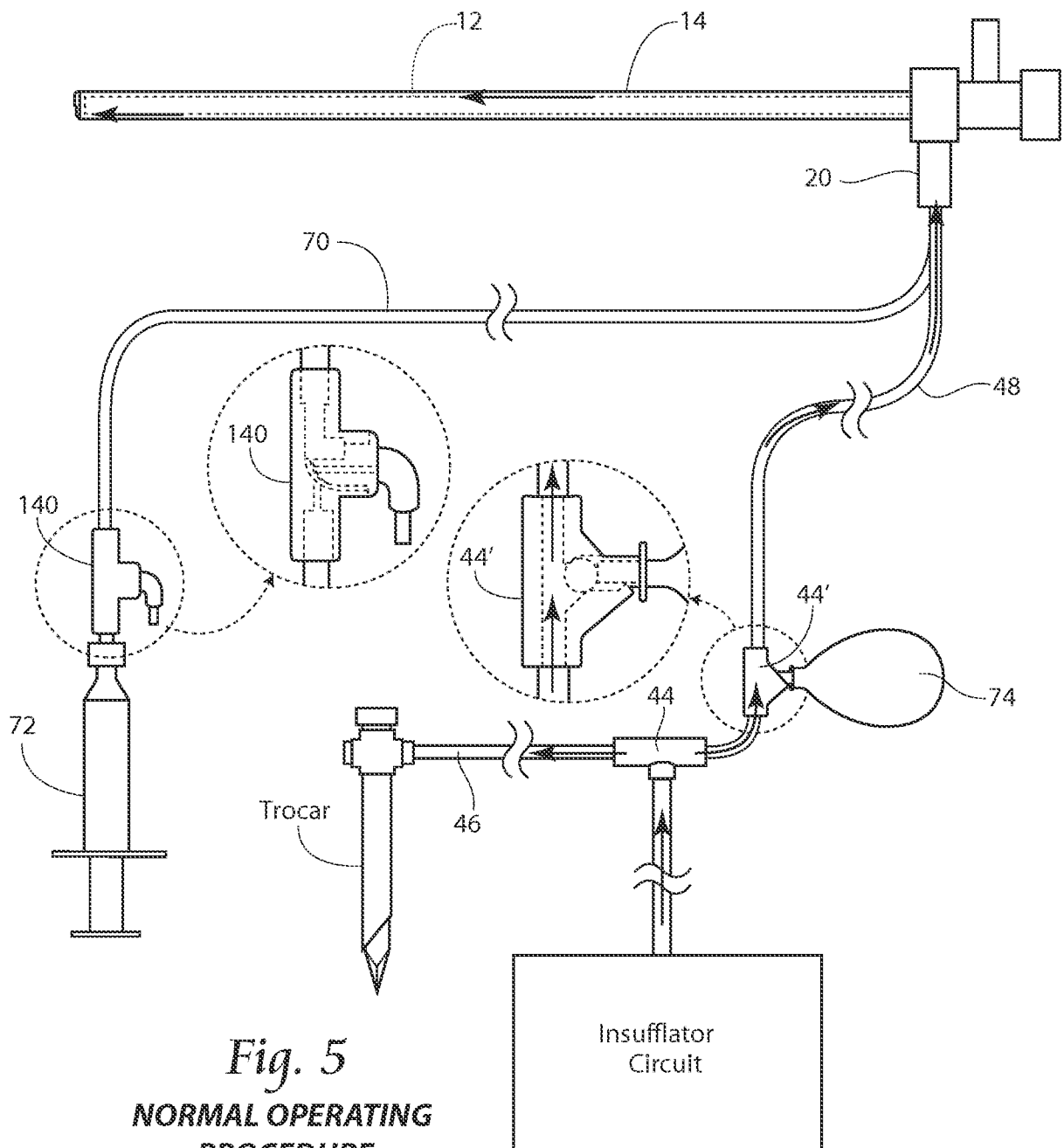
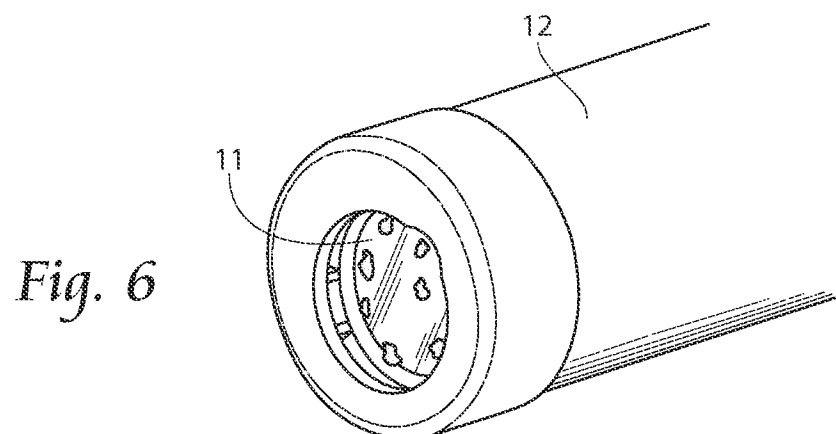
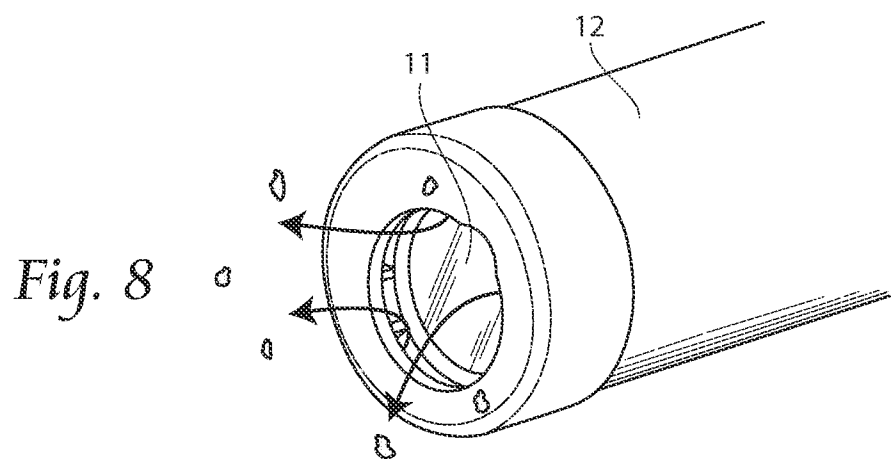
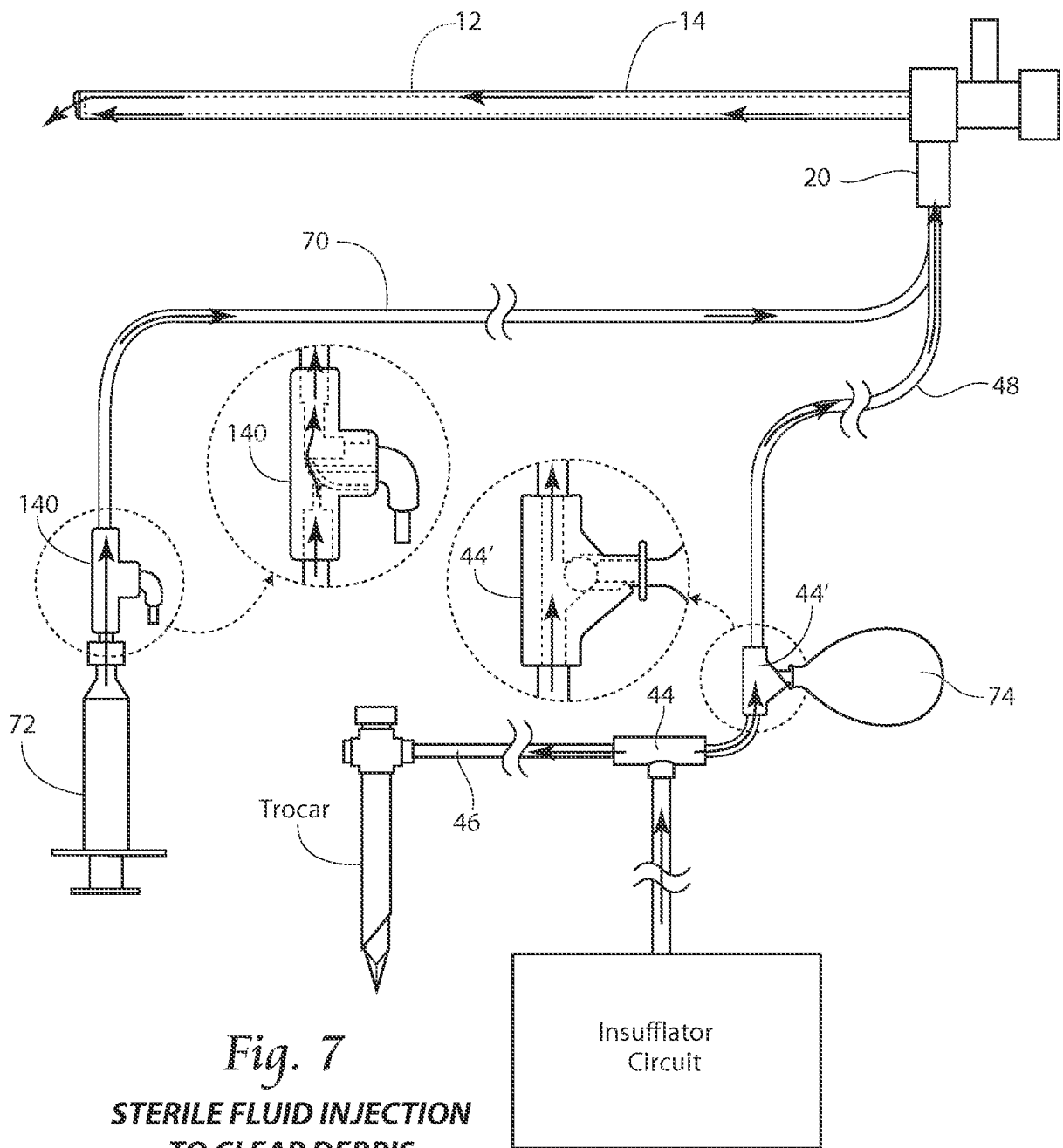


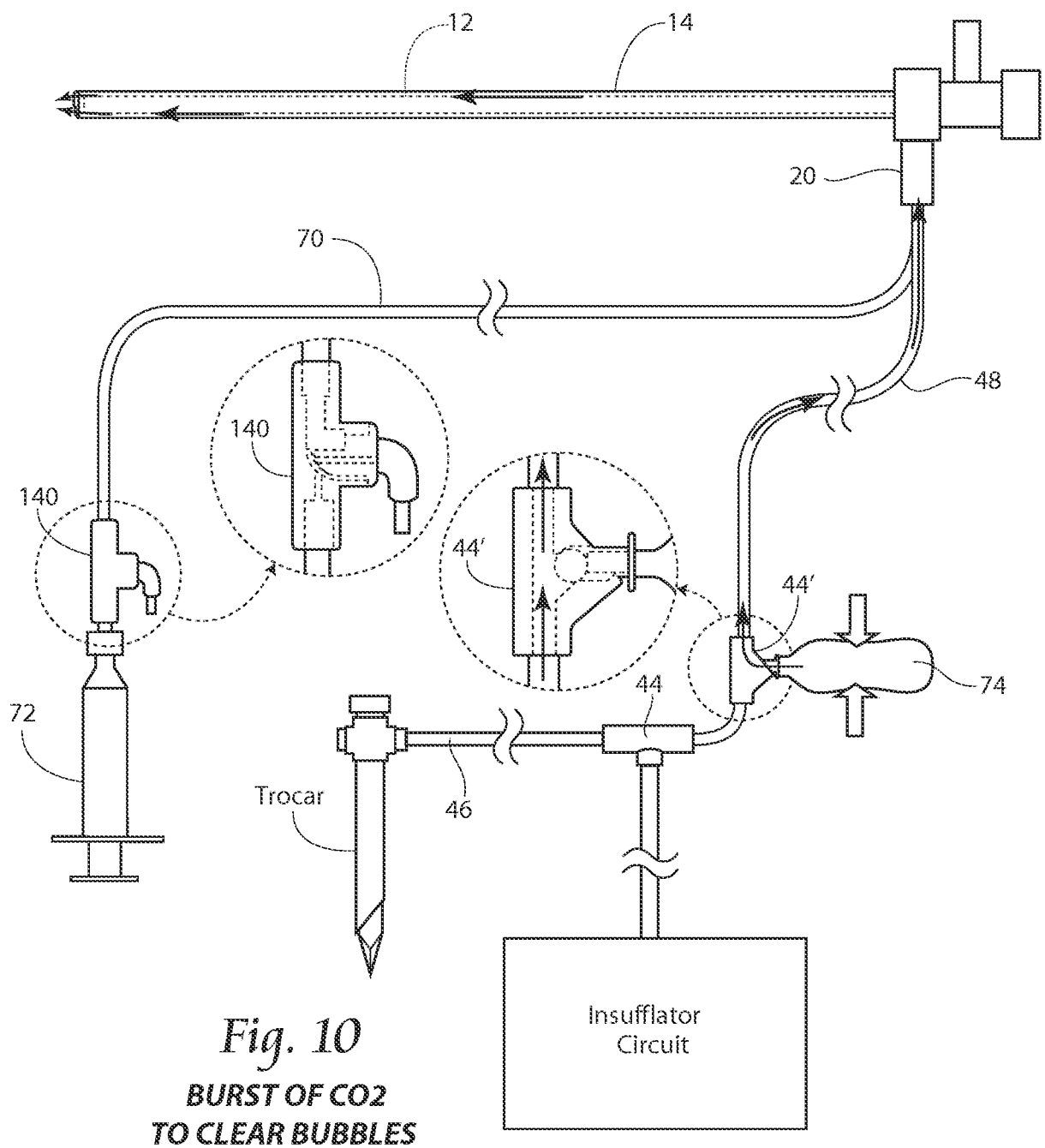
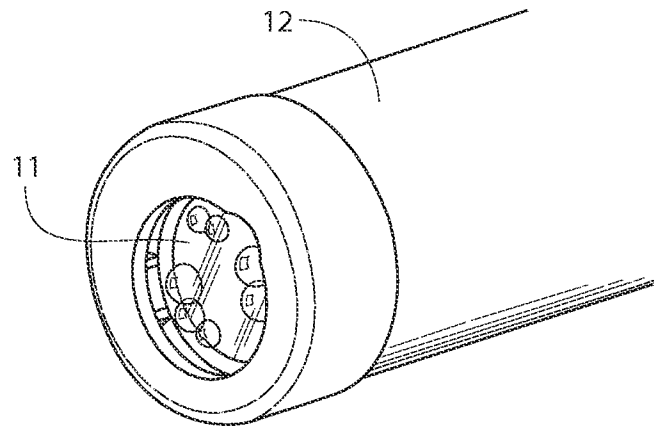
Fig. 5
**NORMAL OPERATING
PROCEDURE**

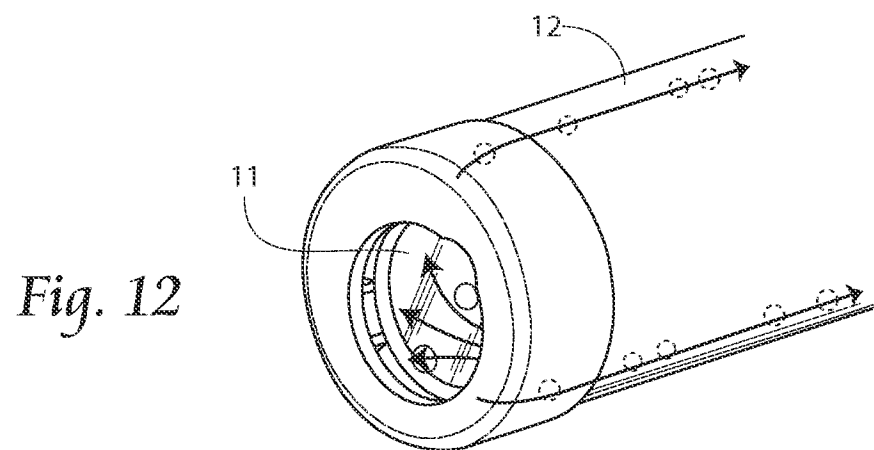
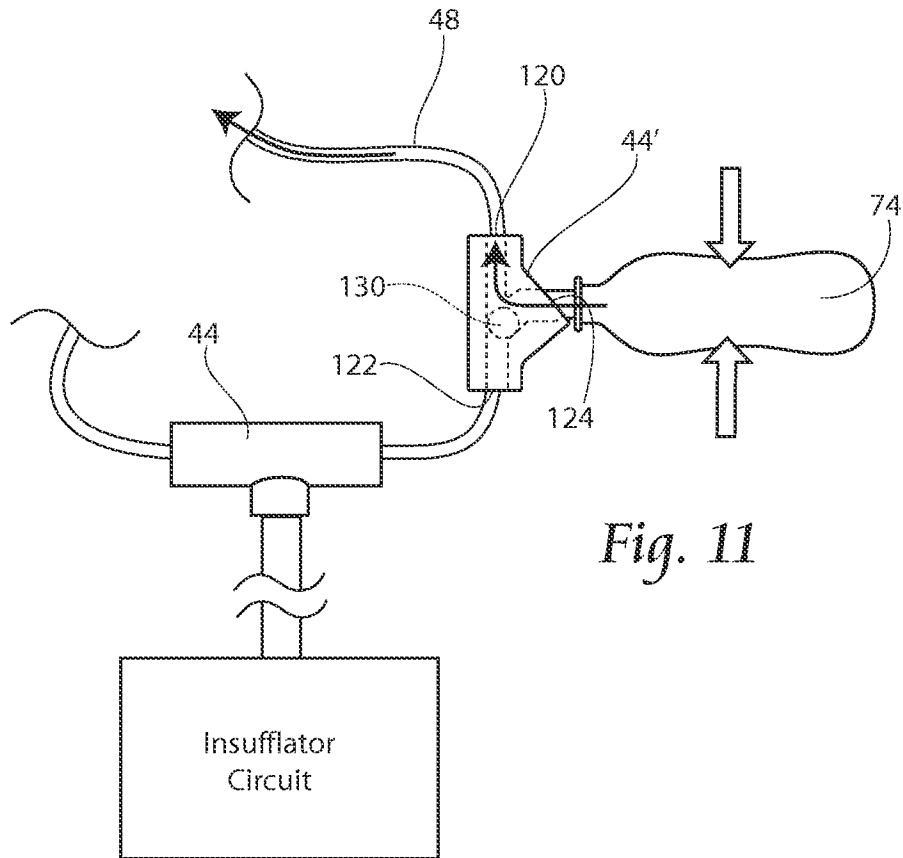


6/29

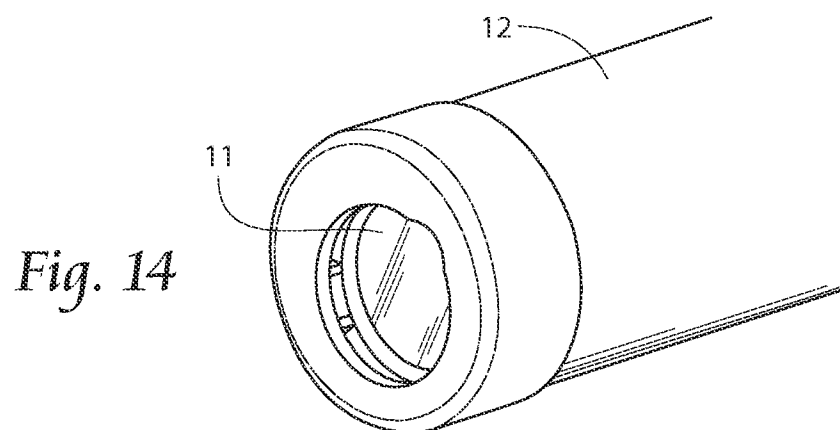
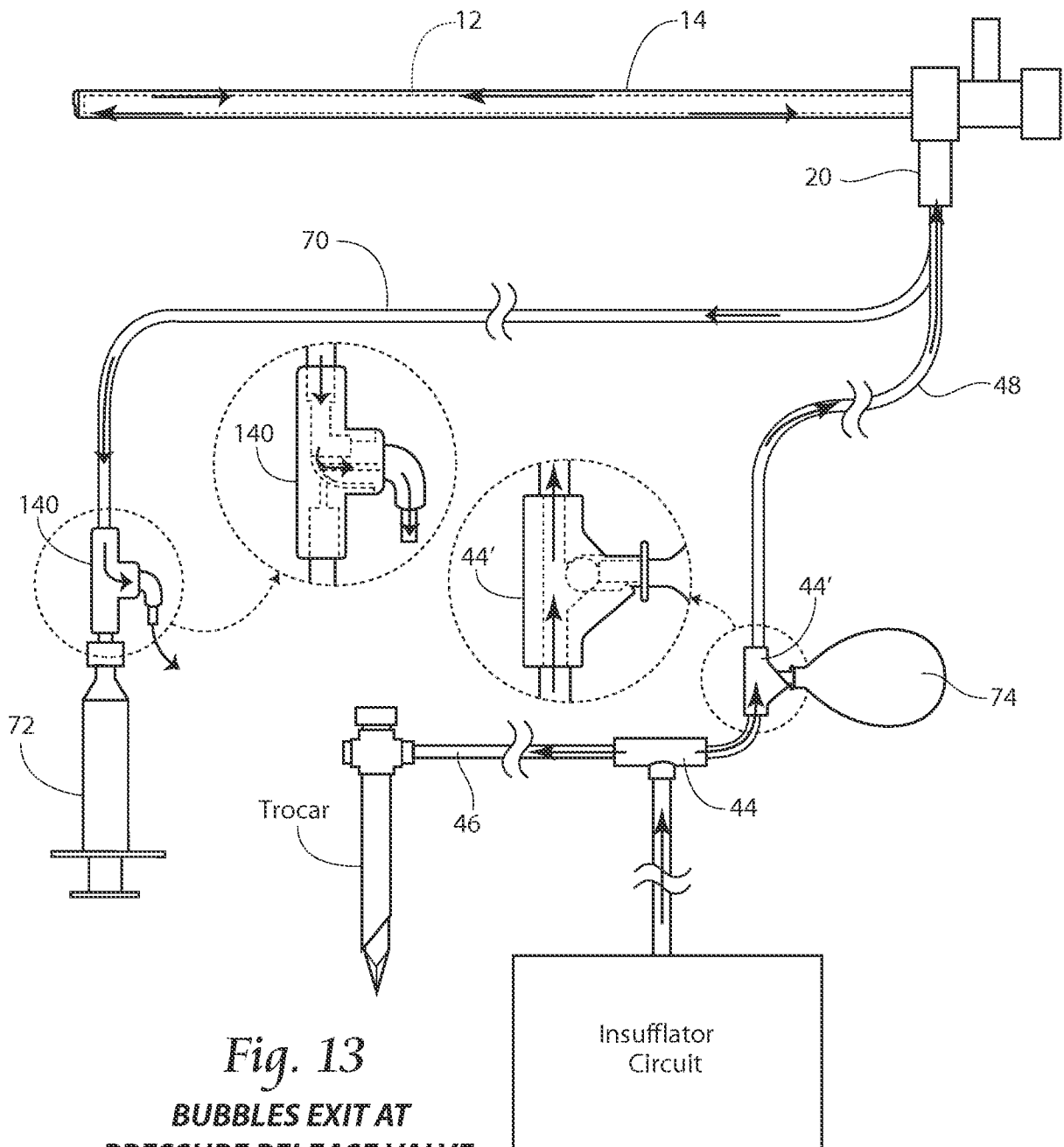


7/29

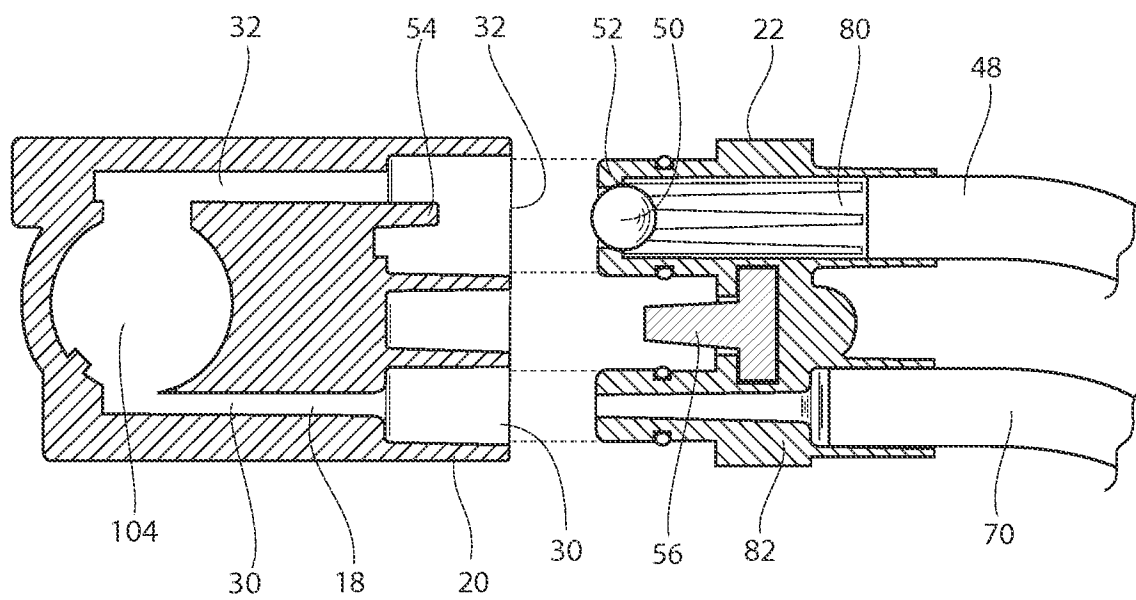
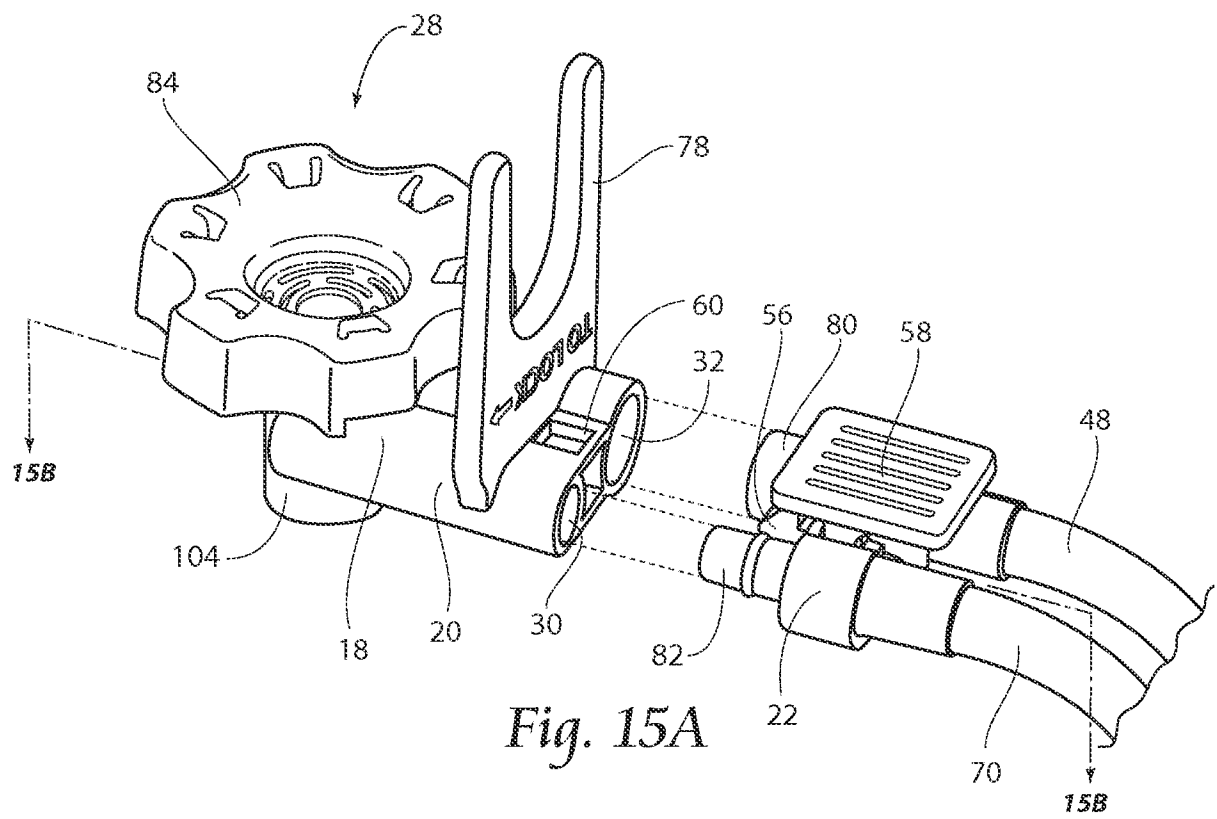
Fig. 9



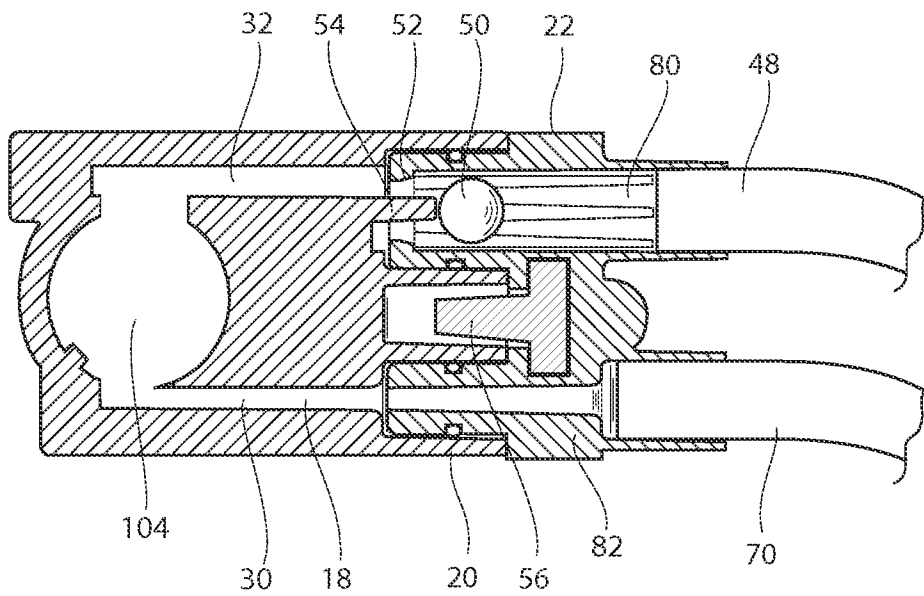
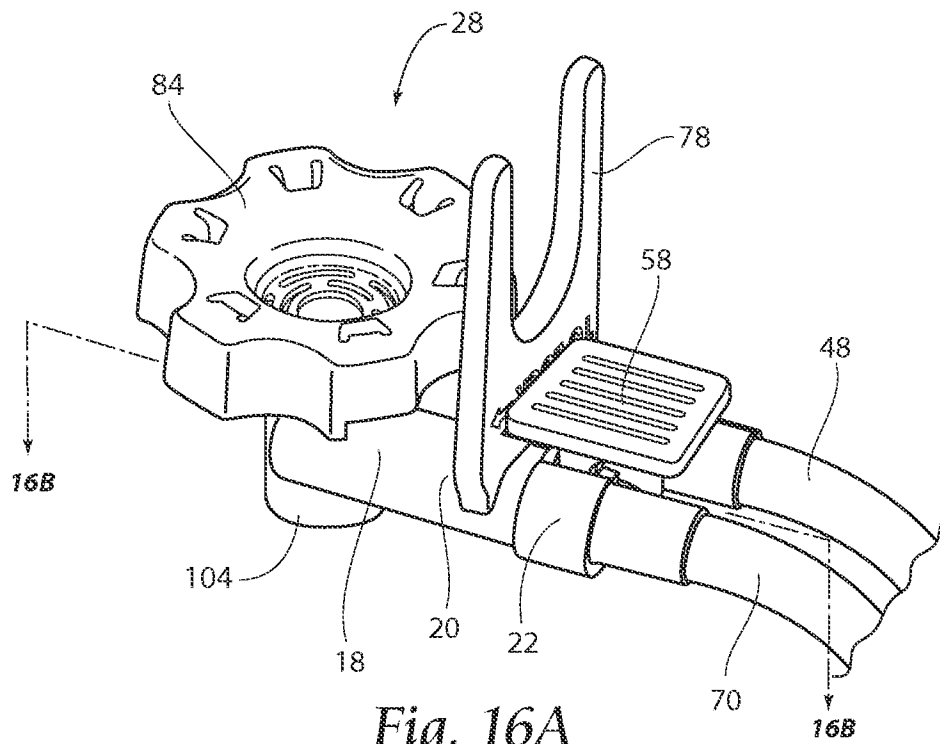
9/29



10/29



11/29



12/29

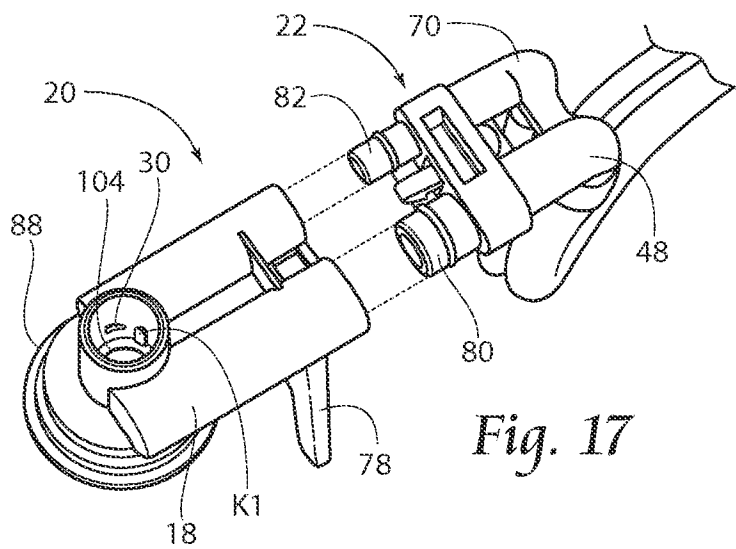


Fig. 17

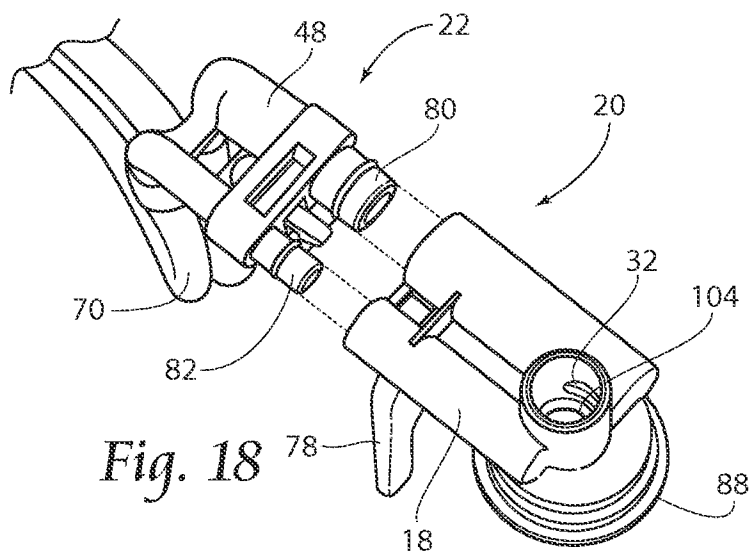


Fig. 18

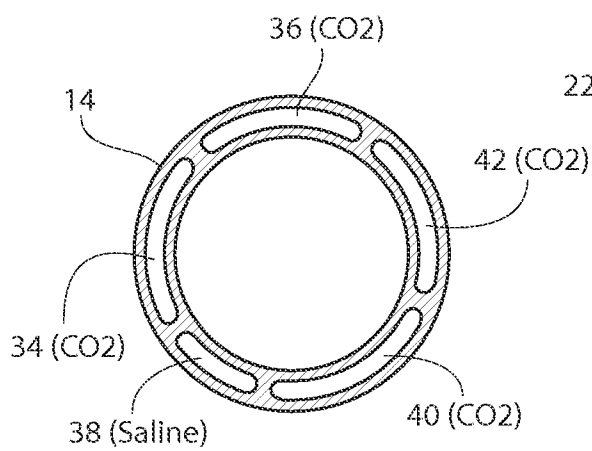


Fig. 19

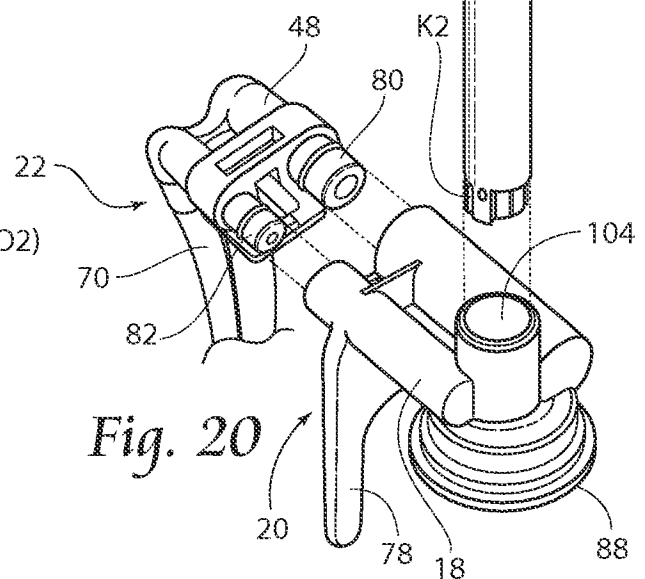


Fig. 20

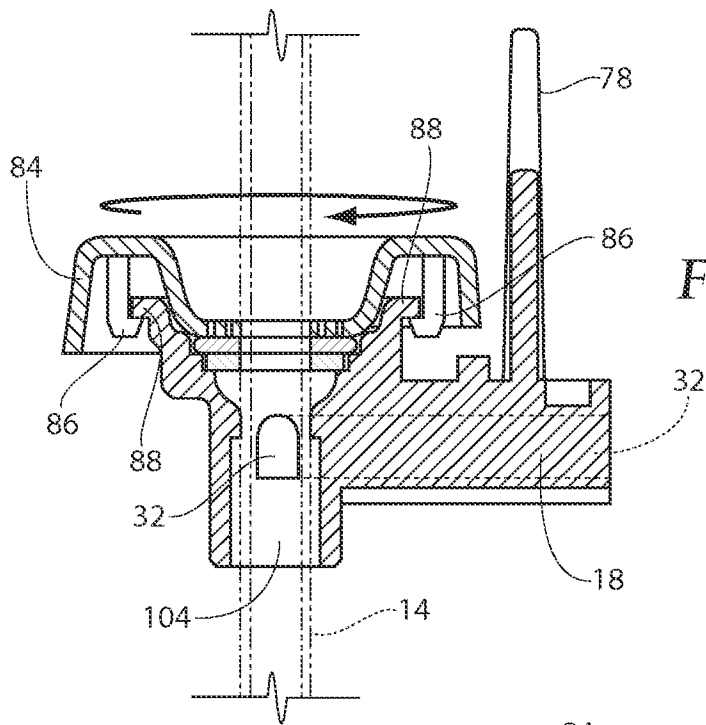


Fig. 21A

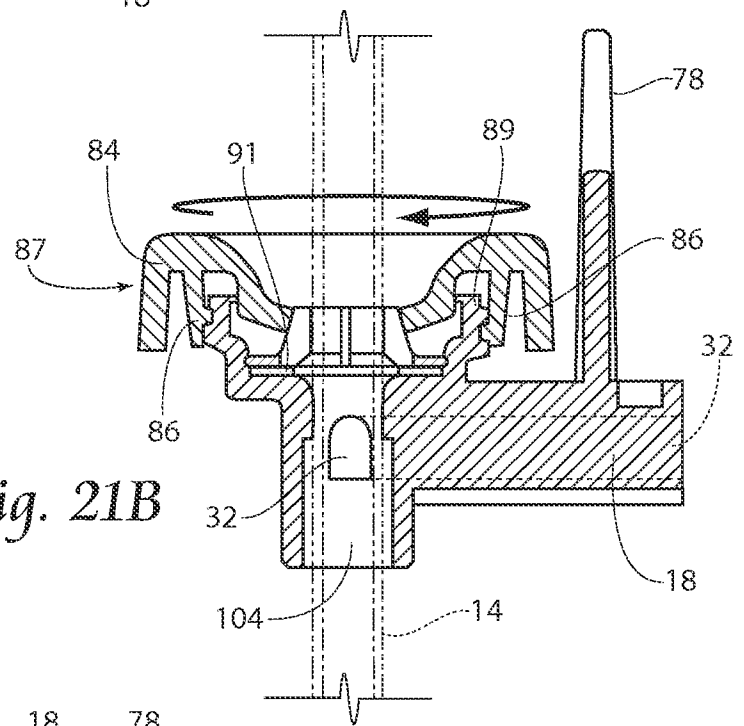


Fig. 21B

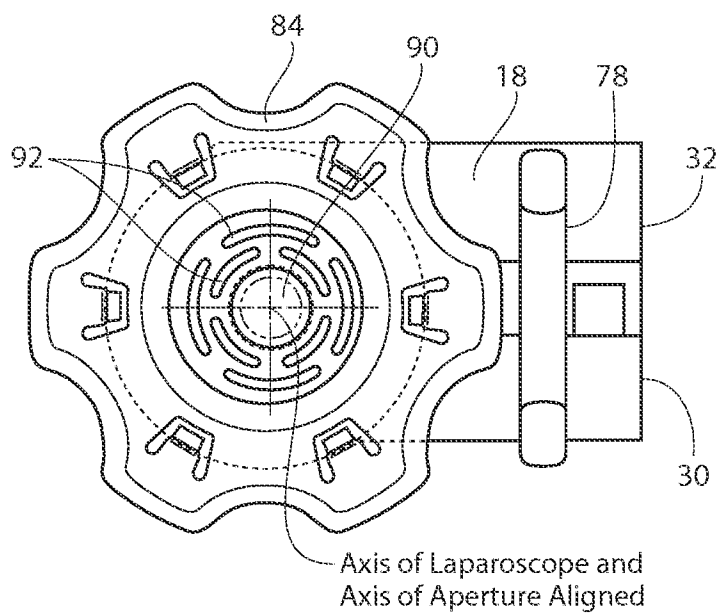


Fig. 22A
UNLOCKED

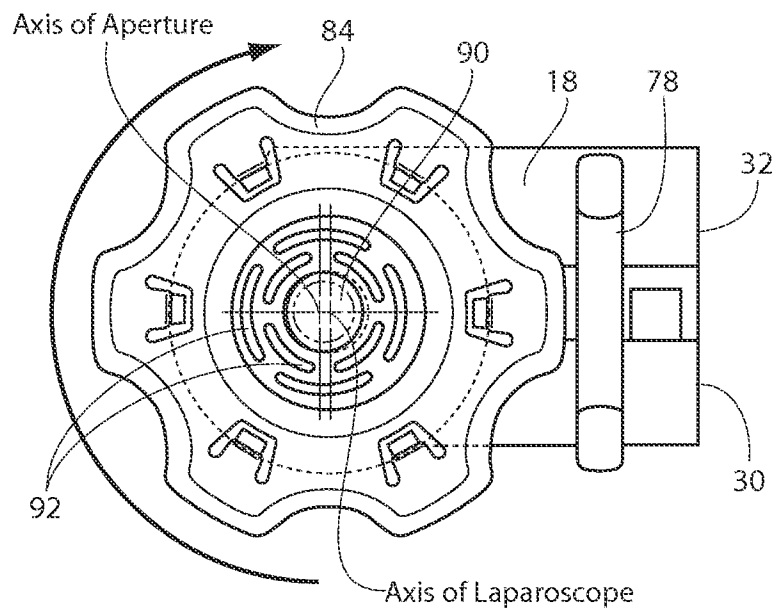


Fig. 22B
LOCKED

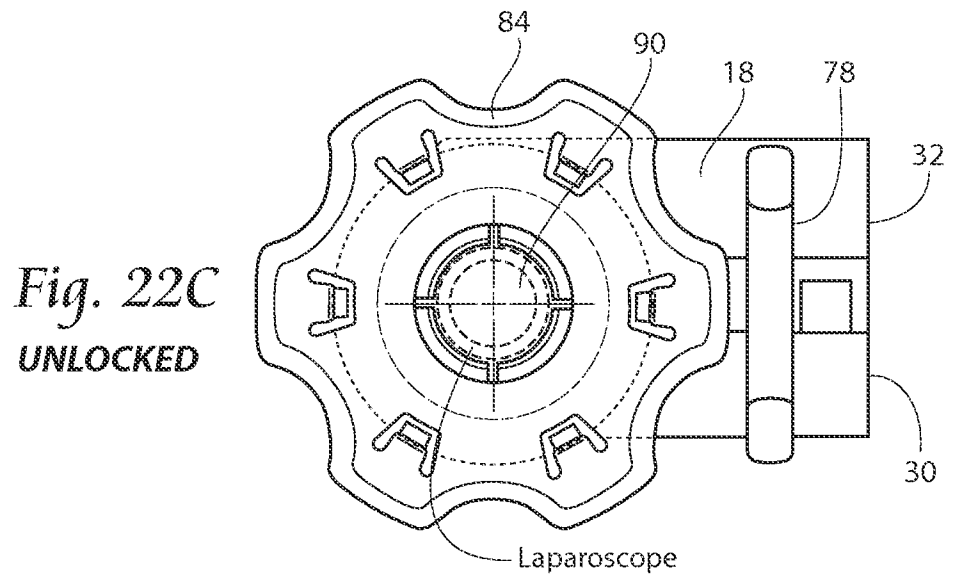


Fig. 22C
UNLOCKED

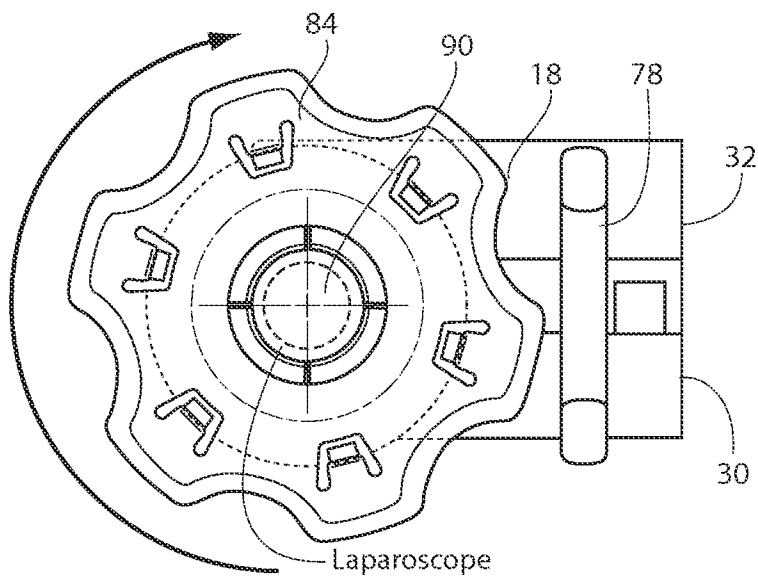


Fig. 22D
LOCKED

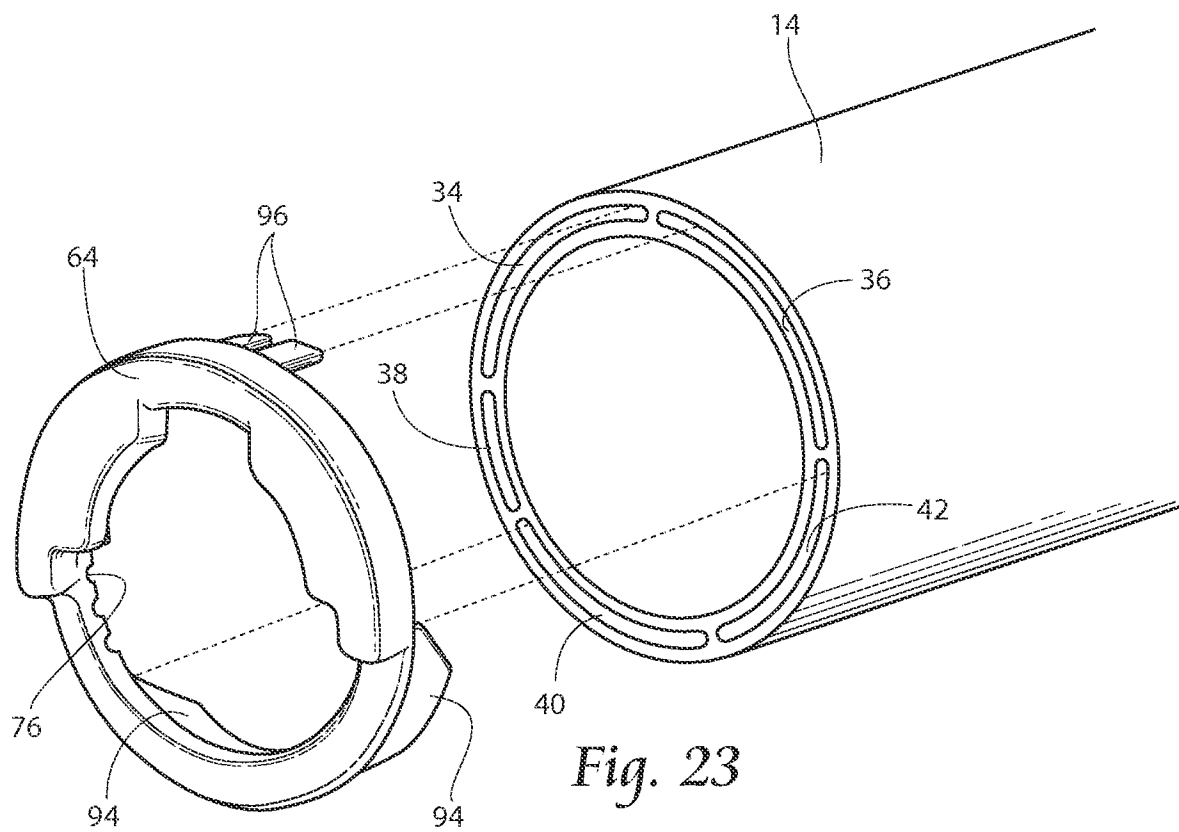


Fig. 23

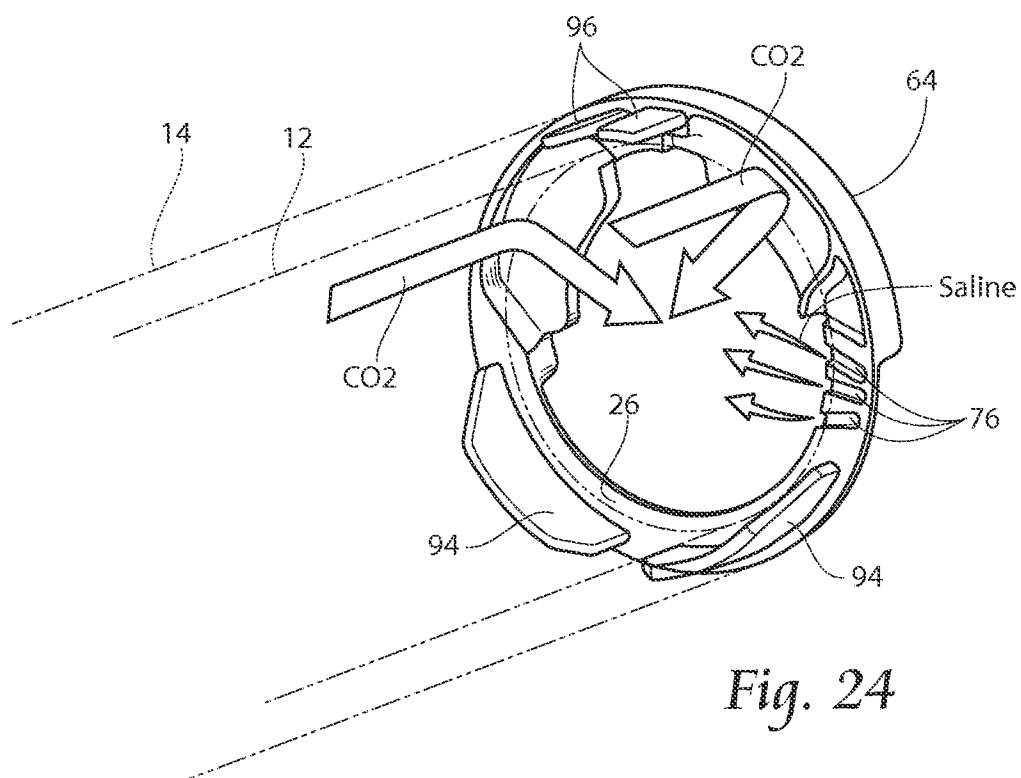
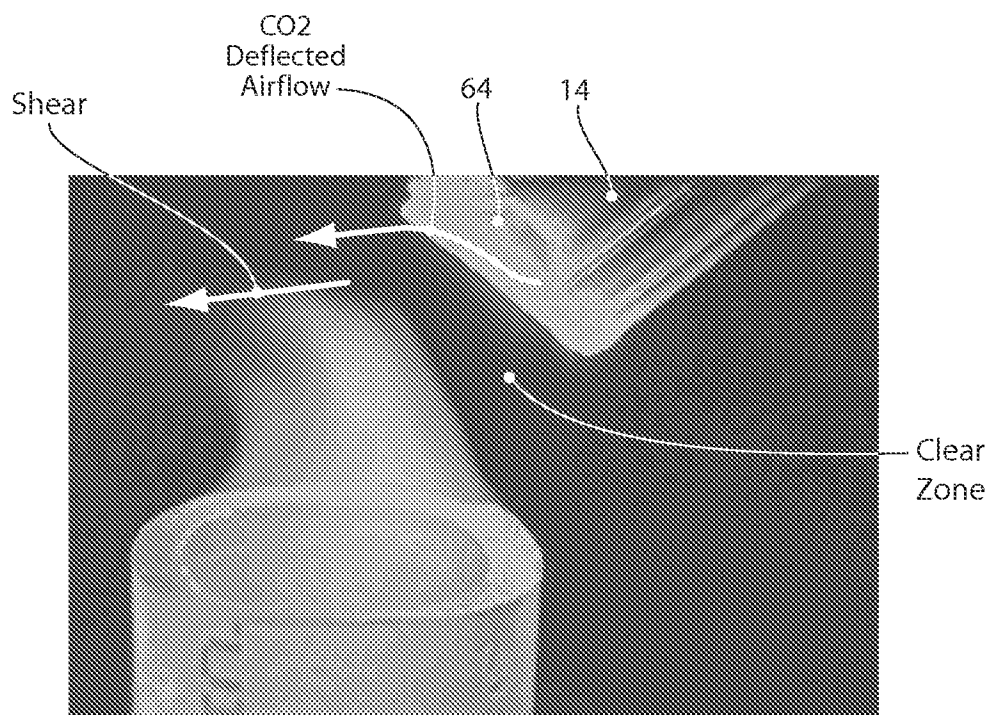
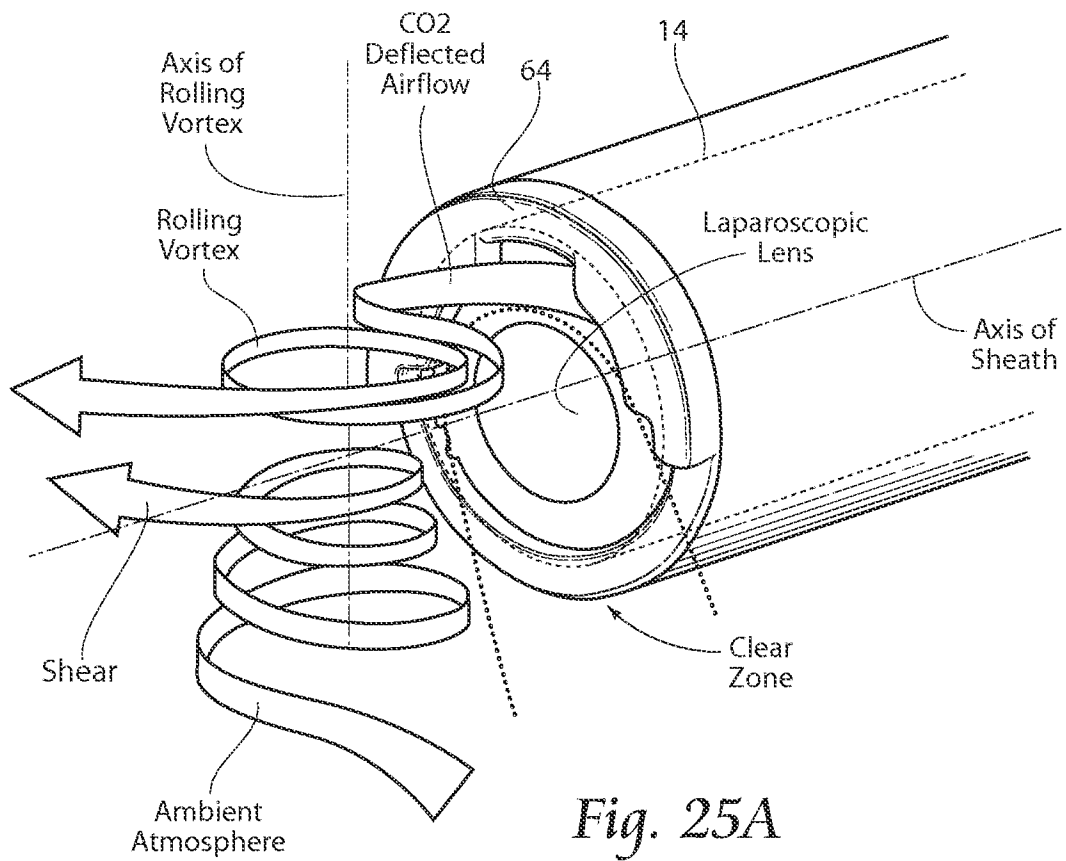
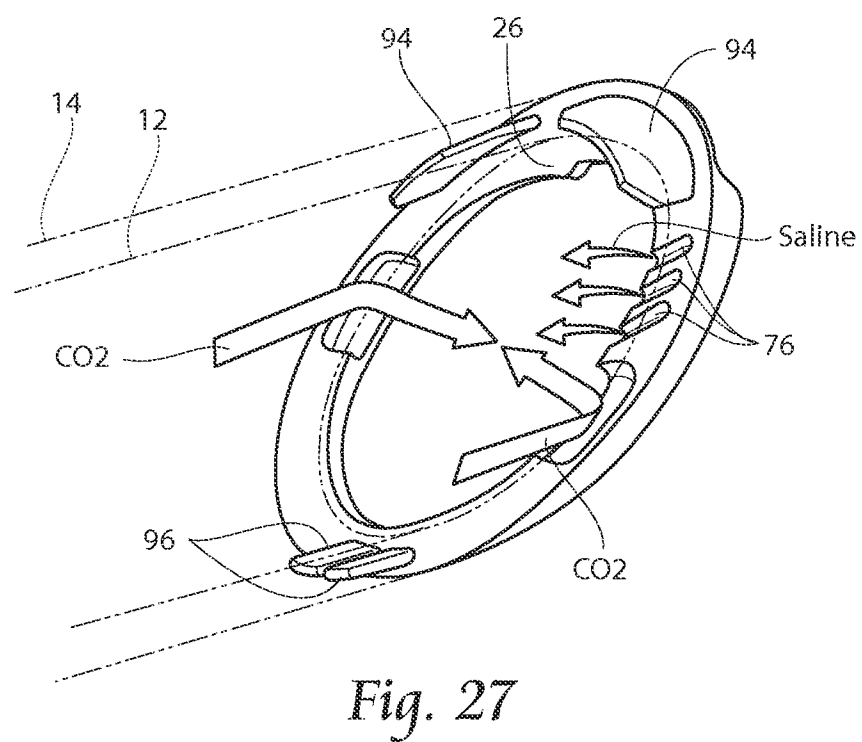
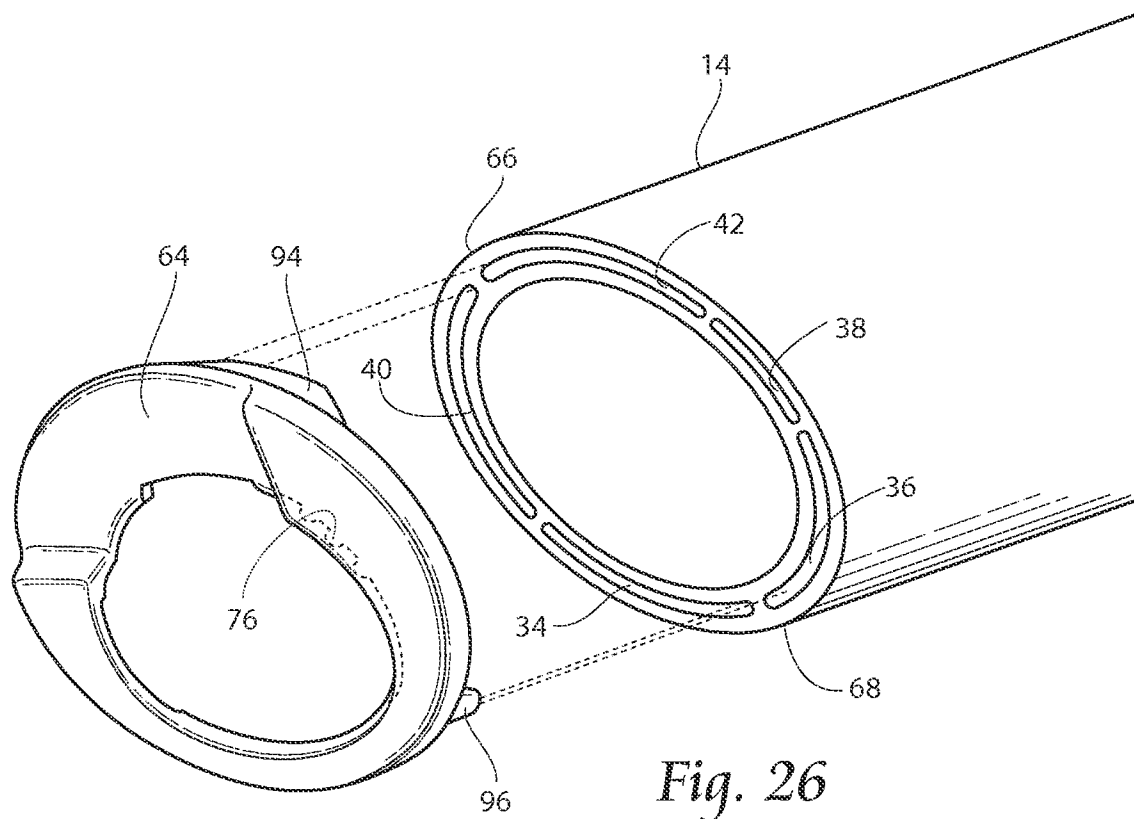
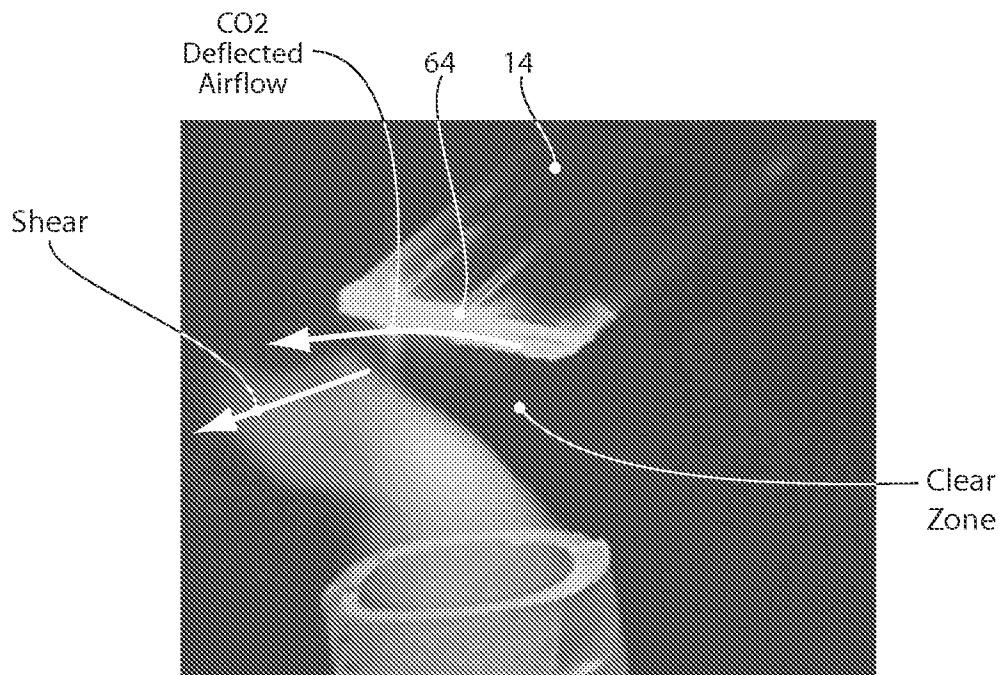
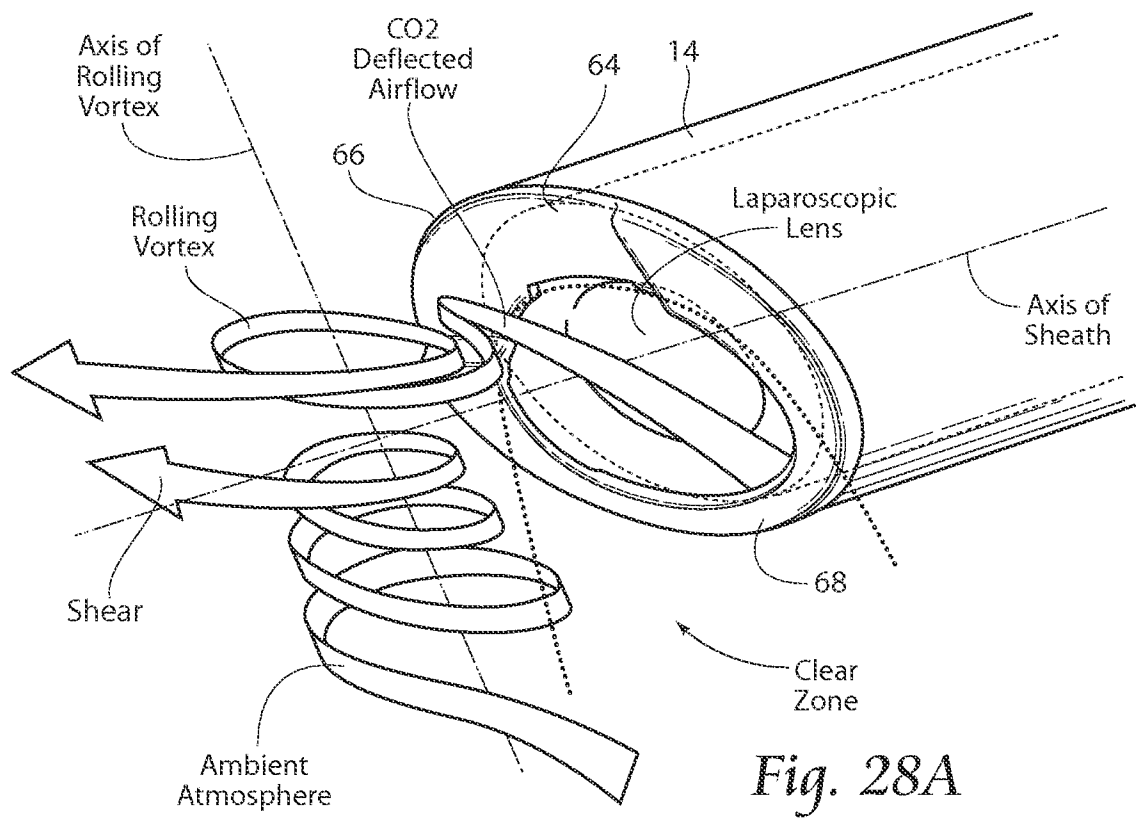
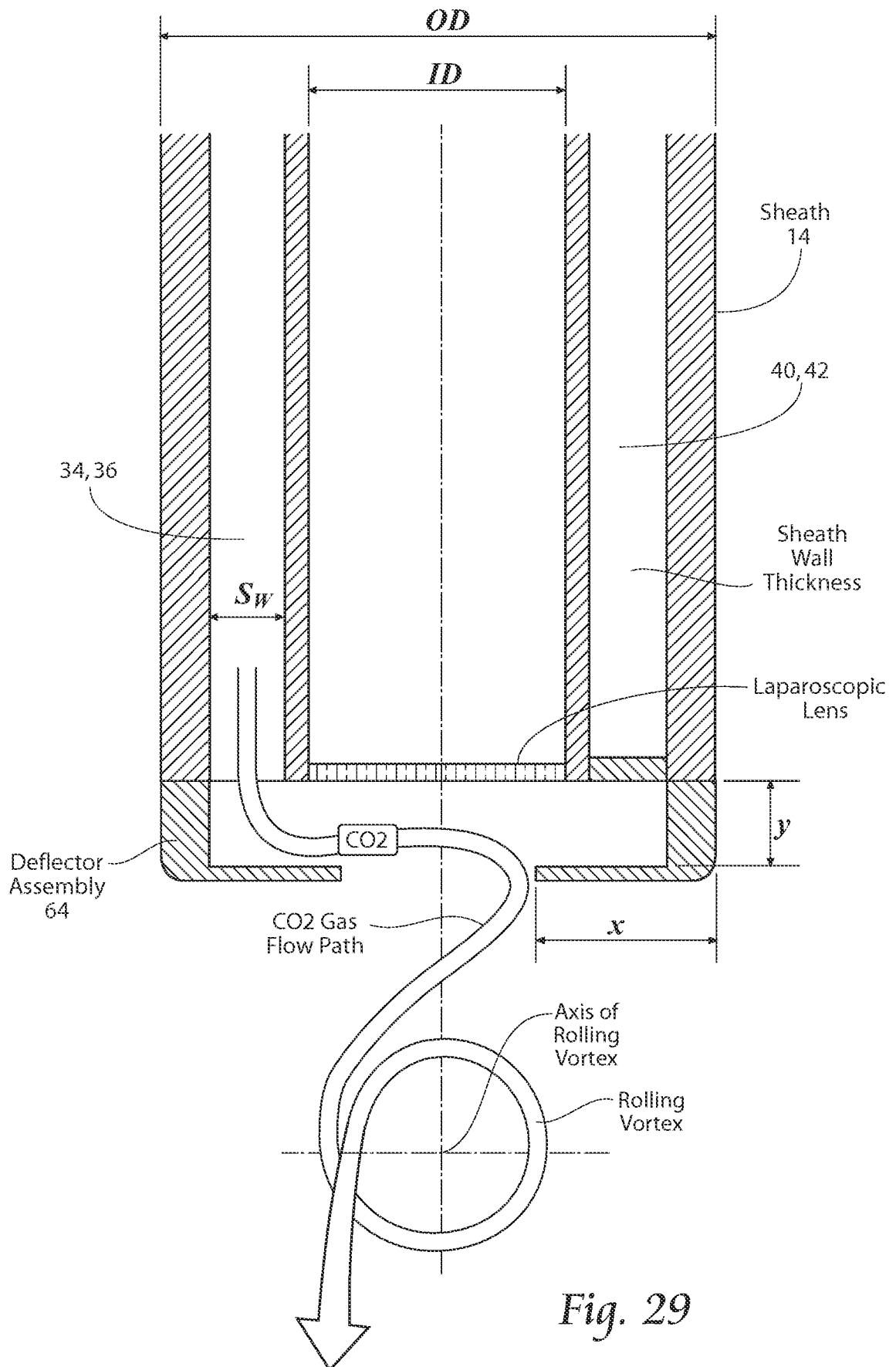


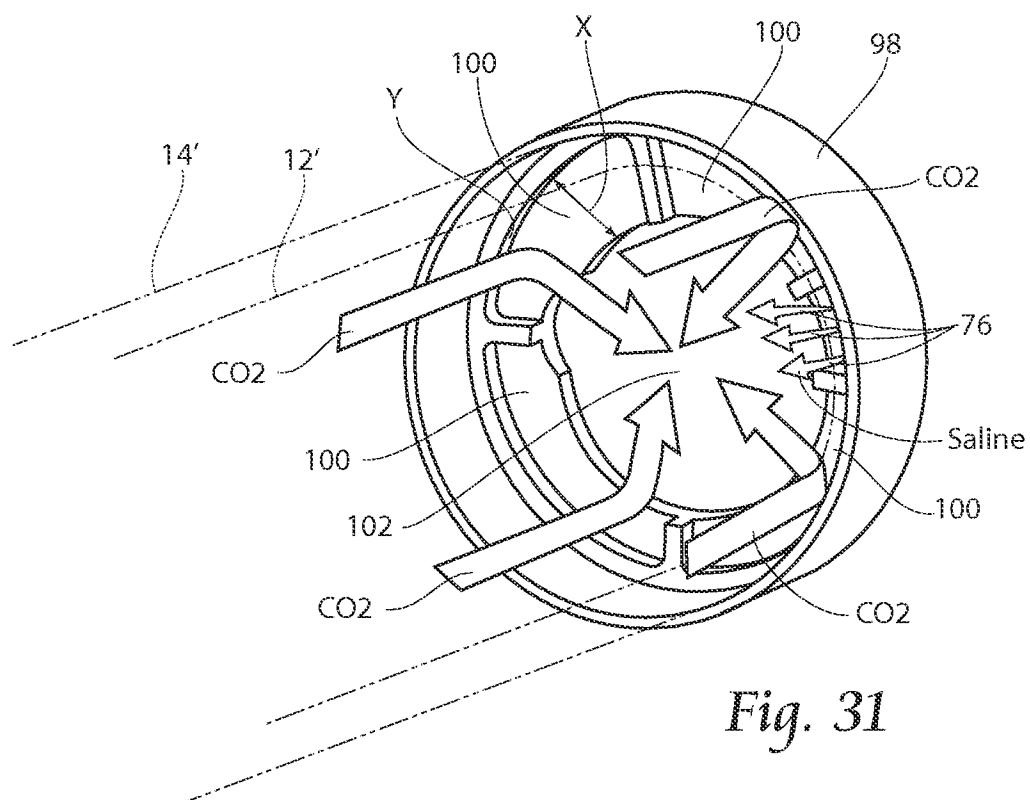
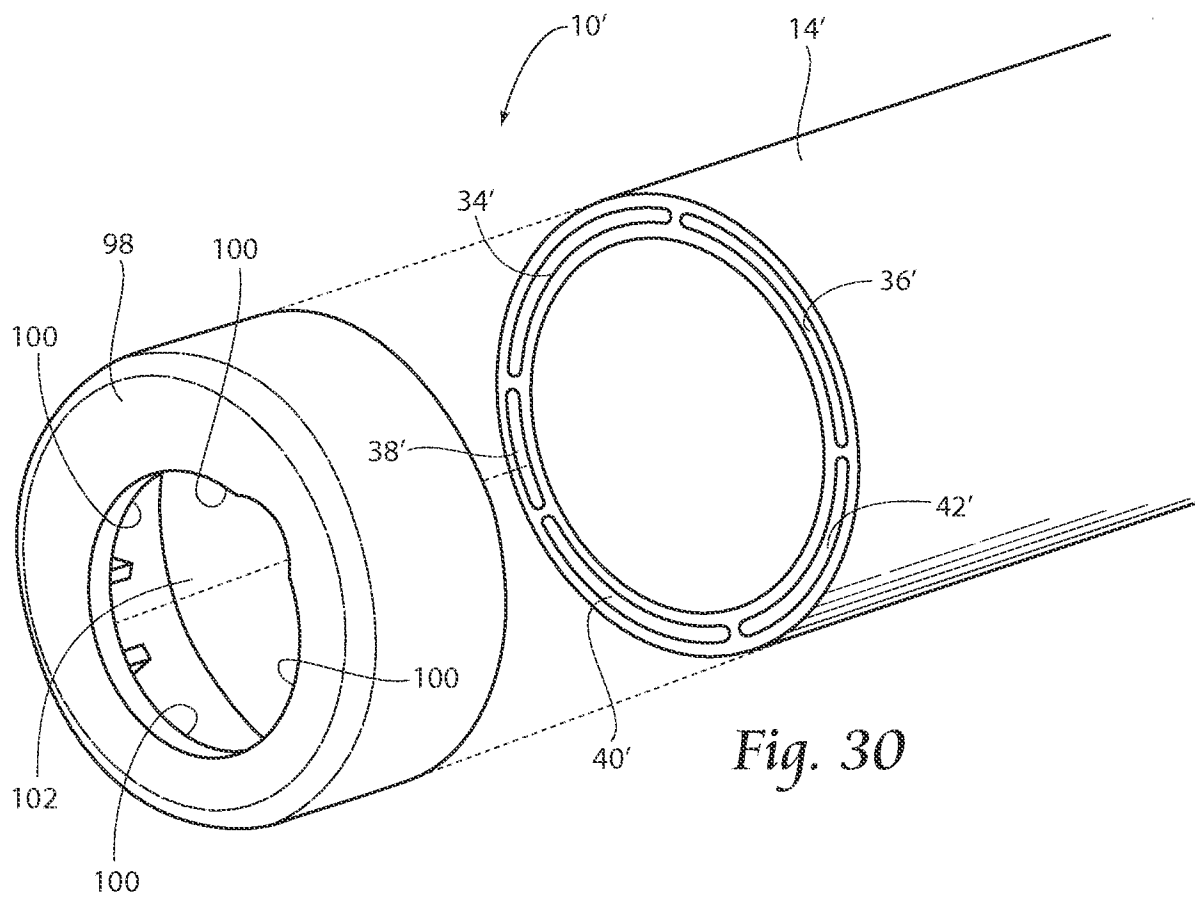
Fig. 24

*Fig. 25B*









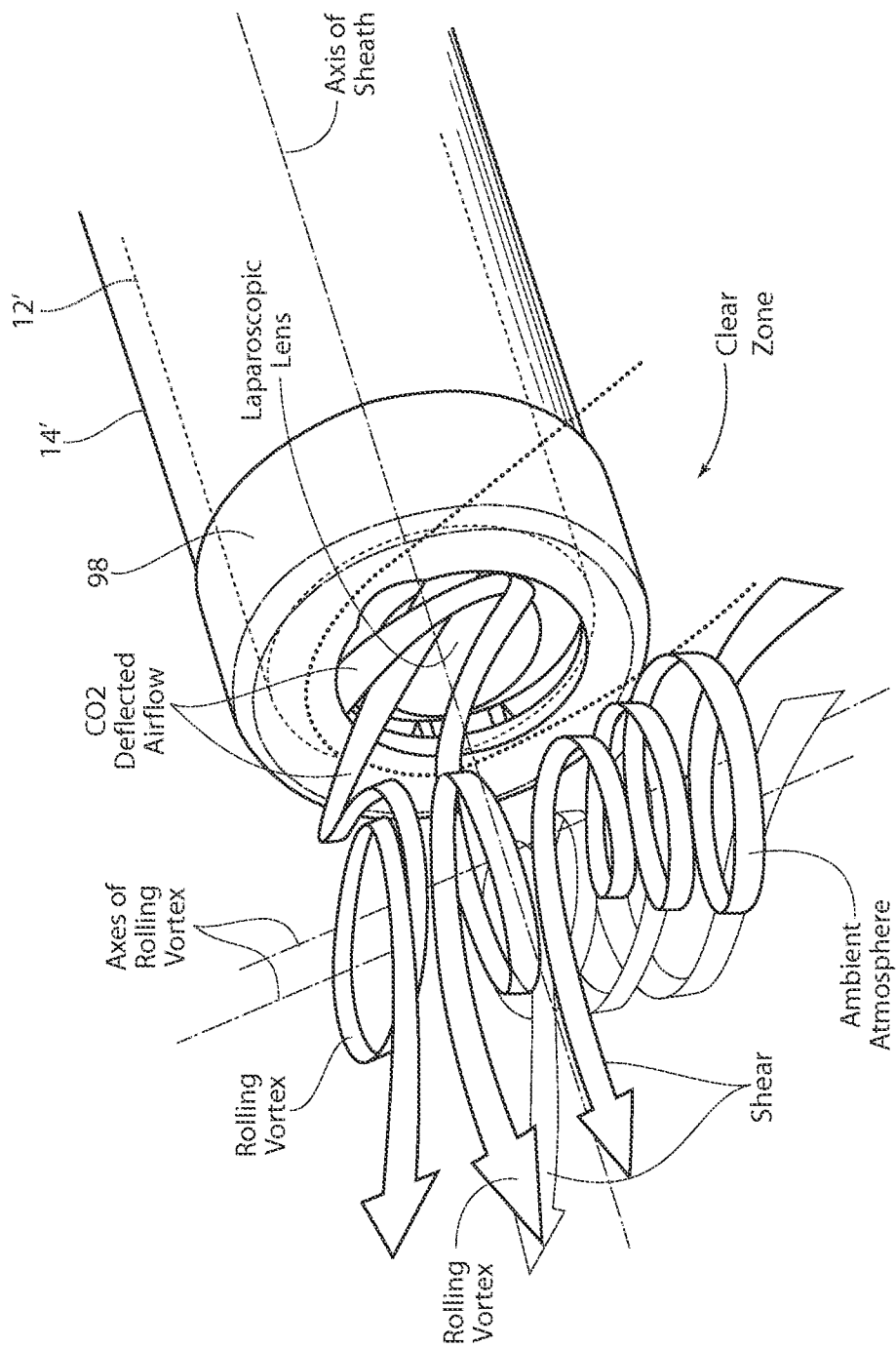
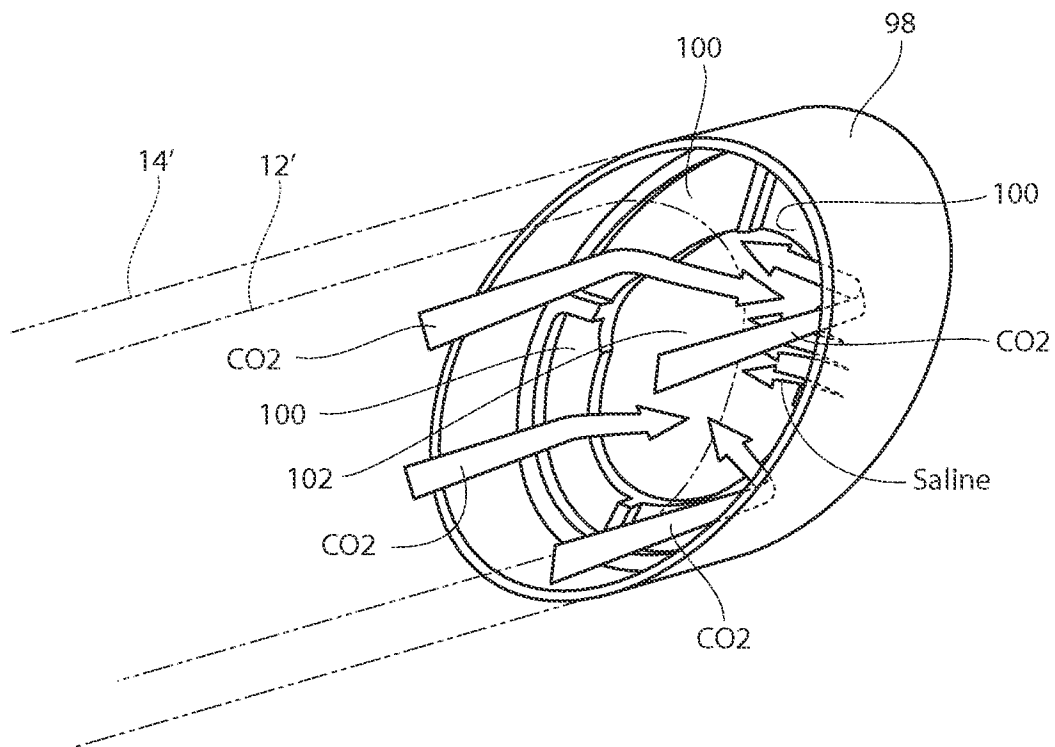
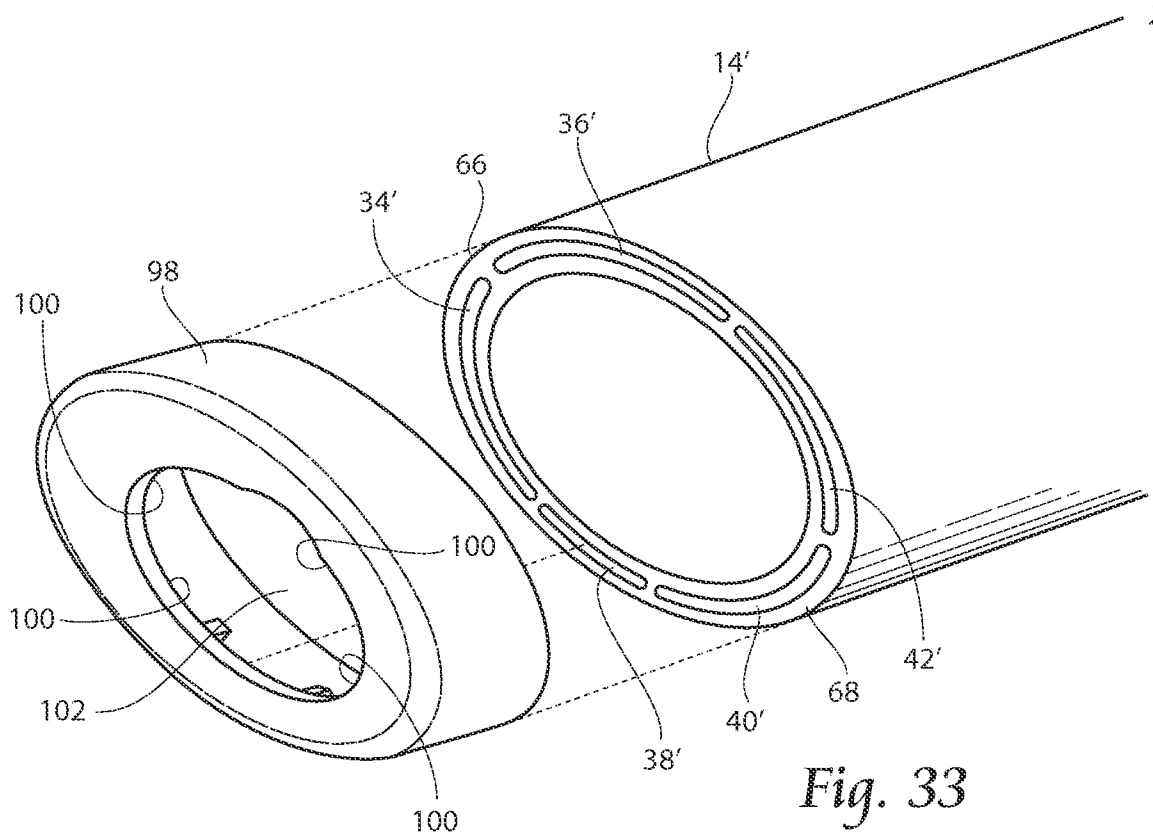


Fig. 32



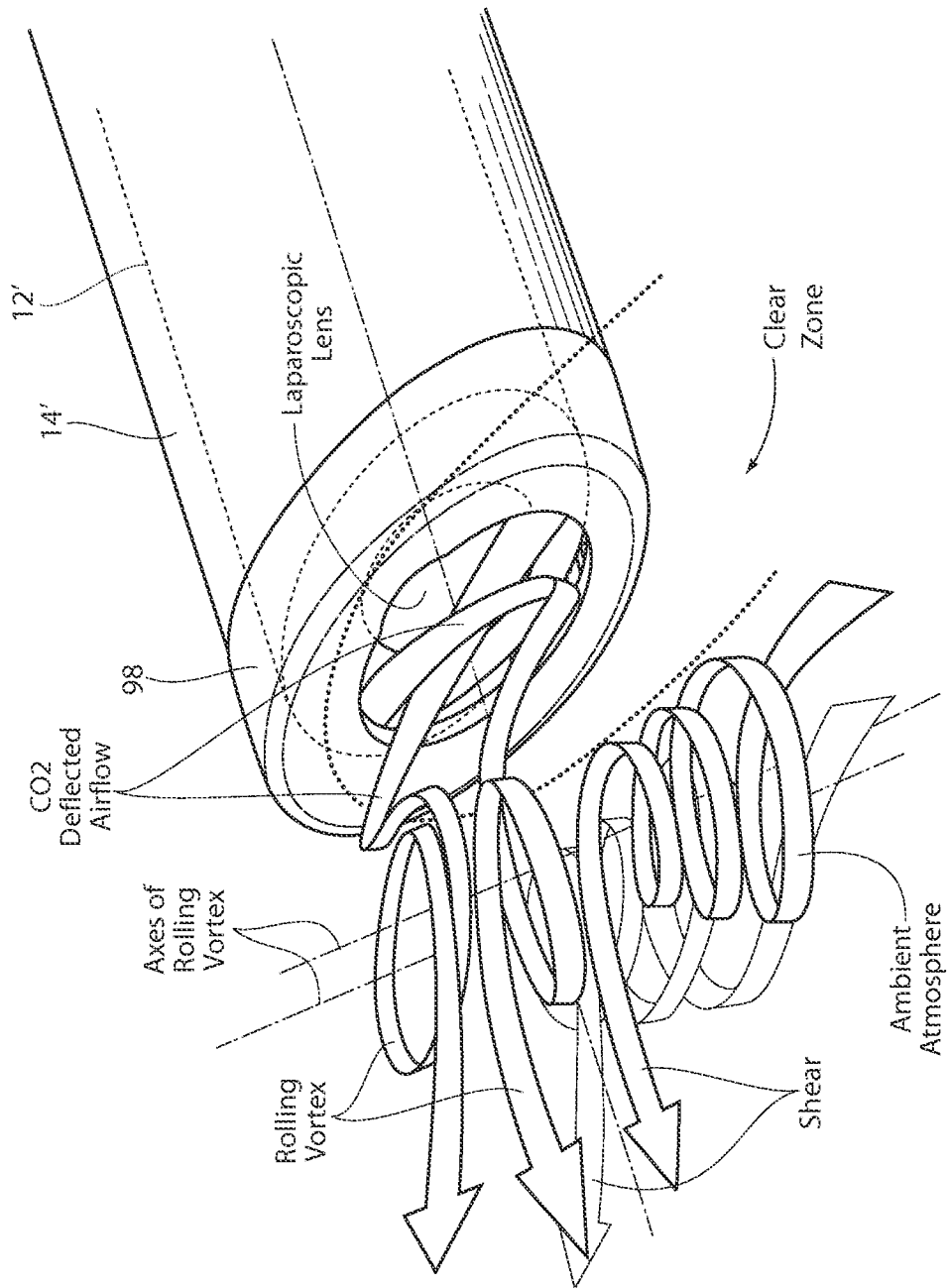


Fig. 35

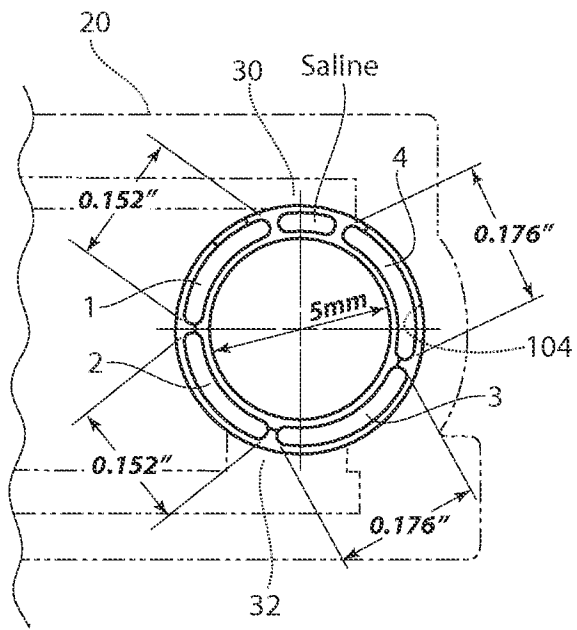


Fig. 36A

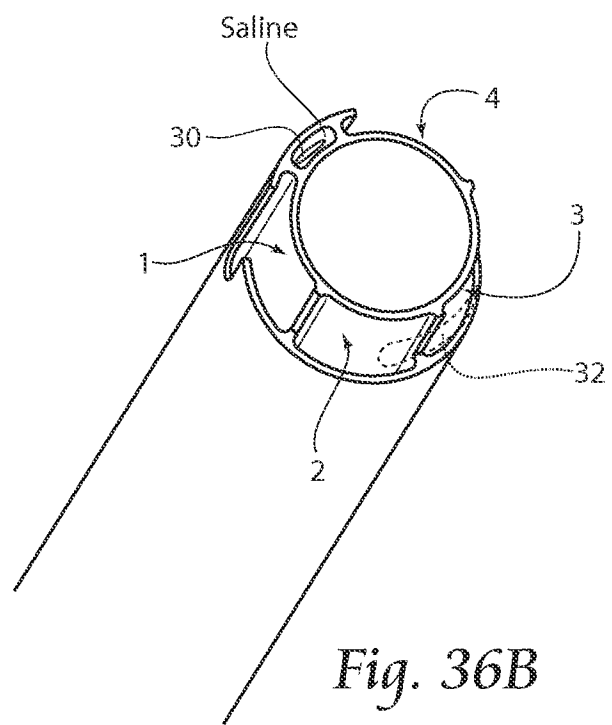


Fig. 36B

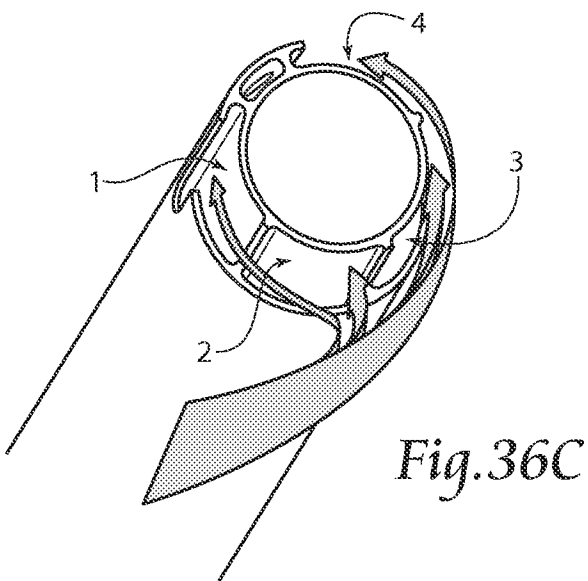


Fig. 36C

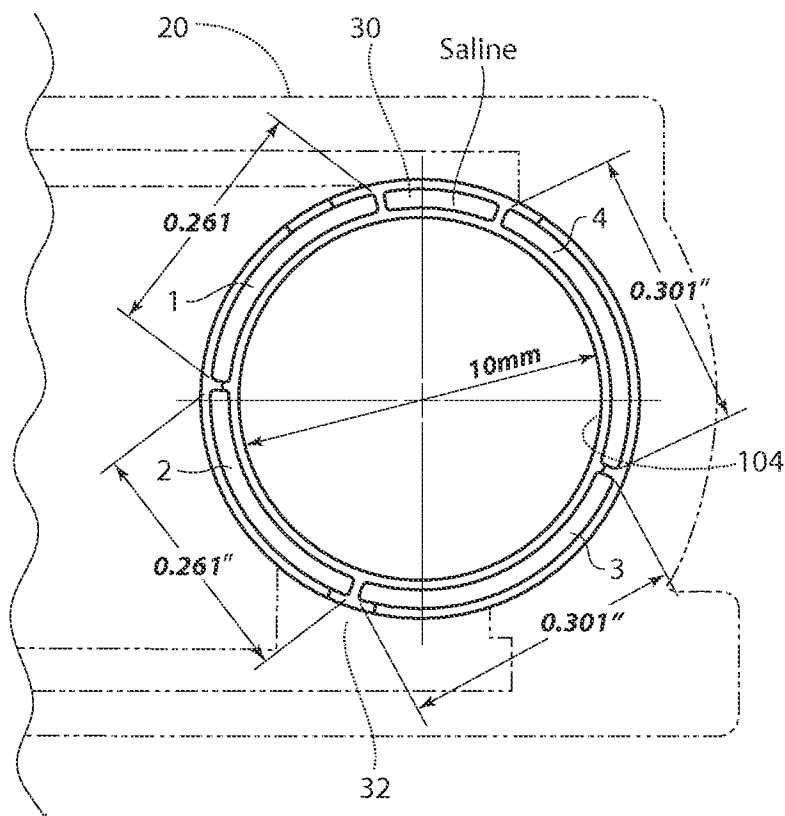


Fig. 37A

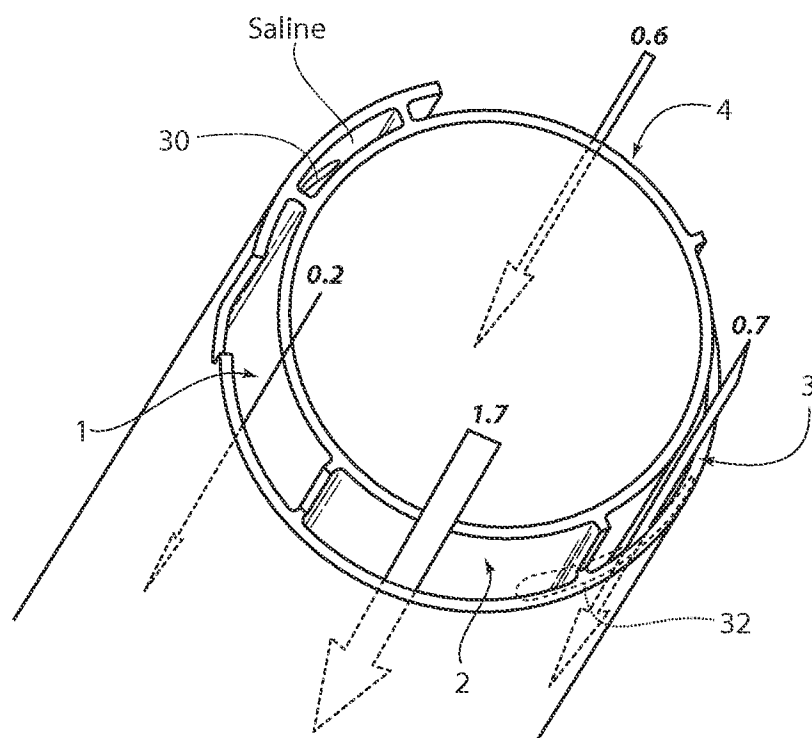


Fig. 37B

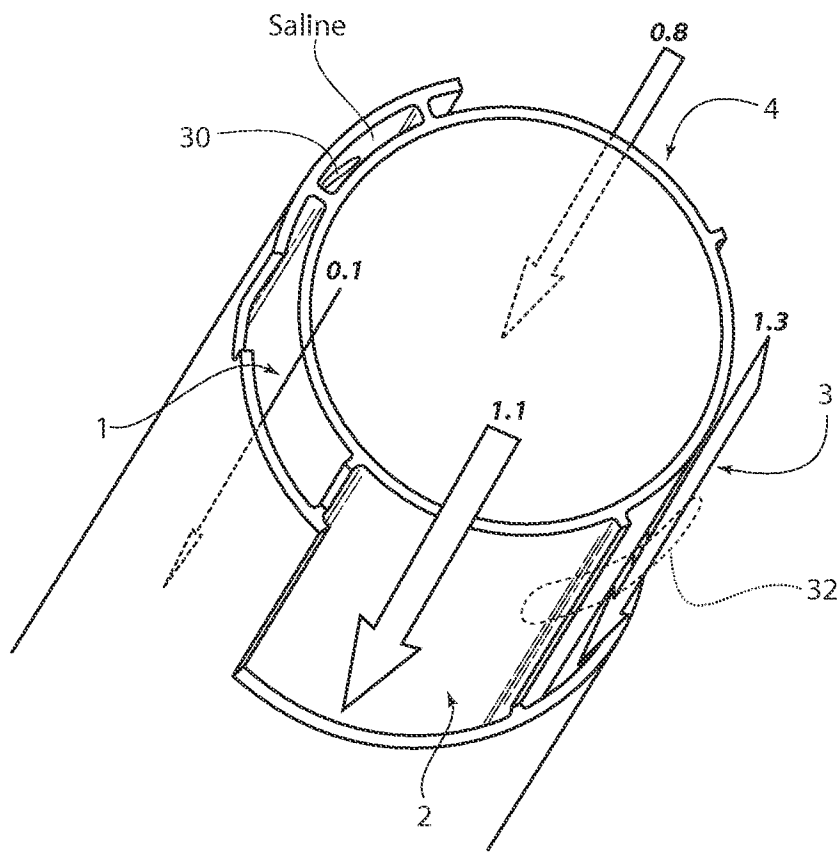


Fig. 38A

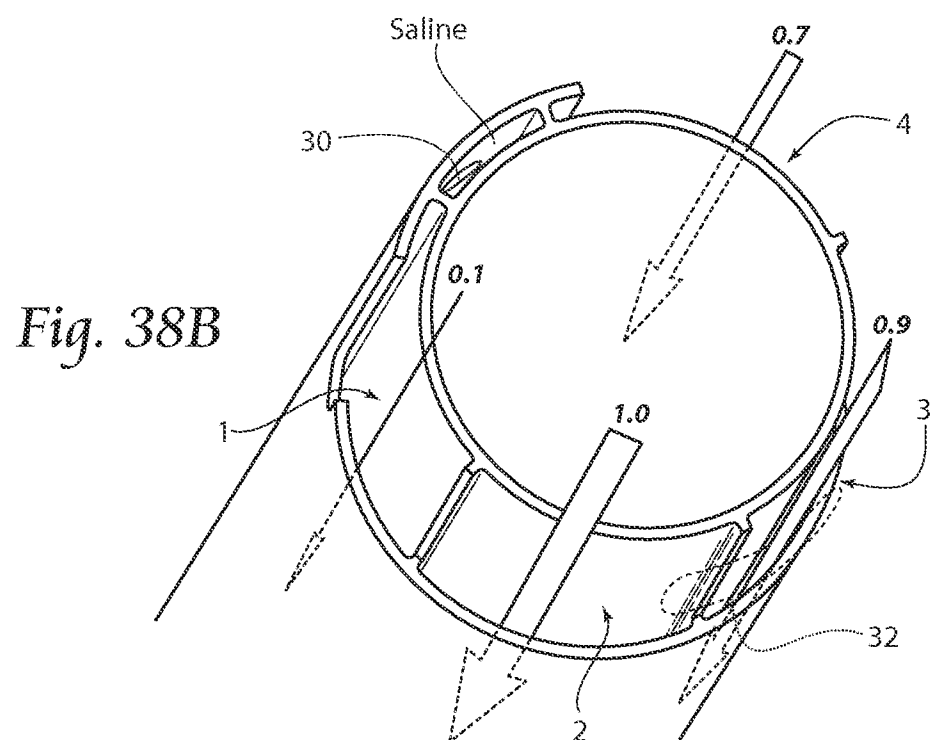
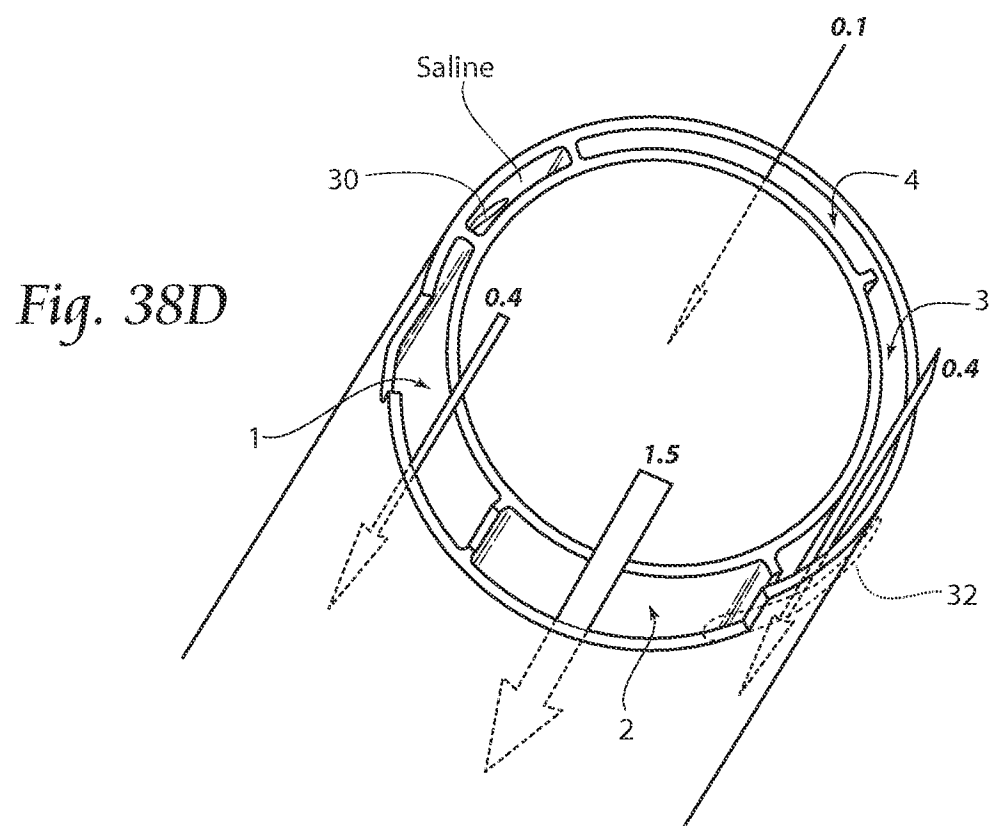
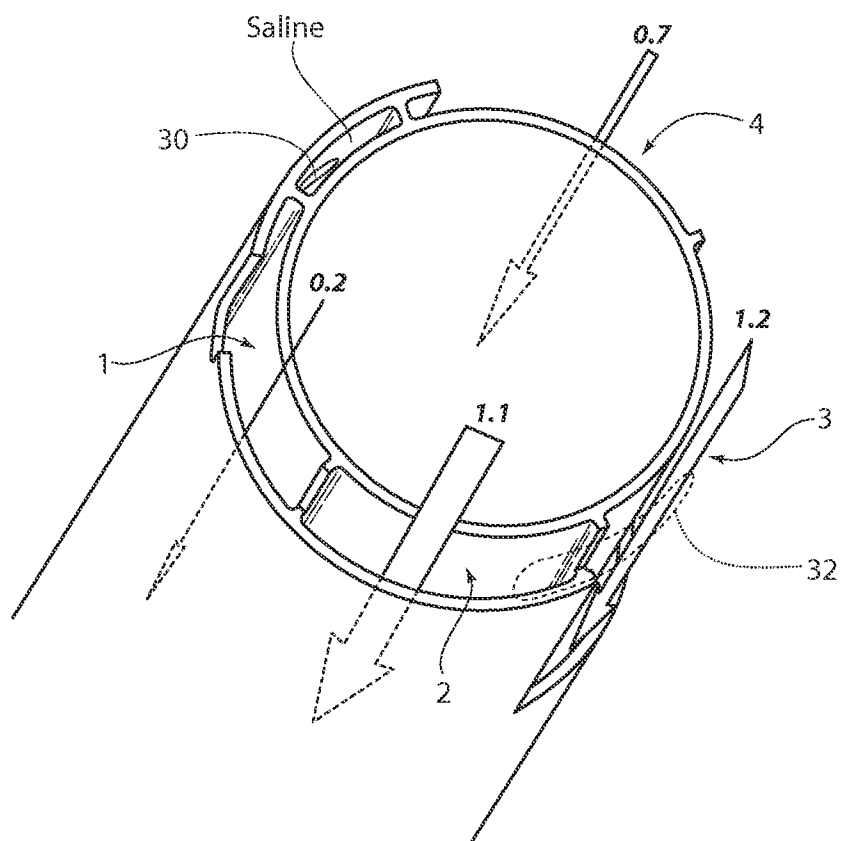


Fig. 38B

27/29



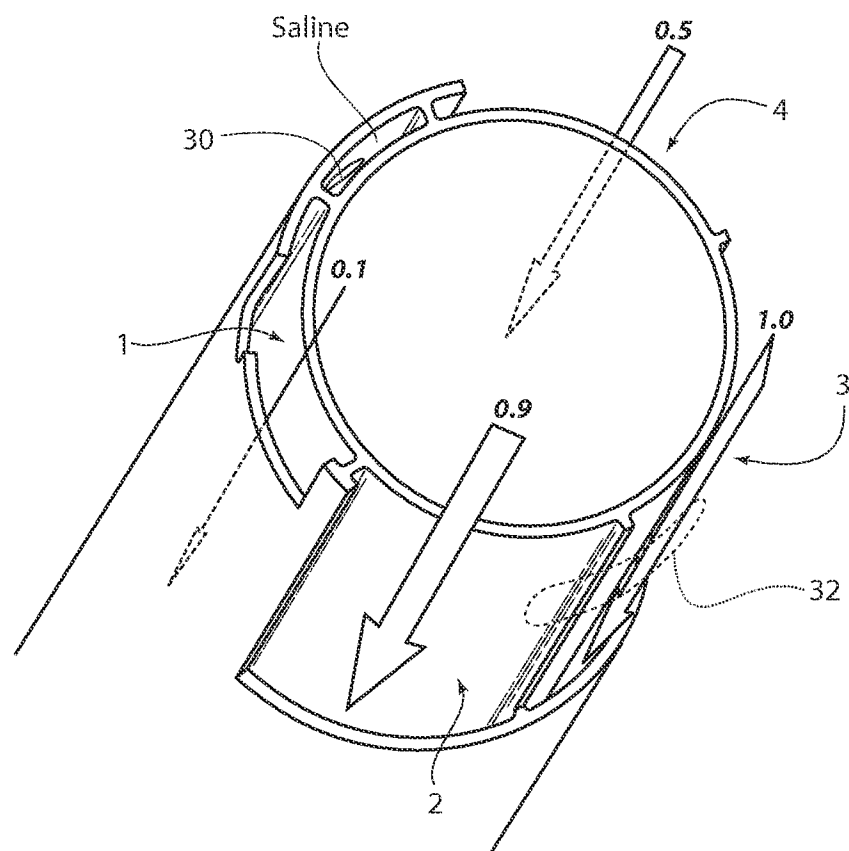


Fig. 39

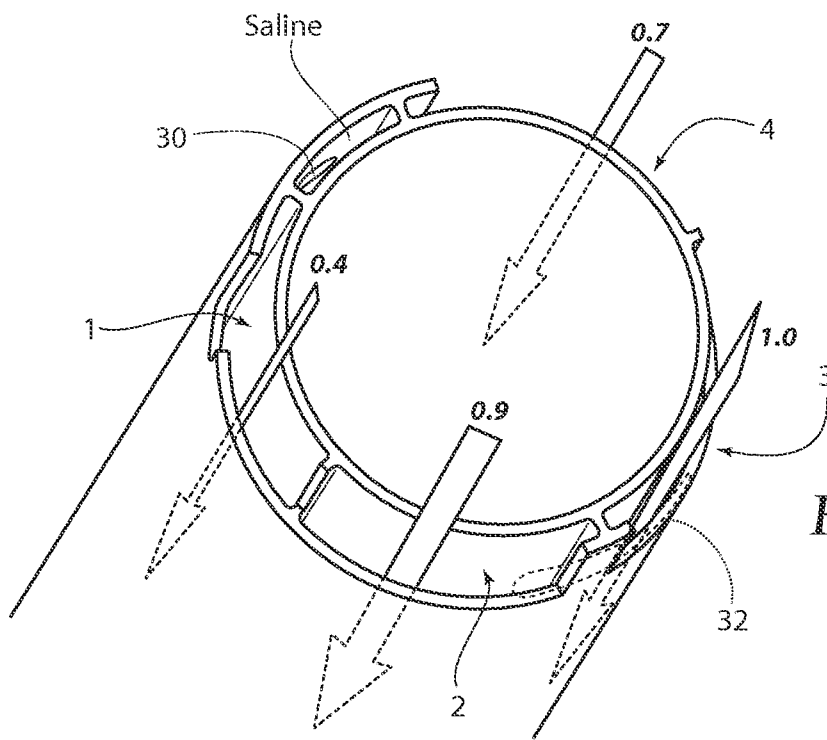


Fig. 40A

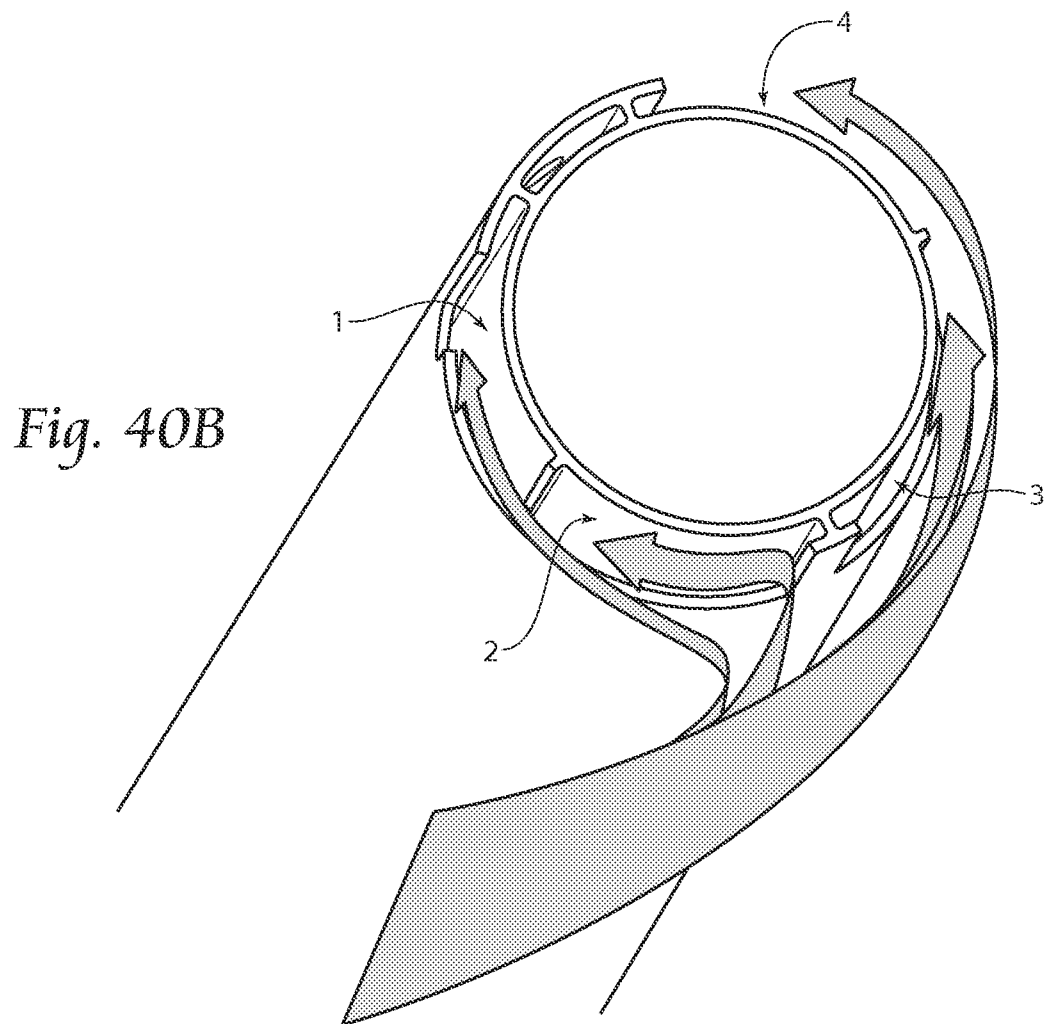


Fig. 40B

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 11/46621

A. CLASSIFICATION OF SUBJECT MATTER

IPC(8) - A61B 1/04 (2011.01)

USPC - 600/123

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

USPC: 600/123

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
USPC: 600/101, 121, 123, 153, 156, 157, 160, 169 (keyword limited; terms below)

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

PubWEST(PGPB, USPT, EPAB, JPAB); Google

Search Terms Used: angle, sheath, sleeve, insufflat\$3, docusate sodium, clean\$3, rins\$3, flush\$3, clear\$3, dioctyl sodium sulfosuccinate, quick, connect, exchange, manifold, bubble, lens, vortex, laparoscope, endoscope, wash\$3, imag\$3, ph, neutral

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2010/0168520 A1 (POLL et al) 01 July 2010 (01.07.2010) fig 2B, 4C-4F, 5A-5C, 9A-9B, 14, 18C, para [0041], [0058], [0065]-[0068], [0073], [0080], [0089], [0093], [0097], [0099], [0101], [0105]-[0106], [0130], [0139]	20-21
Y		1-19, 22-25
Y	US 5,339,800 A (WIITA et al) 23 August 1994 (23.08.1994) fig 5, abstract	1-19
Y	US 4,637,814 A (LEIBOFF) 20 January 1987 (20.01.1987) col 7, ln 50-55	22-25
Y	US 6,447,446 B1 (SMITH et al) 10 September 2002 (10.09.2002) col 4, ln 18-23	3-4

☐ Further documents are listed in the continuation of Box C.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

22 November 2011 (22.11.2011)

Date of mailing of the international search report

06 DEC 2011

Name and mailing address of the ISA/US

Mail Stop PCT, Attn: ISA/US, Commissioner for Patents
P.O. Box 1450, Alexandria, Virginia 22313-1450

Facsimile No. 571-273-3201

Authorized officer:

Lee W. Young

PCT Helpdesk: 571-272-4300
PCT OSP: 571-272-7774

专利名称(译)	用于在手术镜的使用期间优化和维持手术视野的可视化的系统和方法		
公开(公告)号	EP2600759A4	公开(公告)日	2013-08-28
申请号	EP2011815331	申请日	2011-08-04
[标]申请(专利权)人(译)	微创设备有限公司		
申请(专利权)人(译)	微创器械有限责任公司		
当前申请(专利权)人(译)	微创器械有限责任公司		
[标]发明人	DRACH GREGORY POLL WAYNE L		
发明人	DRACH, GREGORY POLL, WAYNE, L.		
IPC分类号	A61B1/04		
CPC分类号	A61B1/0008 A61B1/00091 A61B1/00101 A61B1/00119 A61B1/00128 A61B1/00135 A61B1/015 A61B1/126 A61B1/127 A61B1/3132 A61B17/3474 A61B2017/347 A61M13/003 A61M2202/0225 A61M2205/3344		
优先权	61/400900 2010-08-04 US 61/452982 2011-03-15 US		
其他公开文献	EP2600759A1		
外部链接	Espacenet		

摘要(译)

一种视图优化组件，方法和套件，其与腹腔镜结合使用，所述腹腔镜具有位于腹腔镜的轴尖上的透镜，以及吹入CO₂的源。本发明包括多腔护套组件，与护套组件的内腔流体连通的偏转器组件，其中通过内腔的CO₂流与偏转器组件接触时形成涡流，从而防止腹腔镜雾化镜片。