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(54) **ULTRASOUND TRANSDUCER AND ELECTRONIC DEVICE**

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H01L 41/04 (2006.01)
A61B 8/00 (2006.01)

(52) **U.S. Cl.** **310/344**; 367/181; 600/437; 600/459

(58) **Field of Classification Search** 310/334; 367/181; 600/437, 459
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

7,275,298	B2 *	10/2007	Schindel	29/594
7,940,603	B2 *	5/2011	Adachi et al.	367/181
2007/0057603	A1 *	3/2007	Azuma et al.	310/334
2007/0161896	A1 *	7/2007	Adachi et al.	600/437
2009/0058228	A1 *	3/2009	Wakabayashi et al.	310/334
2009/0202083	A1 *	8/2009	Kageyama	381/59
2011/0108838	A1 *	5/2011	Kageyama	257/49

FOREIGN PATENT DOCUMENTS

EP	1 781 067	A1	5/2007
EP	2030698	A1 *	3/2009
JP	2005-510264		4/2005
JP	2006-319713		11/2006
WO	03/035281	A2	5/2003

OTHER PUBLICATIONS

Abstract of WO 03/011749 A2, dated Feb. 13, 2003.

* cited by examiner

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(57) **ABSTRACT**

An ultrasound transducer includes a substrate, an ultrasound transducer cell placed on one surface of the substrate and having a lower electrode, a first gap portion placed on the lower electrode and an upper electrode placed on the first gap portion, a first conductive layer placed on the other surface of the substrate and electrically connected to one of the lower electrode and the upper electrode, an electret film placed on the first conductive layer, an insulating layer placed on the electret film, and a second conductive layer placed on the insulating layer and electrically connected to the one of the lower electrode and the upper electrode not electrically connected to the first conductive layer.

10 Claims, 8 Drawing Sheets

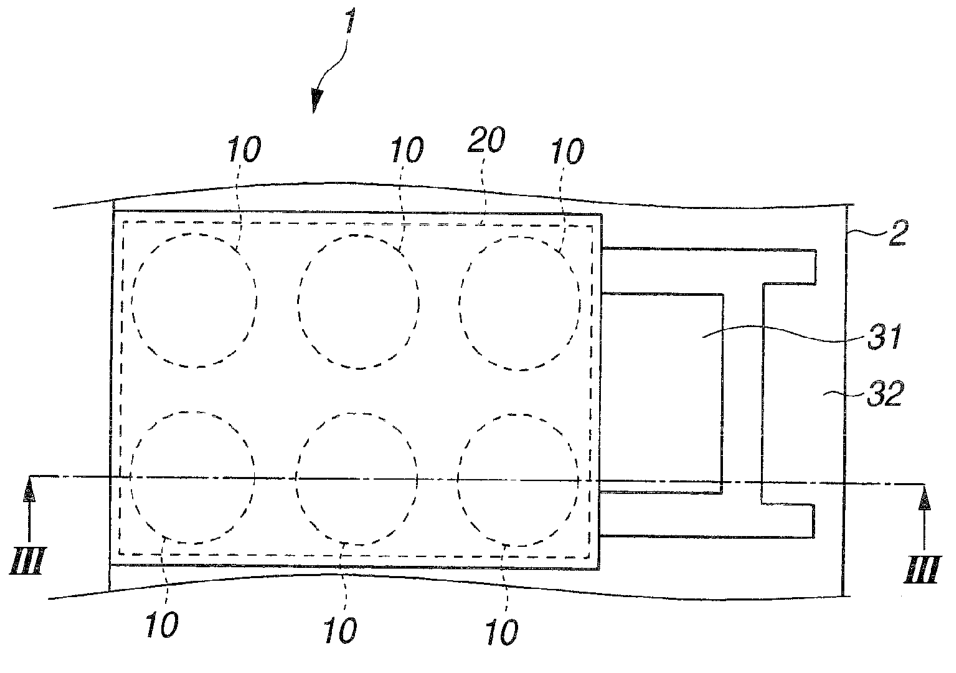


FIG.1

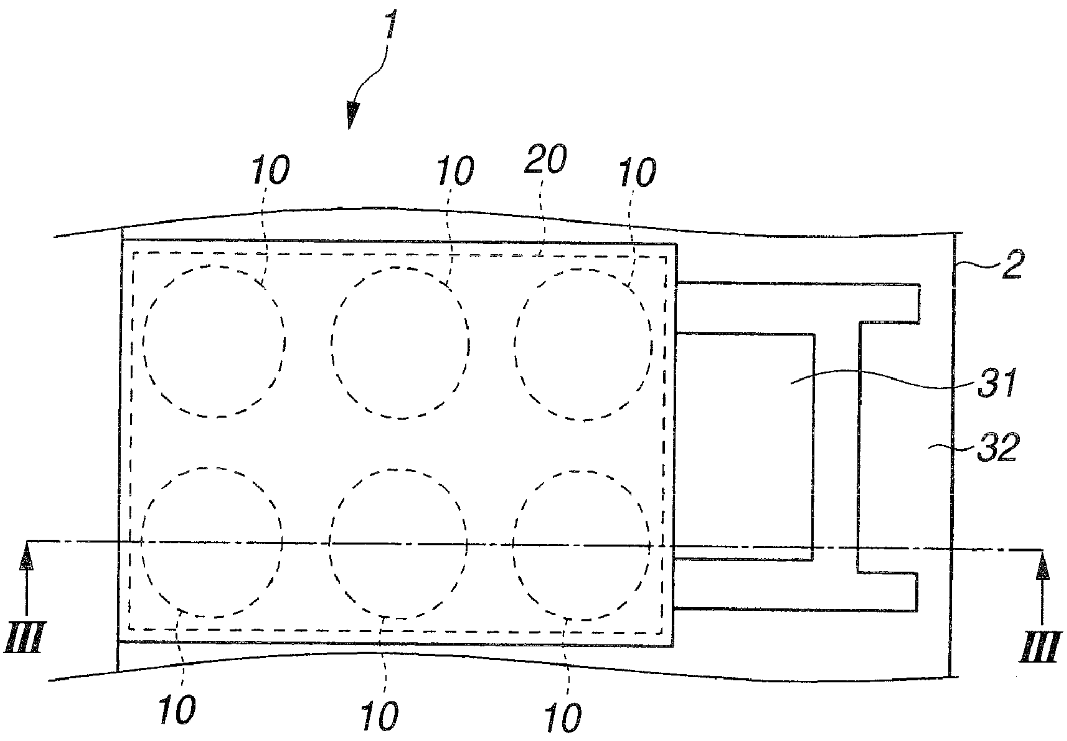


FIG.2

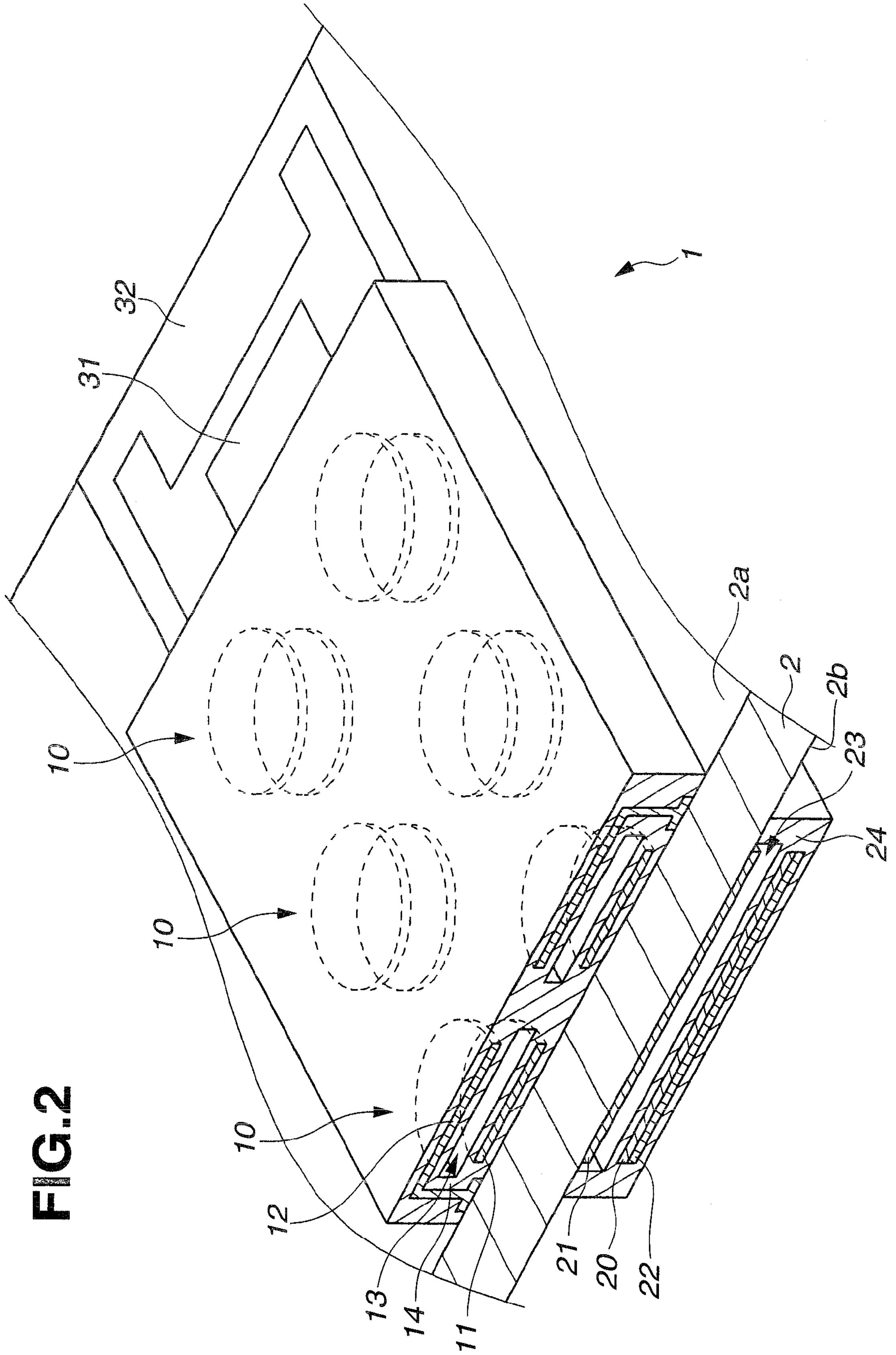


FIG.3

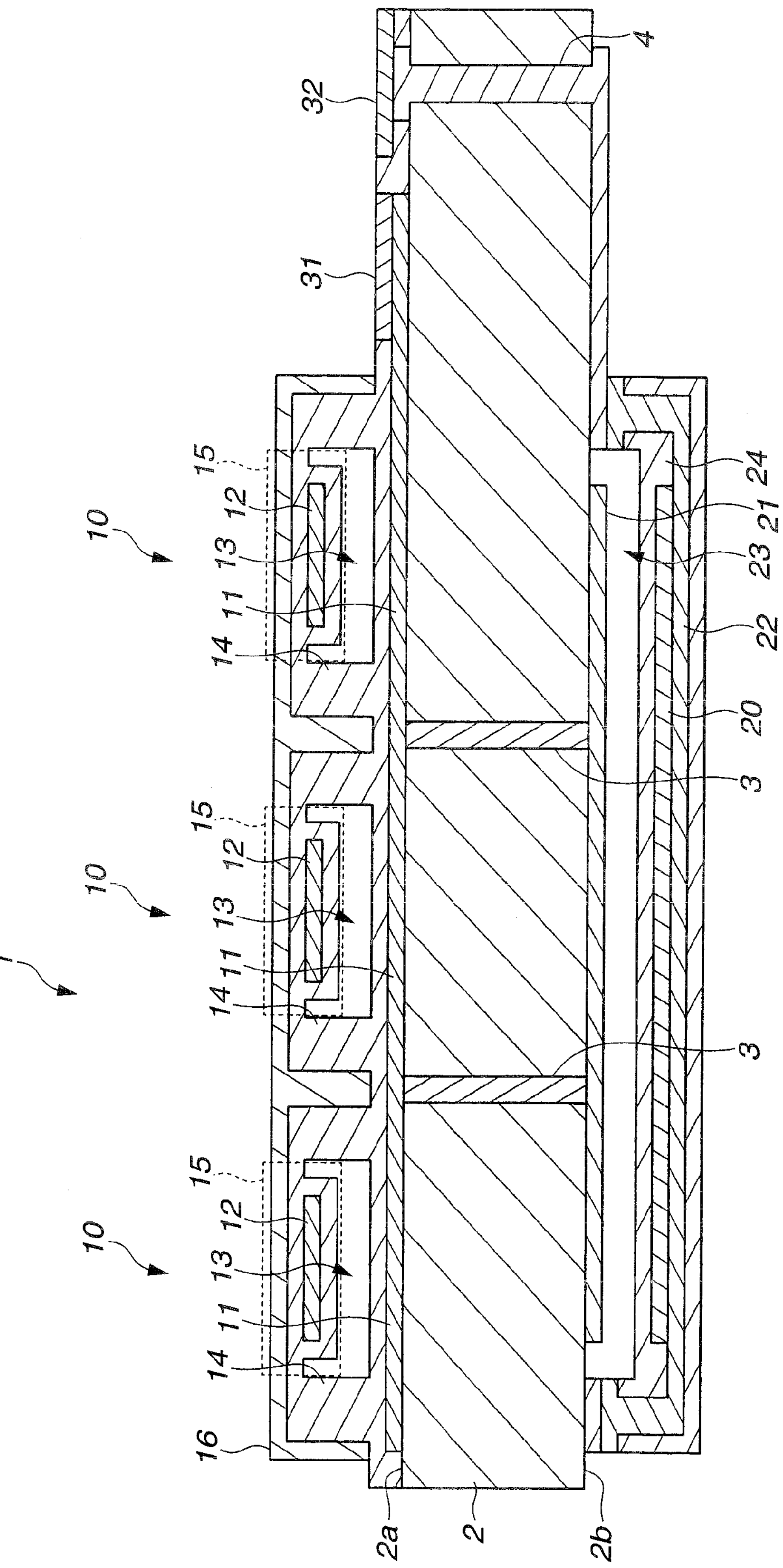


FIG.4

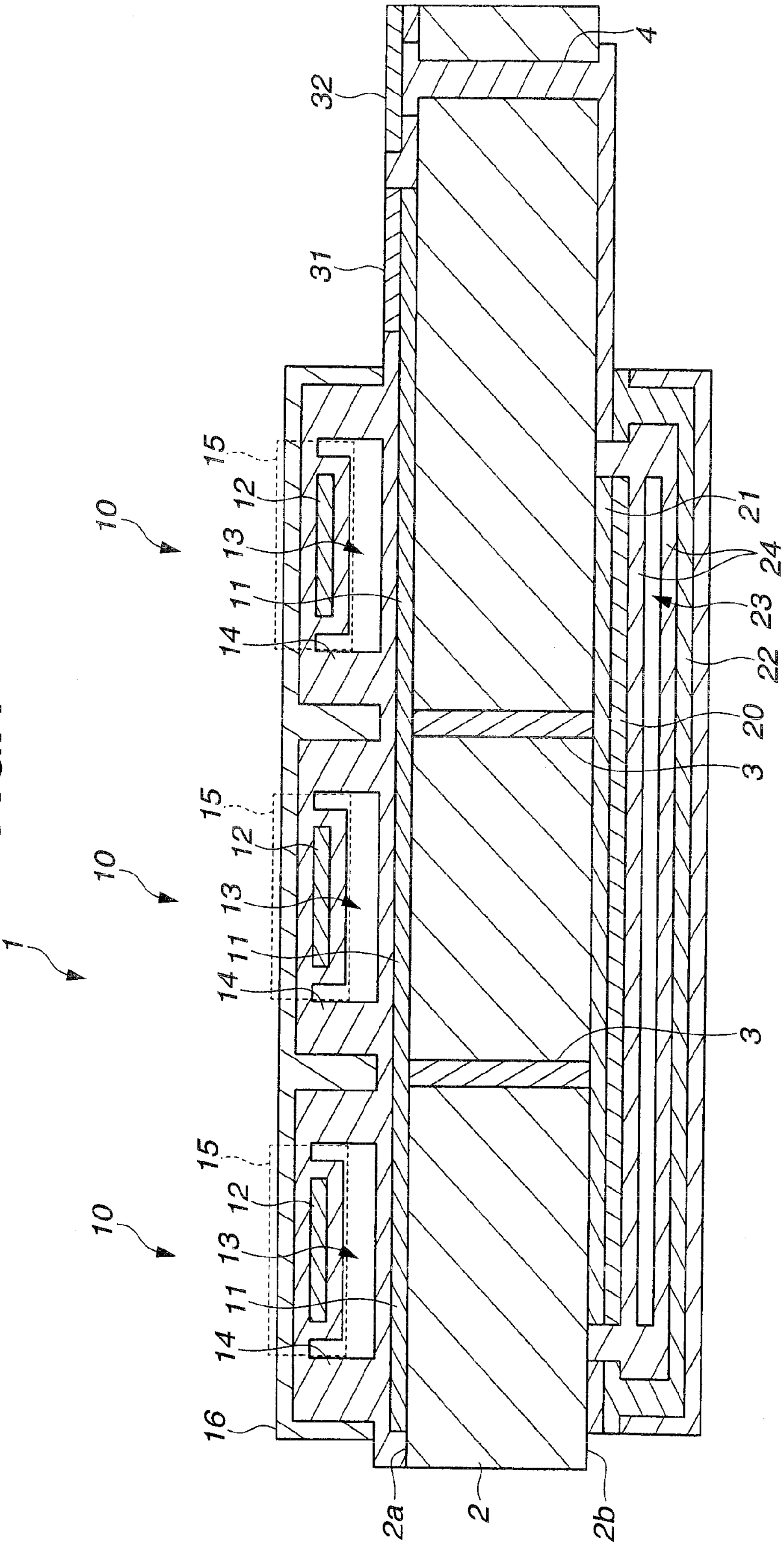
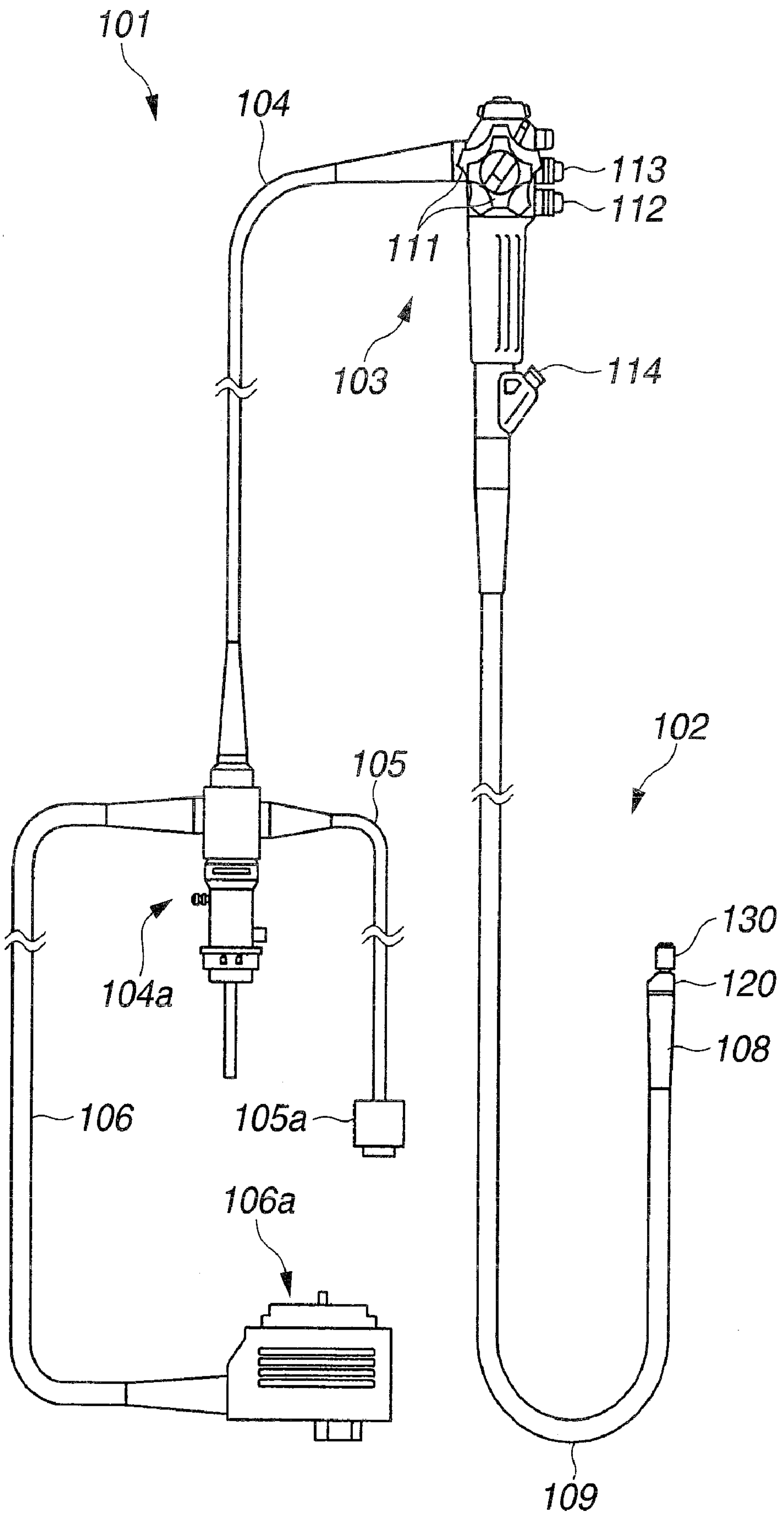


FIG.5


101
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103
114
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105
104a
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120
108
106
105a
106a
109

FIG.6

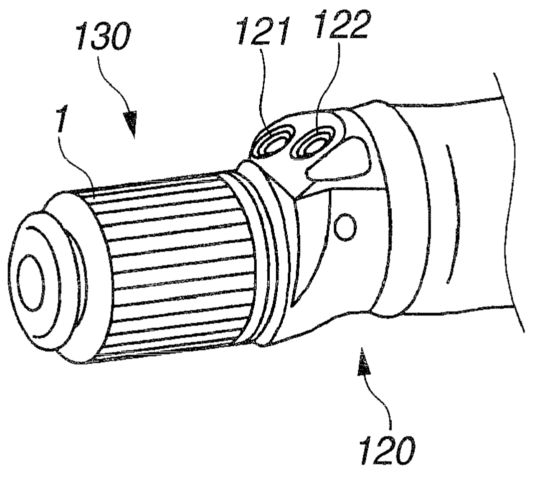


FIG.7

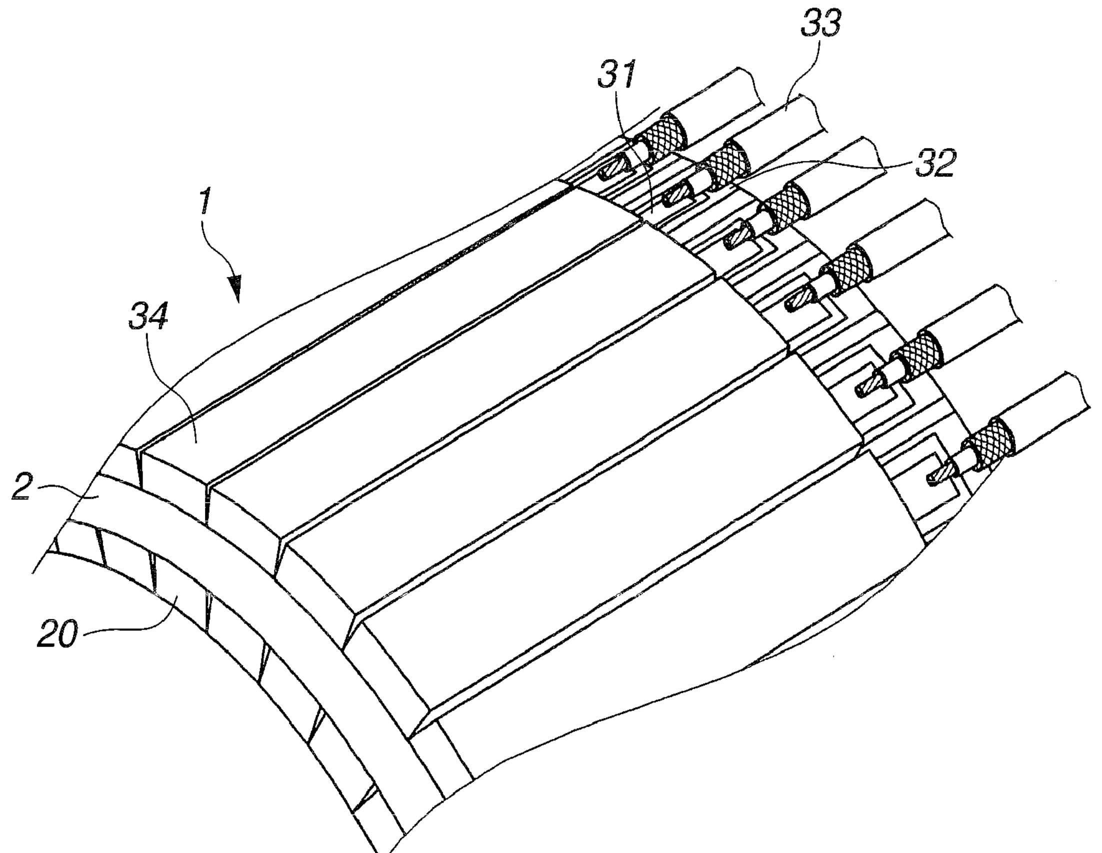


FIG.8

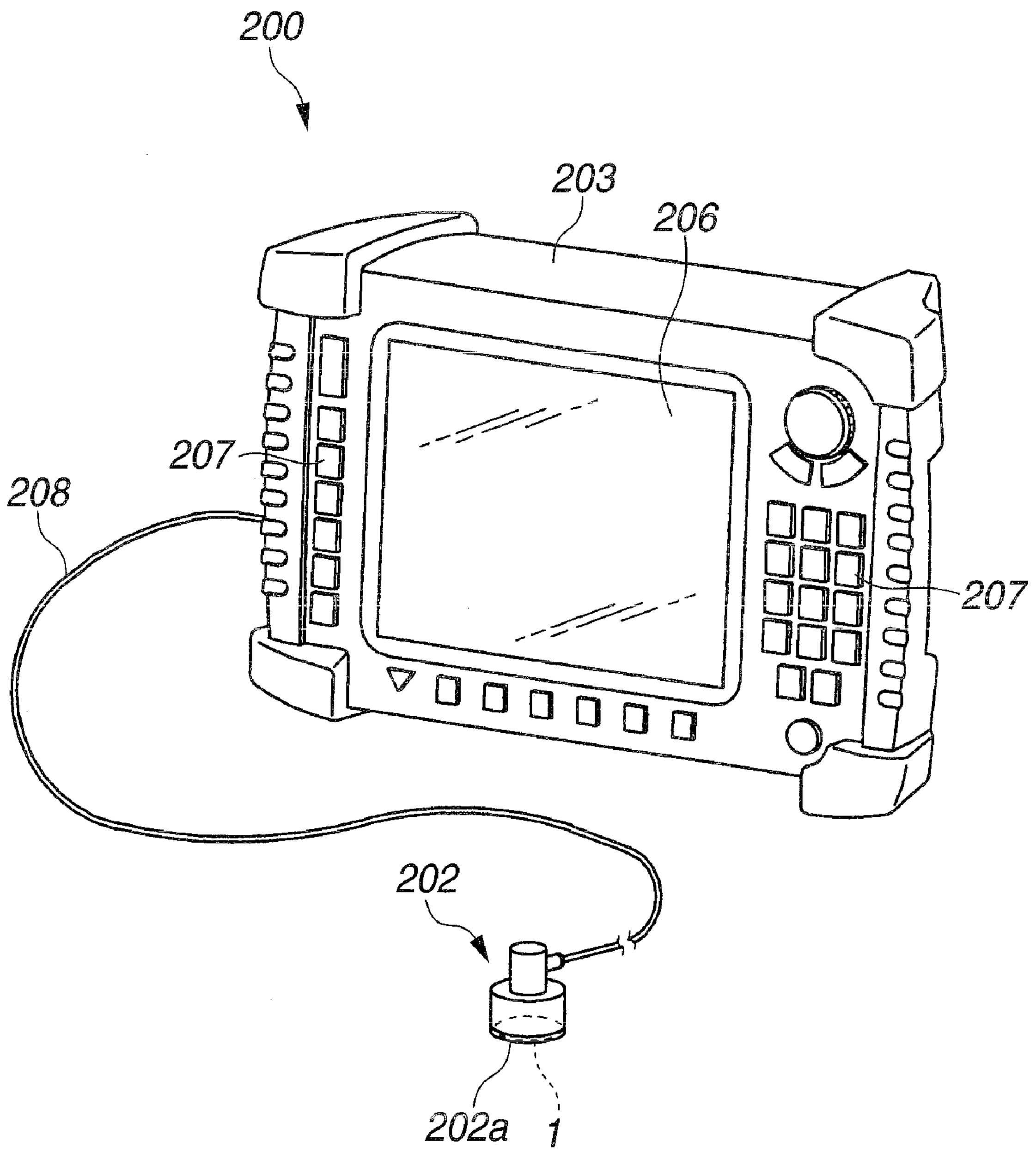
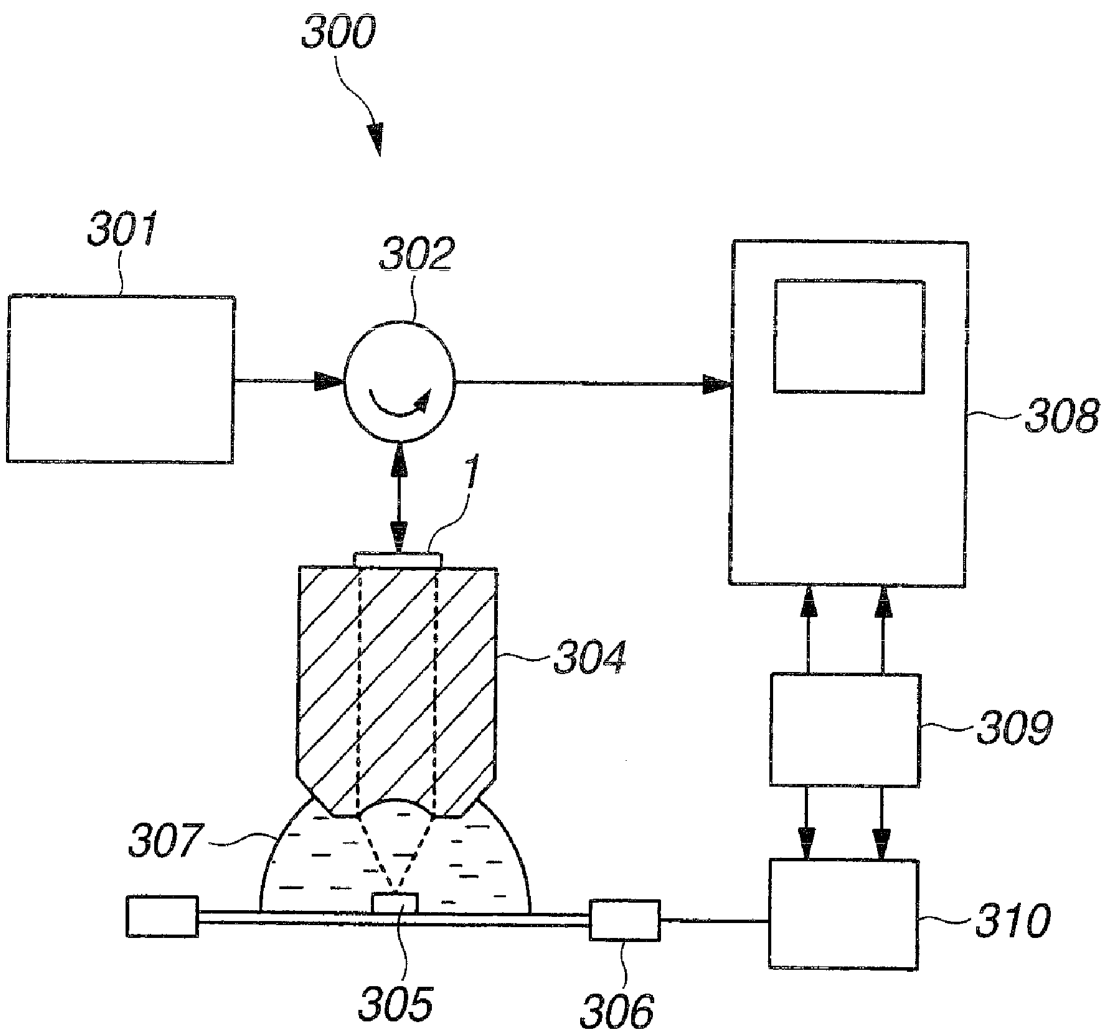


FIG.9



ULTRASOUND TRANSDUCER AND ELECTRONIC DEVICE

This application claims benefit of Japanese Application No. 2008-107038 filed in Japan on Apr. 16, 2008, the contents of which are incorporated by this reference.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention relates to a capacitive ultrasound transducer configured by having an electret and an electronic device.

2. Description of the Related Art

Piezoelectric elements made of a ceramic piezoelectric material PZT (lead zirconate titanate) have been chiefly used as an ultrasound transducer. In recent years, a capacitive ultrasound transducer such as the one disclosed in Japanese Patent Application Laid-Open Publication No. 2005-510264 has attracted attention.

The capacitive ultrasound transducer is configured by having a pair of electrodes formed of an upper electrode and a lower electrode facing each other through a gap portion formed therebetween, and transmits or receives ultrasound through vibration of a membranous portion including the upper electrode (also referred to as "membrane" or "diaphragm").

The capacitive ultrasound transducer converts an ultrasound signal into an electrical signal on the basis of changes in electrostatic capacity between the upper and lower electrodes when receiving ultrasound and, therefore, requires application of a DC bias voltage between the upper and lower electrodes particularly at the time of reception.

From the viewpoint of reducing the power consumption and size of an ultrasound transducer, it is preferable to reduce or set to zero the voltage value of the DC bias voltage. As a technique to reduce the DC bias voltage, a technique of producing a potential difference between the upper and lower electrodes of the capacitive ultrasound transducer by providing between the upper and lower electrodes an electret film holding electric charge is known.

SUMMARY OF THE INVENTION

An ultrasound transducer according to the present invention includes a substrate, an ultrasound transducer cell placed on one surface of the substrate and having a lower electrode, a first gap portion placed on the lower electrode and an upper electrode placed on the first gap portion, a first conductive layer placed on the other surface of the substrate and electrically connected to one of the lower electrode and the upper electrode, an electret film placed on the first conductive layer, an insulating layer placed on the electret film, and a second conductive layer placed on the insulating layer and electrically connected to the one of the lower electrode and the upper electrode not electrically connected to the first conductive layer.

The above and other objects, features and advantages of the invention will become more clearly understood from the following description referring to the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. **1** is a plan view of an ultrasound transducer seen in a direction of transmission of ultrasound;

FIG. **2** is a schematic perspective view of a configuration of the ultrasound transducer;

FIG. **3** is a sectional view taken along line III-III in FIG. **1**;

FIG. **4** is a sectional view of a modified example of the ultrasound transducer;

FIG. **5** is a diagram schematically showing a configuration of an ultrasound endoscope;

FIG. **6** is a perspective view of a distal end portion of the ultrasound endoscope;

FIG. **7** is a perspective view of an ultrasound transmitting/receiving portion;

FIG. **8** is a diagram schematically showing a configuration of an ultrasound flaw detection apparatus; and

FIG. **9** is a diagram schematically showing a configuration of an ultrasound microscope.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

A preferred embodiment of an ultrasound transducer will be described below with reference to the accompanying drawings. In the figures referred to in the following description, the scales on which components are drawn are changed so that the components are shown in such sizes as to be recognizable in the figures. The present invention is not limited to the numbers and shapes of the components, the ratios of the sizes of the components and the relative positional relationships between the components shown in the figures.

FIG. **1** is a plan view of an ultrasound transducer seen in the direction of transmission of ultrasound. FIG. **2** is a schematic perspective view of a configuration of the ultrasound transducer. FIG. **3** is a sectional view taken along line III-III in FIG. **1**. FIG. **4** is a sectional view of a modified example of the ultrasound transducer.

An ultrasound transducer **1** has an ultrasound transducer cell **10** provided on one surface **2***a* of a substrate **2**, and an electret film **20** provided on the other surface **2***b* of the substrate **2**.

The positional relationship in the top-bottom direction between two components provided on the one surface **2***a* or the other surface **2***b* of the substrate **2** is defined in such a manner that the one of the components remoter from the surface than the other in the direction of a normal to the surface is referred to as the upper one. For example, in the sectional view shown in FIG. **3**, an upper electrode **12** is described as being provided above a lower electrode **11** on the one surface **2***a* of the substrate **2**, and a second conductive layer **22** is described as being provided above a first conductive layer **21** on the other surface **2***b* of the substrate **2**.

The material forming the substrate **2** is not limited to a particular one. The substrate **2** may be formed of a material having an electrically conductive property or a material having an electrically insulating property. In the present embodiment, the substrate **2** is formed of a publicly insulating material, such as a silicon oxide, a silicon nitride, quartz, sapphire, crystallized quartz, alumina, zirconia, glass or a resin.

The ultrasound transducer cell **10** is configured by having the lower electrode **11** in the form of a flat plate provided on the one surface **2***a* of the substrate **2**, and the upper electrode **12** in the form of a flat plate provided above the lower electrode **11** so as to face the lower electrode **11** through a first gap portion **13** formed therebetween.

The upper electrode **12** is supported generally parallel to the lower electrode **11** by an insulating layer **14** provided on the lower electrode **11** and formed of a material having an electrically insulating property. When the ultrasound transducer cell **10** transmits or receives ultrasound, a membranous portion **15** including the upper electrode **12** and the insulating layer **14** positioned above the first gap portion **13** vibrates.

It is preferred from the viewpoint of acoustic characteristics that the shape of the membranous portion **15** as seen in a direction perpendicular to the major surfaces of the substrate **2** is circular, as illustrated. However, the shape of the membranous portion **15** may alternatively be oval, elliptic or polygonal. In a case where a plurality of ultrasound transducer cells **10** are provided in one ultrasound transducer **1**, the ultrasound transducer cells **10** may have a plurality of types of membranous portions **15** having different shapes.

It is preferred that the insulating layer **14** is provided so as to cover at least one of the surface of the lower electrode **11** on the first gap portion **13** side and the surface of the upper electrode **12** on the first gap portion **13** side and have the function to prevent the lower electrode **11** and the upper electrode **12** from contacting and shorting to each other.

In the present embodiment, the lower electrode **11** is electrically connected to a signal electrode pad **31** formed on the surface **2***a* of the substrate **2**, as shown in FIG. **3**. The upper electrode **12** is electrically connected by wiring not shown to a ground electrode pad **32** formed on the surface **2***a* of the substrate **2**.

The signal electrode pad **31** and the ground electrode pad **32** are electrodes provided in a state of being exposed at such positions as not to overlap the ultrasound transducer cell **10** as seen in a direction perpendicular to the surface **2***a* of the substrate **2**. A drive circuit which drives the ultrasound transducer **1** is electrically connected to the ultrasound transducer cell **10** via the signal electrode pad **31** and the ground electrode pad **32**.

A protective film **16** made of a resin may be provided on the ultrasound transducer cell **10**, for example, as shown in FIG. **3**, for the purpose of preventing oxidization, preventing damage, improving moisture resistance, or the like.

On the other surface **2***b* of the substrate **2** opposite from the surface on which the above-described ultrasound transducer cell **10** is provided, the electret film **20** for producing a potential difference between the lower electrode **11** and the upper electrode **12** of the ultrasound transducer cell **10** is provided.

The configuration on the other surface **2***b* of the substrate **2** will be described in detail. The first conductive layer **21** in the form of a flat plate formed of an electrically conductive material is first provided on the other surface of the substrate **2**. The first conductive layer **21** is electrically connected to the lower electrode **11** via a through electrode **3** in a via hole formed through the substrate **2**.

The electret film **20** is provided above the first conductive layer **21**. An insulating layer having an electrically insulating property is interposed between the first conductive layer **21** and the electret film **20**. The electret film **20** is a publicly electret film having the function to permanently hold positive or negative charge. The method of configuring and forming the electret film **20** is not particularly specified.

For example, if the electret film **20** is formed of an inorganic film, the electret film **20** is formed by injecting charge into an inorganic film formed of a silicon compound, a hafnium compound or the like by means of an ion beam or corona discharge. The electret film **20** may have a multilayer structure formed of a plurality of kinds of material. For example, it is preferable that the electret film **20** is formed of SiO_2 and is covered with an insulating film formed of SiN because dissipation of held charge is limited even under a high-temperature condition.

For example, if the electret film **20** is formed of an organic film, the electret film **20** is formed by injecting charge into a resin film formed of fluororesin, polyimide, polypropylene, polymethylpentene or the like by means of corona discharge.

In the present embodiment, the insulating layer interposed between the first conductive layer **21** and the electret film **20** is configured of a second gap portion **23** and an insulating film **24** formed of a material having an electrical insulating property.

The insulating layer interposed between the first conductive layer **21** and the electret film **20** is not limited to this form. For example, the insulating layer may be in such a form that the electret film **20** and the first conductive layer **21** are electrically insulated from each other only by the second gap portion **23** or only by the insulating film **24**.

Covering the surface of the electret film **20** with the insulating film **24** as in the present embodiment is more preferable because dissipation of charge held by the electret film **20** can be limited thereby.

The second conductive layer **22** in the form of a flat plate formed of an electrically conductive material and opposed generally parallel to the first conductive layer **21** is provided on the electret film **20**, i.e., on the side of the electret film **20** opposite from the first conductive layer **21** side. The electret film **20** and the second conductive layer **22** may be provided in contact with each other, or an electrically conductive or electrically insulating film capable of preventing oxidization of the surface of the second conductive layer **22** may be interposed between the electret film **20** and the second conductive layer **22**.

The second conductive layer **22** is electrically connected to the ground electrode pad **32** via a through electrode **4** in a via hole formed through the substrate **2**. That is, the second conductive layer **22** is electrically connected to the upper electrode **12**.

The configuration for electrically connecting the first conductive layer **21** and the second conductive layer **22** to the lower electrode **11** and the upper electrode **12** in the present embodiment is not exclusively adopted. For example, a configuration may alternatively be adopted in which the first conductive layer **21** and the second conductive layer **22** are electrically connected to the lower electrode **11** and the upper electrode **12** via pieces of wiring provided so as to extend along an outer peripheral portion of the substrate **2** in a roundabout fashion.

The above-described electret film **20** and the second conductive layer **22** are supported by the insulating film **24**. In other words, the insulating film supports the electret film **20** and the second conductive layer **22** so that the second gap portion **23** is formed between the electret film **20** and the first conductive layer **21**, and so that the first conductive layer **21** and the second conductive layer **22** are generally parallel to each other.

If, as shown in FIG. **3**, the second gap portion **23** is formed as a closed space, i.e., in an airtight manner, and if the surface of the first conductive layer **21** is exposed in the second gap portion **23**, it is preferable to evacuate the second gap portion **23** or to fill the second gap portion **23** with a dry inert gas for the purpose of preventing oxidization of the first conductive layer **21**. If the second gap portion is not formed in an airtight manner, it is preferable to cover the surface of the first conductive layer **21** with a protective film for preventing oxidization.

The arrangement including the electret film **20** may alternatively be such that, as shown in FIG. **4**, the electret film **20** is provided on the first conductive layer **21** in contact with the same; the insulating layer formed of the insulating film **24** containing the second gap portion **23** is provided on the electret film **20**; and the second conductive layer **22** is provided on the insulating layer.

The effects of the ultrasound transducer **1** having the above-described configuration will be described below.

In the ultrasound transducer **1** having the above-described configuration, the electret film **20** for causing a potential difference between the lower electrode **11** and the upper electrode **12** of the ultrasound transducer cell **10** is provided on the surface (**2***b*) of the substrate **2** opposite from the surface (**2***a*) on which the ultrasound transducer cell **10** is provided.

In the ultrasound transducer **1** according to the present embodiment, therefore, the thickness of the electret film **20** and the distance between the lower electrode **11** and the upper electrode **12** can be set independently of each other.

That is, according to the present embodiment, in contrast with the conventional capacitive ultrasound transducer having an electret film provided between upper and lower electrodes, the distance between the lower electrode **11** and the upper electrode **12** is reduced to increase the electrostatic capacity between these electrodes, thereby improving the sound pressure of transmitted ultrasound and the sensitivity to received ultrasound. Also, the thickness of the electret film **20** can be increased to such a value as to be capable of permanently holding charge with stability.

By having the electret film **20**, therefore, the ultrasound transducer **1** according to the present embodiment has an output and sensitivity higher than those of the conventional ultrasound transducer while reducing the DC bias voltage applied between the lower electrode **11** and the upper electrode **12** or eliminating the need for application of the DC bias voltage.

The ultrasound transducer according to the present embodiment is capable of increasing the thickness of the electret film **20** in comparison with the conventional ultrasound transducer and is, therefore, capable of stabilizing the charge holding performance of the electret film **20** and maintaining the performance for a long time period.

In the present embodiment, the electret film **20** is provided at such a position as to be superposed on the ultrasound transducer cell **10** as seen in a direction perpendicular to the major surfaces of the substrate **2** and, therefore, the ultrasound transducer **1** according to the present embodiment can be realized in the same size as the conventional ultrasound transducer in which an electret film is provided between upper and lower electrodes.

In general, some ultrasound transducer is used in a state of having the surface for transmitting or receiving ultrasound maintained in contact with a liquid for the purpose of enabling ultrasound to propagate without being attenuated. On the other hand, in some case, the electret film **20** loses charge by contact with moisture. In the present embodiment, the electret film **20** is provided on the side opposite from the surface for transmitting or receiving ultrasound, thereby enabling prevention of permeation of moisture into the electret film **20** and improving the durability of the ultrasound transducer **1**.

With the conventional ultrasound transducer having an electret film provided between upper and lower electrodes, there is a problem that charge held by the electret film dissipates under the influence of components of an atmosphere, humidity and temperature in a manufacturing process performed after injecting charge in the electret film. Conventionally, therefore, there are only a limited number of processing methods executable after injection of charge into a material forming the electret film or after injection of charge into the electret film.

In contrast, in manufacturing the above-described ultrasound transducer **1**, the ultrasound transducer cell **10** to be provided on the surface **2***a* of the substrate **2** and the electret film **20** to be provided on the other surface **2***b* of the substrate **2** can be combined after being respectively manufactured separately from each other.

Therefore, the electret film **20** can be provided in the ultrasound transducer **1** without being placed in an environment which may cause dissipation of charge held by the electret film **20** after injection of charge into the electret film **20**. That is, the ultrasound transducer **1** having the above-described configuration has an improved degree of design freedom with which a selection from construction materials, a selection from processing methods and the like are made and can therefore be implemented with improved performance at a lower price in comparison with the conventional ultrasound transducer. Because of the improvement in the degree of design freedom with which construction materials are selected, the ultrasound transducer **1** can be constituted of a material of a reduced environmental load, for example, a lead-free material.

The above-described ultrasound transducer **1** can be manufactured by using various manufacturing techniques such as a semiconductor manufacturing technique and a micromachining technique. Therefore, the method of forming the ultrasound transducer **1** is not particularly specified. However, a micro-electro-mechanical system (MEMS) process for example may be used. An ultrasound transducer made by a MEMS process is ordinarily called a capacitive micromachined ultrasonic transducer (c-MUT).

Examples of electronic devices to which the ultrasound transducer of the present invention can be applied will be described with reference to FIGS. **5** to **9**.

A mode in which the ultrasound transducer **1** of the present invention is applied to an ultrasound endoscope as an example of an ultrasound diagnostic apparatus will be described with reference to FIGS. **5** to **7**. FIG. **5** is a diagram schematically showing a configuration of an ultrasound endoscope. FIG. **6** is a perspective view of a configuration of a distal end portion of the ultrasound endoscope. FIG. **7** is a perspective view of an ultrasound transmitting/receiving portion.

As shown in FIG. **5**, an ultrasound endoscope **101** in the present embodiment is configured mainly of an elongated insertion portion **102** to be inserted into the body of a subject, an operation portion **103** positioned at a proximal end of the insertion portion **102**, and a universal cord **104** extending from a side portion of the operation portion **103**.

An endoscope connector **104***a* to be connected to a light source device (not shown) is provided on a proximal end portion of the universal cord **104**. From the endoscope connector **104***a*, an electric cable **105** detachably connected to a camera control unit (not shown) through an electric connector **105***a* extends. An ultrasound cable **106** detachably connected to an ultrasound observation apparatus (not shown) through an ultrasound connector **106***a* also extends from the endoscope connector **104***a*.

The insertion portion **102** is configured by providing, in order from the distal end side, one adjacent to another, a distal end rigid portion **120** formed of a rigid member, a bending portion **108** capable of bending operation positioned at a rear end of the distal end rigid portion **120**, and a flexible tube portion **109** positioned at a rear end of the bending portion **108**, extending to a distal end portion of the operation portion **103**, small in diameter, elongated and having flexibility. An ultrasound transmitting/receiving portion **130** for transmitting or receiving ultrasound, described below, is provided on the distal end side of the distal end rigid portion **120**.

The operation portion **103** is provided with an angle knob **111** for controlling the bending portion **108** in bending in a desired direction, air supply and water supply button **112** for performing air supply and water supply operations, a suction button **113** for performing a suction operation, and a treatment instrument insertion opening **114**, which is an inlet for a treatment instrument to be introduced into a body cavity.

As shown in FIG. **6**, the distal end rigid portion **120** is provided with an illumination lens (not shown) constituting an illumination optical section for irradiating illumination light to a portion to be observed, an objective lens **121** constituting an observation optical section for capturing an optical image of a portion to be observed, an opening **122** for suction and for forceps, through which a excised part is sucked in or a treatment instrument is projected, and air supply and water supply opening (not shown) for air supply and water supply.

In the ultrasound transmitting/receiving portion **130** provided on the distal end of the distal end rigid portion **120**, as shown in FIG. **7**, a plurality of ultrasound transducers **1** are configured being arrayed in cylindrical form, with ultrasound transducer cells **10** facing radially outwardly.

A substrate **2** is constituted of a material having flexibility, e.g., polyimide and is rounded into a cylindrical shape. On an outer peripheral surface of the substrate **2** rounded into a cylindrical shape, ultrasound transducer elements **34** each constituted of a plurality of ultrasound transducer cells **10** and provided as a smallest drive unit are arrayed along a circumferential direction, and electrets **20** corresponding to the plurality of ultrasound transducer elements **34** are provided on an inner peripheral surface of the substrate **2**.

Signal electrode pads **31** and ground electrode pads **32** corresponding to the plurality of ultrasound transducer elements **34** are formed on the outer peripheral surface of the substrate **2**. Ends of coaxial cables **33** passed through an ultrasound cable **106** are electrically connected to the signal electrode pads **31** and the ground electrode pads **32**. Other ends of the coaxial cables are passed through the ultrasound cable **106** to be electrically connected to the ultrasound connector **106***a*.

The ultrasound transducer **1** of the present invention is applicable to publicly ultrasound diagnosis apparatuses as well as to the above-described ultrasound endoscope. For example, the ultrasound transducer **1** may be applied to an ultrasound probe type of ultrasound endoscope, a capsule type of ultrasound endoscope or to an ultrasound diagnosis apparatus arranged to transmit ultrasound from the outside of a subject into the subject and receive ultrasound from the subject.

A mode in which the ultrasound transducer **1** of the present invention is applied to an ultrasound flaw detection apparatus as an example of a nondestructive inspection apparatus will be described with reference to FIG. **8**. FIG. **8** is a diagram schematically showing a configuration of an ultrasound flaw detection apparatus.

An ultrasound flaw detection apparatus **200** has a probe **202** for transmitting and receiving ultrasound, and an apparatus main unit **203** for controlling the probe **202**.

A display device **206** which displays an image for flaw detection is provided at a center of a front face of the apparatus main unit **203**, and switches **207** having various roles are provided in the vicinity of the display device **206**.

The probe **202** is connected to the apparatus main unit **203** by a composite coaxial cable **208**. One ultrasound transducer **1** or a plurality of ultrasound transducers **1** are provided in a contact surface portion **202***a* of the probe **202** to be brought into contact with a subject.

The ultrasound flaw detection apparatus **200** issues ultrasound while maintaining the contact surface portion **202***a* of the probe **202** in contact with a subject and can detect a flaw in the subject through a change in reflection of the ultrasound without breaking the subject.

The ultrasound transducer **1** of the present invention is applicable to publicly nondestructive inspection apparatuses as well as to the above-described ultrasound flaw detection apparatus. For example, the ultrasound transducer **1** may be applied to a thickness measuring apparatus for measuring the thickness of a subject by transmitting and receiving ultrasound.

An example of an application of the ultrasound transducer **1** of the present invention to an ultrasound microscope will be described with reference to FIG. **9**. FIG. **9** is a diagram showing a configuration of an ultrasound microscope in the present embodiment.

An ultrasound microscope **300** applies a radiofrequency signal generated in a radiofrequency oscillator **301** to an ultrasound transducer **1** according to the present invention through a circulator **302** to convert the radiofrequency signal into ultrasound. This ultrasound is converged with an acoustic lens **304**. At the point of this convergence, a specimen **305** is placed. The specimen **305** is held by a sample holder **306** and a space between the specimen **305** and the lens surface of the acoustic lens **304** is filled with a coupler **307** such as water. Reflected waves from the specimen **305** are received by the transducer **1** through the acoustic lens **304** to be converted into an electrical reflection signal. The electric signal outputted from the ultrasound transducer **1** in correspondence with the received ultrasound is inputted to a display device **308** through the circulator **302**. The sample holder **306** is driven in a horizontal plane in directions along two axes: X- and Y-axes by a scanning device **310** controlled by a scanning circuit **309**.

The ultrasound microscope **300** configured as described above can quantify an elastic characteristic of the specimen **305** by applying ultrasound to the specimen **305** and evaluating an acoustic characteristic of the specimen **305** and can evaluate the structure of a thin film.

Having described the preferred embodiments of the invention referring to the accompanying drawings, it should be understood that the present invention is not limited to those precise embodiments and various changes and modifications thereof could be made by one skilled in the art without departing from the spirit or scope of the invention as defined in the appended claims.

What is claimed is:

1. An ultrasound transducer comprising:
a substrate;
an ultrasound transducer cell placed on one surface of the substrate and having a lower electrode, a first gap portion placed on the lower electrode and an upper electrode placed on the first gap portion;
a first conductive layer placed on the other surface of the substrate and electrically connected to one of the lower electrode and the upper electrode;
an electret film placed on the first conductive layer;
an insulating layer placed on the electret film; and
a second conductive layer placed on the insulating layer and electrically connected to the one of the lower electrode and the upper electrode not electrically connected to the first conductive layer.

2. The ultrasound transducer according to claim **1**, wherein the insulating layer includes a pair of insulating films and a second gap portion interposed between the pair of insulating films.

3. The ultrasound transducer according to claim **2**, wherein the substrate has flexibility.

4. The ultrasound transducer according to claim **1**, wherein the substrate has flexibility.

5. An electronic device comprising the ultrasound transducer according to claim **1**.

6. An ultrasound transducer comprising:

a substrate;

an ultrasound transducer cell placed on one surface of the substrate and having a lower electrode, a first gap portion placed on the lower electrode and an upper electrode placed on the first gap portion;

a first conductive layer placed on the other surface of the substrate and electrically connected to one of the lower electrode and the upper electrode;

an insulating layer placed on the first conductive layer;

an electret film placed on the insulating layer; and

a second conductive layer placed on the electret film and electrically connected to the one of the lower electrode and the upper electrode not electrically connected to the first conductive layer.

7. The ultrasound transducer according to claim **6**, wherein the insulating layer includes a pair of insulating films and a second gap portion interposed between the pair of insulating films.

8. The ultrasound transducer according to claim **7**, wherein the substrate has flexibility.

9. The ultrasound transducer according to claim **6**, wherein the substrate has flexibility.

10. An electronic device comprising the ultrasound transducer according to claim **6**.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE

CERTIFICATE OF CORRECTION

PATENT NO. : 8,026,651 B2
APPLICATION NO. : 12/424118
DATED : September 27, 2011
INVENTOR(S) : Katsuhiro Wakabayashi et al.

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

On the title page item (73), should read:

(73) Assignee: Olympus Medical Systems Corp., Tokyo (JP)
Olympus Corporation, Tokyo (JP)

Signed and Sealed this
Thirty-first Day of January, 2012

David J. Kappos
Director of the United States Patent and Trademark Office

专利名称(译)	超声换能器和电子设备		
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[标]申请(专利权)人(译)	奥林巴斯医疗株式会社		
申请(专利权)人(译)	奥林巴斯医疗系统股份有限公司.		
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摘要(译)

超声换能器包括基板，放置在基板的一个表面上并具有下电极的超声换能器单元，放置在下电极上的第一间隙部分和放置在第一间隙部分上的上电极，放置在第一导电层上的第一导电层基板的另一个表面并且电连接到下电极和上电极中的一个，驻留在第一导电层上的驻极体膜，放置在驻极体膜上的绝缘层，以及放置在绝缘层上的第二导电层和电连接到下电极和上电极中的一个，不与第一导电层电连接。