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Nita et al.

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(54) **CONNECTOR FOR SECURING
ULTRASOUND CATHETER TO
TRANSDUCER**

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patent is extended or adjusted under 35
U.S.C. 154(b) by 130 days.

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Related U.S. Application Data

(63) Continuation of application No. 10/666,459, filed on
Sep. 19, 2003, now Pat. No. 6,942,620.

(51) **Int. Cl.**
A61B 8/14 (2006.01)

(52) **U.S. Cl.** **600/459**; 600/300; 600/407;
600/437

(58) **Field of Classification Search** 600/407-480,
600/300; 604/19, 20
See application file for complete search history.

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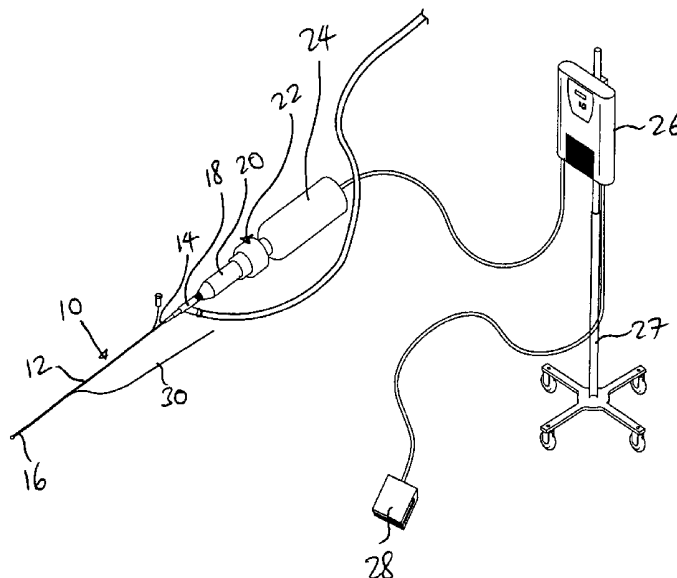
Assistant Examiner—Nasir Shahrestani

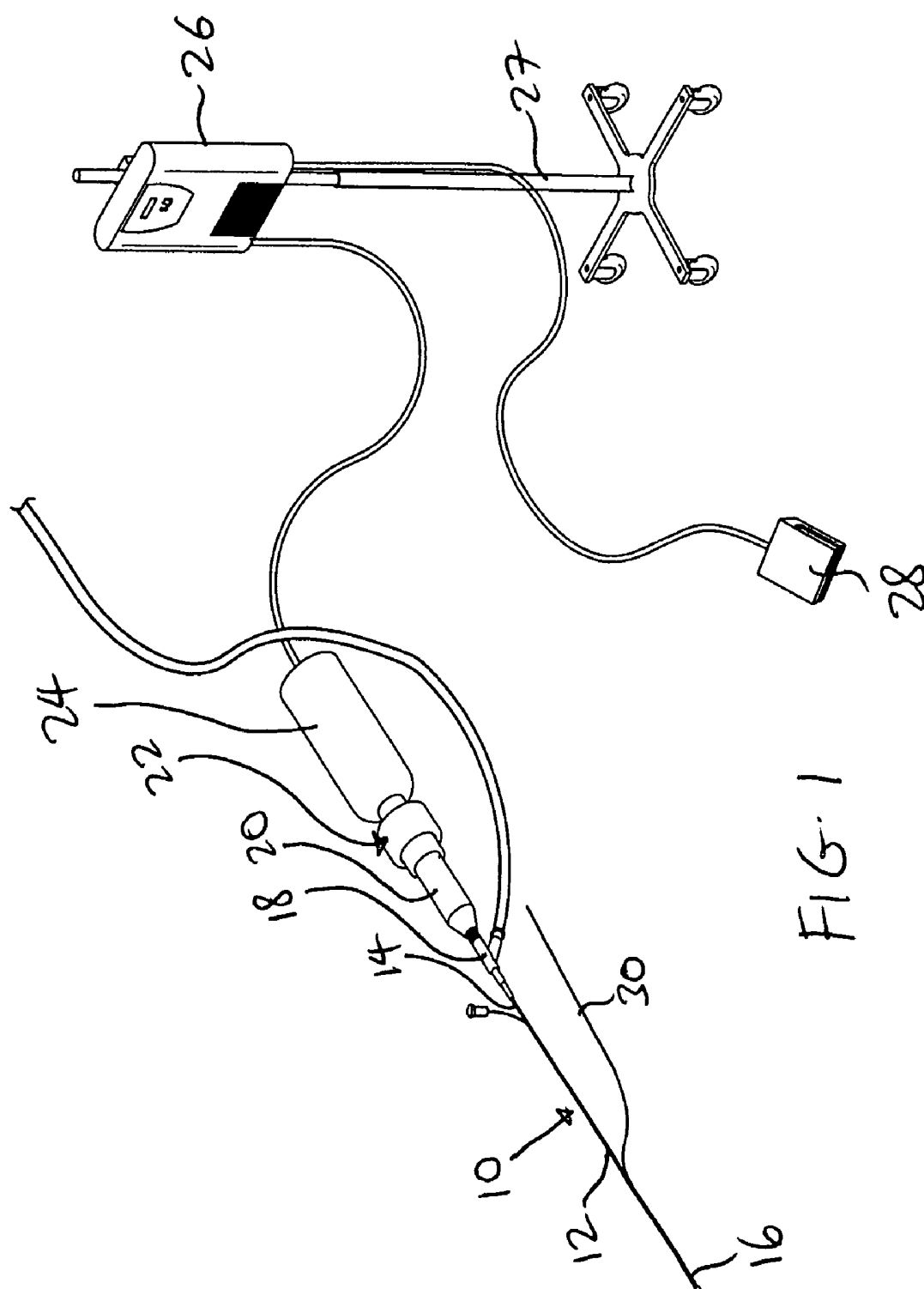
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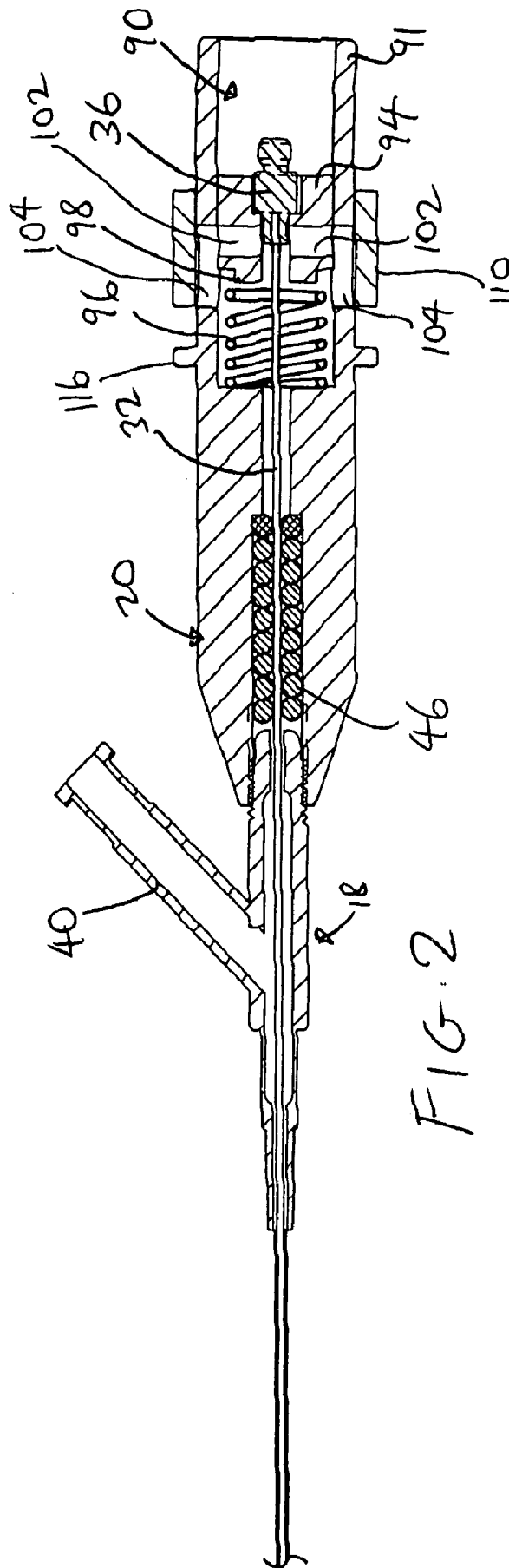
(57) **ABSTRACT**

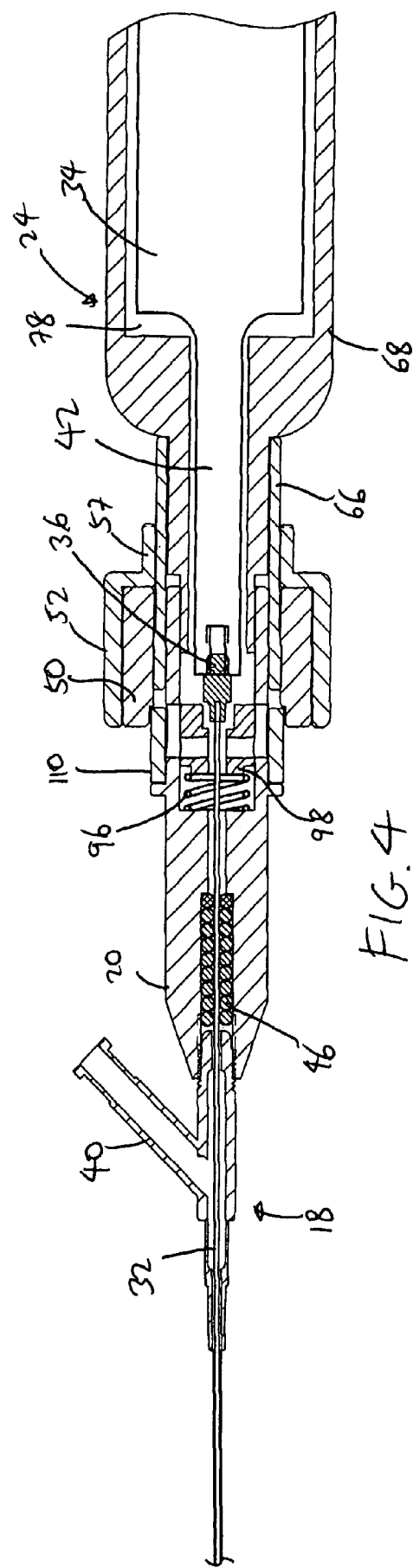
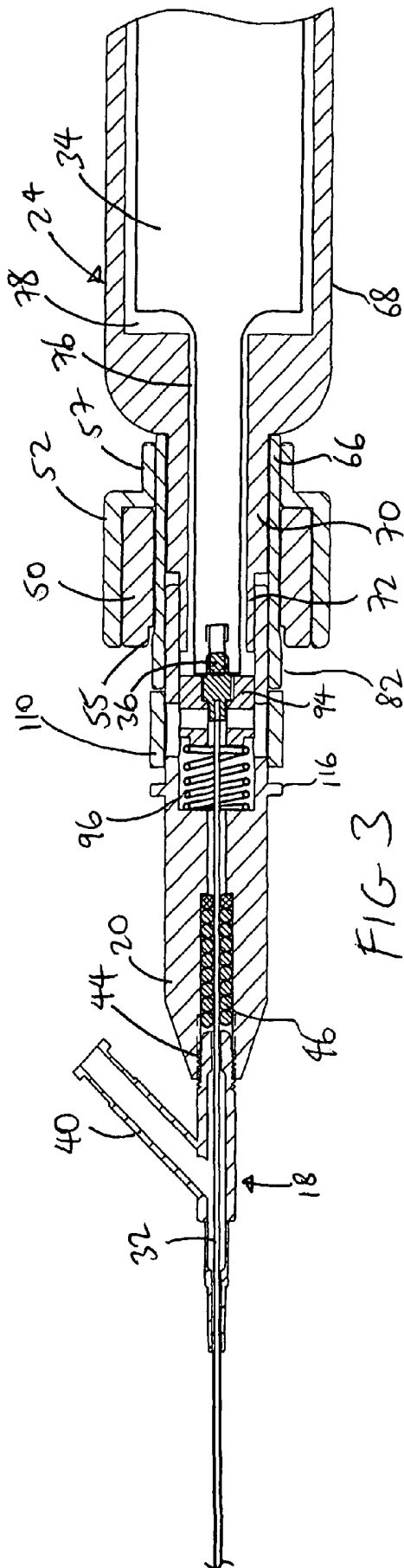
An ultrasound system has an ultrasound transducer having a transducer housing and a horn provided at the distal end of the transducer housing, an ultrasound transmission member, a sonic connector that is connected to the horn and the proximal end of the ultrasound transmission member, and a catheter knob having a proximal end that is coupled to the distal end of the transducer housing. The catheter knob has a proximal bore that houses the sonic connector. The system also includes a nesting piece that is retained inside the proximal bore of the catheter knob. The nesting piece can be moved from a first position where the sonic connector is received inside the nesting piece to a second position where the sonic connector is separated from the nesting piece when ultrasound energy is being propagated through the ultrasound transmission member.

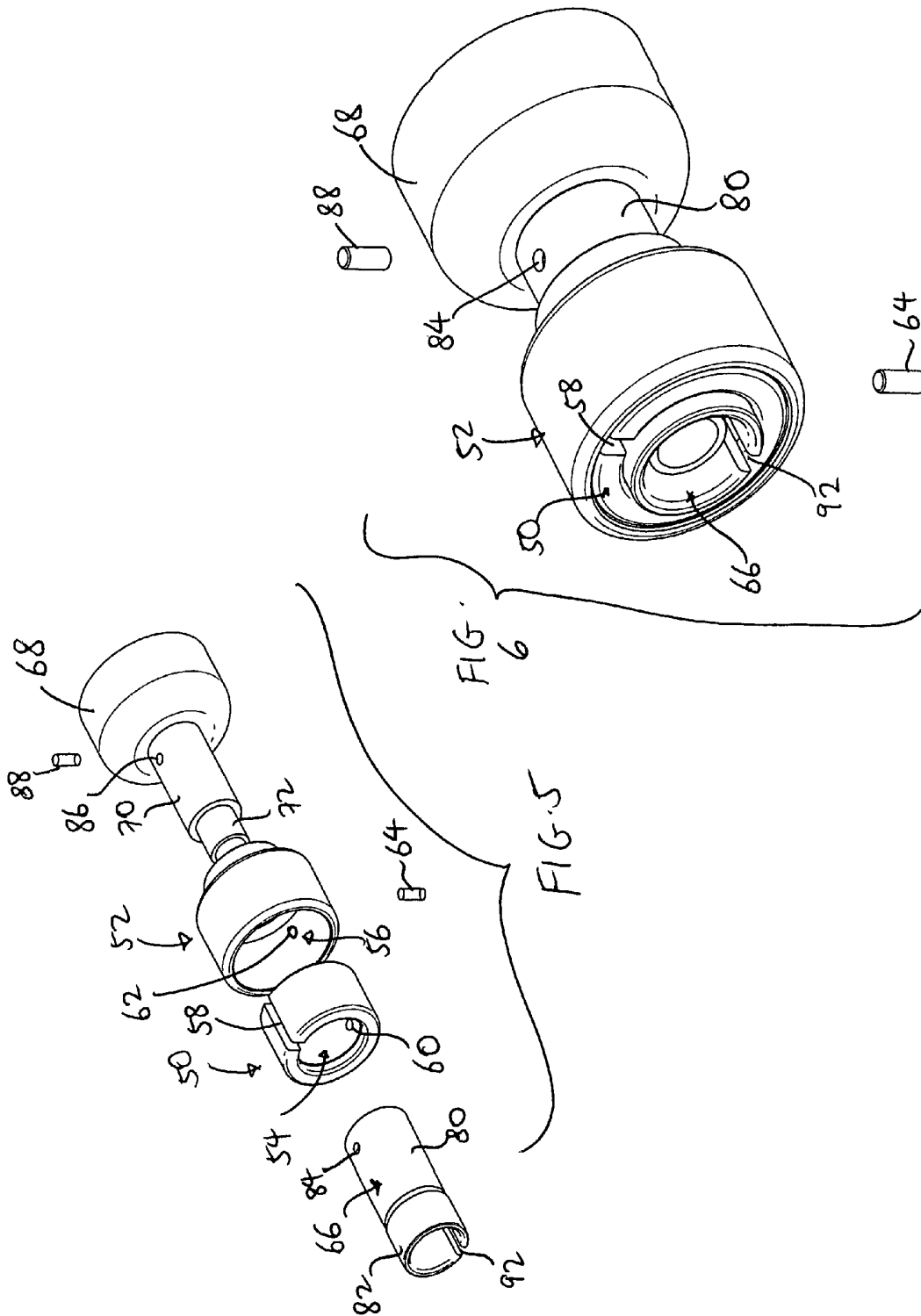
1 Claim, 7 Drawing Sheets

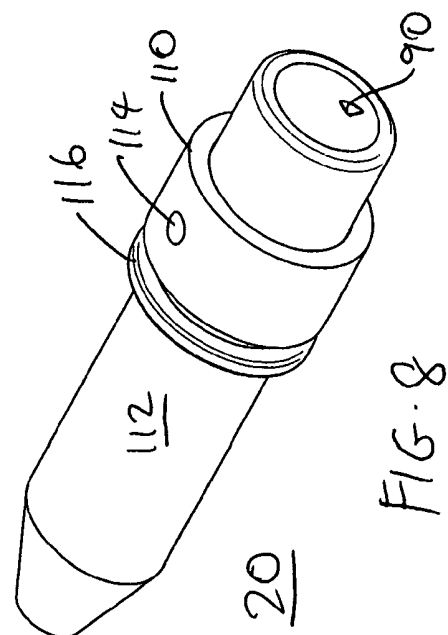
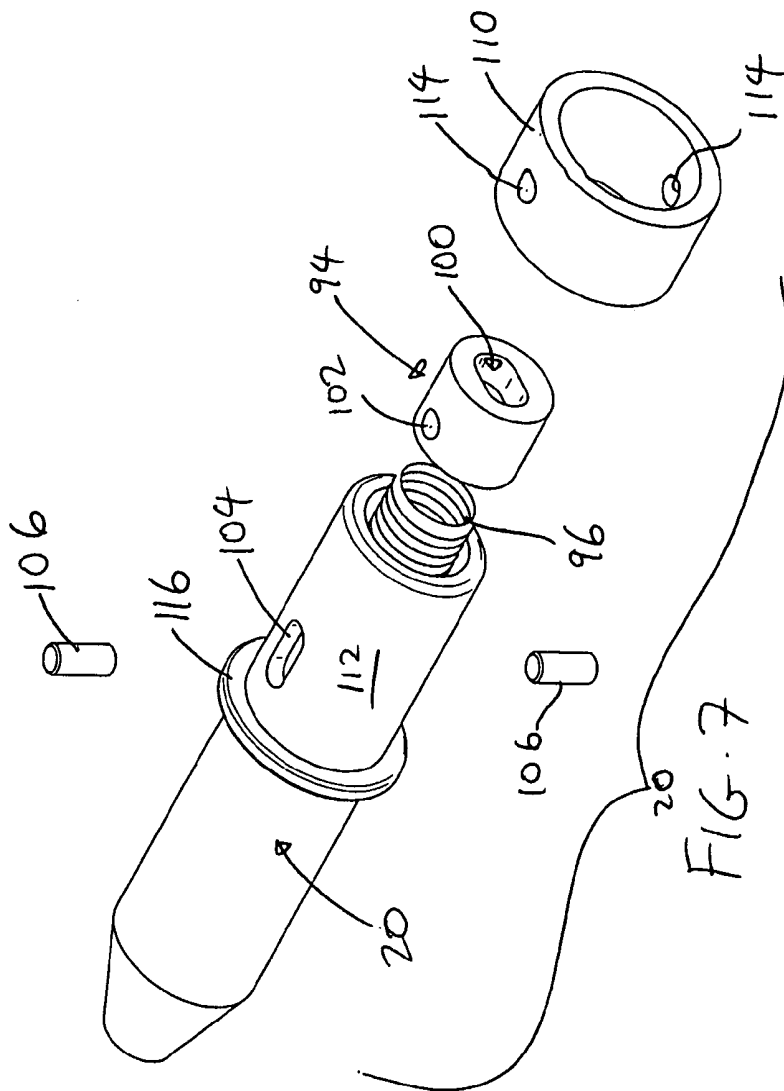


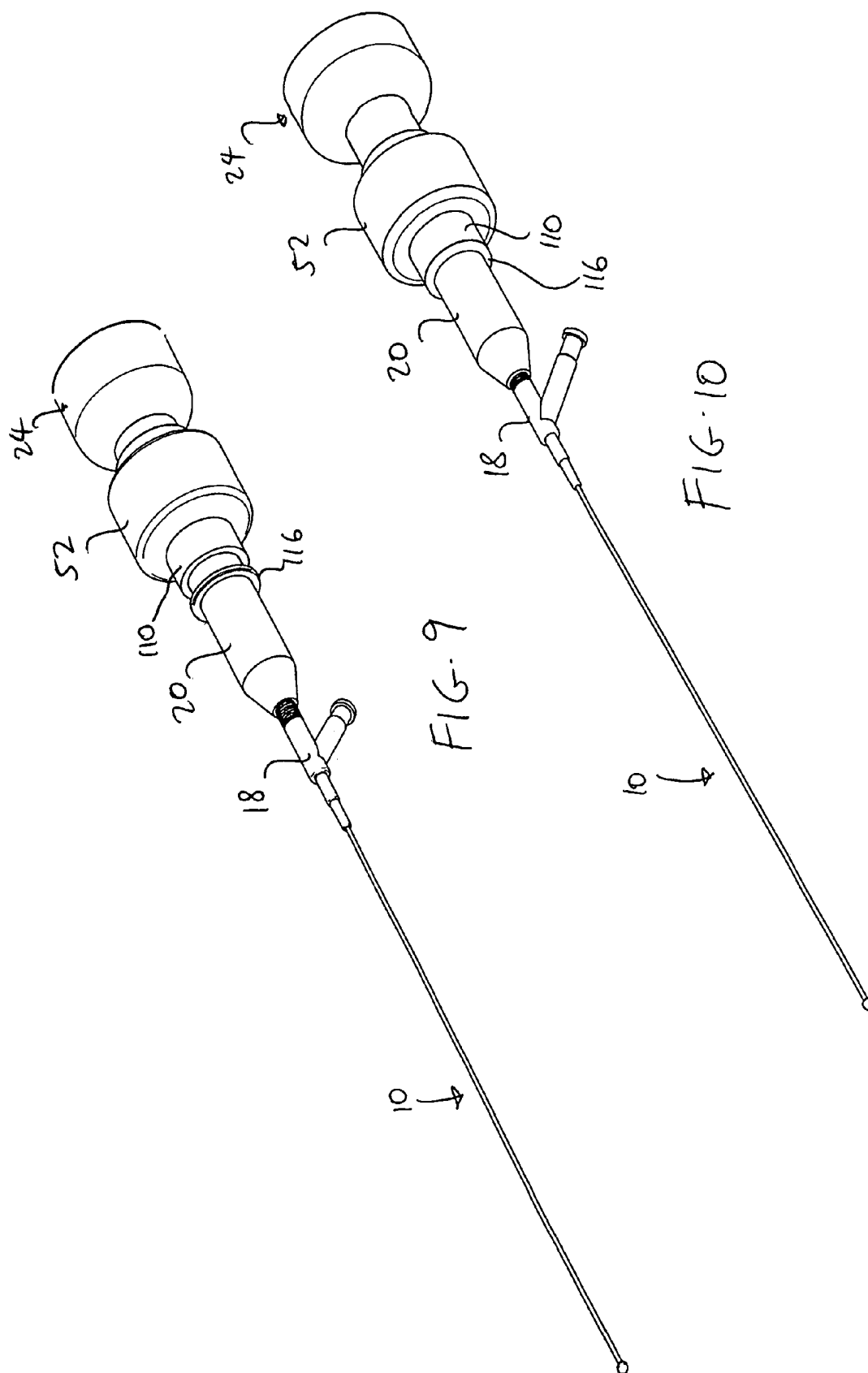


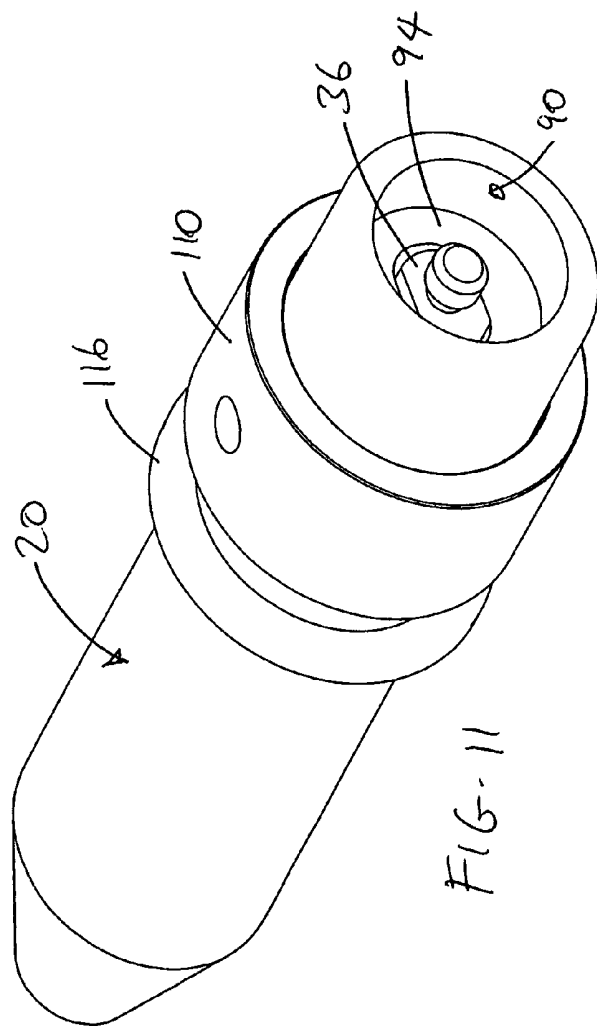
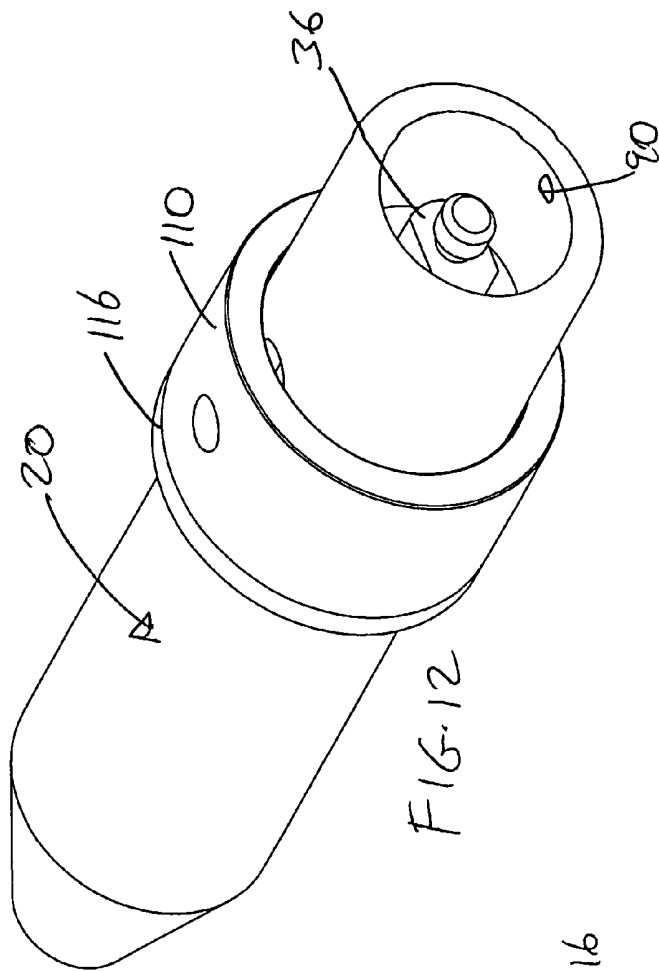












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CONNECTOR FOR SECURING ULTRASOUND CATHETER TO TRANSDUCER

RELATED CASES

This is a continuation of Ser. No. 10/666,459, filed Sep. 19, 2003, now pending.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention pertains to medical equipment, and more particularly, to a device and method for attaching an ultrasound catheter to an ultrasound transducer which prevents frequency shifts and minimizes the mechanical impact of the handling connection area during a medical procedure.

2. Description of the Prior Art

A number of ultrasound systems and devices have heretofore been proposed for use in ablating or removing obstructive material from blood vessels. Ultrasound catheters have been utilized to ablate various types of obstructions from blood vessels of humans and animals. Successful applications of ultrasound energy to smaller blood vessels, such as the coronary arteries, require the use of relatively small diameter ultrasound catheters which are sufficiently small and flexible to undergo transluminal advancement through the tortuous vasculature of the aortic arch and coronary tree. These ultrasound catheters incorporate a very small diameter ultrasound transmission member which extends through such catheters. The proximal end of the ultrasound transmission member is typically connected to an ultrasound transducer via a sonic connector.

The attachment of the ultrasound transmission member to an ultrasound transducer plays a very important role in ultrasound energy propagation. The attachment region needs to be accurately aligned and free of mechanical stress and other interfaces. For example, undesirable stress at the attachment region can be caused by pressing upon, pushing, pulling, torquing, bending or bumping the attachment region during use of the ultrasound catheter. In addition, it is preferable for the sonic connector to be free from any interface (i.e., contact) with any other component during energy transmission. Otherwise, such stresses and interfaces can negatively impact the propagation of ultrasound energy through the ultrasound transmission member. Contact of the sonic connector with any other part of the catheter housing during the delivery of ultrasound energy might also cause a shift in frequency and impact performance.

Thus, there still exists a need for an improved connection of the proximal end of the ultrasound transmission member to an ultrasound transducer.

SUMMARY OF THE DISCLOSURE

It is an object of the present invention to provide an improved connection between the ultrasound catheter and the ultrasound transducer.

It is yet another object of the present invention to improve the propagation of ultrasound energy by limiting and minimizing the impact of undesirable external forces.

In order to accomplish the objects of the present invention, there is provided an ultrasound system and method of using the ultrasound system during a medical procedure. The ultrasound system has an ultrasound transducer having a transducer housing and a horn provided at the distal end of the transducer housing, an ultrasound transmission member, a

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sonic connector that is connected to the horn and the proximal end of the ultrasound transmission member, and a catheter knob having a proximal end that is coupled to the distal end of the transducer housing. The catheter knob has a proximal bore that houses the sonic connector. The system also includes a nesting piece that is retained inside the proximal bore of the catheter knob. The nesting piece can be moved from a first position where the sonic connector is received inside the nesting piece to a second position where the sonic connector is separated from the nesting piece when ultrasound energy is being propagated through the ultrasound transmission member.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a perspective view of an ultrasound system according to one embodiment of the present invention.

FIG. 2 is a cross-sectional view of the Y-connector and catheter knob of the system of FIG. 1.

FIG. 3 is a cross-sectional view of the Y-connector, the catheter knob, the slide collar assembly and the transducer housing of the system of FIG. 1 with the slide collar assembly in the non-supporting position.

FIG. 4 is a cross-sectional view of the Y-connector, the catheter knob, the slide collar assembly and the transducer housing of the system of FIG. 1 with the slide collar assembly in the supporting position.

FIG. 5 is an exploded perspective view of some of the elements of the slide collar assembly of the system of FIG. 1.

FIG. 6 is an assembled perspective view of the elements of FIG. 5.

FIG. 7 is an exploded perspective view of the catheter knob of the system of FIG. 1.

FIG. 8 is an assembled perspective view of the catheter knob of FIG. 7.

FIG. 9 is a perspective view of the system of FIG. 1 with the slide collar assembly in the non-supporting position.

FIG. 10 is a perspective view of the system of FIG. 1 with the slide collar assembly in the supporting position.

FIG. 11 is a perspective view of the catheter knob of the system of FIG. 1 with the slide collar assembly in the non-supporting position.

FIG. 12 is a perspective view of the catheter knob of the system of FIG. 1 with the slide collar assembly in the supporting position.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

The following detailed description is of the best presently contemplated modes of carrying out the invention. This description is not to be taken in a limiting sense, but is made merely for the purpose of illustrating general principles of embodiments of the invention. The scope of the invention is best defined by the appended claims. In certain instances, detailed descriptions of well-known devices, compositions, components, mechanisms and methods are omitted so as to not obscure the description of the present invention with unnecessary detail.

FIG. 1 illustrates an ultrasound system according to the present invention for use in ablating and removing occlusive material inside the vessel of an animal or human being. The ultrasound system includes an ultrasonic catheter device 10 which has an elongate catheter body 12 having a proximal end 14, a distal end 16, and defining at least one lumen extending longitudinally therethrough. The ultrasound catheter device 10 is operatively coupled at its proximal end 14, by way of a

Y-connector **18**, a catheter knob **20**, and a slide collar assembly **22**, to an ultrasound transducer housing **24**. As shown in FIGS. 3-4, an ultrasound transducer **34** is housed inside the transducer housing **24**. The ultrasound transducer **34** is connected to a signal generator **26**, which can be provided with a foot actuated on-off switch **28**. The signal generator **26** can be supported by an IV pole **27**. When the on-off switch **28** is depressed, the signal generator **26** sends an electrical signal to the ultrasound transducer **34**, which converts the electrical signal to ultrasound energy. Such ultrasound energy subsequently passes through the catheter device **10** and is delivered to the distal end **16**.

Referring also to FIGS. 2-4, an ultrasound transmission member **32** extends through the lumen of the catheter **10** from the distal end **16** to the proximal end **14**. The ultrasound transducer **34** is coupled via a sonic connector **36** (described in greater detail below) to the ultrasound transmission member **32**, so that the ultrasound energy can be passed through the sonic connector **36** and the ultrasound transmission member **32** to be delivered to the distal end **16** of the catheter **10**. A guidewire **30**, which can be any conventional monorail or over-the-wire guidewire, may be utilized in conjunction with the catheter **10** in a manner that is well-known in the catheter art.

The frontal portion of the Y-connector **18** is connected to the proximal end **12** of the catheter **10** using techniques that are well-known in the catheter art. An injection pump (not shown) or IV bag (not shown) can be connected, by way of an infusion tube (not shown), to an infusion port or sidearm **40** of the Y-connector **18**. The injection pump can be used to infuse coolant fluid (e.g., 0.9% NaCl solution) into and/or through the lumen of the catheter **10**. Such flow of coolant fluid may be utilized to prevent overheating of the ultrasound transmission member **32** extending longitudinally through the lumen of the catheter **10**. Such flow of the coolant fluid through the lumen of the catheter **10** serves to bathe the outer surface of the ultrasound transmission member **32**, thereby providing for an equilibration of temperature between the coolant fluid and the ultrasound transmission member **32**. Thus, the temperature and/or flow rate of coolant fluid may be adjusted to provide adequate cooling and/or other temperature control of the ultrasound transmission member **32**. In addition to the foregoing, the injection pump may be utilized to infuse a radiographic contrast medium into the catheter **10** for purposes of imaging. Examples of iodinated radiographic contrast media which may be selectively infused into the catheter **10** via the injection pump are commercially available as Angiovisc 370 from Berlex Labs, Wayne, N.J. and Hexabrix from Malinkrodt, St. Louis, Mo.

The proximal end of the ultrasound transmission member **32** is attached to the sonic connector **36** which is configured to effect operative and removable attachment of the proximal end of the ultrasound transmission member **32** to the distal horn **42** of the ultrasound transducer **34**. The sonic connector **36** is preferably configured and constructed to permit passage of ultrasound energy through the ultrasound transmission member **32** with minimal lateral side-to-side movement of the ultrasound transmission member **32** while, at the same time, permitting unrestricted longitudinal forward/backward vibration or movement of the ultrasound transmission member **32**.

The ultrasound transmission member **32** may be formed of any material capable of effectively transmitting the ultrasonic energy from the ultrasound transducer **34** to the distal end **16** of the catheter **10**, including but not necessarily limited to metal, plastic, hard rubber, ceramic, fiber optics, crystal, polymers, and/or composites thereof. In accordance with one

aspect of the invention, all or a portion of the ultrasound transmission member **32** may be formed of one or more materials which exhibit super-elasticity. Such materials should preferably exhibit super-elasticity consistently within the range of temperatures normally encountered by the ultrasound transmission member **32** during operation of the catheter **10**. Specifically, all or part of the ultrasound transmission member **32** may be formed of one or more metal alloys known as "shape memory alloys". Such super-elastic metal alloys are well-known in the art and will not be described in any further detail herein.

The proximal end of the Y-connector **18** is attached to the distal end of the catheter knob **20** by threadably engaging the proximal end of the Y-connector **18** inside a threaded distal bore **44** at the distal end of the catheter knob **20**. O-rings **46** are provided in the threaded distal bore **44** to minimize transverse vibrations. The proximal end of the catheter knob **20** receives the extension **70** of the transducer housing **24** and is supported by the slide collar assembly **22**. The slide collar assembly **22** is positioned over the distal end of the transducer housing **24**, and has a non-supporting position where the slide collar assembly **22** is retracted towards the transducer housing **24**, and has a supporting position where the slide collar assembly **22** is extended to cover at least a portion of the catheter knob **20**. Thus, the slide collar assembly **22** functions as a support member that is disposed on the transducer housing **24** to support at least a portion of the catheter knob **20**.

Referring also to FIGS. 5 and 6, the slide collar assembly **22** has an inner ring **50** (also referred to as collar **50**) and an outer ring **52** (also referred to as collar **52**). The inner ring **50** has a bore **54** and a longitudinal slit **58** that extends through the length of the inner ring **50**. The distal portion of the bore **54** can be stepped as shown at **55** (see FIG. 3) to function as a pushing surface that pushes a nesting piece **94** (described below) in a distal direction as the inner ring **50** is moved from the non-supporting position to the supporting position. The outer ring **52** also has a bore **56**, and has a narrowed proximal end **57**. The inner ring **50** is retained inside the bore **56** of the outer ring **52** and abuts the narrowed proximal end **57** which acts as a stop to limit the proximal movement of the inner ring **50**. Each of the inner ring **50** and the outer ring **52** has an opening **60** and **62**, respectively, that are aligned with each other and that are adapted to receive a locking pin **64**. A tubular inner sleeve **66** extends through the inside of the bore **54** of the inner ring **50** to ensleeve the first extension **70** of the transducer housing **24**, as explained below. The sleeve **66** has a proximal section **80** and an enlarged distal section **82**. The inner ring **50** is normally fitted around the proximal section **80** when the slide collar assembly **22** is in the non-supporting position, but the inner ring **50** is fitted around the distal section **82** when the slide collar assembly **22** is in the supporting position. Thus, providing the distal section **82** in an enlarged configuration allows for the inner ring **50** to achieve a friction-fit with the distal section **82**, while the inner ring **50** experiences a loose fit over the proximal section **80**.

The transducer housing **24** has a cylindrical wall **68** having a distal extension that comprises two stepped cylindrical extensions **70** and **72** extending from the distal end of the cylindrical wall **68**. The first extension **70** is attached to the distal end of the cylindrical wall **68**, and has a greater outer diameter than the second extension **72** that is attached to the distal end of the first extension **70**. A throughbore **76** extends from the hollow interior **78** of the cylindrical wall **68** and through the extensions **70** and **72**. The throughbore **76** can have the same diameter throughout its length. The second extension **72** is adapted to be received inside the proximal bore **90** of the catheter knob **20**, while the first extension **70** is

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received inside the sleeve 66. In addition, an opening 84 is provided in the proximal section 80 of the sleeve 66 and is aligned with a corresponding opening 86 on the first extension 70, with the openings 84, 86 adapted to receive a locking pin 88 that secures the sleeve 66 to the first extension 70 at a fixed position.

A longitudinal slot 92 is provided on the sleeve 66. When the slide collar assembly 22 is in the non-supporting position (i.e., inner ring 50 positioned over the proximal section 80), the slot 92 is opened. However, when the slide collar assembly 22 is moved to the supporting position, the inner ring 50 is positioned over the distal section 82 and compresses the enlarged distal section 82 to close the slot 92. With the slot 92 closed, the sleeve 66 provides a frictional grip of the proximal end 91 of the catheter knob 20.

Referring now to FIGS. 2-4 and 7-8, the catheter knob 20 has a proximal bore 90 that can be sleeved over the second extension 72 in a manner such that the outer surface of the catheter knob 20 can be substantially flush with the outer surface of the first extension 70 (as best shown in FIGS. 3 and 4). The proximal bore 90 houses the sonic connector 36 and a nesting piece 94. An elastic element 96, such as a spring, is seated in the distal part of the proximal bore 90, and has one end carried on a projection 98 provided at the distal end of the nesting piece 94. The nesting piece 94 has a generally cylindrical configuration and has a receptacle 100 which functions to selectively retain the sonic connector 36, as will be explained in greater detail below. In addition, a control ring 110 is positioned around the outer surface 112 of the catheter knob 20. The control ring 112 cooperates with the nesting piece 94 to move the nesting piece 94 in a reciprocal manner inside the proximal bore 90 of the catheter knob 20, as explained below.

The nesting piece 94 has two opposite and aligned openings 102; only the top opening 102 is shown in FIG. 7, but the bottom opening is the same and is aligned on a straight line with the top opening 102. Similarly, the catheter knob 20 has two opposite and aligned channels 104; only the top channel 104 is shown in FIG. 7, but the bottom channel is the same and is aligned on a straight line with the top channel 104. In addition, the control ring 110 has two opposite and aligned openings 114. The channels 104 and the openings 102, 114 are aligned, as best shown in FIGS. 3 and 4. Two opposing pins 106 are provided, with each pin 106 adapted to be fitted inside a corresponding set of channel 104 and openings 102, 114, so as to couple the control ring 110 and the nesting piece 94 as a unitary moving piece. The width of the channels 104 define the distal and proximal limits of movement for the control ring 110 and the nesting piece 94. The catheter knob 20 also has an annular flange 116 provided about its outer surface 112 that also defines the distal limit of the movement of the control ring 110.

In use, the sonic connector 36 is shown in FIGS. 3-4 as connecting the transducer horn 42 (e.g., with a threaded connection) with the ultrasound transmission member 32. The sonic connector 36 is always located at a fixed position inside the proximal bore 90 of the catheter knob 20. When the slide collar assembly 22 is in the non-supporting position shown in FIGS. 3, 9 and 11, the elastic element 96 normally biases the nesting piece 94 in the proximal direction so that the sonic connector 36 is received inside the receptacle 100 of the nesting piece 94 to be supported by the nesting piece 94. The proximal movement of the nesting piece 94 will cause the pins 106 to move in the proximal direction inside the channels 104, thereby causing the control ring 110 to move proximally away from the flange 116. The outer ring 52 and the inner ring 50 are positioned completely over the proximal section 80 of

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the sleeve 66, with the narrowed proximal end 57 positioned adjacent the cylindrical wall 68 of the transducer housing 24.

When the slide collar assembly 22 is now moved from the non-supporting position to the supporting position shown in FIGS. 4, 10 and 12, the user pushes the outer ring 52 in the distal direction. The step 55 on the distal end of the inner ring 50 engages the proximal end of the control ring 110 and pushes the control ring 110 in the distal direction. Movement of the control ring 110 in the distal direction will cause the pins 106 to move in the distal direction inside the channels 104, thereby causing the nesting piece 94 to counter the bias of the elastic element 96 and move in the distal direction. As the nesting piece 94 moves in the distal direction, the sonic connector 36 becomes free from the receptacle 100 of the nesting bore 94. In addition, the distal movement of the inner ring 50 will cause the inner surface of the inner ring 50 to engage the enlarged distal section 82 of the sleeve 66, which functions to close the slot 92 so as to frictionally grip the proximal portion 91 of the knob 20 when the slide collar assembly 22 is in the supporting position. The flange 116 and the width of the channels 104 function as stops to limit the distal movement of the control ring 110.

In the supporting position, the sonic connector 36 is not supported by the nesting piece 94 so that the sonic connector 36 can be free from any component or material interfaces, thereby promoting improved ultrasound energy propagation. The medical procedure can then be carried out while the slide collar assembly 22 is in the supporting position. Upon completion of the medical procedure, the above-described steps are reversed. In particular, the combined inner and outer rings 50, 52 (slide collar assembly 22) are retracted in the proximal direction so that they are now positioned over the proximal section 80 of the sleeve 66. The bias of the elastic element 96 will push the nesting piece 94 in the proximal direction so that the sonic connector 36 is received inside the receptacle 100 of the nesting piece 94. In addition, the proximal movement of the nesting piece 94 will cause the pins 106 to move in the proximal direction inside the channels 104, thereby causing the control ring 110 to move proximally away from the flange 116. Now, the catheter 10 can be disconnected from the transducer 34.

While the description above refers to particular embodiments of the present invention, it will be understood that many modifications may be made without departing from the spirit thereof. The accompanying claims are intended to cover such modifications as would fall within the true scope and spirit of the present invention.

What is claimed is:

1. A method of using an ultrasound system during a medical procedure, comprising:

a. providing an ultrasound system having:

an elongate flexible catheter having a proximal end, a distal end, and at least one lumen extending longitudinally therethrough;

an ultrasound transmission member extending through the lumen of the catheter body, the ultrasound transmission member having a proximal end;

an ultrasound transducer having a transducer horn;

a sonic connector that is directly connected to the proximal end of the ultrasound transmission member and attached to the transducer horn; and

a mechanism that is moveable with respect to the sonic connector; and

b. moving the mechanism from a first position where the sonic connector is attached to the transducer horn, to a second position where ultrasound energy is being propagated through the ultrasound transmission member;

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wherein the mechanism immediately surrounds the sonic connector when the mechanism is in the first position, and the mechanism is spaced-apart from, and does not surround, the sonic connector when the mechanism is in

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the second position to minimize energy loss during ultrasound energy propagation.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 7,758,510 B2
APPLICATION NO. : 11/192749
DATED : July 20, 2010
INVENTOR(S) : Nita et al.

Page 1 of 1

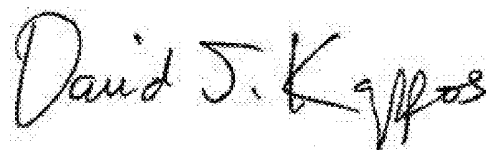
It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At Column 1, Line 8 (approximately), please delete “now pending.” and insert --now Pat. No.
6,942,620.--, therefor.

At Column 3, Line 49, please delete “Malinkrodt,” and insert --Mallinckrodt--, therefor.

At Column 6, Line 60, in Claim 1, after “attached” please insert --to--.

Signed and Sealed this
Twelfth Day of July, 2011

A handwritten signature in black ink, reading "David J. Kappos". The signature is written in a cursive, flowing style with a large initial "D" and a stylized "K".

David J. Kappos
Director of the United States Patent and Trademark Office

专利名称(译)	用于将超声导管固定到换能器的连接		
公开(公告)号	US7758510	公开(公告)日	2010-07-20
申请号	US11/192749	申请日	2005-07-29
[标]申请(专利权)人(译)	FLOWCARDIA		
申请(专利权)人(译)	FLOWCARDIA INC.		
当前申请(专利权)人(译)	FLOWCARDIA INC.		
[标]发明人	NITA HENRY TRAN MARTINOS		
发明人	NITA, HENRY TRAN, MARTINOS		
IPC分类号	A61B8/14 A61B6/00 A61B8/12		
CPC分类号	A61B8/12 A61B8/445 A61B17/320068 C08L2201/12 A61B2017/00867		
助理审查员(译)	SHAHRESTANI, 纳西尔		
其他公开文献	US20050283080A1		
外部链接	Espacenet USPTO		

摘要(译)

超声系统具有超声换能器，其具有换能器壳体和设置在换能器壳体的远端处的喇叭，超声传输构件，连接到喇叭和超声传输构件的近端的声波连接器，以及导管旋钮具有近端，该近端连接到换能器壳体的远端。导管旋钮具有容纳声波连接器的近端孔。该系统还包括嵌套件，该嵌套件保持在导管旋钮的近端孔内。嵌套件可以从第一位置移动到第二位置，在第一位置，声波连接器被接收在嵌套件内，在第二位置，当超声能量传播通过超声传输构件时，声波连接器与嵌套件分离。

