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CHANG et al.(10) **Pub. No.: US 2014/0257110 A1**(43) **Pub. Date: Sep. 11, 2014**(54) **ULTRASOUND PROBE STRUCTURE OF
GUIDING THE PUNCTURE NEEDLE**(30) **Foreign Application Priority Data**

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CHEN, Miaoli County (TW)(52) **U.S. Cl.**
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USPC **600/461**(73) Assignees: **National Health Research Institutes,**
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(TW)(57) **ABSTRACT**

An ultrasound probe structure dedicated for guiding the puncture needle. It has a passage in the center of the structure and the diameter of the passage is equal to the outer diameter of puncture needle. The bony and non-bony tissues can be distinguished according to the strength of the echoes so that the puncture needle can be guided to avoid hitting the bony tissue before or during insertion.

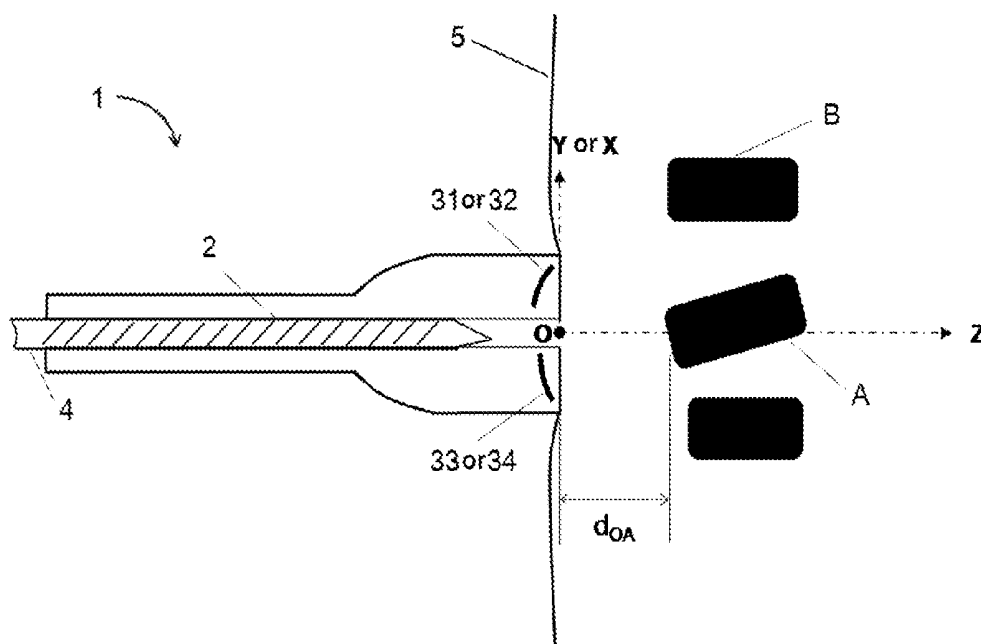
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FIG. 1A

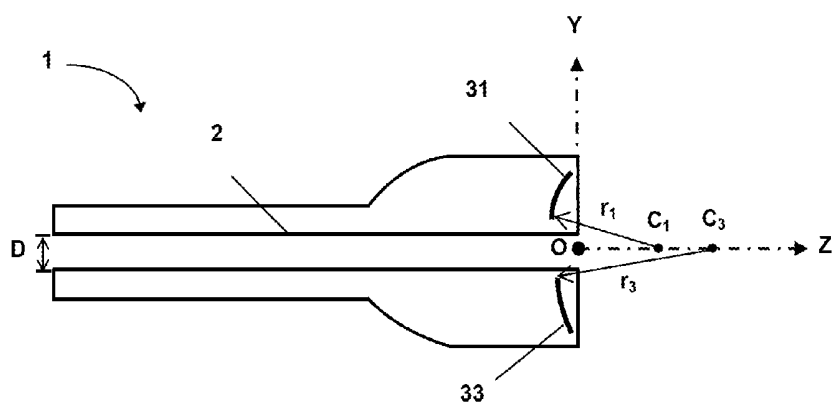


FIG. 1B

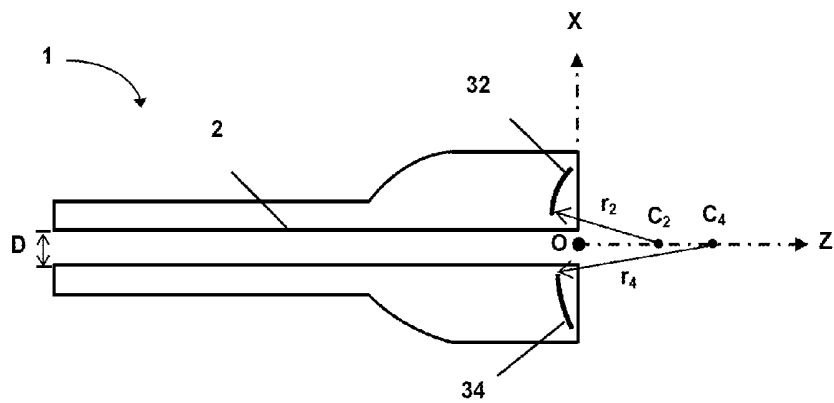


FIG. 1C

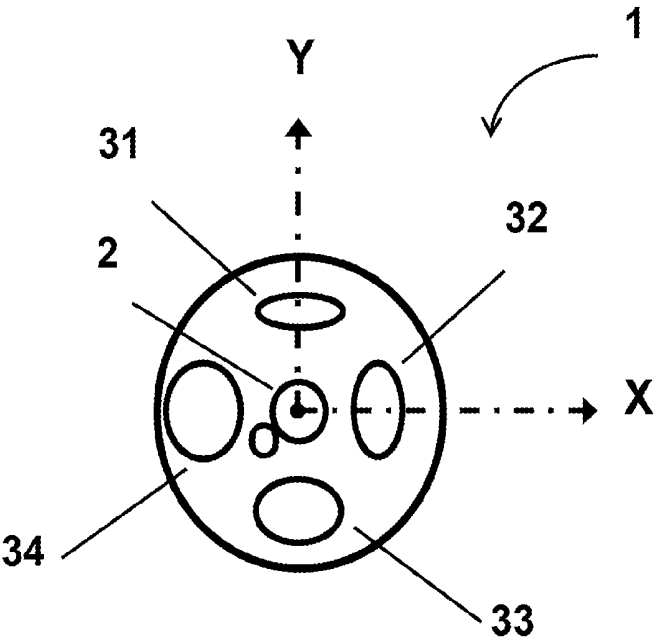


FIG. 2A

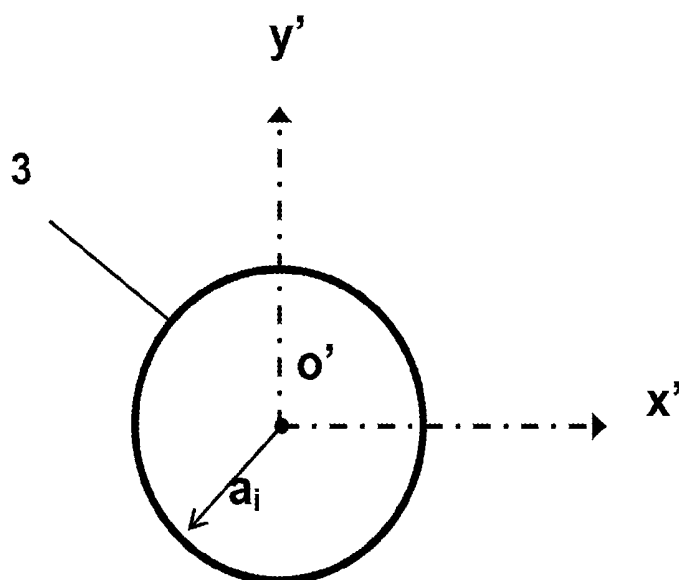


FIG. 2B

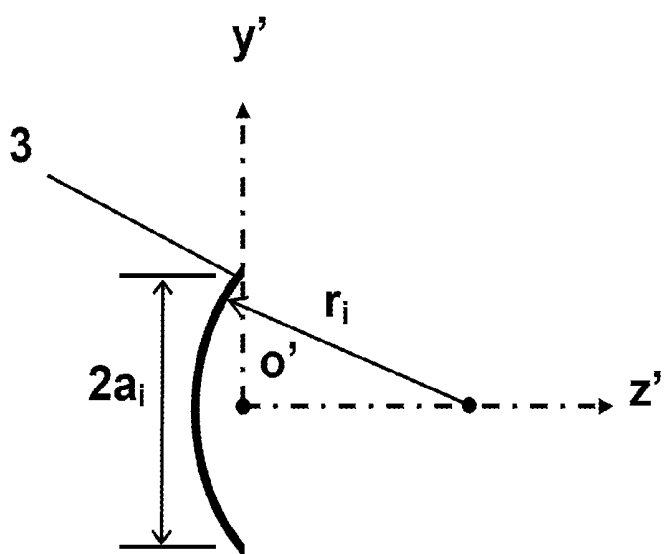


FIG. 3A

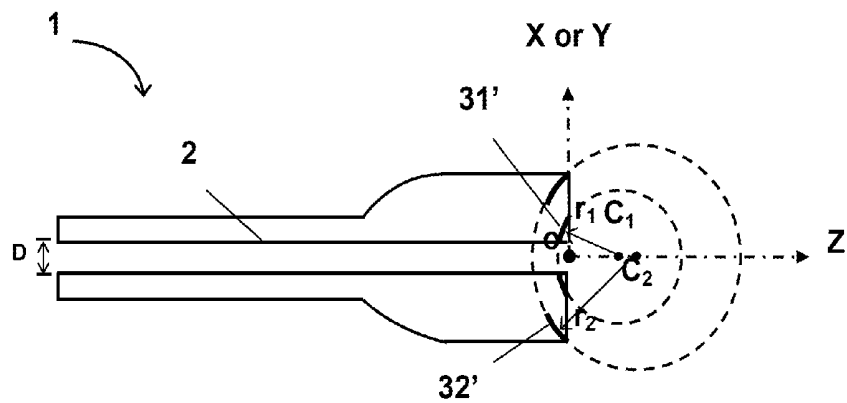


FIG. 3B

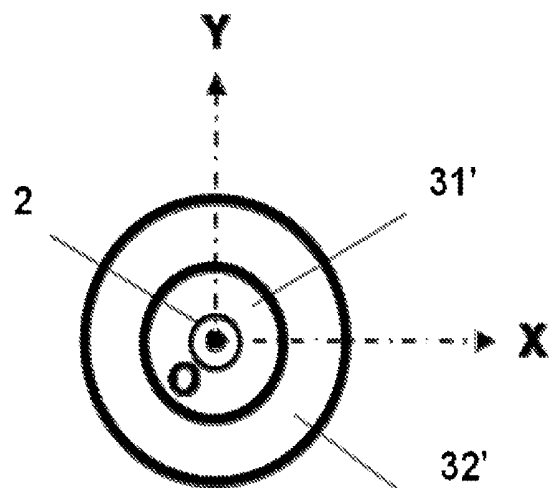


FIG. 3C

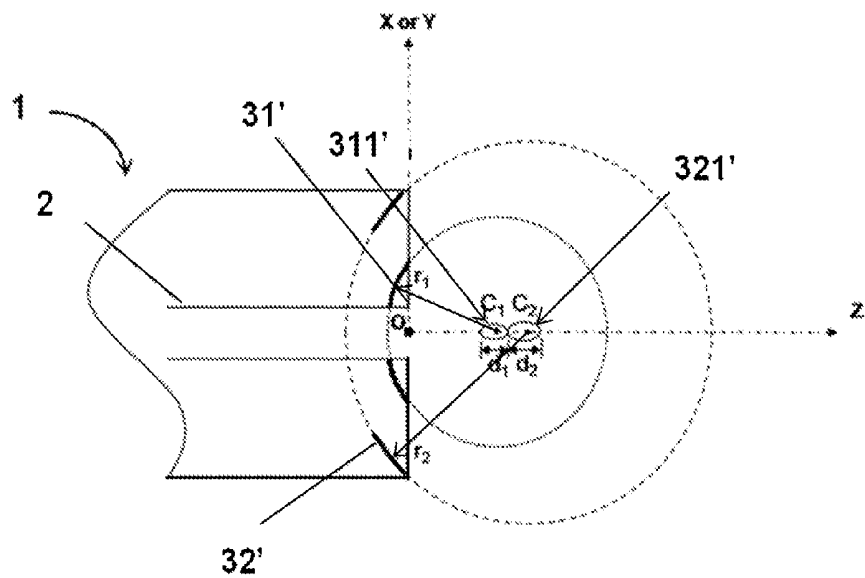


FIG. 4A

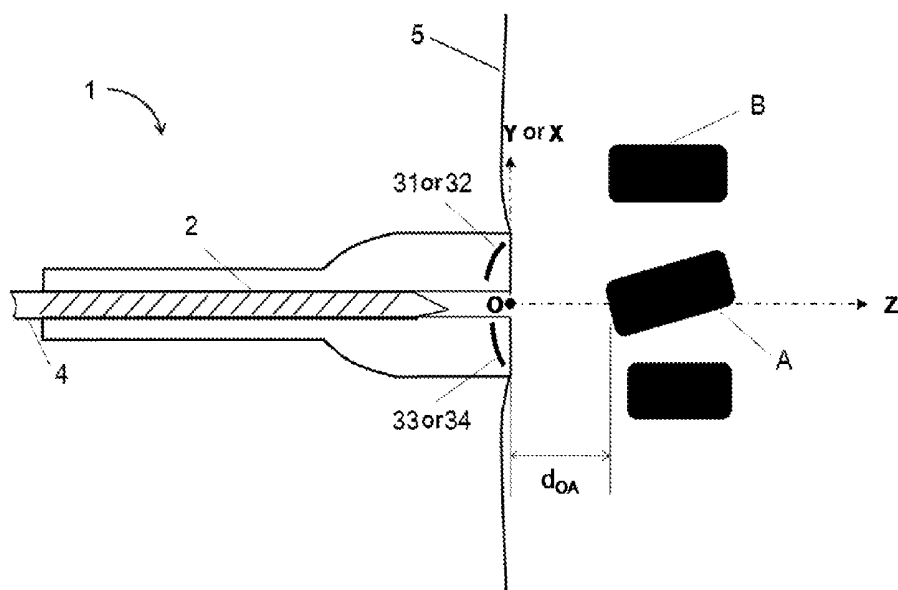


FIG. 4B

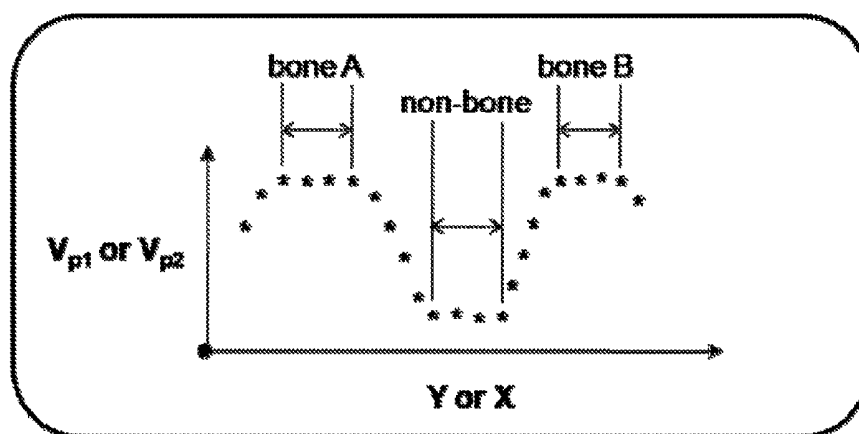


FIG. 5A

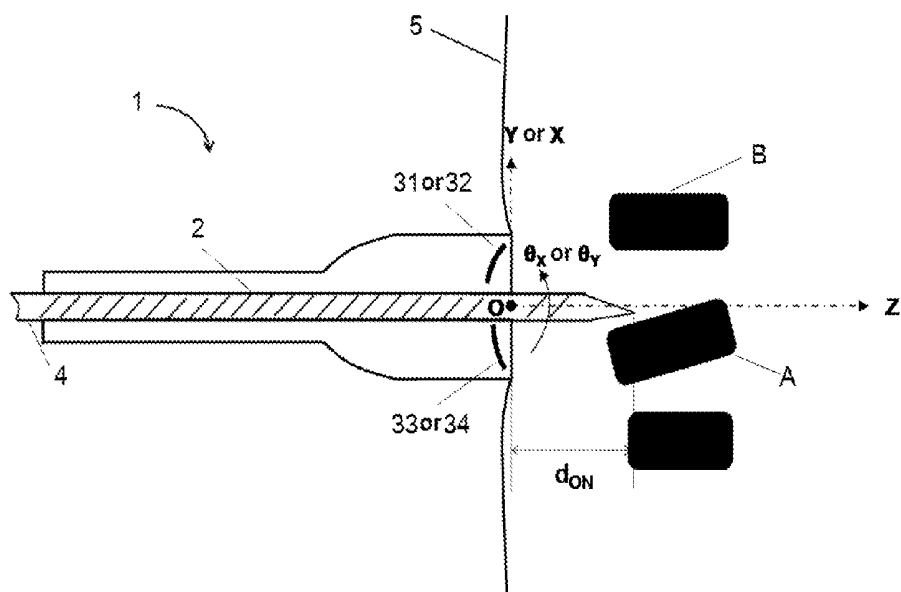
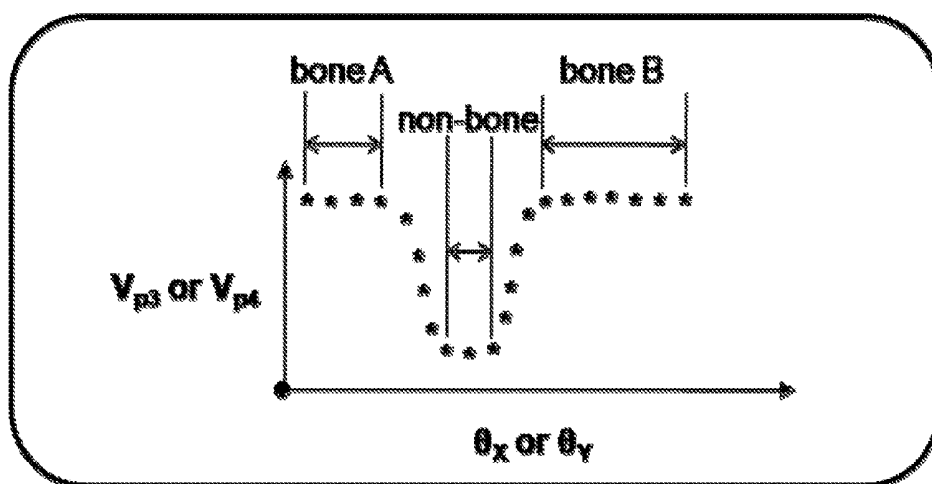


FIG. 5B



ULTRASOUND PROBE STRUCTURE OF GUIDING THE PUNCTURE NEEDLE

FIELD OF THE INVENTION

[0001] The present invention relates generally to an ultrasound probe with special structure, which is quite different from ordinary ones. Its operation frequency, radius of curvature, aperture diameter and special configuration of the piezoelectric transducer provide the insertion pathway of the needle, which is punctured into tissues, to be the same as the direction of the ultrasound guiding beam.

BACKGROUND OF THE INVENTION

[0002] Currently, the technique of tissue puncture for medical purpose is widely employed in clinics, such as anesthesia, analgesia, biopsy, aspiration, and etc. In a case, for example, during the procedure of epidural block in traditional way, it is not avoidable to hit the bony tissue under the blind fashion for needle puncture.

[0003] In recent years, the technique of needle puncture guided by ultrasound imaging for nerve block is frequently employed in clinics. Generally, a doctor operates the puncture needle with one or two hands and the other hand or a physician assistant operates the ultrasound probe to derive the image of tissues. It can be imagined that this kind of procedure is not ideal for two-man's or one-man's operation due to possible difficulty of coordination.

[0004] The recent ultrasound imaging systems for needle guidance in the market include GE LOGIQ e, Philips HD11 XE, SonoSite MicroMaxx, Zonare Medical Systems zone ultra, and etc. However, the ultrasound probes in those systems are unable to integrate with the puncture needle, or the ultrasound probe and the puncture needle are separate elements, so that the direction of ultrasound beam is not co-axial with the directions of the needle during puncture. In other words, the directions of ultrasound beam and the pathway of needle insertion will be not the same in these systems.

SUMMARY OF THE INVENTION

[0005] The objective of this invention is to provide an ultrasound probe with capability of integrating the puncture needle with co-axial feature, in the direction of ultrasound beam and the pathway of needle puncturing

[0006] One feature of this invention is the integration of the ultrasound probe and the puncture needle. The geometric center of the ultrasound probe is designed with an adaptive passage corresponding to the outer diameter of the puncture needle for allowing the puncture needle to pass through.

[0007] Another feature of this invention is that either for A-mode or B-mode ultrasound probe is relatively easy to operate.

[0008] Another advantage of this invention is that the ultrasound probe includes at least two focal lengths, aperture diameters, and operation frequencies. The best focal length and the frequency may be designed according to the anatomical structure and the distribution of the puncture site close to the bone tissue.

[0009] To achieve the aims mentioned above, an ultrasound probe structure is provided and comprises an ultrasound probe, arranged a hollow passage in the center of the ultrasound probe; wherein the size of a focal zone and the operation frequency of each transducer are used to determine the range of a detecting area of the ultrasound probe.

[0010] So that the manner in which the above recited features of the present invention can be understand in detail, a more particular description of the invention, briefly summarized above, may be obtained by reference to embodiments, some of which are illustrated in the appended drawings. It is noted, however, that the appended drawings illustrate only typical embodiments of this invention and are therefore not to be considered limiting of its scope, for the invention may admit to other equally effective embodiments.

BRIEF DESCRIPTION OF THE DRAWINGS

[0011] FIG. 1A is a sectional view showing a first embodiment of a center of a probe structure in YZ plan in accordance with this invention.

[0012] FIG. 1B is a sectional view showing the first embodiment of the center of the probe structure in XZ plan in accordance with this invention.

[0013] FIG. 1C is a sectional view showing the first embodiment of the center of the probe structure in XY plan in accordance with this invention.

[0014] FIG. 2A is a sectional view showing a first embodiment of a piezoelectric transducer in X'Y' plan in accordance with this invention.

[0015] FIG. 2B is a sectional view showing a first embodiment of a piezoelectric transducer in Y'Z' plan in accordance with this invention.

[0016] FIG. 3A is a sectional view showing a second embodiment of a center of a probe structure in XZ or YZ plan in accordance with this invention.

[0017] FIG. 3B is a sectional view showing the second embodiment of the center of the probe structure in XZ plan in accordance with this invention.

[0018] FIG. 3C is a sectional view showing a second embodiment of a piezoelectric transducer in XZ or YZ plan in accordance with this invention.

[0019] FIG. 4A is a schematic drawing showing the operation before puncturing in accordance with this invention.

[0020] FIG. 4B is a schematic drawing showing the echo signal before puncturing in accordance with this invention.

[0021] FIG. 5A is a schematic drawing showing the operation while puncturing in accordance with this invention.

[0022] FIG. 5B is a schematic drawing showing the echo signal while puncturing in accordance with this invention.

DETAILED DESCRIPTION OF THE INVENTION

[0023] The terms used in this specification generally have their ordinary meanings in the art, within the context of the invention, and in the specific context where each term is used. Certain terms that are used to describe the invention are discussed below, or elsewhere in the specification, to provide additional guidance to the practitioner regarding the description of the invention. For convenience, certain terms may be highlighted, for example using italics and/or quotation marks. The use of highlighting has no influence on the scope and meaning of a term; the scope and meaning of a term is the same, in the same context, whether or not it is highlighted. It will be appreciated that same thing can be said in more than one way. Consequently, alternative language and synonyms may be used for any one or more of the terms discussed herein, nor is any special significance to be placed upon whether or not a term is elaborated or discussed herein. Synonyms for certain terms are provided. A recital of one or more synonyms does not exclude the use of other synonyms. The

use of examples anywhere in this specification including examples of any terms discussed herein is illustrative only, and in no way limits the scope and meaning of the invention or of any exemplified term. Likewise, the invention is not limited to various embodiments given in this specification.

[0024] Unless otherwise defined, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention pertains. In the case of conflict, the present document, including definitions will control.

[0025] The ultrasound probe in this invention may have at least one piezoelectric transducer, and the corresponding operations of the probe with four transducers, which demonstrate for A-mode only, are described in below as an example, respectively.

[0026] The center of the ultrasound probe **1** of this invention has a circular hollow passage **2**, shown as FIGS. 1A and 2A. The size of the diameter D of the hollow passage **2** is designed according to the diameter of the puncture needle. The ultrasound probe **1** includes a plurality of piezoelectric transducers. This embodiment is described with four piezoelectric transducers, shown as FIG. 1C. Each piezoelectric transducer has a spherical bowl structure, and all piezoelectric transducers are arranged to surround the hollow passage **2**. The arrangement is that the radii of the piezoelectric transducers are disposed with the same O-Z center line of the ultrasound probe **1**, such as the first piezoelectric transducer **31**, the second piezoelectric transducer **32**, the third piezoelectric transducer **33**, and the fourth piezoelectric transducer **34** with radii of curvature $r_1 \sim r_4$ respectively, shown as FIGS. 1A and 1B. Such arrangement may be confirmed that each piezoelectric transducer is capable of deriving the strongest echo signal on the path which the puncture needle goes forward. And the radii of the transducers curvatures and the aperture diameters of the transducers may be designed to make the ultrasound probe **1** to detect the A-mode signal from shallow to deep. The similar arrangement can also be applied to a linear array or phase array B-mode ultrasound probe. The radii of curvature $r_1 \sim r_4$ of the first, second, third, and fourth piezoelectric transducers **31**, **32**, **33**, **34** are $r_1 > r_2 > r_3 > r_4$. Therefore, the range of depth detected by the ultrasound probe **1** may be $C_1 \sim C_4$ (FIGS. 1A and 1B).

[0027] Please refer to FIGS. 2A and 2B, the piezoelectric transducer **3** is further described. The detecting range along the O'-Z' line of the ultrasound probe **1** is determined by the width of the focal zone of each piezoelectric transducer **3**. The aperture diameter of the piezoelectric transducer **3** is $2a_i$, the radius of curvature of the piezoelectric transducer **3** is r_i , and the f-number of the piezoelectric transducer **3** is defined as $r_i/2a_i$. The width of focal zone of the piezoelectric transducer **3** is proportional to the f-number thereof, thus the width of focal zone is adjusted by the f-number. However, the lateral resolution of the piezoelectric transducer **3** may be reduced while the width of the focal zone is increased. The lateral resolution may be increased by the relationship, that is, the operation frequency is inversely proportional to the focal length. Accordingly, the ultrasound probe **1** may be designed with several different piezoelectric transducers **3** to adjust the detecting range to achieve different aspects of clinical application.

[0028] Another structure of the ultrasound probe and the arrangement of the piezoelectric transducer are shown as FIGS. 3A and 3B. The center of the ultrasound probe **1** of this invention is a circular hollow passage **2**. The diameter D of the

hollow passage **2** is designed according to the diameter of the puncture needle. The ultrasound probe **1** includes a plurality of piezoelectric transducer **3**. This embodiment is described with two piezoelectric transducers **3**. These two piezoelectric transducers **3** have curved ring structure, and the radii of curvature C_1 and C_2 are disposed with the same O-Z center line of the ultrasound probe **1**, shown as the radii of curvature r_1 and r_2 of the first and second piezoelectric transducers **31'** and **32'** in FIG. 3A. Such arrangement may be confirmed that each piezoelectric transducer **3** is capable of deriving the strongest echo signal from tissues in the path which the puncture needle **4** goes forward. And the operation frequencies, the radii of curvature and the aperture diameters of the transducers may be designed to make the ultrasound probe **1** detect the A-mode signal from shallow to deep. Same idea is also applicable to the B-mode structure. The first and second focal zones **311'**, **321'** shown as FIG. 3C are generated by the first and second piezoelectric transducers **31'** and **32'**. The focal lengths of the first and second focal zones **311'**, **321'** are d_1 and d_2 respectively, and the depth range detected by the ultrasound probe **1** may be $d_1 + d_2$.

[0029] The operation of this invention is shown as FIGS. 4A and 4B. Before the puncture needle **4** is inserted into skin **5**, the doctor may operate the ultrasound probe **1** to move along Y or X direction, shown as FIG. 4A, and recognize the bone tissue by the strength of the echo signal from tissues. When the distance d_{OA} between the bone tissue and the ultrasound probe **1** is within the range, which is able to detect the first piezoelectric transducer **31** or the second piezoelectric transducer **32**, the relationship of the peak amplitude of the echo signal and the ultrasound probe **1** in the Y or X direction may be shown as FIG. 4B, that is, the VP1 and VP2 are referred to the peak amplitudes of echo signals detected by the first and second piezoelectric transducers **31** and **32**, respectively.

[0030] In addition, when the O-Z center line of the ultrasound probe **1** passes through the bone tissue A as shown in FIG. 4B, the voltage value of the echo signal is relatively high and the doctor may move the ultrasound probe **1** to either Y or X direction. When the voltage value of the echo signal is relatively low, the doctor may continuously move the ultrasound probe **1** in the same direction till the voltage value of the echo signal becomes high again. Therefore, the doctor may be informed the range of low echo signal, and further the non-bone area in the Y or X direction is recognized. Once the non-bone area is confirmed the doctor starts to insert the needle.

[0031] When the puncture needle **4** is inserted in the body, the echo signal of the deep bone tissue may be detected by the third piezoelectric transducer **33** or by the fourth piezoelectric transducer **34** and the inserting depth d_{ON} may be estimated by the scaling bars marked on the puncture needle **4**. The doctor may confirm the echo signal of the third piezoelectric transducer **33** or the fourth piezoelectric transducer **34** with the value of d_{ON} . When the puncture needle **4** is encountered the condition which is shown as FIG. 5A, the peak amplitudes of echo signals V_{P3} and V_{P4} detected by the third piezoelectric transducer **33** or the fourth piezoelectric transducer **34** shall display relatively high values. When θ_x or θ_y is zero degree, shown as FIG. 5B, V_{P3} and V_{P4} are relatively high. At this time, the doctor may rotate the ultrasound probe **1** along the Y or X axis. When θ_x or θ_y is located in the some range, i.e. the O-Z center line of the ultrasound probe **1** does not pass through the bone tissue A and the bone tissue B, V_{P3} and V_{P4}

shall have relatively low values. At this time, the doctor may continuously insert the needle until the target is reached. The configuration of various piezoelectric transducers in the ultrasound probe with coaxial feature of the ultrasound beam and the direction of needle insertion path can be realized by using the technique mentioned above.

[0032] The operation of the transducer, shown as FIGS. 3A and 3B, is similar to that mentioned above, that is, the depths of the bone tissue may be detected by the size of focal zones of different piezoelectric transducers.

[0033] The foregoing description of the exemplary embodiments of the invention has been presented only for the purposes of illustration and description and is not intended to be exhaustive or to limit the invention to the precise forms disclosed. Many modifications and variations are possible in light of the above teaching.

[0034] The embodiments and examples were chosen and described in order to explain the principles of the invention and their practical application so as to enable others skilled in the art to utilize the invention and various embodiments and with various modifications as are suited to the particular use contemplated. Alternative embodiments will become apparent to those skilled in the art to which the present invention pertains without departing from its spirit and scope. Accordingly, the scope of the present invention is defined by the appended claims rather than the foregoing description and the exemplary embodiments described therein.

[0035] Some references, which may include patents, patent applications and various publications, are cited and discussed in the description of this invention. The citation and/or discussion of such references is provided merely to clarify the description of the present invention and is not an admission that any such reference is "prior art" to the invention described herein. All references cited and discussed in this specification are incorporated herein by reference in their entireties and to the same extent as if each reference was individually incorporated by reference.

What is claimed is:

1. An ultrasound probe structure, at least comprising: an ultrasound probe, arranged a hollow passage in the center of the ultrasound probe; a plurality of transducers, arranged to surround the passage; wherein the size of a focal zone and the operation frequency of each transducer are used to determine the range of detecting area of the ultrasound probe.
2. The probe structure as claimed in claim 1, wherein, a diameter of the passage is designed according to a diameter of the puncture needle.
3. The probe structure as claimed in claim 1, wherein, the shape of each transducer is a spherical bowl shape or a curved ring shape.
4. The probe structure as claimed in claim 1, wherein, an arrangement of the transducers is that the radius of curvature of each transducer is disposed with the center line of the ultrasound probe.
5. The probe structure as claimed in claim 3, wherein, the detecting area of the transducer which has the spherical bowl shape is determined by its focal width; and the range of detecting area of the transducer which has the curved ring shape is determined by its focal length.
6. The probe structure as claimed in claim 5, wherein, the focal width of the transducer which has the spherical bowl shape is adjusted by the f number and the operation frequency, wherein the f number is defined as $r_i/2a_i$, r_i is the radius of the transducer, and $2a_i$ is the aperture diameter of the transducer.
7. The probe structure as claimed in claim 5, wherein, the focal length of the transducer which has the curved ring shape is adjusted by the f number and the operation frequency.
8. The probe structure as claimed in claim 3, wherein, the lateral resolution of the transducer which has the spherical bowl shape or the transducer which has the curved ring shape is improved by increase the operation frequency.

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摘要(译)

一种专用于引导穿刺针的超声探头结构。它在结构的中心有一个通道，通道的直径等于穿刺针的外径。可以根据回声的强度来区分骨和非骨组织，从而可以引导穿刺针以避免在插入之前或插入期间撞击骨组织。

