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(54) **ADAPTIVELY PERFORMING CLUTTER
FILTERING IN AN ULTRASOUND SYSTEM**

(52) **U.S. Cl. 600/453; 382/260**

(57) **ABSTRACT**

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Embodiments of adaptively performing clutter filtering are disclosed. In one embodiment, by way of non-limiting example, an ultrasound system comprises: an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object to output a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image; and a processing unit in communication with the ultrasound data acquisition unit and being configured to calculate a power difference value corresponding to each of the pixels based on the plurality of ultrasound data, determine whether the power difference value is equal to or larger than a first threshold value, and if the power difference value is equal to or larger than the first threshold value, then perform first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then perform second clutter filtering upon the plurality of ultrasound data.

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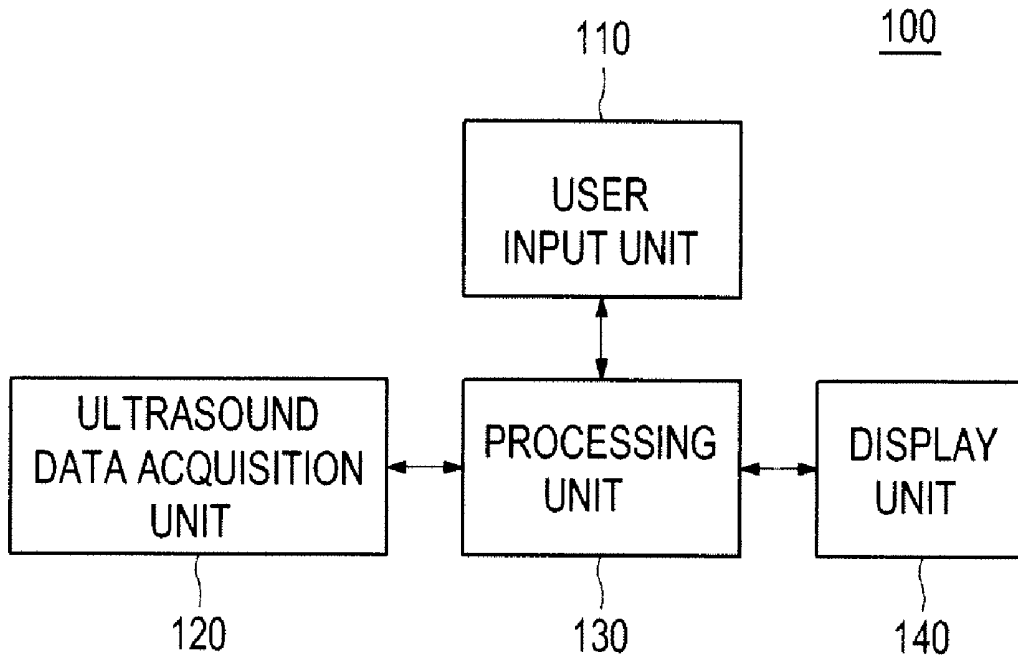


FIG. 1

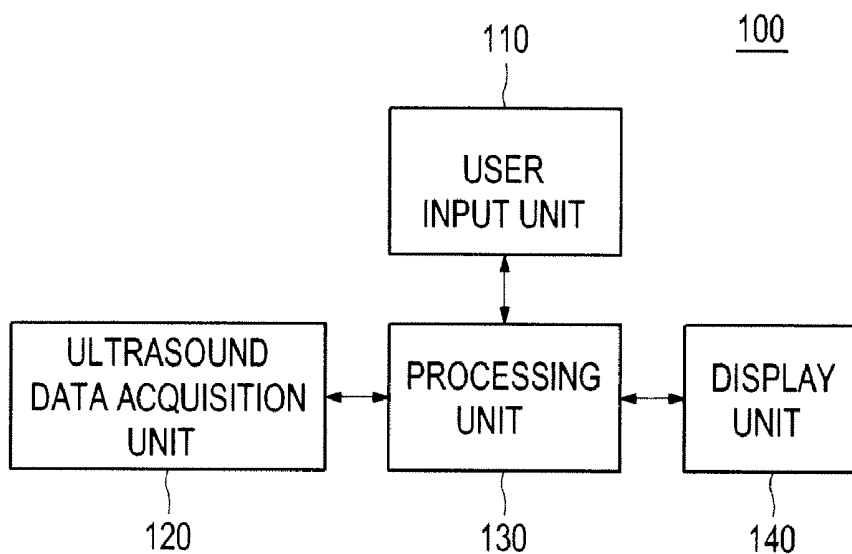


FIG. 2

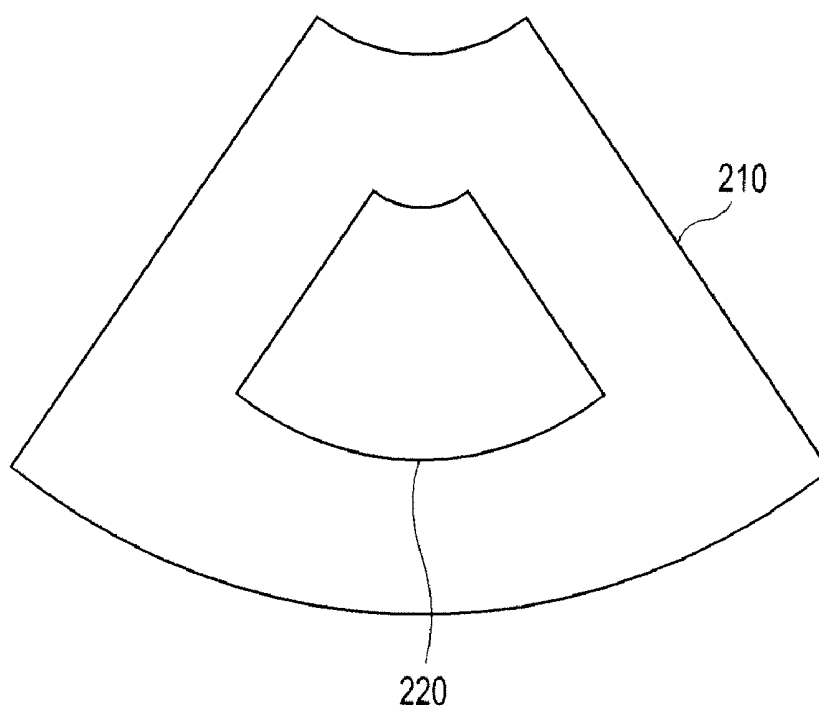


FIG. 3

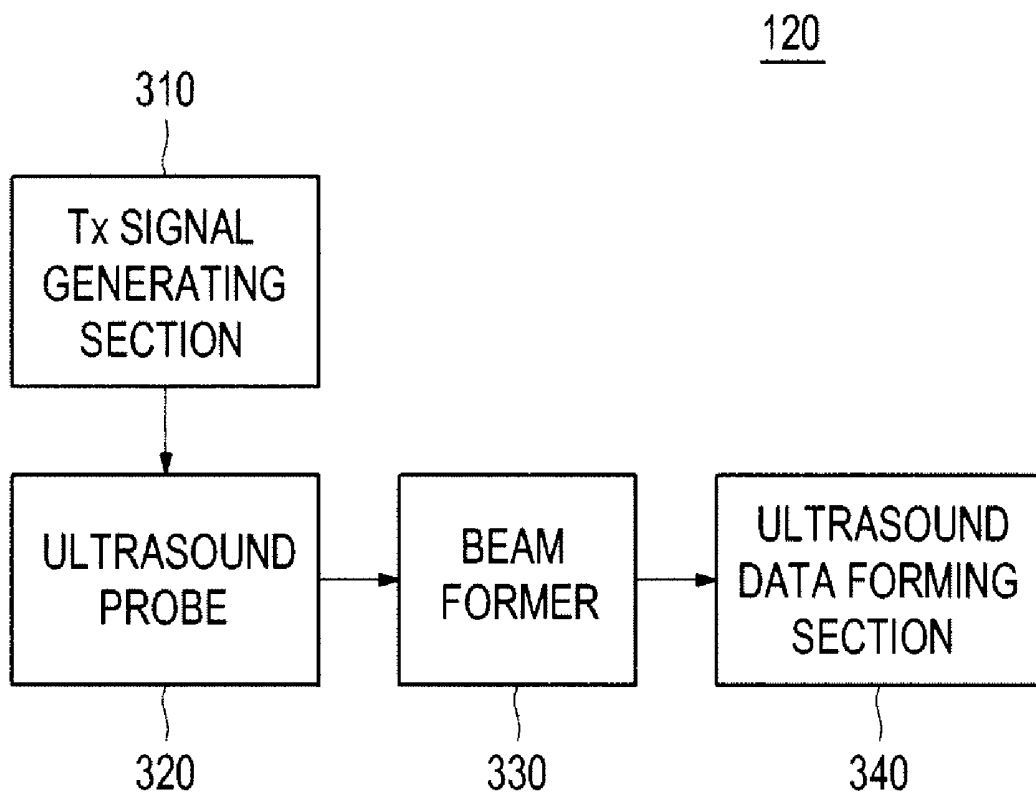


FIG. 4

130

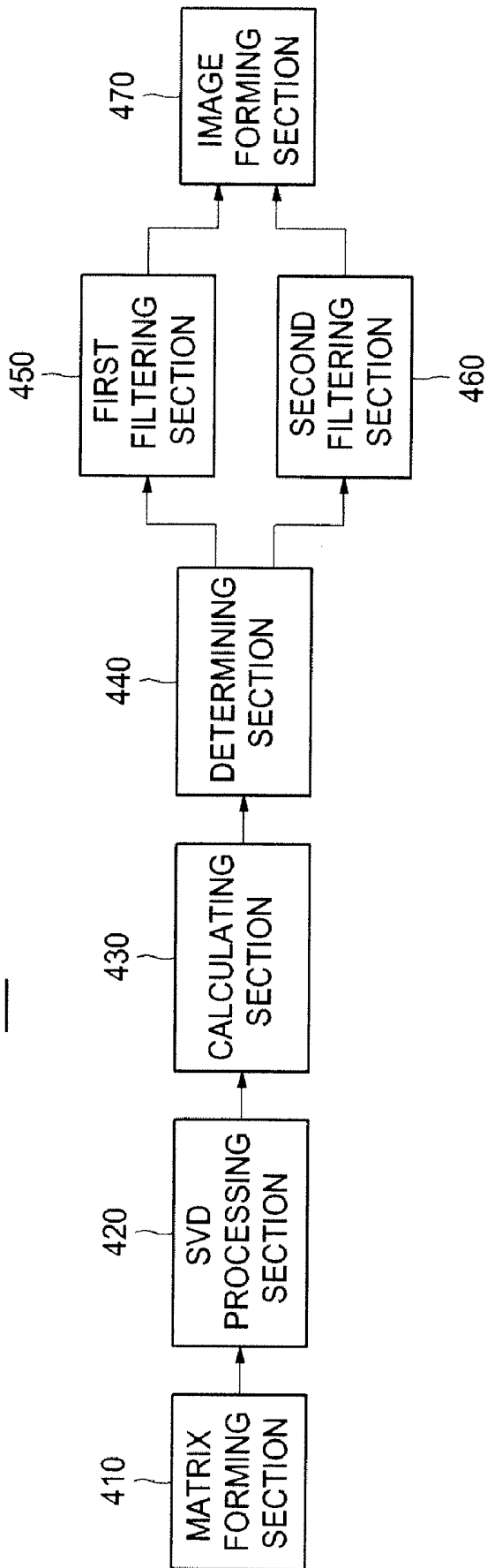


FIG. 5

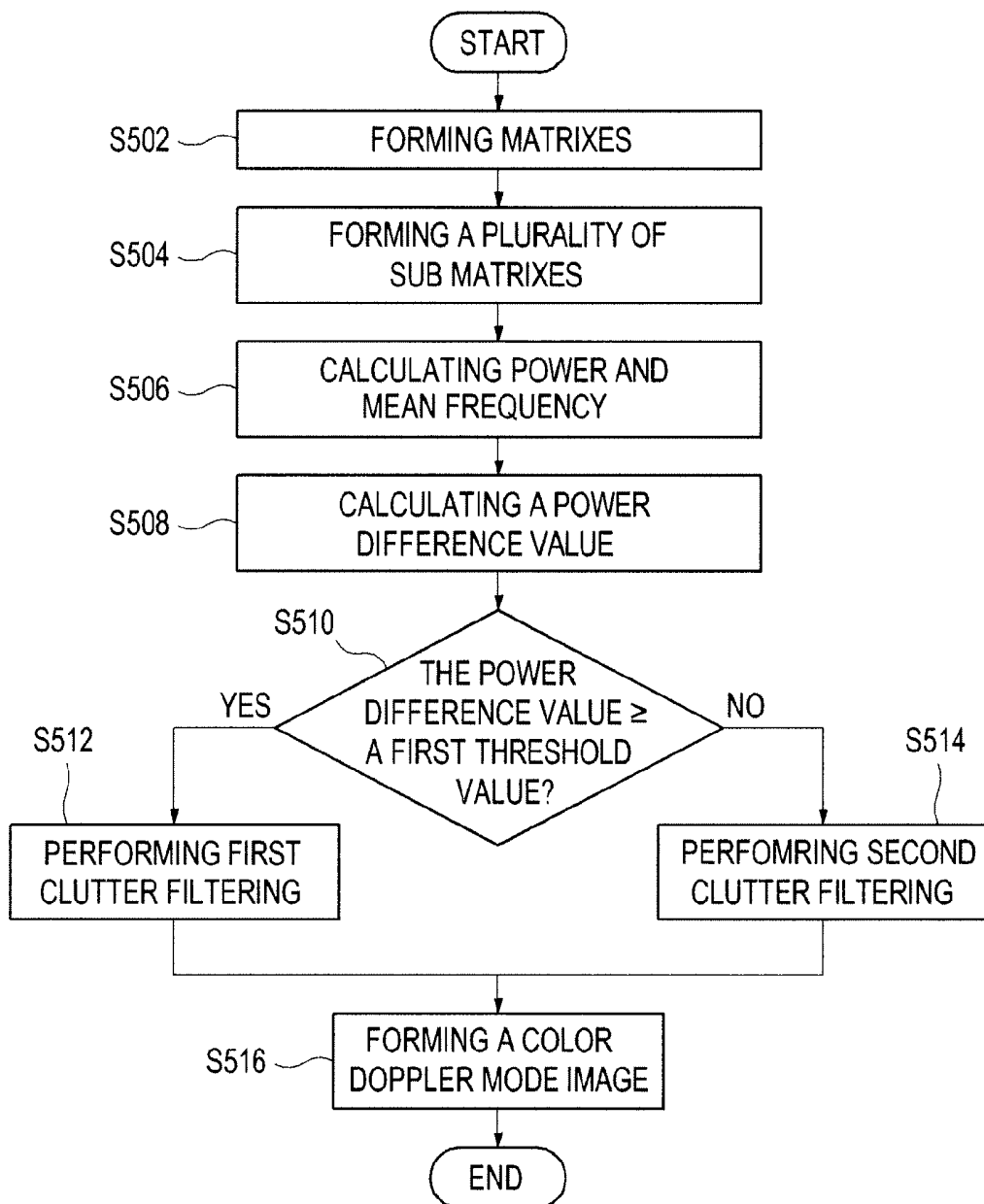
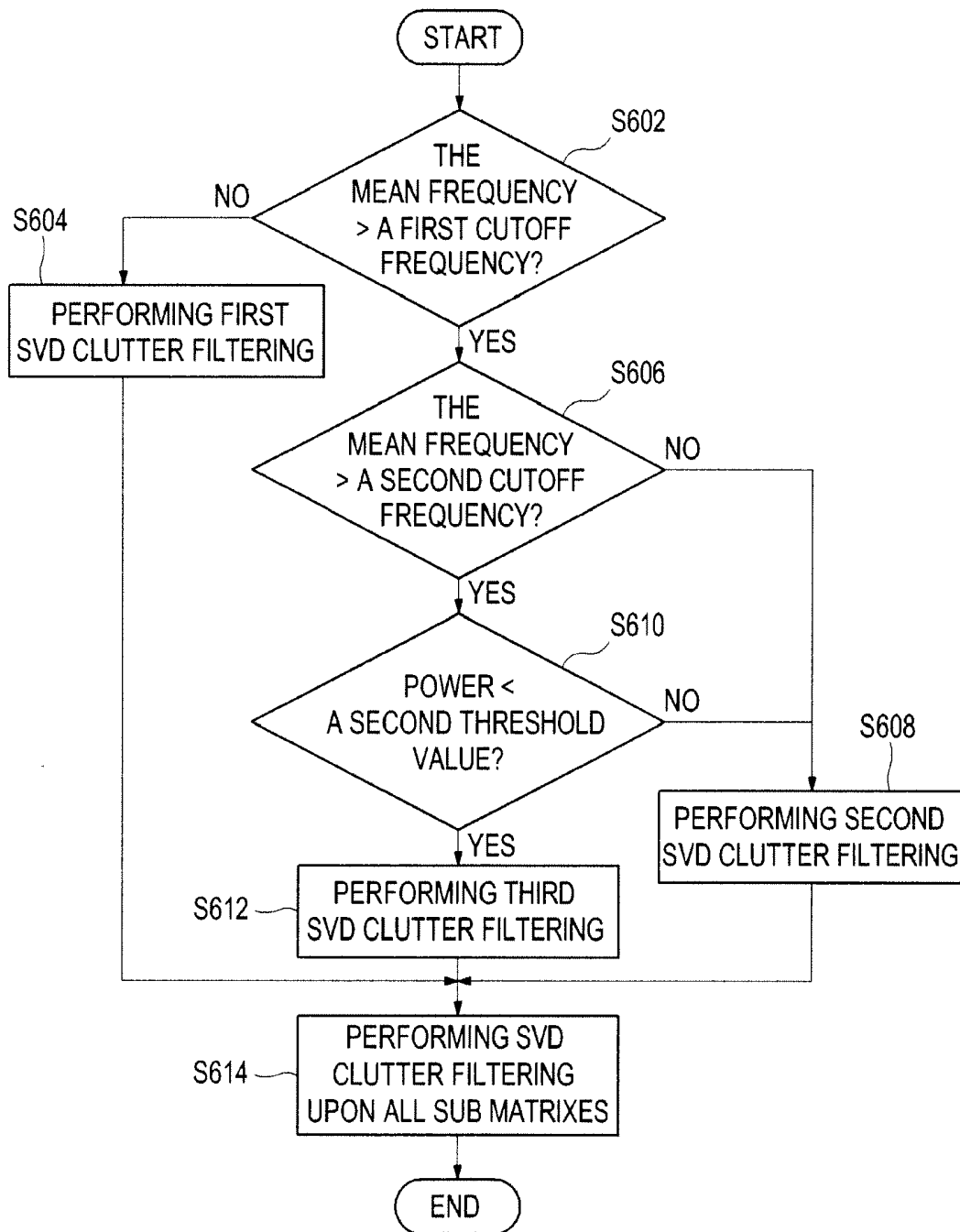


FIG. 6



ADAPTIVELY PERFORMING CLUTTER FILTERING IN AN ULTRASOUND SYSTEM

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] The present application claims priority from Korean Patent Application No. 10-2009-0110223 filed on Nov. 16, 2009, the entire subject matter of which is incorporated herein by reference.

TECHNICAL FIELD

[0002] The present disclosure generally relates to ultrasound systems, and more particularly to adaptively performing clutter filtering in an ultrasound system.

BACKGROUND

[0003] An ultrasound system has become an important and popular diagnostic tool since it has a wide range of applications. Specifically, due to its non-invasive and non-destructive nature, the ultrasound system has been extensively used in the medical profession. Modern high-performance ultrasound systems and techniques are commonly used to produce two or three-dimensional ultrasound images of internal features of a target object (e.g., human organs).

[0004] To provide the ultrasound images, the ultrasound system operates in various image modes such as a brightness mode (B mode), a Doppler mode and the like to acquire ultrasound images for diagnosis.

[0005] In the Doppler mode, the ultrasound system provides a color Doppler mode image showing velocities of moving objects such as the heart, blood flow, etc. The color Doppler mode image may be formed based on Doppler signals obtained by alternately transmitting and receiving ultrasound signals to and from a target object. The Doppler signals may include a low frequency signal (so-called clutter signal) due to the motion of a cardiac wall or valve of a heart. The clutter signal may have an amplitude which is over 100 times greater than that of pure Doppler signals indicative of velocities of the blood flow. The clutter signal may be an obstacle for accurately detecting the velocity of blood flow. Thus, it is required to remove the clutter signal from the Doppler signals for an accurate velocity detection of the blood flow. The ultrasound system typically adopts a clutter filter that may be a high pass filter, an eigenvector-based clutter filter, a singular value decomposition (SVD) clutter filter and the like to remove the clutter signal from the Doppler signals.

SUMMARY

[0006] Embodiments for adaptively setting an optimal image parameter in an ultrasound system are disclosed herein. In one embodiment, by way of non-limiting example, an ultrasound system comprises: an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object to thereby output a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image; and a processing unit in communication with the ultrasound data acquisition unit and being configured to calculate a power difference value corresponding to each of the pixels based on the plurality of ultrasound data, determine whether the power difference value is equal to or larger than a first threshold value, and if the power difference value is equal to or larger than the first threshold value, then perform first clutter filtering upon the plurality of ultrasound data, or if

the power difference value is less than the first threshold value, then perform second clutter filtering upon the plurality of ultrasound data.

[0007] In another embodiment, there is provided a method of performing clutter filtering, comprising: a) acquiring a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image for a target object; b) calculating a power difference value corresponding to each of the pixels based on the plurality of ultrasound data; c) determining whether the power difference value is equal to or larger than a first threshold value; and d) if the power difference value is equal to or larger than the first threshold value, then performing first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then performing second clutter filtering upon the plurality of ultrasound data.

[0008] In yet another embodiment, there is provided a computer readable medium comprising computer executable instructions configured to perform the following acts: a) acquiring a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image for a target object; b) calculating a power difference value corresponding to each of the pixels based on the plurality of ultrasound data; c) determining whether the power difference value is equal to or larger than a first threshold value; and d) if the power difference value is equal to or larger than the first threshold value, then performing first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then performing second clutter filtering upon the plurality of ultrasound data.

[0009] The Summary is provided to introduce a selection of concepts in a simplified form that are further described below in the Detailed Description. This Summary is not intended to identify key or essential features of the claimed subject matter, nor is it intended to be used in determining the scope of the claimed subject matter.

BRIEF DESCRIPTION OF THE DRAWINGS

[0010] FIG. 1 is a block diagram showing an illustrative embodiment of an ultrasound system.

[0011] FIG. 2 is a schematic diagram showing an example of a brightness mode (B mode) image and a region of interest (ROI).

[0012] FIG. 3 is a block diagram showing an illustrative embodiment of an ultrasound data acquisition unit.

[0013] FIG. 4 is a block diagram showing an illustrative embodiment of a processing unit.

[0014] FIG. 5 is a flow chart showing a process of adaptively performing clutter filtering.

[0015] FIG. 6 is a flow chart showing a process of performing SVD clutter filtering.

DETAILED DESCRIPTION

[0016] A detailed description may be provided with reference to the accompanying drawings. One of ordinary skill in the art may realize that the following description is illustrative only and is not in any way limiting. Other embodiments of the present invention may readily suggest themselves to such skilled persons having the benefit of this disclosure.

[0017] FIG. 1 is a block diagram showing an illustrative embodiment of an ultrasound system. Referring to FIG. 1, the ultrasound system 100 may include a user input unit 110. The user input unit 110 may be configured to receive input infor-

mation from a user. FIG. 2 is a schematic diagram showing an example of a brightness mode (B mode) image and a region of interest (ROI). In one embodiment, the input information may include information for setting the ROI 220 on the B mode image 210 of a target object, as shown in FIG. 2. The ROI 220 may include a color box for obtaining a color Doppler mode image. The user input unit 110 may include a control panel, a mouse, a keyboard and the like.

[0018] The ultrasound system 100 may further include an ultrasound data acquisition unit 120. The ultrasound data acquisition unit 120 may be configured to transmit and receive ultrasound signals to and from the target object to thereby output ultrasound data.

[0019] FIG. 3 is a block diagram showing an illustrative embodiment of the ultrasound data acquisition unit. Referring to FIG. 3, the ultrasound data acquisition unit 120 may include a transmit (Tx) signal generating section 310, an ultrasound probe 320, a beam former 330 and an ultrasound data forming section 340.

[0020] The Tx signal generating section 310 may be configured to generate Tx signals. In one embodiment, the Tx signal generating section 310 may generate first Tx signals for obtaining the B mode image 210, and a plurality of second Tx signals for obtaining a color Doppler mode image corresponding to the ROI 220 based on a predetermined ensemble number. The ensemble number may represent the number of transmitting and receiving ultrasound signals in order to obtain Doppler signals corresponding to each of the scan-lines.

[0021] The ultrasound probe 320 may include a plurality of elements (not shown) for reciprocally converting between ultrasound signals and electrical signals. The ultrasound probe 320 may be configured to transmit ultrasound data to the target object in response to the Tx signals provided from the Tx signal generating section 310. The ultrasound probe 320 may further receive ultrasound echo signals reflected from the target object to thereby form received signals. The received signals may be analog signals.

[0022] In one embodiment, the ultrasound probe 320 may transmit ultrasound signals to the target object in response to the first Tx signals provided from the Tx signal generating section 310. The ultrasound probe 320 may further receive ultrasound echo signals reflected from the target object to thereby form first received signals. The ultrasound probe 320 may further transmit ultrasound signals to the target object in response to each of the plurality of second Tx signals provided from the Tx signal generating section 310. The ultrasound probe 320 may further receive ultrasound echo signals reflected from the target object to thereby form a plurality of second received signals.

[0023] The beam former 330 may be configured to convert the received signals provided from the ultrasound probe 320 into digital signals. The beam former 330 may further apply delays to the digital signals in consideration of distance between the elements and focal points to thereby output digital receive-focused signals.

[0024] In one embodiment, the beam former 330 may convert the first received signals provided from the ultrasound probe 320 into first digital signals. The beam former 330 may further apply delays to the first digital signals in consideration of distance between the elements and focal points to thereby output first digital receive-focused signals. The beam former 330 may further convert the plurality of second received signals provided from the ultrasound probe 320 into a plural-

ity of second digital signals. The beam former 330 may further apply delays to the plurality of second digital signals in consideration of distance between the elements and focal points to thereby output a plurality of second digital receive-focused signals.

[0025] The ultrasound data forming section 340 may be configured to form ultrasound data based on the digital receive-focused signals provided from the beam former 330. The ultrasound data forming section 340 may further perform signal processing (e.g., gain control, etc) upon the digital receive-focused signals.

[0026] In one embodiment, the ultrasound data forming section 340 may form first ultrasound data based on the first digital receive-focused signals provided from the beam former 330. The first ultrasound data may be radio frequency (RF) data. However, it should be noted herein that the first ultrasound data may not be limited thereto. The ultrasound data forming section 340 may further form a plurality of second ultrasound data corresponding to the ensemble number based on the plurality of second digital receive-focused signals provided from the beam former 330. The second ultrasound data may be in-phase/quadrature (IQ) data. However, it should be noted herein that the second ultrasound data may not be limited thereto.

[0027] Referring back to FIG. 1, the ultrasound system 100 may further include a processing unit 130 in communication with the user input unit 110 and the ultrasound data acquisition unit 120. FIG. 4 is a block diagram showing an illustrative embodiment of the processing unit 130. Referring to FIG. 4, the processing unit 130 may include a matrix forming section 410, a singular value decomposition (SVD) processing section 420, a calculating section 430, a determining section 440, a first filtering section 450, a second filtering section 460 and an image forming section 470.

[0028] FIG. 5 is a flow chart showing a process of adaptively performing clutter filtering. The matrix forming section 410 may form matrixes corresponding to pixels of the color Doppler mode image based on the plurality of second ultrasound data, at step S502 in FIG. 5. As one example, when the plurality of second ultrasound data corresponding to a pixel of the color Doppler mode image are 2, 3, 5, 6, 7 and 8, the matrix forming section 410 may form a matrix HM having 3x2 size based on the plurality of second ultrasound data 2, 3, 5, 6, 7 and 8 as the following equation.

$$HM = \begin{bmatrix} 2 & 3 \\ 5 & 6 \\ 7 & 8 \end{bmatrix} \quad (1)$$

[0029] The matrix may include a Hankel matrix. However, it should be noted herein that the matrix may not be limited thereto.

[0030] The SVD processing section 420 may perform the SVD upon the matrixes formed by the matrix forming section 410 to thereby form a plurality of sub matrixes corresponding to each of the matrixes, at step S504 in FIG. 5. The methods of performing the SVD are well known in the art. Thus, they have not been described in detail so as not to unnecessarily obscure the present invention. As one example, the SVD processing unit 420 may perform the SVD upon the matrix HM to thereby form sub matrixes SM1 and SM2 corresponding to the matrix HM as the following equation.

$$SM1 = \begin{bmatrix} 2.3130 & 2.7353 \\ 5.0430 & 5.9637 \\ 6.8629 & 8.1159 \end{bmatrix}, \quad (2)$$

$$SM2 = \begin{bmatrix} -0.3130 & 0.2647 \\ -0.0430 & 0.0363 \\ 0.1371 & -0.1159 \end{bmatrix}$$

[0031] The calculating section 430 may calculate power for each of the plurality of sub matrixes formed by the SVD processing section 420, at step S506 in FIG. 5. As one example, the calculating section 430 may rearrange the sub matrix SM1 as the following equation.

$$SM1 = \left[SM1(1, 1), \frac{SM1(1, 2) + SM1(2, 1)}{2}, \frac{SM1(3, 1) + SM1(2, 2)}{2}, SM1(3, 2) \right] \quad (3)$$

$$= [2.3130, 3.8891, 6.4133, 8.1159]$$

[0032] The calculating section 430 may further perform an autocorrelation upon the rearranged sub matrix SM1 to thereby calculate the power corresponding to the rearranged sub matrix SM1. The calculating section 430 may further rearrange the sub matrix SM2 as the above equation. The calculating section 430 may further perform an autocorrelation upon the rearranged sub matrix SM2 to thereby calculate the power corresponding to the sub matrix SM2.

[0033] The calculating section 430 may further calculate a mean frequency for each of the plurality of sub matrixes formed by the SVD processing section 420, at step S506 in FIG. 5. As one example, the calculating section 430 may perform an autocorrelation upon the rearranged sub matrix SM1 to thereby calculate the mean frequency corresponding to the rearranged sub matrix SM1. The calculating section 430 may further perform an autocorrelation upon the rearranged sub matrix SM2 to thereby calculate the mean frequency corresponding to the sub matrix SM2.

[0034] The calculating section 430 may calculate a power difference value among the plurality of sub matrixes for each of the pixels, at step S508 in FIG. 5.

[0035] The determining section 440 may compare the power difference value with a predetermined first threshold value for each of the pixels, at step S510 in FIG. 5. If it is determined that the power difference value is equal to or larger than the first threshold value, then the first filtering section 450 may perform first clutter filtering upon the plurality of sub matrixes for each of the pixels, at step S512 in FIG. 5. In one embodiment, the first clutter filtering may include SVD clutter filtering.

[0036] FIG. 6 is a flow chart showing a process of performing the SVD clutter filtering. The first filtering section 450 may compare the mean frequency with a predetermined first cutoff frequency for each of the plurality of sub matrixes, at step S602 in FIG. 6.

[0037] If it is determined that the mean frequency is equal to or less than the first cutoff frequency, then the first filtering section 450 may perform the SVD clutter filtering ("first SVD clutter filtering") for removing the corresponding sub matrix as a clutter signal component, at step S604 in FIG. 6. As one

example, the first filtering section 450 may compare the mean frequency of the sub matrix SM1 with the first cutoff frequency. If it is determined that the mean frequency of the sub matrix SM1 is equal to or less than the first cutoff frequency, then the first filtering section 450 may perform the first SVD clutter filtering for removing the sub matrix SM1 as the clutter signal component.

[0038] Alternatively, if it is determined that the mean frequency is larger than the first cutoff frequency, then the first filtering section 450 may compare the mean frequency of the corresponding sub matrix with a predetermined second cutoff frequency, at step S606 in FIG. 6. The second cutoff frequency may be larger than the first cutoff frequency.

[0039] Then, if it is determined that the mean frequency is equal to or less than the second cutoff frequency, then the first filtering section 450 may perform the SVD clutter filtering ("second SVD clutter filtering") for performing a matrix operation upon the corresponding sub matrix as a Doppler signal component, at step S608 in FIG. 6. The matrix operation may include a matrix addition operation.

[0040] As one example, if it is determined that the mean frequency of the sub matrix SM1 is equal to or less than the first cutoff frequency, and the mean frequency of the sub matrix SM2 is larger than the first cutoff frequency and is equal to or less than the second cutoff frequency, then the first filtering section 450 may perform the first SVD clutter filtering upon the sub matrix SM1, which is removed as a clutter signal component, and perform the second SVD clutter filtering upon the sub matrix SM2 to thereby form the clutter-filtered second ultrasound data M as the following equation.

$$M = SM2 = \begin{bmatrix} -0.3130 & 0.2647 \\ -0.0430 & 0.0363 \\ 0.1371 & -0.1159 \end{bmatrix} \quad (4)$$

[0041] As another example, when the mean frequencies of the sub matrixes SM1 and SM2 are larger than the first cutoff frequency and are equal to or less than the second cutoff frequency, the first filtering section 450 may perform the second SVD clutter filtering upon the sub matrixes SM1 and SM2 to thereby form clutter-filtered second ultrasound data M as the following equation.

$$M = SM1 + SM2 = \begin{bmatrix} 2 & 3 \\ 5 & 6 \\ 7 & 8 \end{bmatrix} \quad (5)$$

[0042] Alternatively, if the mean frequency is larger than the second cutoff frequency, then the first filtering section 450 may compare the power of the corresponding sub matrix with a predetermined second threshold value, at step S610 in FIG. 6.

[0043] If the power is equal to larger than the second threshold value, then the first filtering section 450 may perform the second SVD clutter filtering upon the corresponding sub matrix as mentioned above. Alternatively, if it is determined that the power is less than the second threshold value, then the first filtering section 450 may perform the SVD clutter filtering ("third SVD clutter filtering") for removing the corresponding sub matrix as a noise component, at step S612 in FIG. 6.

[0044] Then, the first filtering section **450** may perform the SVD clutter filtering upon all sub matrixes for each of the pixels of the color Doppler mode image at step **S614** in FIG. **6**.

[0045] Referring back to FIG. **5**, if it is determined that the power difference value is less than the first threshold value, then the second filtering section **460** as shown in FIG. **4** may perform second clutter filtering upon the plurality of second ultrasound data, at step **S514** in FIG. **5**. The second clutter filtering may include infinite impulse response, regression filtering, eigenvector based filtering and the like. However, it should be noted herein that the second clutter filtering may not be limited thereto.

[0046] The image forming section **470** may form the color Doppler mode image based on the clutter-filtered second ultrasound data, at step **S516** in FIG. **5**. The image forming section **470** may further form the B mode image based on the first ultrasound data provided from the ultrasound data acquisition unit **120**, as shown in FIG. **1**.

[0047] Referring back to FIG. **1**, the ultrasound system **100** may further include the display unit **140**. The display unit **140** may display the color Doppler mode image. The display unit **140** may further display the B mode image.

[0048] In another embodiment, the present invention may provide a computer readable medium comprising computer executable instructions configured to perform the following acts: a) acquiring a plurality of ultrasound data corresponding to each of pixels of a color Doppler mode image for a target object; b) calculating a power difference value corresponding to each of the pixels based on the plurality of ultrasound data; c) determining whether the power difference value is equal to or larger than a first threshold value; and d) if the power difference value is equal to or larger than the first threshold value, then performing first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then performing second clutter filtering upon the plurality of ultrasound data. The computer readable medium may comprise a floppy disk, a hard disk, a memory, a compact disk, a digital video disk, etc.

[0049] Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the spirit and scope of the principles of this disclosure. More particularly, numerous variations and modifications are possible in the component parts and/or arrangements of the subject combination arrangement within the scope of the disclosure, the drawings and the appended claims. In addition to variations and modifications in the component parts and/or arrangements, alternative uses will also be apparent to those skilled in the art.

What is claimed is:

1. An ultrasound system, comprising:

an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object to output a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image; and

a processing unit in communication with the ultrasound data acquisition unit and being configured to calculate a power difference value corresponding to each of the pixels based on the plurality of ultrasound data, determine whether the power difference value is equal to or larger than a first threshold value, and if the power difference value is equal to or larger than the first threshold

value, then perform first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then perform second clutter filtering upon the plurality of ultrasound data.

2. The ultrasound system of claim **1**, wherein the first clutter filtering comprises singular value decomposition (SVD) clutter filtering, and

wherein the second clutter filtering comprises any one of infinite impulse response, regression filtering and eigenvector based filtering.

3. The ultrasound system of claim **2**, wherein the processing unit comprises:

a matrix forming section configured to form a matrix corresponding to each of the pixels based on the plurality of ultrasound data;

a SVD processing section configured to perform the SVD upon the matrix to form a plurality of sub matrixes corresponding to each of the matrixes;

a calculating section configured to calculate a mean frequency and a power corresponding to each of the plurality of sub matrixes, and calculate the power difference value among the plurality of sub matrixes based on the power;

a determining section configured to determine whether the power difference value is equal to or larger than the first threshold value; and

a first filtering section configured to, if the power difference value is equal to or larger than the first threshold value, perform the first clutter filtering upon the plurality of sub matrixes by using the mean frequency and the power.

4. The ultrasound system of claim **3**, wherein the first filtering section is configured to:

compare the mean frequency with a predetermined first cutoff frequency;

if it is determined that the mean frequency is equal to or less than the first cutoff frequency, perform first SVD clutter filtering for removing the sub matrix corresponding to the mean frequency as a clutter signal component;

if it is determined that the mean frequency is larger than the first cutoff frequency, compare the mean frequency with a predetermined second cutoff frequency, wherein the second cutoff frequency is larger than the first cutoff frequency; and

if it is determined that the mean frequency is equal to or less than the second cutoff frequency, perform second SVD clutter filtering for performing a matrix operation upon the sub matrix corresponding to the mean frequency as a Doppler signal component.

5. The ultrasound system of claim **4**, wherein the matrix operation comprises a matrix addition operation.

6. The ultrasound system of claim **4**, wherein the first filtering section is further configured to:

if it is determined that the mean frequency is larger than the second cutoff frequency, compare the power of the sub matrix corresponding to the mean frequency with a predetermined second threshold value;

if it is determined that the power is less than the second threshold value, perform third SVD clutter filtering for removing the sub matrix as a noise component; and

if it is determined that the power is equal to or larger than the second threshold value, perform the second SVD clutter filtering upon the sub matrix corresponding to the power.

7. A method of performing clutter filtering, comprising:
- a) acquiring a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image for a target object;
 - b) calculating a power difference value corresponding to each of the pixels based on the plurality of ultrasound data;
 - c) determining whether the power difference value is equal to or larger than a first threshold value; and
 - d) if the power difference value is equal to or larger than the first threshold value, then performing first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then performing second clutter filtering upon the plurality of ultrasound data.
8. The method of claim 7, wherein the first clutter filtering comprises singular value decomposition (SVD) clutter filtering, and wherein the second clutter filtering comprises one of infinite impulse response, regression filtering and eigenvector based filtering.
9. The method of claim 8, wherein the step b) comprises: forming a matrix corresponding to each of the pixels based on the plurality of ultrasound data; performing the SVD upon the matrix to thereby form a plurality of sub matrixes corresponding to each of the matrixes; calculating a power and a mean frequency corresponding to each of the plurality of sub matrixes; and calculating the power difference value among the plurality of sub matrixes based on the power.
10. The method of claim 9, wherein the step d) comprises:
- d1) comparing the mean frequency with a predetermined first cutoff frequency;
 - d2) if it is determined that the mean frequency is equal to or less than the first cutoff frequency, performing first SVD clutter filtering for removing the sub matrix corresponding to the mean frequency as a clutter signal component;
 - d3) if it is determined that the mean frequency is larger than the first cutoff frequency, comparing the mean frequency with a predetermined second cutoff frequency, wherein the second cutoff frequency is larger than the first cutoff frequency; and
 - d4) if it is determined that the mean frequency is equal to or less than the second cutoff frequency, performing second SVD clutter filtering for performing a matrix operation upon the sub matrix corresponding to the mean frequency as a Doppler signal component.
11. The method of claim 10, wherein the matrix operation comprises a matrix addition operation.
12. The method of claim 10, wherein the step d) further comprises:
- d5) if it is determined that the mean frequency is larger than the second cutoff frequency, comparing the power of the sub matrix corresponding to the mean frequency with a predetermined second threshold value;
 - d6) if it is determined that the power is less than the second threshold value, performing third SVD clutter filtering for removing the sub matrix as a noise component; and
 - d7) if it is determined that the power is equal to or larger than the second threshold value, performing the second SVD clutter filtering upon the sub matrix corresponding to the power.
13. A computer readable medium comprising computer executable instructions configured to perform following acts:
- a) acquiring a plurality of ultrasound data corresponding to each pixel of a color Doppler mode image for a target object;
 - b) calculating a power difference value corresponding to each of the pixels based on the plurality of ultrasound data;
 - c) determining whether the power difference value is equal to or larger than a first threshold value; and
 - d) if the power difference value is equal to or larger than the first threshold value, then performing first clutter filtering upon the plurality of ultrasound data, or if the power difference value is less than the first threshold value, then performing second clutter filtering upon the plurality of ultrasound data.

* * * * *

专利名称(译)	在超声系统中自适应地执行杂波滤波		
公开(公告)号	US20110118606A1	公开(公告)日	2011-05-19
申请号	US12/878903	申请日	2010-09-09
[标]申请(专利权)人(译)	金泰YUN		
申请(专利权)人(译)	金泰YUN		
当前申请(专利权)人(译)	MEDISON CO. , LTD.		
[标]发明人	KIM TAE YUN		
发明人	KIM, TAE YUN		
IPC分类号	A61B8/00 G06K9/40		
CPC分类号	G01S15/8981		
优先权	1020090110223 2009-11-16 KR		
其他公开文献	US8684934		
外部链接	Espacenet USPTO		

摘要(译)

公开了自适应地执行杂波滤波的实施例。在一个实施例中，作为非限制性示例，超声系统包括：超声数据获取单元，被配置为向目标对象发送超声信号和从目标对象接收超声信号，以输出对应于彩色多普勒的每个像素的多个超声数据。模式图像;处理单元，与超声数据获取单元通信，用于根据多个超声数据计算每个像素对应的功率差值，确定功率差值是否等于或大于第一阈值如果功率差值等于或大于第一阈值，则对多个超声数据执行第一杂波滤波，或者如果功率差值小于第一阈值，则执行第二杂波滤波在多个超声数据上。

