



US007815570B2

(12) **United States Patent**
Eshel et al.

(10) **Patent No.:** **US 7,815,570 B2**
(45) **Date of Patent:** ***Oct. 19, 2010**

(54) **NON-INVASIVE ULTRASONIC BODY
CONTOURING**

(75) Inventors: **Yoram Eshel**, Tel Aviv (IL); **Ilia
Vitsnudel**, Even Yehuda (IL)

(73) Assignee: **Ultrashape Ltd.**, Yoqneam Illite (IL)

(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 186 days.

This patent is subject to a terminal dis-
claimer.

(21) Appl. No.: **11/808,632**

(22) Filed: **Jun. 12, 2007**

(65) **Prior Publication Data**

US 2008/0281201 A1 Nov. 13, 2008

Related U.S. Application Data

(63) Continuation of application No. 10/250,955, filed as
application No. PCT/IL01/01220 on Dec. 31, 2001,
now abandoned, and a continuation-in-part of applica-
tion No. 10/021,238, filed on Oct. 29, 2001, now Pat.
No. 7,347,855, which is a continuation-in-part of
application No. 09/752,530, filed on Jan. 3, 2001, now
Pat. No. 6,607,498.

(51) **Int. Cl.**
A61B 8/00 (2006.01)

(52) **U.S. Cl.** **600/437; 600/439; 600/443;
600/447; 600/2; 600/10; 601/2; 601/3; 604/22;
606/2.5**

(58) **Field of Classification Search** 600/437,
600/439, 443, 447, 2, 10, 407; 601/2, 3;
604/22; 606/2.5

See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

3,735,755 A 5/1973 Eggleton et al.
4,605,009 A 8/1986 Procelot et al.

(Continued)

FOREIGN PATENT DOCUMENTS

EP 1060728 12/2000

(Continued)

OTHER PUBLICATIONS

Rohrich, et al., "Comparative Lipoplasty Analysis of in Vivo-Treated
Adipose Tissue", Plastic and Reconstruction Journal, 105:2152-
2158, 2000.

(Continued)

Primary Examiner—Brian Casler

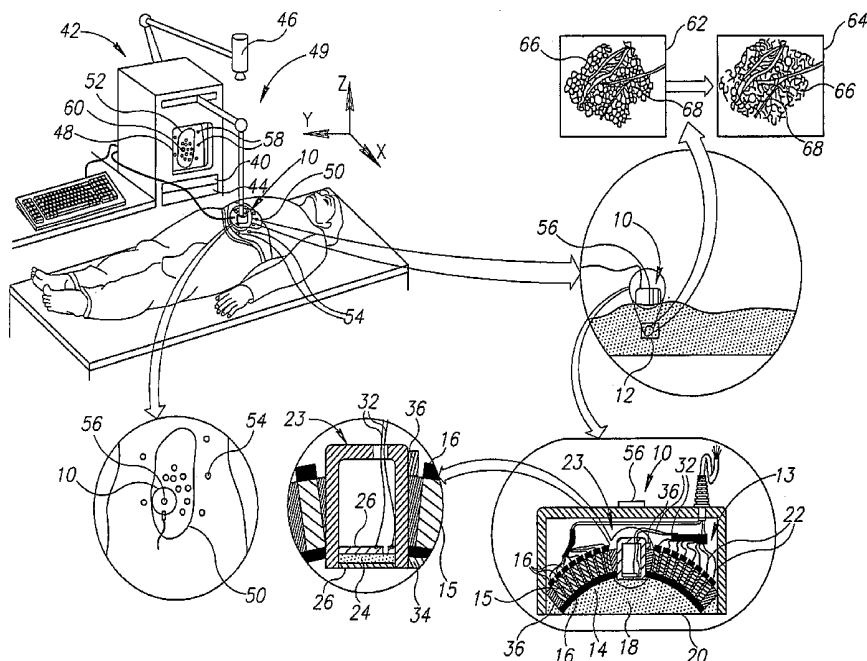
Assistant Examiner—Joel M Lamprecht

(74) *Attorney, Agent, or Firm*—Fennemore Craig, P.C.

(57) **ABSTRACT**

A methodology and system for lysing adipose tissue includ-
ing directing ultrasonic energy at a multiplicity of target vol-
umes within the region, which target volumes contain adipose
tissue, thereby to selectively lyse the adipose tissue in the
target volumes and generally not lyse non-adipose tissue in
the target volumes and computerized tracking of the multi-
plicity of target volumes notwithstanding movement of the
body.

50 Claims, 8 Drawing Sheets



U.S. PATENT DOCUMENTS

4,886,491 A 12/1989 Parisi et al.
 4,938,216 A 7/1990 Lele
 4,951,653 A 8/1990 Fry et al.
 4,986,275 A 1/1991 Ishida et al.
 5,005,579 A 4/1991 Wurster et al.
 5,079,952 A 1/1992 Nakaso et al.
 5,080,102 A 1/1992 Dory
 5,111,822 A 5/1992 Dory
 5,143,063 A 9/1992 Fellner
 5,143,073 A 9/1992 Dory
 5,209,221 A 5/1993 Riedlinger
 5,211,164 A 5/1993 Allen
 5,301,660 A 4/1994 Rattner
 5,419,761 A 5/1995 Narayanan et al.
 5,431,621 A 7/1995 Dory
 5,507,790 A 4/1996 Weiss
 5,526,815 A 6/1996 Granz et al.
 5,618,275 A 4/1997 Bock
 5,640,371 A 6/1997 Schmidt et al.
 5,643,179 A 7/1997 Fujimoto
 5,694,936 A 12/1997 Fujimoto et al.
 5,884,631 A 3/1999 Silberg
 5,944,663 A 8/1999 Kuth et al.
 5,948,011 A 9/1999 Knowlton
 6,038,467 A 3/2000 DeBliek et al.
 6,039,048 A 3/2000 Silberg
 6,071,239 A 6/2000 Cribbs et al.
 6,086,535 A 7/2000 Ishibashi et al.
 6,113,558 A 9/2000 Rosenschein et al.
 6,206,873 B1 3/2001 Paolini et al.
 6,384,516 B1 5/2002 Fraser

6,595,934 B1 7/2003 Hissong et al.
 6,607,498 B2 8/2003 Eshel
 6,645,162 B2 11/2003 Friedman et al.
 6,684,097 B1 1/2004 Parel et al.
 7,331,951 B2 2/2008 Eshel et al.
 2003/0083536 A1 5/2003 Eshel et al.
 2006/0241440 A1 10/2006 Eshel et al.

FOREIGN PATENT DOCUMENTS

GB 2303552 2/1997
 JP 11155894 12/1997
 WO WO9503740 2/1995
 WO WO9853787 12/1998
 WO WO0053263 9/2000

OTHER PUBLICATIONS

Ter Haar, et al, "Evidence for Acoustic Cavitation in Vivo" Thresholds for Bubble Formation with 0.75-MHz Continuous Wave and Pulsed Beams, IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control, vol. Uffc-33, No. 2, pp. 162-164, Mar. 1986.
 Vykholdtseva, et al, "Histologic Effects of High Intensity Pulsed Ultrasound Exposure with Subharmonic Emission in Rabbit Brain in Vivo", Ultrasound in Medicine & Biology, vol. 21, No. 7, pp. 969-979, 1995.
 Muir, et al, "Prediction of nonlinear acoustic effects at biomedical frequencies and intensities", Ultrasound in Medicine & Biology, vol. 6, pp. 345-357, 1980.
 Tavakkoli, et al, "A Piezocomposite shock wave generator with electronic focusing capability: application for producing cavitation-induced lesions in rabbit liver", Ultrasound in Medicine & Biology, vol. 23, No. 1, pp. 107-115, 1997.

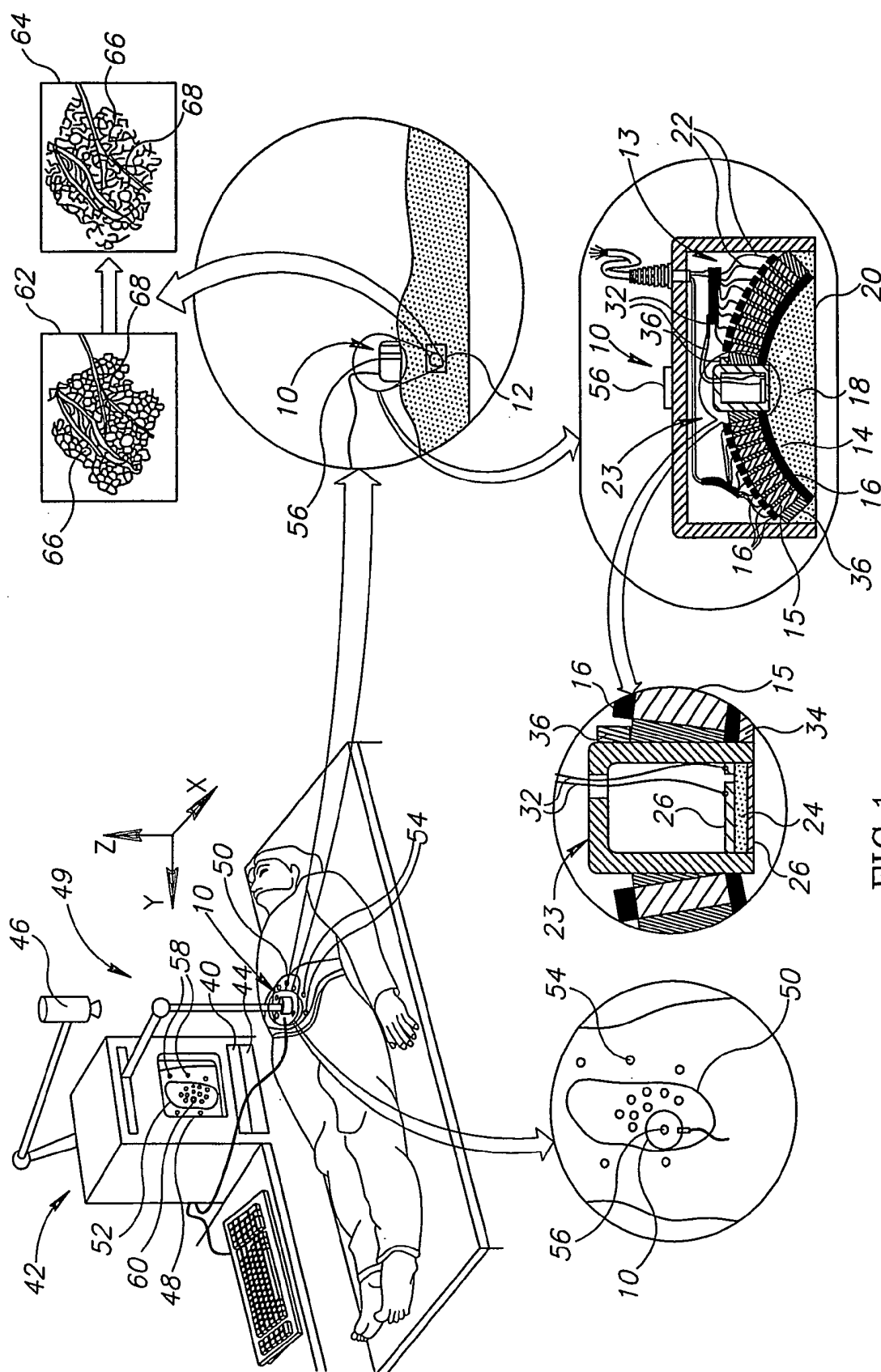


FIG. 1

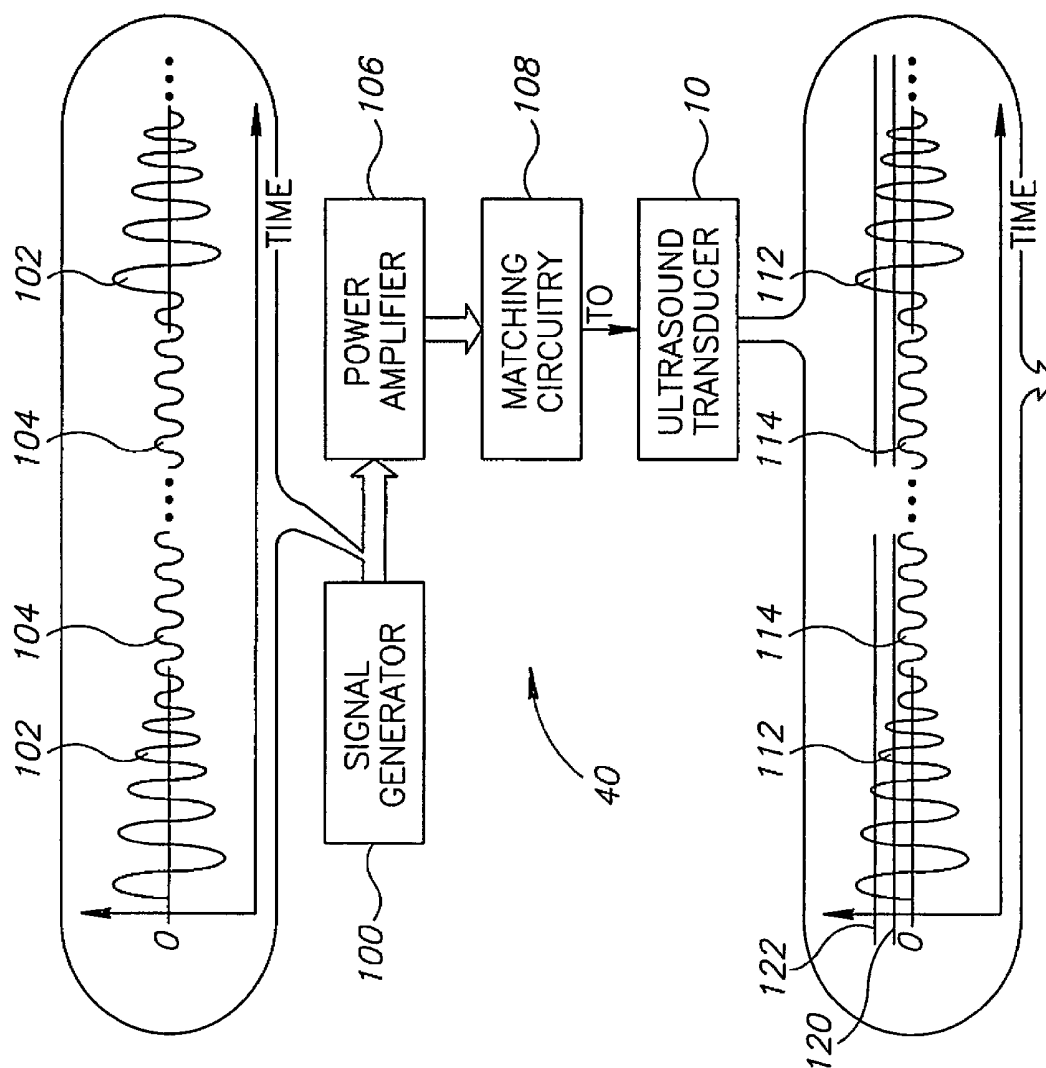


FIG.2

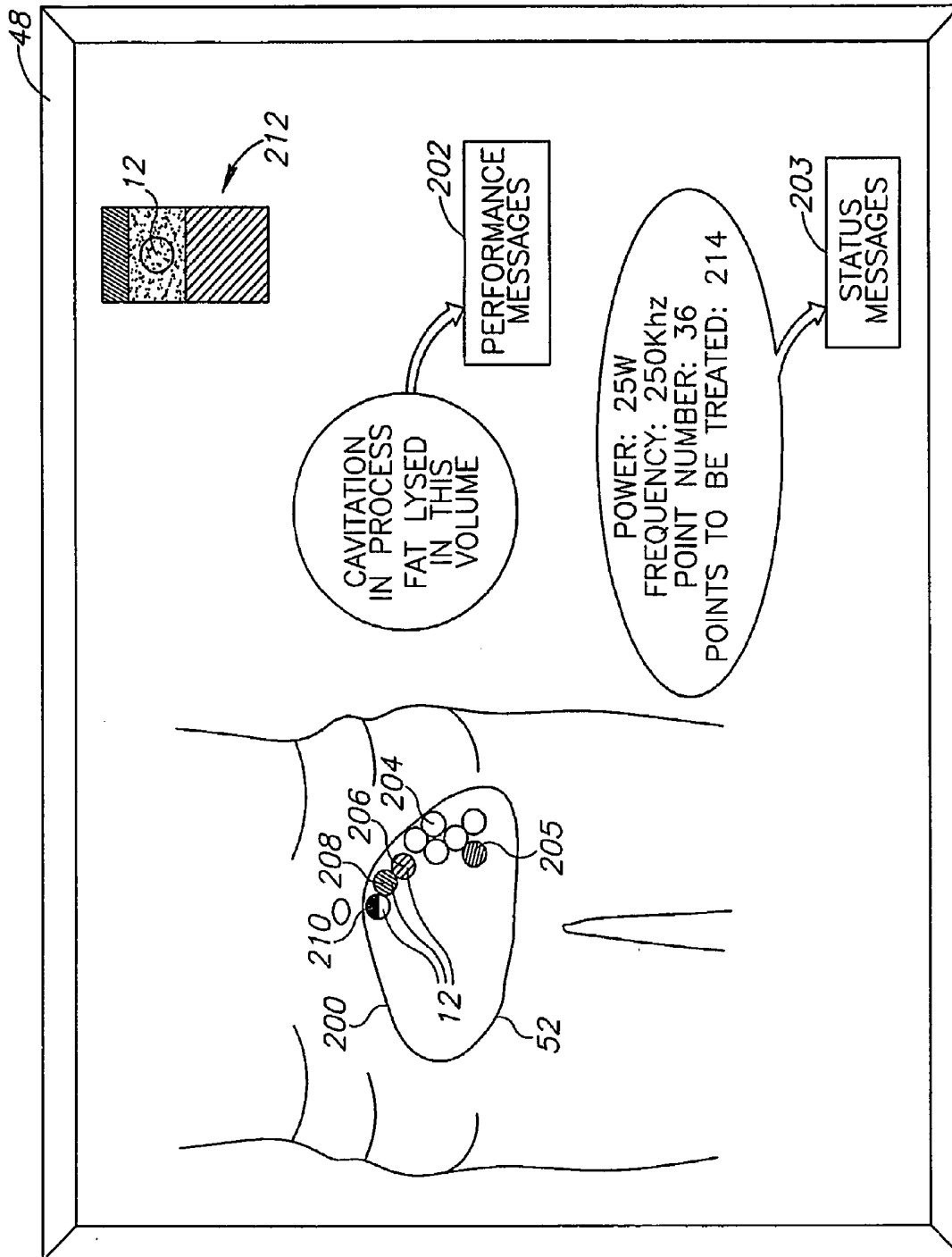


FIG. 3A

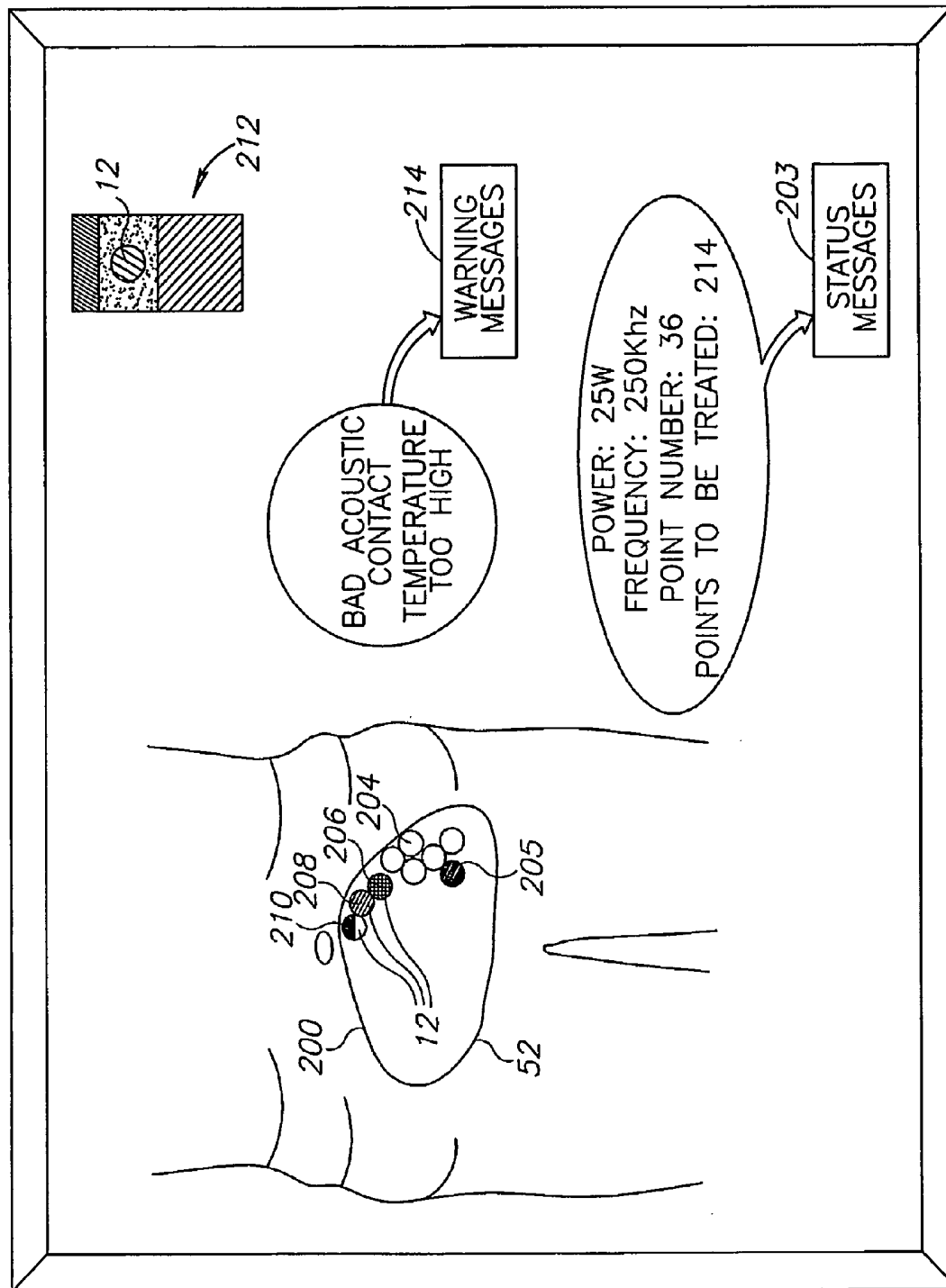


FIG. 3B

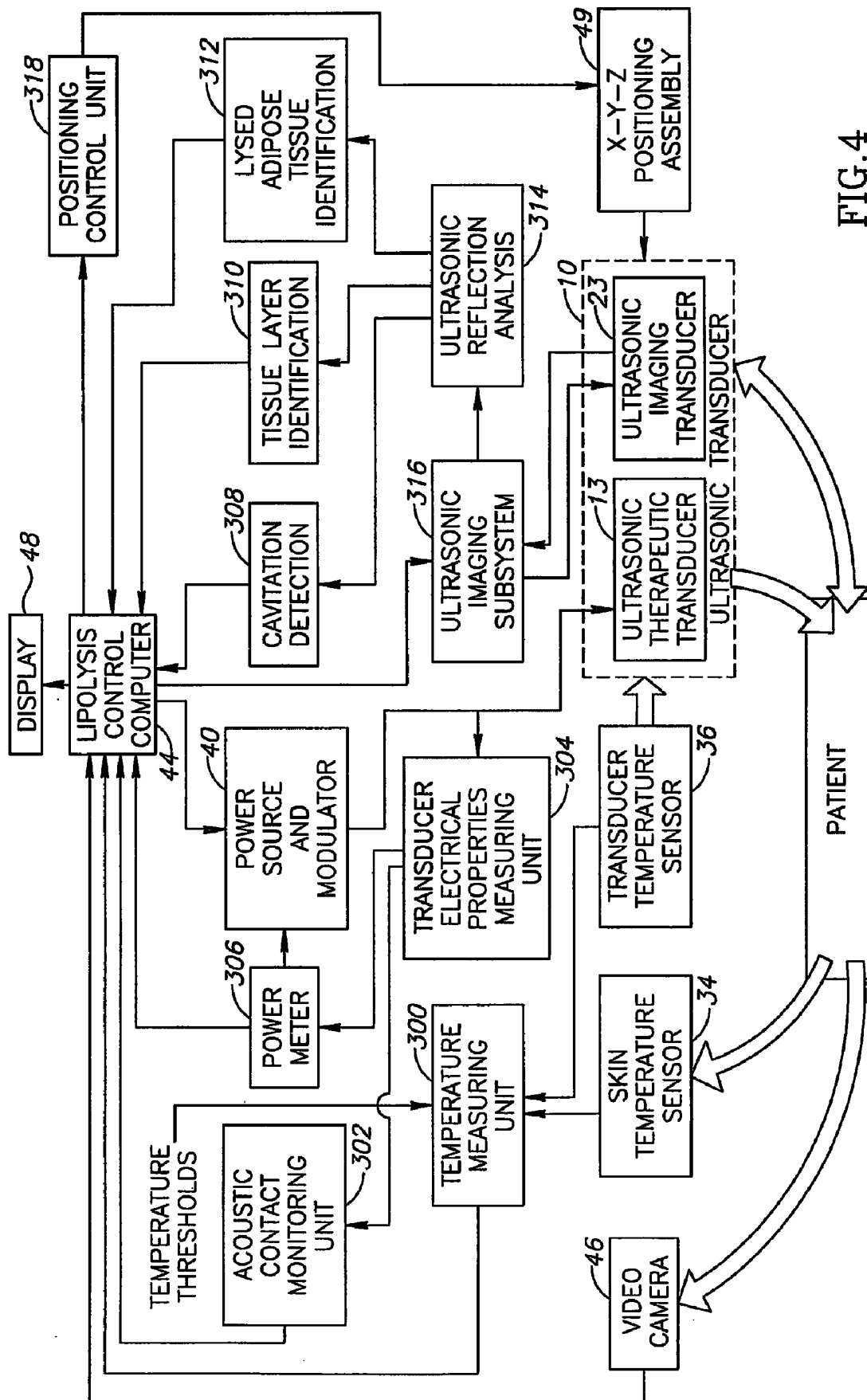


FIG. 4

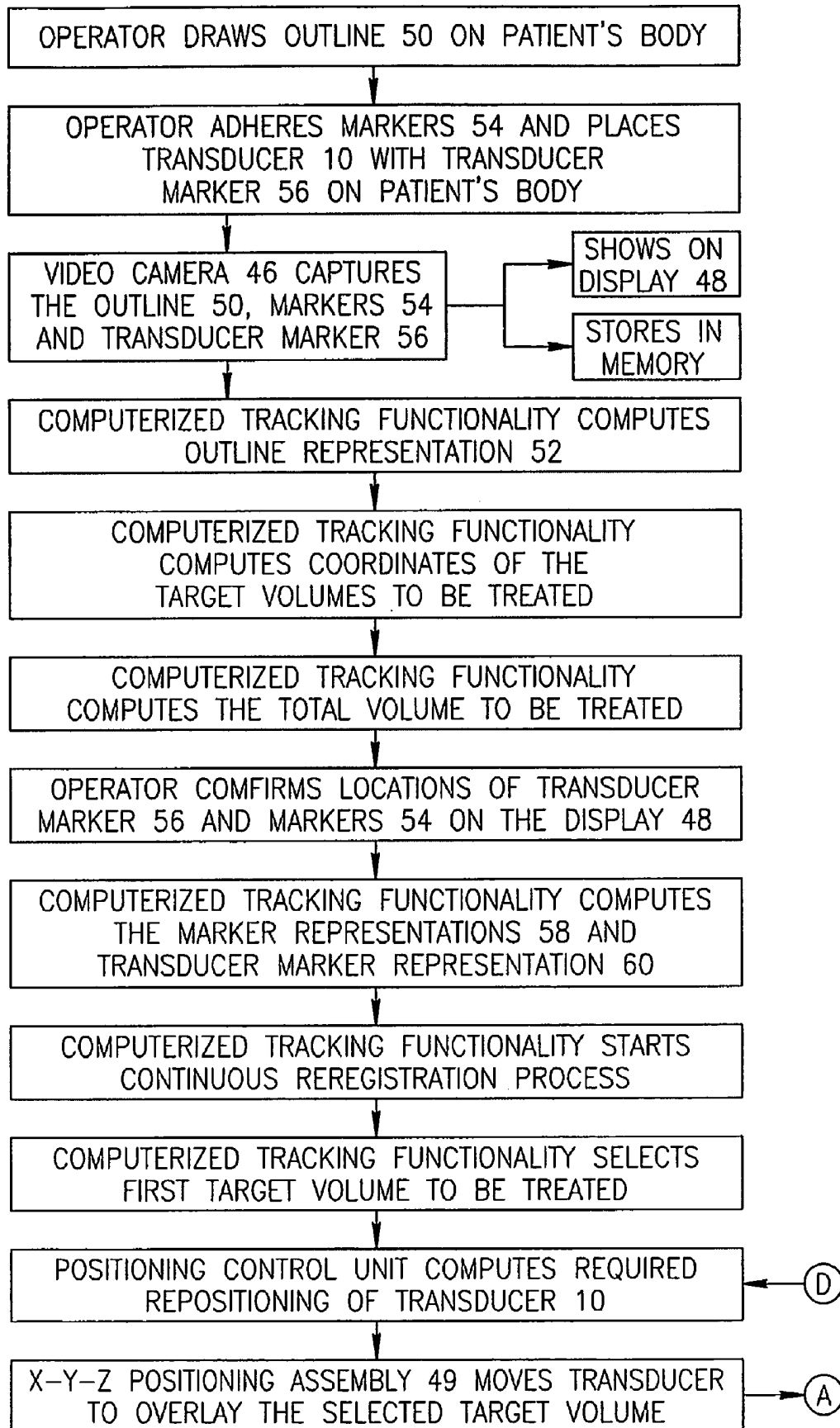


FIG.5A

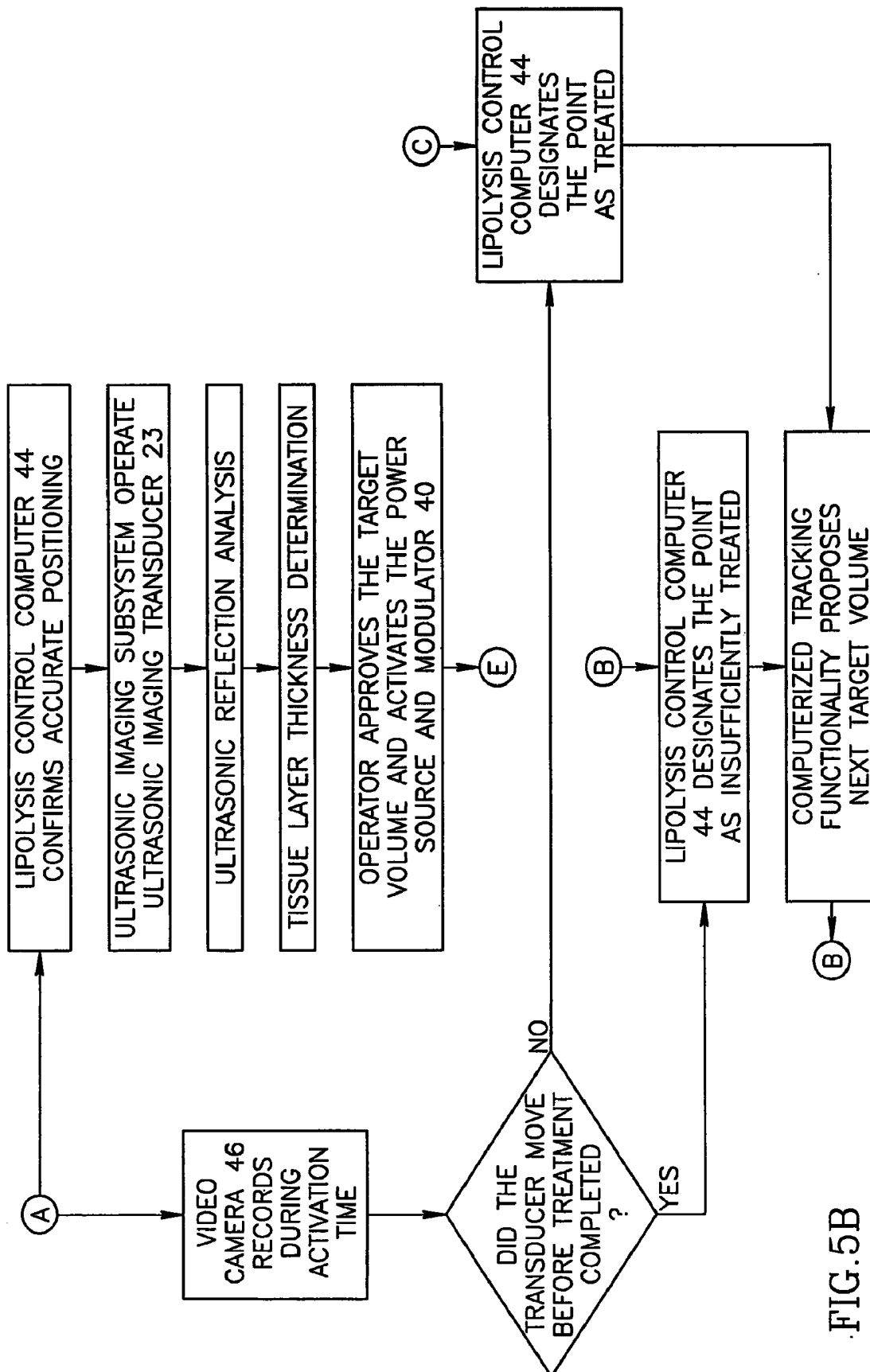
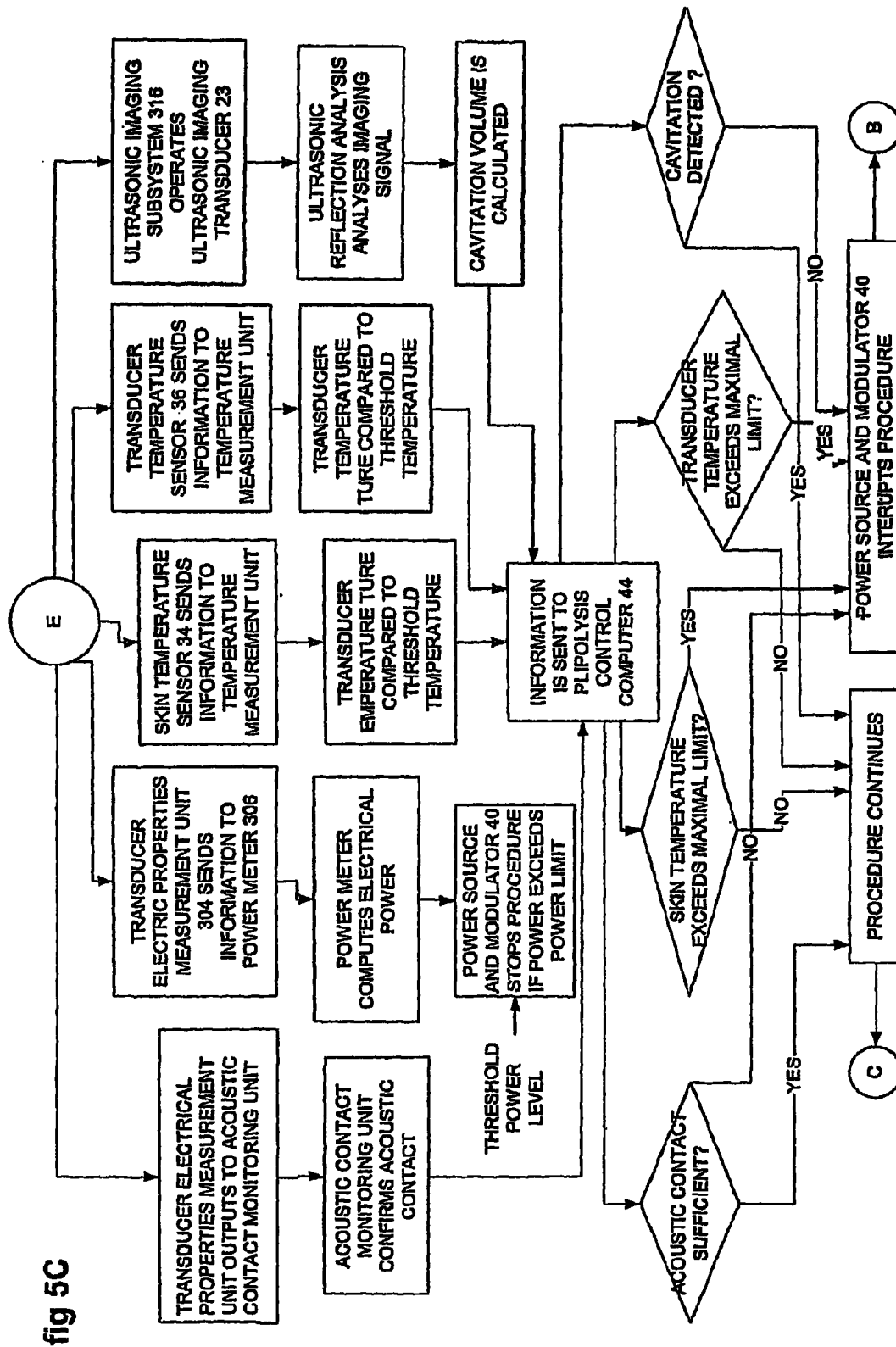


FIG. 5B



1

NON-INVASIVE ULTRASONIC BODY CONTOURING

CROSS-REFERENCE TO RELATED APPLICATIONS

The present application is a continuation and claims benefit of U.S. application Ser. No. 10/250,955 filed Dec. 12, 2003, now abandoned, which was filed in the U.S. Patent and Trade-mark Office on Dec. 31, 2001 as a continuation-in-part of U.S. patent application Ser. No. 09/752,530 filed Jan. 3, 2001 which is the national phase of PCT application PCT/IL01/01220 filed Dec. 31, 2001 and a continuation in part of U.S. patent application Ser. No. 10/021,238 filed Oct. 29, 2001. The disclosures of all these applications, including all appendices thereof, are incorporated herein by reference.

FIELD OF THE INVENTION

The present invention relates to lipolysis generally and more particularly to ultrasonic lipolysis.

BACKGROUND OF THE INVENTION

The following U.S. Patents are believed to represent the current state of the art:

U.S. Pat. Nos. 4,986,275; 5,143,063; 5,143,073; 5,209,221; 5,301,660; 5,431,621; 5,507,790; 5,526,815; 5,884,631; 6,039,048; 6,071,239; 6,113,558; 6,206,873

SUMMARY OF THE INVENTION

The present invention seeks to provide improved apparatus and methodology for ultrasonic lipolysis.

There is thus provided in accordance with a preferred embodiment of the present invention a method for lysing adipose tissue including the steps of:

directing focused ultrasonic energy at a target volume in a region of a body containing adipose tissue; and

modulating the focused ultrasonic energy so as to selectively lyse the adipose tissue in the target volume and generally not lyse non-adipose tissue in the target volume.

Additionally in accordance with a preferred embodiment of the present invention, there is provided a method for lysing adipose tissue including the steps of:

generating, at a source outside a body, ultrasonic energy which selectively generally lyses adipose tissue and generally does not lyse non-adipose tissue; and

directing the ultrasonic energy, from the source outside the body, at a target volume of a body containing adipose tissue.

Further in accordance with a preferred embodiment of the present invention there is provided a method for lysing adipose tissue including the steps of:

defining a region in a body at least partially by detecting spatial indications on the body; and

directing ultrasonic energy at a multiplicity of target volumes within the region, which target volumes contain adipose tissue, thereby to selectively lyse the adipose tissue in the target volumes and generally not lyse non-adipose tissue in the target volumes.

Additionally in accordance with a preferred embodiment of the present invention, there is provided a method for lysing adipose tissue including the steps of:

directing ultrasonic energy at a multiplicity of target volumes within the region, which target volumes contain adipose

2

tissue, thereby to selectively lyse the adipose tissue in the target volumes and generally not lyse non-adipose tissue in the target volumes; and

computerized tracking of the multiplicity of target volumes notwithstanding movement of the body

There is additionally provided in accordance with a preferred embodiment of the present invention apparatus for lysing adipose tissue including:

a focused ultrasonic energy director, directing focused ultrasonic energy at a target volume in a region of a body containing adipose tissue; and

a modulator, cooperating with the energy director to produce a focused ultrasonic energy so as to selectively lyse the adipose tissue in the target volume and generally not lyse non-adipose tissue in the target volume.

There is further provided in accordance with a preferred embodiment of the present invention apparatus for lysing adipose tissue including:

a source outside a body generating ultrasonic energy;

an ultrasonic energy director, which employs the ultrasonic energy to selectively generally lyse adipose tissue and generally not lyse non-adipose tissue in a target volume of a body containing adipose tissue.

There is additionally provided in accordance with a preferred embodiment of the present invention apparatus for lysing adipose tissue including the steps of:

a region definer, defining a region in a body at least partially by detecting spatial indications on the body; and

a director, directing ultrasonic energy at a multiplicity of target volumes within the region, which target volumes contain adipose tissue thereby to selectively lyse the adipose tissue in the target volumes and generally not lyse non-adipose tissue in the target volumes.

There is still further provided in accordance with a preferred embodiment of the present invention apparatus for lysing adipose tissue including:

a director, directing ultrasonic energy at a multiplicity of target volumes within the region, which target volumes contain adipose tissue, thereby to selectively lyse the adipose tissue in the target volumes and generally not lyse non-adipose tissue in the target volumes; and

computerized tracking functionality providing computerized tracking of the multiplicity of target volumes notwithstanding movement of the body.

Preferably, directing focused ultrasonic energy generally prevents lysis of tissue outside of the target volume.

In accordance with a preferred embodiment of the present invention, the method also includes ultrasonic imaging of the region at least partially concurrently with directing the focused ultrasonic energy at the target volume.

Preferably, directing includes positioning at least one ultrasonic transducer relative to the body in order to direct the focused ultrasonic energy at the target volume.

The directing may also include varying the focus of at least one ultrasonic transducer in order to direct the focused ultrasonic energy at the target volume. Varying the focus may change the volume of the target volume, and/or the distance of the target volume from the at least one ultrasonic transducer.

The directing may also include positioning at least one ultrasonic transducer relative to the body in order to direct the focused ultrasonic energy at the target volume.

The method preferably also includes sensing ultrasonic energy coupling to an external surface of the body adjacent the target volume.

The method preferably additionally includes sensing of cavitation at the target volume.

Preferably, directing takes place from an ultrasonic transducer located outside of the body.

In accordance with a preferred embodiment of the present invention, the ultrasonic energy has a frequency in a range of 50 KHz-1000 KHz, more preferably in a range of 100 KHz-500 KHz, and most preferably in a range of 150 KHz-300 KHz.

Preferably, the modulating provides a duty cycle between 1:2 and 1:250, more preferably between 1:5 and 1:30 and most preferably between 1:10 and 1:20.

In accordance with a preferred embodiment of the present invention, the modulating provides between 2 and 1000 sequential cycles at an amplitude above a cavitation threshold, more preferably between 25 and 500 sequential cycles at an amplitude above a cavitation threshold and most preferably between 100 and 300 sequential cycles at an amplitude above a cavitation threshold.

Preferably, the modulating includes modulating the amplitude of the ultrasonic energy over time.

Preferably, directing includes directing focused ultrasonic energy at a multiplicity of target volumes in a time sequence.

In accordance with a preferred embodiment of the present invention, directing includes directing focused ultrasonic energy at plural ones of the multiplicity of target volumes at times which at least partially overlap.

Preferably, at least some of the multiplicity of target volumes at least partially overlap in space.

In accordance with a preferred embodiment of the present invention, the method includes defining the region by marking at least one surface of the body. The method may also include defining the region by selecting at least one depth in the body and/or by detecting adipose tissue in the body and/or by detecting non-lysed adipose tissue.

Preferably, directing also includes defining the target volumes as unit volumes of non-lysed adipose tissue within the region.

In accordance with a preferred embodiment of the present invention, modulating the ultrasonic energy so as to selectively lyse the adipose tissue in the multiplicity of target volumes proceeds sequentially in time wherein selective lysis of adipose tissue in each target volume takes place only following detection of non-lysed adipose tissue therein.

Preferably, the method also includes computerized tracking of the multiplicity of target volumes notwithstanding movement of the body.

Preferably, the computerized tracking includes sensing changes in the position of markings on the body and employing sensed changes for tracking the positions of the target volumes in the body.

Preferably, the modulation provides a decreasing amplitude over time which exceeds a cavitation threshold.

BRIEF DESCRIPTION OF THE DRAWINGS AND APPENDIX

The present invention will be understood and appreciated more fully from the following detailed description, taken in conjunction with the drawings and appendix in which:

FIG. 1 is a simplified pictorial illustration of the general structure and operation of ultrasonic lipolysis apparatus constructed and operative in accordance with a preferred embodiment of the present invention;

FIG. 2 is a simplified block diagram illustration of a preferred power source and modulator showing a pattern of variation of ultrasonic pressure over time in accordance with a preferred embodiment of the present invention;

FIGS. 3A and 3B are simplified pictorial illustrations of the appearance of an operator interface display during normal operation and faulty operation respectively;

FIG. 4 is a simplified block diagram illustration of an ultrasonic lipolysis system constructed and operative in accordance with a preferred embodiment of the present invention; and

FIGS. 5A, 5B and 5C are together a simplified flowchart illustrating operator steps in carrying out lipolysis in accordance with a preferred embodiment of the present invention.

BRIEF DESCRIPTION OF THE APPENDIX

The Appendix includes computer listings which, taken together, form a computational tracking functionality in accordance with a preferred software embodiment of the present invention.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

Reference is now made to FIG. 1, which is a simplified pictorial illustration of the general structure and operation of ultrasonic lipolysis apparatus constructed and operative in accordance with a preferred embodiment of the present invention. As seen in FIG. 1, an ultrasonic energy generator and director, such as an ultrasonic transducer 10, disposed outside a body, generates ultrasonic energy which, by suitable placement of the transducer 10 relative to the body, is directed to a target volume 12 inside the body and is operative to selectively generally lyse adipose tissue and generally not lyse non-adipose tissue in the target volume.

A preferred embodiment of ultrasonic energy generator and director useful in the present invention comprises an ultrasonic therapeutic transducer 13 including a curved phased array 14 of piezoelectric elements 15, typically defining a portion of a sphere or of a cylinder, and having conductive coatings 16 on opposite surfaces thereof. The piezoelectric elements 15 may be of any suitable configuration, shape and distribution. An intermediate element 18, formed of a material, such as polyurethane, which has acoustic impedance similar to that of soft mammalian tissue, generally fills the curvature defined by phased array 14 and defines a contact surface 20 for engagement with the body, typically via a suitable coupling gel (not shown). Contact surface 20 may be planar, but need not be.

Suitably modulated AC electrical power is supplied by conductors 22 to conductive coatings 16 to cause the piezoelectric elements 15 to provide a desired focused acoustic energy output.

In accordance with a preferred embodiment of the present invention an imaging ultrasonic transducer subassembly 23 is incorporated within transducer 10 and typically comprises a piezoelectric element 24 having conductive surfaces 26 associated with opposite surfaces thereof. Suitably modulated AC electrical power is supplied by conductors 32 to conductive surfaces 26 in order to cause the piezoelectric element 24 to provide an acoustic energy output. Conductors 32, coupled to surfaces 26, also provide an imaging output from imaging ultrasonic transducer subassembly 23.

It is appreciated that any suitable commercially available ultrasonic transducer may be employed or alternatively, imaging ultrasonic transducer subassembly 23 may be eliminated.

It is further appreciated that various types of ultrasonic transducers 10 may be employed. For example, such transducers may include multiple piezoelectric elements, multi-

layered piezoelectric elements and piezoelectric elements of various shapes and sizes arranged in a phase array.

In a preferred embodiment of the present invention shown in FIG. 1, the ultrasonic energy generator and director are combined in transducer 10. Alternatively, the functions of generating ultrasonic energy and focusing such energy may be provided by distinct devices.

In accordance with a preferred embodiment of the present invention, a skin temperature sensor 34, such as an infrared sensor, may be mounted alongside imaging ultrasonic transducer subassembly 23. Further in accordance with a preferred embodiment of the present invention a transducer temperature sensor 36, such as a thermocouple, may also be mounted alongside imaging ultrasonic transducer subassembly 23.

Ultrasonic transducer 10 preferably receives suitably modulated electrical power from a power source and modulator assembly 40, forming part of a control subsystem 42. Control subsystem 42 also typically includes a lipolysis control computer 44, having associated therewith a camera 46, such as a video camera, and a display 48. A preferred embodiment of power source and modulator assembly 40 is illustrated in FIG. 2 and described hereinbelow. Ultrasonic transducer 10 is preferably positioned automatically or semi-automatically as by an X-Y-Z positioning assembly 49. Alternatively, ultrasonic transducer 10 may be positioned at desired positions by an operator.

In accordance with a preferred embodiment of the present invention, camera 46 is operative for imaging a portion of the body on which lipolysis is to be performed. A picture of the portion of the patient's body viewed by the camera is preferably displayed in real time on display 48.

An operator may designate the outline of a region containing adipose tissue. In accordance with one embodiment of the present invention, designation of this region is effected by an operator marking the skin of a patient with an outline 50, which outline is imaged by camera 46 and displayed by display 48 and is also employed by the lipolysis control computer 44 for controlling the application of ultrasonic energy to locations within the region. A computer calculated representation of the outline may also be displayed on display 48, as designated by reference numeral 52. Alternatively, the operator may make a virtual marking on the skin, such as by using a digitizer (not shown), which also may provide computer calculated outline representation 52 on display 48.

In addition to the outline representation 52, the functionality of the system of the present invention preferably also employs a plurality of markers 54 which are typically located outside the region containing adipose tissue, but may be located inside the region designated by outline 50. Markers 54 are visually sensible markers, which are clearly seen by camera 46, captured by camera 46 and displayed on display 48. Markers 54 may be natural anatomic markers, such as distinct portions of the body or alternatively artificial markers such as colored stickers. These markers are preferably employed to assist the system in dealing with deformation of the region nominally defined by outline 50 due to movement and reorientation of the body. Preferably, the transducer 10 also bears a visible marker 56 which is also captured by camera 46 and displayed on display 48.

Markers 54 and 56 are typically processed by computer 44 and may be displayed on display 48 as respective computed marker representations 58 and 60 on display 48.

FIG. 1 illustrates the transducer 10 being positioned on the body over a location within the region containing adipose tissue. Blocks designated by reference numerals 62 and 64 show typical portions of a region containing adipose tissue, respectively before and after lipolysis in accordance with a

preferred embodiment of the invention. It is seen from a comparison of blocks 62 and 64 that, in accordance with a preferred embodiment of the present invention, within the region containing adipose tissue, the adipose tissue, designated by reference numeral 66, is lysed, while non-adipose tissue, such as connective tissue, designated by reference numeral 68, is not lysed.

Reference is now FIG. 2, which is a simplified block diagram illustration of a preferred power source and modulator assembly 40 (FIG. 1), showing a pattern of variation of ultrasonic pressure over time in accordance with a preferred embodiment of the present invention. As seen in FIG. 2, the power source and modulator assembly 40 preferably comprises a signal generator 100 which provides a time varying signal which is modulated so as to have a series of relatively high amplitude portions 102 separated in time by a series of typically relatively low amplitude portions 104. Each relatively high amplitude portion 102 preferably corresponds to a cavitation period and preferably has a decreasing amplitude over time.

Preferably the relationship between the time durations of portions 102 and portions 104 is such as to provide a duty cycle between 1:2 and 1:250, more preferably between 1:5 and 1:30 and most preferably between 1:10 and 1:20.

Preferably, the output of signal generator 100 has a frequency in a range of 50 KHz-1000 KHz, more preferably between 100 KHz-500 KHz and most preferably between 150 KHz-300 KHz.

The output of signal generator 100 is preferably provided to a suitable power amplifier 106, which outputs via impedance matching circuitry 108 to an input of ultrasonic transducer 10 (FIG. 1), which converts the electrical signal received thereby to a corresponding ultrasonic energy output. As seen in FIG. 2, the ultrasonic energy output comprises a time varying signal which is modulated correspondingly to the output of signal generator 100 so as to having a series of relatively high amplitude portions 112, corresponding to portions 102, separated in time by a series of typically relatively low amplitude portions 114, corresponding to portions 104.

Each relatively high amplitude portion 102 preferably corresponds to a cavitation period and has an amplitude at a target volume 12 (FIG. 1) in the body which exceeds a cavitation maintaining threshold 120 and preferably has a decreasing amplitude over time. At least an initial pulse of each relatively high amplitude portion 112 has an amplitude at the target volume 12, which also exceeds a cavitation initiation threshold 122.

Relatively low amplitude portions 114 have an amplitude which lies below both thresholds 120 and 122.

Preferably the relationship between the time durations of portions 112 and portions 114 is such as to provide a duty cycle between 1:2 and 1:250, more preferably between 1:5 and 1:30 and most preferably between 1:10 and 1:20.

Preferably, the ultrasonic energy output of ultrasonic transducer 10 has a frequency in a range of 50 KHz-1000 KHz, more preferably between 100 KHz-500 KHz and most preferably between 150 KHz-300 KHz.

Preferably, each high amplitude portion 112 is comprised of between 2 and 1000 sequential cycles at an amplitude above the cavitation maintaining threshold 120, more preferably between 25 and 500 sequential cycles at an amplitude above the cavitation maintaining threshold 120 and most preferably between 100 and 300 sequential cycles at an amplitude above the cavitation maintaining threshold 120.

Reference is now made to FIGS. 3A and 3B, which are simplified pictorial illustrations of the appearance of an operator interface display during normal operation and faulty

operation respectively. As seen in FIG. 3A, during normal operation, display 48 typically shows a plurality of target volumes 12 (FIG. 1) within a calculated target region 200, typically delimited by outline representation 52 (FIG. 1). Additionally, display 48 preferably provides one or more pre-programmed performance messages 202 and status messages 203.

It is seen the various target volumes 12 are shown with different shading in order to indicate their treatment status. For example, unshaded target volumes, here designated by reference numerals 204 have already experienced lipolysis. A blackened target volume 12, designated by reference numeral 205 is the target volume next in line for lipolysis. A partially shaded target volume 206 typically represents a target volume which has been insufficiently treated to achieve complete lipolysis, typically due to an insufficient treatment duration.

Other types of target volumes, such as those not to be treated due to insufficient presence of adipose tissue therein or for other reasons, may be designated by suitable colors or other designations, and are here indicated by reference numerals 208 and 210.

Typical performance messages 202 may include "CAVITATION IN PROCESS" and "FAT LYSED IN THIS VOLUME". Typical status messages 203 may include an indication of the power level, the operating frequency, the number of target volumes 12 within the calculated target region 200 and the number of target volumes 12 which remain to undergo lipolysis.

Display 48 also preferably includes an graphical cross sectional indication 212 derived from an ultrasonic image preferably provided by imaging ultrasonic transducer subassembly 23 (FIG. 1). Indication 212 preferably indicates various tissues in the body in cross section and shows the target volumes 12 in relation thereto. In accordance with a preferred embodiment of the present invention, indication 212 may also provide a visually sensible indication of cavitation within the target volume 12.

Turning to FIG. 3B, it is seen that during abnormal operation, display 48 provides pre-programmed warning messages 214.

Typical warning messages may include "BAD ACOUSTIC CONTACT", "TEMPERATURE TOO HIGH". The "TEMPERATURE TOO HIGH" message typically relates to the skin tissue, although it may alternatively or additionally relate to other tissue inside or outside of the target volume or in transducer 10 (FIG. 1).

Reference is now made to FIG. 4, which illustrates an ultrasonic lipolysis system constructed and operative in accordance with a preferred embodiment of the present invention. As described hereinabove with reference to FIG. 1 and as seen in FIG. 4, the ultrasonic lipolysis system comprises a lipolysis control computer 44, which outputs to a display 48. Lipolysis control computer 44 preferably receives inputs from video camera 46 (FIG. 1) and from a temperature measurement unit 300, which receives temperature threshold settings as well as inputs from skin temperature sensor 34 (FIG. 1) and transducer temperature sensor 36 (FIG. 1). Temperature measurement unit 300 preferably compares the outputs of both sensors 34 and 36 with appropriate threshold settings and provides an indication to lipolysis control computer 44 of exceedance of either threshold.

Lipolysis control computer 44 also preferably receives an input from an acoustic contact monitoring unit 302, which in turn preferably receives an input from a transducer electrical properties measurement unit 304. Transducer electrical properties measurement unit 304 preferably monitors the output

of power source and modulator assembly 40 (FIG. 1) to ultrasonic therapeutic transducer 13.

An output of transducer electrical properties measurement unit 304 is preferably also supplied to a power meter 306, which provides an output to the lipolysis control computer 44 and a feedback output to power source and modulator assembly 40.

Lipolysis control computer 44 also preferably receives inputs from cavitation detection functionality 308, tissue layer identification functionality 310 and lysed adipose tissue identification functionality 312, all of which receive inputs from ultrasonic reflection analysis functionality 314. Ultrasonic reflection analysis functionality 314 receives ultrasonic imaging inputs from an ultrasonic imaging subsystem 316, which operates ultrasonic imaging transducer 23 (FIG. 1).

Lipolysis control computer 44 provides outputs to power source and modulator assembly 40, for operating ultrasonic therapeutic transducer 13, and to ultrasonic imaging subsystem 316, for operating ultrasonic imaging transducer 23. A positioning control unit 318 also receives an output from lipolysis control computer 44 for driving X-Y-Z positioning assembly 49 (FIG. 1) in order to correctly position transducer 10, which includes ultrasonic therapeutic transducer 13 and ultrasonic imaging transducer 23.

Reference is now made to FIGS. 5A, 5B and 5C, which are together a simplified flowchart illustrating operator steps in carrying out lipolysis in accordance with a preferred embodiment of the present invention. As seen in FIG. 4A, initially an operator preferably draws an outline 50 (FIG. 1) on a patient's body. Preferably, the operator also adheres stereotactic markers 54 (FIG. 1) to the patient's body and places transducer 10, bearing marker 56, at a desired location within outline 50.

Camera 46 (FIG. 1) captures outline 50 and markers 54 and 56. Preferably, outline 50 and markers 54 and 56 are displayed on display 48 in real time. The output of camera 46 is also preferably supplied to a memory associated with lipolysis control computer 44 (FIG. 1).

A computerized tracking functionality preferably embodied in lipolysis control computer 44 preferably employs the output of camera 46 for computing outline representation 52, which may be displayed for the operator on display 48. The computerized tracking functionality also preferably computes coordinates of target volumes for lipolysis treatment, as well as adding up the total volume of tissue sought to undergo lipolysis.

Preferably, the operator confirms the locations of markers 54 and 56 on display 48 and the computerized tracking functionality calculates corresponding marker representations 58 and 60.

In accordance with a preferred embodiment of the present invention the computerized tracking functionality employs markers 54 and marker representations 58 for continuously maintaining registration of outline 50 with respect to outline representation 52, and thus of target volumes 12 with respect to the patient's body, notwithstanding movements of the patient's body during treatment, such as due to breathing or any other movements, such as the patient leaving and returning to the treatment location.

The computerized tracking functionality selects an initial target volume to be treated and positioning control unit 318 (FIG. 4), computes the required repositioning of transducer 10. X-Y-Z positioning assembly 49 repositions transducer 10 to overlie the selected target volume.

Referring additionally to FIG. 5B, it is seen that following repositioning of transducer 10, the lipolysis control computer 44 confirms accurate positioning of transducer 10 with respect to the selected target volume. The ultrasonic imaging

subsystem **316** (FIG. **4**) operates ultrasonic imaging transducer **23**, causing it to provide an ultrasonic reflection analysis functionality **314** for analysis.

Based on an output from ultrasonic reflection analysis functionality **314**, the thicknesses of the various tissue layers of the patient are determined. Upon receiving an indication of the tissue layer thicknesses, an operator may approve the selected target volume and activates the power source and modulator assembly **40** (FIG. **1**).

Turning additionally to FIG. **5C**, it is seen that the following functionalities take place:

Transducer electrical properties measurement unit **304** provides an output to acoustic contact monitoring unit **302**, which determines whether sufficient acoustic contact with the patient is present, preferably by analyzing the current and voltage at therapeutic transducer **13**.

Transducer electrical properties measurement unit **304** provides an output to power meter **306**, which computes the average electrical power received by the therapeutic transducer **13**. If the average electrical power received by the therapeutic transducer **13** exceeds a predetermined threshold, operation of the power source and modulator assembly **40** may be automatically terminated.

Skin temperature sensor **34** measures the current temperature of the skin at transducer **10** and supplies it to temperature measurement unit **300**, which compares the skin temperature to the threshold temperature. Similarly, transducer temperature sensor **36** measures the current temperature at transducer **10** and supplies it to temperature measurement unit **300**, which compares the transducer temperature to the threshold temperature. The outputs of temperature measurement unit **300** are supplied to lipolysis control computer **44**.

The ultrasonic imaging subsystem **316** operates ultrasonic imaging transducer **23** and receives an imaging output, which is analyzed by ultrasonic reflection analysis functionality **314**. The result of this analysis is employed for cavitation detection and a cavitation detection output is supplied to lipolysis control computer **44**.

Should any of the following four conditions occur, the power source and modulator assembly **40** automatically terminates operation of therapeutic transducer **13**. Should none of the following conditions occur, the automatic operation of power source and modulator assembly **40** continues:

1. Acoustic contact is insufficient.
2. Skin temperature exceeds threshold temperature level.
3. Transducer **13** temperature exceeds threshold temperature level.
4. Cavitation is not detected.

Returning to FIG. **5B**, it is noted that during automatic operation of power source and modulator assembly **40**, video camera **46** preferably records the target region and notes whether the transducer **10** remained stationary during the entire treatment duration of the selected target volume **12**. If so, and if none of the aforesaid four conditions took place, lipolysis control computer **44** confirms that the selected target volume was treated. The computerized tracking functionality of lipolysis control computer **44** then proposes a further target volume **12** to be treated.

If, however, the transducer **10** did not remain stationary for a sufficient duration, the selected target volume is designated by lipolysis control computer **44** as having been insufficiently treated.

It is appreciated that by using multiple transducers multiplicity of target volumes can be treated at various time patterns such as sequential time patterns or partially overlapping time patterns.

It is also appreciated that the multiplicity of target volumes may also overlap in space or partially overlap in space.

The Appendix includes a software object code for the computational tracking functionality and includes the following steps:

- 1). Provide a PC computer, such as an Intel-based Pentium III 800 MHz computer with Microsoft Windows 2000 operating system, a hard disk with a minimal capacity of 10 GB, 1 available PCI slot and a 17" computer screen.
- 2). Matrox Orion Frame Grabber Hardware installation/configuration:
 - a). Remove/Disable the VGA board present in the PC computer.
 - b). Place the Matrox Orion Frame Grabber board available from Matrox (1055 boul. St-Regis, Dorval, Quebec Canada H9P 2T4) into an available PCI slot in the PC computer.
 - c). Under Microsoft Windows 2000, on booting the computer, Microsoft Windows' Plug-and-Play system detects a new Multimedia Video Device and requests to assign it a driver. At this point, click Cancel.
 - d). Install the JAI CV-S3200 DSP Surveillance Color CCD Camera available from JAI America Inc., 23046 Avenida de la Carlota, Suite 450, Laguna Hills, Calif. 92653 United States and connect to the Matrox Orion Framer Grabber.
 - e). Set the computer screen impedance switches, red, green, and blue inputs to 75 ohms.
 - f). Set the computer screen synchronization inputs to high impedance and external sync mode.
 - g). Connect the computer screen to Matrox Orion's 15-pin female VGA output connector (DB-15).
- 3). Matrox MIL-Lite software (version 6.1) installation:
 - a). Run the Matrox MIL-Lite setup.exe program and follow the default prompts.
 - b). Run the Matrix Expansion Pack (version 1.0).
 - c). Choose "PAL-YC mode of grabbing" when prompted.
 - d). Establish the RS-232 serial communication between the PC and the JAI camera by registering and installing the "JAI Camera ActiveX object"
- 4). Track Software Installation:
 - a). Create the following respective directories:
 - (1). <Track root>—a root directory for Track project
 - (2). <Track root>\Src—contains source code files
 - (3). <Track root>\Debug—contains an executable file for Track project
 - (4). <Track root>\Images—contains BMP files for debugging the interior region detection process.
 - (5). <Track root>\Log—contains log files and BMP image of the scene
 - (6). <Track root>\Timing—contains timing data files for debugging
 - b). Create the file TRACKOBJ.HEX based on the Appendix and place it into a temporary directory.
 - c). Unhex the computer listing TRACKOBJ.HEX using HEX. IT V1.8 or greater by John Augustine, 3129 Earl St., Laureldale, Pa. 19605 creating file TRACKOBJ.ZIP
 - d). Decompress the file TRACKOBJ.ZIP using WINZIP version 6.2 or greater, extracting all files into a temporary directory essentially extracting the following file objects:
 - 1). CAMERADLG.OBJ
 - 2). DISPLAYFUNCS.OBJ
 - 3). IMAGEPROC.OBJ
 - 4). INTERIORREGION.OBJ
 - 5). MARKERS.OBJ
 - 6). NODES.OBJ
 - 7). PARAMETER.SDLG.OBJ
 - 8). STDAFX.OBJ
 - 9). TRACK.OBJ

- 10). TRACK.RES
- 11) TRACKDLG.OBJ
- 12). TRANSDUCER.OBJ
- 13). UTILS.OBJ
- 14). VIDEOMATROX.OBJ

e). Compile the Object code stored in the temporary directory created in step 4d using Microsoft Visual C++ compiler version 6.0 The resulting application is created: TRACK-.EXE

f). To run the Track software, execute the program TRACK.EXE and follow the on-line help to operate the program.

It is appreciated that the software components of the present invention may, if desired, be implemented in ROM (read-only memory) form. The software components may, generally, be implemented in hardware, if desired, using conventional techniques.

It is appreciated that the particular embodiment implemented by the Appendix is intended only to provide an extremely detailed disclosure of the present invention and is not intended to be limiting.

It will be appreciated by persons skilled in the art that the present invention is not limited by what has been particularly shown and described hereinabove. Rather the scope of the present invention includes both combinations and subcombinations of the various features described hereinabove as well as variations and modifications which would occur to persons skilled in the art upon reading the specification and which are not in the prior art.

What is claimed is:

1. A method for lysing adipose tissue comprising the steps of:

generating, at a source outside a body, ultrasonic energy; and

directing said ultrasonic energy, from said source outside said body, at one or more target volumes of a body containing both adipose tissue and non-adipose tissue; wherein directing ultrasonic energy is performed upon receiving an indication from a cavitation detector and upon detection of non-lysed adipose tissue in the one or more target volumes, wherein said ultrasonic energy selectively lyses adipose tissue in said one or more target volumes and generally does not lyse said non-adipose tissue in said one or more target volumes, which receive said ultrasonic energy.

2. The method according to claim 1, wherein the indication from the cavitation detector is indicative of cavitation.

3. The method according to claim 1, wherein the indication from the cavitation detector is indicative of no cavitation.

4. The method for lysing adipose tissue according to claim 1 and wherein said directing ultrasonic energy generally prevents lysis of tissue outside of said one or more target volumes.

5. The method for lysing adipose tissue according to claim 1 and also comprising: ultrasonic imaging of said region at least partially concurrently with directing said ultrasonic energy at said one or more target volumes.

6. The method for lysing adipose tissue according to claim 1 and wherein said directing comprises positioning at least one ultrasonic transducer relative to said body in order to direct said ultrasonic energy at said one or more target volumes.

7. The method for lysing adipose tissue according to claim 1 and wherein said directing comprises varying the focus of at least one ultrasonic transducer in order to direct said focused ultrasonic energy at said one or more target volumes.

8. The method for lysing adipose tissue according to claim 7 and wherein varying the focus changes the volume of said one or more target volumes.

9. The method for lysing adipose tissue according to claim 7 and wherein varying the focus changes the distance of said one or more target volumes from said at least one ultrasonic transducer.

10. The method for lysing adipose tissue according to claim 5 and wherein said directing comprises positioning at least one ultrasonic transducer relative to said body in order to direct said ultrasonic energy at said one or more target volumes.

11. The method for lysing adipose tissue according to claim 5 and wherein said directing comprises varying the focus of at least one ultrasonic transducer in order to direct said focused ultrasonic energy at said one or more target volumes.

12. The method for lysing adipose tissue according to claim 9 and wherein varying the focus changes the volume of said one or more target volumes.

13. The method for lysing adipose tissue according to claim 9 and wherein varying the focus changes the distance of said one or more target volumes from said at least one ultrasonic transducer.

14. The method for lysing adipose tissue according to claim 1 and also comprising sensing ultrasonic energy coupling to an external surface of said body adjacent said one or more target volumes.

15. The method for lysing adipose tissue according to claim 1 and wherein said ultrasonic energy has a frequency in a range of 50 KHz-1000 KHz.

16. The method for lysing adipose tissue according to claim 1 and wherein said ultrasonic energy has a frequency in a range of 100 KHz-500 KHz.

17. The method for lysing adipose tissue according to claim 1 and wherein said ultrasonic energy has a frequency in a range of 150 KHz-300 KHz.

18. The method for lysing adipose tissue according to claim 1 and also comprising modulating said ultrasonic energy wherein said modulating provides a duty cycle between 1:2 and 1:250.

19. The method for lysing adipose tissue according to claim 1 and also comprising modulating said ultrasonic energy wherein said modulating provides a duty cycle between 1:5 and 1:30.

20. The method for lysing adipose tissue according to claim 1 and also comprising modulating said ultrasonic energy wherein said modulating provides a duty cycle between 1:10 and 1:20.

21. The method for lysing adipose tissue according to claim 18 and wherein said modulating provides between 2 and 1000 sequential cycles at an amplitude above a cavitation threshold.

22. The method for lysing adipose tissue according to claim 18 and wherein said modulating provides between 25 and 500 sequential cycles at an amplitude above a cavitation threshold.

23. The method for lysing adipose tissue according to claim 18 and wherein said modulating comprises modulating the amplitude of said ultrasonic energy over time.

24. The method according to claim 1, further comprising defining a region in the body at least partially by detecting spatial indications on said body, wherein said region comprises the one or more target volumes of the body.

25. The method according to claim 1, and wherein said directing comprises directing focused ultrasonic energy at a multiplicity of target volumes.

26. The method according to claim 25, further comprising computerized tracking of said multiplicity of target volumes notwithstanding movement of said body.

27. Apparatus for lysing adipose tissue comprising:

a focused ultrasonic energy director, adapted for directing focused ultrasonic energy at one or more target volumes in a region of a body, said one or more target volumes containing both adipose tissue and non-adipose tissue; and

a modulator, cooperating with said energy director, said modulator is adapted to produce a focused ultrasonic energy so as to selectively lyse said adipose tissue in said one or more target volumes and generally not lyse non-adipose tissue in said one or more target volumes, which receive said ultrasonic energy, wherein said modulator is adapted to produce the focused-ultrasonic energy upon receiving an indication from a cavitation detector and upon receiving an indication of non-lysed adipose tissue in the one or more target volumes.

28. The apparatus according to claim 27, wherein the indication from the cavitation detector is indicative of cavitation.

29. The apparatus according to claim 27, wherein the indication from the cavitation detector is indicative of no cavitation.

30. The apparatus for lysing adipose tissue according to claim 27, and wherein said director ultrasonic energy generally prevents lysis of tissue outside of said one or more target volumes.

31. The apparatus for lysing adipose tissue according to claim 27 and also comprising: ultrasonic imager adapted for providing ultrasonic imaging of said region at least partially concurrently with directing said ultrasonic energy at said one or more target volumes.

32. The apparatus for lysing adipose tissue according to claim 27 and wherein said director comprises a positioner adapted to positioning at least one ultrasonic transducer relative to said body in order to direct said ultrasonic energy at said one or more target volumes.

33. The apparatus for lysing adipose tissue according to claim 27 and wherein said director is further adapted to vary the focus of at least one ultrasonic transducer in order to direct said focused ultrasonic energy at said one or more target volumes.

34. The apparatus for lysing adipose tissue according to claim 33 and wherein varying the focus changes the volume of said one or more target volumes.

35. The apparatus for lysing adipose tissue according to claim 33 and wherein varying the focus changes the distance of said one or more target volumes from said at least one ultrasonic transducer.

36. The apparatus for lysing adipose tissue according to claim 32 and wherein said director is further adapted to posi-

tion at least one ultrasonic transducer relative to said body in order to direct said ultrasonic energy at said one or more target volumes.

37. The apparatus for lysing adipose tissue according to claim 32 and wherein said director is further adapted to vary the focus of at least one ultrasonic transducer in order to direct said focused ultrasonic energy at said one or more target volumes.

38. The apparatus for lysing adipose tissue according to claim 27 and also comprising a sensor adapted to sense ultrasonic energy coupling to an external surface of said body adjacent said one or more target volumes.

39. The apparatus for lysing adipose tissue according to claim 27 and wherein said ultrasonic energy has a frequency in a range of 50 KHz-1000 KHz.

40. The apparatus for lysing adipose tissue according to claim 27 and wherein said ultrasonic energy has a frequency in a range of 100 KHz-500 KHz.

41. The apparatus for lysing adipose tissue according to claim 27 and wherein said ultrasonic energy has a frequency in a range of 150 KHz-300 KHz.

42. The apparatus for lysing adipose tissue according to claim 27 wherein said modulator is adapted to provide a duty cycle between 1:2 and 1:250.

43. The apparatus for lysing adipose tissue according to claim 27 wherein said modulator is adapted to provide a duty cycle between 1:5 and 1:30.

44. The apparatus for lysing adipose tissue according to claim 27 wherein said modulator is adapted to provide a duty cycle between 1:10 and 1:20.

45. The apparatus for lysing adipose tissue according to claim 27 wherein said modulator is adapted to provide between 2 and 1000 sequential cycles at an amplitude above a cavitation threshold.

46. The apparatus for lysing adipose tissue according to claim 27 wherein said modulator is adapted to provide between 25 and 500 sequential cycles at an amplitude above a cavitation threshold.

47. The apparatus for lysing adipose tissue according to claim 46 and wherein said modulator is further adapted to modulate the amplitude of said ultrasonic energy over time.

48. The apparatus according to claim 27, further comprising a region definer adapted to define a region in the body at least partially by detecting spatial indications on said body, wherein said region comprises the one or more target volumes of the body.

49. The apparatus according to claim 27, and wherein said director is further adapted to direct focused ultrasonic energy at a multiplicity of target volumes.

50. The apparatus according to claim 27, further comprising computerized tracking functionality adapted to track said multiplicity of target volumes notwithstanding movement of said body.

* * * * *

专利名称(译)	无创超声波身体轮廓		
公开(公告)号	US7815570	公开(公告)日	2010-10-19
申请号	US11/808632	申请日	2007-06-12
[标]申请(专利权)人(译)	ishel Yoram VITSNUDEL IIIA		
申请(专利权)人(译)	ishel Yoram VITSNUDEL IIIA		
当前申请(专利权)人(译)	ULTRASHAPE LTD.		
[标]发明人	ESHEL YORAM VITSNUDEL ILIA		
发明人	ESHEL, YORAM VITSNUDEL, ILIA		
IPC分类号	A61B8/00 A61B18/00 A61B8/08 A61B17/00 A61B19/00 A61N7/00 A61N7/02		
CPC分类号	A61B17/225 A61B19/5244 A61N7/00 A61B8/08 A61B19/5212 A61B19/56 A61B2017/00022 A61B2017/00084 A61B2017/2253 A61B2019/5265 A61B2019/5272 A61B2019/5276 A61B2019/5437 A61N2007/0008 A61B34/20 A61B34/25 A61B90/361 A61B2034/2065 A61B2034/2072 A61B2090/378 A61B2090/3937		
优先权	10/250955 2003-12-12 US PCT/IL2001/001220 2001-12-31 WO		
其他公开文献	US20080281201A1		
外部链接	Espacenet USPTO		

摘要(译)

用于裂解脂肪组织的方法和系统，包括在该区域内的多个目标体积处引导超声能量，该目标体积包含脂肪组织，从而选择性地裂解目标体积中的脂肪组织并且通常不溶解脂肪组织中的脂肪组织。目标体积和计算机化跟踪多个目标体积，尽管身体运动。

