



US010661309B2

(12) **United States Patent**
Chaggares et al.

(10) **Patent No.:** **US 10,661,309 B2**
(45) **Date of Patent:** **May 26, 2020**

(54) **DUAL FREQUENCY ULTRASOUND
TRANSDUCER INCLUDING AN ULTRAHIGH
FREQUENCY TRANSDUCER STACK AND A
LOW FREQUENCY ULTRASOUND
TRANSDUCER STACK**

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(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 212 days.

(21) Appl. No.: **15/476,898**

(22) Filed: **Mar. 31, 2017**

(65) **Prior Publication Data**

US 2017/0282215 A1 Oct. 5, 2017

Related U.S. Application Data

(60) Provisional application No. 62/317,326, filed on Apr.
1, 2016.

(51) **Int. Cl.**
B06B 1/06 (2006.01)
A61B 8/00 (2006.01)
B06B 1/02 (2006.01)
G10K 11/162 (2006.01)
G10K 11/30 (2006.01)

(Continued)

(52) **U.S. Cl.**
CPC **B06B 1/0614** (2013.01); **A61B 8/4494**
(2013.01); **B06B 1/0207** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC B06B 1/06; B06B 1/0688; B06B 1/02;
B06B 1/0614; B06B 1/0207;
(Continued)

(56) **References Cited**

U.S. PATENT DOCUMENTS

2002/0188200 A1 * 12/2002 Mauchamp A61B 8/00
600/439

2003/0055337 A1 3/2003 Lin
(Continued)

FOREIGN PATENT DOCUMENTS

WO 2009088307 A1 7/2009
WO WO-2009088307 A1 * 7/2009 B06B 1/0292

OTHER PUBLICATIONS

International Searching Authority, International Search Report and
Written Opinion, PCT Patent Application PCT/US2017/025620,
dated Jun. 20, 2017, 12 pages.

Primary Examiner — Hovhannes Baghdasaryan

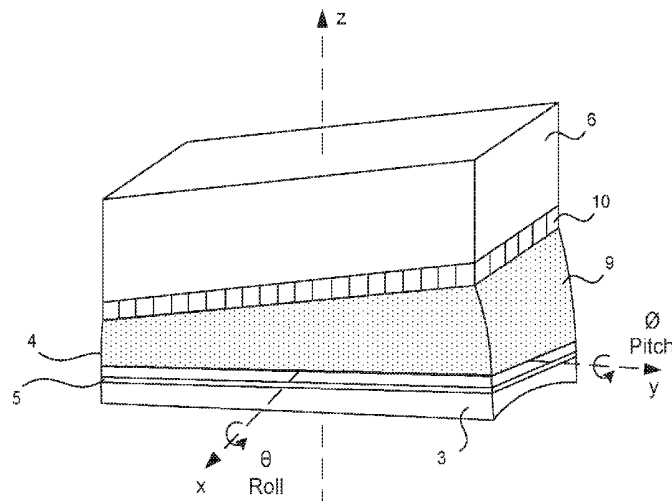
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(57) **ABSTRACT**

A dual frequency ultrasound transducer includes a high frequency ultrasound array and a low frequency transducer positioned behind or proximal to the high frequency ultrasound array. In one embodiment, a dampening material is positioned between a rear surface of the high frequency array and the a front surface of the low frequency array. The dampening preferably is high absorbing of signals at the frequency of the high frequency array but passes signals at the frequency of the low frequency transducer with little attenuation. In additional, or alternatively, the low frequency can angled with respect to the plane of the high frequency transducer to reduce inter-stack multipath reflections. Beam-forming delays compensate for the differences in physical distances between the elements of the low frequency transducer and the plane of the high frequency transducer.

12 Claims, 5 Drawing Sheets



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(51)	Int. Cl. <i>G10K 11/34</i> (2006.01) <i>G01S 15/89</i> (2006.01)	2006/0052699 A1 *	3/2006	Angelsen	A61B 8/14 600/437
		2006/0184022 A1	8/2006	Johnson	
(52)	U.S. Cl. CPC <i>G01S 15/8952</i> (2013.01); <i>G10K 11/162</i> (2013.01); <i>G10K 11/30</i> (2013.01); <i>G10K 11/346</i> (2013.01); <i>B06B 1/0688</i> (2013.01)	2007/0083120 A1 *	4/2007	Cain	A61B 17/22004 600/439
		2008/0319356 A1 *	12/2008	Cain	A61B 17/22004 601/2
(58)	Field of Classification Search CPC G10K 11/162; G10K 11/30; G10K 11/34; G10K 11/346; G01S 15/8952; A61B 8/4494; A61B 8/00 See application file for complete search history.	2008/0319375 A1 *	12/2008	Hardy	A61K 9/0009 604/22
		2009/0178483 A1 *	7/2009	Angelsen	A61B 8/08 73/597
(56)	References Cited U.S. PATENT DOCUMENTS	2010/0036244 A1 *	2/2010	Angelsen	A61B 8/08 600/438
		2012/0267986 A1	10/2012	Galluzzo et al.	
		2014/0150556 A1 *	6/2014	Angelsen	G01S 7/52095 73/627
		2014/0276247 A1 *	9/2014	Hall	A61N 1/0432 601/2
		2005/0277835 A1 *	12/2005	Angelsen	A61B 8/14 600/437

* cited by examiner

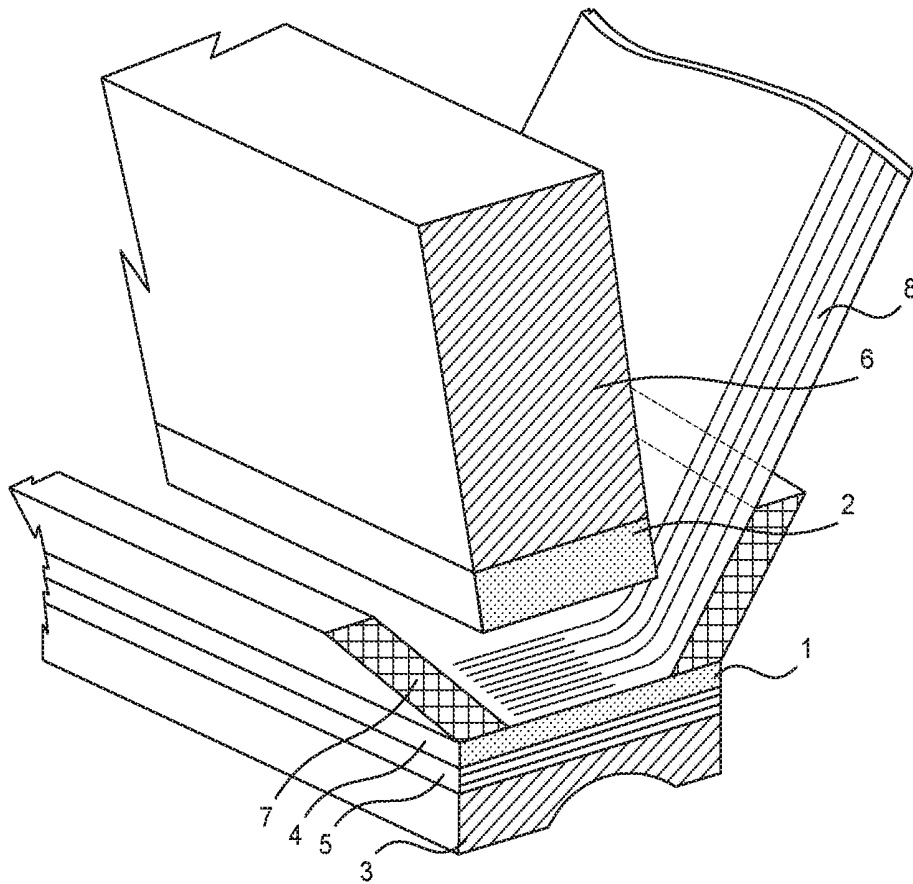


FIG. 1

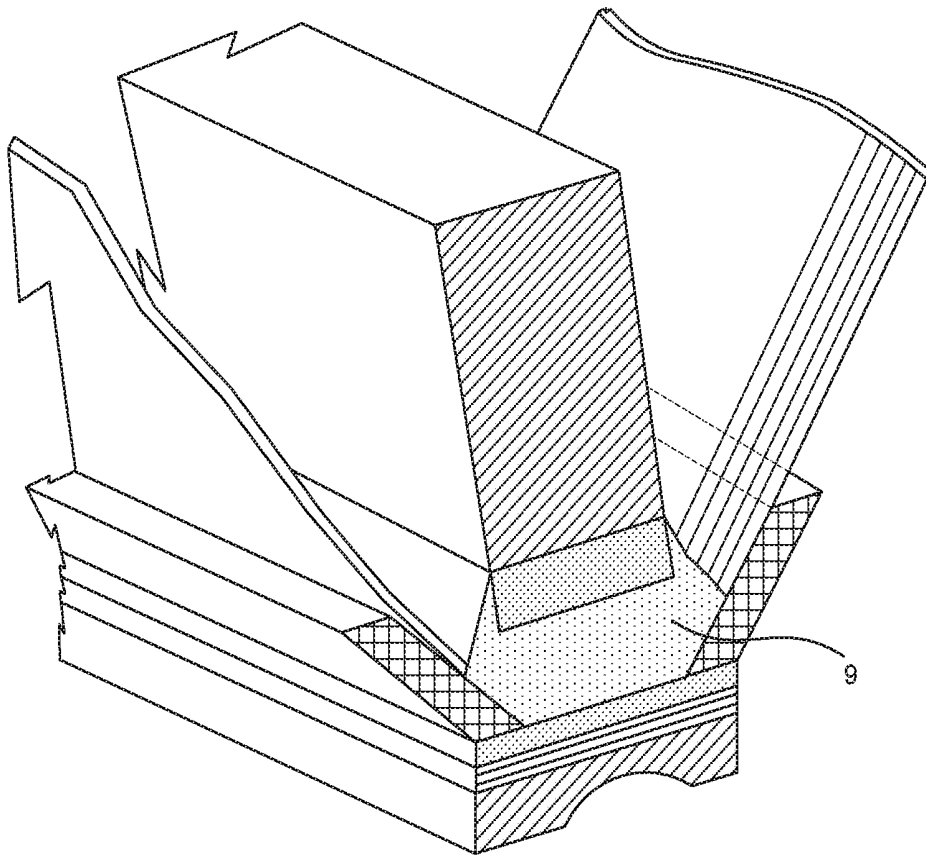


FIG. 2

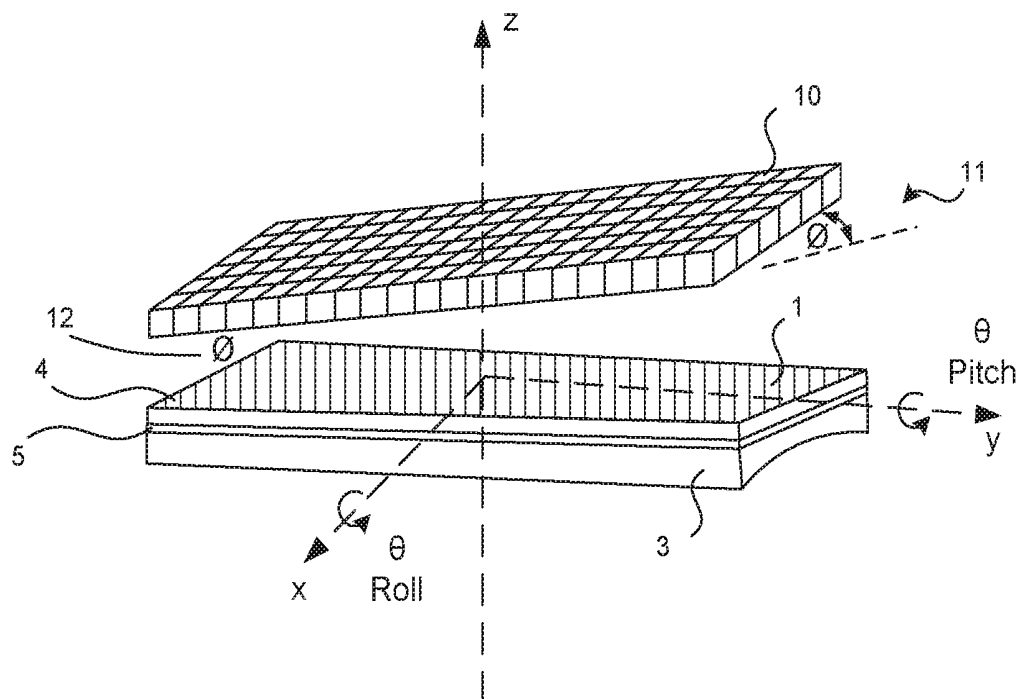


FIG. 3

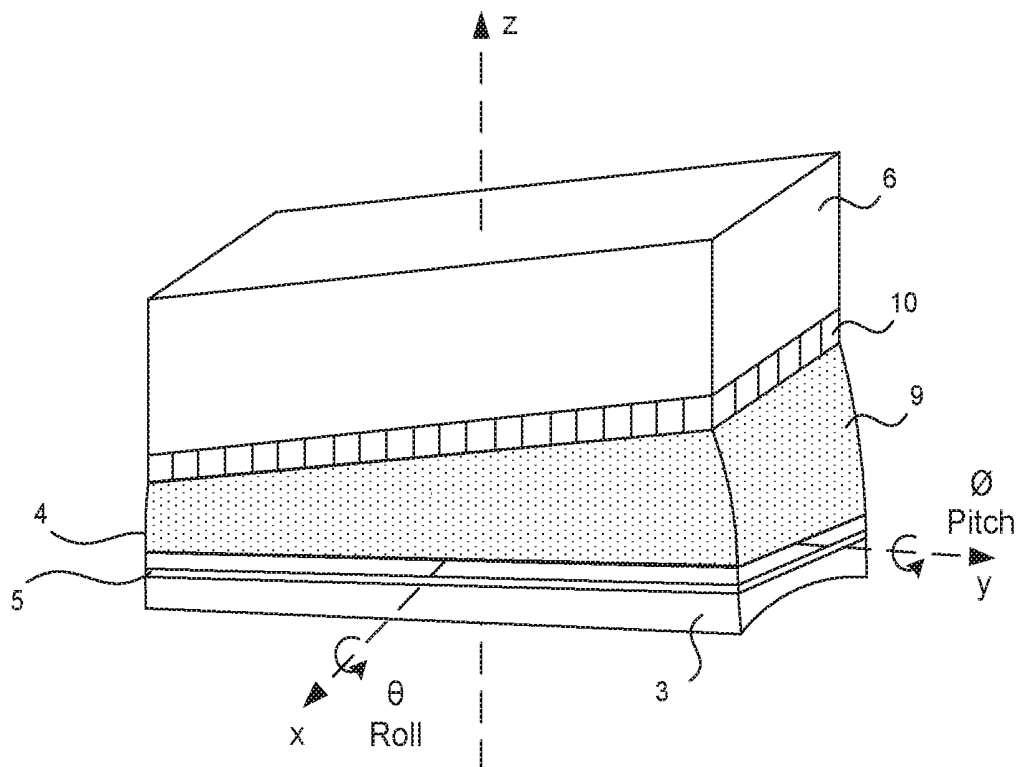


FIG. 4

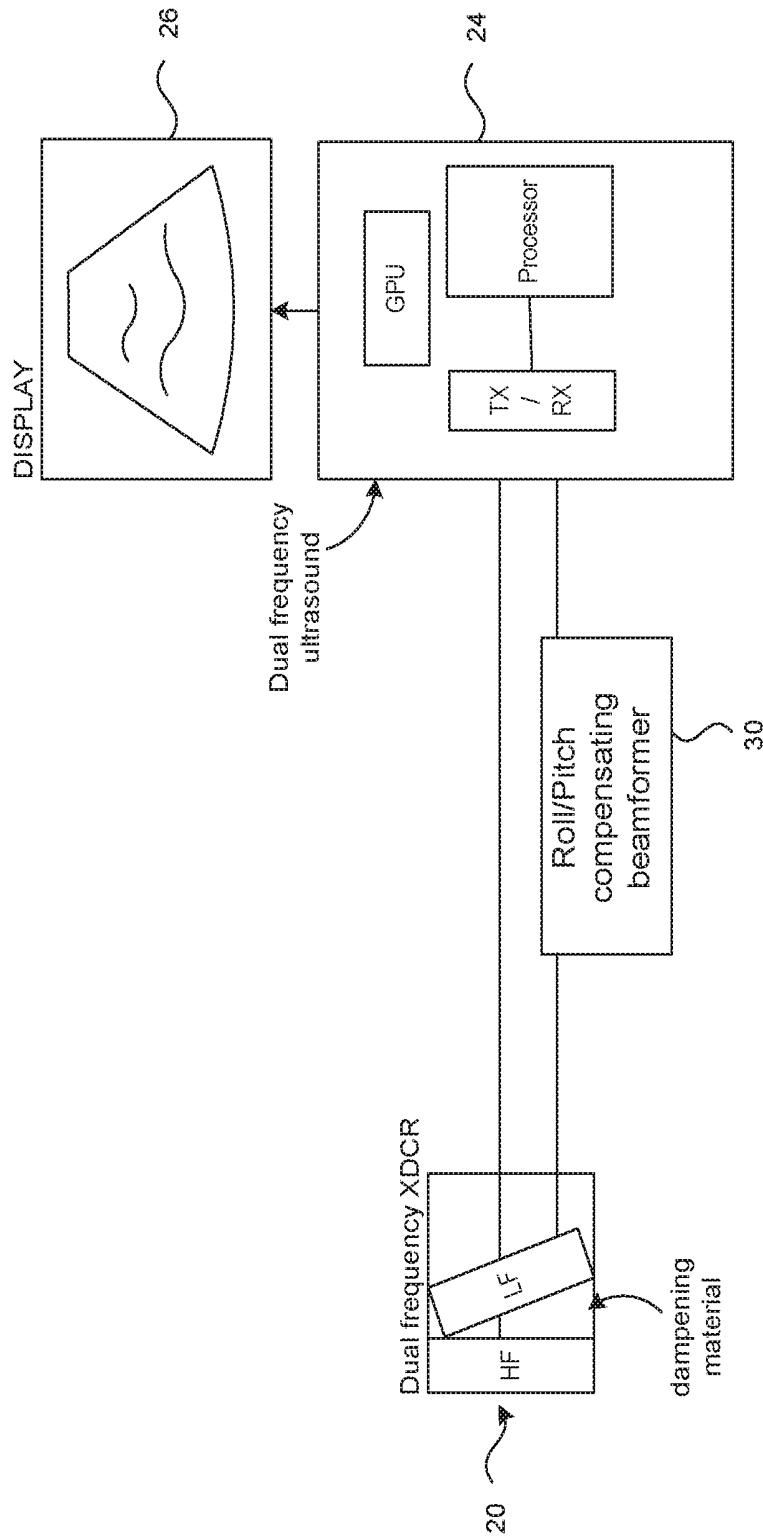


FIG. 5

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DUAL FREQUENCY ULTRASOUND TRANSDUCER INCLUDING AN ULTRAHIGH FREQUENCY TRANSDUCER STACK AND A LOW FREQUENCY ULTRASOUND TRANSDUCER STACK

CROSS-REFERENCE TO RELATED APPLICATION(S)

The present application is related to and claims the benefit of U.S. Provisional Application No. 62/317,326 filed Apr. 1, 2016, which is herein incorporated by reference in its entirety.

TECHNICAL FIELD

The disclosed technology relates to ultrasound imaging transducers and in particular to dual frequency ultrasound imaging transducers.

BACKGROUND

There are several applications for extremely high bandwidth transducers for imaging using non-linear contrast agents and various forms of signal processing designed to enhance tissue contrast resolution and blood detection for example. However, practical limitations to the achievable bandwidth of transducers limit the applications of these promising imaging techniques. Those skilled in the art will be familiar with the concept of dual frequency transducers. The concept of combining two, or even more, transducers into a single acoustic stack or some geometric combination to allow for the use of two bandwidths in concert in some form has been suggested. However, this is a new concept that has not yet found widespread use or success. One significant limitation currently limiting the utility of dual frequency transducers is the lack of an array-based solution. A second challenge is that of superposition of widely differing center frequency transducers on the same acoustic axis.

SUMMARY

As will be explained in further detail below, the disclosed technology relates to dual frequency ultrasound transducers that can be practically manufactured. In one embodiment, a dual frequency transducer includes a high frequency transducer with a low frequency transducer mounted behind or proximal to the high frequency transducer. In one embodiment, a non-linear ultrasound absorbing material is positioned between a front face of the low frequency transducer and a rear surface of the high frequency transducer. In one embodiment, the ultrasound absorbing material strongly absorbs high frequency ultrasound signals while passing low frequency ultrasound signals. In accordance with some aspects of the disclosed technology, the low frequency transducer is oriented at an angle with respect to the high frequency array such that the low frequency stack is rotated about either the axis normal to the azimuthal plane (roll angle), the axis normal to the elevation plane (pitch angle), or both. The resulting orientation of the low frequency array compared with the orientation of the high frequency transducer is such that a front face of the low frequency transducer is not parallel with a front face of the high frequency transducer.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates an embodiment of the disclosed technology showing a dual frequency ultrasound transducer

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including a low frequency (LF) ultrasound transducer stack positioned generally behind, or proximal to, a high frequency (HF) ultrasound stack in accordance with some embodiments of the disclosed technology.

FIG. 2 shows an intermediate acoustic material placed between the low and high frequency stacks in accordance with some embodiments of the disclosed technology.

FIG. 3 depicts a low frequency ultrasound transducer stack that is oriented with one or more of an azimuthal (or roll) and an elevation (or pitch) angle that is offset with respect to an acoustic axis of the HF transducer stack in accordance with some embodiments of the disclosed technology.

FIG. 4 depicts a low frequency ultrasound transducer stack and a backing material coupled to the high frequency ultrasound stack with the intermediate acoustic material in place in accordance with some embodiments of the disclosed technology.

FIG. 5 illustrates a block diagram of a dual frequency ultrasound system including a dual frequency probe and a beamformer that compensates for one or more of a roll or pitch offset of a low frequency transducer in accordance with an embodiment of the disclosed technology.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

In order to realize more of the benefits of a dual frequency transducer, the disclosed technology relates an ultrasound transducer having both high and low frequency elements in the same transducer assembly. In addition, both the low frequency and high frequency transducer elements can be formed as an array to allow beam forming from both the low and high frequency elements. Finally, the low and high frequency elements can have a wide separation of high and low center frequencies of operation to enhance the ultra-wide bandwidth character that is the motivation for making a dual frequency array at all.

In accordance with one embodiment of the technology disclosed herein, a dual frequency transducer design has both low and high frequency array elements that are highly separated in operating frequency, with the HF array having a center frequency (CF) of 15-30 MHz or higher and the LF transducer (which may or may not be a multi-dimensional array) having a CF of about 1-5 MHz. These two transducers are located generally one behind the other (when viewed along a longitudinal axis of a transducer housing that holds the transducers) such that signals to and from the low frequency transducer pass through the high frequency transducer. In addition both transducers share the same elevation lens.

As will be understood by those skilled in the art, challenges related to a coaxial or nearly coaxial dual frequency array of transducers include the difficulty of eliminating reflections, multipath reverberations, and other artifacts arising from acoustic interactions between the components of the LF transducer array and those of the HF transducer array. One skilled in the art will understand that the LF and HF transducers can be chosen to have sufficiently different bandwidths so as to be largely unaffected by reverberations caused by the each other. However, the problems of in-band reflections and multi-path reverberations arising between components of the two acoustic stacks remain.

Impedance matching the LF transducer elements and kerfs to the backing material of the HF array is one approach that could be undertaken to minimize multi-path reverberations. Such impedance matching is challenging since it is

inherently narrow band, and might be different for each material in the stack. If one considers the LF transducer to be an array for example, one skilled in the art will appreciate that impedance matching for the high frequency reverberations will require a different matching solution for the kerfs placed in the LF array compared to the LF transducer elements. Such a solution is highly difficult and impractical. Any impedance mismatch at the face of the LF array will give rise to strong reverberation artifacts in the image created from signals from the HF array.

Two aspects of the technology disclosed herein that can be used alone or in combination, include placing a frequency dependent backing or dampening material that is virtually opaque to HF frequency ultrasound and highly transparent to LF ultrasound (1-5 MHz) between the transducers. In addition or separately, the orientation of the front face of the low frequency transducer can be selected such that it is not parallel to the front face of the HF transducer array to remove multi-path reflection artifacts images produced from signals generated by the HF transducer.

As shown in FIG. 1, a dual frequency transducer includes a high frequency transducer stack 1 and a low frequency transducer 2 that is positioned generally behind or proximal to the high frequency transducer stack 1. The high frequency transducer stack 1 generally comprises an array of elements formed into a sheet of HF piezo material 4 that is coupled to a lens 3 through one or more matching layers 5. A support structure 7 (such as a metal frame e.g. molybdenum) supports the high frequency transducer stack 1 as well as one or more flexible printed circuit boards (PCB) e.g. "flex circuits" (8) used to make connection to the HF elements. In one embodiment, the HF array consists of a 30 MHz element HF ultrasound array built in an oversized frame such that the lens 3 is larger than the typical footprint required to accommodate the 30 MHz array. Suitable techniques for making the HF ultrasound array are described in U.S. Patent Publication No. US2014/0350407 A1 and U.S. Pat. No. 8,316,518, which are herein incorporated by reference in their entireties.

A low frequency transducer 2 (e.g. 2 MHz) is positioned behind the HF transducer stack 1. The low frequency transducer 2 electrodes on front and back (not shown) and has a backing material 6 on its rear surface to attenuate low frequency signals travelling in the rearward direction from the low frequency transducer.

As shown in FIG. 2, an intermediate dampening material 9 is positioned between a front surface of the low frequency transducer 2 and a rear surface of the 30 MHz HF array. The dampening material 9 is designed to be the acoustic backing of the 30 MHz HF array. The dampening material 9 is selected to exhibit very high losses per unit thickness at 30 MHz, but also to act as the front acoustic coupling medium for the low frequency transducer 2 by exhibiting a relatively low loss/unit thickness at 2 MHz. One skilled in the art will understand that acoustic loss coefficients are typically frequency dependent, and some materials exhibit attenuation that is non-linearly dependent on frequency.

One candidate for such an intermediate dampening material 9 that exhibits a non-linear acoustic attenuation is silicone rubber, which is typically employed as a lens material for ultrasound transducers having center frequencies below 10 MHz. Typical silicone materials exhibit acoustic attenuation in the range of 2-4 dB/cm at 2 MHz, while exhibiting over 10 dB/mm at 30 MHz. This property can be leveraged and enhanced in one embodiment of the disclosed technology by adding small (compared to the 2 MHz wavelength e.g. 2-5 um particle size) and relatively

acoustically dissimilar particles to the silicone, causing little change to the low frequency loss, but increasing the loss at 30 MHz to over 25 dB/mm. Suitable choices for the particles include silica powder, silicon dioxide powders, titanium dioxide powders, zirconium dioxide powders or the like, which strongly absorb the high frequency ultrasound signals but due to their size do not act as strong scatterers for the low frequency ultrasound signals. Similarly, other materials besides silicone could be used such as polyurethane, doped epoxies or other materials having highly non-linear loss coefficients versus frequency.

The dampening material 9 enables the placement of the low frequency transducer behind the HF transducer array such that HF ultrasonic waves travelling in the rearward direction from the HF transducer array are attenuated very quickly thereby eliminating any artifact that would arise from internal reflections between the 30 MHz array and the 2 MHz LF transducer. Furthermore, the relatively low attenuation of the powder loaded silicone at 2 MHz allows the low frequency signals to travel out from the 2 MHz low frequency transducer, through the HF piezo sheet 4, and out through the lens 3, making it possible to simultaneously transmit and receive at both high and low frequencies. This embodiment also allows for the use of a composite low frequency transducer or low frequency array with kerfs to be successfully employed, due to the high loss character of the dampening material at 30 MHz. One skilled in the art will understand that if the dampening material was not sufficiently attenuative at high frequency, it would be necessary to attempt to use some form of impedance matching device to ensure that acoustic energy emitted from the HF array and travelling back into the device did not reflect from components of the low frequency transducer and return to the HF array with sufficient energy to give rise to unwanted imaging artifacts.

One skilled in the art will also understand that employing impedance matching to an array with kerfs designed to work efficiently at the LF range or a composite material with such kerfs would present an impractical challenge for the designer and manufacturer, since the LF pitch and kerf dimensions will appear as discrete specular reflectors to the HF energy necessitating a matching system of equal spatial complexity.

As one skilled in the art will understand, the thickness of the dampening material 9 positioned between the high frequency array and the low frequency transducer can be optimized to balance the need for the suppression of multi-path reverberations arising from the HF array with the need for efficient transmission of the LF acoustic energy to the front of the lens. If the layer of dampening material 9 is too thin, then not enough attenuation of the signals from the high frequency transducer will occur. On the other hand, if the layer of dampening material 9 is too thick, then unnecessary losses will occur in the low frequency ultrasound signals and low frequency reverberation could become problematic if it were to persist in time due to an excessively long travel time.

One embodiment of the disclosed technology can have an intermediate dampening material layer 9 made from KE1300T silicone made by Shin Etsu doped with 2-3 um alumina particles to make a material having attenuation coefficients of about 31 dB/mm at 30 MHz and about 2 dB/cm at 2 MHz. An embodiment of the disclosed technology can utilize a layer of this doped silicone having a thickness of about 2.0 mm to achieve a total two way path loss of over 124 dB for the high frequency acoustic wave travelling into the backing and back to the HF array, while

having only about 0.3 dB total one way loss for the LF acoustic energy travelling out of the low frequency transducer 2 toward the lens 3.

In one embodiment, a jig or other tool (not shown) is used to hold the low frequency single element transducer or array 5 transducer at a desired distance away from the high frequency array while the space between the two transducers is filled with the dampening material 9 which is allowed to cure thus fixing the LF transducer in place.

Other intermediate dampening material properties can be 10 achieved and combined with other thicknesses to achieve desirable properties for other dual frequency combinations. For example, a 4 MHz low frequency transducer can be combined with a 20 MHz high frequency array and spaced by 3.0 mm using GE RTV60 (a commercial loaded silicone) 15 for the intermediate dampening material. GE RTV60 exhibits its loss of about 17 dB/mm at 20 MHz and about 3 dB/cm at 4 MHz. This material will result in a two way path loss of about 102 dB for the 20 MHz acoustic energy, and about 0.9 dB loss for the 4 MHz energy. As one experienced in the art 20 will understand, each combination will exhibit different losses at the respective high and low frequencies being used in the dual frequency design. It will further be understood that obtaining acceptable loss values will be more difficult as the two frequencies are chosen closer together since the attenuation coefficient of the coupling medium is a function 25 of frequency.

In another embodiment of the disclosed technology, the low frequency transducer is a 1D, a 1.5D, or a 2D array. The elements of the LF array are connected to conductors (not 30 shown) that apply signals to and receive signals from the array elements. Because the LF array elements are so much larger than those of the HF array, it is not difficult to route conductors to each of the array elements even if they are arranged in more than a single dimension and since the LF array is sized to correspond to the HF array.

In some embodiments of the disclosed technology, the low frequency array is rotated about one or both of its elevation (shown as pitch in FIG. 3) and azimuthal (shown 40 as roll in FIG. 3) axes compared with the axes of the high frequency transducer. One skilled in the art will appreciate that either of these two rotations alone will act to mitigate multipath reflections between the high and low frequency transducers and their components. Together, the two rotations greatly mitigate such multipath reflections. However, 45 such rotations also make coaxial operation of the low and high frequency arrays impossible using normal (perpendicular to the face of the LF stack) beam forming. However, one aspect of the technology disclosed herein will be recognized to overcome this limitation.

In some embodiments of the disclosed technology, the low frequency array is a 1.0D, 1.5D or 2D array that is 50 driven by beamforming hardware and/or software with a delay profile configured to direct the beams produced by the low frequency array in a direction that compensates for the fixed rotational offsets of the LF transducer, thereby allowing the LF array transducer to produce a normal acoustic signal that is coaxial with the signals produced by the high frequency array. As will be understood by those of ordinary skill in the art, beamforming may be done in a processor, DSP or ASIC or other logic by selectively varying one or more of the weights and delays applied to the signals transmitted/received by the arrayed transducer elements to change the effective beam direction. For example, if the transducer is only rotated in the azimuthal direction compared 65 to the forward looking direction of the HF array, then driving signals produced for LF transducer elements can be

driven with an element delay profile that can steer the beam to compensate for the physical rotation of the LF transducer. On the receive side, similar delays/weights are employed for the signals produced by the transducer elements to reconstruct the incoming coaxial beam to compensate for the rotation of the LF transducer with respect to the plane of the HF transducer. If a 1.5D or 2D array is used, then similar software or hardware delays are used for the driving and receive signals to compensate for the rotational offsets of the LF array with respect to the plane of the HF transducer array.

One skilled in the art will appreciate that such an offset in the orientation of the low frequency array with respect to the high frequency array will further mitigate any multipath reflection, allowing the designer to choose the intermediate backing/front coupling material to have a very low loss at low frequency, since it becomes less critical to reduce the high frequency attenuation due to the angled low frequency array orientation. In addition, low frequency inter-stack reverberations will be virtually eliminated with the use of one or more of the azimuthal (roll) and elevation (pitch) offset angles, allowing the designer to optimize the inter-stack distances and materials based on parameters other than simply the minimization of multipath reverberations.

One skilled in the art will understand that the designer can trade off the HF and LF frequency separation, distance between the HF and LF arrays, rotational offset angles, and the attenuation properties of the intermediate dampening material in order to maximize the properties of the dual frequency array to suit the application. For example, a designer could select a high acoustic impedance intermediate damping material such as epoxy doped with heavy particles such as tantalum oxide, hafnium oxide or some other heavy non-conductive particles for example, to improve acoustic bandwidth of the high frequency array. One skilled in the art will understand that a loaded epoxy layer will have much lower acoustic loss at high frequency than, for example, a silicone based layer, giving rise to perhaps unacceptably high multi-path reverberation artifacts. In this case, the designer can employ another aspect of the disclosed technology, specifically the rotational offset angles in for example both elevation and azimuthal directions. The designer can then according to the disclosed technology, employ a 2D array with fixed beam steering and having sufficiently small pitch and directivity properties to provide sufficient steering performance to cancel the offset angles thus achieving a coaxial dual frequency array having highly mitigated multi path reverberations. Again, one skilled in the art will understand that such a 2D array could further be driven with suitable delay profiles combined with the fixed offset profiles to achieve a standard beam focusing and scanning as required with respect to the underlying beam trajectory.

It is further possible for the LF array to be driven with a wide range of beam forming techniques in both transmit and receive while applying the required fixed correction delay profiles to compensate for any pitch and/or roll offsets employed in the design of the DF probe. It will be further understood that correction for fixed pitch and roll offset need not be perfect to provide substantially the same benefits of fully coaxial operation. This invention may be employed to partially correct for pitch and/or roll offsets such that the resulting LF beam has an angular offset from the HF beam, however, as will be understood by those skilled in the art, the LF beam width will generally be larger than the HF beam width by a factor proportional to the high frequency divided by the low frequency. For example, a 2 MHz/30 MHz dual frequency array will have a low frequency beam on the order

of $30/2=15$ times wider than the 30 MHz beam. As such, small angular differences between the axis of the LF and HF arrays are of little consequence up to perhaps as much as 5 degrees for example. It should be understood that correction for rotational offset angles need not be complete and in fact can be intentionally incomplete, employed as an engineering trade-off to allow, for example, the designer to simplify the design of the LF array (i.e. having larger pitch in a 2D array thus allowing less steering correction) while still offsetting the LF stack sufficiently to eliminate multipath reflections in the HF stack.

FIG. 5 is a block diagram of a dual frequency ultrasound system in accordance with one embodiment of the disclosed technology. The system includes a dual frequency transducer 20 having both a high frequency (HF) transducer and low frequency transducer including means for reducing inter-stack multipath reflections by one or more of a dampening material that exhibits high absorption of HF ultrasound signals while passing LF ultrasound signals and an offset in a roll axis, pitch axis or both of the front face of the LF transducer with respect to the HF transducer. Driving signals for the dual frequency transducer are provided by a dual frequency ultrasound machine 24 including conventional components such as transmit/receive circuitry, one or more processors, graphics processing units and memory, communication circuitry etc. A display 26 produces visual images of ultrasound signals captured using both the HF and LF transducer.

A compensating beamformer 30 is provided to compensate for any offset in the roll and/or pitch of the LF transducer. Because the physical orientation of the LF transducer is fixed with respect to the HF transducer, the beamformer can employ fixed delays to steer the transmit and receive beams in a direction that is co-axial or nearly co-axial with the beam produced by the HF transducer. The beamformer 30 can be implemented in a number of ways including a digital signal processor (DSP), an application specific integrated circuit (ASIC), an FPGA employing fixed delays and sum operations in the transmit or receive paths, a programmable processor implementing and the like. The beamformer 30 operates in addition to beamforming provided by the ultrasound machine 24 to steer the beams over a sweep angle. It should be noted that it is possible for the ultrasound machine to perform the compensation for offset as part of the LF image beamforming rather than relying on a separate compensating beamformer, and that such an arrangement is not outside the scope of this invention.

From the foregoing, it will be appreciated that specific embodiments of the disclosed technology have been described herein for purposes of illustration, but that various modifications may be made without deviating from the scope of the disclosed technology. For example although the disclosed embodiments are describes as a 30 MHz HF transducer and a 2 MHz LF transducer, it will be appreciated that the center frequencies of the transducers could be changed. Accordingly, the disclosed technology is not limited except as by the appended claims. In addition, one skilled in the art will understand that many configurations of LF array and offset angles could be devised in light of the aspects of this invention to produce numerous configurations of coaxial and nearly coaxial dual frequency array based probes.

We claim:

1. A dual frequency ultrasound transducer having a low frequency (LF) ultrasound transducer positioned behind a high frequency (HF) transducer array such that they both share a common acoustic axis and including a dampening

layer disposed between a front face of the low frequency transducer and a rear face of the high frequency transducer array for reducing inter-stack multipath reflections, wherein the dampening layer has attenuation properties that increase non-linearly with increasing frequency; and

wherein the dampening layer exhibits acoustic attenuation of about 2-4 dB/cm at about 2 MHz, and the dampening layer exhibits acoustic attenuation of at least 10 dB/mm at about 30 MHz.

2. The dual frequency transducer of claim 1 where the LF transducer is an arrayed transducer.

3. The dual frequency ultrasound transducer of claim 1, wherein the dampening layer is an elastomer having a high coefficient of attenuation for signals produced by the high frequency ultrasound array and a low coefficient of attenuation for signals produced by the low frequency ultrasound transducer.

4. The dual frequency ultrasound transducer of claim 3, wherein the elastomer is silicone.

5. The dual frequency ultrasound transducer of claim 3, wherein the elastomer is doped with a powder that acts as scatterers for signals produced by the high frequency ultrasound array but do not substantially affect the signals produced by the low frequency transducer.

6. A dual frequency array comprising:

a low frequency (LF) 1D, 1.5D, or 2D array positioned behind a high frequency (HF) array such that the LF array is rotated in one or more of roll and pitch such that a first axis normal to a front face of the HF transducer is not parallel with a second axis normal to a front face of the LF transducer; and

a beam former configured to adjust a direction of transmit and receive beams of the LF array such that the LF and HF arrays beams both share a common acoustic axis.

7. The dual frequency array of claim 6, further comprising: a dampening layer positioned between the low frequency array and the high frequency array for reducing the inter stack multipath reflections, wherein the dampening layer has attenuation properties that increase non-linearly with increasing frequency.

8. The dual frequency array of claim 7, wherein the dampening layer has an arbitrary acoustic impedance.

9. The dual frequency array of claim 6 further comprising a common acoustic lens positioned on a front side of the HF array.

10. A dual frequency ultrasound array comprising:

a low frequency (LF) array positioned behind a high frequency (HF) array such that the LF array is rotated in one or more of roll and pitch such that a first axis normal to a front face of the HF transducer is not parallel with a second axis normal to a front face of the LF transducer;

a beam former configured to adjust a direction of transmit and receive beams of the LF array such that the LF and HF arrays beams both share a common acoustic axis; and

an intermediate layer positioned between the LF array and HF array having attenuation properties that increase non-linearly with increasing frequency;

wherein the intermediate layer exhibits acoustic attenuation of about 2-4 dB/cm at about 2 MHz, and the intermediate layer exhibits acoustic attenuation of at least 10 dB/mm at about 30 MHz.

11. A dual frequency array comprising:

a low frequency transducer positioned behind a high frequency array such that the low and high frequency arrays both share a substantially common acoustic axis;

an intermediate layer positioned between the low and high frequency array having attenuation properties that increase non-linearly with increasing frequency; and an acoustic lens that is common to both the low and high frequency arrays;

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wherein the intermediate layer exhibits acoustic attenuation of about 2-4 dB/cm at about 2 MHz, and the intermediate layer exhibits acoustic attenuation of at least 10 dB/mm at about 30 MHz.

12. A dual frequency array comprising:

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a low frequency (LF) transducer positioned behind a high frequency (HF) transducer such that the LF transducer is rotated in one or more of roll and pitch such that a first axis normal to a front face of the HF transducer is not parallel with a second axis normal to a front face of the LF transducer; and

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a beam former configured to adjust beams transmitted by the LF transducer for the offset set in roll and/or pitch.

* * * * *

专利名称(译)	双频超声换能器，包括超高频换能器叠层和低频超声换能器叠层		
公开(公告)号	US10661309	公开(公告)日	2020-05-26
申请号	US15/476898	申请日	2017-03-31
[标]申请(专利权)人(译)	富士胶片索诺声公司		
申请(专利权)人(译)	FUJIFILM SONOSITE, INC.		
当前申请(专利权)人(译)	FUJIFILM SONOSITE, INC.		
[标]发明人	CHAGGARES NICHOLAS CHRISTOPHER PANG GUOFENG HIRSON DESMOND		
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IPC分类号	B06B1/06 G10K11/34 G10K11/30 G10K11/162 B06B1/02 G01S15/89 A61B8/00		
CPC分类号	G10K11/30 B06B1/0207 A61B8/4494 G01S15/8952 B06B1/0614 G10K11/346 G10K11/162 B06B1/0688 G01S15/8915 G10K11/02 G10K11/355		
代理机构(译)	贝克博茨L.L.P.		
优先权	62/317326 2016-04-01 US		
其他公开文献	US20170282215A1		
外部链接	Espacenet		

摘要(译)

双频超声换能器包括高频超声阵列和定位在高频超声阵列后面或附近的低频换能器。在一个实施例中，阻尼材料位于高频阵列的后表面和低频阵列的前表面之间。衰减优选地是在高频阵列的频率处对信号的高吸收，而在低频换能器的频率处以很小的衰减传递信号。另外地或可替代地，低频可以相对于高频换能器的平面成角度，以减少叠层间多径反射。波束成形延迟补偿了低频换能器的元件与高频换能器的平面之间的物理距离差异。

