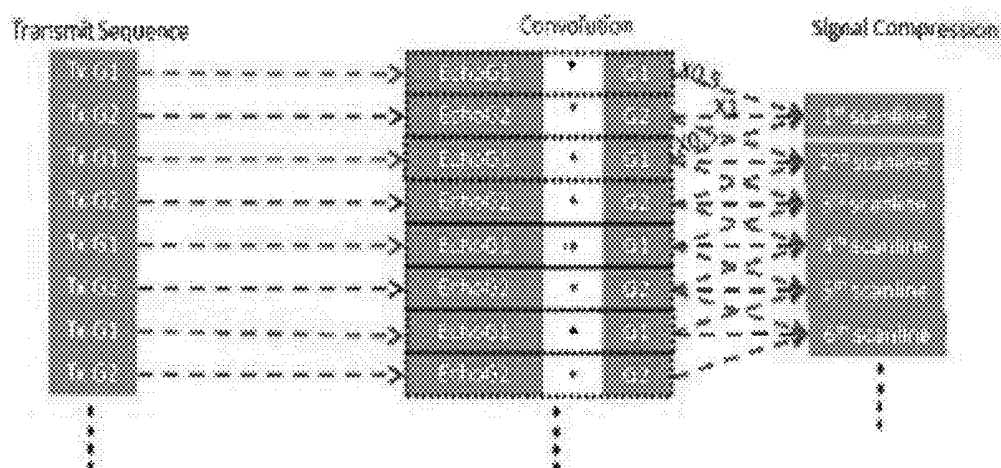




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Park et al.(10) **Pub. No.: US 2014/0276063 A1**(43) **Pub. Date: Sep. 18, 2014**(54) **SYSTEMS AND METHODS FOR PRODUCING
AN IMAGE FROM A ROTATIONAL
INTRAVASCULAR ULTRASOUND DEVICE****Publication Classification**(51) **Int. Cl.***A61B 8/00* (2006.01)*A61B 8/08* (2006.01)*A61B 8/12* (2006.01)(52) **U.S. Cl.**CPC *A61B 8/4461* (2013.01); *A61B 8/12*
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Diego, CA (US)(21) Appl. No.: **14/207,815**(22) Filed: **Mar. 13, 2014****Related U.S. Application Data**(60) Provisional application No. 61/778,757, filed on Mar.
13, 2013.

(57)

ABSTRACTThe invention generally relates systems and methods to for
producing an image from a rotational intravascular ultra-
sound device.

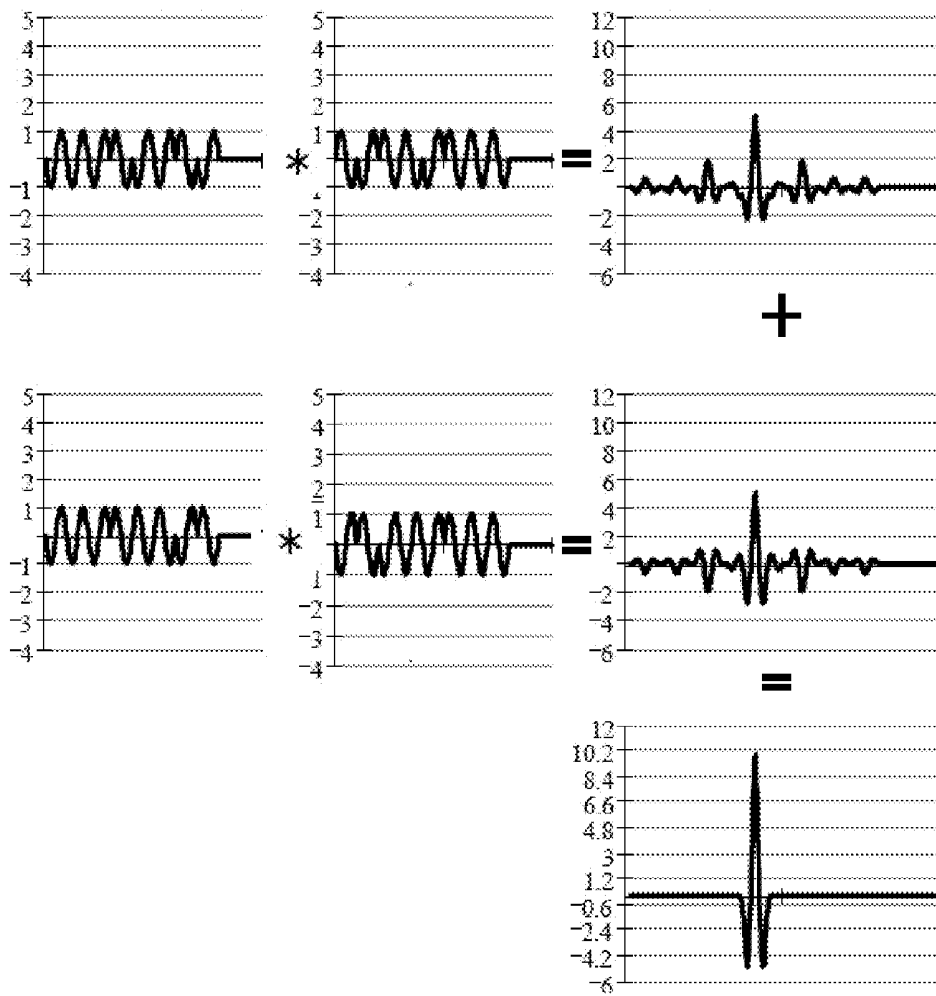


FIG. 1

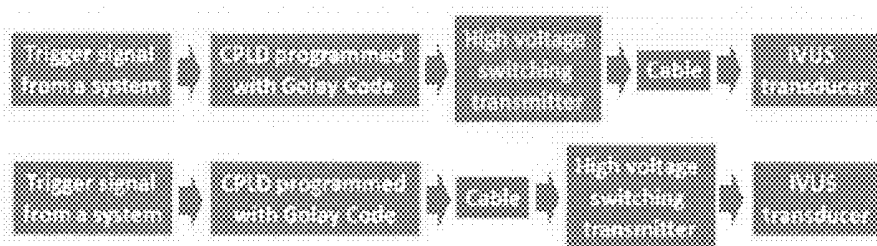


FIG. 2

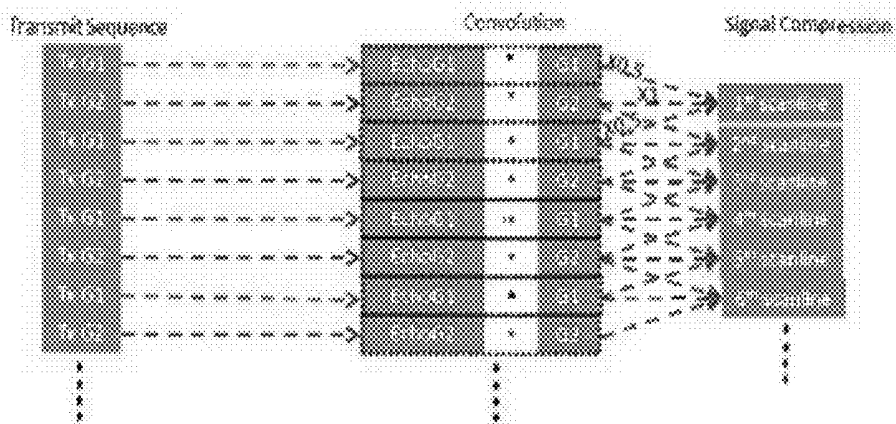


FIG. 3

SYSTEMS AND METHODS FOR PRODUCING AN IMAGE FROM A ROTATIONAL INTRAVASCULAR ULTRASOUND DEVICE

RELATED APPLICATION

[0001] The present application claims the benefit of and priority to U.S. provisional patent application Ser. No. 61/778,757, filed Mar. 13, 2013, the content of which is incorporated by reference herein in its entirety.

FIELD OF THE INVENTION

[0002] The invention generally relates to systems and methods to for producing an image from a rotational intravascular ultrasound device.

BACKGROUND

[0003] In ultrasound imaging, spatial resolution and depth penetration are important parameters to quantitatively assess image quality. Generally, the wavelength at the ultrasound center frequency determines spatial resolution, with resolution improving as the frequency increases. However, tissue attenuation typically increases as a linear function of frequency, even becoming nonlinear at higher frequencies (e.g., greater than 40 MHz) commonly employed in intravascular ultrasound imaging applications. Although high frequency ultrasound facilitates high resolution imaging in the near field, the depth penetration may be compromised, rendering the deep tissue structures difficult to identify.

[0004] To enhance the depth penetration without the loss of spatial resolution, transmit voltage levels are typically increased to deliver more transmit energy to the imaging target. However, this approach is limited both by regulations of diagnostic medical ultrasound and by the nature of the intravascular ultrasound imaging environment, such as the long cable length between ultrasound transducer elements and imaging system electronics and the small size of electronics integrated with the catheter mounted transducer.

[0005] Rather than increasing the transmit voltage levels, coded excitation methods using elongated modulated transmit bursts have been employed to address the dilemma of maintaining depth of penetration while increasing operating frequency for improved spatial resolution. This method is called pulse compression. An ultrasound imaging apparatus using pulse compression employs a coded long pulse instead of the conventional short pulse. One type of coded excitation methods uses Golay codes. A Golay code is a binary code modulated with a short burst. Two different binary code (of particular sequence) constitute a Golay pair. When two codes are separately decoded and summed, range sidelobes are completely eliminated with only the main lobe remaining. Due to that characteristic of Golay codes, there have been great endeavors to take advantage of Golay codes in ultrasound imaging apparatuses.

[0006] In practice, the range sidelobes are not completely removed, due to nonlinear propagation of ultrasound within tissue structures, motion artifacts, and other non-idealities. Particularly for rotational intravascular ultrasound, the continuous rotation causes a slight angular misalignment for adjacent A-scans used to produce a Golay pair, resulting in increased range sidelobe levels.

SUMMARY

[0007] The invention uses short burst modulated Golay codes with a multi-beam approach to suppress the motion artifact in Golay code rotational intravascular ultrasound (IVUS). The multi-beam strategy for use with Golay codes involves alternately transmitting complementary Golay codes and then summing an odd number (greater than one) of weighted, decoded A-scans.

[0008] In certain aspects, the invention provides methods for producing an image from a rotational intravascular ultrasound device. The methods involve alternately transmitting complementary Golay codes to a plurality of transducers in an intravascular ultrasound device. Additionally, the methods involve receiving echoes of the complementary codes from the transducers and performing pulse compression of the echoes. The pulse compression involves weighting the received echoes and summing an odd number of weighted echoes, in which a center echo is given a weighted value of 1.0 and weighted sums of its neighbors constitute complementary echoes of a Golay pair. An image is produced from the compressed echoes, and that image may be displayed. Methods of the invention may additionally involve computing convolution of the received echoes of the complementary codes.

[0009] Any technique known in the art may be used to produce the Golay codes. In certain embodiments, the Golay codes are produced by applying a bi-phase window over the Golay codes. The bi-phase window may be one of a bi-phase rectangular window, a bi-phase Hamming window, a bi-phase Hanning window and bi-phase Bartlett window.

[0010] Another aspect of the invention provides a system for producing an ultrasound image from a rotational intravascular ultrasound device. The system includes a processor, and a plurality of beam modules coupled to the processor. Each module includes a receiver for receiving a trigger signal from the processor, a complex programmable logic device programmed with a Golay code, a high voltage switching transmitter, and an ultrasound transducer.

[0011] The processor alternately transmits trigger signals to the beam modules, thereby causing the beam modules to alternately transmit complementary Golay codes. The processor receives echoes of the complementary codes. The processor performs pulse compression of the echoes that includes weighting the received echoes and summing an odd number of weighted echoes, in which a center echo is given a weighted value of 1.0 and weighted sums of its neighbors constitute complementary echoes of a Golay pair. The processor produces an image from the compressed echoes. The processor is coupled to a display device and causes the image to be displayed.

BRIEF DESCRIPTION OF THE DRAWINGS

[0012] FIG. 1 is a set of graphs showing the principle of side lobe cancellation using pair of Golay complementary sequences of length 8.

[0013] FIG. 2 illustrate a system of the invention.

[0014] FIG. 3 is a diagram showing how methods of the invention are performed.

DETAILED DESCRIPTION

[0015] The invention generally relates systems and methods to for producing an image from a rotational intravascular ultrasound (IVUS) device. Systems and methods of then

invention are particularly useful for rotational IVUS. In a rotational IVUS catheter, a single transducer having a piezo-electric crystal is rapidly rotated (e.g., at approximately 1800 revolutions per minute) while the transducer is intermittently excited with an electrical pulse. The excitation pulse causes the transducer to vibrate, sending out a series of transmit pulses. The transmit pulses are sent at a frequency that allows time for receipt of echo signals. The sequence of transmit pulses interspersed with receipt signals provides the ultrasound data required to reconstruct a complete cross-sectional image of a vessel.

[0016] The general design and construction of rotational IVUS catheters is shown, for example in Yock, U.S. Pat. Nos. 4,794,931, 5,000,185, and 5,313,949; Sieben et al., U.S. Pat. Nos. 5,243,988, and 5,353,798; Crowley et al., U.S. Pat. No. 4,951,677; Pomeranz, U.S. Pat. No. 5,095,911, Griffith et al., U.S. Pat. No. 4,841,977, Maroney et al., U.S. Pat. No. 5,373,849, Born et al., U.S. Pat. No. 5,176,141, Lancee et al., U.S. Pat. No. 5,240,003, Lancee et al., U.S. Pat. No. 5,375,602, Gardineer et al., U.S. Pat. No. 5,373,845, Seward et al., Mayo Clinic Proceedings 71(7):629-635 (1996), Packer et al., Cardiac Conference 833 (1994), "Ultrasound Cardioscopy," Eur. J.C.P.E. 4(2):193 (June 1994), Eberle et al., U.S. Pat. No. 5,453,575, Eberle et al., U.S. Pat. No. 5,368,037, Eberle et al., U.S. Pat. No. 5,183,048, Eberle et al., U.S. Pat. No. 5,167,233, Eberle et al., U.S. Pat. No. 4,917,097, Eberle et al., U.S. Pat. No. 5,135,486, and other references well known in the art relating to intraluminal ultrasound devices and modalities. The catheter will typically have proximal and distal regions, and will include an imaging tip located in the distal region. Such catheters have an ability to obtain echographic images of the area surrounding the imaging tip when located in a region of interest inside the body of a patient. The catheter, and its associated electronic circuitry, will also be capable of defining the position of the catheter axis with respect to each echographic data set obtained in the region of interest.

[0017] Systems and methods of the invention use Golay codes. Use of Golay codes in ultrasound is described for example in U.S. Pat. Nos. 7,535,797; 6,958,042; 6,663,565; 6,638,227; 6,491,631; 6,375,618; 6,350,240; 6,312,384; 6,210,332; 6,186,949; and 6,146,328, the content of each of which is incorporated by reference herein in its entirety.

[0018] Golay complementary sequences are pairs of binary codes, belonging to a bigger family of signals called complementary pairs, which consist of two codes of the same length N whose auto-correlation functions have side-lobes equal in magnitude but opposite in sign. Summing them up results in a composite auto-correlation function with a peak of $2N$ and zero side-lobes. FIG. 1 illustrates the principle of the side-lobe-canceling for a pair of signed of length equal to 8 bits each.

[0019] There are essentially several algorithms for generating Golay pairs. Let the variables a_i and b_i ($i=1, 2, \dots, n$) are the elements of two n -long complementary series equal either '+1' or '-1', [3],

$$A = a_1, a_2, \dots, a_n;$$

$$B = b_1, b_2, \dots, b_n. \quad (1)$$

[0020] The ordered pair (A;B) are Golay sequences of length n if and only if their associated polynomials

$$\begin{aligned} A(x) &= a_1 + a_2x + \dots + a_nx^{n-1}, \\ B(x) &= b_1 + b_2x + \dots + b_nx^{n-1}, \end{aligned} \quad (2)$$

satisfy the identity

$$A(x)A(x^{-1}) + B(x)B(x^{-1}) = 2n \quad (3)$$

in the Laurent polynomial ring $Z[x, x^{-1}]$.

[0021] Let their respectable auto-correlation functions N_A and N_B of the sequences A and B respectively be defined by

$$N_A(j) = \sum_{i \in Z} a_i a_{i+j} \quad (4)$$

$$N_B(j) = \sum_{i \in Z} b_i b_{i+j}$$

where we set $a_k = 0$ if $k \notin (1 \dots n)$. Now condition (3) can be expressed by the sum $N_A + N_B$, and

$$N_A(j) + N_B(j) = \begin{cases} 2N, & j = 0 \\ 0, & j \neq 0 \end{cases} \quad (5)$$

The sum of both autocorrelation function is at $j=0$ and zeroing otherwise.

[0022] The second, recursive method for constructing the Golay's sequences is presented below. Let the variables $a(i)$ and $b(i)$ be the elements ($i=0, 1, 2, \dots, 2^n-1$) of two complementary sequences with elements $+1$ and -1 of length 2^n

$$\begin{aligned} a_0(i) &= \delta(i) \\ b_0(i) &= \delta(i) \end{aligned} \quad (6)$$

$$\begin{aligned} a_n(i) &= a_{n-1}(i) + b_{n-1}(i - 2^{n-1}) \\ b_n(i) &= a_{n-1}(i) - b_{n-1}(i - 2^{n-1}) \end{aligned} \quad (7)$$

where $\delta(i)$ is the Kronecker delta function.

[0023] Equation (7) shows that in each step the new elements of the sequences are produced by concatenation of elements $a_n(i)$ and $b_n(i)$ of the length n .

[0024] Example:

[0025] Let $n=1$, then i takes values 0 and 1.

$$a_1(0) = a_0(0) + b_0(-1) = 1;$$

$$b_1(0) = a_0(0) - b_0(-1) = 1;$$

$$a_1(1) = a_0(1) + b_0(0) = 1;$$

$$b_1(1) = a_0(1) - b_0(0) = -1.$$

[0026] As final results we obtain two complementary sequences of the length 2^n :

$$a_1 = \{1, 1\};$$

$$b_1 = \{1, -1\}.$$

Once these operations are performed recursively for $n=2, 3, 4, \dots$ the following complementary sequences are obtained:

$$a_2 = \{1, 1, 1, -1\};$$

$$b_2 = \{1, 1, -1, 1\}.$$

$$a_3 = \{1, 1, 1, -1, 1, 1, -1, 1\};$$

$$b_3 = \{1, 1, 1, -1, -1, -1, 1, -1\}.$$

$$a_4=\{1, 1, 1, -1, 1, 1, -1, 1, 1, 1, -1, -1, -1, 1, -1\};$$

$$b_4=\{1, 1, 1, -1, 1, 1, -1, 1, -1, -1, 1, 1, 1, -1, 1\}.$$

Similar method of generating the complementary code pairs, differing only in the applied mathematical formalism has been described by Mendieta and al. (Complementary sequence correlations with applications to reflectometry studies, Instrumentation and Development, 3, 6, 1996), the content of which is incorporated by reference herein in its entirety.

[0027] FIGS. 2-3 illustrate systems and methods of the invention. The system includes a processor, and a plurality of beam modules coupled to the processor. Each module includes a receiver for receiving a trigger signal from the processor, a complex programmable logic device programmed with a Golay code, a high voltage switching transmitter, and an ultrasound transducer.

[0028] The processor alternately transmits trigger signals to the beam modules, thereby causing the beam modules to alternately transmit complementary Golay codes. In the first instance of ultrasound transmission, odd transducers of the transducer array transmit ultrasound pulse signals corresponding to first code sequence (Golay code 1 (G1)). Even transducers the transducer array transmit ultrasound pulse signals corresponding to the second code sequence (Golay code 2 (G2)). Transmission of ultrasound pulse signals to a target object, such as a human body, and reception of reflected signals from the target object occur simultaneously. Switching between even transducers and odd transducers of the transducer array with respect to corresponding Golay codes in the first and second ultrasound transmissions reduces the grating lobes. The grating lobe is the peak of a beam pattern generated when the ultrasound signals is supplemented in an unwanted way.

[0029] The processor receives echoes of the complementary codes. The processor performs pulse compression of the echoes that includes weighting the received echoes and summing an odd number of weighted echoes, in which a center echo is given a weighted value of 1.0 and weighted sums of its neighbors constitute complementary echoes of a Golay pair. For example, FIG. 3 shows that three beams are used for generating one composite Golay coded excitation scan line. The figure shows that each transmit signal is paired with a member of a Golay code. The system is set-up such that the pairs alternate (G1, G2, G1, G2, G1, G2 etc). Looking at the top three beams as an example. The first scan line is produced by summing one member of the pair from Golay code 2 and both members of the pair of Golay code 1. A member of the pair of Golay code 2 is the center line with the pairs of Golay code 1 adjacent to the member of the pair of Golay code 2. The weighting for the center beam (Golay code 2) is 1.0, while the weights for the neighboring beams (Golay code pair G1 and G1) are each 0.5. In this manner, the pair from Golay code 1 cancel each other, leaving only center line beam of the member of Golay code 2, thereby removing sidelobes for scanline 1 and eliminating motion artifacts for that scan line.

[0030] The process is then repeated for each scan line and image is assembled from the scan lines. The processor is coupled to a display device and causes the image to be displayed.

INCORPORATION BY REFERENCE

[0031] References and citations to other documents, such as patents, patent applications, patent publications, journals,

books, papers, web contents, have been made throughout this disclosure. All such documents are hereby incorporated herein by reference in their entirety for all purposes.

EQUIVALENTS

[0032] Various modifications of the invention and many further embodiments thereof, in addition to those shown and described herein, will become apparent to those skilled in the art from the full contents of this document, including references to the scientific and patent literature cited herein. The subject matter herein contains important information, exemplification and guidance that can be adapted to the practice of this invention in its various embodiments and equivalents thereof.

What is claimed is:

1. A method for producing an image from a rotational intravascular ultrasound device, the method comprising:
 - alternately transmitting complementary Golay codes to a plurality of transducers in a intravascular ultrasound device;
 - receiving echoes of the complementary codes from the transducers;
 - performing pulse compression of the echoes that comprises weighting the received echoes and summing an odd number of weighted echoes, wherein a center echo is given a weighted value of 1.0 and weighted sums of its neighbors constitute complementary echoes of a Golay pair; and
 - producing an image from the compressed echoes.
2. The method according to claim 1, further comprising displaying the image.
3. The method according to claim 1, wherein the Golay codes are produced by applying a bi-phase window over the Golay codes.
4. The method according to claim 3, wherein the bi-phase window is one of a bi-phase rectangular window, a bi-phase Hamming window, a bi-phase Hanning window and bi-phase Bartlett window.
5. The method according to claim 1, wherein the method further comprises computing convolution of the received echoes of the complementary codes.
6. A system for producing an ultrasound image from a rotational intravascular ultrasound device, the system comprising:
 - a processor; and
 - a plurality of beam modules coupled to the processor, each module comprising:
 - a receiver for receiving a trigger signal from the processor;
 - a complex programmable logic device programmed with a Golay code;
 - a high voltage switching transmitter; and
 - an ultrasound transducer.
7. The system according to claim 6, wherein the processor alternately transmits trigger signals to the beam modules, thereby causing the beam modules to alternately transmit complementary Golay codes.
8. The system according to claim 7, wherein the processor receives echoes of the complementary codes.
9. The system according to claim 8, wherein the processor performs pulse compression of the echoes that comprises weighting the received echoes and summing an odd number of weighted echoes, wherein a center echo is given a weighted

value of 1.0 and weighted sums of its neighbors constitute complementary echoes of a Golay pair.

10. The system according to claim **9**, wherein the processor produces an image from the compressed echoes.

11. The system according to claim **9**, wherein the processor is coupled to a display device and causes the image to be displayed.

12. The system according to claim **11**, wherein the Golay codes are produced by applying a bi-phase window over the Golay codes.

13. The system according to claim **12**, wherein the bi-phase window is one of a bi-phase rectangular window, a bi-phase Hamming window, a bi-phase Hanning window and bi-phase Bartlett window.

14. The system according to claim **11**, wherein the processor causes convolution of the received echoes of the complementary codes.

* * * * *

专利名称(译)	用于从旋转血管内超声装置产生图像的系统和方法		
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[标]申请(专利权)人(译)	火山公司		
申请(专利权)人(译)	火山CORPORATION		
当前申请(专利权)人(译)	火山CORPORATION		
[标]发明人	PARK JINHYOUNG CORL PAUL DOUGLAS		
发明人	PARK, JINHYOUNG CORL, PAUL DOUGLAS		
IPC分类号	A61B8/00 A61B8/08 A61B8/12		
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外部链接	Espacenet USPTO		

摘要(译)

本发明一般涉及用于从旋转血管内超声装置产生图像的系统和方法。

