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(54) **PROVIDING AN ULTRASOUND SPATIAL COMPOUND IMAGE IN AN ULTRASOUND SYSTEM**

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(75) Inventors: **Jeong Sik Kim**, Seoul (KR); **Jae Keun Lee**, Seoul (KR)

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(73) Assignee: **Samsung Medison Co., Ltd.**, Kangwon-do (KR)

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(51) **Int. Cl.**
A61B 8/00 (2006.01)

(52) **U.S. Cl.**
USPC **600/443**

(58) **Field of Classification Search**
USPC 600/443
See application file for complete search history.

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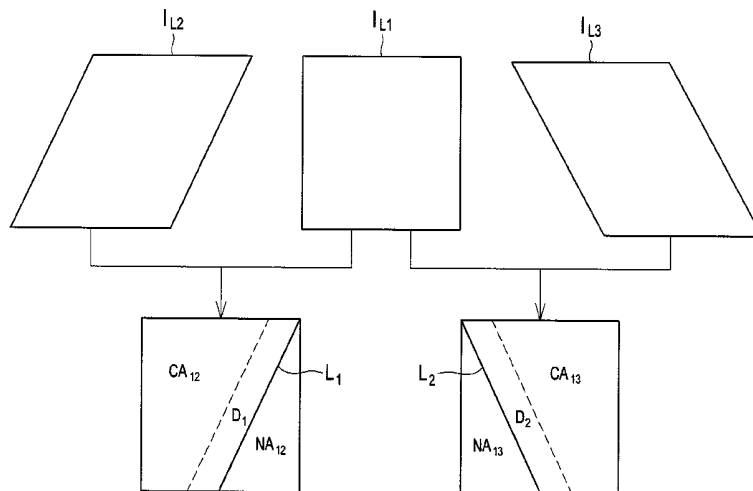
Primary Examiner — Jonathan Cwern

(74) *Attorney, Agent, or Firm* — McDermott Will & Emery LLP

(57) **ABSTRACT**

An ultrasound system includes an ultrasound data acquisition unit and a processing unit. The ultrasound data acquisition unit transmits and receives ultrasound signals to and from a target object based on a plurality of steering angles to output a plurality of ultrasound data for obtaining a plurality of ultrasound images corresponding to the steering angles. The processing unit forms the ultrasound images based on the ultrasound data, decomposes each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component, performs a blending process of removing a seam artifact upon the low and high pass images for each of the ultrasound images, forms a plurality of restoration images by composing the blended low and high pass images, and forms an ultrasound spatial compound image based on the restoration images.

11 Claims, 5 Drawing Sheets



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FIG. 1

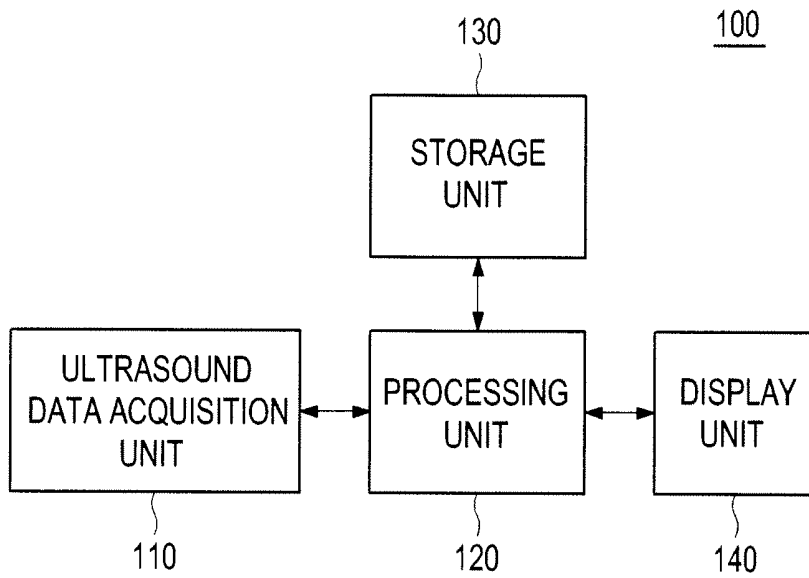


FIG. 2

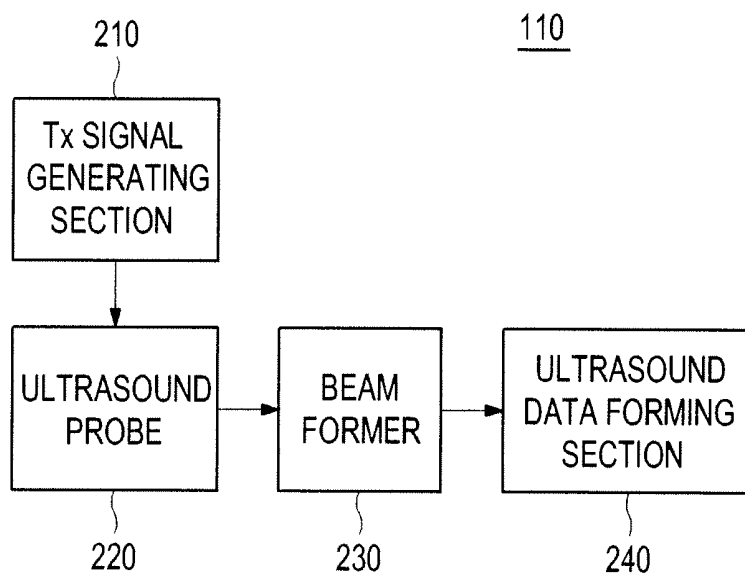


FIG. 3

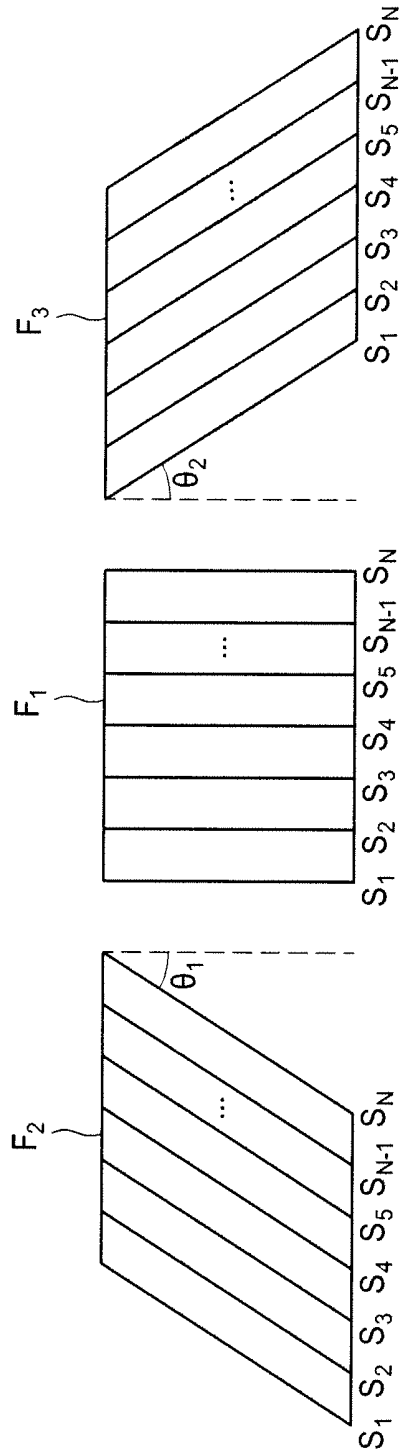


FIG. 4

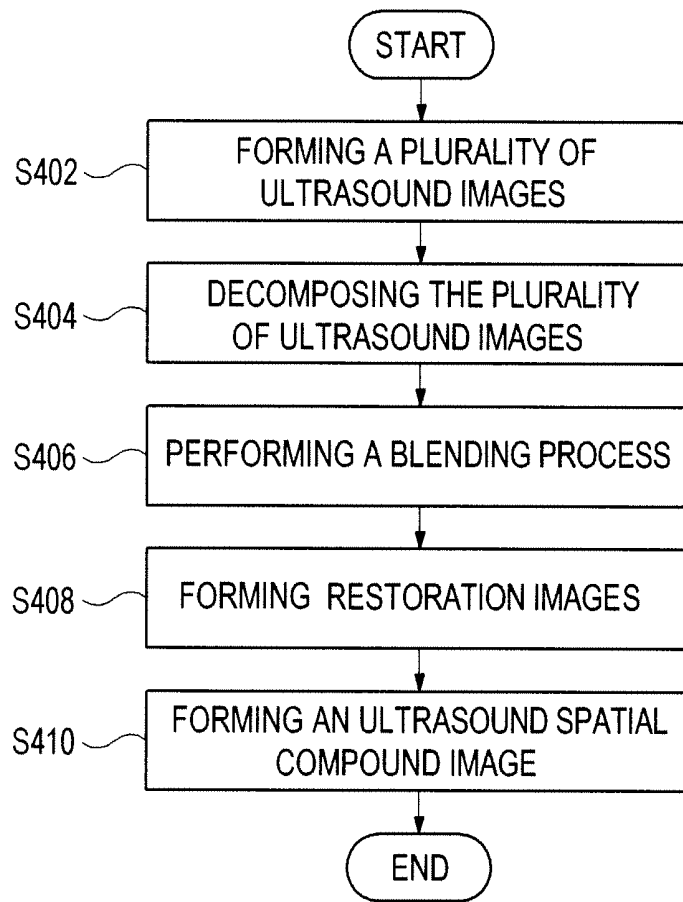


FIG. 5

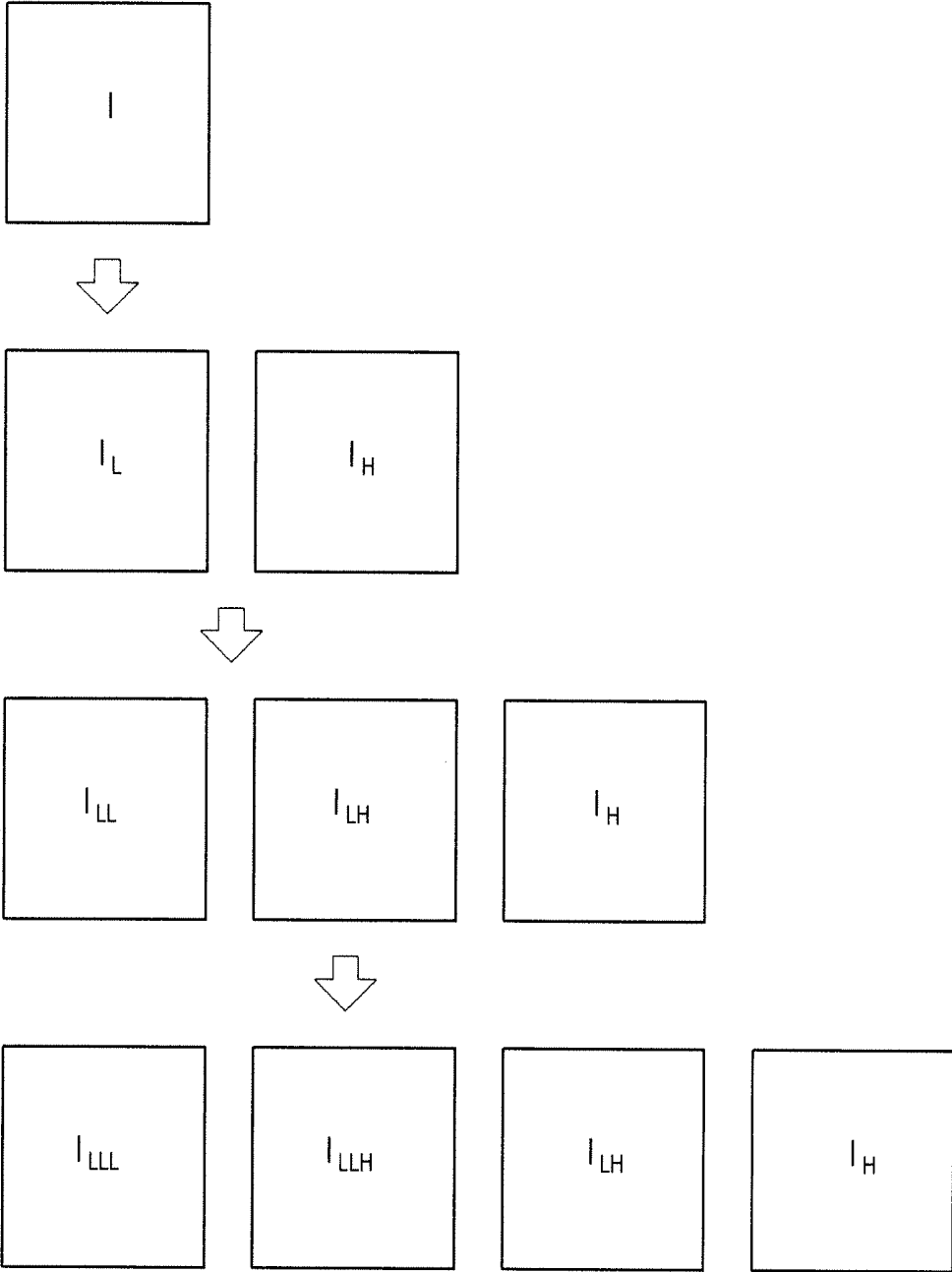
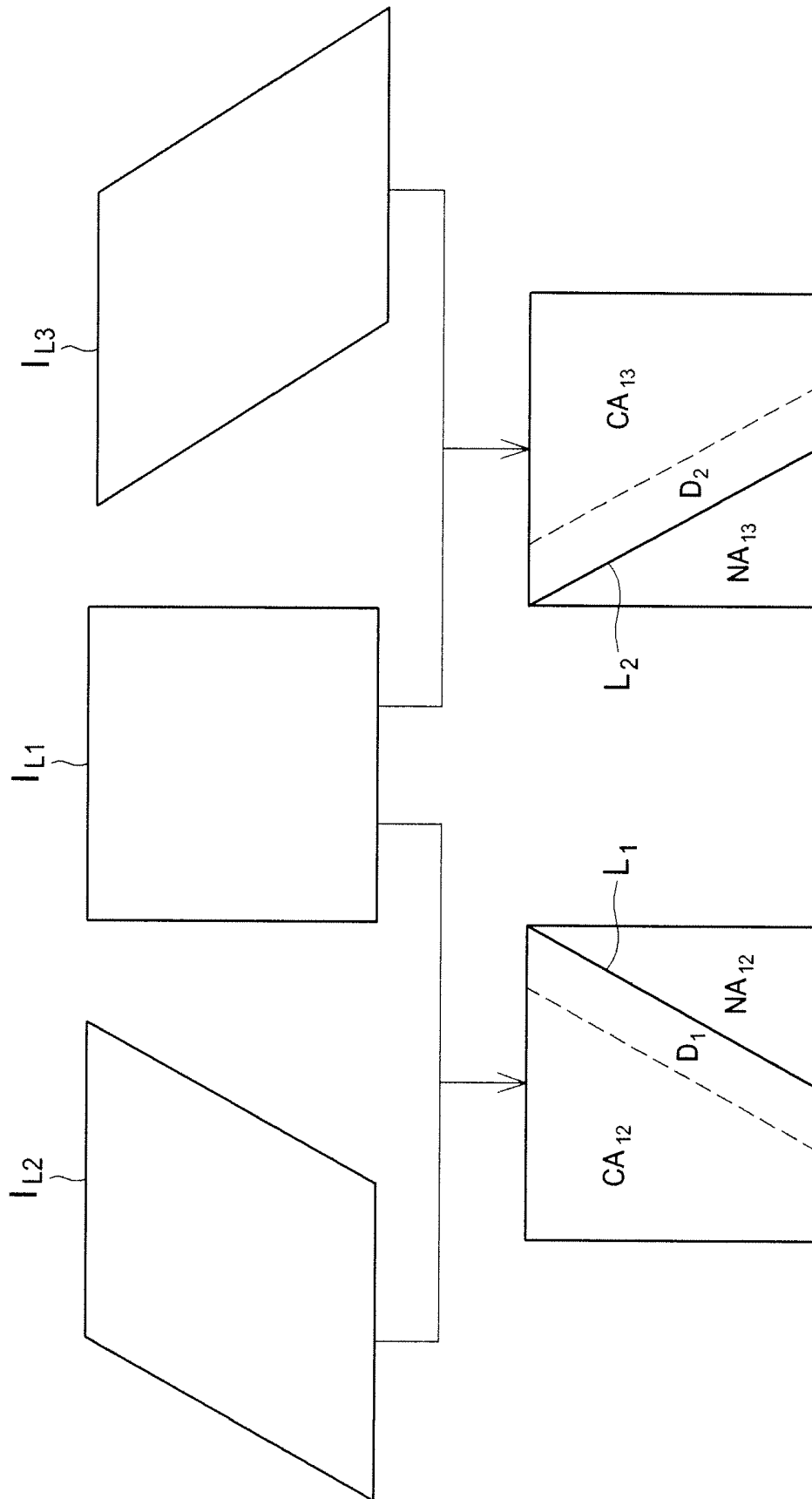


FIG. 6



PROVIDING AN ULTRASOUND SPATIAL COMPOUND IMAGE IN AN ULTRASOUND SYSTEM

CROSS-REFERENCE TO RELATED APPLICATIONS

The present application claims priority from Korean Patent Application No. 10-2009-0111747 filed on Nov. 19, 2009, the entire subject matter of which is incorporated herein by reference.

TECHNICAL FIELD

The present disclosure generally relates to ultrasound systems, and more particularly to providing an ultrasound spatial compound image in an ultrasound system.

BACKGROUND

An ultrasound system has become an important and popular diagnostic tool since it has a wide range of applications. Specifically, due to its non-invasive and non-destructive nature, the ultrasound system has been extensively used in the medical profession. Modern high-performance ultrasound systems and techniques are commonly used to produce two or three-dimensional diagnostic images of internal features of an object (e.g., human organs).

The ultrasound system transmits and receives ultrasound signals to and from a target object to thereby form a 2D (two-dimensional) ultrasound image or a 3D (three-dimensional) ultrasound image. Various techniques have been analyzed to enhance resolution of the ultrasound image. Spatial compounding is one of such techniques.

Spatial compounding is an imaging technique for forming a single compounding image by combining ultrasound images obtained from multiple points and angles. That is, the ultrasound system electronically steers scan-lines at different steering angles to thereby form a plurality of ultrasound images. The ultrasound system may then compound the ultrasound image to form an ultrasound spatial compound image.

Border lines of the ultrasound images are represented on the ultrasound spatial compound image. That is, a seam artifact occurs when the ultrasound spatial compound image is formed by compounding the ultrasound images. Thus, there is a problem in that the quality of the ultrasound spatial compound image becomes poor.

SUMMARY

Embodiments for providing a plurality of slice images in an ultrasound system are disclosed herein. In one embodiment, by way of non-limiting example, an ultrasound system comprises: an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object based on a plurality of steering angles to thereby output a plurality of ultrasound data for obtaining a plurality of ultrasound images corresponding to the plurality of steering angles; and a processing unit in communication with the ultrasound data acquisition unit, the processing unit being configured to form the plurality of ultrasound images based on the plurality of ultrasound data, decompose each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component, perform a blending process for removing a seam artifact upon the low pass image and the high pass image for each of the ultrasound images, form a plurality of

restoration images by composing the blended low pass image and the high pass image, and form an ultrasound spatial compound image based on the plurality of restoration images.

In another embodiment, there is provided a method of providing an ultrasound spatial compound image comprising: a) forming a plurality of ultrasound images based on a plurality of ultrasound data, wherein the plurality of ultrasound images correspond to a plurality of steering angles; b) decomposing each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component; c) performing a blending process of removing a seam artifact upon the low pass image and the high pass image for each of the ultrasound images; d) forming a plurality of restoration images by composing the blended low pass image and the high pass image; and e) forming an ultrasound spatial compound image based on the plurality of restoration images.

In yet another embodiment, there is provided a computer readable medium comprising computer executable instructions configured to perform the following acts: a) forming a plurality of ultrasound images based on a plurality of ultrasound data, wherein the plurality of ultrasound images correspond to a plurality of steering angles; b) decomposing each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component; c) performing a blending process of removing a seam artifact upon the low pass image and the high pass image for each of the ultrasound images; d) forming a plurality of restoration images by composing the blended low pass image and the high pass image; and e) forming an ultrasound spatial compound image based on the plurality of restoration images.

The Summary is provided to introduce a selection of concepts in a simplified form that are further described below in the Detailed Description. This Summary is not intended to identify key or essential features of the claimed subject matter, nor is it intended to be used in determining the scope of the claimed subject matter.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram showing an illustrative embodiment of an ultrasound system.

FIG. 2 is a block diagram showing an illustrative embodiment of an ultrasound data acquisition unit.

FIG. 3 is a schematic diagram showing an example of a plurality of steering angles and a plurality of ultrasound images corresponding to the plurality of steering angles.

FIG. 4 is a flow chart showing a process of forming an ultrasound spatial compound image.

FIG. 5 is a schematic diagram showing an example of decomposing an ultrasound image into an N-level low pass image and an N-level high pass image.

FIG. 6 is a schematic diagram showing an example of a plurality of low pass images corresponding to the plurality of ultrasound images, boundary areas and blending areas.

DETAILED DESCRIPTION

A detailed description may be provided with reference to the accompanying drawings. One of ordinary skill in the art may realize that the following description is illustrative only and is not in any way limiting. Other embodiments of the present invention may readily suggest themselves to such skilled persons having the benefit of this disclosure.

Referring to FIG. 1, an ultrasound system 100 in accordance with an illustrative embodiment is shown. As depicted

therein, the ultrasound system **100** may include an ultrasound data acquisition unit **110**. The ultrasound data acquisition unit **110** may be configured to transmit and receive ultrasound signals to and from a target object to thereby output ultrasound data.

FIG. **2** is a block diagram showing an illustrative embodiment of the ultrasound data acquisition unit **110**. Referring to FIG. **2**, the ultrasound data acquisition unit **110** may include a transmit (Tx) signal generating section **210**, an ultrasound probe **220**, a beam former **230** and an ultrasound data forming section **240**.

The Tx signal generating section **210** may be configured to generate Tx signals. In one embodiment, the Tx signal generating section **210** may generate a plurality of Tx signals with different Tx patterns such that scan-lines are steered at different steering angles. Thus, a plurality of ultrasound images corresponding to the respective steering angles may be obtained. The ultrasound image may include a brightness mode (B mode) image. However, it should be noted herein that the ultrasound image may not be limited thereto.

FIG. **3** is a schematic diagram showing an example of a plurality of steering angles and the plurality of ultrasound images corresponding to the plurality of steering angles. Referring to FIG. **3**, the Tx signal generating section **210**, as shown in FIG. **2**, may generate first Tx signals for obtaining a first ultrasound image F_1 , where the scan-lines S_1 to S_N are not steered, second Tx signals for obtaining a second ultrasound image F_2 , where the scan-lines S_1 to S_N are electronically steered at a steering angle θ_1 , and third Tx signals for obtaining a third ultrasound image F_3 , where the scan-lines S_1 to S_N are electronically steered at a steering angle θ_2 .

Referring back to FIG. **2**, the ultrasound probe **220** may include a plurality of elements (not shown) for reciprocally converting between ultrasound signals and electrical signals. The ultrasound probe **220** may be configured to transmit ultrasound signals into the target object in response to the Tx signals provided from the Tx signal generating section **210**. The ultrasound probe **220** may further receive ultrasound echo signals reflected from the target object to thereby form received signals. The received signals may be analog signals.

In one embodiment, the ultrasound probe **220** may transmit ultrasound signals to the target object in response to the first Tx signals provided from the Tx signal generation section **210**. The ultrasound probe **220** may further receive ultrasound echo signals reflected from the target object to thereby form first received signals. The ultrasound probe **220** may further transmit ultrasound signals to the target object in response to the second Tx signals provided from the Tx signal generation section **210**. The ultrasound probe **220** may receive ultrasound echo signals reflected from the target object to thereby form second received signals. The ultrasound probe **220** may further transmit ultrasound signals to the target object in response to the third Tx signals provided from the Tx signal generation section **210**. The ultrasound probe **220** may further receive ultrasound echo signals reflected from the target object to thereby form third received signals.

The beam former **230** may be configured to convert the received signals into digital signals. The beam former **230** may further apply delays to the digital signals in consideration of focal points and distance between the elements to thereby form digital receive-focused signals.

In one embodiment, the beam former **230** may convert the first received signals provided from the ultrasound probe **220** into first digital signals. The beam former **230** may further apply delays to the first digital signals in consideration of focal points and distance between the elements to thereby form first digital receive-focused signals. The beam former

230 may further convert the second received signals provided from the ultrasound probe **220** into second digital signals. The beam former **230** may further apply delays to the second digital signals in consideration of focal points and distance between the elements to thereby form second digital receive-focused signals. The beam former **230** may further convert the third received signals provided from the ultrasound probe **220** into third digital signals. The beam former **230** may further apply delays to the third digital signals in consideration of focal points and distance between the elements to thereby form third digital receive-focused signals.

The ultrasound data forming section **240** may be configured to form ultrasound data based on the digital receive-focused signals provided from the beam former **230**. The ultrasound data forming section **240** may further perform signal processing (e.g., gain control, etc) upon the digital receive-focused signals.

In one embodiment, the ultrasound data forming section **240** may form first ultrasound data corresponding to the first digital receive-focused signals provided from the beam former **230**. The ultrasound data forming section **240** may further form second ultrasound data corresponding to the second digital receive-focused signals provided from the beam former **230**. The ultrasound data forming section **240** may further form third ultrasound data corresponding to the third digital receive-focused signals provided from the beam former **230**.

Referring back to FIG. **1**, the ultrasound system **100** may further include a processing unit **120** in communication with the ultrasound data acquisition unit **110**.

FIG. **4** is a flow chart showing a process of forming an ultrasound spatial compound image. The processing unit **120**, as shown in FIG. **1**, may be configured to form the plurality of ultrasound images based on the plurality of ultrasound data provided from the ultrasound data acquisition unit **110**, at step **S402**.

In one embodiment, the processing unit **120** may form the first ultrasound image F_1 as shown in FIG. **3** based on the first ultrasound data provided from the ultrasound data acquisition unit **110**. The processing unit **120** may further form the second ultrasound image F_2 as shown in FIG. **3** based on the second ultrasound data provided from the ultrasound data acquisition unit **110**. The processing unit **120** may further form a third ultrasound image F_3 as shown in FIG. **3** based on the third ultrasound data provided from the ultrasound data acquisition unit **110**.

The processing unit **120** may be configured to decompose each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component, at step **S404**.

The processing unit **120** may decompose each of the ultrasound images into the low pass image and the high pass image by using a low pass filter as following equation.

$$I_L = I * G, I_H = I - I_L \quad (1)$$

I represents the ultrasound image, I_L represents the low pass image, I_H represents the high pass image, $*$ represents convolution, and G represents the low pass filter. The low pass filter may include two-dimensional Gaussian filter. However, it should be noted herein that the low pass filter may be not limited thereto.

FIG. **5** is a schematic diagram showing an example of decomposing an ultrasound image into an N ($N \geq 2$)-level low pass image and an N -level high pass image. In another

embodiment, the processing unit **120** may decompose each of the ultrasound images I into a first-level low pass image I_L and a first-level high pass image I_H by using a first low pass filter. The processing unit **120** may further decompose the first-level low pass image I_L into a second-level low pass image I_{LL} and a second-level high pass image I_{LH} by using a second low pass filter. A cutoff frequency of the second low pass filter is lower than that of the first low pass filter. The processing unit **120** may further decompose the second-level low pass image I_{LL} into a third-level low pass image I_{LLL} and a third-level high pass image I_{LLH} by using a third low pass filter. The cutoff frequency of the third low pass filter is lower than that of the second low pass filter.

Referring back to FIG. 4, the processing unit **120** may be configured to perform a blending process upon the decomposed low pass image and high pass image for each of the ultrasound, at step S406. The blending process may include an alpha-blending process. However, it should be noted herein that the blending process may be not limited thereto.

More particularly, the processing unit **120** may detect boundary lines of the low pass images corresponding to the plurality of ultrasound images. The processing unit **120** may detect boundary lines of the high pass images corresponding to the plurality of ultrasound images. The processing unit **120** may further set blending areas having a predetermined size on the low pass images and the high pass images based on the detected boundary lines. The processing unit **120** may further perform the blending process upon the low pass images and the high pass images based on the blending areas.

Referring to FIG. 6, the processing unit **120** may detect a boundary line L_1 of the low pass image I_{L1} corresponding to the first ultrasound image F_1 as shown in FIG. 3 and the low pass image I_{L2} corresponding to the second ultrasound image F_2 as shown in FIG. 3. The processing unit **120** may further set a blending area D_1 having the predetermined size on the low pass image I_{L1} and the low pass image I_{L2} based on the boundary line L_1 . The processing unit **120** may further perform the blending process upon the low pass image I_{L1} and the low pass image I_{L2} for applying a first weight value a_1 to pixels of the blending area D_1 adjacent to an area NA_{12} and applying a second weight value ($a_2=1-a_1$) to pixels of the blending area D_1 adjacent to an area CA_{12} . The area NA_{12} may be a non-overlapped area of the low pass image I_{L1} and the low pass image I_{L2} . In addition, the area CA_{12} may be an overlapped area of the low pass image I_{L1} and the low pass image I_{L2} . That is, the weight value, which may be applied to the blending area D_1 , may vary from a_1 to a_2 , as going from a boundary of the area NA_{12} and the blending area D_1 and a boundary of the area CA_{12} and the blending area D_1 . As shown in FIG. 6, the processing unit **120** may further detect a boundary line L_2 of the low pass image I_{L1} corresponding to the first ultrasound image F_1 as shown in FIG. 3 and the low pass image I_{L3} corresponding to the third ultrasound image F_3 as shown in FIG. 3. The processing unit **120** may further set a blending area D_2 having the predetermined size on the low pass image I_{L1} and the low pass image I_{L3} based on the boundary line L_2 . The processing unit **120** may further perform the blending process upon the low pass image I_{L1} and the low pass image I_{L3} for applying the first weight value a_1 to pixels of the blending area D_2 adjacent to an area NA_{13} and applying the second weight value ($a_2=1-a_1$) to pixels of the blending area D_2 adjacent to an area CA_{13} . The area NA_{13} may be a non-overlapped area of the low pass image I_{L1} and the low pass image I_{L3} . Further, the area CA_{13} may be an overlapped area of the low pass image I_{L1} and the low pass image I_{L3} . The

processing unit **120** may perform the blending process upon the high pass images corresponding to the ultrasound images F_1 to F_3 as mentioned above.

The processing unit **120** may be configured to compose the blended low pass images and high pass images to thereby form a plurality of restoration images corresponding to the plurality of ultrasound images at step S408 in FIG. 4.

In one embodiment, the processing unit **120** may compose the blended low pass image and high pass image corresponding to the first ultrasound image F_1 as shown in FIG. 3 to thereby form a first restoration image corresponding to the first ultrasound image F_1 . The processing unit **120** may further compose the blended low pass image and high pass image corresponding to the second ultrasound image F_2 as shown in FIG. 3 to thereby form a second restoration image corresponding to the second ultrasound image F_2 . The processing unit **120** may further compose the blended low pass image and high pass image corresponding to the third ultrasound image F_3 as shown in FIG. 3 to thereby form a third restoration image corresponding to the third ultrasound image F_3 .

The processing unit **120** may be configured to perform spatial compound imaging upon the plurality of restoration images to thereby form an ultrasound spatial compound image at step S410. The methods of performing the spatial compound imaging are well known in the art. Thus, they have not been described in detail so as not to unnecessarily obscure the present invention. In one embodiment, the processing unit **120** may perform the spatial compound imaging upon the first restoration image, the second restoration image and the third restoration image to thereby form the ultrasound spatial compound image.

Referring back to FIG. 1, the ultrasound system may further include a storage unit **130**. The storage unit **130** may store the ultrasound data acquired by the ultrasound data acquisition unit **110**. The storage unit **130** may further store the plurality of ultrasound images formed by the processing unit **120**.

The ultrasound system may further include a display unit **140**. The display unit **140** may display the ultrasound spatial compound image formed by the processing unit **120**. The display unit **140** may further display the plurality of ultrasound images formed by the processing unit **120**.

In another embodiment, the present invention may provide a computer readable medium comprising computer executable instructions configured to perform following acts: a) acquiring a plurality of ultrasound data for obtaining a plurality of ultrasound images corresponding to a plurality of steering angles; b) forming the plurality of ultrasound image based on the plurality of ultrasound data; c) decomposing each of the plurality of ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component; d) performing a blending process for removing a seam artifact upon the low pass image and the high pass image for each of the plurality of ultrasound images; and e) form an ultrasound spatial compound image based on the blended low pass image and high pass image. The computer readable medium may comprise a floppy disk, a hard disk, a memory, a compact disk, a digital video disk, etc.

Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the spirit and scope of the principles of this disclosure. More particularly, numerous variations and modifications are possible in the component parts and/or arrange-

ments of the subject combination arrangement within the scope of the disclosure, the drawings and the appended claims. In addition to variations and modifications in the component parts and/or arrangements, alternative uses will also be apparent to those skilled in the art.

What is claimed is:

1. An ultrasound system, comprising:

an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object based on a plurality of steering angles to thereby output a plurality of ultrasound data for obtaining a plurality of ultrasound images corresponding to the steering angles; and

a processing unit in communication with the ultrasound data acquisition unit, the processing unit being configured to form the ultrasound images based on the ultrasound data, decompose each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component, perform a blending process for removing a seam artifact upon the low pass image and the high pass image corresponding to each of the ultrasound images, form a plurality of restoration images by composing the blending-processed low and high pass images corresponding to each of the ultrasound images, and form an ultrasound spatial compound image based on the restoration images,

wherein the processing unit is configured to perform the blending process upon the low pass image or the high pass image of one of the plurality of ultrasound images with the low pass image or the high pass image, respectively, of another one of the plurality of ultrasound images.

2. The ultrasound system of claim 1, wherein the processing unit is configured to decompose each of the ultrasound images into the low pass image and the high pass image by using a low pass filter.

3. The ultrasound system of claim 1, wherein the processing unit is configured to:

detect first boundary lines of the low pass images and second boundary lines of the high pass images; set first blending area having a predetermined size on the low pass images based on the first boundary lines and second blending areas having the predetermined size on the high pass images based on the second boundary lines; and

perform the blending process upon the low pass images and the high pass images based on the first blending areas and the second blending areas.

4. The ultrasound system of claim 3, wherein the processing unit is configured to perform the blending process by applying a first weight value to pixels of the first blending areas adjacent to a non-overlapped area of the low pass images, applying a second weight value to pixels of the first blending areas adjacent to an overlapped area of the low pass images, applying the first weight value to pixels of the second blending areas adjacent to a non-overlapped area of the high pass images, and applying the second weight value to pixels of the second blending areas adjacent to an overlapped area of the high pass images.

5. The ultrasound system of claim 1, wherein the blending process comprises an alpha blending process.

6. A method of providing an ultrasound spatial compound image, comprising:

a) forming a plurality of ultrasound images based on a plurality of ultrasound data, wherein the ultrasound images correspond to a plurality of steering angles;

b) decomposing each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component;

c) performing a blending process for removing a seam artifact upon the low pass image and the high pass image corresponding to each of the ultrasound images;

d) forming a plurality of restoration images by composing the blending-processed low and high pass images corresponding to each of the ultrasound images; and

e) forming an ultrasound spatial compound image based on the restoration images,

wherein the blending process is performed upon the low pass image or the high pass image of one of the plurality of ultrasound images with the low pass image or the high pass image, respectively, of another one of the plurality of ultrasound images.

7. The method of claim 6, wherein the step b) comprises: decomposing each of the ultrasound images by using a low pass filter.

8. The method of claim 6, wherein the step c) comprises:

c1) detecting first boundary lines of the low pass images and second boundary lines of the high pass images;

c2) setting first blending areas on the low pass images based on the first boundary lines and second blending areas on the high pass images based on the second boundary lines; and

c3) performing the blending process upon the low pass images and the high pass images based on the first blending areas and the second blending areas.

9. The method of claim 8, wherein the step c3) comprises: applying a first weight value to pixels of the first blending areas adjacent to a non-overlapped area of the low pass images;

applying a second weight value to pixels of the first blending areas adjacent to an overlapped area of the low pass images;

applying the first weight value to pixels of the second blending areas adjacent to a non-overlapped area of the high pass images; and

applying the second weight value to pixels of the second blending areas adjacent to an overlapped area of the high pass images.

10. The method of claim 6, wherein the blending process comprises an alpha blending process.

11. A non-transitory computer readable medium comprising computer executable instructions for performing following steps of:

a) forming a plurality of ultrasound images based on a plurality of ultrasound data, wherein the ultrasound images corresponding to a plurality of steering angles;

b) decomposing each of the ultrasound images into a low pass image having a low frequency component and a high pass image having a high frequency component;

c) performing a blending process for removing a seam artifact upon the low pass image and the high pass image corresponding to each of the ultrasound images;

d) forming a plurality of restoration images by composing the blending-processed low and high pass images; and

e) forming an ultrasound spatial compound image based on the restoration images,

wherein the blending process is performed upon the low pass image or the high pass image of one of the plurality of ultrasound images with the low pass image or the high pass image, respectively, of another one of the plurality of ultrasound images.

专利名称(译)	在超声系统中提供超声空间复合图像		
公开(公告)号	US8727990	公开(公告)日	2014-05-20
申请号	US12/882902	申请日	2010-09-15
[标]申请(专利权)人(译)	金桢SIK 李宰瑾		
申请(专利权)人(译)	金桢SIK 李宰瑾		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD.		
[标]发明人	KIM JEONG SIK LEE JAE KEUN		
发明人	KIM, JEONG SIK LEE, JAE KEUN		
IPC分类号	A61B8/00		
CPC分类号	G01S15/8995 G06T2207/20221 G06T5/50		
代理机构(译)	MCDERMOTT WILL & EMERY LLP		
优先权	1020090111747 2009-11-19 KR		
其他公开文献	US20110118604A1		
外部链接	Espacenet USPTO		

摘要(译)

超声系统包括超声数据获取单元和处理单元。超声数据获取单元基于多个转向角向目标对象发送超声信号并从目标对象接收超声信号，以输出多个超声数据，以获得与转向角对应的多个超声图像。处理单元基于超声数据形成超声图像，将每个超声图像分解为具有低频分量的低通图像和具有高频分量的高通图像，执行去除接缝伪影的混合处理。每个超声图像的低通和高通图像通过合成混合的低通和高通图像形成多个恢复图像，并基于恢复图像形成超声空间复合图像。

