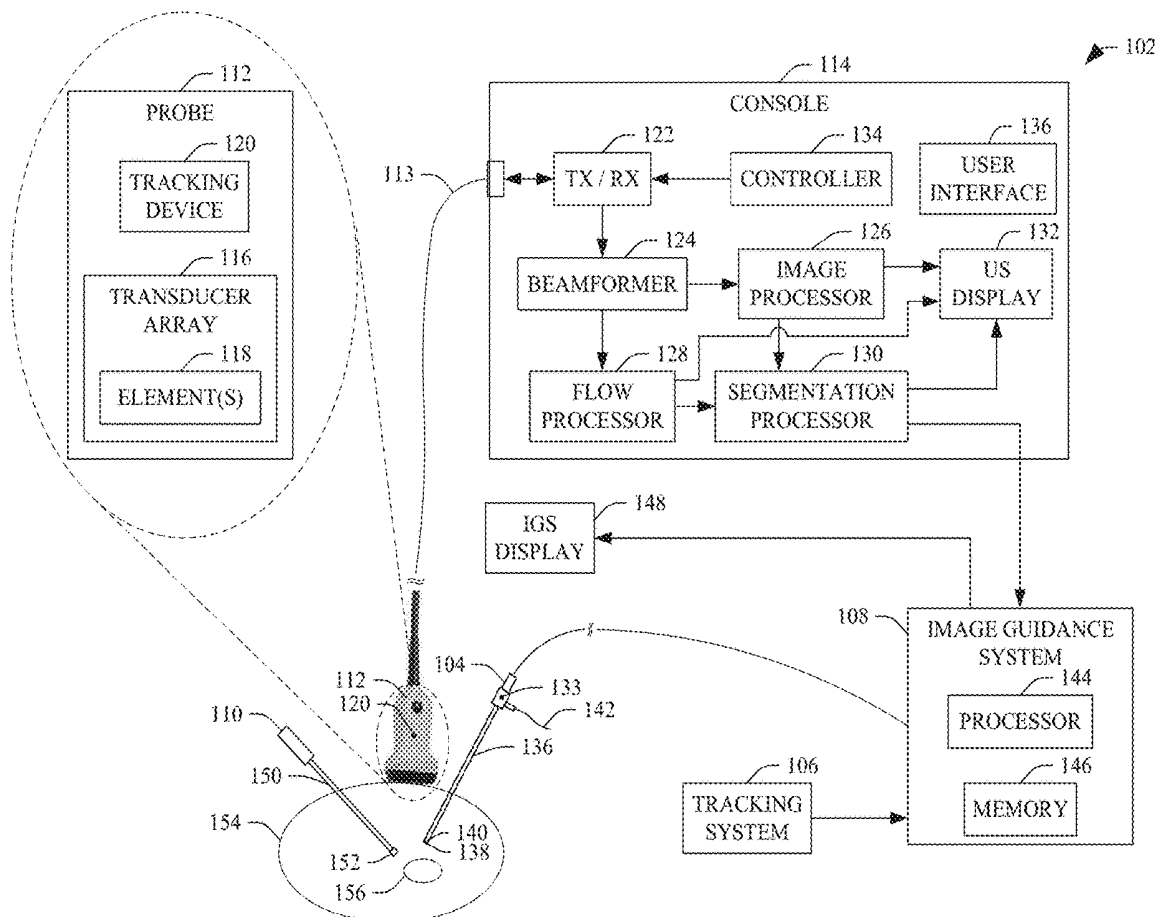




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GRAN et al.(54) **COMBINATION ULTRASOUND / OPTICAL
IMAGE FOR AN IMAGE-GUIDED
PROCEDURE**(71) Applicant: **B-K Medical Aps**, Herlev (DK)(72) Inventors: **Fredrik GRAN**, Limhamn (SE);
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2034/2065 (2016.02); **A61B 1/06** (2013.01)(57) **ABSTRACT**

A system includes an image guidance system with a memory with computer executable instruction, a processor configured to execute the computer executable instructions, and a display. The computer executable instructions cause the processor to: receive a three-dimensional model of vasculature from an ultrasound imaging system, receive a real-time optical feed of an interior of a cavity from an optical camera-based guidance system, receive a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system, receive a second spatial location of the optical camera-based guidance system, and overlay the optical feed with the three-dimensional model based on the first and second tracking signals. The display is configured to visually present the optical feed with the three-dimensional model overlaid thereover.



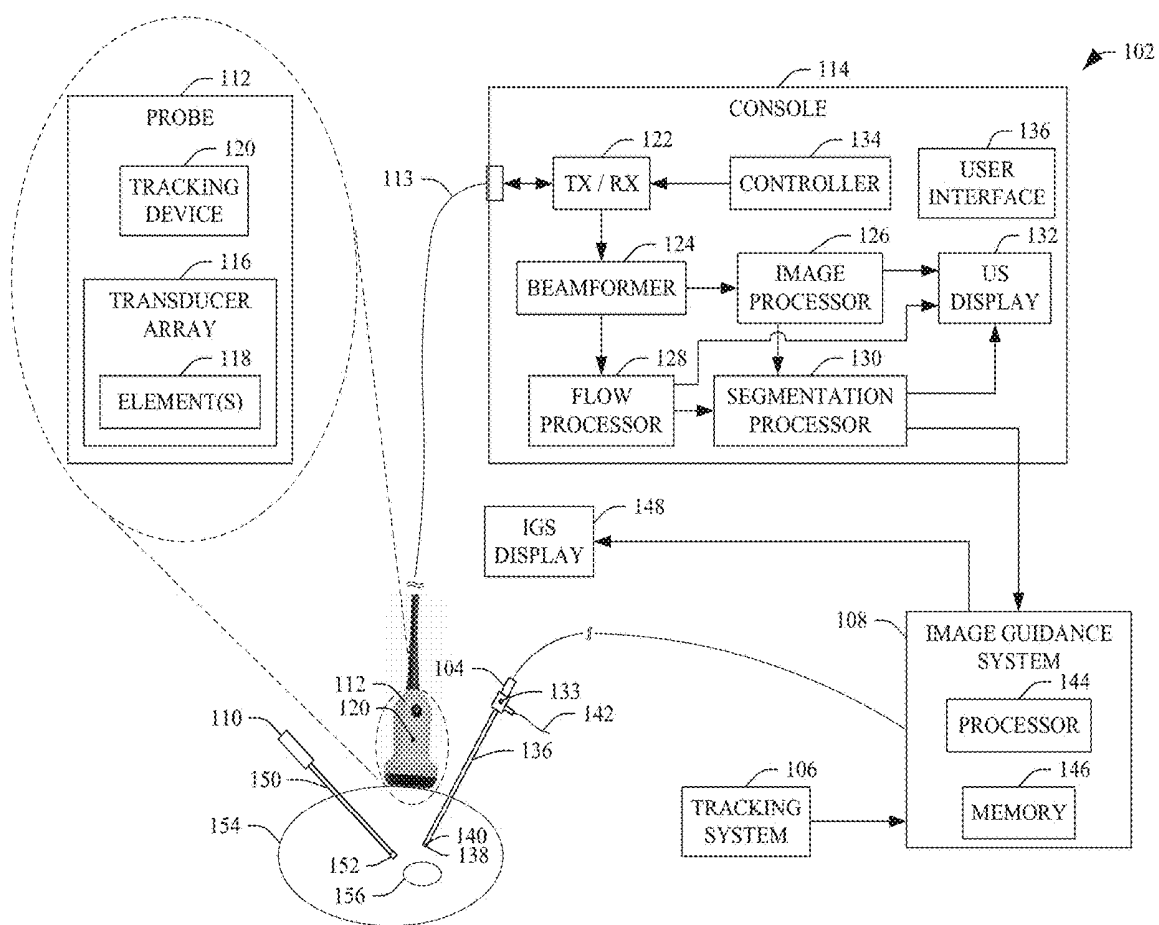


FIGURE 1

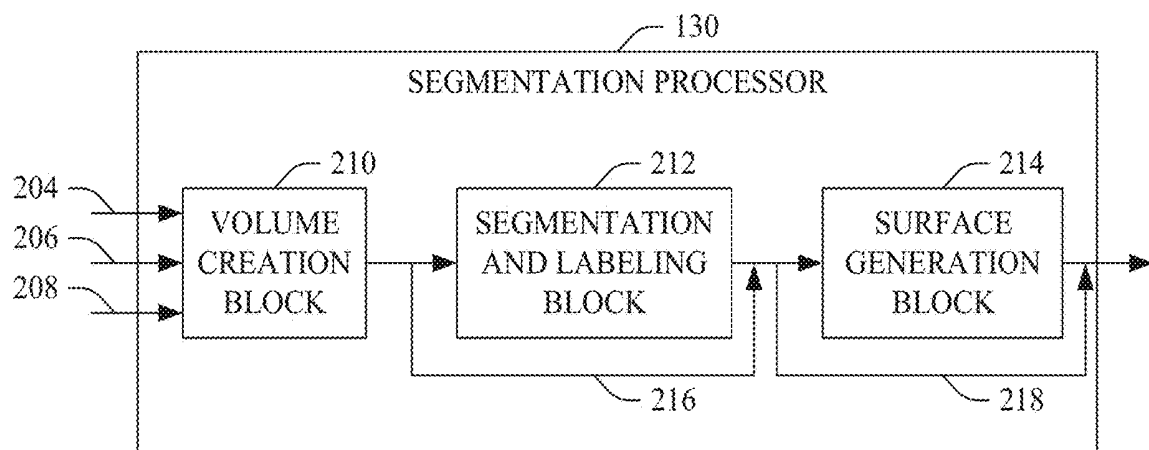


FIGURE 2

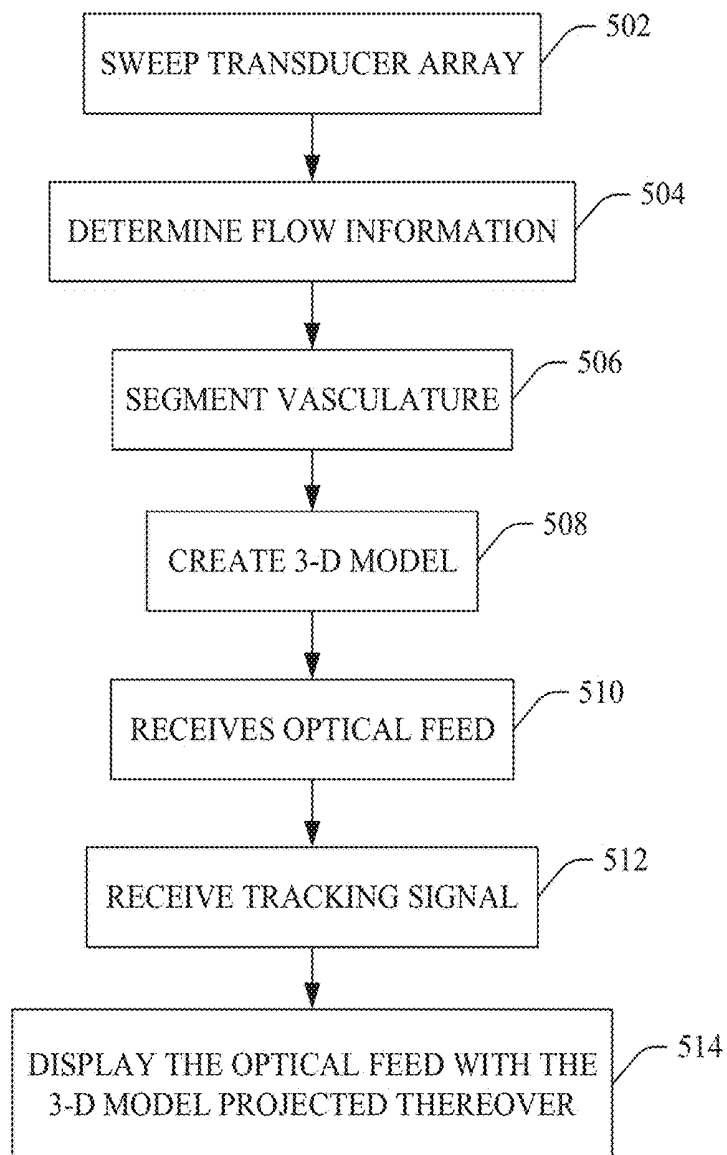


FIGURE 5

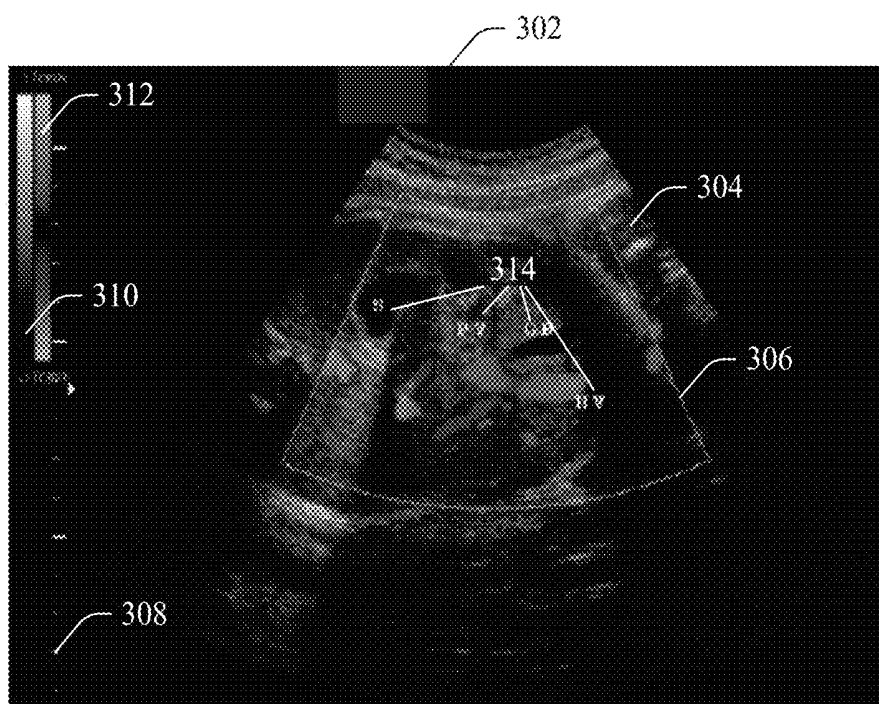


FIGURE 3

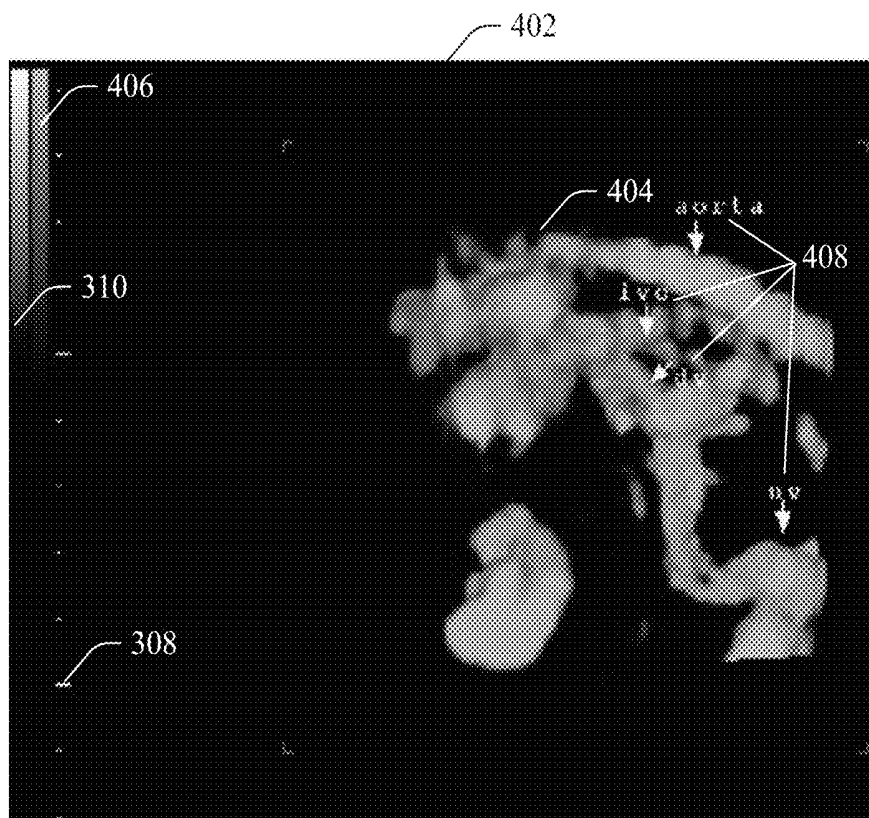


FIGURE 4

COMBINATION ULTRASOUND / OPTICAL IMAGE FOR AN IMAGE-GUIDED PROCEDURE

TECHNICAL FIELD

[0001] The following generally relates to image guidance and more particularly to a combination ultrasound/optical image for an image guided procedure.

BACKGROUND

[0002] An image-guided procedure includes a procedure within a cavity of an object where the clinician cannot see into the cavity through the object and instead uses a displayed image of the inside of the cavity as a guide to maneuver and employ an instrument in the cavity. In one example, this includes a surgeon operating an optical camera-based guidance system while performing the procedure. The procedure could be a resection, cauterization, cryotherapy, biopsy, ablation, etc. The optical camera-based guidance system can be a laparoscope in laparoscopy, a microscope in neuro surgery, an optical interface of a surgical robot, etc.

[0003] With such a procedure, the surgeon can only see the surface of the tissue to be treated and not the tissue below the surface of the tissue to be treated. In order to avoid inadvertently damaging other tissue, e.g., cutting a vessel just below the surface of the tissue being treated, the surgeon has relied on a pre-operative image (e.g., computed tomography (CT) or magnetic resonance (MRI)) and/or a real-time image (e.g., ultrasound (US)). Unfortunately, a pre-operative image is limited in that it does not represent a current state of the tissue, which may have shifted or deformed since the imaging, and it is difficult to concurrently treat the tissue while scanning with the ultrasound probe.

SUMMARY

[0004] Aspects of the application address the above matters, and others.

[0005] In one aspect, a system includes an image guidance system with a memory with computer executable instruction, a processor configured to execute the computer executable instructions, and a display. The computer executable instructions cause the processor to: receive a three-dimensional model of vasculature from an ultrasound imaging system, receive a real-time optical feed of an interior of a cavity from an optical camera-based guidance system, receive a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system, receive a second spatial location of the optical camera-based guidance system, and overlay the optical feed with the three-dimensional model based on the first and second tracking signals. The display is configured to visually present the optical feed with the three-dimensional model overlaid thereover.

[0006] In another aspect, a method includes receiving a three-dimensional model of vasculature from an ultrasound imaging system. The method further includes receiving a real-time optical feed of an interior of a cavity from an optical camera-based guidance system. The method further includes receiving a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system. The method further includes receiving a second spatial location of the optical camera-based guidance system. The

method further includes overlaying the optical feed with the three-dimensional model based on the first and second tracking signals. The method further includes displaying the optical feed with the three-dimensional model overlaid thereover.

[0007] In another aspect, a computer readable medium is encoded with computer executable instructions. The computer executable instructions, when executed by a processor of a computer, cause the processor to: receive a three-dimensional model of vasculature from an ultrasound imaging system, receive a real-time optical feed of an interior of a cavity from an optical camera-based guidance system, receive a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system, receive a second spatial location of the optical camera-based guidance system, overlay the optical feed with the three-dimensional model based on the first and second tracking signals, and display the optical feed with the three-dimensional model overlaid thereover.

[0008] Those skilled in the art will recognize still other aspects of the present application upon reading and understanding the attached description.

BRIEF DESCRIPTION OF THE DRAWINGS

[0009] The application is illustrated by way of example and not limited by the figures of the accompanying drawings, in which like references indicate similar elements and in which:

[0010] FIG. 1 schematically illustrates an example ultrasound system with a color flow mapping processor;

[0011] FIG. 2 schematically illustrates a non-limiting examples of the segmentation processor of the ultrasound system.

[0012] FIG. 3 shows an example color flow image;

[0013] FIG. 4 shows an example Power-Doppler image; and

[0014] FIG. 5 illustrates an example method in accordance with an embodiment herein.

DETAILED DESCRIPTION

[0015] The following general describes an approach to visualizing vasculature during an image-guided procedure of tissue. In one instance, this includes sweeping an array of an ultrasound transducer over the tissue while acquiring at least flow data (e.g., color flow mode (CFM), Doppler, etc.), creating a three-dimensional (3-D) volume with the scanned image plains, segmenting vasculature from the 3-D volume based on the flow data to create a 3-D model of the vasculature, and displaying the 3-D model overlaid over an optical image of an optical camera-based guidance system while performing the procedure. The 3-D model, in one instance, provides image-guidance on location of vasculature so that the surgeon can avoid/minimize damaging the vasculature.

[0016] FIG. 1 illustrates a system **100** including ultrasound imaging system **102**, an optical camera-based guidance system **104**, a tracking system **106**, an image-guidance system **108**, and at least one instrument **110** configured for resection, cauterization, cryotherapy, biopsy, ablation, etc.

[0017] The ultrasound imaging system **102** includes a probe **112** and an ultrasound console **114**, which interface through suitable complementary hardware (e.g., a cable **113**, as shown) and/or wireless interfaces. The probe **112** includes

a transducer array **116** with one or more transducer elements **118**. The transducer array **116** can be one- or two-dimensional, linear, curved, and/or otherwise shaped, fully populated, sparse and/or a combination thereof, etc. In one instance, the transducer array **116** is configured to mechanically and/or electrically rotate to capture 3-D data.

[0018] The one or more transducer elements **118** are configured to convert an excitation electrical signal to an ultrasound pressure field. The one or more transducer elements **118** are also configured to convert a received ultrasound pressure field (an echo) into an electrical (e.g., analog radio frequency, RF) signal. The ultrasound pressure field, in one instance, is produced in response to a transmitted ultrasound pressure field interacting with structure, such as blood cells flowing in a portion of a vessel and/or other tissue, and/or other tissue.

[0019] The probe **112** further includes a probe tracking device **120**, which include one or more tracking elements. One or more of the tracking elements can be external to the device **120** and/or one or more of the tracking elements can be internal to the device **120**. In one instance, the one or more of the tracking elements include one or more of an emitter, a transmitter, and/or a passive sensor. Examples of such tracking devices include an electro-magnetic tracking device, an optical tracking device, an inertial tracking device, and/or other tracking device. Tracking devices are discussed in Birkfellner et al., "Tracking Devices," In: Peters T., Cleary K. (eds) Image-Guided Interventions. Springer, Boston, Mass., 2008.

[0020] Transmit and receive circuitry (TX/RX) **122** is configured to generate the excitation signal conveyed to the transducer array **116** for at least flow imaging, including 3-D imaging by manual and/or electrical-mechanical sweeping of the transducer array **116**. The TX/RX **122** is also configured to process the electrical signal corresponding to the received echo signal. The TX/RX **122**, in one instance, is further configured to pre-condition and/or pre-process the signal (e.g., amplify, digitize, etc.). Other processing is also contemplated herein.

[0021] The illustrated embodiment shows the transmit and receive operations are performed by the same circuitry, the TX/RX **122**. In a variation, the transmit and receive operations are performed by separate circuitry, e.g., transmit circuitry for transmit operations and separate receive circuitry for receive operations. One or more switches and/or other device(s) can be used to switch between transmit and receive operations and/or transmit and receive circuitry by electrically connecting and electrically disconnecting transmit and receive circuitry.

[0022] A beamformer **124** beamforms the signal, e.g., via delay-and-sum beamforming and/or other beamforming. The beamformer **124** outputs the beamformed data. An image processor **126** processes the beamformed data. For B-mode imaging, this includes generating a sequence of focused, coherent echo samples along focused scanlines of a scanplane. The image processor **126** can also be configured to generate an A-mode, C-mode, and/or other ultrasound imaging mode image.

[0023] A flow processor **128** processes the beamformed data and generates flow images. Suitable flow processing includes color flow, Doppler and/or other flow processing. Generally, color flow is an enhanced form of Doppler that uses color to highlight the direction of blood flow. In some embodiments, the flow processor **128** is also configured to

detect presence of flow (i.e. flow or no flow per voxel), e.g., using high pass filtering, singular value decomposition, principal component analysis, spatial coherence factors, etc.

[0024] Example approaches are discussed in Birkeland, et al., "Doppler-based 3D Blood Flow Imaging and Visualization," Proceeding SCCG '13 Proceedings of the 29th Spring Conference on Computer Graphics, Pages 115-122, May 1-3, 2013, Torp, "Clutter Rejection Filters in Color Flow Imaging: A Theoretical Approach," IEEE Transactions on Ultrasonics, Ferroelectrics, and Frequency Control, Vol. 44, No. 2, March 1997, and Demene et al., "Spatiotemporal Clutter Filtering of Ultrafast Ultrasound Data Highly Increases Doppler and fUltrasound Sensitivity," IEEE Transactions on Medical Imaging, Vol. 34, No. 11, November 2015.

[0025] A segmentation processor **130** is configured to segment the beamformed data based on the flow data. For example, in one instance, the segmentation processor **130**, for each scan plane, distinguishes flow from surrounding tissue, and generates 3-D model representing vasculature tissue (i.e. blood vessels). In one instance, this includes comparing the data in each scan plane to a predetermined threshold and classifying regions satisfying the predetermined threshold as flow data and classifying other regions as non-flow data. The regions classified as flow data is then segmented and used to generate the 3-D model. In some embodiments, the segmentation processor **130** utilizes the B-mode images to refine the 3-D model, e.g., at border between the vasculature tissue and the surrounding tissue.

[0026] FIG. 2 schematically illustrates a non-limiting example of the segmentation processor **130**. Inputs to the segmentation processor **130** include tracking data **204**, a flow image **206**, and a tissue-flow mask **208**. The tracking data **204** come from the tracking device **120** and tracking system **106**. The flow image **206** and the tissue-flow mask **208** are produced by the flow processor **128**. The flow image **206** can be a color-flow image or a power doppler image. The tissue-flow mask **208** can be a separate data stream or incorporated in the flow image **206**. The tissue flow-mask consists typically of values between 0 and 1 indicating the probability that a given pixel of the flow image is true blood flow (value of 1) or not (value of 0).

[0027] Briefly turning to FIGS. 3 and 4, examples of a color flow image and a power doppler image are shown. FIG. 3 shows a 2D ultrasound image **302** consisting of a B-mode image **304** overlaid with a color flow image **306**. The display also includes a standard depth axis **308** and color-bars **310** and **312** for the B-mode image **304** and the color flow image **306**, respectively. FIG. 3 further shows labels **314** for predetermined anatomical structures, which in the illustrated case are: umbilical vein (UV), stomach (S), portal vein (PV), and gallbladder. FIG. 4 shows a screenshot **402** consisting of a 3D-rendered Power-Doppler image **404**, the depth axis **308**, the color-bar **310** for the B-mode image, and a color bar **406** for the Power-Doppler image **404**. The overlay includes labels **408** for predetermined anatomical structures, which in this case are: aorta; inferior vena cava (ivc); ductus venosus (dv); and umbilical vein (uv). The user can rotate, translate and zoom the vessels rendered in 3D.

[0028] Returning to FIG. 2, The flow image **206** and the tissue-flow mask **208** can be 2D planar images, or 3D volumetric scans, depending on the probe **112**. In all cases, the tracking data **204** include coordinates and orientation of

the origin of the images. The volume creation block **210** maps the flow image **206** to a volumetric image. The created volume can be displayed directly to the user by the US display **132** by employing techniques such as volume rendering or maximum intensity projection. An example of this is discussed in Fishman et al., "Volume Rendering versus Maximum Intensity Projection in CT Angiography: What Works Best, When, and Why," *Radiographics*, vol. 26, no. 3, pp. 905-922, 2006. In this case, the blocks **212** and **214** are bypassed by employing data paths **216** and **218**.

[**0029**] The segmentation and labeling block **212** clusters the voxels that belong to the same vessel and assigns them labels. An example of this is described in Bradski et al., "Learning OpenCV. Computer Vision with the OpenCV Library", ISBN 9780596156022, O'Reilly Media, 2008. The output of the segmentation and labeling block **212** can be sent to the US display **132**. The surface generation block **214** uses the labeled voxel data to create triangle meshes of the surface of the vessel walls. Examples of suitable approaches are discussed in Treece et al., "Regularized marching tetrahedra: Improved iso-surface extraction," *Comput. Graph.*, vol. 23, no. 4, pp. 583-598, 1999, Treece et al., "Fast surface and volume estimation from non-parallel cross-sections, for freehand three-dimensional ultrasound," *Med. Image Anal.*, vol. 3, no. 2, pp. 141-173, 1999, and Treece et al., "Surface interpolation from sparse cross sections using region correspondence," *IEEE Trans. Med. Imaging*, vol. 19, no. 11, pp. 1106-1114, 2000.

[**0030**] A display (US Display) **132** is configured to display images, e.g., B-mode, flow images, and/or the 3-D model. A controller **134** is configured to control one or more of the components of the ultrasound imaging system **100**. Such control can be based on available modes of operation such as B-mode and/or flow mode, etc. A user interface **136** includes one or more input devices such as a keyboard, a trackball, a mouse, a touch sensitive screen, etc. configured to allow a user to interact with the ultrasound imaging system **102**.

[**0031**] In this example, the optical camera-based guidance system **104** includes a laparoscope **133**, which includes a shaft **136**, a camera **138** disposed at a first end of the shaft **136**, a light guide **140** disposed at the first end of the shaft **136**, a light source **140** in optical communication with the light guide **140**, and a laparoscope tracking device **142**, which include one or more tracking elements. Other suitable systems include a microscope, an optical interface of a surgical robot, etc. One or more of the tracking elements can be external to the tracking device **142** and/or one or more of the tracking elements can be internal to the tracking device **142**. In one instance, the one or more of the tracking elements include one or more of an emitter, a receiver, and/or a passive sensor. Examples of such tracking devices include an electro-magnetic tracking device, an optical tracking device, an inertial tracking device, and/or other tracking device. Tracking devices are discussed in Birkfellner et al.

[**0032**] The tracking system **106** interacts with the probe tracking device **120** and the laparoscope tracking device **142**, registers their spatial coordinate systems, and determines a location and an orientation of the probe tracking device **120** and the laparoscope tracking device **142** relative to each other. For example, where the probe tracking device **120** and/or the laparoscope tracking device **142** includes magnets, the tracking system **106** measures a magnetic field

strength of the magnets, which depends on a distance and direction of the magnets to the tracking system **106**, and the strength and direction is used to determine location and orientation. In another example, where the probe tracking device **120** and/or the laparoscope tracking device **142** includes external optical elements, the tracking system **106** includes an optical device such as a video camera that records the spatial orientation of the optical elements to determine location and orientation.

[**0033**] Examples of suitable tracking system **106** are described in U.S. patent application US 2010/0298712 A1, filed Feb. 10, 2010, and entitled "Ultrasound Systems Incorporating Position Sensors and Associated Method," and U.S. Pat. No. 8,556,815 B2, filed May 6, 2010, and entitled "Freehand Ultrasound Imaging Systems and Methods for Guiding Elongate Instruments," both of which are incorporated herein by reference in their entireties. Another example is discussed in U.S. Pat. No. 7,835,785 B2, filed Oct. 4, 2005, and entitled "DC Magnetic-Based Position and Orientation Monitoring system for Tracking Medical Instruments." Other tracking systems are discussed in Birkfellner et al. Other approaches are also contemplated herein.

[**0034**] The image guidance system **108** includes at least a processor **144** (e.g., a central processing unit, a microprocessor, etc.) and memory **146** (e.g., physical memory, etc.). The image guidance system **108** receives the 3-D model from the console **114** of the ultrasound imaging system **102**, the optical signal/feed from the optical camera-based guidance system **104**, and the tracking signal from the tracking system **106**, and displays, via a display (IGS Display) **148**, the optical signal/feed from the optical camera-based guidance system **104** overlaid with the 3-D model based on the tracking signal. In one instance, the memory **146** include an augmented reality algorithm, the processor **144** executes the augmented reality algorithm to combine the optical signal/feed and the 3-D model. Other approaches are also contemplated herein. Depth information can be added through shading, fading, intensity, color, etc.

[**0035**] The at least one instrument **110** includes a shaft **150** and a device **152** disposed at a first end of the shaft **150**. The device **152** can include a suitable device for resection, cauterization, cryotherapy, biopsy, ablation, etc. For example, the device **152** can include a grasper, scissors, a stapler, etc.

[**0036**] The probe **112** of the ultrasound imaging system **102**, the optical camera-based guidance system **104**, and the at least one instrument **110** are shown in connection with an object **154** and material of interest **156** within the object **154**. Where the object **154** is a patient, a portal such as a trocar or the like may first be placed through the wall of the object **154** and the optical camera-based guidance system **104** and the at least one instrument **110** are inserted into cannulas of the trocars and into the cavity of the object **154**.

[**0037**] FIG. 5 illustrates an example method in accordance with an embodiment herein.

[**0038**] It is to be understood that the following acts are provided for explanatory purposes and are not limiting. As such, one or more of the acts may be omitted, one or more acts may be added, one or more acts may occur in a different order (including simultaneously with another act), etc.

[**0039**] At **502**, the transducer array **116** is swept over the material of interest **156**.

[**0040**] At **504**, the flow processor **128** determined flow information from the acquired data.

[0041] At 506, the segmentation processor 130 segments vasculature from the acquired data with the flow information.

[0042] At 508, the segmentation processor 130 creates the 3-D model of the vasculature with the segmentation.

[0043] At 510, the image guidance system 108 receives an optical feed from the optical camera-based guidance system 104.

[0044] At 512, the image guidance system 108 receives the tracking signal from the tracking system 106.

[0045] At 514, the image guidance system 108 displays the optical feed with the 3-D model projected thereon based on the tracking signal, which aligns their coordinate systems.

[0046] This process can be repeated one or more times during the procedure and/or after the procedure, e.g., to validate vasculature was avoided.

[0047] The 3-D model can be static and outline the average contours of the vasculature or dynamic and show pulsation of the flow.

[0048] Depth information can be added through shading, fading, intensity, color, etc. The user utilizes the displayed information to guide the instrument 110 to the material of interest 156 and treat the material of interest 156 with the instrument 110.

[0049] The above may be implemented by way of computer readable instructions, encoded or embedded on computer readable storage medium (which excludes transitory medium), which, when executed by a computer processor(s) (e.g., central processing unit (CPU), microprocessor, etc.), cause the processor(s) to carry out acts described herein. Additionally, or alternatively, at least one of the computer readable instructions is carried by a signal, carrier wave or other transitory medium, which is not computer readable storage medium.

[0050] The application has been described with reference to various embodiments. Modifications and alterations will occur to others upon reading the application. It is intended that the invention be construed as including all such modifications and alterations, including insofar as they come within the scope of the appended claims and the equivalents thereof.

What is claimed is:

1. A system, comprising:

an image guidance system, including:

- a memory with computer executable instructions;
- a processor configured to execute the computer executable instructions, which causes the processor to:
 - receive a three-dimensional model of vasculature from an ultrasound imaging system;
 - receive a real-time optical feed of an interior of a cavity from an optical camera-based guidance system;
 - receive a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system;
 - receive a second spatial location of the optical camera-based guidance system; and
 - overlay the optical feed with the three-dimensional model based on the first and second signals; and
- a display configured to visually present the optical feed with the three-dimensional model overlaid thereover.

2. The system of claim 1, wherein the three-dimensional model is a static model that outlines average contours of the vasculature.

3. The system of claim 1, wherein the three-dimensional model is a dynamic model that visually presents pulsation of a flow.

4. The system of claim 1, wherein the ultrasound imaging system comprises:

- a probe with a transducer array to acquire three-dimensional data of the vasculature;
- a beamformer configured to beamform the acquired data;
- a flow processor configured to produce flow data from the beamformed data; and
- a segmentation processor configured to produce the three-dimensional model from the flow data.

5. The system of claim 4, the ultrasound imaging system further comprises:

- an image processor configured to produce a B-mode image from the beamformed data, wherein the segmentation processor refines the three-dimensional model with the B-mode image.

6. The system of claim 4, further comprising:

- a tracking device of the probe; and
- a tracking system configured to interact with the tracking device to produce the first tracking signal.

7. The system of claim 1, wherein the optical camera-based guidance system comprises:

- a shaft;
- a light disposed at a first end;
- an optical device disposed at the first end;
- a light source in optical communication with the light; and
- an optical path from the optical device to the processor.

8. The system of claim 7, further comprising:

- a tracking device of the optical camera-based guidance system; and
- a tracking system configured to interact with the tracking device to produce the second tracking signal.

9. The system of claim 1, wherein the optical feed shows a location of an instrument in the cavity.

10. The system of claim 1, wherein the three-dimensional model shows vasculature behind an outer surface tissue being treated by an instrument in the cavity.

11. A method, comprising:

- receiving a three-dimensional model of vasculature from an ultrasound imaging system;
- receiving a real-time optical feed of an interior of a cavity from an optical camera-based guidance system;
- receiving a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system;
- receiving a second spatial location of the optical camera-based guidance system; and
- overlaying the optical feed with the three-dimensional model based on the first and second tracking signals; and
- displaying the optical feed with the three-dimensional model overlaid thereover.

12. The method of claim 11, wherein the three-dimensional model is a static model that outlines average contours of the vasculature.

13. The method of claim 11, wherein the three-dimensional model is a dynamic model that visually presents pulsation of the flow.

14. The method of claim **11**, further comprising:
acquiring three-dimensional data of the vasculature;
beamforming the acquired data;
producing flow data from the beamformed data; and
segmenting the three-dimensional model from the flow data.

15. The method of claim **11**, wherein the optical feed shows a location of an instrument in the cavity, and the three-dimensional model shows vasculature behind an outer surface tissue being treated by the instrument in the cavity.

16. A computer readable medium encoded with computer executable instructions which when executed by a processor of a computer causes the processor to:

- receive a three-dimensional model of vasculature from an ultrasound imaging system;
- receive a real-time optical feed of an interior of a cavity from an optical camera-based guidance system;
- receive a first tracking signal indicative of a first spatial location of a probe of the ultrasound imaging system;

- receive a second spatial location of the optical camera-based guidance system;
- overlay the optical feed with the three-dimensional model based on the first and second tracking signals; and
- display the optical feed with the three-dimensional model overlaid thereover.

17. The computer readable medium of claim **16**, wherein the three-dimensional model is a static model that outlines average contours of the vasculature.

18. The computer readable medium of claim **16**, wherein the three-dimensional model is a dynamic model that visually presents pulsation of the flow.

19. The computer readable medium of claim **16**, wherein the optical feed shows a location of an instrument in the cavity.

20. The computer readable medium of claim **16**, wherein the three-dimensional model shows vasculature behind an outer surface tissue being treated by the instrument in the cavity.

* * * * *

专利名称(译)	组合超声/光学图像以进行图像引导程序		
公开(公告)号	US20190380786A1	公开(公告)日	2019-12-19
申请号	US16/009631	申请日	2018-06-15
[标]申请(专利权)人(译)	B-K医疗公司		
申请(专利权)人(译)	B-k医疗APS		
当前申请(专利权)人(译)	B-k医疗APS		
[标]发明人	GRAN FREDRIK NIKOLOV SVETOSLAV IVANOV		
发明人	GRAN, FREDRIK NIKOLOV, SVETOSLAV IVANOV		
IPC分类号	A61B34/20 A61B8/08 A61B8/00 A61B1/313 A61B1/06 G06T17/00		
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外部链接	Espacenet USPTO		

摘要(译)

一种系统，包括图像引导系统，该图像引导系统具有带有计算机可执行指令的存储器，配置为执行计算机可执行指令的处理器以及显示器。所述计算机可执行指令使所述处理器：从超声成像系统接收脉管系统的三维模型，从基于光学相机的引导系统接收腔内部的实时光学馈送，接收第一跟踪信号指示超声成像系统的探头的第一空间位置，接收基于光学相机的引导系统的第二空间位置，并基于第一和第二跟踪信号将光馈送与三维模型重叠。显示器被配置为在视觉上呈现光学馈送，其上覆盖有三维模型。

