

FIG. 1

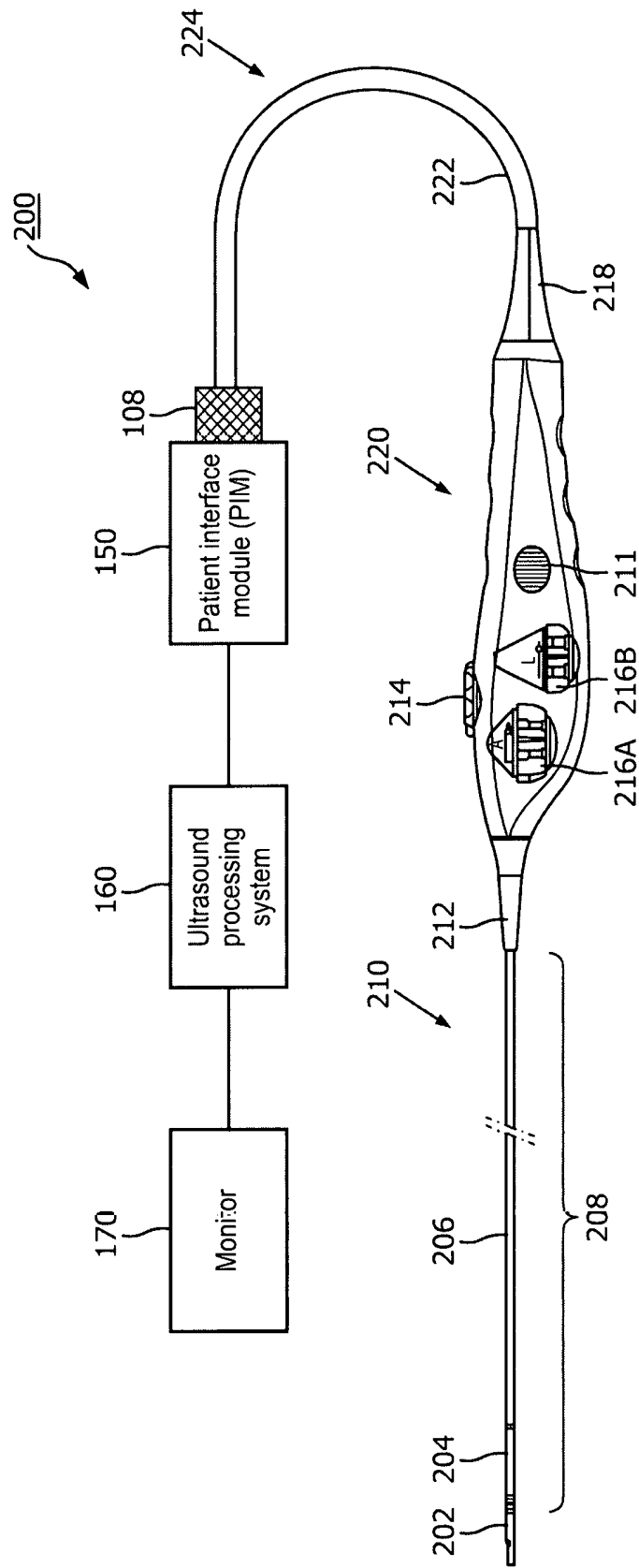


FIG. 2

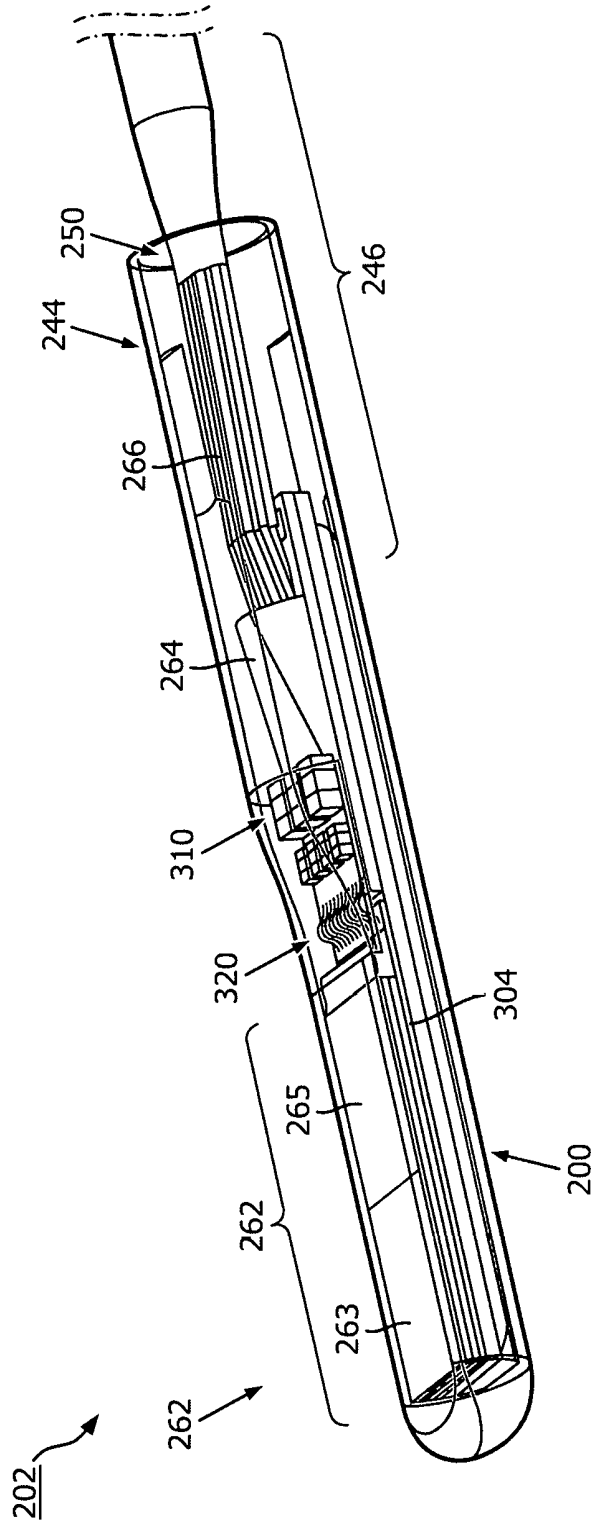


FIG. 3

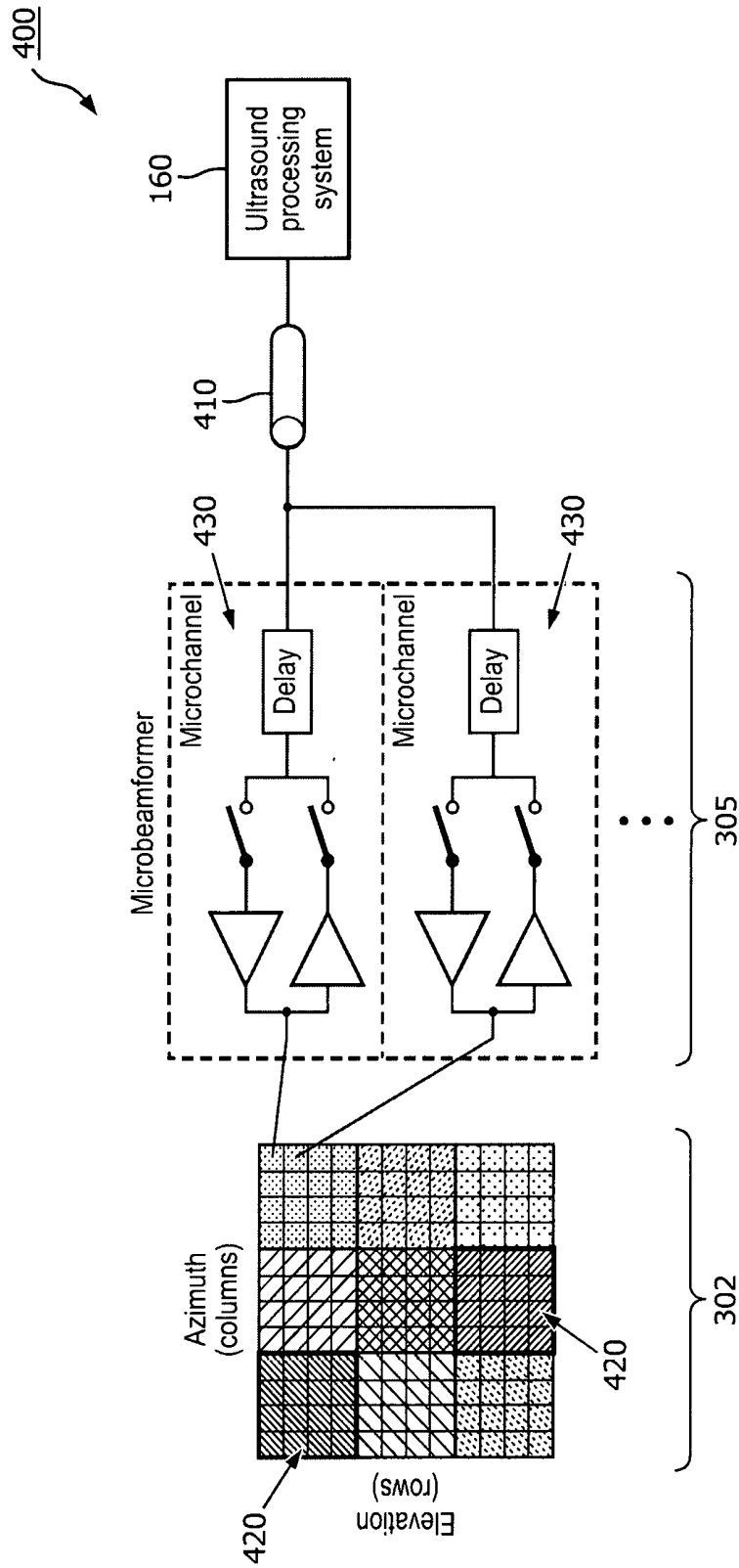


FIG. 4

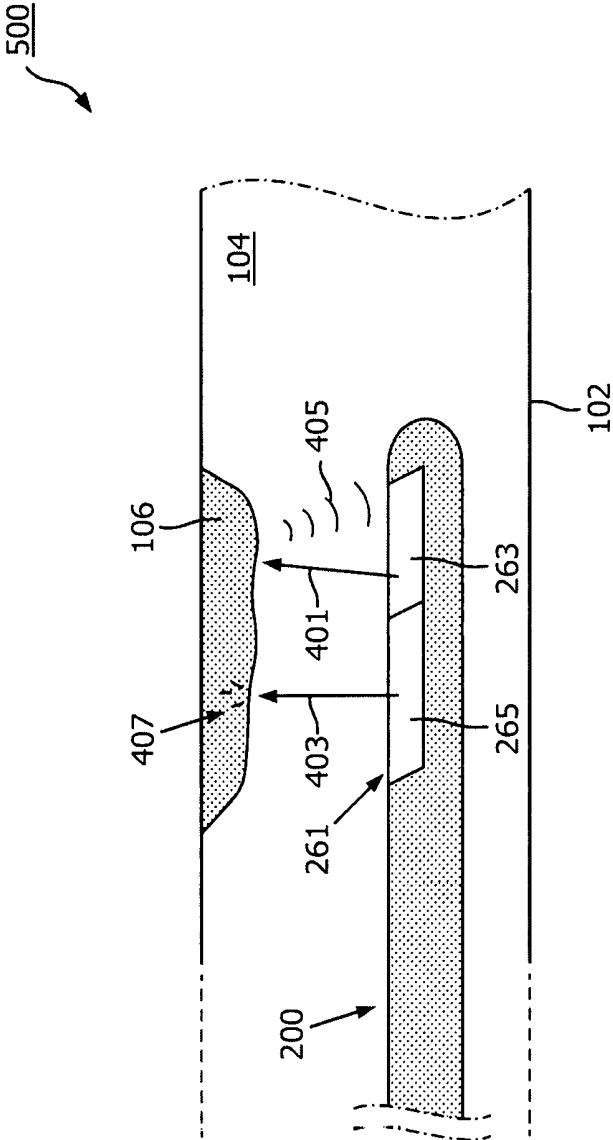


FIG. 5

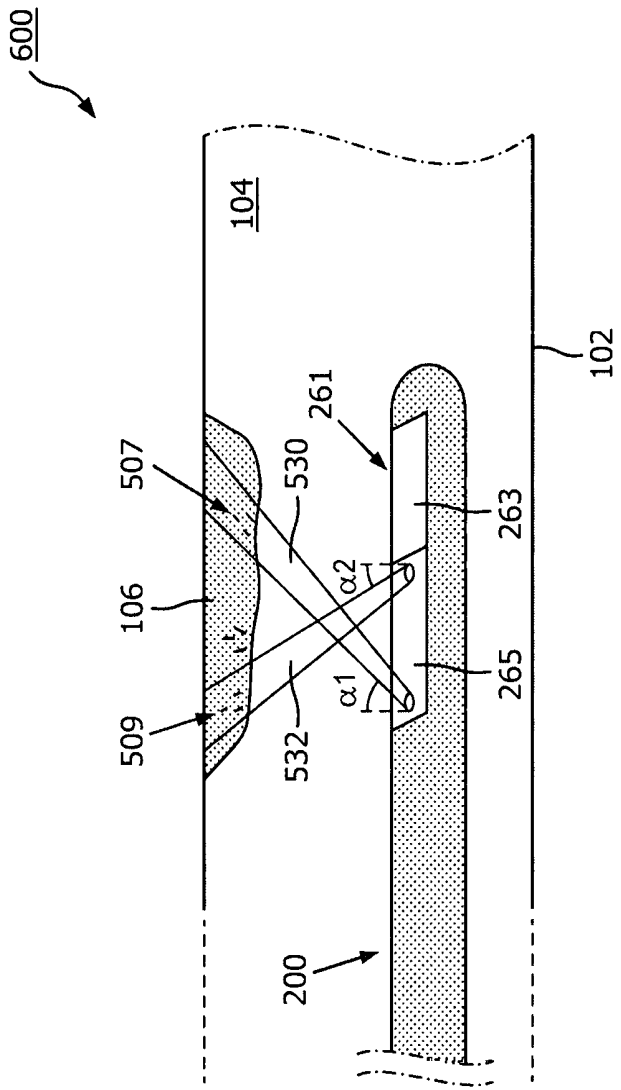


FIG. 6

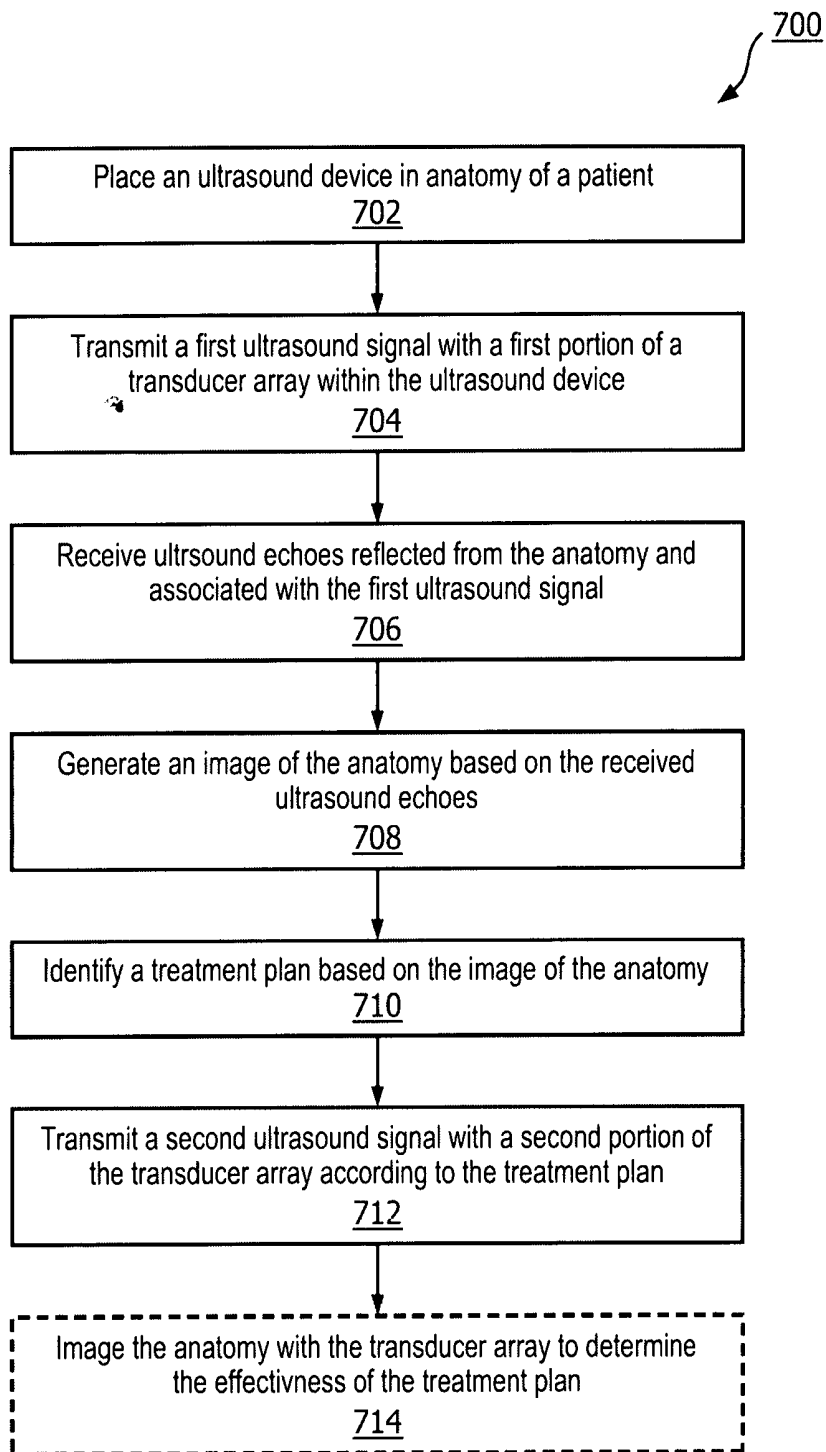


FIG. 7

## INTRACARDIAC THERAPEUTIC AND DIAGNOSTIC ULTRASOUND DEVICE

### TECHNICAL FIELD

[0001] The present disclosure relates generally to ultrasound devices, and in particular, ultrasound devices with transducers that may be used for therapeutic and diagnostic applications.

### BACKGROUND

[0002] Diagnostic and therapeutic ultrasound catheters have been designed for use inside many areas of the human body. In the cardiovascular system, a common diagnostic ultrasound method is intraluminal ultrasound imaging with intra-cardiac echocardiography (ICE) being a specific example of intraluminal imaging. Typically, a single rotating transducer or an array of transducer elements is used to transmit ultrasound at the tips of the catheters. The same transducers (or separate transducers) are used to receive echoes from the tissue. A signal generated from the echoes is transferred to a console which allows for the processing, storing, display, or manipulation of the ultrasound-related data.

[0003] Intraluminal imaging catheters such as ICE catheters (e.g., Siemens Acunav, St. Jude ViewFlex) are usually used to image heart and surrounding structures, for example, to guide and facilitate medical procedures, such as trans-septal lumen punctures, left atrial appendage closures, atrial fibrillation ablation, and valve repairs. Commercially-available ICE catheters have distal ends which can be articulated by a steering mechanism located in a handle at the proximal end of the catheter. For example, an intraluminal imaging catheter such as an ICE catheter may be inserted through the femoral or jugular vein when accessing the anatomy, and steered in the heart to acquire images necessary to the safety of the medical procedures.

[0004] Existing ICE catheters are used only for imaging procedures. After imaging procedures are complete, the catheters are usually removed and other systems are inserted into the vasculature of a patient to treat areas of interest identified by the imaging procedures. The removal and insertion of multiple tools may be time consuming and may increase health risks to the patient.

### SUMMARY

[0005] An ultrasound system is provided by the present disclosure. The ultrasound system can include an ultrasound device that is configured to be placed inside of the anatomy of a patient. The ultrasound device may include a transducer array with a number of transducer elements. The transducer array may include a first portion and a second portion. The first portion may be used for diagnostic procedures that may include transmitting ultrasound signals and receiving ultrasound echoes with the first portion. The second portion may be used for therapeutic procedures including transmitting ultrasound signals. The ultrasound signals transmitted for therapeutic purposes may have a lower frequency than those transmitted for diagnostic purposes. Exemplary technical advancements described herein include an ultrasound system that may be used to image and treat a patient without removing and replacing equipment. Furthermore, the ultra-

sound system may be configured to provide ultrasound signals at different angles without physically moving the ultrasound device.

[0006] An ultrasound system is provided by the present disclosure, which may include: an ultrasound device that may include: a flexible elongate member configured to be positioned within anatomy of a patient, the flexible elongate member comprising a proximal portion and a distal portion; and an ultrasound transducer array positioned at the distal portion of the flexible elongate member, wherein the ultrasound transducer array includes a plurality of transducer elements arranged in a first segment and a second segment, wherein the first segment is configured to emit a first ultrasound signal with a first frequency and the second segment is configured to emit a second ultrasound signal with a second frequency different than the first frequency.

[0007] In some embodiments, the second frequency is lower than the first frequency. In particular, the first frequency may be between 10 MHz and 70 MHz and the second frequency is between 1 kHz and 5 MHz. The ultrasound transducer array may be a two-dimensional array, wherein the first segment is disposed on a first portion of the two-dimensional array and the second segment is disposed on a second portion of the two-dimensional array adjacent the first portion. In some embodiments, the first segment comprises a high resonant frequency material and the second segment comprises a low resonant frequency material. The ultrasound transducer array may include at least one of PZT, CMUT, or PMUT.

[0008] In some embodiments, the first segment of the ultrasound transducer array is configured to receive ultrasound echoes reflected from the anatomy and associated with the first ultrasound signal. The ultrasound system may further include a computing device in communication with the ultrasound transducer array and configured to produce an ultrasound image based on the received ultrasound echoes. The system may further include a controller disposed at the distal portion of the flexible elongate member and in communication with the ultrasound transducer array. In some embodiments, the ultrasound transducer array is configured to direct the second ultrasound signal to a first portion of anatomy and a second portion of anatomy different from the first portion of anatomy without moving the ultrasound transducer array.

[0009] The ultrasound device may further include a switch to selectively switch between transmitting signals with the first segment and the second segment. The ultrasound device may further include a substrate including electrical conductors connected to the ultrasound transducer array, the electrical conductors configured to selectively switch between transmitting signals with the first segment and the second segment. The flexible elongate member may include a first cable configured to control transmission of signals of the first segment and a second cable configured to control transmission of signals of the second segment. The flexible elongate member may include a third cable configured to control transmission of signals of both the first segment and the second segment.

[0010] A method of transmitting ultrasound signals is provided by the present disclosure, which may include: transmitting, with a first segment of an ultrasound transducer array of an ultrasound device positioned within anatomy of a patient, a first ultrasound signal with a first frequency to image an area of interest of the anatomy; receiving, with the

first segment of the ultrasound transducer array, ultrasound echoes reflected from the anatomy and associated with the first ultrasound signal; and transmitting, with a second segment of the ultrasound transducer array, a second ultrasound signal with a second frequency to an area of interest within the anatomy.

**[0011]** In some embodiments, the method further includes generating, with a controller, an image of the area of interest based on the second ultrasound signal. The method may include generating a treatment plan based on the image of the area of interest. The method may include transmitting, with the second segment of the ultrasound transducer array, the second ultrasound signal to perform a therapeutic procedure based on the treatment plan. The therapeutic procedure may include an ultrasound cavitation procedure that includes forming ultrasound cuts into calcification within the anatomy. The therapeutic procedure may include preparing a portion of the anatomy for delivery of medication.

**[0012]** In some embodiments, the second ultrasound signal has a lower frequency than the first ultrasound signal. In particular, the frequency of the first ultrasound signal may be between 10 MHz and 70 MHz and a frequency of the second ultrasound signal may be between 1 kHz and 5 MHz. The method may include placing the ultrasound device within the anatomy of the patient. The method may include directing transmission of the second ultrasound signal from the second segment to a first portion of the area of interest and directing transmission of a third ultrasound signal from the second segment to a second portion of the area of interest different than the first portion of the area of interest without moving the ultrasound transducer array.

**[0013]** Additional aspects, features, and advantages of the present disclosure will become apparent from the following detailed description.

#### BRIEF DESCRIPTION OF THE DRAWINGS

**[0014]** Illustrative embodiments of the present disclosure will be described with reference to the accompanying drawings, of which:

**[0015]** FIG. 1 is a schematic diagram of an ultrasound system according to embodiments of the present disclosure.

**[0016]** FIG. 2 is a schematic diagram of an ultrasound system including a handle according to embodiments of the present disclosure.

**[0017]** FIG. 3 is a top view of a tip member according to embodiments of the present disclosure.

**[0018]** FIG. 4 is a schematic diagram illustrating the beam-forming of an ultrasound device according to embodiments of the present disclosure.

**[0019]** FIG. 5 is a schematic diagram illustrating aspects of an ultrasound device according to embodiments of the present disclosure.

**[0020]** FIG. 6 is another schematic diagram illustrating aspects of an ultrasound device according to embodiments of the present disclosure.

**[0021]** FIG. 7 is a flowchart illustrating a method of transmitting ultrasound signals according to embodiments of the present disclosure.

#### DETAILED DESCRIPTION

**[0022]** For the purposes of promoting an understanding of the principles of the present disclosure, reference will now be made to the embodiments illustrated in the drawings, and

specific language will be used to describe the same. It is nevertheless understood that no limitation to the scope of the disclosure is intended. Any alterations and further modifications to the described devices, systems, and methods, and any further application of the principles of the present disclosure are fully contemplated and included within the present disclosure as would normally occur to one skilled in the art to which the disclosure relates. For example, while the ultrasound system is described in terms of transmitting ultrasound signals and receiving ultrasound echoes, it is understood that it is not intended to be limited to this application. In particular, it is fully contemplated that the features, components, and/or steps described with respect to one embodiment may be combined with the features, components, and/or steps described with respect to other embodiments of the present disclosure. For the sake of brevity, however, the numerous iterations of these combinations will not be described separately.

**[0023]** FIG. 1 is a diagrammatic schematic view of an ultrasound system 100 according to some embodiments of the present disclosure. The system 100 can include an ultrasound device 110, a patient interface module (PIM) 150, an ultrasound processing system 160, and/or a monitor 170. The ultrasound device 110 is structurally arranged (e.g., sized and/or shaped) to be positioned within anatomy 102 of a patient. The ultrasound device 110 obtains ultrasound imaging data from within the anatomy 102 and applies ultrasound therapy to the anatomy 102. The ultrasound processing system 160 can control the acquisition of ultrasound imaging data and/or the application of ultrasound therapy, and generates an image of the anatomy 102 (using the ultrasound imaging data received via the PIM 150) that is displayed on the monitor 170.

**[0024]** Generally, the ultrasound device 110 can be a catheter, a guide catheter, or a guide wire. The ultrasound device 110 includes a flexible elongate member 116. As used herein, “elongate member” or “flexible elongate member” includes at least any thin, long, flexible structure structurally arranged (e.g., sized and/or shaped) to be positioned within a lumen 104 of the anatomy 102. For example, a distal portion 114 of the flexible elongate member 116 is positioned within the lumen 104, while a proximal portion 112 of the flexible elongate member 116 is positioned outside of the body of the patient. The flexible elongate member 116 can include a longitudinal axis LA. In some instances, the longitudinal axis LA can be a central longitudinal axis of the flexible elongate member 116. In some embodiments, the flexible elongate member 116 can include one or more polymer/plastic layers formed of various grades of nylon, Pebax, polymer composites, polyimides, and/or Teflon. In some embodiments, the flexible elongate member 116 can include one or more layers of braided metallic and/or polymer strands. The braided layer(s) can be tightly or loosely braided in any suitable configuration, including any suitable per in count (pic). In some embodiments, the flexible elongate member 116 can include one or more metallic and/or polymer coils. All or a portion of the flexible elongate member 116 may have any suitable geometric cross-sectional profile (e.g., circular, oval, rectangular, square, elliptical, etc.) or non-geometric cross-sectional profile. For example, the flexible elongate member 116 can have a generally cylindrical profile with a circular cross-sectional profile that defines an outer diameter of the flexible elongate member 116. For example, the outer diameter of the flexible

elongate member **116** can be any suitable value for positioning within the anatomy **102**, including between approximately 1 Fr and approximately 15 Fr, including values such as 3.5 Fr, 5 Fr, 7 Fr, 8.2 Fr, 9 Fr, and/or other suitable values both larger and smaller.

[0025] The ultrasound device **110** may or may not include one or more lumens extending along all or a portion of the length of the flexible elongate member **116**. The lumen of the ultrasound device **110** can be structurally arranged (e.g., sized and/or shaped) to receive and/or guide one or more other diagnostic and/or therapeutic instruments. If the ultrasound device **110** includes lumen(s), the lumen(s) may be centered or offset with respect to the cross-sectional profile of the device **110**. In the illustrated embodiment, the ultrasound device **110** is a catheter and includes a lumen at the distal portion **114** of the flexible elongate member **116**. A guide wire **140** extends through the lumen of the ultrasound device **110** between an exit/entry port **142** and an exit/entry port at a distal end **118** of the flexible elongate member **116**. Generally, the guide wire **140** is a thin, long, flexible structure that is structurally arranged (e.g., sized and/or shaped) to be disposed within the lumen **104** of the anatomy **102**. During a diagnostic and/or therapeutic procedure, a medical professional typically first inserts the guide wire **140** into the lumen **104** of the anatomy **102** and moves the guide wire **140** to a desired location within the anatomy **102**, such as adjacent to an occlusion **106**. The guide wire **140** facilitates introduction and positioning of one or more other diagnostic and/or therapeutic instruments, including the ultrasound device **110**, at the desired location within the anatomy **102**. For example, the ultrasound device **110** moves through the lumen **104** of the anatomy **102** along the guide wire **140**. In some embodiments, the lumen of the ultrasound device **110** can extend along the entire length of the flexible elongate member **116**. In the illustrated embodiment, the exit/entry port **142** is positioned proximally of components **120**, **130**, and **145** of the ultrasound device **110**. In some embodiments, the exit/entry port **142**, the exit/entry port at the distal end **118**, and/or the lumen of the ultrasound device **110** is positioned distally of the components **120**, **130**, and **145**. In some embodiments, the ultrasound device **110** is not used with a guide wire, and the exit/entry port **142** can be omitted from the ultrasound device **110**.

[0026] The anatomy **102** may represent any fluid-filled or surrounded structures, both natural and man-made. For example, the anatomy **102** can be within the body of a patient. Fluid can flow through the lumen **104** of the anatomy **102**. In some instances, the ultrasound device **110** can be referenced as an intraluminal device. The anatomy **102** can be a vessel, such as a blood vessel, in which blood flows through the lumen **104**. In some instances, the ultrasound device **110** can be referenced as an intravascular device. In various embodiments, the blood vessel is an artery or a vein of a patient's vascular system, including cardiac vasculature, peripheral vasculature, neural vasculature, renal vasculature, and/or any other suitable anatomy/lumen inside the body. The anatomy **102** can be tortuous in some instances. For example, the device **110** may be used to examine any number of anatomical locations and tissue types, including without limitation, organs including the liver, heart, kidneys, gall bladder, pancreas, lungs, esophagus; ducts; intestines; nervous system structures including the brain, dural sac, spinal cord and peripheral nerves; the urinary tract; as well as valves within the blood, chambers

or other parts of the heart, and/or other systems of the body. In addition to natural structures, the device **110** may be used to examine man-made structures such as, but without limitation, heart valves, stents, shunts, filters and other devices.

[0027] The occlusion **106** of the anatomy **102** is generally representative of any blockage or other structural arrangement that results in a restriction to the flow of fluid through the lumen **104**, for example, in a manner that is deleterious to the health of the patient. For example, the occlusion **106** narrows the lumen **104** such that the cross-sectional area of the lumen **104** and/or the available space for fluid to flow through the lumen **104** is decreased. Where the anatomy **102** is a blood vessel, the occlusion **106** may be a result of plaque buildup, including without limitation plaque components such as fibrous, fibro-lipidic (fibro fatty), necrotic core, calcified (dense calcium), blood, fresh thrombus, and/or mature thrombus. In some instances, the occlusion **106** can be referenced as thrombus, a stenosis, and/or a lesion. Generally, the composition of the occlusion **106** will depend on the type of anatomy being evaluated. Healthier portions of the anatomy **102** may have a uniform or symmetrical profile (e.g., a cylindrical profile with a circular cross-sectional profile). The occlusion **106** may not have a uniform or symmetrical profile. Accordingly, diseased portions of the anatomy **102**, with the occlusion **106**, will have a non-symmetric and/or otherwise irregular profile. While the anatomy **102** is illustrated in FIG. 1 as having a single occlusion **106**, it is understood that the devices, systems, and methods described herein have similar application for anatomy having multiple occlusions.

[0028] The ultrasound device **110** includes ultrasound structures **120** and **130** at the distal portion **114** of the flexible elongate member **116**. The structures **120** and **130** are configured to emit ultrasonic energy into the anatomy **102** while the device **110** is positioned within the lumen **104**. In some embodiments, the two ultrasound structures **120** and **130** are distinct. In other embodiments, the two structures **120** and **130** are the same ultrasound component or part of the same ultrasound component. One of the structures **120**, **130** is configured for diagnostic use, while the other of the structures **120**, **130** is configured for therapeutic use. For example, the structures **120**, **130** can emit different frequencies of ultrasonic energy into the anatomy **102** depending on whether the ultrasonic energy is being used for diagnosis, such as imaging, and/or treatment.

[0029] In some embodiments, the structures **120** and/or **130** include ultrasound transducer(s). For example, the ultrasound structures **120** and/or **130** can be configured to generate and emit ultrasound energy into the anatomy **102** in response to being activated by an electrical signal. In some embodiments, the structures **120** and/or **130** include a single ultrasound transducer. In some embodiments, the structures **120** and/or **130** include an ultrasound transducer array including more than one ultrasound transducer. For example, an ultrasound transducer array can include any suitable number of individual transducers between 2 transducers and 1000 transducers, including values such as 2 transducers, 4 transducers, 36 transducers, 64 transducers, 128 transducers, 500 transducers, 812 transducers, and/or other values both larger and smaller. The ultrasound transducer array **120** and/or **130** can be any suitable configuration, such as phased array including a planar array, a curved array, a circumferential array, an annular array, etc. For example, the ultrasound transducer array **120** and/or **130** can be a one-

dimensional array or a two-dimensional array in some instances. In some instances, the structures **120** and/or **130** can be a rotational ultrasound device. The active area of the ultrasound structures **120** and/or **130** can include one or more transducer materials and/or one or more segments of ultrasound elements (e.g., one or more rows, one or more columns, and/or one or more orientations) that can be uniformly or independently controlled and activated. The active area of the ultrasound structures **120** and/or **130** can be patterned or structured in various basic or complex geometries. The structures **120** and/or **130** can be disposed in a side-looking orientation (e.g., ultrasonic energy emitted perpendicular and/or orthogonal to the longitudinal axis LA) and/or a forward-looking orientation (e.g., ultrasonic energy emitted parallel to and/or along the longitudinal axis LA). In some instances, the structures **120** and/or **130** is structurally arranged to emit and/or receive ultrasonic energy at an oblique angle relative to the longitudinal axis LA, in a proximal or distal direction. In some embodiments, ultrasonic energy emission can be electronically steered by selective triggering of one or more transducer elements of the array in structures **120** and/or **130**.

**[0030]** The ultrasound transducer(s) of the structures **120** and/or **130** can be a piezoelectric micromachined ultrasound transducer (PMUT), capacitive micromachined ultrasonic transducer (CMUT), single crystal, lead zirconate titanate (PZT), PZT composite, other suitable transducer type, and/or combinations thereof. Depending on the transducer material, the manufacturing process for ultrasound transducer(s) can include dicing, kerfing, grinding, sputtering, wafer technologies (e.g., SMA, sacrificial layer deposition), other suitable processes, and/or combinations thereof.

**[0031]** In some embodiments, the structure **120** is configured to obtain ultrasound imaging data associated with the anatomy **102**, such as the occlusion **106**. The ultrasound imaging data obtained by the structure **120** can be used by a medical professional to diagnose the patient, including evaluating the occlusion **106** of the anatomy **102**. For imaging, the structure **120** can be configured to both emit ultrasonic energy into the lumen **104** and/or the anatomy **102**, and to receive reflected ultrasound echoes representative of fluid and/or tissue of lumen **104** and/or the anatomy **102**. As described herein, the structure **120** can be an ultrasound imaging element, such as an ultrasound transducer and/or an ultrasound transducer array. For example, the ultrasound imaging element **120** generates and emits ultrasound energy into the anatomy **102** in response to transmission of an electrical signal to the structure **120**. For imaging, the ultrasound imaging element **120** generates and transmits an electrical signal representative of the received reflected ultrasound echoes from the anatomy **102** (e.g., to the PIM **150** and/or ultrasound processing system **160**). In various embodiments, the structure **120** can obtain imaging data associated with intravascular ultrasound (IVUS) imaging, forward looking intravascular ultrasound (FL-IVUS) imaging, intravascular photoacoustic (IVPA) imaging, intracardiac echocardiography (ICE), transesophageal echocardiography (TEE), and/or other suitable imaging modalities.

**[0032]** For diagnosis and/or imaging, the center frequency of the ultrasound structure **120** can be between 10 MHz and 70 MHz, for example, including values such as 10 MHz, 20 MHz, 40 MHz, 45 MHz, 60 MHz, and/or other suitable values both larger and smaller. For example, lower frequen-

cies (e.g., 10 MHz, 20 MHz) can advantageously penetrate further into the anatomy **102**, such that more of the anatomy **102** is visible in the ultrasound images. Higher frequencies (e.g., 45 MHz, 60 MHz) can be better suited to generate more detailed ultrasound images of the anatomy **102** and/or fluid within the lumen **104**. In some embodiments, the frequency of the ultrasound structure **120** is tunable. For imaging, in some instances, the ultrasound structure **120** can be tuned to receive wavelengths associated with the center frequency and/or one or more harmonics of the center frequency. In some instances, the frequency of the emitted ultrasonic energy can be modified by the voltage of the applied electrical signal and/or the application of a biasing voltage to the ultrasound structure **120**.

**[0033]** In some embodiments, the structure **130** is configured to apply an ultrasound therapy to the anatomy **102**, such as the occlusion **106**. For example, the structure **130** emits sound waves that damage the structure of the occlusion **106**. In that regard, the device **110** and/or the structure **130** can be referenced as a lithotripsy device. The ultrasonic energy emitted by the structure **130** can create micro fractures in the occlusion **106**. For example, the structure **130** can deliver ultrasonic energy in a targeted manner to cause cavitation (e.g., wave force cavitation, thermal cavitation, etc.) of the occlusion **106**. Delivery of ultrasound therapy by the structure **130** advantageously facilitates thrombus dilution and/or vessel preparation. For example, ultrasound therapy can be applied prior to delivery of a pharmacological agent to the anatomy **102**. The pharmacological agent can be a thrombolytic agent, a fibrinolytic agent, plasmin, plasminogen activator, urokinase, streptokinase, collagenase, heparinoid, anti-thrombin drug, any other suitable drug, and/or combinations thereof. As described herein, Pharmacological uptake can be advantageously improved as a result of the degradation of the occlusion **106** by the ultrasonic energy. By compromising the structure of the occlusion **106**, additional surface area is available for the pharmacological agent to contact and/or penetrate the anatomy **102**. Accordingly, the efficacy of the treatment and the health of the patient are improved.

**[0034]** In some embodiments, the structure **130** is an ultrasound element, such as an ultrasound transducer and/or ultrasound transducer array. For example, the ultrasound processing system **160** can be configured to generate and emit ultrasound energy into the anatomy **102** in response to transmission of an electrical signal to the structure **130**. Unlike the structure **120**, which is used of ultrasound imaging, the structure **130** need not be configured to receive ultrasonic echoes reflected the anatomy **102** and generate a representative electrical signal. For example, in some embodiments, the structure **130** is not an ultrasound element that generates ultrasound energy. Rather, the structure **130** can be an intermediate component that is configured to deliver ultrasound energy generated an ultrasound component separate from the device **110** (e.g., an external ultrasound transducer positioned outside of the body of the patient). For ultrasound therapy, the center frequency of the ultrasound structure **130** can be between 1 kHz and 5 MHz, for example, including values such as 50 kHz, 500 kHz, 1 MHz, 3 MHz, and/or other suitable values both larger and smaller. In some embodiments, the frequency of the ultrasound structure **130** is tunable. For example, the frequency of the emitted ultrasonic energy can be modified by the

voltage of the applied electrical signal and/or the application of a biasing voltage to the ultrasound structure 130.

[0035] In some embodiments, such as when the structures 120 and 130 both include ultrasound transducers, the structures 120 and 130 can be configured to generate and to emit ultrasound energy, and to generate electrical signals representative of the received ultrasound echoes. One of the structures 120, 130 can be operated in diagnostic and/or imaging mode (generates and emits ultrasound energy, and generates electrical signals representative of the received ultrasound echoes), while the other of the structures 120, 130 is operated in therapeutic mode (generates and/or emits ultrasound energy).

[0036] In some embodiments, the ultrasound device 110 includes a treatment component 145. For example, the treatment component 145 can include a balloon, a stent, a needle, an ablation electrode, mechanical cutting component, a rotational cutting device, an aspiration device, and/or other suitable devices. The treatment component 145 can be a targeted drug delivery device, a drug coated balloon, a drug coated stent, and/or other suitable device configured to deliver a pharmacological agent to the anatomy 102, such as the occlusion 106. For example, the pharmacological agent can be delivered to the anatomy 102 by the treatment component 145 after the ultrasound therapy is applied to the anatomy 102 by the ultrasound structure 130. In other embodiments, the ultrasound device 110 omits the treatment component 145.

[0037] Generally, the components 120, 130, and/or 145 are positioned at the distal portion of the flexible elongate member 116. The relative positioning of the components 120, 130, and/or 140 can vary in different embodiments. In the illustrated embodiment, the diagnostic and/or imaging ultrasound structure 120 is positioned proximally of the therapeutic ultrasound structure 130. In other embodiments, the therapeutic ultrasound structure 130 is positioned proximally of the diagnostic and/or imaging ultrasound structure 120. In embodiments which include the treatment component 145, the treatment component 145 can be positioned proximally of the ultrasound structures 120 and/or 130, distally of the ultrasound structures 120 and/or 130, or between the ultrasound structures 120 and/or 130.

[0038] The ultrasound structures 120 and/or 130 can include one or more electrical conductors extending along the length from the flexible elongate member 116. The electrical conductor(s) are in communication with the ultrasound structures 120, 130 at the distal portion 114, and an interface 156 at the proximal portion 112. The electrical conductors carry electrical signals between the ultrasound processing system 160 and the ultrasound structures 120, 130. For example, activation and/or control signals can be transmitted from the ultrasound processing system 160 to the ultrasound structures 120, 130 via the electrical conductors. Electrical signals representative of the reflected ultrasound echoes can be transmitted from the ultrasound structures 120 and/or 130 to the ultrasound processing system 160 via the electrical conductors. In some embodiments, the same electrical conductors can be used for communication between the ultrasound processing system 160 and the ultrasound structures 120 and/or 130. In other embodiments, different electrical conductors of the device 110 can be used for communication between the ultrasound processing system

160 and the ultrasound structure 120, and between the ultrasound processing system 160 and the ultrasound structure 130.

[0039] The ultrasound device 110 includes an interface 156 at the proximal portion 112 of the flexible elongate member 116. In some embodiments, the interface 156 can include a handle. For example, handle can include one or more actuation mechanisms to control movement of the device 110, such as deflection of the distal portion 114. In some embodiments, the interface 156 can include a telescoping mechanism that allows for pullback of the device 110 through the lumen. In some embodiments, the interface 156 can include a rotation mechanism to rotate one or more components of the device 110 (e.g., the flexible elongate member 116, the ultrasound structures 120, 130). In some embodiments, the interface 156 includes a user interface component (e.g., one or more buttons, a switch, etc.) for a medical professional to selectively activate the ultrasound structure 120 for imaging or the ultrasound structure 130 for therapy. In other embodiments, a user interface component of the PIM 150, the ultrasound processing system 160 and/or the monitor 170 allows a medical profession to selectively activate the ultrasound structure 120 for imaging or the ultrasound structure 130 for therapy. A conduit including, e.g., electrical conductors, extends between the interface 156 and the connector 108. The connector 108 can be configured to mechanically and/or electrically couple the device 110 to the PIM 150.

[0040] The ultrasound processing system 160, the PIM 150, and/or the ultrasound device 110 (e.g., the interface 156, the ultrasound structures 120 and/or 130, etc.) can include one or more controllers. The controllers can be integrated circuits, such as application specific integrated circuits (ASIC), in some embodiments. The controllers can be configured to select the particular transducer element(s) to be used for transmit and/or receive, to provide the transmit trigger signals to activate the transmitter circuitry to generate an electrical pulse to excite the selected transducer element(s), and/or to accept amplified echo signals received from the selected transducer element(s) via amplifiers of controllers. Multiple ASIC configurations with various numbers of master circuits and slave circuits can be used to create a single ultrasound wave or multi-firing ultrasound wave device.

[0041] In some embodiments, the PIM 150 performs preliminary processing of the ultrasound echo data prior to relaying the data to the computer or console. In examples of such embodiments, the PIM 150 performs amplification, filtering, and/or aggregating of the data. In an embodiment, the PIM 150 also supplies high- and low-voltage DC power to support operation of the device 110 including circuitry associated with the ultrasound structures 120 and/or 130. The PIM 150 can be an isolation device as, in various surgical settings, patient safety requirements mandate physical and electrical isolation of the patient from one or more high voltage components.

[0042] The ultrasound processing system 160 receives imaging data (e.g., electrical signals representative of the ultrasound echo data) from the ultrasound structure 120 by way of the PIM 150. The ultrasound processing system 160 can include processing circuit, such as processor and/or memory. The ultrasound processing system 160 processes the data to reconstruct an image of the anatomy. The ultrasound processing system 160 outputs image data such

that an image of the anatomy **102**, such as a cross-sectional IVUS image of a vessel, is displayed on the monitor **170**. The ultrasound processing system **160** and/or the monitor **170** can include one or more user interface elements (e.g., touchscreen, keyboard, mouse, virtual buttons on a graphical user interface, physical buttons, etc.) to allow a medical professional to control the device **110**, including one or more parameters of the ultrasound structures **120**, **130**.

[0043] FIG. 2 is a schematic diagram of an ultrasound system **200** according to embodiments of the present disclosure. The ultrasound system **200** may illustrate similar aspects to the ultrasound system **100** as shown in FIG. 1. In particular, the ultrasound system **200** may have the same functionality as the ultrasound system **100** as well as additional features that are described in more detail with reference to FIGS. 2-7. The ultrasound system **200** may include an ultrasound device **210**, a connector **224**, a PIM **150**, an ultrasound processing system **160**, and a monitor **170**. The ultrasound device **210** may include a tip member **202** at the tip of a flexible elongate member **208** and a handle **220**. In some embodiments, the tip member **202** may be used for diagnostic purposes (i.e., imaging of anatomy) as well as therapeutic purposes (i.e., treating portions of anatomy). The flexible elongate member **208** may include a distal portion **204** and a proximal portion **206**. The distal end of the distal portion **204** may be attached to the tip member **202**. The proximal end of the proximal portion **206** may be attached to the handle **220**, for example, by a resilient strain reliever **212**. The handle **220** may be used for manipulation and/or manual control of the ultrasound device **210**. The tip member **202** may include an imaging core with ultrasound transducer elements and associated circuitry. The handle **220** may include actuators **216**, a clutch **214**, and other steering control components for steering the ultrasound device **210**. The steering may include deflecting the tip member **202** and the distal portion **204**, as described in greater details herein.

[0044] The handle **220** may be connected to the connector **224** via a second strain reliever **218** and a connection cable **222**. The connector **224** may be configured to provide suitable configurations for interconnecting the PIM **150**, ultrasound processing system **160**, and monitor **170** to the tip member **202**. In operation, a physician or a clinician may advance the flexible elongate member **208** into the anatomy of the patient, such as within a vessel or other structure within the heart of the patient. By controlling the actuators **216** and the clutch **214** on the handle **220**, the physician or clinician can steer the flexible elongate member **208** to a position near an area of interest to be imaged. For example, a first actuator **216A** may deflect the tip member **202** and the distal portion **204** in a left-right plane and a second actuator **216B** may deflect the tip member **202** and the distal portion **204** in an anterior-posterior plane. The clutch **214** may include a locking mechanism to lock the positions of the actuators **216**, and in effect, lock the deflection of the flexible elongate member **208** while the tip member **202** is used to image or treat the area of interest.

[0045] In some embodiments, the tip member **202** may be used for diagnostic processes and therapeutic processes. A diagnostic process may include imaging areas of interest by activating the ultrasound transducer elements on the tip member **202** to produce ultrasonic energy. This ultrasound energy may be referred to as ultrasound signals which may be directed into a portion of the anatomy from the transducer assembly. A portion of the ultrasonic energy from the signal

may be reflected by the area of interest and the surrounding anatomy as ultrasound echoes. These ultrasound echoes may be received by the ultrasound transducer elements, as shown in more detail with reference to FIG. 4. The connector **224** may transfer the received echo signals to the PIM **150** and/or ultrasound processing system **160** where an ultrasound image based on the received echo signals is reconstructed and displayed on the monitor **170**. In some embodiments, the ultrasound system **200** is used to generate two-dimensional and three-dimensional images. In some examples, the ultrasound system **200** may be used for generating X-plane images at two different viewing directions perpendicular to each other. In some embodiments, the PIM **150** may control the activation of the ultrasound transducer elements and the reception of the echo signals to generate various images from different viewpoints.

[0046] The tip member **202** may also be used for treating areas of interest within the anatomy of the patient. For example, the tip member **202** may be used to transmit ultrasound energy for treatment purposes, such as preparing areas of interest for the introduction of medication or for ultrasound cavitation. As discussed below, the ultrasound signals used for diagnostic purposes may be transmitted from a different section of the tip member **202** than the ultrasound signals used for therapeutic purposes.

[0047] In some embodiments, a button, toggle, or switch **211** is disposed on the handle **220** and may be used to toggle between a diagnostic functionality and a therapeutic functionality for the tip member **202**. For example, an operator may activate the switch **211** to a “diagnostic mode” in which the tip member **202** transmits ultrasound signals and receives ultrasound echoes for diagnostic purposes. The operator may then activate the switch to a “therapeutic mode” in which the tip member **202** transmits ultrasound signals for therapeutic purposes, without receiving ultrasound echoes. In other embodiments, the tip member **202** may be used for diagnostic and therapeutic purposes simultaneously, such as transmitting ultrasound signals to treat an area of interest while simultaneously imaging the area of interest.

[0048] The ultrasound system **200** may be utilized in a variety of applications such as transeptal punctures, left atrial appendage closures, atrial fibrillation ablation, and valve repairs and can be used to image vessels and structures within a living body. Although the ultrasound system **200** is described in the context of intraluminal imaging procedures, the ultrasound system **200** may be suitable for use with any catheterization procedure, e.g., ICE. In addition, the tip member **202** may include any suitable physiological sensor or component for diagnostic, treatment, and/or therapy. For example, the tip member **202** may include imaging components, an ablation component, a cutting component, a morcellation component, a cavitation component, a pressure-sensing component, a flow-sensing component, a temperature-sensing component, and/or combinations thereof.

[0049] FIG. 3 is a perspective view of the tip member **202** described above with respect to FIG. 2. The tip member **202** may include an imaging core **262** that is positioned at a distal portion of the tip member **202**. The imaging core **262** may be coupled to an electrical cable **266** via an electrical interconnection **264**. The electrical cable **266** may extend through the alignment portion **244** and the interface portion

**246** of the inner cavity **250**. The electrical cable **266** can further extend through the flexible elongate member **108** as shown in FIG. 1.

[0050] The configuration and structure of the tip member **202** may provide several benefits. The benefits include providing safe and easy delivery of the catheter, providing improved tensile strength for steering and navigation, providing consistent alignment, and providing improved image quality. For example, the outer geometry of the tip member **202** may be configured to provide smooth surfaces and smooth edges with small radii. The smooth edges reduce friction when the tip member **202** traverses a vessel during insertion. The smooth surfaces prevent tears and/or damages to tissue structures during the insertion. In addition, the smooth edges and smooth surfaces can facilitate crossing of a septum or other anatomical feature during a catheterization procedure. In some embodiments, the material type and the wall thickness of the tip member **202** are selected to minimize acoustic distortion, attenuation, and/or reflection. The internal geometry of the tip member **202** is configured to facilitate alignment during manufacturing. The tip member **202** can also include other features, for example, a guidewire lumen, one or more holes, or other geometry to accommodate additional devices or features such as pressure sensors, drug delivery mechanisms, and/or any suitable interventional features.

[0051] The imaging core **262** may include a transducer array **261** including one or more transducers as well as a controller **304** connected to the transducer array **261**. The transducer array **261** may be configured to transmit ultrasound signals into the anatomy of the patient. In some embodiments, the transducer array **261** operates with intravascular ultrasound (IVUS) modality and is configured to provide data for IVUS images. In some embodiments, the transducer array **261** is configured to produce IVUS virtual histology (VH) images. Detecting and characterizing plaque using IVUS with VH are described in, for example, U.S. Pat. No. 6,200,268 entitled "VASCULAR PLAQUE CHARACTERIZATION" issued Mar. 13, 2001 with D. Geoffrey Vince, Barry D. Kuban and Anuja Nair as inventors, U.S. Pat. No. 6,381,350 entitled "INTRAVASCULAR ULTRASONIC ANALYSIS USING ACTIVE CONTOUR METHOD AND SYSTEM" issued Apr. 30, 2002 with Jon D. Klingensmith, D. Geoffrey Vince and Raj Shekhar as inventors, U.S. Pat. No. 7,074,188 entitled "SYSTEM AND METHOD OF CHARACTERIZING VASCULAR TISSUE" issued Jul. 11, 2006 with Anuja Nair, D. Geoffrey Vince, Jon D. Klingensmith and Barry D. Kuban as inventors, U.S. Pat. No. 7,175,597 entitled "NON-INVASIVE TISSUE CHARACTERIZATION SYSTEM AND METHOD" issued Feb. 13, 2007 with D. Geoffrey Vince, Anuja Nair and Jon D. Klingensmith as inventors, U.S. Pat. No. 7,215,802 entitled "SYSTEM AND METHOD FOR VASCULAR BORDER DETECTION" issued May 8, 2007 with Jon D. Klingensmith, Anuja Nair, Barry D. Kuban and D. Geoffrey Vince as inventors, U.S. Pat. No. 7,359,554 entitled "SYSTEM AND METHOD FOR IDENTIFYING A VASCULAR BORDER" issued Apr. 15, 2008 with Jon D. Klingensmith, D. Geoffrey Vince, Anuja Nair and Barry D. Kuban as inventors and U.S. Pat. No. 7,463,759 entitled "SYSTEM AND METHOD FOR VASCULAR BORDER DETECTION" issued Dec. 9, 2008 with Jon D. Klingensmith, Anuja Nair, Barry D. Kuban and D. Geoffrey Vince,

as inventors, the teachings of which are hereby incorporated by reference herein in their entireties.

[0052] In some embodiments, the controller **304** is a micro-beam-forming integrated circuit (IC). The controller may directly control the transmission and reception of ultrasound signals by the transducer array, including switching between diagnostic and therapeutic modes. In some embodiments, the transducer array **261** is mounted directly on the controller **304** and is electrically connected to the transducer array **261**. The controller **304** may be disposed on a core element with a round shape. In some embodiments, elements of the transducer array **261** may be attached to the controller **304** by flip-chip mounting or grown directly on top of the controller **304**. In some embodiments, an electrical cable **266** may be terminated directly to the controller **304**, or may be terminated to an interposer **310** of suitable material such as a rigid or flexible printed circuit assembly. The interposer **310** may then be connected to the controller **304** via any suitable means such as wire bondings **320**.

[0053] In some embodiments, the transducer array **261** includes a two-dimensional, rectangular matrix array with a number of transducer elements. The transducer array **261** may also include one or more one-dimensional array components. The transducer array **261** may include materials such as PZT, PZT composites, CMUT, PMUT, single crystals, or any combination of these. The transducer elements of the transducer array **261** may be piezoelectric or micromachined ultrasonic transducer (MUT) elements. The transducer array **261** may include an active area in which signals are transmitted and received by transducer elements. The transducer array **261** may also include inactive areas such as the underside of the array or edges of the array where mounting device are disposed. In some embodiments, the transducer array **261** comprises 800 or more transducer elements. In other embodiments, the transducer array **261** may include between 32 and 1000 transducer elements. For example, the transducer array can include 32, 64, 128, 256, 512, 640, 768, or any other suitable number of transducer elements. For example, a one-dimensional array may have 32 transducer elements and a two-dimensional array may have 32, 64, or more transducer elements. In other embodiments, the transducer array **261** may have other shapes, such as square, elliptical, circular, or irregular shapes. The shape of the active area of the transducer array **261** may include multiple alternating columns and rows and/or concentric circles or other shapes.

[0054] In some embodiments, the tip member **202** may include a transducer array **261** connected to the PIM **150** with fewer than 30 wires that include signal lines, power lines, and control lines. In some embodiments, the 30 wires or less include 6-12 signal lines, preferably include 8 signal lines. In other embodiments, the number of signal lines is between 10 and 20, for example, 12 signal lines, 16 signal lines, or any other suitable number of signal lines.

[0055] In some examples, the transducer array **261** is configured for two-dimensional and three-dimensional imaging. For example, a one-dimensional portion of the transducer array **261** may be used to generate two-dimensional images while a two-dimensional portion of the transducer array **261** may be used to generate two- or three-dimensional images.

[0056] In some embodiments, the transducer array **261** may similar to the ultrasound transducer array of structure **130** as shown in FIG. 1. In particular, the transducer array

**261** may be configured to generate signals within a tunable range of 1 kHz and 70 MHz. In some embodiments, the first segment **263** of the transducer array **261** may be configured to provide signals for diagnostic procedures and the second segment **265** may be configured to provide signals for therapeutic procedures. For example, the first segment **263** may be configured to transmit ultrasound signals at an area of interest and receive reflected ultrasound echoes. The first segment **263** may be connected to processing systems (such as the ultrasound processing system **160** as shown in FIGS. 1 and 2) via the electrical cable **266** such that the reflected ultrasound echoes can be processed into one or more images of the area of interest. The second segment **265** may be configured to transmit ultrasound signals for therapeutic purposes and may not be configured to receive reflected ultrasound echoes.

[0057] In some embodiments, the first segment **263** is populated with a high resonant frequency material and the second segment **265** is populated with a low resonant frequency material. In some embodiments, these materials include different compositions. In other embodiments, these materials include the same composition but the voltage applied to the first segment **263** is not the same as the voltage applied to the second segment **265**.

[0058] Although in the example of FIG. 3 the transducer array **261** includes only a first segment **263** and a second segment **265**, in other embodiments, more segments may be included. For example, the transducer array **261** may include 1, 3, 4, 5, 6 or other numbers of segments which may be used to transmit ultrasound signals with different ranges of frequencies.

[0059] FIG. 4 is a schematic diagram **400** illustrating the beam-forming of an ultrasound system according to embodiments of the present disclosure. Beam-forming of ultrasound signals can occur before ultrasound signals are transmitted by the transducer array **261** or after the ultrasound echoes are received by the transducer array **261**. Embodiments of the present disclosure, such as the beam-forming applications of the present disclosure, may include features similar to those described in U.S. Provisional App. No. \_\_\_\_\_, filed \_\_\_\_\_ (Atty Dkt. No. 2016PF01099/44755.1630PV01), U.S. Provisional App. No. \_\_\_\_\_, filed \_\_\_\_\_ (Atty Dkt. No. 2016PF01087/44755.1632PV01), U.S. Provisional App. No. 62/401,464, filed Oct. 29, 2016, U.S. Provisional App. No. 62/401,686, filed Oct. 29, 2016, and/or U.S. Provisional App. No. 62/401,525, filed Oct. 29, 2017, the entireties of which are hereby incorporated by reference herein.

[0060] The diagram **400** includes the tip member **202** including an array of transducer elements **302** and a micro-beam-former IC **305**. In some embodiments, the array of transducer elements **302** forms a portion of the transducer array **261**. The micro-beam-former IC **305** may be part of the controller **304**, or alternatively, a separate component that this connected to the transducer array **261**. The micro-beam-former IC **305** may be coupled to the array of transducer elements **302** at the distal portion of the ultrasound device **210**. As shown, the array of transducer elements **302** is divided into one or more subarrays of transducer elements **420**. For example, the array of transducer elements **302** may be divided into nine subarrays of transducer elements **420** that each has 16 transducer elements arranged as 4 by 4. In some embodiments, the first segment **263** and second segment **265** may include one or more subarrays of transducer elements **420**.

[0061] The micro-beam-former IC **305** may include a plurality of microchannels **430** that may each separately beam-form the signals received from transducer elements of a corresponding subarray of transducer elements **420**. As shown in FIG. 4, for example, the microchannels **430** each comprise a delay for alignment of the signals received from the transducer elements of a subarray of transducer elements **420**. As shown, the microchannels delay lines **430** of each subarray of transducer elements **420** may be separately coupled to one coaxial cable **410** such that the received signals of each subarray of transducer elements **420** are transferred through a separate channel, e.g., coaxial cable **410**, to the ultrasound processing system **160**.

[0062] In some embodiments, the micro-beam-former IC **305** is configured to control the array of transducer elements **302**. For example, the micro-beam-former IC **305** may control the activation of particular transducer elements of the array of transducer elements **302** as well as controlling the angle at which ultrasound signals are transmitted by the transducer elements. The micro-beam-former IC **305** may also control the frequency of transmitted ultrasound signals. Furthermore, the micro-beam-former IC **305** may perform beam forming for a plurality of transducer elements of each of the subarrays of transducer elements **420** of the array of transducer elements **302**.

[0063] In some embodiments, the tip member **202** includes an electrical cable **266** that includes two or more signal lines that are coupled to the micro-beam-former IC **305**. Each of signal lines is associated with one of the subarrays of transducer elements **420** of the array of transducer elements **302** to transfer beam formed imaging signals of the associated subarray. For example, each signal line corresponds to a particular subarray of transducer elements **420** and is configured to receive the beam-formed signals specific to the corresponding subarray.

[0064] In some embodiments, the electrical cable **266** further includes one or more power lines for feeding power to the micro-beam-former IC **305** and one or more control lines for communicating control signals to the micro-beam-former IC **305**.

[0065] In some embodiments, the micro-beam-former IC **305** includes multiple microchannel delay lines **430**. The microchannel delay lines **430** are used to perform the beam forming for the plurality of transducer elements of each of the two or more subarrays of transducer elements **420**. In some examples, the multiple microchannel delay lines **430** include at least one of a charge coupled device, an analog random access memory, or a tapped analog delay line. In some examples, the first beam-formed signals and the second beam-formed signals are transmitted via a connection cable to the ultrasound processing system **160** of FIGS. 1 and 2.

[0066] FIG. 5 is a diagrammatic schematic view **500** of a tip member **202** of an ultrasound system **200** within the anatomy **102** of a patient. As discussed above, the tip member **202** may include a transducer array **261** including a first segment **263** and a second segment **265**. In some embodiments, the first segment **263** of the imaging core **262** is configured to transmit signals **401** into the anatomy **102** for diagnostic purposes. These signals may reflect off various formations in the anatomy and ultrasound echoes **405** may be produced. The first segment **263** may also be configured to receive the ultrasound echoes **405** associated with the signals **401**. These ultrasound echoes may be

transmitted to processing systems (such as the ultrasound processing system 160 as shown in FIGS. 1 and 2) to produce images of the anatomy 102.

[0067] The second segment 265 may be configured to transmit signals 403 for therapeutic procedures. For example, the signals 403 may be transmitted to treat a portion of the anatomy 102, such as an occlusion 106 with a vessel 104 as shown in FIG. 4. The signals 403 may create micro fractures 407 in the occlusion 106, which may aid in treating the occlusion 106. The signals 401, 403 may be transmitted from different angles without moving the tip member 202. In some embodiments, the micro fractures 407 may weaken or soften the occlusion 106 which may be entirely removed in another procedure.

[0068] FIG. 6 is another diagrammatic schematic view 600 of a tip member 202 within the anatomy 102 of a patient. The transducer array 261 on the tip member 202 may be configured to transmit ultrasound signals from different areas of the transducer array 261. Furthermore, the transducer array 261 may be configured to allow control over various parameters of the pulses, such as frequency, pulse amplitude, pulse length, signal pattern, and transmission angle. These parameters may be controlled by an automated process or a user controlled process. This may allow the transducer array 261 to image and provide optimized treatment to various portions of the anatomy without moving the tip member.

[0069] In some embodiments, the first segment 263 and the second segment 265 of the transducer array 261 may be configured for transmitting ultrasound signals at different angles. In the example of FIG. 6, ultrasound signals 530 are transmitted with an angle  $\alpha 1$ . The ultrasound signals are directed at a first area of interest. Ultrasound signals 532 may be transmitted with angle  $\alpha 2$  and may be directed at a second area of interest. Angle  $\alpha 2$  may be different than  $\alpha 1$  and ultrasound signals 532 may be transmitted from a different location on the transducer array 261 than ultrasound signals 530. In some embodiments, the ultrasound signals 530, 532 may be used for cavitation and may create micro fractures 507, 509 in the anatomy. Since the ultrasound signals 530, 532 are transmitted at different angles, the micro fractures 507, 509 may have different orientations. This may allow an operator make various angular ultrasound cuts into areas of interest (such as calcification or plaque) without moving the tip member 202. The transducer array 261 may also provide frequency and power optimization to control the depth of cuts which may allow for precise cavitation procedures. Ultrasound signals may be transmitted with varying amplitudes, widths, and shapes by varying the ultrasound transducer elements used to transmit the ultrasound signals. For example, a controller may be used to activate a large number of transducer elements in a circular pattern which may result in the transmission of a large cylindrical or conical signal pattern. Alternatively, the controller may be used to activate a small number of ultrasound elements in a rectangular pattern which may result in the transmission of a small, rectangular or pyramidal signal pattern. The strength and frequency of ultrasound signals in these patterns may also be varied.

[0070] FIG. 7 provides a flow diagram illustrating a method 700 of transmitting ultrasound signals. As illustrated, the method 700 includes a number of enumerated steps, but embodiments of the method 700 may include additional steps before, after, and in between the enumerated

steps. In some embodiments, one or more of the enumerated steps may be omitted, performed in a different order, or performed concurrently. The method 700 may be performed using any of the systems and devices referred to in FIGS. 1-6.

[0071] At step 702, the method 700 may include placing an ultrasound device in anatomy of a patient. The ultrasound device may be the ultrasound device 210 including the tip member 202 as shown in FIG. 2. In other embodiments, the ultrasound device may be a rotational, flat phased array, or circumferential phased array device. In some embodiments, an operator may use a handle such as handle 220 as shown in FIG. 2 to manipulate an elongate flexible member of the ultrasound device 210 to an area of interest in the anatomy, such as a vessel or chamber of the heart. The ultrasound device may be used to image the anatomy of the patient during the manipulation of the ultrasound device, such as to aid the operator in maneuvering through the vasculature of the patient.

[0072] At step 704, the method 700 may include transmitting a first ultrasound signal with a first portion of a transducer array within the ultrasound device. The first ultrasound signal may be transmitted while the ultrasound device is in a diagnostic mode. In some embodiments, the transducer array is disposed on a tip member on a distal portion of the ultrasound device. In some embodiments, the first portion of the transducer array includes a number of transducer elements which may be controlled independently. The first ultrasound signal may be directed at various angles to a portion of the anatomy without physically moving the tip member. The first ultrasound signal (and subsequent signals) may be sent with a tunable wave range to optimize visualization of the anatomy. For example, an operator may be able to change the frequency of each signal based on the measured anatomy and the desired imaging or therapeutic effects of the signal. The first ultrasound signal may be reflected off the anatomy in the form of ultrasound echoes, some of which may travel back toward the transducer array.

[0073] At step 706, the method 700 may include receiving ultrasound echoes reflected from the anatomy and associated with the first ultrasound signal. The ultrasound echoes may be received by the same portion of the transducer array that transmitted the first ultrasound signal. In some embodiments, the data from the ultrasound echoes may be analyzed by a controller within the ultrasound device (such as adjacent to the transducer array) or communicated by a cable or other means to a processing device outside the patient. In some embodiments, the transducer array may be an intravascular ultrasound (IVUS) array that is configured to transmit and receive IVUS signals.

[0074] At step 708, the method 700 may include generating an image of the anatomy based the received ultrasound echoes. The image of the anatomy may be a two- or three-dimensional image of the anatomy. In some embodiments, the image is an IVUS VH image. The image of the anatomy may be displayed on a display device such as a computer monitor. The image may be accompanied by measured data, such as data on the diameter, calcification, and density of vessels and other anatomical structures. In some embodiments, the age and hardness of calcium may be measured by the system through analysis of the images of the anatomy.

[0075] At step 710, the method 700 may include identifying a treatment plan based on image of the anatomy. In

some embodiments, the image of the anatomy may be analyzed by the system automatically to detect problems (i.e., calcification, occlusions, plaques, abnormalities in the anatomy, etc.). The system may be used to identify a treatment plan based on problems in the image. In some embodiments, the treatment plan may include a therapeutic procedure to be performed by the ultrasound device.

[0076] At step 712, the method 700 may include transmitting a second ultrasound signal with a second portion of the transducer array according to the treatment plan. The second ultrasound signal may be transmitted while the ultrasound device is in a cavitation or therapeutic mode. The mode of the ultrasound device may be switched by an operator, such as by using the switch 211 as shown in FIG. 2. The second portion of the transducer array may be adjacent to the first portion and may include a number of transducer elements. In some embodiments, the second portion is configured to transmit ultrasound signals but not receive ultrasound signals. In some embodiments, an optical frequency, pulse amplitude, and pulse length of the second ultrasound signal may be determined by a controller based on the treatment plan identified in step 710. The second ultrasound signal may have a frequency lower than that of the first ultrasound signal. In some embodiments, the second ultrasound signal is transmitted to perform a therapeutic procedure such as creating micro fractures in the anatomy and/or treating the anatomy in preparation for delivery of a drug. The second signal may be transmitted at varying angles or frequencies. The second portion of the transducer array may be used to transmit other ultrasound signals, such that a pattern of fractures with different angles may be produced in a portion of the anatomy without moving the transducer array. In some embodiments, step 712 may be repeated to carry out one or more therapeutic procedures. In particular, the ultrasound device may be switched to different modes and transmit different ultrasound signals. For example, a second ultrasound signal may be transmitted to prepare a vessel for a treatment. A third ultrasound signal (or a further series of ultrasound signals) may then be transmitted to perform the treatment, such as creating micro fractures within an occlusion.

[0077] At step 714, the method 700 may optionally include imaging the anatomy with the transducer array to determine the effectiveness of the treatment plan. In some embodiments, the mode of the ultrasound device may be switched from therapeutic mode to diagnostic mode for this step. In some embodiments, the first portion may be used to transmit another ultrasound signal and receive the reflected ultrasound echoes to determine if the desired effect has been achieved. In some embodiments, the ultrasound device may be used to image anatomy after treatment to identify further problem areas or conditions (such as identifying emboli in the anatomy after a procedure). The steps of method 700 may be repeated to identify treatment plans, carry out the treatment plans, and determine the effectiveness of treatment. In some embodiments, the ultrasound device may be changed from diagnostic to therapeutic modes throughout the procedures. Other therapeutic procedures may also be used to treat the patient during and after these steps, such as dilating diseased areas using a balloon catheter, placing correctly sized stents, and delivering drugs.

[0078] The systems, devices, and methods of the present disclosure can include features described in U.S. Provisional App. No. \_\_\_\_\_ (Atty. Dkt. No. 2017PF02284/44755.

1807PV01), U.S. Provisional App. No. \_\_\_\_\_ (Atty. Dkt. No. 2017PF02285/44755.1808PV01), filed on an even date herewith, U.S. Provisional App. No. \_\_\_\_\_ (Atty. Dkt. No. 2017PF02287/44755.1809PV01), filed on an even date herewith, and/or U.S. Provisional App. No. \_\_\_\_\_ (Atty. Dkt. No. 2017PF02289/44755.1811PV01), filed on an even date herewith, the entireties of which are hereby incorporated by reference herein.

[0079] Persons skilled in the art will recognize that the apparatus, systems, and methods described above can be modified in various ways. Accordingly, persons of ordinary skill in the art will appreciate that the embodiments encompassed by the present disclosure are not limited to the particular exemplary embodiments described above. In that regard, although illustrative embodiments have been shown and described, a wide range of modification, change, and substitution is contemplated in the foregoing disclosure. It is understood that such variations may be made to the foregoing without departing from the scope of the present disclosure. Accordingly, it is appropriate that the appended claims be construed broadly and in a manner consistent with the present disclosure.

What is claimed is:

1. An ultrasound system, comprising:  
an ultrasound device, comprising:

a flexible elongate member configured to be positioned within anatomy of a patient, the flexible elongate member comprising a proximal portion and a distal portion; and

an ultrasound transducer array positioned at the distal portion of the flexible elongate member, wherein the ultrasound transducer array includes a plurality of transducer elements arranged in a first segment and a second segment, wherein the first segment is configured to emit a first ultrasound signal with a first frequency and the second segment is configured to emit a second ultrasound signal with a second frequency different than the first frequency.

2. The ultrasound system of claim 1, wherein the second frequency is lower than the first frequency.

3. The ultrasound system of claim 1, wherein the first frequency is between 10 MHz and 70 MHz and the second frequency is between 1 kHz and 5 MHz.

4. The ultrasound system of claim 1, wherein the ultrasound transducer array is a two-dimensional array, wherein the first segment is disposed on a first portion of the two-dimensional array and the second segment is disposed on a second portion of the two-dimensional array adjacent the first portion.

5. The ultrasound system of claim 1, wherein the first segment comprises a high resonant frequency material and the second segment comprises a low resonant frequency material.

6. The ultrasound system of claim 1, wherein the ultrasound transducer array comprises at least one of PZT, CMUT, or PMUT.

7. The ultrasound system of claim 1, wherein the first segment of the ultrasound transducer array is configured to receive ultrasound echoes reflected from the anatomy and associated with the first ultrasound signal.

8. The ultrasound system of claim 7, further comprising:  
a computing device in communication with the ultrasound transducer array and configured to produce an ultrasound image based on the received ultrasound echoes.

9. The ultrasound system of claim 1, further comprising a controller disposed at the distal portion of the flexible elongate member and in communication with the ultrasound transducer array.

10. The ultrasound system of claim 1, wherein the ultrasound transducer array is configured to direct the second ultrasound signal to a first portion of anatomy and a second portion of anatomy different from the first portion of anatomy without moving the ultrasound transducer array.

11. The ultrasound system of claim 1, wherein the ultrasound device further comprises a switch to selectively switch between transmitting signals with the first segment and the second segment.

12. The ultrasound system of claim 1, wherein the ultrasound device further comprises a substrate including electrical conductors connected to the ultrasound transducer array, the electrical conductors configured to selectively switch between transmitting signals with the first segment and the second segment.

13. The ultrasound system of claim 1, wherein the flexible elongate member comprises a first cable configured to control transmission of signals of the first segment and a second cable configured to control transmission of signals of the second segment.

14. The ultrasound system of claim 1, wherein the flexible elongate member comprises a third cable configured to control transmission of signals of both the first segment and the second segment.

15. A method of transmitting ultrasound signals, comprising:

transmitting, with a first segment of an ultrasound transducer array of an ultrasound device positioned within

anatomy of a patient, a first ultrasound signal with a first frequency to image an area of interest of the anatomy;

receiving, with the first segment of the ultrasound transducer array, ultrasound echoes reflected from the anatomy and associated with the first ultrasound signal; and

transmitting, with a second segment of the ultrasound transducer array, a second ultrasound signal with a second frequency to an area of interest within the anatomy.

16. The method of claim 15, further comprising generating, with a controller, an image of the area of interest based on the second ultrasound signal.

17. The method of claim 16, further comprising transmitting, with the second segment of the ultrasound transducer array, the second ultrasound signal to perform a therapeutic procedure based on the image of the area of interest.

18. The method of claim 17, wherein the therapeutic procedure comprises an ultrasound cavitation procedure that includes forming ultrasound cuts into calcification within the anatomy.

19. The method of claim 18, wherein the therapeutic procedure comprises preparing a portion of the anatomy for delivery of medication.

20. The method of claim 15, further comprising directing transmission of the second ultrasound signal from the second segment to a first portion of the area of interest and directing transmission of a third ultrasound signal from the second segment to a second portion of the area of interest different than the first portion of the area of interest without moving the ultrasound transducer array.

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专利名称(译)	心内治疗和诊断超声设备		
公开(公告)号	<a href="#">US20190053783A1</a>	公开(公告)日	2019-02-21
申请号	US15/998480	申请日	2018-08-15
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
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优先权	62/545927 2017-08-15 US		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

摘要(译)

提供了用于使用超声进行诊断和治疗过程的系统，方法和设备。超声信号可以由位于患者的解剖结构内的超声装置中的超声换能器发送和/或接收。超声换能器可以布置成阵列，使得阵列的第一段配置成发送超声脉冲并接收超声回波用于诊断过程，并且阵列的第二段配置成发送超声脉冲用于治疗过程。接收的超声回波可用于生成解剖结构的二维或三维图像。

