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- (71) Applicant (for all designated States except US): **ESI, INC.** [US/US]; 2915 Everest Lane North, Plymouth, MN 55447 (US).
- (72) Inventors; and
- (75) Inventors/Applicants (for US only): **PRAGER, Thomas, C.** [US/US]; 1819 N. Rainbow Ranch Road, Wimberley, TX 78676 (US). **BURBA, Thomas, A.** [US/US]; 2915 Everest Lane North, Plymouth, MN 55447 (US). **HARDTEN, David, R.** [US/US]; 2515 Kelly Avenue, Orono, MN 55331 (US). **RYDER, William, T.** [US/US]; 7900 Bavaria Road, Victoria, MN 55386 (US).
- (74) Agent: **JAEGER, Hugh, D.**; Hugh D. Jaeger, P.A., 150 Lake Street West, Suite 106, P.O. Box 432, Wayzata, MN 55391-0432 (US).
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(54) Title: IMMERSION BAG SYSTEM FOR USE WITH AN ULTRASOUND PROBE

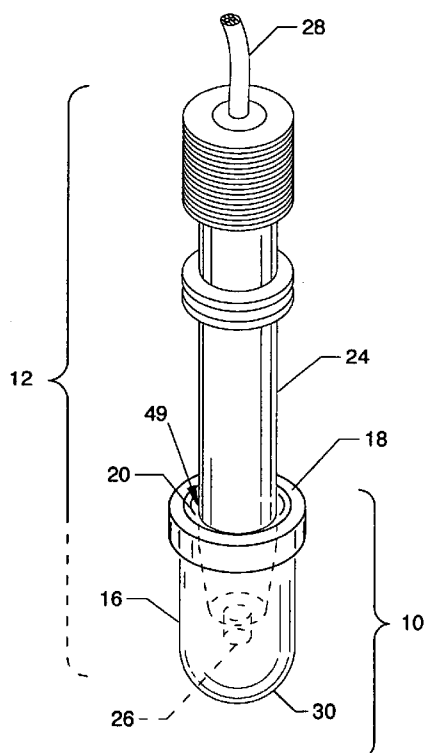


FIG. 1

(57) Abstract: An immersion bag system for use with an ultrasound probe to overcome near field artifact includes a flexible thin wall thickness immersion bag with an attached flexible collar having an integral internal seal. The immersion bag contains a gel or other ultrasound transmission medium and is sealingly and removably attached by a mutually formed probe/seal valve to the tip end of an ultrasound probe. The immersion bag is able to conform to a cornea, as well as to other surfaces, whether flat or irregular, thereby enabling an ultrasound probe to be used easily on such surfaces. An ultrasound probe in use with the immersion bag system is maintained at a distance above the contact surface of the immersion bag and is positionable about the vertical axis while the immersion bag maintains stationary conformal contact with the structure against which it is in contact.

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IMMERSION BAG SYSTEM FOR USE WITH AN ULTRASOUND PROBE

CROSS REFERENCES TO RELATED APPLICATIONS

5 **[0001]** This patent application is a continuation-in-part of Application No. 11/356,873 entitled "Immersion Bag System for Use With an Ultrasound Probe" filed on February 17, 2006, which is pending.

BACKGROUND OF THE INVENTION

FIELD OF THE INVENTION

10 **[0002]** The present invention primarily applies to the medical device field, and more particularly, pertains to an immersion bag system having an immersion bag of acoustically invisible material and a flexible sealing collar which when engaged with a body of an ultrasound probe forms a deformable valve which can also serve as
15 a pressure release valve. The bag encapsulates the distal end of and is incorporated into use with an ultrasound probe. The immersion bag system, suitable for containment of a gel or other aqueous medium of any suitable viscosity, overcomes near field artifact allowing the examination of shallow anatomical structures. In operation of the invention the distal end of the ultrasound probe, including a
20 transducer, is immersed in the gel or other aqueous medium.

[0003] Definition of "near field artifact". Typically, a stationary ultrasound probe passes or scans over just 10 degrees during ultrasound scanning, but by physically moving the ultrasound probe transducer head back and forth via a motor or other suitable means, a range of 120 degrees can be examined. However, when the
25 ultrasound probe transducer head moves, the consequential pulsating of the ultrasound waves collide with one another creating interference which results in an acoustic dead zone. Structures contained within this dead zone cannot be visualized and this is termed "near field artifact". Therefore, examining shallow/superficial tissue with a moving ultrasound probe, anatomical structures within the near field
30 artifact cannot be visualized because of the near field artifact.

[0004] This invention has medical and industrial applications by enhancing the ability to exam shallow/superficial structures amenable to ultrasound evaluation. Medical and industrial sonogram examinations may be improved by this method of overcoming near field artifact (defined previously). This includes:

- 5 a. anterior ocular structures, e.g., the cornea, iris, iris angle, lens, ciliary body;
- b. skin lesions, e.g., skin cancers, cysts, or neoplasms;
- c. vascular structure/flow assessment; and,
- d. industrial monitoring of flow characteristics in tubing.

10

DESCRIPTION OF THE PRIOR ART

[0005] Ultrasound scans of the eye or other areas of the body are performed using an ultrasound probe and a coupling medium placed between the ultrasound probe tip and the surface of the area being scanned during examination. The medium, such as a gel or other less viscous aqueous medium, allows for the transmission of ultrasound waves between the ultrasound probe and through human tissue or other structures. To reduce or eliminate the near field artifact, the ultrasound probe tip and the superficial structures under examination, such as blood vessels or anterior aspects of the eye, must be separated at a distance from each other and not in direct contact.

20 A common method of accomplishing this is to use a cylindrical shaped cup that is open on both ends which can contain gel or other suitable aqueous medium and which is placed over the area of the examining surface. The use of an open cylindrical shaped cup requires that the operator fill the cup with gel or other suitable aqueous medium. An excessive filling of the cup may result in undesirable overrun

25 of the cup when the tip of the ultrasound probe is introduced therein and the coupling gel, e.g., methylcellulose, may be an eye irritant. An insufficient filling of the cup results in less than desirable ultrasound scan examination because the near field artifact opaque zone cannot be overcome, thus preventing an examination of the structure under study. More importantly, if a cylinder with an open bottom, i.e., a

30 cup, is used, the gel or other suitable aqueous medium must be at a depth to allow a

sufficient probe distance from the exam surface to overcome the opaque zone created by the near field artifact. The acoustically transparent immersion bag of the present invention eliminates the need for tedious and correct medium filling to a proper level and provides for ultrasound probe separation from the exam surface to overcome the

5 near field artifact, thereby allowing visualization of superficial structures of the body and/or other structures during the ultrasound exam. Further, with the open cylinder technique, the ultrasound probe may readily come into contact with the sensitive cornea of the eye. Transmission of microorganisms is possible with the open cylinder technique as sterilization of the ultrasound probe is difficult and time consuming.

SUMMARY OF THE INVENTION

[0006] The general purpose of the present invention is the creation of an immersion bag system, portions of which are fabricated from acoustically invisible material such as polyethylene, hydrophilic plastic or other suitable thin flexible material which encapsulate the tip of an ultrasound probe. The immersion bag, suitable for containment of a gel or other aqueous medium, overcomes near field artifact thereby allowing the examination of shallow/superficial structures. The immersion bag is permanently attached to a flexible collar which seals around the distal end of the closely associated ultrasound probe outer case. When the ultrasound probe is inserted into the immersion bag, the immersion bag becomes a cylindrical or other shaped bag with positive internal pressure. During an examination, this internal positive pressure in the immersion bag inhibits the ultrasound probe from moving forward and contacting nearby structures, such as the cornea of the eye. Also, the ultrasound probe is encapsulated by the sterile immersion bag, thus reducing the likelihood of transmission of microorganisms from patient-to-patient.

[0007] According to one or more embodiments of the present invention, there is an immersion bag system having a flexible compressible collar and an immersion bag attached thereto which is collectively used to encapsulate the tip portion of an ultrasound probe. The immersion bag system, which can contain preloaded or site loaded gel or other suitable aqueous medium, engages and surrounds the distal end of the ultrasound probe to an adequate depth to overcome the near field artifact. The mutually secured immersion bag and flexible collar are comprised of flexible and pliable materials. Specifically, the flexible collar includes an open end for inserting the ultrasound probe and also includes an integral flexible seal. The acoustically invisible immersion bag is attached to the flexible collar, each having annular qualities. A lip of the immersion bag is permanently secured within the flexible collar by a rigid or semi-rigid capture ring or by other suitable attachment methods. Additionally, the flexible seal, which is integral to the flexible collar, frictionally engages the body of the ultrasound probe upon introduction therein to form a deformable probe/seal valve therebetween which is watertight. By inserting the

ultrasound probe into the partially liquid filled immersion bag, slight hydraulic (internal) pressure is created effectively eliminating bag material wrinkles, which is a source of acoustical artifact, thereby forming and ensuring a smooth surface shape of the immersion bag. A consequence of positive internal hydraulic pressure is the resistance created on the ultrasound probe when moved into the immersion bag, thereby minimizing the possibility of physical contact by the ultrasound probe with the superficial structures under examination, such as the sensitive cornea of the eye. Canting or otherwise reorienting of the ultrasound probe with respect to the flexible seal and flexible collar can deformingly open the probe/seal valve to lower internal bag air pressure or can release excess gel or aqueous medium from the immersion bag. To maintain immersion bag shape and integrity, venting can be provided by one or more self-sealing valves to release air, excess gel, or other excess aqueous medium from the immersion bag during insertion of the ultrasound probe or during operation of the invention in order to maintain positive internal immersion bag pressure. The internal pressure and bag tension also provides resistance and tactile feedback to the operator when moving the ultrasound probe toward the immersion bag end. This internal immersion bag pressure and bag tension offsets the ultrasound probe tip from the examined surface, thus overcoming near field artifact, and due to resistance, maintains spacing between the transducer and the immersion bag end. The end of the immersion bag is conformally reshaped to mirror and envelop the examining surface upon contact. Moreover, being flexible and pliable, the immersion bag conforms to irregularly shaped anatomical areas, such as, but not limited to, the cornea, nose region or eyelid.

[0008] The flexible immersion bag accommodates off-center and angular positioning of the ultrasound probe for off-center ultrasound scans such as a lesion on the side of the eye (sclera). Thus, while the immersion bag is immobile, the ultrasound probe can be angled within the immersion bag. The immersion bag end also can be rolled on the examined surface for acquiring angled ultrasound images at various angles while still maintaining a spaced relationship with the examined surface. This minimizes potential damage to sensitive and delicate tissues such as the

cornea. The ultrasound probe and immersion bag containing the liquid medium can easily be moved and repositioned on different anatomical areas to be examined without consequence to the cornea.

[0009] One significant aspect and feature of the present invention is a sterile acoustically invisible immersion bag of an immersion bag system that fully encapsulates one end of an ultrasound probe.

5 [0010] Another significant aspect and feature of the present invention includes an acoustically invisible immersion bag system where a flexible collar including a flexible seal and a rigid or semi-rigid capture ring in cooperation with an immersion bag surrounds and engages the distal end portion of the ultrasound probe.

10 [0011] Still another significant aspect and feature of the present invention is the flexible collar and closely associated structure which effectively secures and seals to the ultrasound probe body to form a probe/seal valve which is deformable.

[0012] Still another significant aspect and feature of the present invention is an immersion bag system which can be preloaded or loaded on site with a gel or other aqueous medium.

15 [0013] Yet another significant aspect and feature of the present invention is an immersion bag wherein gel or other aqueous medium is contained and encapsulated about and between the distal end of an ultrasound probe and the interior of the immersion bag.

20 [0014] Another significant aspect and feature of the present invention is a flexible collar which can include controlled pressure venting for air, gases, gels or other aqueous medium.

25 [0015] Yet another significant aspect and feature of the present invention is where a flexible immersion bag accommodates off-center positioning of the ultrasound probe for off-center ultrasound scans; hence, the immersion bag is stationary and the ultrasound probe moves within the immersion bag or can be rolled on the examined area and achieve similar results so there is no or minimal abrasive contact with delicate or sensitive structures.

30 [0016] Another significant aspect and feature of the present invention is an immersion bag including a flexible collar that functions in cooperation with the body of an ultrasound probe to form a self-sealing valve which can by itself or in combination with additional valves with the flexible collar provide passive control of

the internal pressure in the immersion bag during ultrasound probe insertion, thereby preventing the immersion bag from bursting by allowing air and excessive filler medium to escape.

5 [0017] Another significant aspect and feature of the present invention is the utilization of internal immersion bag hydraulic pressure and bag material tension creating buoyancy and resistance on the ultrasound probe when the operator is moving the ultrasound probe deeper into the immersion bag into close proximity with the examined surface. Further, once the ultrasound probe has been inserted into the immersion bag, the consequential positive hydraulic pressure is a safety feature
10 minimizing the likelihood of the ultrasound probe making physical contact with nearby superficial structures such as the cornea of the eye. Thus, there is an offset of the ultrasound probe from the examined surface that overcomes near field artifact.

 [0018] Another embodiment of the present invention includes additional aspects and features wherein:

15 [0019] Another significant aspect and feature of the present invention is the use of a maneuvering ring which surrounds a flexible collar and other closely associated components to provide a measured amount of rigidity in order that the user can grasp and position the immersion bag with respect to the eye.

 [0020] Another significant aspect and feature of the present invention is the
20 use of a maneuvering ring having an interior annular receptor groove which engages, couples and mates with an exterior annular ring of the flexible collar for mutual joining thereof in order to fasteningly accommodate the lip of the immersion bag and other closely associated components.

 [0021] Another significant aspect and feature of the present invention is the
25 use of an O-ring or band to depress a portion of the immersion bag lip into an annular interior groove of a capture ring to secure the immersion bag to the capture ring.

 [0022] Yet another significant aspect and feature of the present invention is the use of an immersion bag substantially having a conical shape for the greatest portion thereof which includes an end which is arcuate in profile, whereby such an
30 arcuate end reversibly conforms to the shape of the cornea.

[0023] Yet another significant aspect and feature of the present invention is that examination of ocular structures does not require coupling gel on the bag outer surface.

[0024] Having thus briefly described one or more embodiments of the present invention and having mentioned some significant aspects and features of the present invention, it is the principal object of the present invention to provide a acoustically invisible immersion bag system that overcomes near field artifact by surrounding the
5 tip portion of an ultrasound probe tip with gel or liquid contained in an immersion bag removably secured by the use of a probe/seal valve to and about an ultrasound probe via a flexible collar that may contain self-sealing valve structure for venting excess air or excess liquid.

BRIEF DESCRIPTION OF THE DRAWINGS

[0025] Other objects of the present invention and many of the attendant advantages of the present invention will be readily appreciated as the same becomes better understood by reference to the following detailed description when considered
5 in connection with the accompanying drawings, in which like reference numerals designate like parts throughout the figures thereof and wherein:

[0026] **FIG. 1** is an isometric view of an immersion bag system, the present invention, shown in use surrounding the tip of an ultrasound probe;

[0027] **FIG. 2** is provided to show a partially exploded view of the ultrasound
10 immersion bag system and a typical ultrasound probe for use therewith;

[0028] **FIG. 3** is a cross section view along line 3-3 of **FIG. 4** in order to show both the general structure of a flexible collar and to show valve structure extending through a flexible collar wall;

[0029] **FIGS. 4 and 5** are top and bottom views, respectively, of the
15 immersion bag flexible collar;

[0030] **FIG. 6** is a partial cross section view showing the engagement of the immersion bag system with the tip of the ultrasound probe;

[0031] **FIG. 7** illustrates a sterile immersion bag system surrounding the tip of an ultrasound probe and contacting the cornea of an eye as utilized during an
20 ultrasound scan of the central portion of the eye and illustrating how the near field artifact is overcome;

[0032] **FIG. 8** illustrates the ultrasound probe with the immersion bag system in close engagement with a cornea of an eye for an ultrasound scan of a noncentral portion of the eye where the ultrasound probe is depicted at an angle within the
25 stationary but flexible immersion bag and maintaining positive pressure to minimize the chance of damaging sensitive/delicate tissue such as the cornea of the eye.

[0033] **FIG. 9**, an alternative embodiment, is a cross section view of a one-piece flexible collar;

[0034] **FIGS. 10 and 11** are top and bottom views, respectively, of the
30 one-piece flexible immersion bag;

[0035] FIG. 12 is a partial cross section view showing engagement of the immersion bag system by the tip of the ultrasound probe;

[0036] FIG. 13, an alternative embodiment, is an isometric view of an immersion bag system shown affixed to and in use with another form of the
5 ultrasound probe;

[0037] FIG. 14 is a partially exploded view of the sterile immersion bag system incorporated to frictionally engage the lower nontapered portion of the ultrasound probe;

[0038] FIG. 15 is an exploded isometric top view of the immersion bag
10 system shown distanced from the ultrasound probe;

[0039] FIG. 16 is an exploded isometric bottom view of the immersion bag system shown distanced from the ultrasound probe;

[0040] FIG. 17 is a cross section view of the one-piece flexible collar shown in FIGS. 15 and 16 along line 17-17 of FIG. 15 in order to show the general
15 structure of the flexible collar;

[0041] FIG. 18 is a cross section view of the one-piece maneuvering ring along line 18-18 of FIG. 15 in order to show the general structure of the maneuvering ring;

[0042] FIGS. 19 and 20 are top and bottom views respectively of the flexible
20 collar including the flexible seal;

[0043] FIG. 21 is a partial cross section view showing engagement of the immersion bag system by the tip of the ultrasound probe;

[0044] FIG. 22 is a view like FIG. 21 where sideways force is exerted upon the ultrasound probe thereby urging the ultrasound probe off center with respect to the
25 flexible seal; and,

[0045] FIG. 23 is a top view in partial cross section along line 23-23 of FIG. 22 showing the off-center location of the ultrasound probe and the gap created by the deforming of the annular sealing aspect of the probe/seal valve to open the probe/seal valve.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0046] **FIG. 1** is an isometric view of an immersion bag system 10, the present invention, shown affixed to and in use with an ultrasound probe 12. The lower region of the ultrasound probe 12 is sealed in close association with the following components comprising the immersion bag system 10, each with flexible qualities including: a flexible immersion bag 16, a flexible collar 18 having an integral flexible seal 20, and a capture ring 22 which can be rigid or semi-rigid, all of which are shown in **FIG. 2**. The body 24 of the ultrasound probe 12 generally is tubular in shape and includes a transducer 26 at one end and also houses other internal components associated with operation of the transducer 26. The upper region of the ultrasound probe body 24 includes suitable geometrically configured external structure about the upper region thereof. A control/power cable 28 exits from one end of the ultrasound probe 12 for connection to external support components associated with operation of the transducer 26.

[0047] FIG. 2 is a partially exploded view of the sterile immersion bag system 10 incorporated to frictionally engage the lower portion of the ultrasound body 24. The structure of the immersion bag system 10 includes the immersion bag 16, the flexible collar 18, the flexible seal 20 integral to the flexible collar 18, and
5 the rigid or semi-rigid capture ring 22 collectively having features suitable for providing sealed communication of the immersion bag system 10 with respect to the lower portion, i.e., the body 24, of the ultrasound probe 12.

[0048] The flexible seal 20 which is integral to the flexible collar 18 is of a general annular shape each being fashioned of a flexible material, such as, but not
10 limited to, foam, preferably close cell foam, latex, rubber, plastic, or other suitable flexible and pliable material, and includes aligned and connecting generally annular-shaped structure. Once engaged onto the ultrasound probe 12, the flexible seal 20 is watertight permitting examinations in any position (e.g., patient sitting upright or laying down).

[0049] The immersion bag 16 is formed of a thin and flexible pliable acoustically invisible material (for example and demonstration, in a range of 0.1 micron to 250 microns), such as polyethylene, hydrophilic plastic, or other suitable material, which is capable of containing a gel or other suitable medium and which allows the passage of ultrasound waves. The immersion bag 16 preferably has a
15 general cylindrical shape for the greatest portion thereof and includes an end 30 which is dome and/or bullet shaped and also includes an interior 32. In the alternative, as shown in FIG. 14, an immersion bag 16a can have a conical shape for the greatest portion thereof and can include an end 30a which has an arcuate profile. The top of the immersion bag 16 is reversed a short distance outwardly and about
20 itself to form a lip 34 of annular shape extending about the upper region of the immersion bag 16 for accommodation of the capture ring 22. The capture ring 22 is of a general annular shape fashioned of a rigid or semi-rigid material, such as, but not limited to, plastic or other suitable material.
25

[0050] FIG. 3 is a cross section view of the one-piece flexible collar 18, also shown in detail in FIGS. 4, 5 and 6. The cross section view of FIG. 3 is taken along line 3-3 of FIG. 4 in order to show both the general structure of the flexible collar 18 and to show the structure of the valving extending through the wall thereof. The continuously formed flexible collar 18 is comprised of a plurality of geometrically configured and connecting structures including: a vertically oriented outer wall 36 which forms the periphery of the flexible collar 18, a horizontally oriented top wall 38 which intersects the upper region of the outer wall 36 and extends inwardly a short distance, an angled transition wall 40 extending inwardly and downwardly from the top wall 38 to intersect the flexible seal 20, and the flexible seal 20 extending downwardly from the lower portion of the transition wall 40. The lower portion of the flexible seal 20 is canted in slightly to ensure forcible flexed contact of the inner periphery of the flexible seal 20 with the body 24 of the ultrasound probe 12. An arrangement and the relationship of the ultrasound probe 12 with the flexible seal 20 results in an annular shaped deformable probe/seal valve 49 which is formed as shown in FIG. 6, whereby such an arrangement and relationship is perfected by the engagement of the body 24 of the ultrasound probe 12 with the inner circumference of the flexible seal 20. Other annular regions are formed by the previously described structure of the flexible collar 18 including a top opening 42 incorporating the angled inner periphery of the transition wall 40 as a guide structure for insertion of a probe body, such as the probe body 24, through the flexible collar 18 and through a middle opening 44 formed by the inner periphery of the flexible seal 20. A capture annulus 46 is formed near the junction of the inside surface of the outer wall 36 and the region underlying the top wall 38 for captured accommodation of the lip 34 of the immersion bag 16 in cooperation with the capture ring 22. An expansive bottom opening 48 is provided extending between the lower region of the capture annulus 46 and below the bottom edge of the flexible seal 20 through which an ultrasound probe body, such as the probe body 24, can pass while still maintaining slideable engagement with the flexible seal 20. One or more self-sealing valves 50a-50n of arcuate and other structure are located along, about and extending through the

transition wall 40. The cross section of the self-sealing valves 50a-50n, such as shown at self-sealing valve 50n, discloses a triangular shape having an elongated arcuate opening 52 at the outwardly facing surface of the transition wall 40 narrowing to a closed but actuatable elongated arcuate slit 54 at the inwardly facing surface of the transition wall 40. The triangular shape extends as an extruded arcuate shape along a suitable arc, such as 20° for the purpose of example and illustration.

[0051] FIGS. 4 and 5 are top and bottom views, respectively, of the flexible collar 18 including the flexible seal 20, the later of which when in intimate engagement with the body 24 of the ultrasound probe 12 cooperatively functions as a part of the probe/seal valve 49 itself. Shown in particular are the self-sealing valves 50a-50n in the flexible collar 18 and the annular structure of the flexible collar 18. The self-sealing valves 50a-50n vent the interior 32 of the immersion bag 16 when the tip of the ultrasound probe 12 is introduced into the interior 32 of the immersion bag 16. Air, gas, liquids, gels, or other mediums or fluids can be displaced or vented through the self-sealing valves 50a-50n during introduction of the tip of the ultrasound probe 12 or during further operation of the invention. The size of the self-sealing valves 50a-50n is shown in exaggerated form for purposes of illustration. In actual practice, the slits at the upper portions of the self-sealing valves 50a-50n, which alternatively can be in the form of narrow gaps or holes or other suitable structure, are parted by the force of the expelled or displaced air, gas, liquid, aqueous mediums, gel, or the like, and modulate toward or to a closed state upon equalization between the interior 32 of the immersion bag 16 and ambient pressure. The self-sealing valves 50a-50n could also be of different sized structure to operate across a pressure relief range. The purpose of the structure of the self-sealing valves 50a-50n is to prevent breakage of the immersion bag 16 by displacing air and to act as a fluid overflow. The self-sealing valves 50a-50n ensure adequate hydraulic force to remove wrinkles in the immersion bag 16 which result in acoustic artifacts (typically, arcuate shaped noise above the examining surface). Such hydraulic force also provides resistance so that the ultrasound probe 12 does not come into direct contact with superficial structures, such as the delicate cornea of the eye.

[0052] FIG. 6 is a partial cross section view showing engagement of the immersion bag 16 by the tip of the ultrasound probe 12. The immersion bag system 10 shown includes the flexible collar 18 including the flexible seal 20, the capture ring 22, and the immersion bag 16 fully arranged and assembled using the structural features of such components in suitable engagement made possible by the elastic qualities of the involved components in combination with the fixation of the lip 34 of the immersion bag 16 within the capture annulus 46 by the capture ring 22, such as by the use of heat staking, tape, an O-ring, bands (not shown) which preferably are elastic, adhesive or other suitable attachment devices or methods. Additionally, the lip 34 of the immersion bag 16 is secured in the capture annulus 46 and sealingly held against the inner surface of the outer wall 36 by the forcible positioning of and the forcible engagement of the capture ring 22. The flexible seal 20 flexes to sealingly accommodate and frictionally engage and seal against the body 24 of the ultrasound probe 12 forming the probe/seal valve 49, as previously described. The tip of the ultrasound probe 12 is positioned within the interior 32 of the immersion bag 16, wherein the transducer 26 is spaced sufficiently from the end 30 of the immersion bag 16 to allow flexing of end 30 about the surface of the eye and to prevent contact of the transducer 26 with end 30 of the immersion bag during such flexing.

MODE OF OPERATION

[0053] FIGS. 7 and 8 illustrate the immersion bag system 10 in use with an ultrasound probe 12 engaging a cornea 56 of an eye 58 for an ultrasound scan, e.g., of the central and non-central aspects of the eye 58, respectively. The immersion bag system 10 can be furnished as a sterile prepackaged disposable unit. The immersion bag 16 can be manually filled with water, gel 60 or other suitable ultrasound transmission medium, such as other aqueous medium, or the immersion bag 16 can be prefilled and covered by a removable top seal to contain the gel 60 or other aqueous medium within the immersion bag 16, wherein the top seal is removed prior to introducing the end of the probe body 24 into the flexible collar 18 and into the immersion bag 16. When examining ocular structures, coupling gel on the bag outer surface is not required. This is a unique feature of this invention. However, the use of gel on the bag exterior may be considered in cutaneous or industrial applications. Also, a foil sealed external container can hold an adequate amount of transducer coupling medium external to the immersion bag 16 for manual loading. During introduction of the end of the probe body 24 into the flexible collar 18 and the immersion bag 16, the flexible seal 20 flexingly and transitionally seals against the body 24 of the ultrasound probe 12 and concurrently forms the probe/seal valve 49. This ensures that the gel 60 or other aqueous medium is contained within the interior 32 of the immersion bag 16 and positive pressure is created. By exerting sideways force, using the ultrasound probe 12 against the flexible seal 20 or by rocking or angulating the ultrasound probe 12 against the flexible seal 20, a gap is created by deforming the probe/seal valve 49 to expel excess internal pressure, air and liquid overfill allowing a reduction in immersion bag internal pressure to a desired level and a desired bag shape. The previously described self-sealing valves 50a-50n are parted when the internal pressure of the immersion bag 16 exceeds a certain level in order to maintain the integrity of the immersion bag 16 and releases enough air, gas, liquid, gel, or other aqueous medium to reduce the internal pressure of the immersion bag 16 to a safe level and to prevent the immersion bag 16 from bursting while still maintaining a suitable internal positive pressure within the immersion

bag 16. The ultrasound probe 12 is introduced a suitable distance (depending on probe transducer frequency) into the interior 32 of the immersion bag 16 filled with gel 60 or other aqueous medium to overcome near field artifact where the transducer 26 preferably maintains a suitable spacing from the immersion bag end 30 and thus from the cornea 56 or other near surface where the possibility of direct contact with structures under examination are minimized. The distal end of the invention, i.e., the immersion bag 16, comes in direct contact with the cornea 56 or other superficial structure, and upon initial contact, the end 30 of the immersion bag 16 intimately contacts and begins conformal reshaping to and about the surface of the cornea 56 or other superficial structure, while yet maintaining suitable spacing between the transducer 26 and the cornea 56 to overcome near field artifact. Also, the immersion bag 16 conforms to the surface under examination whether regular or irregular. The external ultrasound equipment is then energized after the ultrasound probe 12 is placed into the immersion bag 16 containing liquid/gel that has coupling fluid on the inside enabling an ultrasound scan of suitable width across the anterior aspects of the eye or other superficial structure. An ultrasound scan across a noncentral portion of the eye 58, such as the sclera or white of the eye or other superficial structure, can be accomplished, such as shown in **FIG. 8**, where the ultrasound probe 12 and the flexible collar 18 is unitarily repositioned off center and to the side of the immersion bag 16 while maintaining the central original end 30 point of mutual contact. Contact with the examining surface remains in intimate contact due to the flexible nature of the immersion bag 16. Thus, there is minimal drag across sensitive and delicate structures such as the cornea, reducing the chance of abrasion. Although the invention is described for use with an eye, the principles of the invention also apply to use about other superficial areas of a body whether human, animal for ocular, cutaneous or vascular purposes or inanimate objects such as tubing carrying fluid. When the ultrasound probe 12 is inserted through the flexible collar 18, the flexible seal 20 will be pulled downwardly, whereby this action will open one or more of the self-sealing valves 50a-50n. Concurrently, the flexible seal 20 can function as a deformed component of the probe/seal valve 49 by forcing

the ultrasound probe 12 against the flexible seal 20 in one or another direction or by angulation or by rocking thereby deforming the probe/seal valve 49 and creating one or more gaps at the flexible seal. Thus, as the ultrasound probe 12 is moved into position as it is inserted into the immersion bag 16, a slight pressure is maintained as
5 the ultrasound probe 12 stops moving downwards, whereby excess filler gel/liquid or air has been simultaneously displaced. By angulating and/or forcing the body of the ultrasound probe 12 against one side of the probe/seal valve 49, one or more gaps can be created (such as gap 122 shown in **FIGS. 22 and 23** of an alternative embodiment), thereby opening the probe/seal valve 49 to release internal pressure, trapped air and/or
10 excess fluid.

[0054] **FIG. 9** is a cross section view of a one-piece flexible collar 62 for use with an immersion bag system 10a, an alternative embodiment, also shown in detail in **FIGS. 10, 11 and 12**. The flexible collar 62 is of a general annular shape fashioned preferably of a flexible material, such as foam, preferably close cell foam, latex, rubber or of other suitable flexible and pliable materials. The cross section view of **FIG. 9** is taken along line 9-9 of **FIG. 10** in order to show both the general structure of the flexible collar 62 and to show the structure of the valving extending through the wall thereof. The continuously formed flexible collar 62 is comprised of a plurality of geometrically configured and connecting structures including a vertically oriented outer wall 64 which forms the periphery of the flexible collar 62, a horizontally oriented top wall 66 which intersects the upper region of the outer wall 64 and extends inwardly a short distance, a vertically oriented inner wall 68 extending downwardly from the top wall 66, and an angled transition wall 70 extending inwardly and downwardly from the lower portion of the inner wall 68 and a downwardly extending seal flexible 72 extending from the angled transition wall 70. The lower portion of the flexible seal 72 can be canted in slightly to ensure forcible flexed contact of the inner periphery of the flexible seal 72 with the body 24 of the ultrasound probe 12. Other annular regions are formed by the previously described structure of the flexible collar 62 including a top opening 74 incorporating the angled inner periphery of the transition wall 70 and the inner periphery of the inner wall 68 as a guide structure for insertion of a probe body, such as the probe body 24, through the flexible collar 62, and a bottom opening 76 formed by the inner periphery of the flexible seal 72. A capture annulus 78 is formed near the junction of the inside surface of the outer wall 64 and the region underlying the top wall 66 for captured accommodation of the lip 34 of the immersion bag 16 in cooperation with the capture ring 22. One or more self-sealing valves 80a-80n, preferably of arcuate structure, are located along, about and extending vertically through the inner face of the flexible seal 72. The cross section of the self-sealing valves 80a 80n, such as shown at self-sealing valve 80a, discloses an elongated arcuate structure. The self-sealing valves 80a-80n are shown in the open position, such as when venting excess

pressures or fluid medium therethrough. In the nonventing position, the shape of the self-sealing valves 80a-80n would assume a flattened position against the body 24 of the ultrasound probe 12, but would modulate toward the open position during releasing of pressure or of fluid medium.

[0055] FIGS. 10 and 11 are top and bottom views, respectively, of the flexible collar 62, including the flexible seal 72. Shown in particular are the self-sealing valves 80a-80n in the flexible collar 62 and the annular structure of the flexible collar 62. The self-sealing valves 80a-80n vent the interior 32 of the immersion bag 16 when the tip of the ultrasound probe 12 is introduced into the interior 32 of the immersion bag 16. Air, gas, liquids, gels, or other mediums or fluids can be displaced or vented through the self-sealing valves 80a-80n during introduction of the tip of the ultrasound probe 12 or during further operation of the invention. The size of the self-sealing valves 80a-80n is shown in exaggerated form for purposes of illustration. In actual practice, the option of additional self-sealing valves 50a-50n, which alternatively can be in the form of narrow gaps, slits or of related shape decreasing geometry structure or other suitable structure, are parted by the force of the expelled or displaced air, gas, liquid, aqueous mediums, gel, or the like, and modulate toward or to a closed state upon equalization between the interior 32 of the immersion bag 16 and ambient pressure. The self-sealing valves 80a-80n could be of different sized structure to operate across a pressure relief range. The purpose of the structure of the self-sealing valves 80a-80n or optional/additional self-sealing valves 50a-50n is to prevent breakage of the immersion bag 16 by displacing air and to act as a fluid overflow. The self-sealing valves 80a-80n ensure adequate hydraulic force to remove wrinkles in the immersion bag 16 which result in acoustic artifacts (typically, arcuate shaped noise above the examining surface). Such hydraulic force also provides resistance so that the ultrasound probe 12 is prevented from coming into direct contact with the cornea of the eye.

[0056] FIG. 12 is a partial cross section view showing engagement of the immersion bag 16 by the tip of the ultrasound probe 12. The immersion bag system 10a shown includes the flexible collar 62, including the flexible seal 72, the capture ring 22, and the immersion bag 16 fully arranged and assembled using the structural features of such components in suitable engagement made possible by the elastic qualities of the involved components in combination with the fixation of the lip 34 of the immersion bag 16 within the capture annulus 78 by the capture ring 22 using heat staking, adhesive or other suitable attachment. Additionally, the lip 34 of the immersion bag 16 is secured in the capture annulus 78 and sealingly held against the inner surface of the outer wall 64 by the forcible positioning of and the forcible engagement of the capture ring 22. The flexible seal 72 flexes to sealingly accommodate and frictionally engage and seal against the body 24 of the ultrasound probe 12 in the formation of the probe/seal valve 49a. The tip of the ultrasound probe 12 is positioned within the interior 32 of the immersion bag 16, wherein the transducer 26 is spaced sufficiently from the end 30 of immersion bag 16 to allow flexing of the end 30 in a spaced relationship with the eye and to prevent contact of the transducer 26 with the end 30 of immersion bag 16 during such flexing. The mode of operation of this first alternative embodiment is substantially the same as described for the immersion bag system 10, the only difference being that the flexible collar 62 is substituted for the flexible collar 18.

[0057] FIG. 13 is an isometric view of an immersion bag system 10b, an alternative embodiment, shown affixed to and in use with another form of the ultrasound probe 12, herein designated as ultrasound probe 12a. The lower region of the ultrasound probe 12a is sealed in close association with the following components

5 comprising the immersion bag system 10b each with flexible or semi-rigid qualities including: an immersion bag 16a, a flexible collar 82 having an integral flexible seal 84, and a capture ring 86 which can be rigid or semi-rigid having an annular groove 88 and an opening 89, each of which are shown in FIG. 14. The lower region of the ultrasound probe 12a also closely associates with other components of the

10 immersion bag system 10a, including an O-ring 90, preferably having flexible qualities, and a rigid maneuvering ring 92, each of which are also shown in FIG. 14. The body 24a of the ultrasound probe 12a is, for the most part, a tapered tubular structure including tapered body section 24b and a nontapered body section 24c, and includes a transducer 26a at one end and also houses other internal components

15 associated with operation of the transducer 26a. A control/power cable 28a exits from one end of the ultrasound probe 12a for connection to external support components associated with operation of the transducer 26a.

[0058] FIG. 14 is a partially exploded view of the sterile immersion bag system 10b incorporated to frictionally engage the nontapered body section 24c of the ultrasound body 24a of the ultrasound probe 12a. The structure of the immersion bag system 10b includes the immersion bag 16a, the flexible collar 82, the flexible seal 84
5 integral to the flexible collar 82, the capture ring 86 which can be rigid or semi-rigid, the O-ring 90 and the maneuvering ring 92, collectively, having features suitable for providing sealed communication and/or maneuvering of the immersion bag system 10b with respect to the lower portion, i.e., the nontapered body section 24c of the ultrasound probe 12a.

10 [0059] The flexible seal 84, which is integral to the flexible collar 82, is of a general annular shape, each being fashioned of a flexible material, such as, but not limited to, foam, preferably close cell foam, latex, rubber, plastic, or other suitable flexible and pliable material, and includes aligned and connecting generally annular-shaped structure. Once engaged onto the nontapered body section 24c of the
15 ultrasound probe 12a, the flexible seal 84 is watertight permitting examinations in any position (e.g., patient sitting upright or laying down).

[0060] The immersion bag 16a is formed of a thin and flexible pliable acoustically invisible material (for example and demonstration, in a range of 0.1 micron to 250 microns), such as polyethylene, hydrophilic plastic or other suitable
20 material which is capable of containing a gel or other suitable medium and which allows the passage of ultrasound waves. The immersion bag 16a preferably is substantially a conical shape for the greatest portion thereof and includes an end 30a which is arcuate in profile and also includes an interior 32a. The top of the immersion bag 16a is reversed a short distance outwardly and about itself to form a
25 lip 34a of annular shape extending about the upper region of the immersion bag 16a for accommodation of the capture ring 86. The lip 34a is shown as it would subsequently appear when affixed over and around, and forced and depressed into the annular groove 88 of the capture ring 86 by the O-ring 90, thereby forming an inwardly directed annular depression 93 thereabout, such as when securing the lip 34a
30 of the immersion bag 16a to the capture ring 86. A suitable size small band may be

substituted for use in lieu of the O-ring 90, whereby the band can be used to depress the lip 34a into the annular groove 88 of the capture ring 86 to form the annular depression 93, or the band can be of greater vertical proportion to forcibly direct the broad portion of the lip 34a against outer periphery of the capture ring 86 to connect
5 the lip 34a of the immersion bag 16a to the capture ring 86. The O-ring 90 or the described bands and the capture ring 86 may also be used in the previously described embodiments to fasten the lip 34 of the immersion bag 16 to the capture ring 22. The capture ring 86 is of a general annular shape fashioned of a rigid or semi-rigid material, such as, but not limited to, plastic or other suitable material.

[0061] **FIG. 15** is an exploded isometric top view of the immersion bag system 10b shown distanced from the ultrasound probe 12a, and **FIG. 16** is an exploded isometric bottom view of the immersion bag system 10b shown distanced from the ultrasound probe 12a.

[0062] FIG. 17 is a cross section view of the one-piece flexible collar 82, also shown in FIGS. 15 and 16, taken along line 17-17 of FIG. 15 in order to show the general structure of the flexible collar 82. The continuously formed flexible collar 82 is comprised of a plurality of geometrically configured and connecting structures including a vertically oriented outer wall 94 having an externally located annular ring 96 which has a beveled profile forming the periphery of the flexible collar 82, a horizontally oriented bottom wall 98 which is annular and which intersects the lower region of the outer wall 94 and extends inwardly a short distance, a horizontally oriented top wall 100 which intersects the upper region of the outer wall 94 and extends inwardly a short distance, an angled transition wall 102 extending inwardly and downwardly from the top wall 100 to intersect the flexible seal 84, and the flexible seal 84 extending downwardly and inwardly from the lower portion of the transition wall 102. The lower portion of the flexible seal 84 is canted in slightly to ensure forcible flexed contact of the inner periphery of the flexible seal 84 with the nontapered body section 24c of the ultrasound probe 12a. An arrangement and relationship of the ultrasound probe 12a with the flexible seal 84 results in an annular shaped deformable probe/seal valve 49b which is formed as shown in FIG. 21, whereby such an arrangement and relationship is perfected by the engagement of the nontapered body section 24c of the body 24a of the ultrasound probe 12a with the inner circumference of the flexible seal 84. Other annular regions are formed by the previously described structure of the flexible collar 82 including a top opening 104 bordered by the angled inner periphery of the transition wall 102 and a middle opening 106 bordered by the angled inner periphery of the flexible seal 84, the combination of which serve as a guide structure for insertion of a probe body, such as the probe body 24a, partially through the flexible collar 82. A capture annulus 108 is formed by the junction of the inside surface of the outer wall 94, the region underlying a portion of the top wall 100 and the inside surface of the bottom wall 98 for captured accommodation of the lip 34a of the immersion bag 16a and the capture ring 86 and O-ring 90. An expansive bottom opening 110 is provided generally extending between and bounded by the lower to mid-region of the capture

annulus 108 and the bottom edge of the flexible seal 84 through which a portion of the nontapered body section 24c of the ultrasound probe 12a can maintain slideable sealed engagement with the flexible seal 84. One or more optional self-sealing valves 109 in tubular or cylindrical form or of other suitable structure are shown in
5 dashed lines located along, about and extending through the transition wall 102 offering communication between ambient and the interior 32a of the immersion bag 16a.

[0063] FIG. 18 is a cross section view of the one-piece maneuvering ring 92 along line 18-18 of FIG. 15 in order to show the general structure of the maneuvering ring 92. The maneuvering ring 92 frictionally engages over and about the combined structure of the flexible collar 82, the O-ring 90, the lip 34a of the immersion bag 16a, the immersion bag 16a, and the capture ring 86 as shown in FIG. 21. The use of the maneuvering ring 92 supplies a structure having a measured amount of rigidity in order that the user can grasp and position the immersion bag 16b with respect to the eye or other surface being examined without the danger of disturbing the integrity of the probe/seal valve 49b. The interior geometry of the maneuvering ring 92 snappingly engages the exterior geometry of the flexible collar 82 in mutual coaxial engagement to secure about the capture ring 86, the lip 34a of the immersion bag 16a, and the O-ring 90. The maneuvering ring 92 includes an annular outer wall 110, a bottom wall 112 which intersects and extends inwardly a short distance from the bottom of the outer wall 110, a top opening 114, an annular receptor groove 116 adjacent the top opening 114 recessingly extending into the inner surface of the outer wall 110, a middle opening 118 adjacent and below the receptor groove 116, and a beveled bottom opening 120 located below and adjacent the middle opening 118 and between the inner edge of the bottom wall 112. The receptor groove 116 of the maneuvering ring 92 snappingly engages the annular ring 96 extending from the flexible collar 82 as the flexible collar 82 gains entry through and into the structure of the maneuvering ring 92, first by entering the top opening 114 followed by entry adjacent the annular receptor groove 116 and finally into the middle opening 118 where resistance to further positioning is subsequently offered by contact with the bottom wall 112.

[0064] FIGS. 19 and 20 are top and bottom views, respectively, of the flexible collar 82, including the flexible seal 84. Also shown is one optional self-sealing valve 109 extending through the transition wall 102 of the flexible collar 82 and other annular structure of the flexible collar 82. The use of one or more optional self-sealing valves 109 can be utilized to vent the interior 32a of the immersion bag 16a when the tip of the ultrasound probe 12a is introduced into the interior 32a of the immersion bag 16a. Air, gas, liquids, gels, or other mediums or fluids can be displaced or vented through the optional self-sealing valve(s) 109 during introduction of the tip of the ultrasound probe 12a or during further operation of the invention. The size of the optional self-sealing valve(s) 109 is shown in exaggerated form for purposes of illustration. In actual practice, the choice of including optional self-sealing valve(s) 109 or of self-sealing valves 50a-50n which alternatively can be in the form of narrow gaps, slits or of related shape decreasing geometry structure or other suitable structure, are parted by the force of the expelled or displaced air, gas, liquid, aqueous mediums, gel, or the like, and modulate toward or to a closed state upon equalization between the interior 32a of the immersion bag 16a and ambient pressure. The self-sealing valve(s) 109 could be of different sized similar structure to operate across a pressure relief range. The purpose of the structure of the optional/additional self-sealing valve(s) 109 or optional/additional self-sealing valves 50a-50n is to prevent breakage of the immersion bag 16a by displacing air and to act as a fluid overflow. The optional self-sealing valve(s) 109 can ensure adequate hydraulic force to remove wrinkles, if any, in the immersion bag 16a, which result in acoustic artifacts (typically, arcuate shaped noise above the examining surface). Such hydraulic force also provides resistance so that the ultrasound probe 12a is prevented from coming into direct or indirect contact with the cornea of the eye.

[0065] FIG. 21 is a partial cross section view showing engagement of the immersion bag 16a of the immersion bag system 10b by the tip of the ultrasound probe 12a, i.e., the nontapered body section 24c. The immersion bag system 10b shown includes the flexible collar 82, including the flexible seal 84, the capture ring 86, and the immersion bag 16a fully arranged and assembled using the structural features of such components in suitable engagement made possible by the elastic qualities of the involved components in combination with the fixation of the lip 34a and the juxtaposed upper portion of the immersion bag 16a within the capture annulus 108 by frictional engagement between the capture annulus 108 and the capture ring 86. Other additional fixation and securing methods can be used in addition, such as, but not limited to, the use of heat staking, adhesive, or other suitable attachment. Additionally, the lip 34a of the immersion bag 16a is sealingly held between the inner surface of the outer wall 94 of the flexible collar 82 by the forced positioning of and by the forced engagement of the capture ring 86 against the lip 34a in cooperation with the spongy and elastic qualities of the flexible collar 82. The flexible seal 84 flexes to sealingly accommodate and frictionally engage and seal against the nontapered body section 24c of the ultrasound probe 12a in the formation of the probe/seal valve 49b. The tip of the ultrasound probe 12a is positioned within the interior 32a of the immersion bag 16a, wherein the transducer 26a is spaced sufficiently from the end 30a of immersion bag 16a to allow flexing of the end 30a in a spaced relationship with the eye and to prevent contact of the transducer 26a with the end 30a of immersion bag 16a during such flexing. The mode of operation of this second alternative embodiment is substantially the same as described for the immersion bag system 10a, the difference being that the flexible collar 82 is substituted for the flexible collar 62, the shape of the immersion bag 16a is substantially conical with an arcuate end 30a and the maneuvering ring 92 is included. In this embodiment, the general shape of the immersion bag 16a is a combination of a conical shape terminating in an arcuate shape, whereby such a combination provides a minimum, i.e., not an excessive amount of material at the site of contact with the cornea, thereby minimizing bunching or folding of the immersion

bag 16a. The arcuate shape of the end 30a reverses upon contact with the cornea 56 to conformingly drape about the shape of the cornea in one-to-one correlation. Although the flexible collar 82 has been characterized as being an alternative to the flexible collars 18 and 62, neither collar is to be construed as being preferred over the
5 other--each have equal stature.

[0066] FIG. 22 is a view like FIG. 21 where sideways force is exerted upon the ultrasound probe 12a, thereby urging the ultrasound probe 12a off center with respect to the flexible seal 84 of the flexible collar 82 to create a gap 122 between the flexible seal 84 and the nontapered section 24c of the ultrasound probe 12a, thus opening the probe/seal valve 49b to allow transfer of air or aqueous medium through the gap 122. The geometry of the probe/seal valve 49b is influenced by this action to open the probe/seal valve 49b. The geometry of the probe/seal valve 49b can be otherwise influenced by angulating or rocking the ultrasound probe 12a to cause deformation of and opening of the probe/seal valve 49b by creating other gap(s) to allow transfer of air or aqueous medium through such gap(s). The flexible qualities of the flexible seal 84 accommodate such movement of the ultrasound probe 12a.

[0067] **FIG. 23** is a top view in partial cross section along line 23-23 of **FIG. 22** showing the off-center location of the ultrasound probe 12a and the gap 122 created by the deforming of the annular sealing aspect of the probe/seal valve 49b to open the probe/seal valve 49b. Gaps are also created in the previous embodiments in
5 the same manner as just described with reference to **FIGS. 22 and 23**.

[0068]	PARTS LIST
	10 immersion bag system
	10a immersion bag system
	10b immersion bag system
5	12 ultrasound probe
	12a ultrasound probe
	16 immersion bag
	16a immersion bag (conical)
	18 flexible collar
10	20 flexible seal
	22 capture ring
	24 body
	24a body
	24b tapered body section
15	24c nontapered body section
	26 transducer
	26a transducer
	28 control/power cable
	28a control/power cable
20	30 end
	30a end
	32 interior
	32a interior
	34 lip
25	34a lip
	36 outer wall
	38 top wall
	40 transition wall
	42 top opening
30	44 middle opening
	46 capture annulus
	48 bottom opening
	49 probe/seal valve
	49a probe/seal valve
35	49b probe/seal valve
	50a-n self-sealing valves
	52 opening
	54 slit
	56 cornea
40	58 eye
	60 gel
	62 flexible collar
	63 flexible seal
	64 outer wall
45	66 top wall

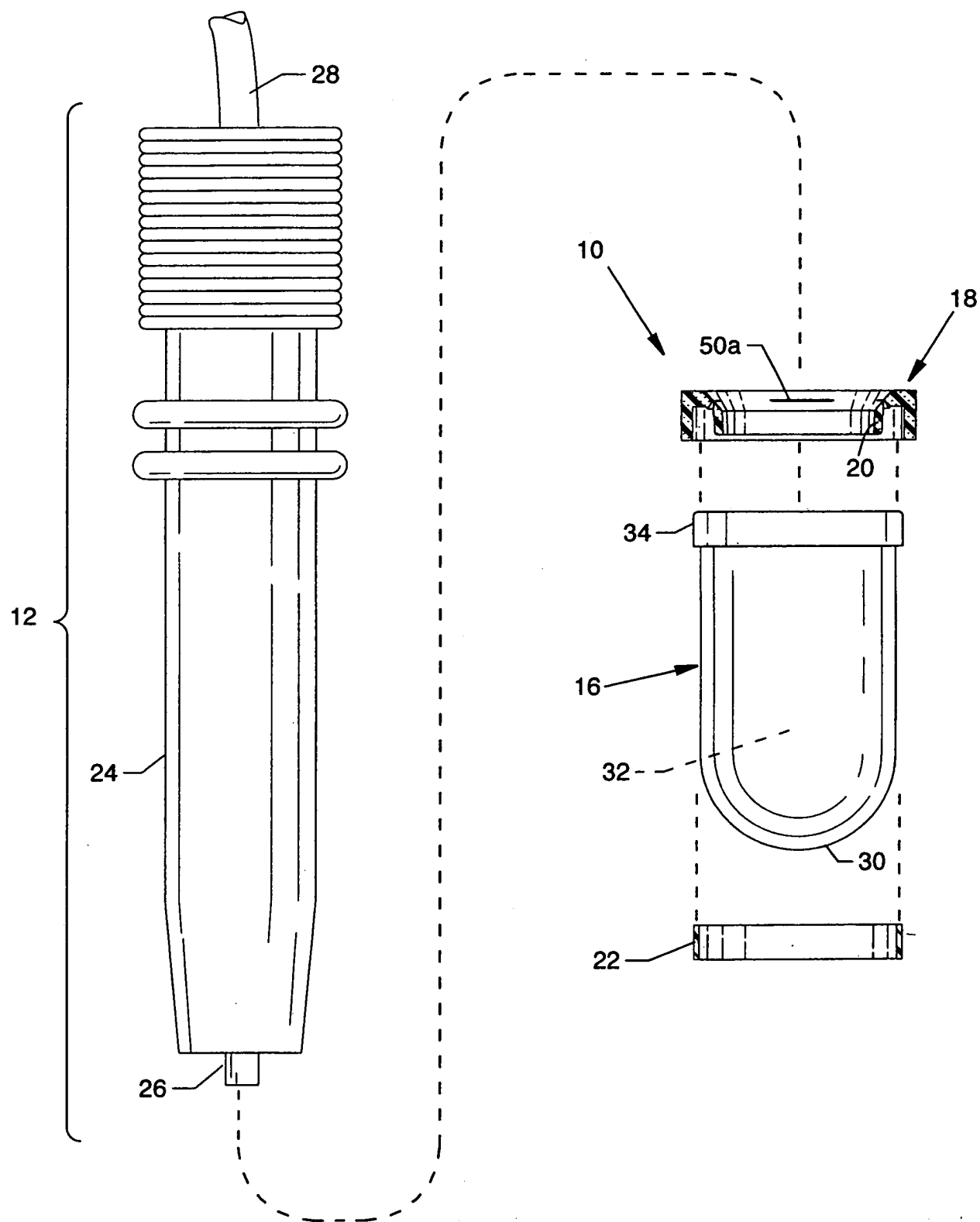
	68	inner wall
	70	angled transition wall
	72	flexible seal
	74	top opening
5	76	bottom opening
	78	capture annulus
	80a-n	self-sealing valves
	82	flexible collar
	84	flexible seal
10	86	capture ring
	88	annular groove
	89	opening
	90	O-ring
	92	maneuvering ring
15	93	annular depression
	94	outer wall
	96	annular ring
	98	bottom wall
	100	top wall
20	102	transition wall
	104	top opening
	106	middle opening
	108	capture annulus
	109	self sealing valve
25	110	outer wall
	112	bottom wall
	114	top opening
	116	receptor groove
	118	middle opening
30	120	bottom opening
	122	gap

[0069] Various modifications can be made to the present invention without departing from the apparent scope thereof.

IT IS CLAIMED:

1. A sterile immersion bag system having a flexible collar with an inner seal, which itself can act as a probe/seal valve which may be deformed by off-center actuation of an ultrasound probe to allow a slight air passage after the ultrasound probe is in place to allow for the passage of air or liquid, thus allowing and limiting
5 the pressure in an attached bag. These aforementioned recesses having any number of different forms.

2. Coupling gel (which may be an eye irritant) on the bag outer surface is not required for use with ocular exams. However, gel may be required for cutaneous or industrial applications.



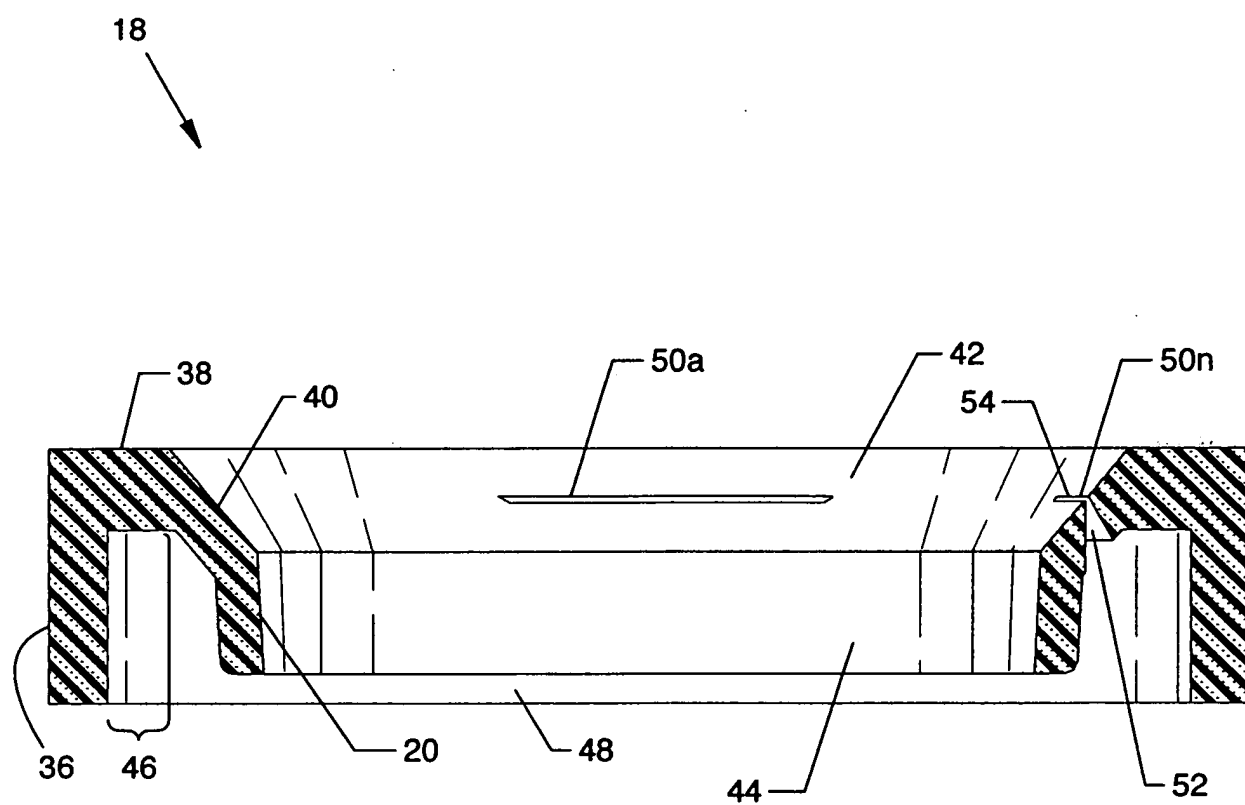


FIG. 3

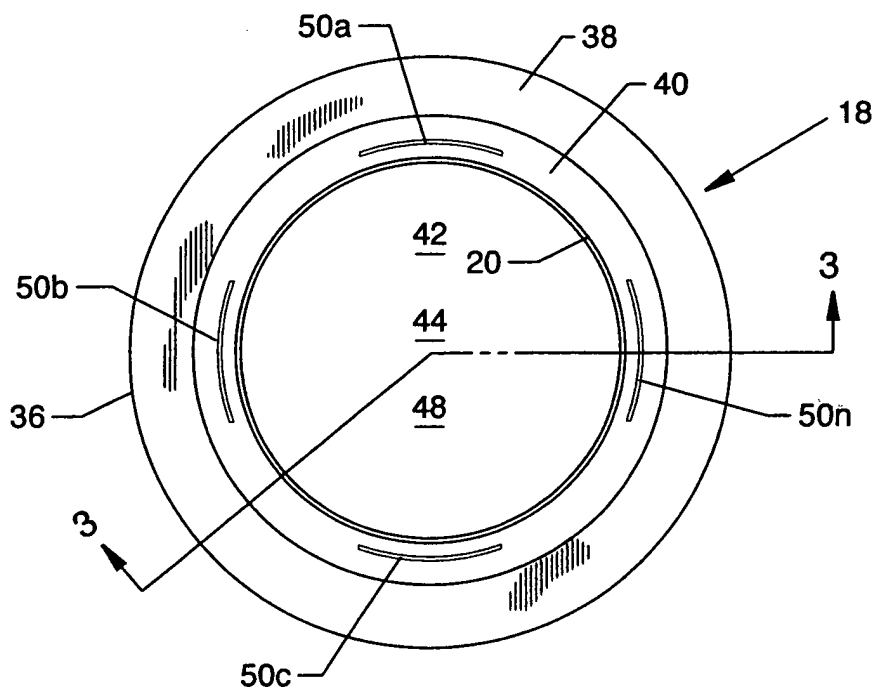


FIG. 4

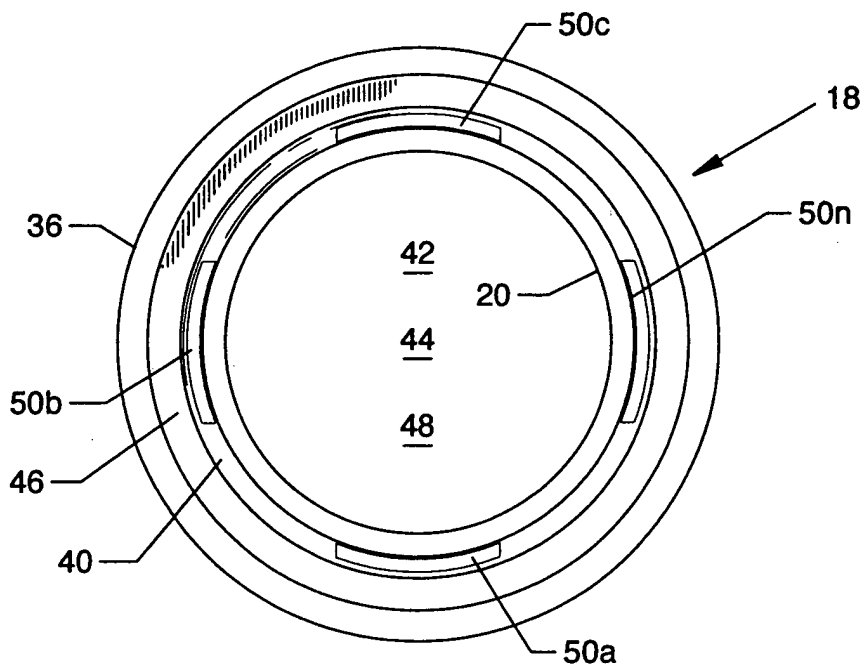


FIG. 5

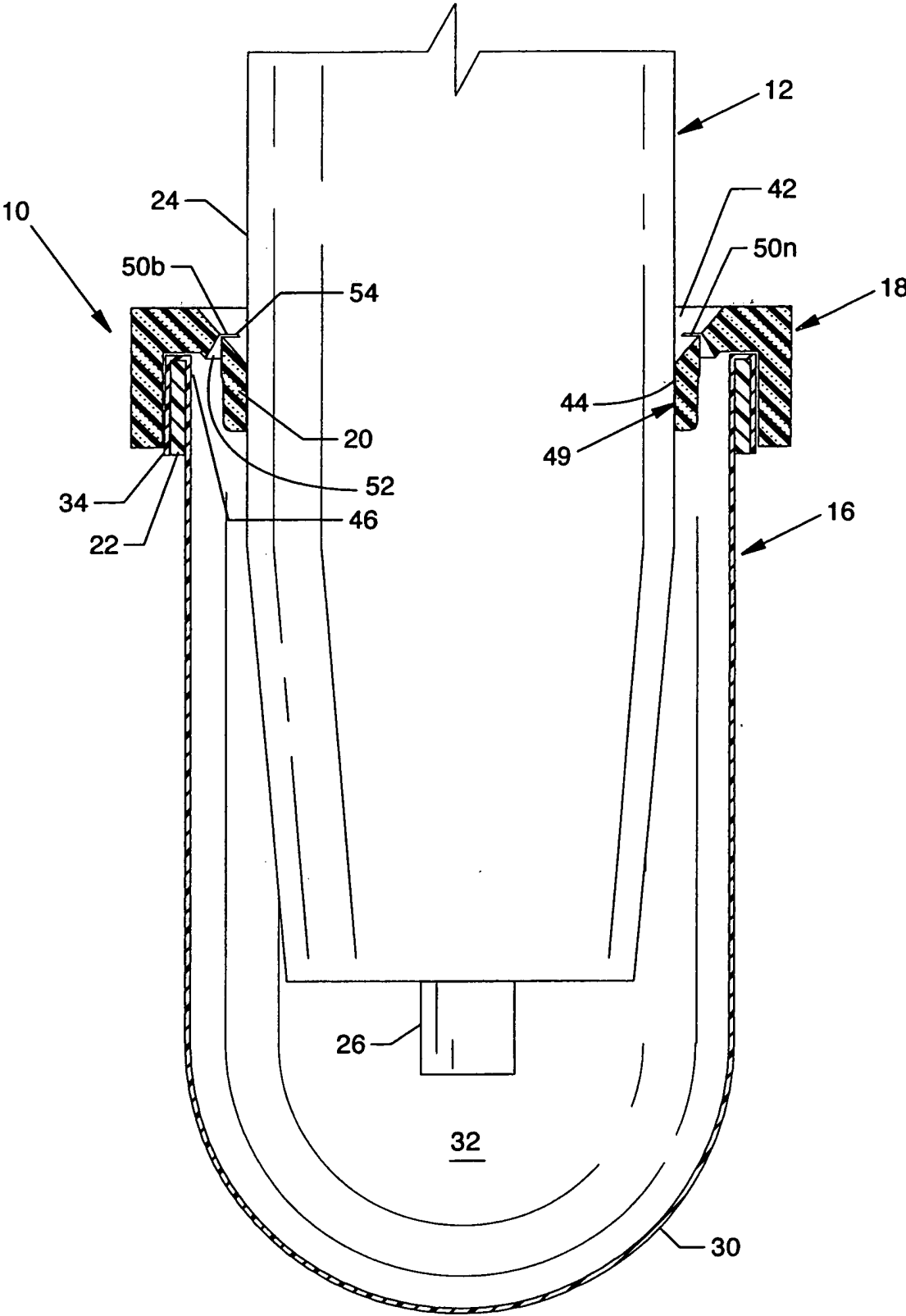


FIG. 6

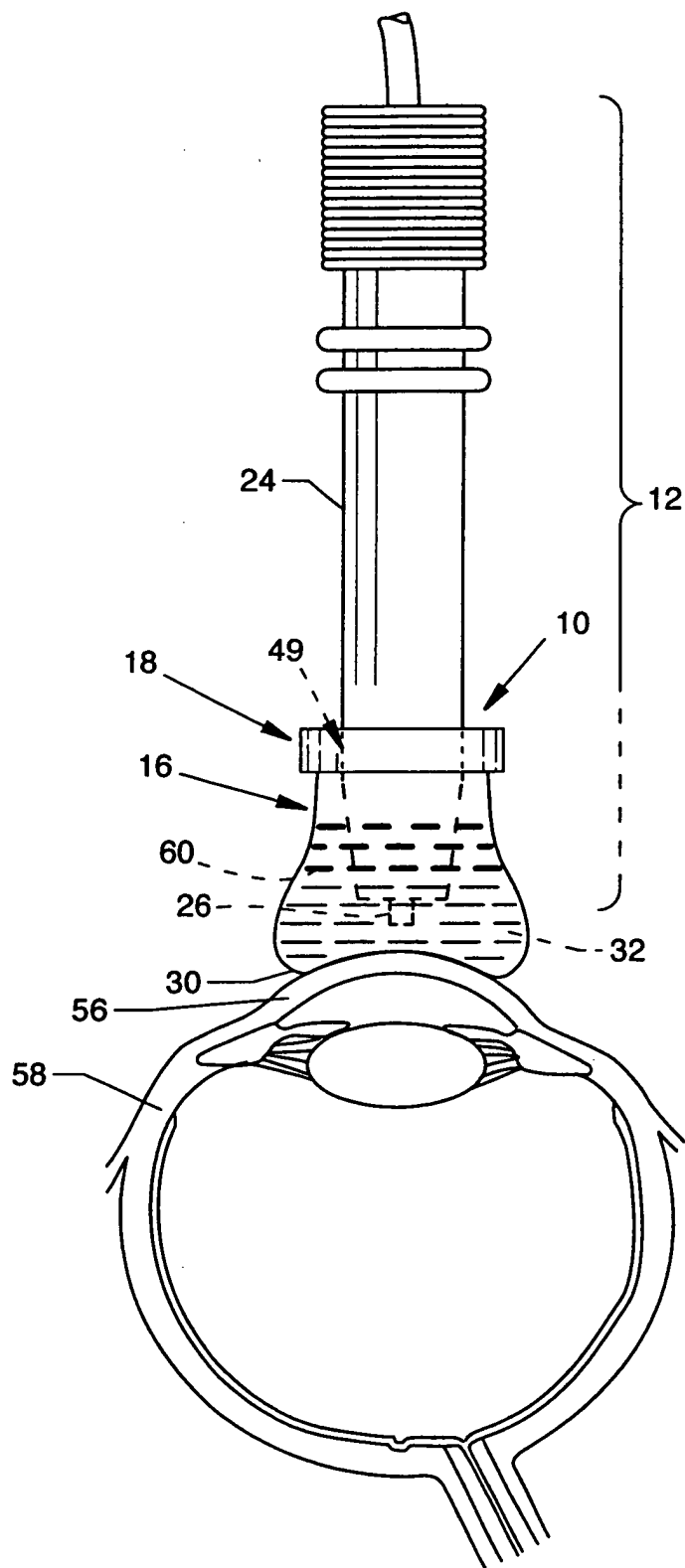


FIG. 7

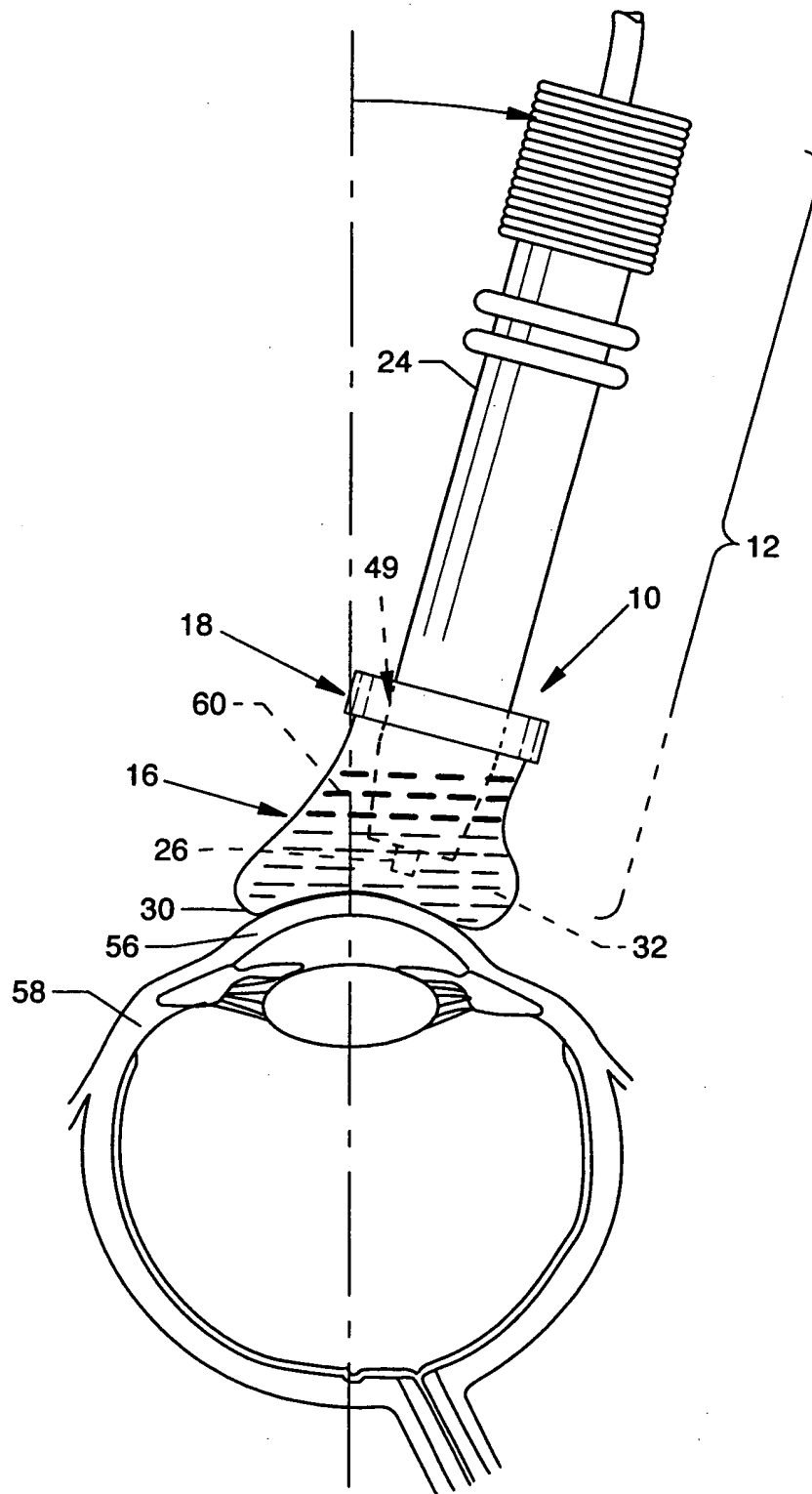


FIG. 8

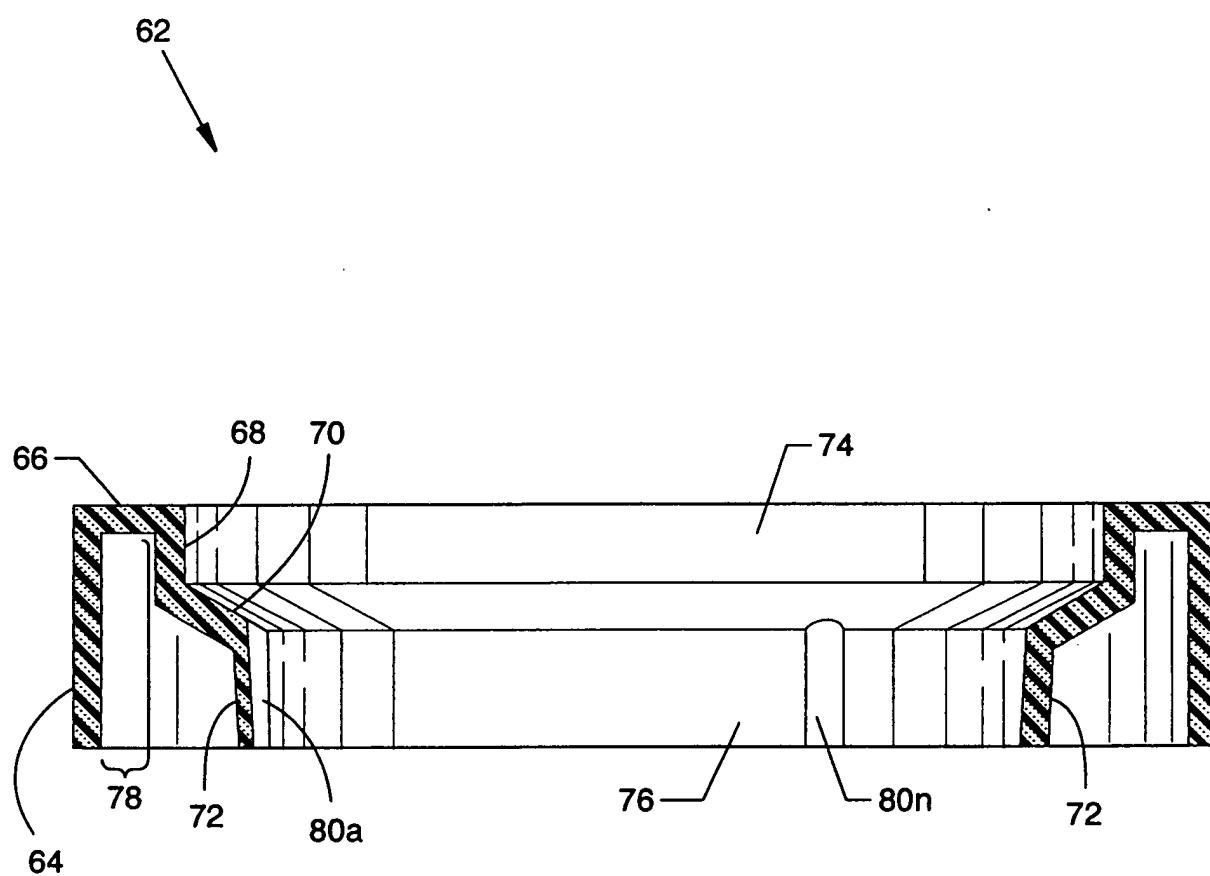


FIG. 9

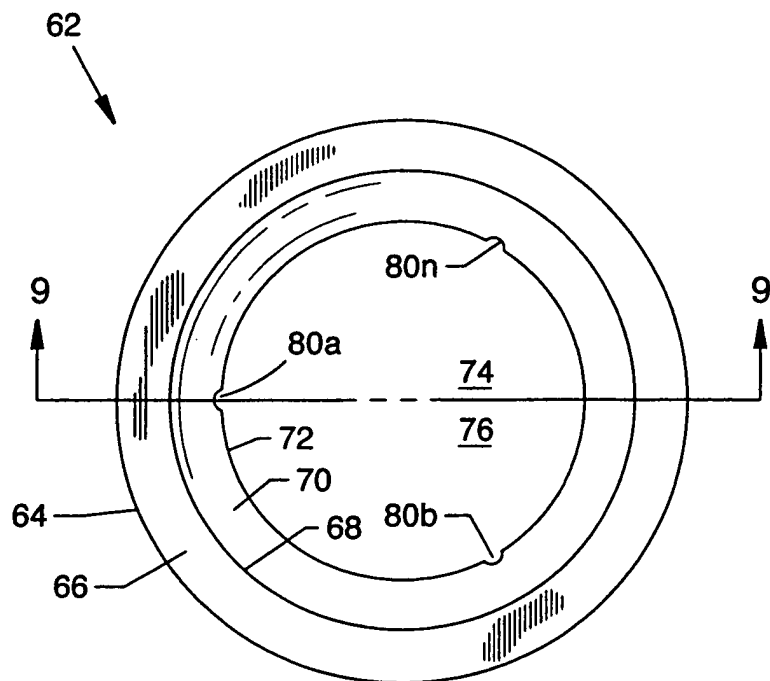


FIG. 10

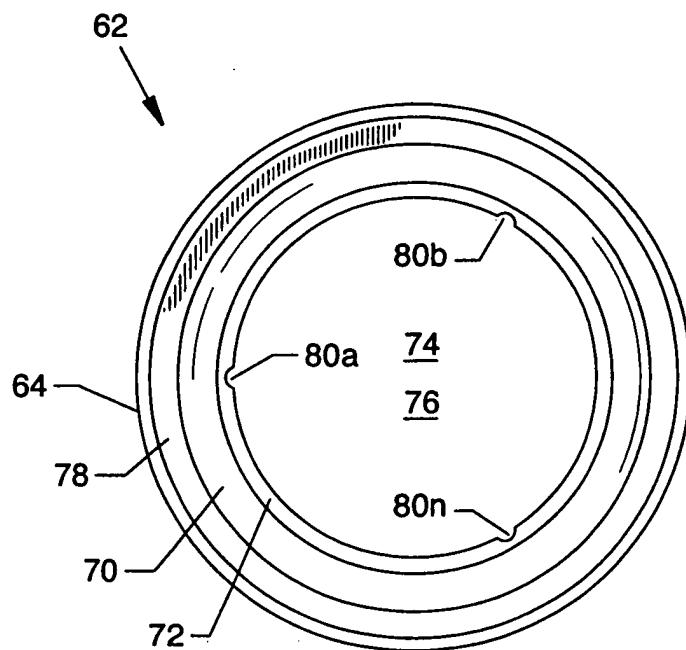


FIG. 11

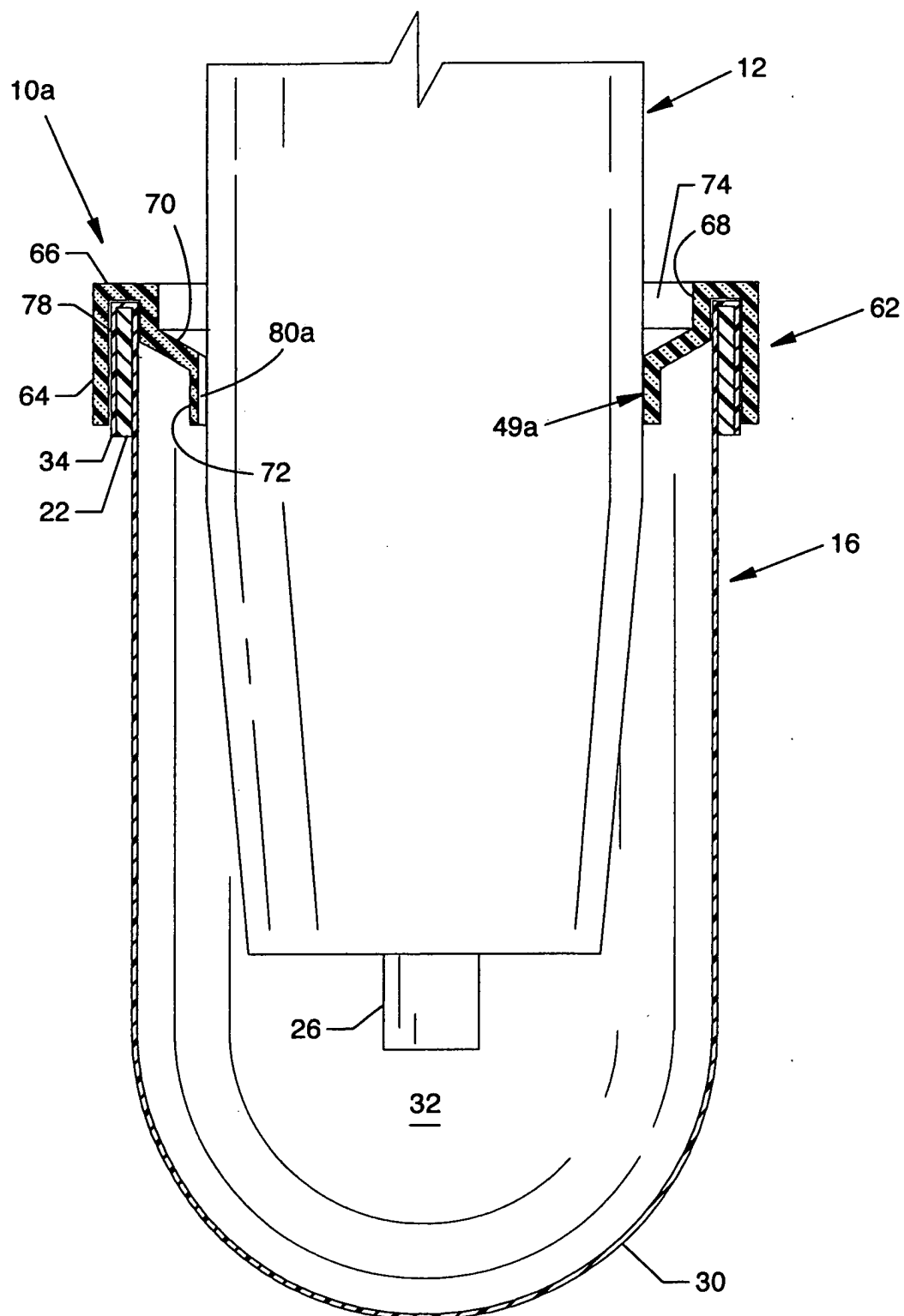


FIG. 12

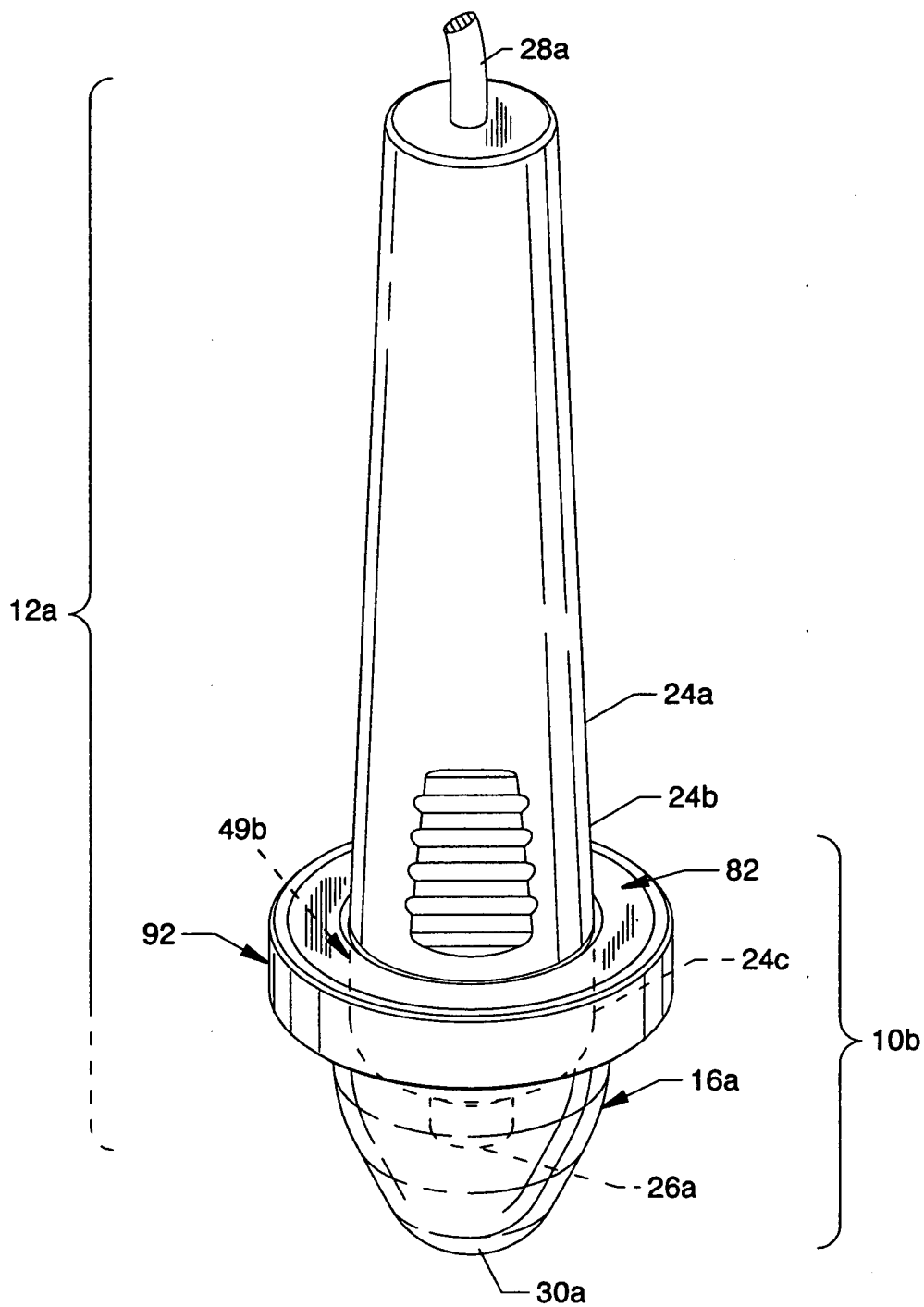


FIG. 13

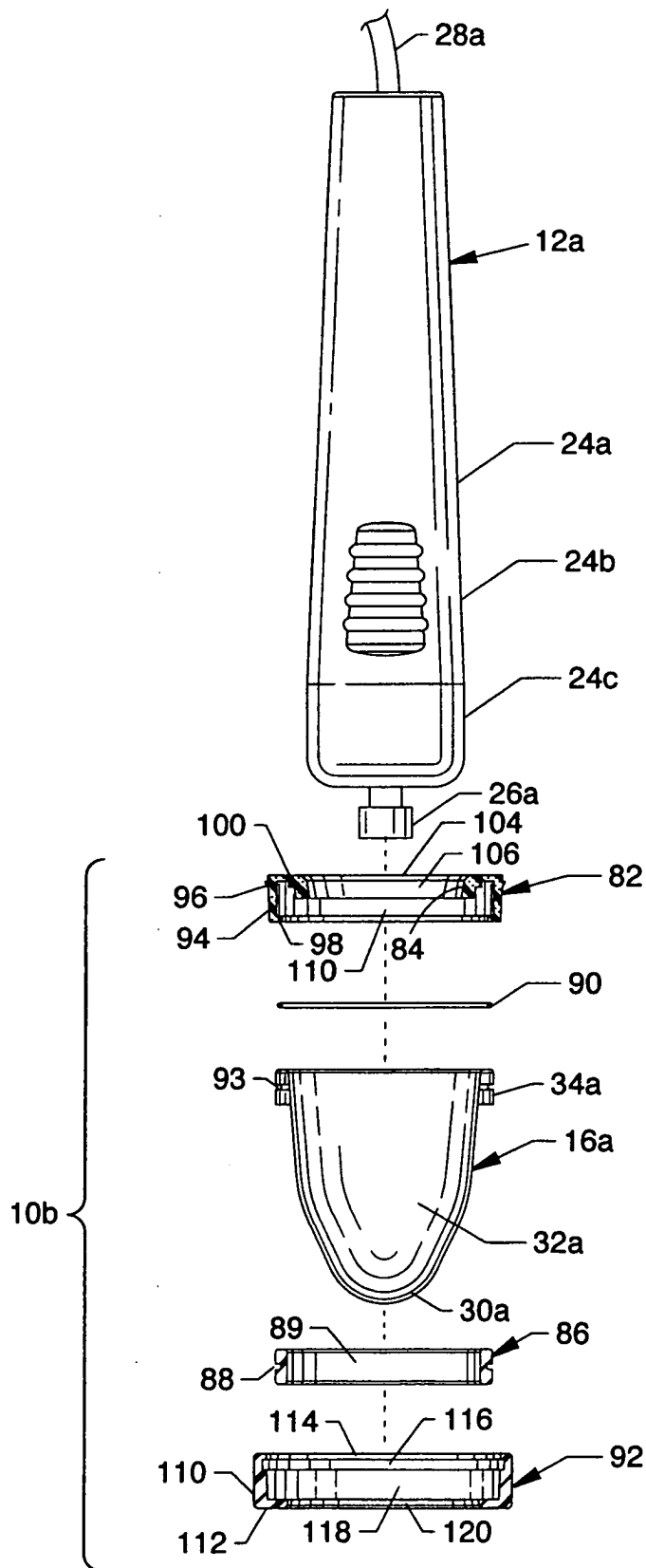


FIG. 14

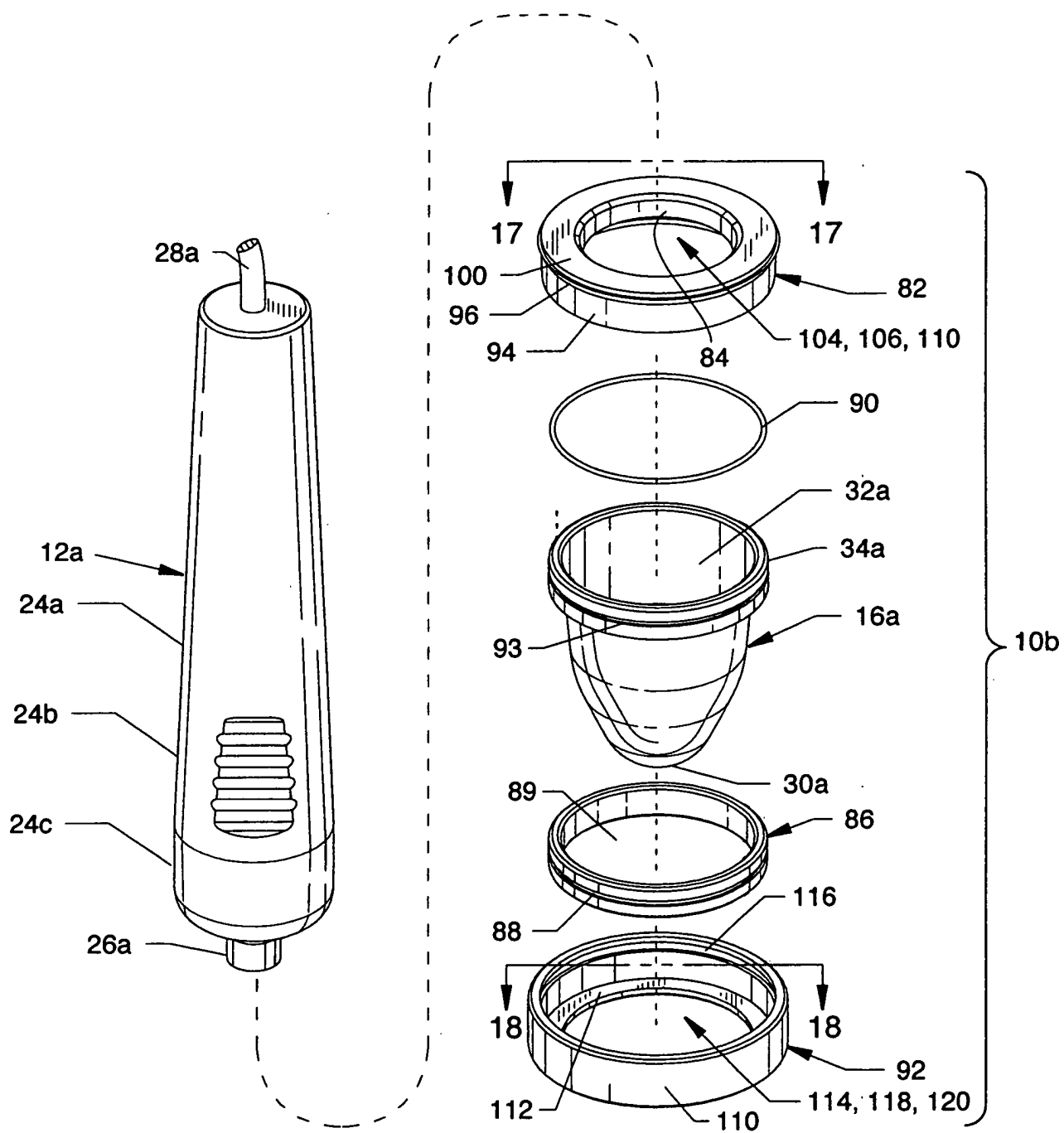


FIG. 15

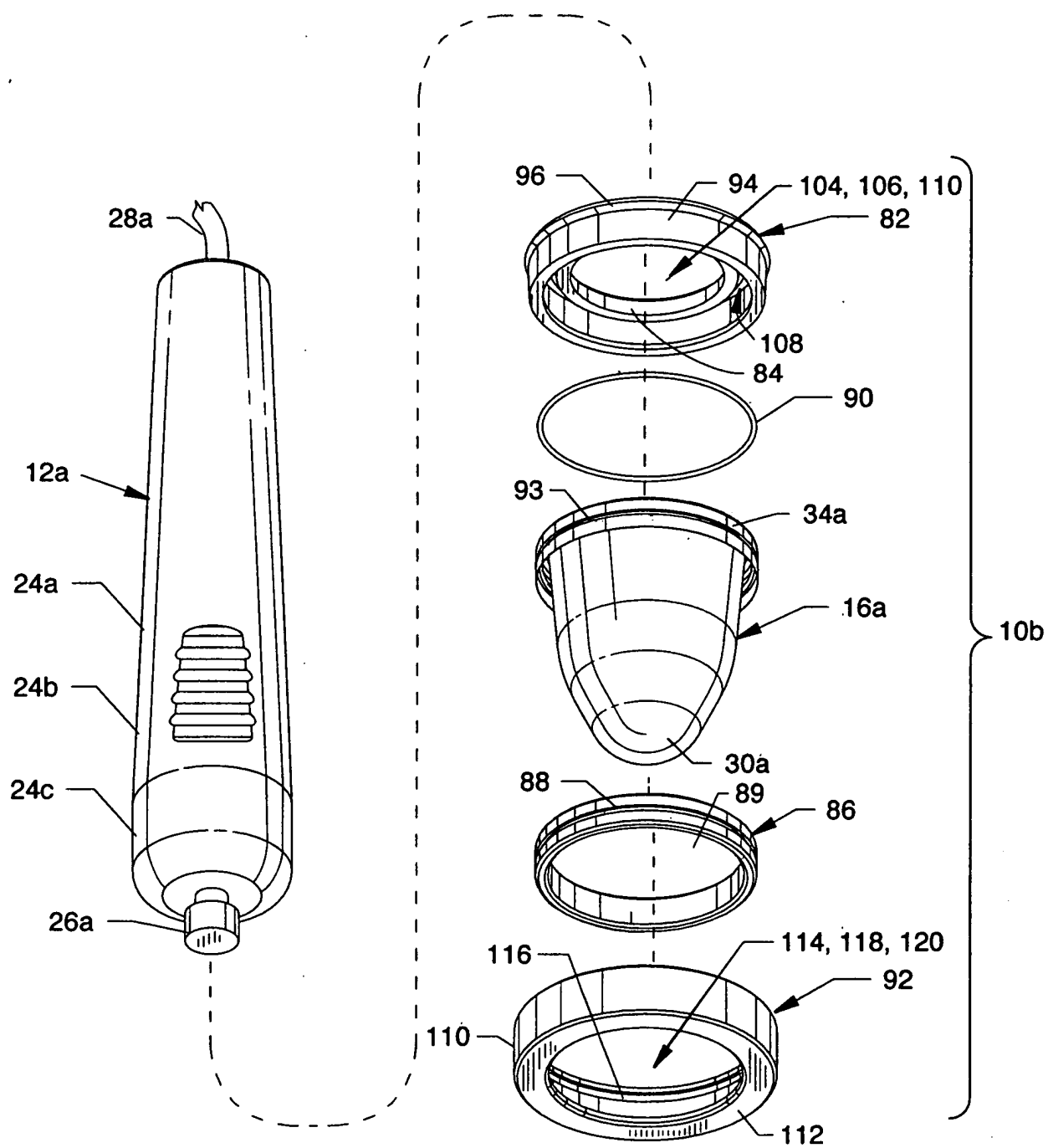


FIG. 16

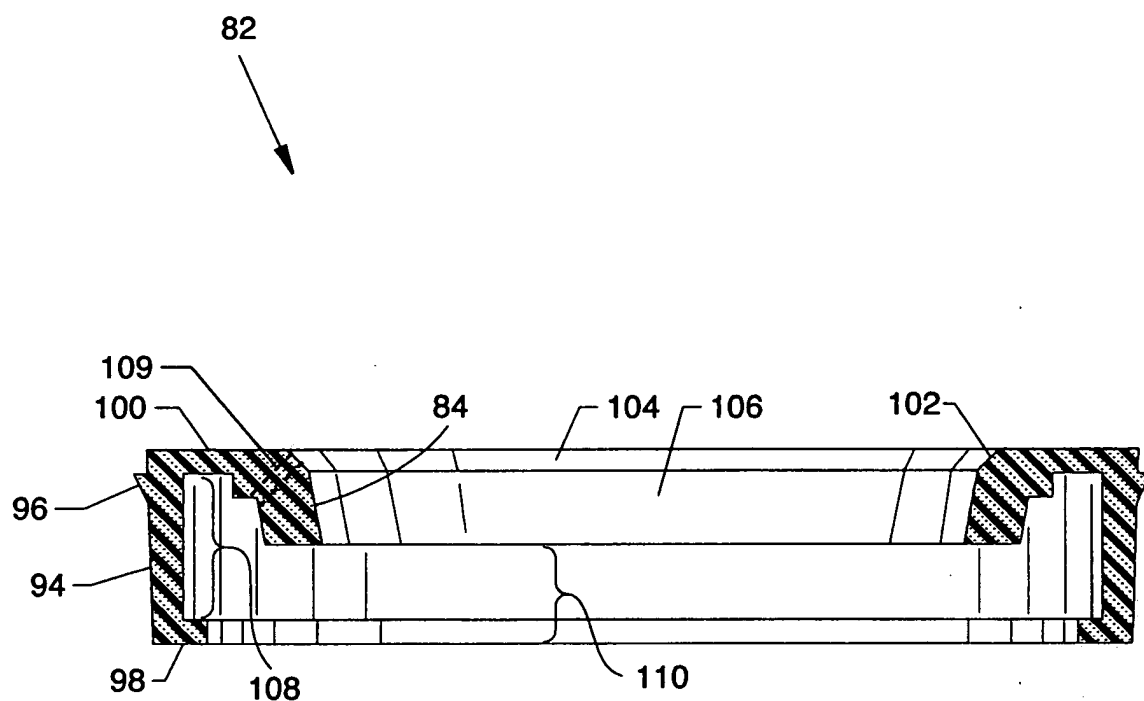


FIG. 17

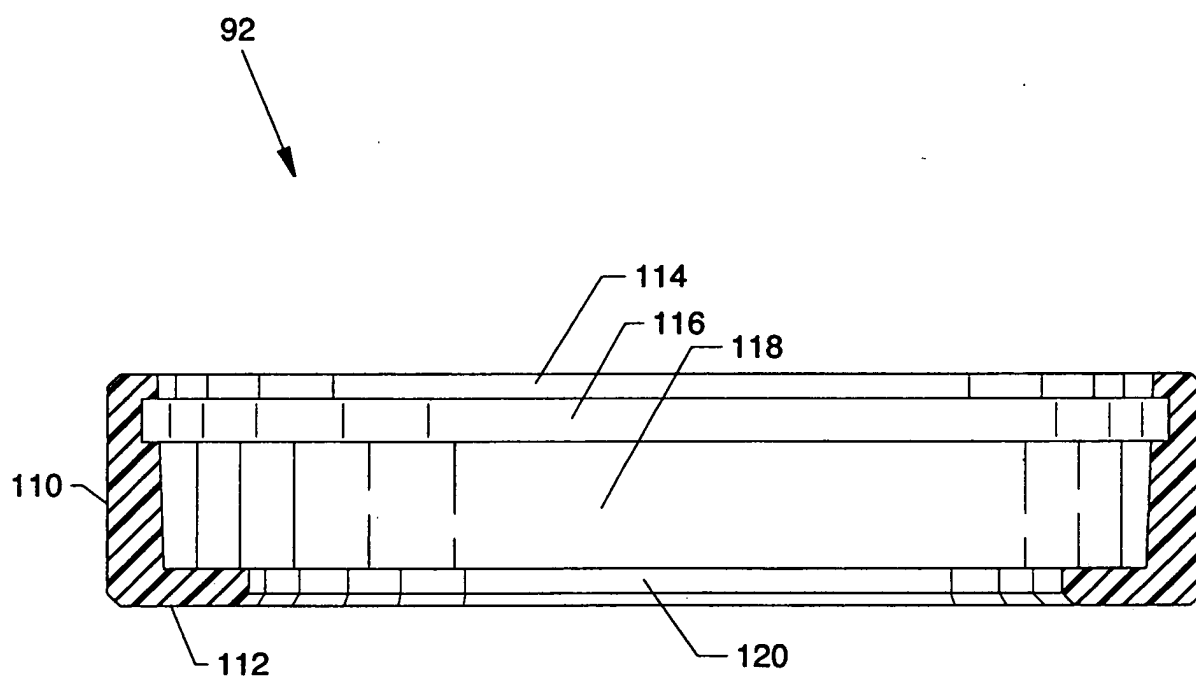


FIG. 18

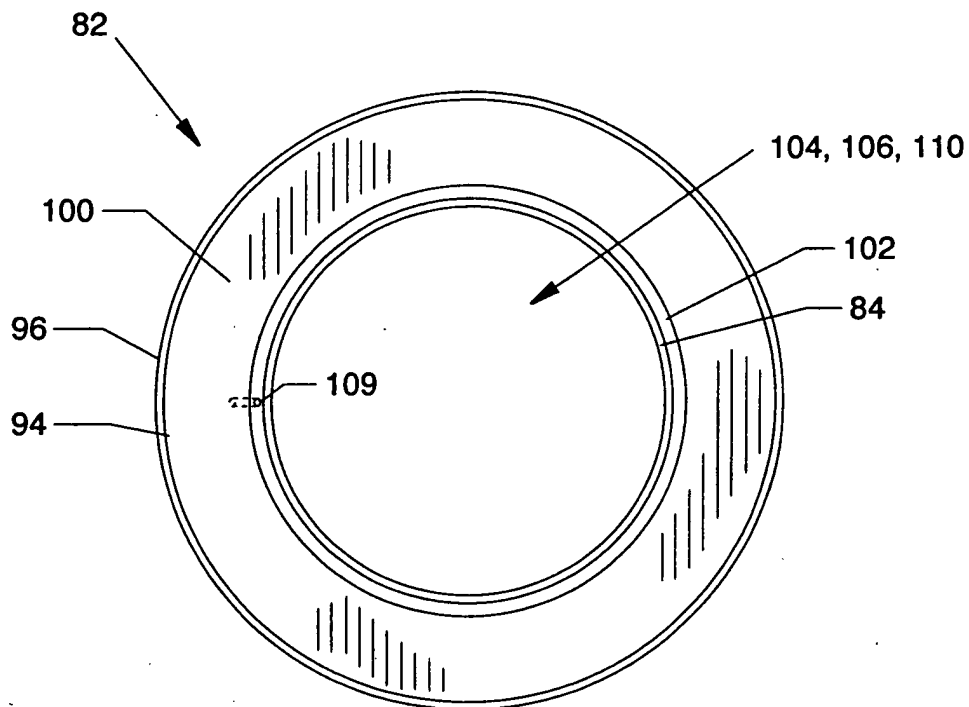


FIG. 19

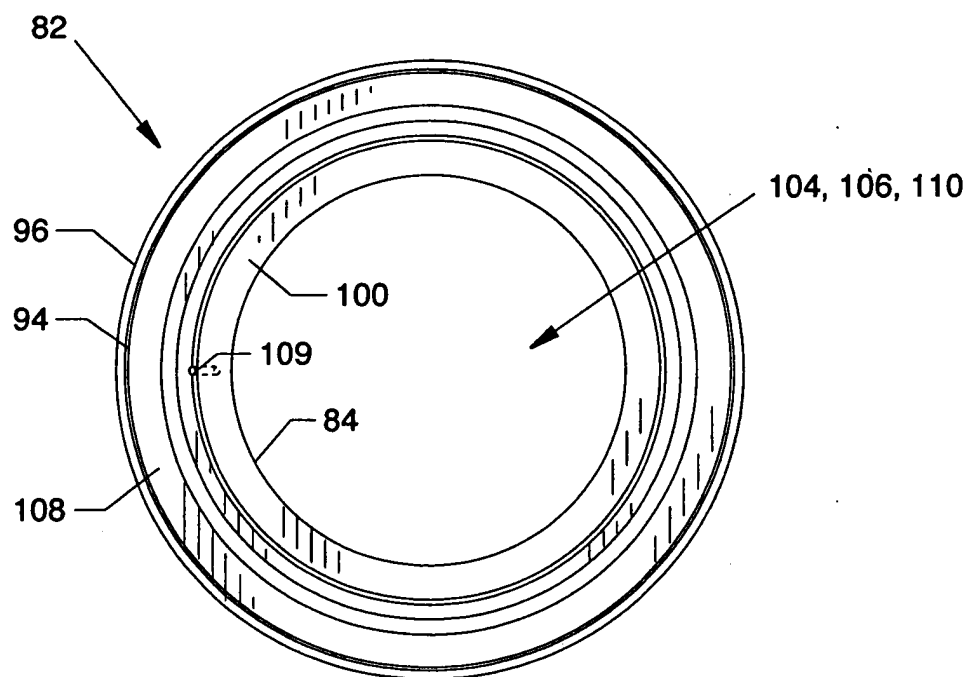


FIG. 20

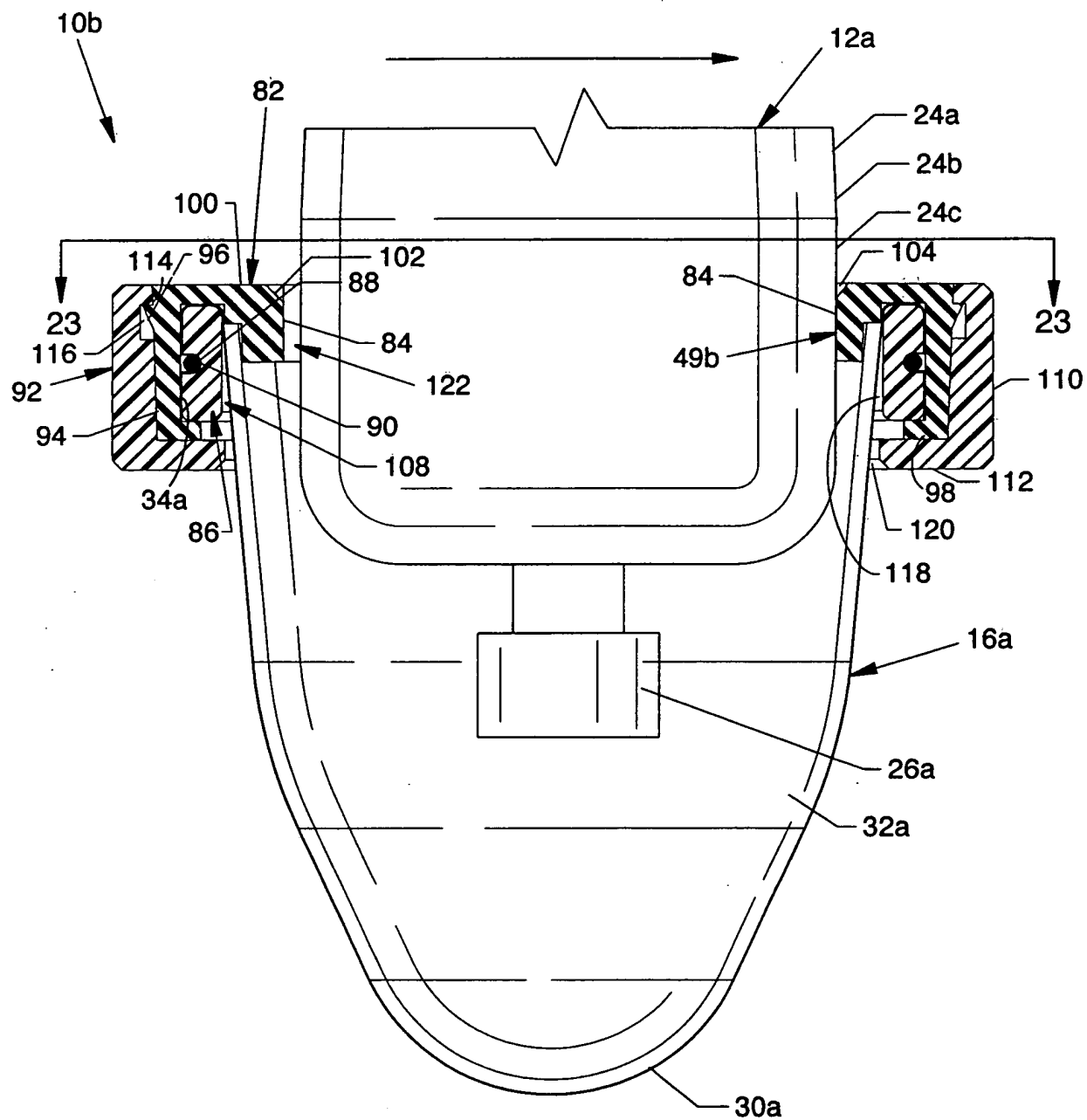


FIG. 22

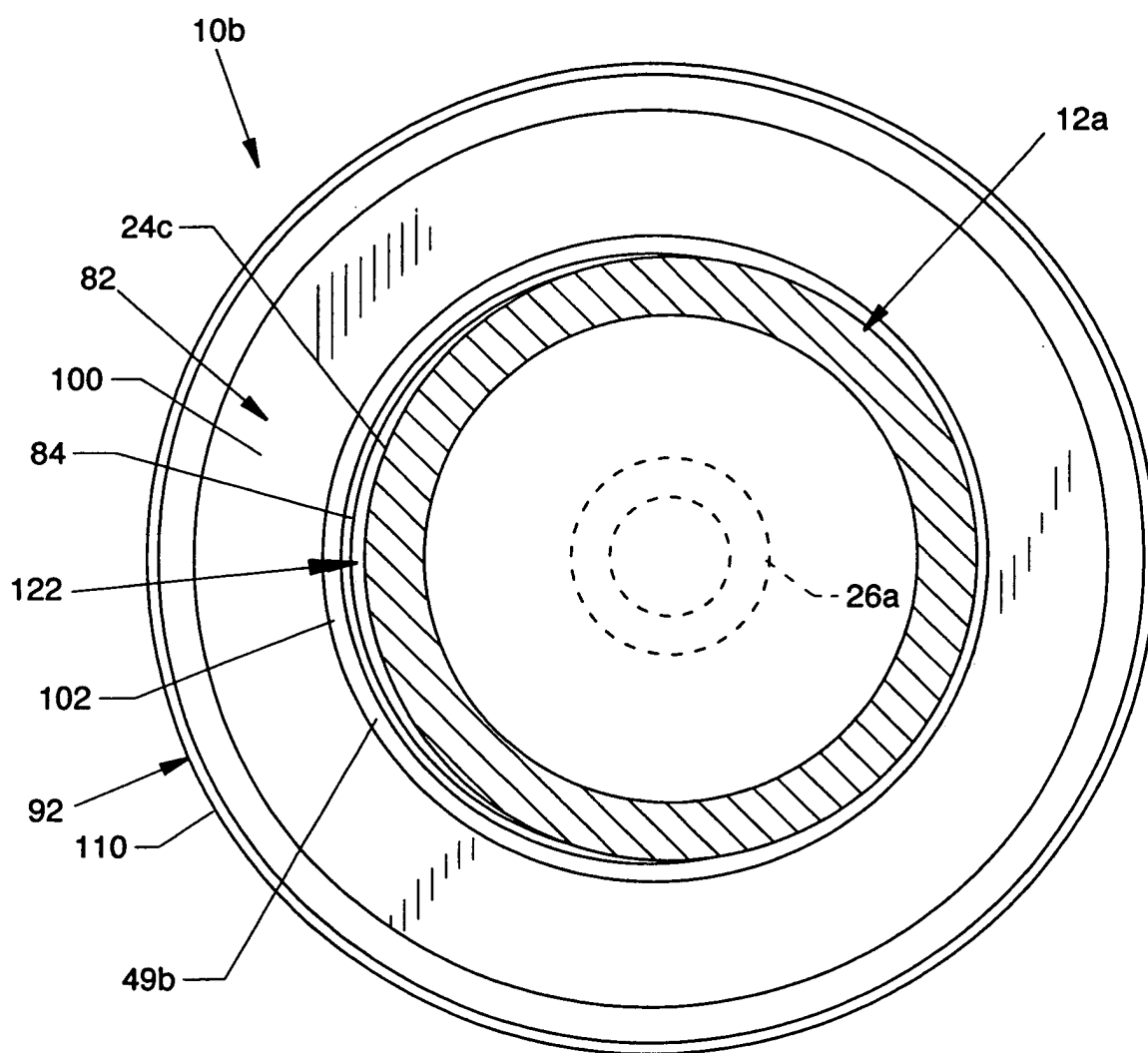


FIG. 23

专利名称(译)	浸入式袋系统，用于超声波探头		
公开(公告)号	EP2150221A2	公开(公告)日	2010-02-10
申请号	EP2008713232	申请日	2008-01-23
[标]申请(专利权)人(译)	ESI		
申请(专利权)人(译)	ESI , INC.		
当前申请(专利权)人(译)	ESI , INC.		
[标]发明人	PRAGER THOMAS C BURBA THOMAS A HARDTEN DAVID R RYDER WILLIAM T		
发明人	PRAGER, THOMAS, C. BURBA, THOMAS, A. HARDTEN, DAVID, R. RYDER, WILLIAM, T.		
IPC分类号	A61F9/007 A61B8/00		
CPC分类号	A61B8/4281 A61B8/10 G01N29/28		
优先权	11/701235 2007-02-01 US		
其他公开文献	EP2150221A4		
外部链接	Espacenet		

摘要(译)

一种与超声探头一起使用以克服近场伪影的浸没袋系统包括柔性薄壁厚度浸没袋，其具有附接的柔性套环，其具有整体内部密封。浸没袋包含凝胶或其他超声传输介质，并且通过相互形成的探针/密封阀密封地且可移除地附接到超声探针的尖端。浸没袋能够贴合角膜以及其他表面，无论是平坦的还是不规则的，从而使得超声探头能够容易地在这样的表面上使用。与浸没袋系统一起使用的超声探头保持在浸没袋的接触表面上方一定距离处，并且可围绕垂直轴定位，同时浸没袋保持与其接触的结构固定保形接触。