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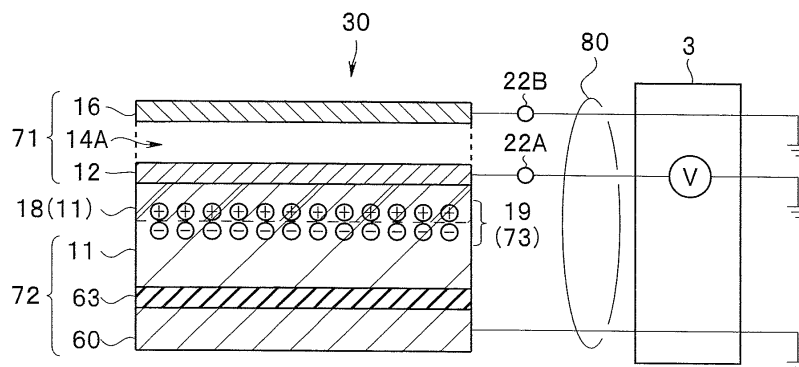
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(54) **ULTRASOUND UNIT AND ULTRASOUND ENDOSCOPE**

(57) An ultrasound unit 30 includes: ultrasound elements 20 each including a plurality of ultrasound cells 10 formed on a substrate 11 including a semiconductor, the plurality of ultrasound cells 10 each including an upper electrode 16 having a ground potential and a lower electrode 12 to which a drive signal is applied, the upper electrode 16 and the lower electrode 12 being arranged facing each other via a cavity 14A and thereby forming a first capacitor 71; a package member 60 in which the

plurality of ultrasound elements 20 are disposed, the package member 60 having a ground potential; and an insulation member 63 disposed between the package member 60 and each of the ultrasound elements 20. A second capacitor 72 is formed as a result of the insulation member 63 serving as a gap, and a capacity of a third capacitor 73 serially connected to the second capacitor 72 is smaller than a capacity of the second capacitor 72.

FIG.8



Description

Disclosure of Invention

Technical Field

Problem to be Solved by the Invention

[0001] The present invention relates to an ultrasound unit in which ultrasound elements each including capacitive micro-machined ultrasound cells formed on a semiconductor substrate are disposed on a package member via an insulation member, and an ultrasound endoscope including the ultrasound unit.

5 **[0007]** An object of an embodiment of the present invention is to provide an ultrasound unit having high receiving sensitivity, and an ultrasound endoscope including the ultrasound unit.

Background Art

10 Means for Solving the Problem

[0002] Ultrasound diagnosis in which a diagnosis is made by applying ultrasound to an object to be examined to form an image of a state of the inside of the body from echo signals is widespread. An ultrasound endoscope system is one of diagnostic apparatuses used for ultrasound diagnosis. An ultrasound endoscope includes an ultrasound unit disposed at a distal end portion of an insertion portion to be inserted into a body. The ultrasound unit has a function that converts electric signals to ultrasound and transmits the ultrasound to the inside of the body and receives the ultrasound reflected by the inside of the body and converts the ultrasound to electric signals.

[0008] An ultrasound unit according to an embodiment of the present invention includes: ultrasound elements each including a plurality of ultrasound cells formed on a substrate including a semiconductor, the plurality of ultrasound cells each including an upper electrode having a ground potential and a lower electrode to which a drive signal is applied, the upper electrode and the lower electrode being arranged facing each other via a cavity and thereby forming a first capacitor; a package member in which the plurality of the ultrasound elements are disposed, the package member having a ground potential; and an insulation member disposed between the package member and each of the ultrasound elements. A second capacitor is formed as a result of the insulation member serving as a gap, and a capacity of a third capacitor formed so as to be serially connected to the second capacitor is smaller than a capacity of the second capacitor.

[0003] As an ultrasound cell for an ultrasound unit, Japanese Patent Application Laid-Open Publication No. 2006-50314 discloses a capacitive micro-machined ultrasonic transducer (cMUT) manufactured using an MEMS technique.

[0009] Also, an ultrasound endoscope according to another embodiment includes: an insertion portion including a distal end portion in which an ultrasound unit is disposed, the ultrasound unit including ultrasound elements each including a plurality of ultrasound cells formed on a substrate including a semiconductor, the plurality of ultrasound cells each including an upper electrode having a ground potential and a lower electrode to which a drive signal is applied, the upper electrode and the lower electrode being arranged facing each other via a cavity and thereby forming a first capacitor, a package member in which the plurality of the ultrasound elements are disposed, the package member having a ground potential, and an insulation member disposed between the package member and each of the ultrasound elements, in which a second capacitor is formed as a result of the insulation member serving as a gap and a capacity of a third capacitor formed so as to be serially connected to the second capacitor is smaller than a capacity of the second capacitor; an operation portion disposed on a proximal end portion side of the insertion portion; and a universal cord provided so as to extend from the operation portion.

[0004] An ultrasound cell for a cMUT transmits/receives ultrasound by means of vibration of a membrane including an upper electrode arranged facing a lower electrode via a cavity. In transmission, upon application of a voltage between the electrodes, the upper electrode is pulled to the lower electrode by an electrostatic force, whereby the membrane including the upper electrode is deformed. When the voltage application ceases, the membrane recovers to its original shape by means of an elastic force. Ultrasound is generated by the deformation/recovery of the membrane.

[0005] On the other hand, in reception, the membrane is deformed by received ultrasound energy, whereby a distance between the upper electrode and the lower electrode changes. Using a change of a capacity C1 of a capacitor formed by the upper electrode and the lower electrode by ΔC , the received ultrasound energy is converted to an electric signal.

[0006] Here, because of, e.g., the structure of the ultrasound unit, a parasitic capacity Cp, which is not changed by the received ultrasound energy, may be added to the capacity C1 of the capacitor based on which a reception signal is formed. In that case, a capacity change rate decreases from $\Delta C/C1$ to $\Delta C/(C1+Cp)$ even where the received ultrasound energy has a same strength, resulting in receiving sensitivity decrease.

Advantage of the Invention

55 **[0010]** An embodiment of the present invention enables provision of an ultrasound unit having high receiving sensitivity, and an ultrasound endoscope including the ultrasound unit.

Brief Description of the Drawings

[0011]

Fig. 1 is a diagram of a configuration of an endoscope system including an ultrasound endoscope according to an embodiment;

Fig. 2 is a perspective view of a distal end portion of the ultrasound endoscope according to the embodiment;

Fig. 3 is a perspective view of an ultrasound unit according to the embodiment;

Fig. 4 is an exploded view of the ultrasound unit according to the embodiment;

Fig. 5 is a cross-sectional view of the ultrasound unit according to the first embodiment along line V-V in Fig. 4;

Fig. 6 is a diagram illustrating a configuration of a conventional ultrasound unit;

Fig. 7 is a diagram of an equivalent circuit in the conventional ultrasound unit;

Fig. 8 is a diagram illustrating a configuration of the ultrasound unit according to the first embodiment;

Fig. 9 is a diagram of an equivalent circuit in the ultrasound unit according to the first embodiment;

Fig. 10 is a diagram of a configuration of an ultrasound unit according to a second embodiment; and

Fig. 11 is a diagram of an equivalent circuit in the ultrasound unit according to the second embodiment.

Best Mode for Carrying Out the Invention

<First Embodiment>

[0012] An ultrasound unit 30 and an ultrasound endoscope 2 including the ultrasound unit 30 (hereinafter referred to as "ultrasound unit 30 and the like") according to a first embodiment will be described with reference to the drawings. Note that each of the drawings is a schematic diagram for description and, e.g., counts and sizes of components and ratios in size among the components are different from those of actual ones.

<Configuration of ultrasound endoscope>

[0013] As illustrated in Fig. 1, the ultrasound endoscope 2 provides an ultrasound endoscope system 1 jointly with an ultrasound observation apparatus 3 and a monitor 4. The ultrasound endoscope 2 includes an elongated insertion portion 41 to be inserted into a body, an operation portion 42 disposed at a proximal end of the insertion portion 41, and a universal cord 43 extending from the operation portion 42.

[0014] A connector 44A to be connected to a light source apparatus (not illustrated) is disposed at a proximal end portion of the universal cord 43. A cable 45 to be connected to a camera control unit (not illustrated) via

a connector 45A, and a cable 46 to be connected to the ultrasound observation apparatus 3 via a connector 46A extend from the connector 44A. The monitor 4 is connected to the ultrasound observation apparatus 3.

[0015] The insertion portion 41 is provided by providing a distal end rigid portion (hereinafter referred to as "distal end portion") 47, a bending portion 48 positioned at a rear end of the distal end portion 47 and a flexible tube portion 49 positioned at a rear end of the bending portion 48, the flexible tube portion 49 having a small diameter, a long length and flexibility and leading to the operation portion 42, consecutively in this order from the distal end side.

[0016] As illustrated in Fig. 2, in the distal end portion 47 of the insertion portion 41, the ultrasound unit 30 in which a plurality of ultrasound elements 20 are radially arranged is disposed. Note that the ultrasound unit may be of a convex scanning type in which a plurality of ultrasound elements 20 are arranged in a convex shape or of a linear scanning type in which a plurality of ultrasound elements 20 are arranged on a planar surface.

<Configuration of ultrasound unit>

[0017] Next, a configuration of the ultrasound unit 30 will be described with reference to Figs. 3, 4 and 5. Note that in Fig. 4, etc., a package member 60 is illustrated in a flat plate shape.

[0018] As illustrated in Fig. 3, the ultrasound unit 30 is a radial transducer in which a plurality of ultrasound elements 20 each having a rectangular shape in plan view are cylindrically arranged at regular intervals on an outer circumferential face of the package member 60 having a cylindrical shape in such a manner that long sides of the ultrasound elements 20 are parallel to one another.

[0019] As illustrated in Fig. 4, an insulation member 63 including a backing material 61 and joining layers 62A and 62B are disposed between each ultrasound element 20 and the package member 60. Each ultrasound element 20, which is a basic unit that transmits/receives ultrasound, includes a silicon substrate 11 as a base, the silicon substrate 11 including a first principal surface 20SA and a second principal surface 20SB facing the first principal surface 20SA. In a roughly center portion of the first principal surface 20SA of the ultrasound element 20, a transmission/reception section 21 that transmits/receives ultrasound is formed, and in opposite end portions of the first principal surface 20SA, respective external electrodes 22A and 22B are disposed. As illustrated in Fig. 3, the external electrodes 22A and 22B are connected to respective lead wires 81A and 81B of cables 80. The lead wires 81B are ground potential wires and may be a common wiring for the plurality of ultrasound elements 20. For example, shield wires of the cable 80 can be used as the lead wires 81B.

[0020] The cable 80 is inserted through the distal end portion 47, the bending portion 48, the flexible tube portion 49, the operation portion 42, the universal cord 43

and the cable 46, and is connected to the ultrasound observation apparatus 3 via the connector 46A.

[0021] In the transmission/reception section 21, a plurality of capacitive micro-machined ultrasound cells 10 are arranged in a matrix. Note that Fig. 4 schematically illustrates only a part of the ultrasound cells 10. Also, the ultrasound cells 10 may be arranged in such a manner that the ultrasound cells 10 are fitted in a recess portion formed in the substrate.

[0022] As illustrated in Fig. 5, in each of the ultrasound cells 10 formed on the silicon substrate 11, an upper electrode 16, which is included in a membrane, is arranged facing a lower electrode 12 via a cavity (void portion) 14A. The cavity (void portion) 14A is formed by etching of an interelectrode insulation layer 14. Note that an upper insulation layer and a protection film, which are not illustrated, are formed on the upper electrode 16.

[0023] Also, on the silicon substrate 11, an insulation layer 15 including silicon oxide is formed; however, the insulation layer 15 includes through holes and thus the lower electrode 12 and the silicon substrate are electrically connected. In other words, the insulation layer 15 can be regarded as being virtually not formed.

[0024] Note that the external electrode 22A of the ultrasound element 20 is a common electrode for the lower electrode 12 of the plurality of ultrasound cells 10, and the external electrode 22B is a common electrode for the upper electrode 16 of the plurality of ultrasound cells 10. Thus, the plurality of ultrasound cells 10 included in one ultrasound element 20 is simultaneously driven.

[0025] The package member 60 includes a conductive material such as SUS, but may include a conductive layer formed on at least one surface of a non-conductive base material such as a resin. For safety, a conductive member to be inserted into a living body is maintained at the ground potential. In other words, the package member 60 is maintained at the ground potential, as with the upper electrodes 16, via a non-illustrated lead wire. The package member 60 may be connected to the lead wires 81B that maintain the upper electrodes 16 at the ground potential.

[0026] The plurality of ultrasound elements 20 are disposed on the outer circumferential face of the package member 60 by the respective joining layers 62 (62A and 62B) via the respective backing materials 61.

[0027] For the backing materials 61 that absorb unnecessary ultrasound, any of various materials can be used and either an inorganic material or an organic material can be employed. In particular, a material obtained by mixing a filler into an epoxy-based resin or a rubber-based material having a large attenuation rate is preferable because such material can effectively absorb unnecessary vibration. For the filler, it is preferable to use a material having a density that is higher than that of the epoxy resin or the rubber-based material, which is a matrix material, because such material can further effectively attenuate unnecessary vibration. Also, for the joining layers 62 (62A and 62B), it is preferable to use, e.g., an

epoxy-based adhesive containing 0.5 to 2% of a silane coupling agent.

[0028] The backing material 61 and the joining layers 62A and 62B, which each include an elastic member, are all insulating materials, and can be regarded as one insulation member 63 as a whole. The insulation member 63 may arbitrarily be set according to the materials, sizes and the like of the respective components, for example, in such a manner that a thickness of the backing material 61 is set to 50 to 200 μm and respective thicknesses of the joining layers 62A and 62B are set to 0.5 to 2.0 μm . Also, a structure that does not have three joining layers, that is, uses no backing material 61 may be employed, and in this case, an unitary insulation member 63 is made to have a thickness that is equal to or exceeds a thickness enough to ensure insulation required for driving the ultrasound element 20 for transmission/reception.

[0029] Then, in the silicon substrate 11, a low-resistance diffusion layer 18 having a polarity that is different from that of the substrate is formed. For example, if the silicon substrate 11 is a p-type semiconductor containing a triad such as boron, an n-type diffusion layer 18 in which a pentad such as phosphorus has been doped from the first principal surface 20SA. The diffusion layer 18 has an impurity density that is higher than that of the silicon substrate 11. In other words, the silicon substrate 11 is a p-semiconductor, and the diffusion layer 18 is an n-semiconductor.

<Operation of ultrasound unit>

[0030] In ultrasound transmission, a drive signal (voltage) is applied to the lower electrodes 12 via the lead wires 81 B and the external electrodes 22A by the control performed by the ultrasound observation apparatus 3. For example, in the case of an n+ diffusion layer and a p-substrate, a positive drive voltage that is higher than the ground potential is applied. On the other hand, in the case of a p+ diffusion layer and an n-substrate, a negative drive voltage that is lower than the ground potential is applied. The upper electrode 16 and the package member 60 are maintained at the ground potential. Note that, in the ultrasound endoscope 2, the upper electrode 16, which is close to the outside, has the ground potential, and thus, the ultrasound endoscope 2 is safer than endoscopes that allow a voltage to be applied to upper electrodes 16.

[0031] On the other hand, in ultrasound reception, the capacities C1 between the lower electrodes 12 and the upper electrodes 16 are measured via the respective external electrodes 22A and 22B by the control performed by the ultrasound observation apparatus 3. In other words, a capacity change ΔC of each first capacitor 71 formed by the relevant lower electrode 12 and the relevant upper electrode 16 with the relevant cavity 14A serving as a gap. In this case, it is preferable that a bias voltage be applied to the lower electrodes 12. The bias voltage has a polarity that is the same as that of the drive

voltage.

[0032] As illustrated in Figs. 6 and 7, in a conventional ultrasound unit 130, a second capacitor 72 having a capacity C_2 , which is formed between a silicon substrate 111 (lower electrode 12) and a package member 60 with an insulation member 63 serving as a gap, is connected in parallel to a first capacitor 71. Furthermore, an overlap region in which an interelectrode insulation layer 14 is interposed between the lower electrode 12 and an upper electrode 16 provides a parasitic capacity whose capacity value does not change, and a sum of a capacity C_0 of the overlap region and C_2 is a total parasitic capacity C_p .

[0033] As a result, as already described, if the capacity of the first capacitor 71 changes by ΔC , the capacity change rate D (%) measured via external electrodes 22A and 22B decreases from $\Delta C/C_1$ to $\Delta C/(C_1+C_p)$ because of the total parasitic capacity C_p . Note that for the below numeric value calculation (estimation), C_0 is regarded as sufficiently small compared to the other capacities. In other words, it is regarded that $C_p = C_2$; however, even if $C_p > C_2$, the embodiment exerts sufficient effects.

[0034] For example, where $C_1 = 13$ pF, $C_2 = 5.3$ pF and $\Delta C = 1.3$ pF, the capacity change rate D decreases from 10.0% to 7.1 %.

[0035] On the other hand, as illustrated in Figs. 8 and 9, in the ultrasound unit 30, upon application of a positive voltage to the lower electrode 12, a potential of the diffusion layer 18 becomes a positive potential, whereby electrons move to the diffusion layer side of the silicon substrate 11. As a result, a depletion layer 19 is formed inside the silicon substrate 11. Since the depletion layer 19 has no conductivity, a third capacitor 73 in which the depletion layer 19 serves as a gap is formed.

[0036] Here, a thickness of the depletion layer 19, that is, a gap length of the third capacitor 73 is nearly 500 μm where the silicon substrate 11, which is a p-semiconductor, has an acceptor density of $5 \times 10^{11} \text{ cm}^{-3}$, the diffusion layer 18, which is an n+ semiconductor, has a donor density of $5 \times 10^{19} \text{ cm}^{-3}$, and an applied voltage is 100V. Thus, where the depletion layer 19 has a permittivity of 11.9, a capacity C_3 of the third capacitor 73 is 1.2 pF.

[0037] As illustrated in Fig. 9, the third capacitor 73 is serially connected to a second capacitor 72 having a capacity C_2 , which is formed as a result of the insulation member 63 serving as a gap, and a sum of the capacities C_2 and C_3 and a capacity C_0 of an overlap region is a total parasitic capacity C_p . A combined capacity C_{10} of the second capacitor 72 and the third capacitor 73 serially connected can be obtained by $C_{10} = (C_2 \times C_3)/(C_2 + C_3)$. In other words, $C_2 > C_{10}$. Here, also, C_0 is regarded as sufficiently small compared to the other capacities, and it is regarded as $C_p = C_{10}$; however, implementation of the present invention is not limited to such calculation method as above.

[0038] In other words, as is publicly known, where the second capacitor 72 and the third capacitor 73 are serially connected, the combined capacity C_{10} becomes smaller

than each of the capacity C_2 of the second capacitor 72 and the capacity C_3 of the third capacitor 73, and the capacity of the capacitor having a smaller capacity becomes dominant. Here, the capacity C_3 of the third capacitor 73 is smaller than the capacity C_2 of the second capacitor 72. Thus, $C_2 > C_{10}$.

[0039] Since the parasitic capacity C_p decreases from C_2 to C_{10} , if the capacity of the first capacitor 71 changes by ΔC , the capacity change rate D (%) measured via the external electrodes 22A and 22B increases from $\Delta C/(C_1+C_2)$ to $\Delta C/(C_1+C_{10})$ compared to cases where no third capacitor 73 is formed.

[0040] For example, where $C_1 = 13$ pF, $C_2 = 5.3$ pF, $C_3 = 1.2$ pF and $\Delta C = 1.3$ pF, the capacity change rate D increases from 7.1% to 9.3%.

[0041] As described above, an ultrasound unit 30 including ultrasound elements 20 in which a low-resistance diffusion layer 18 having a polarity that is different from that of a silicon substrate 11 is formed in the substrate 11 and a third capacitor 73 is formed as a result of a depletion layer 19, which is formed inside the substrate 11 by the diffusion layer 18, serving as a gap has high receiving sensitivity.

[0042] Note that if a negative voltage is applied to the lower electrode 12, effects that are the same as those of the ultrasound unit 30 can be provided by making the silicon substrate be an n- semiconductor and making the diffusion layer be a p+ semiconductor.

[0043] Although the capacity C_3 of the third capacitor is selected in connection with the capacity C_2 of the second capacitor, for further sensitivity enhancement, preferably $C_3 \leq 0.5 \times C_2$, more preferably, $C_3 \leq 0.1 \times C_2$.

[0044] As described above, for reduction of the parasitic capacity C_p , it is only necessary that the third capacitor be serially connected to the second capacitor formed as a result of the insulation member 63 serving as a gap. Thus, not only a method in which a diffusion layer 18 is formed in advance so as to form a third capacitor inside the silicon substrate 11, but also, for example, a method in which a third capacitor is formed by disposing a capacitor having a small capacity at a position halfway through the ground potential wire to which the package member 60 is connected may be employed.

[0045] However, the method in which the diffusion layer 18 is formed in advance according to the embodiment largely facilitates a manufacturing step for disposing a small-capacity capacitor, and thus, is suitable for mass production. In other words, ultrasound elements 20 are obtained by manufacturing the ultrasound elements 20 in one silicon wafer and cutting the silicon wafer into pieces. Thus, it is only necessary to form a diffusion layer on a silicon wafer first in a manufacturing process. Also, the method is particularly preferable because the number of components in the ultrasound unit 30 does not increase.

<Second Embodiment>

[0046] An ultrasound unit 30A and an ultrasound en-

doscope 2A including the ultrasound unit 30A (hereinafter referred to as "ultrasound unit 30A and the like") according to a second embodiment will be described below. Since the ultrasound unit 30A and the like are similar to the ultrasound unit 30 and the like, components having same functions as those of the ultrasound unit 30 and the like are provided with same reference numerals as those of the ultrasound unit 30 and the like and description thereof will be omitted.

[0047] Since the ultrasound unit 30A includes no through holes in an insulation layer 15 of each ultrasound element 20, a lower electrode 12 and a silicon substrate 11 are insulated from each other. Thus, as illustrated in Figs. 10 and 11, a fourth capacitor 74 (capacity C4) in which an insulation layer 15 serves as a gap is provided.

[0048] In the ultrasound unit 30A, upon application of a positive voltage to the lower electrode 12, the insulation layer 15 side of a diffusion layer 18 becomes a negative potential layer, and the opposite side (package member side) becomes a positive potential layer. Thus, as in the ultrasound unit 30, a depletion layer 19 is formed inside the silicon substrate 11. Since the depletion layer 19 has no conductivity, a third capacitor 73 in which the depletion layer 19 serves as a gap is formed.

[0049] As illustrated in Fig. 11, the third capacitor 73 and the fourth capacitor 74 are serially connected to a second capacitor 72 having a capacity C2, which is formed as a result of an insulation member 63 serving as a gap, a sum of an overlap capacity Co and the capacities C2, C3 and C4 is a total parasitic capacity Cp. A combined capacity C11 of the second capacitor 72, the third capacitor 73 and the fourth capacitor 74 serially connected can be obtained by $C11 = (C2 \times C3 \times C4) / (C2 \times C3 + C2 \times C4 + C3 \times C4)$. If the insulation layer 15 is thin, the capacity C4 of the fourth capacitor 74 is relatively large; however, $C2 > C11$. Here, also, Co is regarded as sufficiently small compared to the other capacities, and it is regarded that $Cp = C11$; however, implementation of the present invention is not limited to such calculation method as above.

[0050] Since the parasitic capacity decreases from C2 to C11, a capacity change rate D (%) measured via external electrodes 22A and 22B when the capacity of the first capacitor 71 changes by ΔC increases from $\Delta C / (C1 + C2)$ to $\Delta C / (C1 + C11)$ compared to cases where no third capacitor 73 is formed.

[0051] In other words, the ultrasound unit 30A and the like enable provision of effects that are the same as those of the ultrasound unit 30 and the like.

[0052] Note that, for example, where the insulation layer 15 is formed so as to be thick to make a capacity between the lower electrode 12 and the substrate 11 be lower than the depletion layer capacity, or where a capacitor having a small capacity that is lower than the depletion layer capacity is disposed at a position partway through a ground potential wire to which a package member 60 is connected, in the embodiments, the diffusion layer 18 having a polarity that is different from that of the

substrate 11 is formed so as to form a depletion layer capacity; however, it is possible that such combination is not employed and a diffusion layer having a polarity that is the same as that of the substrate 11 is formed in the substrate.

[0053] The present invention is not limited to the above-described embodiments and the like, and various modification and alterations are possible without departing from the spirit of the present invention. Also, the configuration of any of the embodiments and modifications described above may be combined with that of the other embodiments and the like.

[0054] The present application is filed claiming priority from Japanese Patent Application No. 2012-197407 filed in Japan on September 7, 2012, the disclosure of which is incorporated in the description, the claims and the drawings of the present application by reference.

Claims

1. An ultrasound unit comprising:

ultrasound elements each including a plurality of ultrasound cells formed on a substrate including a semiconductor, the plurality of ultrasound cells each including an upper electrode having a ground potential and a lower electrode to which a drive signal is applied, the upper electrode and the lower electrode being arranged facing each other via a cavity and thereby forming a first capacitor;
a package member in which the plurality of the ultrasound elements are disposed, the package member having a ground potential; and
an insulation member disposed between the package member and each of the ultrasound elements, wherein:

a second capacitor is formed as a result of the insulation member serving as a gap; and
a capacity of a third capacitor formed so as to be serially connected to the second capacitor is smaller than a capacity of the second capacitor.

2. The ultrasound unit according to claim 1, wherein:

the substrate includes a low-resistance diffusion layer having a polarity that is different from a polarity of the substrate; and
the third capacitor is formed as a result of a depletion layer serving as a gap, the depletion layer being formed inside the substrate by the diffusion layer.

3. The ultrasound unit according to claim 2, wherein each of the ultrasound elements includes an insula-

tion layer insulating the substrate and the lower electrode from each other.

4. An ultrasound endoscope comprising:

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an insertion portion provided with an ultrasound unit in a distal end portion of the insertion portion, the ultrasound unit including ultrasound elements each including a plurality of ultrasound cells formed on a substrate including a semiconductor, the plurality of ultrasound cells each including an upper electrode having a ground potential and a lower electrode to which a drive signal is applied, the upper electrode and the lower electrode being arranged facing each other via a cavity and thereby forming a first capacitor, a package member in which the plurality of the ultrasound elements are disposed, the package member having a ground potential, and an insulation member disposed between the package member and each of the ultrasound elements, wherein a second capacitor is formed as a result of the insulation member serving as a gap, and a capacity of a third capacitor formed so as to be serially connected to the second capacitor is smaller than a capacity of the second capacitor; an operation portion disposed on a proximal end portion side of the insertion portion; and a universal cord provided so as to extend from the operation portion.

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5. The ultrasound endoscope according to claim 4, wherein:

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the substrate includes a low-resistance diffusion layer having a polarity that is different from a polarity of the substrate; and the third capacitor is formed as a result of a depletion layer serving as a gap, the depletion layer being formed inside the substrate by the diffusion layer.

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6. The ultrasound endoscope according to claim 5, wherein each of the ultrasound elements includes an insulation layer insulating the substrate and the lower electrode from each other.

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FIG.1

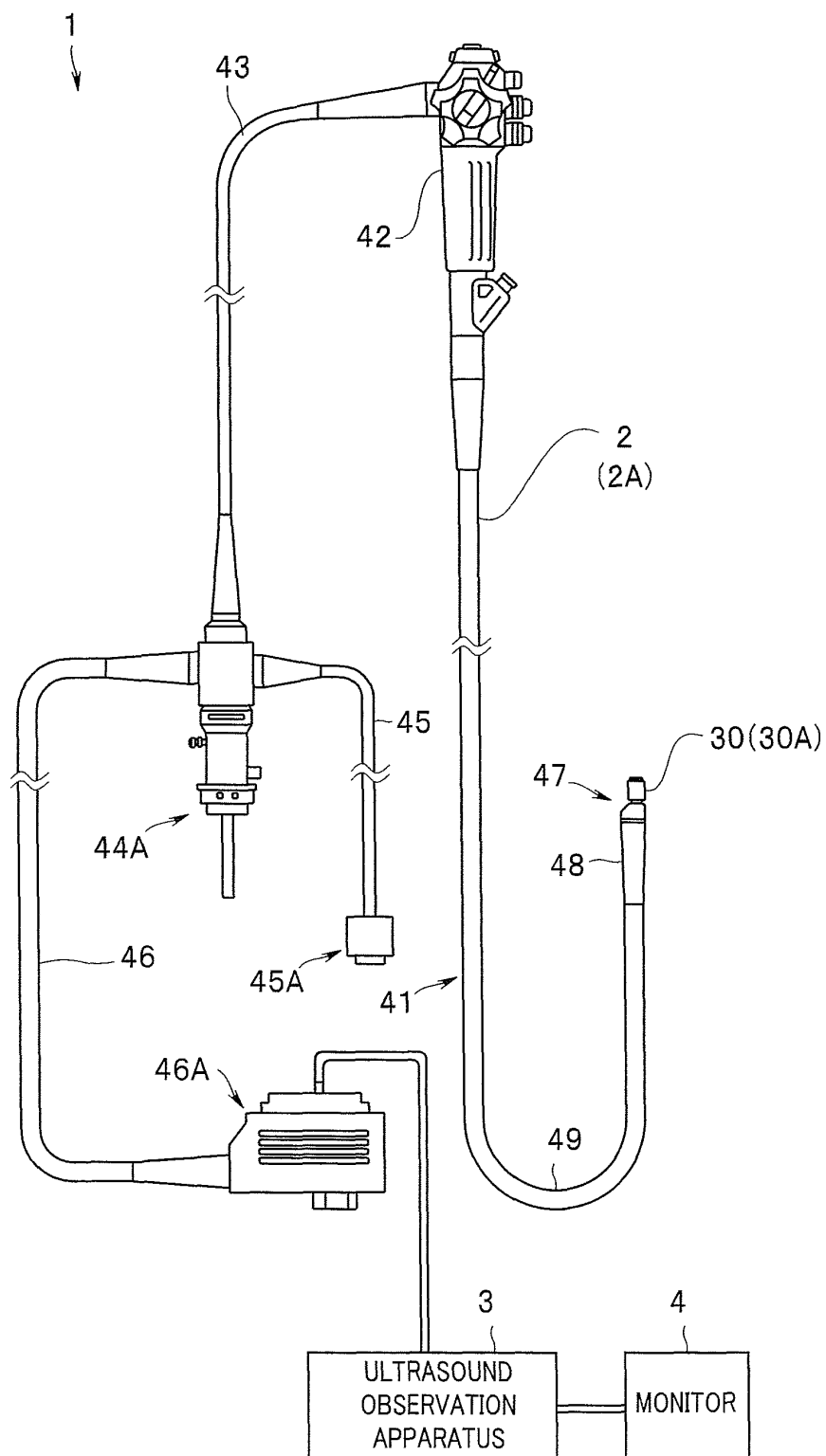


FIG.2

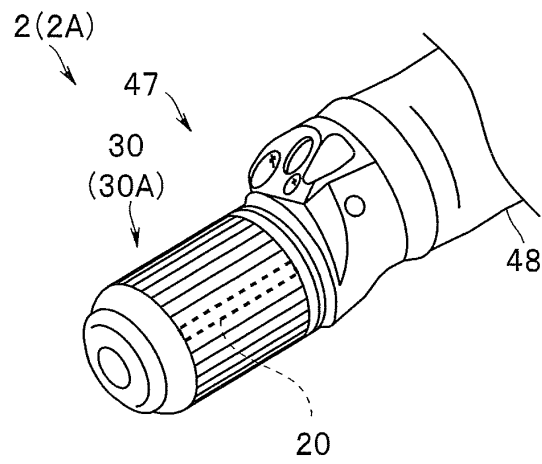


FIG.3

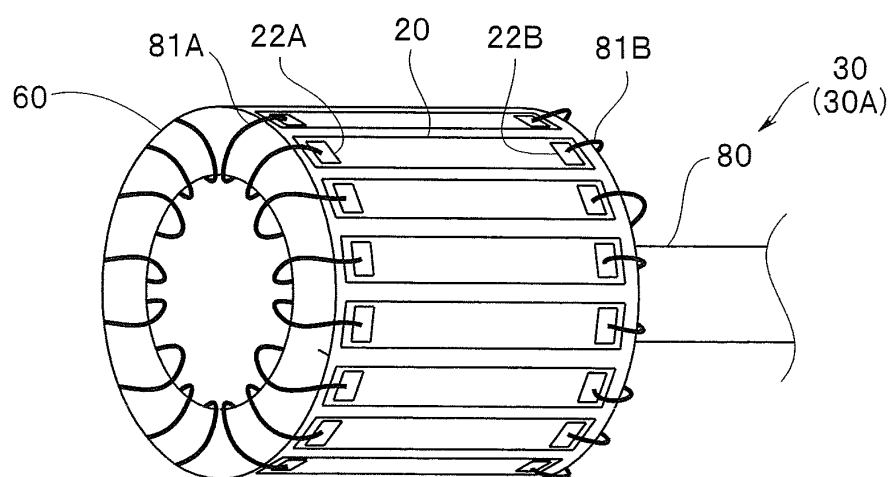


FIG.4

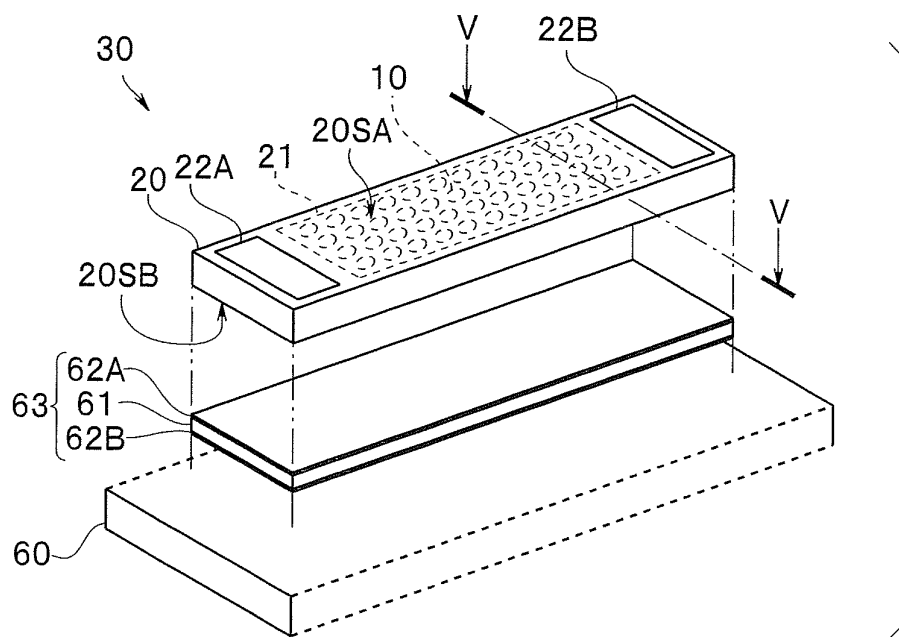


FIG.5

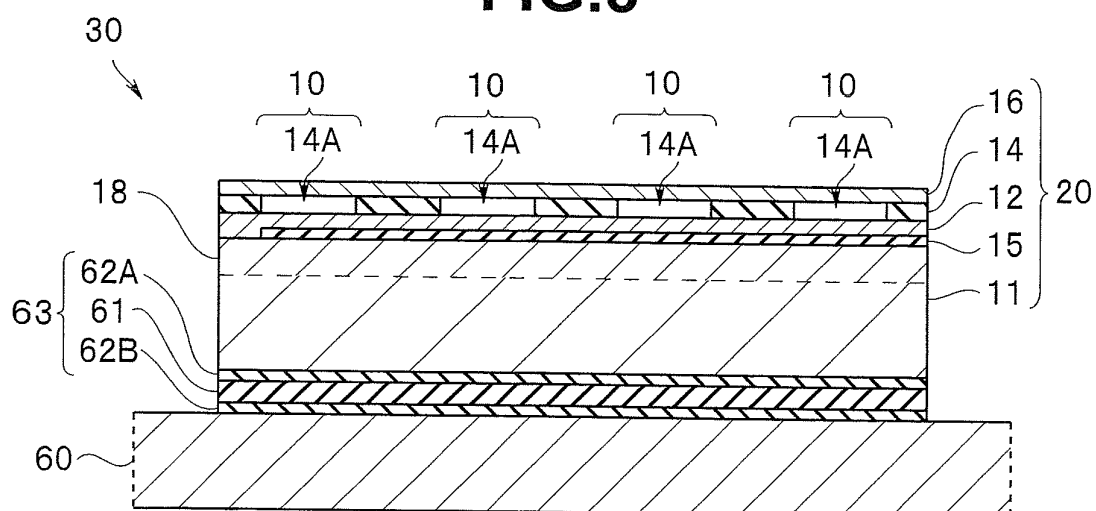


FIG.6

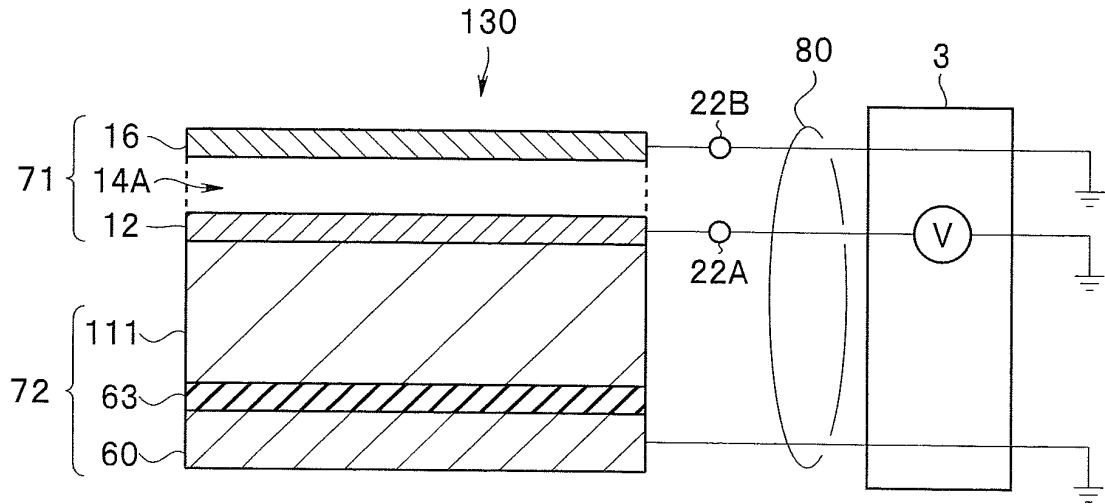


FIG.7

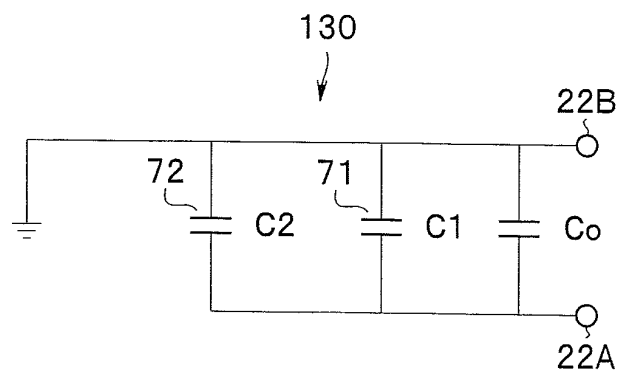


FIG.8

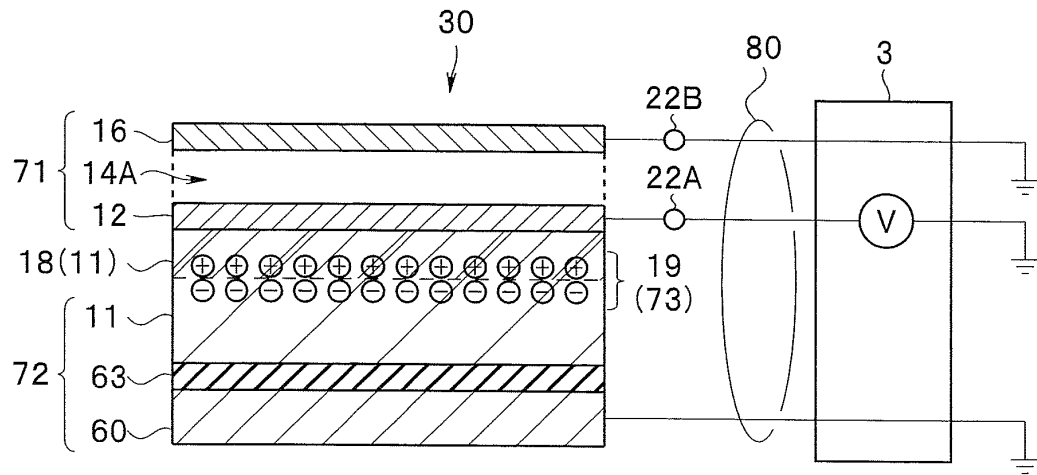


FIG.9

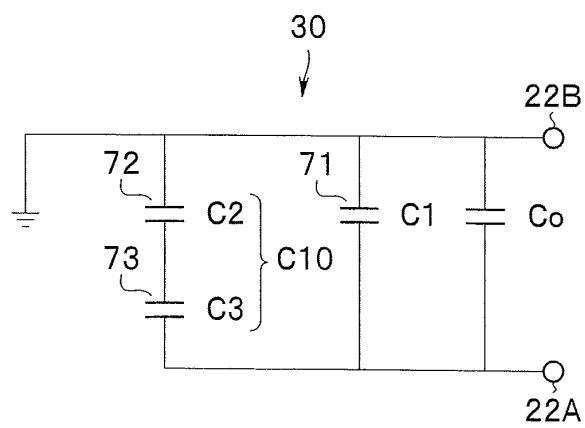


FIG.10

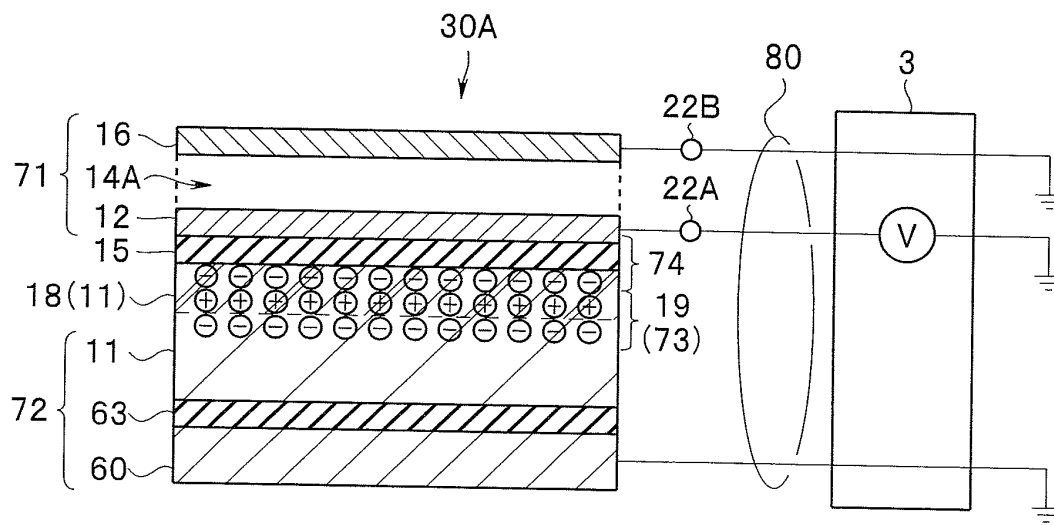
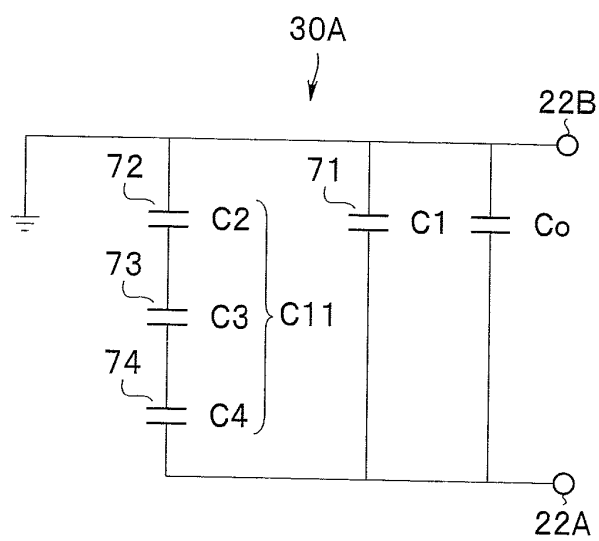


FIG.11



INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2013/061387

A. CLASSIFICATION OF SUBJECT MATTER

A61B8/12(2006.01) i, H04R19/00(2006.01) i

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B8/12, H04R19/00

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

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Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 2009-55473 A (Olympus Medical Systems Corp.), 12 March 2009 (12.03.2009), entire text; all drawings & US 8047995 B2 & EP 2030698 A1 & DE 602008002869 D & CN 101378605 A	1-6
A	JP 2009-50560 A (Olympus Medical Systems Corp.), 12 March 2009 (12.03.2009), entire text; all drawings & US 8047995 B2 & EP 2030698 A1 & DE 602008002869 D	1-6

☒ Further documents are listed in the continuation of Box C.☐ See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

10 May, 2013 (10.05.13)

Date of mailing of the international search report

21 May, 2013 (21.05.13)

Name and mailing address of the ISA/
Japanese Patent Office

Authorized officer

Facsimile No.

Telephone No.

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INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2013/061387

C (Continuation).	DOCUMENTS CONSIDERED TO BE RELEVANT	
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 2008-118631 A (Olympus Medical Systems Corp.), 22 May 2008 (22.05.2008), entire text; all drawings & US 2008/0089181 A1	1-6
A	JP 2008-93214 A (Olympus Medical Systems Corp.), 24 April 2008 (24.04.2008), entire text; all drawings & US 2009/0204004 A1 & WO 2008/044727 A1	1-6
A	JP 2008-99036 A (Olympus Medical Systems Corp.), 24 April 2008 (24.04.2008), entire text; all drawings & US 2008/0089180 A1 & EP 1911529 A1	1-6

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REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- JP 2006050314 A [0003]
- JP 2012197407 A [0054]

专利名称(译)	超声波单元和超声波内窥镜		
公开(公告)号	EP2893881A1	公开(公告)日	2015-07-15
申请号	EP2013835242	申请日	2013-04-17
[标]申请(专利权)人(译)	奥林巴斯株式会社		
申请(专利权)人(译)	OLYMPUS CORPORATION		
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IPC分类号	A61B8/12 H04R19/00		
CPC分类号	A61B8/12 A61B8/4444 A61B8/445 A61B8/4483 A61B8/54 B06B1/0292		
优先权	2012197407 2012-09-07 JP		
其他公开文献	EP2893881A4		
外部链接	Espacenet		

摘要(译)

超声单元30包括：超声元件20，每个超声元件20包括形成在包括半导体的基板11上的多个超声单元10，多个超声单元10各自包括具有地电位的上电极16和下电极12，施加驱动信号，上电极16和下电极12通过空腔14A彼此面对地布置，从而形成第一电容器71；封装构件60，其中设置有多数超声元件20，封装构件60具有接地电位；绝缘构件63设置在封装构件60和每个超声波元件20之间。由于绝缘构件63用作间隙而形成第二电容器72，并且第三电容器73的容量与第二电容器73串联连接。第二电容器72小于第二电容器72的容量。

