



(12) **EUROPEAN PATENT APPLICATION**
published in accordance with Art. 153(4) EPC

(43) Date of publication:
14.05.2014 Bulletin 2014/20

(51) Int Cl.:
A61B 8/12 (2006.01)

(21) Application number: **12807399.6**

(86) International application number:
PCT/JP2012/065464

(22) Date of filing: **18.06.2012**

(87) International publication number:
WO 2013/005563 (10.01.2013 Gazette 2013/02)

(84) Designated Contracting States:
AL AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO RS SE SI SK SM TR

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(30) Priority: **04.07.2011 JP 2011148593**

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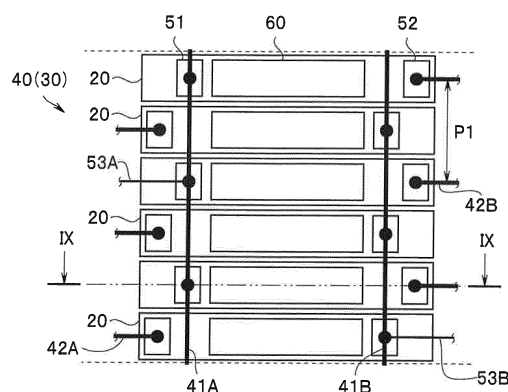
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(54) **ULTRASOUND UNIT AND ULTRASOUND ENDOSCOPE**

(57) An ultrasound unit 30 includes an ultrasound array 40 that has a plurality of ultrasound elements 20, each of which has a first principal surface that is rectangular where a transmitting and receiving portion 60, a signal electrode terminal 52, and a ground electrode terminal 51 are arranged in a longer side direction, longer sides of the ultrasound elements 20 being coupled, one or more short-lines 41 that are connected to a plurality of ground electrode terminals 51, a ground line 43 that

is connected to the short-line 41, and a plurality of signal lines 42, each of which is connected to one of the signal electrode terminals 52, and adjoining ultrasound elements of the ultrasound elements 20 are coupled such that the signal electrode terminals 52 are arranged alternately on opposite sides in the longer side direction of the transmitting and receiving portions 60 that are rectangular.

FIG.8



Description

Technical Field

[0001] The present invention relates to an ultrasound unit having an ultrasound element and an ultrasound endoscope including the ultrasound unit.

Background Art

[0002] An ultrasound endoscope can clearly visualize a wall of a digestive tract, a deep organ, or the like with good image quality free of influence of gas or a bone in a body. In an electron scanning type ultrasound endoscope, an ultrasound unit having an ultrasound array is disposed at a distal end portion. The ultrasound array is constructed by coupling longer sides of a plurality of ultrasound elements, each of which has a first principal surface that is elongated and rectangular. In each ultrasound element, a transmitting and receiving portion, a signal electrode terminal for transmitting and receiving a signal, and a ground electrode terminal at a ground potential are arranged in a longer side direction.

[0003] One signal line (coaxial cable core wire) is connected to the signal electrode terminal of each ultrasound element by, e.g., soldering, and one ground line (coaxial cable shielding wire) is connected to the ground electrode terminal.

[0004] In an ultrasound array in which a disposition pitch for electrode terminals is narrow, i.e., a shorter side of an ultrasound element rectangular in a plan view is short, work of connecting a wire to an electrode terminal is not easy.

[0005] A specification of Japanese Patent No. 4377787 discloses a transducer which connects an ultrasound array and coaxial cables by using a hollow cylindrical member having a relay electrode. In the transducer, electrode terminals of ultrasound elements and relay electrode terminals are connected with wires, and the coaxial cables are connected to the relay electrode terminals.

[0006] In an ultrasound unit with a narrow electrode pitch, however, it may not be easy to connect electrode terminals of ultrasound elements and a relay electrode with wires even by using a hollow cylindrical member having relay electrode terminals.

[0007] That is, an ultrasound unit in which a plurality of ultrasound elements, electrode terminals of which need to be connected to wiring for external connection, are laid out with a narrow pitch may not be easy to manufacture. An ultrasound endoscope including the ultrasound unit may not be easy to manufacture.

[0008] Embodiments of the present invention have as an object to provide an ultrasound unit easy to manufacture and an ultrasound endoscope easy to manufacture.

Disclosure of Invention

Means for Solving the Problem

[0009] An ultrasound unit according to an embodiment of the present invention includes an ultrasound array that has a plurality of ultrasound elements, in each of which a transmitting and receiving portion, a signal electrode terminal, and a ground electrode terminal are disposed, longer sides of the plurality of ultrasound elements being coupled, one or more short-lines that are connected to a plurality of the ground electrode terminals, a ground line that is connected to the short-line, and a plurality of signal lines, each of which is that are connected to one of the signal electrode terminals. The transmitting and receiving portion has a signal electrode for transmitting and receiving ultrasound and a ground electrode, the signal electrode is connected to the signal electrode terminal, and the ground electrode is connected to the ground electrode terminal. Adjoining ultrasound elements of the ultrasound elements are coupled such that the signal electrode terminals are arranged alternately on opposite sides in a longer side direction of the transmitting and receiving portions that are rectangular.

[0010] an ultrasound endoscope according to another embodiment includes a distal end rigid portion having the above-described ultrasound unit.

Brief Description of the Drawings

[0011]

Fig. 1 is an external view for explaining an endoscope system including an ultrasound endoscope according to a first embodiment;

Fig. 2 is a perspective view for explaining a distal end portion of the ultrasound endoscope according to the first embodiment;

Fig. 3 is a perspective view for explaining a configuration of an ultrasound unit according to the first embodiment;

Fig. 4 is a top view of an ultrasound element of the ultrasound unit according to the first embodiment;

Fig. 5 is a cross-sectional view of the ultrasound element of the ultrasound unit according to the first embodiment, taken along line V-V in Fig. 4;

Fig. 6 is a top view of a transmitting and receiving portion of the ultrasound unit according to the first embodiment;

Fig. 7 is a cross-sectional view of the transmitting and receiving portion of the ultrasound unit according to the first embodiment, taken along line VII-VII in Fig. 6;

Fig. 8 is a plan developed view of an ultrasound array of the ultrasound unit according to the first embodiment;

Fig. 9 is a cross-sectional view of the ultrasound array of the ultrasound unit according to the first em-

bodiment, taken along line IX-IX in Fig. 8;

Fig. 10 is a plan developed view of an ultrasound array of an ultrasound unit according to a second embodiment;

Fig. 11 is a plan developed view of an ultrasound array of an ultrasound unit according to a third embodiment;

Fig. 12 is a plan developed view of an ultrasound array of an ultrasound unit according to a fourth embodiment;

Fig. 13 is a cross-sectional view of an ultrasound element of an ultrasound unit according to a fifth embodiment;

Fig. 14 is a cross-sectional view of an ultrasound element of an ultrasound unit according to a sixth embodiment;

Fig. 15 is a top view of an ultrasound array of the ultrasound unit according to the sixth embodiment;

Fig. 16 is a bottom view of the ultrasound array of the ultrasound unit according to the sixth embodiment;

Fig. 17 is a cross-sectional view of an ultrasound element of an ultrasound unit according to a modification 1 of the sixth embodiment; and

Fig. 18 is a cross-sectional view of an ultrasound element of an ultrasound unit according to a modification 2 of the sixth embodiment.

Best Mode for Carrying Out the Invention

<First Embodiment>

[0012] An ultrasound unit (hereinafter referred to as a "US unit") 30 according to a first embodiment and an ultrasound endoscope (hereinafter referred to as a "US endoscope") 2 having the US unit 30 will be described below with reference to the drawings.

<Configuration of Ultrasound Endoscope>

[0013] As shown in Fig. 1, the US endoscope 2 together with an ultrasound survey apparatus 3 and a monitor 4 constitutes an ultrasound endoscope system 1. The US endoscope 2 includes an elongated insertion portion 21 to be inserted into a body, an operation portion 22 which is placed at a proximal end of the insertion portion 21, and a universal cord 23 which extends from a side portion of the operation portion 22.

[0014] A connector 24A which is connected to a light source apparatus (not shown) is disposed at a proximal end portion of the universal cord 23. A cable 25 which is detachably connected to a camera control unit (not shown) via a connector 25A and a cable 26 which is detachably connected to the ultrasound survey apparatus 3 via a connector 26A extend from the connector 24A. The monitor 4 is connected to the ultrasound survey apparatus 3.

[0015] The insertion portion 21 is composed of a distal

end rigid portion (hereinafter referred to as a "distal end portion") 37, a bending portion 38 located at a rear end of the distal end portion 37, and a thin, long, flexible tube portion 39 with flexibility located at a rear end of the bending portion 38 and leading to the operation portion 22, which are provided to be linked in order from a distal end side. The ultrasound unit 30 serving as an ultrasound transmitting and receiving portion is disposed on a distal end side of the distal end portion 37.

[0016] An angle knob 22A which bends and controls the bending portion 38 in a desired direction, an air/water feeding button 22B which performs air feeding and water feeding operation, a suction button 22C which performs suction operation, a treatment instrument insertion port 22D which serves as an inlet for a treatment instrument to be introduced into a body, and the like are disposed at the operation portion 22.

[0017] As shown in Fig. 2, a lens cover 31 for illumination which constitutes an illumination optical system, a lens cover 32 for observation of an observation optical system, a forceps port 33 which doubles as a suction port, and an air/water feeding nozzle (not shown) are disposed at the distal end portion 37 where the US unit 30 that transmits and receives ultrasound is provided.

[0018] As shown in Fig. 3, the US unit 30 includes an ultrasound array (hereinafter referred to as a "US array") 40, short-lines 41A and 41B, ground lines 53A and 53B, and signal lines 42A and 42B. Note that, to refer to each of identical components, a reference numeral obtained by omitting an alphabetic character at an end of any one of reference characters denoting the identical components is used. For example, each of the short-lines 41 A and 4 1 B is referred to as the short-line 41. For example, the short-line 41 A is the short-line 41 on a distal end side, and the short-line 4 1 B is the short-line 41 on a proximal end side.

[0019] The US array 40 is a group of radial type transducers in which longer sides of a plurality of elongated US elements 20 are coupled, and the US elements 20 are arranged to bend in a hollow cylindrical shape. That is, in the US array 40, for example, 200 US elements 20 with shorter sides of not more than 0.1 mm are disposed at a side face of a hollow cylinder having a diameter of 2 mm.

[0020] Note that although the US array 40 is a group of radial type transducers, the US array 40 may be a group of convex type transducers which bends in a convex shape.

[0021] A plurality of signal lines 42 are each connected to a signal electrode terminal 52 of one US element 20. The short-line 41 is a short-line which connects ground electrode terminals 51 of the plurality of US elements 20 and is connected to the ground line 53.

[0022] The plurality of US elements 20 and a coaxial cable bundle 35 are connected via the short-lines 41, the ground lines 53, the signal lines 42, and a cable connection substrate portion (not shown). That is, the coaxial cable bundle 35 is made up of coaxial cables with core

wires equal in number to the plurality of signal lines 42.

[0023] The coaxial cable bundle 35 is inserted through the distal end portion 37, the bending portion 38, the flexible tube portion 39, the operation portion 22, the universal cord 23, and the ultrasound cable 26 and is connected to the ultrasound survey apparatus 3 via the ultrasound connector 26a.

<Configuration of Ultrasound Array>

[0024] As shown in Figs. 4 and 5, a transmitting and receiving portion 60, the signal electrode terminal 52, and the ground electrode terminal 51 are arranged in a longer side direction at a first principal surface 20SA that is rectangular of each US element 20. Note that the drawings are all schematic views for explanation and that ratios of thickness, size, and the like are different from actual ratios.

[0025] In the US element 20, the signal electrode terminal 52 and the ground electrode terminal 51 are arranged across the transmitting and receiving portion 60 from each other. A space where the ground electrode terminal 51 can be arranged is present between the transmitting and receiving portion 60 and the signal electrode terminal 52, and a space where the signal electrode terminal 52 can be arranged is present between the ground electrode terminal 51 and an end face. In other words, the transmitting and receiving portion 60, two signal electrode terminals 52, and two ground electrode terminals 51 can be arranged in the longer side direction at the first principal surface 20SA of the US element 20.

[0026] The signal electrode terminal 52 is connected to a lower electrode 12 which is a signal electrode of the transmitting and receiving portion 60. The ground electrode terminal 51 is connected to an upper electrode 16 which is a ground electrode of the transmitting and receiving portion 60.

[0027] The transmitting and receiving portion 60 generates ultrasound by a signal for driving applied between the lower electrode 12 and the upper electrode 16. The transmitting and receiving portion 60 also generates an electrical signal between the lower electrode 12 and the upper electrode 16 upon receipt of ultrasound.

<Configuration of Transmitting and receiving Portion>

[0028] A configuration of the transmitting and receiving portion 60 will be described with reference to Figs. 6 and 7.

[0029] As shown in Fig. 6, a plurality of capacitance type ultrasound cells (hereinafter referred to as "US cells") 10 are arranged in a matrix at the transmitting and receiving portion 60 of the ultrasound unit 30. The US cells 10 may be arranged in a regular pattern, such as a grid pattern, a staggered pattern, or a triangular mesh pattern, or may be randomly arranged.

[0030] As shown in Fig. 7, the US cell 10 has, on a silicon substrate 11 as a base, the lower electrode 12

connected to the signal electrode terminal 52, a first insulating layer (lower insulating layer) 13, a second insulating layer (upper insulating layer) 15 in which a cavity 14 in a hollow cylindrical shape is formed, the upper electrode 16 connected to the ground electrode terminal 51, and a protective layer 17, which are stacked in order.

[0031] That is, each US cell 10 has a lower electrode portion 12A that is a circular signal electrode portion and a circular upper electrode portion 16A that is a ground electrode portion, which are arranged to face each other via the cavity 14. A plurality of lower electrode portions 12A constitute the lower electrode 12 serving as the signal electrode, and a plurality of upper electrode portions 16A constitute the upper electrode 16 serving as the ground electrode. That is, the lower electrode portions 12A of the plurality of US cells 10 arranged at the identical US element 20 are connected to one another, and the upper electrode portions 16A are also connected to one another.

[0032] The silicon substrate 11 is a substrate in which silicon thermal oxide films 11B and 11C are formed on surfaces of silicon 11A. The lower electrode 12 formed on one surface of the silicon substrate 11 is made of a conductive material, such as metal or silicon. A film of the conductive material is formed over the whole surface of the silicon substrate 11 by, e.g., sputtering. The lower electrode 12 is formed by partially removing the film through etching after forming a mask pattern through photolithography.

[0033] For example, the lower electrode 12 is made up of the circular lower electrode portions 12A and a wiring portion 12B which is provided to extend from an edge portion of the lower electrode 12. The lower electrode portion 12A is connected to the lower electrode portions of the other US cells of the identical US element 20 by the wiring portion 12B.

[0034] The first insulating layer 13 that is made of an insulating material, such as SiN, is formed by, e.g., CVD (chemical vapor deposition) so as to cover the lower electrode 12.

[0035] A sacrificial layer in a shape of the cavity 14 (a solid cylindrical shape) is formed by forming a film of a sacrificial layer material on the first insulating layer 13 and patterning the film.

[0036] Since a thickness of the sacrificial layer corresponds to a height of the cavity 14, the thickness is, for example, 0.05 to 0.3 μm , preferably 0.05 to 0.15 μm . For example, phosphorus glass (PSG: phosphorus-containing silicon oxide), silicon dioxide, polysilicon, metal, or the like is used as the sacrificial layer material.

[0037] The second insulating layer 15 is formed on an upper surface of the first insulating layer 13 where a sacrificial layer pattern is formed by, for example, the same method using the same material as the first insulating layer 13.

[0038] An opening portion (not shown) for admission of an etchant is formed at a predetermined position of the second insulating layer 15 to remove the sacrificial

layer.

[0039] The cavity 14 is formed by etching the sacrificial layer. For example, if phosphorus glass is used for the sacrificial layer, and SiN is used for the first insulating layer 13 and the second insulating layer 15, a hydrofluoric acid solution (buffered HF solution) is used as the etchant.

[0040] The upper electrode 16 that is made up of the upper electrode portion 16A and a wiring portion 16B is formed in the same manner as the lower electrode 12. For example, the upper electrode portion 16A and the lower electrode portion 12A have substantially identical diameters as the cavity 14.

[0041] The cavity 14 is not limited to a solid cylindrical shape and may have, e.g., a polygonal column shape. If the cavity 14 has a polygonal column shape, shapes of the upper electrode portion 16A and the lower electrode portion 12A are preferably polygonal.

[0042] Finally, the protective layer 17 that covers the upper electrode 16 is formed. The protective layer 17 is an insulating layer which is formed by the same method using the same material as the second insulating layer 15. Note that the protective layer 17 may have a double-layered structure in which a skin film with biocompatibility of, e.g., polyparaxylylene is further formed on an insulating layer made of, e.g., SiN.

[0043] In the US cell 10 with the above-described structure shown in Fig. 7, the second insulating layer 15, the upper electrode 16, and the protective layer 17 in a region immediately above the cavity 14 constitute a membrane 18 serving as a vibration portion.

<Configurations of Ultrasound Array and Ultrasound Unit>

[0044] Fig. 8 is a plan developed view of the US unit 30, i.e., an explanatory view showing the plurality of US elements 20 laid out on a radial surface (a side face of a hollow cylinder) in a planar state. Fig. 9 is a cross-sectional view taken along line IX-IX in Fig. 8.

[0045] As has already been described, the longer sides of the plurality of US elements 20 of the US array 40 are coupled. As shown in Fig. 8, the plurality of US elements 20 with an identical configuration are coupled in a state where the US elements 20 are alternately rotated by 180° along the longer side direction such that the signal electrode terminal 52 of each US element 20 and the ground electrode terminal 51 of the adjoining US element 20 adjoin.

[0046] That is, the US array 40 is fabricated by linking the plurality of US elements 20 with an identical structure while changing disposition directions. Thus, the US array 40 is easy to fabricate.

[0047] The signal electrode terminals 52 are laid out in a straight line shape at every other US element on both end face sides of the US array 40. Therefore, a disposition spacing (pitch) P1 for the signal electrode terminals 52 on each end face side is twice a disposition pitch in a

conventional US array in which the signal electrode terminals 52 are continuously laid out. The ground electrode terminals 51 are laid out in a straight line shape at every other US element on the left and on the right of the transmitting and receiving portions 60.

[0048] Note that the US array 40 is arranged in a three-dimensional curved surface shape. Strictly, the term "straight line shape" means "an arc shape" or that "arrangement at the time of projection onto a two-dimensional plane has a straight line shape."

[0049] Since the US unit 30 has the wider disposition pitch P1 for the signal electrode terminals 52, connection of the signal line 42 and the signal electrode terminal 52 is easy. Thus, the ultrasound unit 30 is easy to manufacture, and the ultrasound endoscope 2 having the US unit 30 is easy to manufacture.

[0050] Note that the plurality of signal lines 42 may be each one cable (wire) or the plurality of signal lines 42 may be disposed at a flexible wiring board. A connection method is, for example, solder joining. Since it is easy to enhance connection strength of a connection portion, the ultrasound unit 30 and the ultrasound endoscope 2 are high in reliability.

[0051] Since the plurality of ground electrode terminals 51 are laid out in a straight line shape, all the ground electrode terminals 51 can be connected by the two short-lines 41A and 41B. Each short-line 41 is only connected to the ground line 53 at at least one site.

[0052] The short-line 41 is made of a conductor in a line shape or a ribbon shape, such as aluminum or copper, and is connected to the ground electrode terminal 51 by a known method, such as ultrasound or heat. Alternatively, the short-line 41 may be formed by forming a conductive film made of a conductor, such as aluminum or copper, via, for example, a metal mask. The conductive film can be formed by sputtering, an evaporation method, or an electroplating method.

[0053] Since the plurality of ground electrode terminals 51 need not be connected to respective ground lines 53, the ultrasound unit 30 is easy to manufacture, and the ultrasound endoscope 2 having the ultrasound unit 30 is easy to manufacture.

[0054] Note that it is apparent that even if each ultrasound element has a transmitting and receiving portion in which piezoelectric layers of, e.g., PZT are stacked, instead of the transmitting and receiving portion 60, in which the plurality of capacitance type US cells 10 are laid out, the ultrasound element has same effects.

<Second Embodiment>

[0055] A US unit 30A according to a second embodiment and a US endoscope 2A having the US unit 30A will be described below. Since the US unit 30A and the US endoscope 2A are similar to the US unit 30 and the US endoscope 2, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0056] As shown in Fig. 10, in a US array 40A of the US unit 30A, a plurality of ultrasound elements 20A are coupled such that shorter sides of the ultrasound elements 20A are positioned in a zigzag manner at both end faces of the ultrasound array 40A. Therefore, notch portions 45A and 45B are formed at the both end faces of the ultrasound array 40A. A signal line 42 is provided to extend to a second principal surface 20SB side, i.e., an inner portion side of the ultrasound array 40A in a hollow cylinder shape via the notch portion 45.

[0057] The US unit 30A has the same effects as the US unit 30. Additionally, the signal lines 42 do not protrude from the both end faces of the ultrasound array 40A. Thus, a dimension of a longer side of the US element 20A is shorter in the US unit 30A. The US endoscope 2A including the US unit 30A has a shorter distal end portion 37.

[0058] In addition, the US unit 30A can reduce interference between the adjacent signal lines 42. That is, in the US unit 30 shown in Fig. 8, the signal lines 42A and 42B are led out in parallel with a longitudinal direction of the US element 20. Therefore, the signal lines 42A and 42B become arched, and deflection or the like occurs. If the amount of deflection of the adjoining signal lines 42A and 42B is large, the signal lines 42A and 42B may interfere with one another.

[0059] In contrast, in the US unit 30A shown in Fig. 10, the signal lines 42A and 42B are each passed through the notch 45A or 45B that is an empty space at a predetermined site, and thus the signal lines 42A and 42B are in no danger of interfering with one another.

<Third Embodiment>

[0060] A US unit 30B according to a third embodiment and a US endoscope 2B having the US unit 30B will be described below. Since the US unit 30B and the US endoscope 2B are similar to the US unit 30 and the US endoscope 2, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0061] As shown in Fig. 11, there are two types of ultrasound elements 20B constituting a US array 40B of the US unit 30B. That is, the ultrasound element 20B is either a first ultrasound element 20B1 or a second ultrasound element 20B2. In the first ultrasound element 20B1, a ground electrode terminal 51 is arranged between a signal electrode terminal 52 and a transmitting and receiving portion 60 at a first principal surface 20SA. In the second ultrasound element 20B2, the transmitting and receiving portion 60 is arranged between the ground electrode terminal 51 and the signal electrode terminal 52 at the first principal surface 20SA. The first ultrasound element 20B1 and the second ultrasound element 20B2 are coupled such that the ground electrode terminals 51 adjoin each other.

[0062] Additionally, since the two different ultrasound elements 20B1 and 20B2 are coupled such that shorter

sides are positioned in a zigzag manner, a plurality of notch portions 45A and 45B are formed at both end faces of the US array 40B. A signal line 42 is provided to extend to a second principal surface 20SB side via the notch portion 45.

[0063] As shown in Fig. 11, one short-line 41 is enough in the US unit 30B. Thus, a dimension in a longer side direction of the US element 20B is shorter than the US element 20.

[0064] The US unit 30B has effects which the US unit 30 and the like have and is even shorter. The US endoscope 2B has effects which the US endoscope 2 has and has an even shorter distal end portion 37.

[0065] As has been described above, an ultrasound unit according to the embodiment may have the configuration below.

[0066] An ultrasound unit wherein the plurality of ultrasound elements are made up of a plurality of first ultrasound elements, in each of which the ground electrode terminal is arranged between the signal electrode terminal and the transmitting and receiving portion, and a plurality of second ultrasound elements, in each of which the transmitting and receiving portion is arranged between the ground electrode terminal and the signal electrode terminal, and the first ultrasound elements and the second ultrasound elements are coupled such that the ground electrode terminals adjoin one another.

<Fourth Embodiment>

[0067] A US unit 30C according to a fourth embodiment and a US endoscope 2C having the US unit 30C will be described below. Since the US unit 30C and the US endoscope 2C are similar to the US unit 30 and the US endoscope 2, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0068] As shown in Fig. 12, in a US element 20C of the US unit 30C, a signal electrode terminal 52 is arranged at one end portion, and a ground electrode terminal 51 is arranged at a center of a transmitting and receiving portion 60C which is divided into two, a first transmitting and receiving portion 60A and a second transmitting and receiving portion 60B.

[0069] A signal line (a piece of signal wiring) 42 is provided to extend to a second principal surface 20SB side via a notch portion 45 at an end portion. A plurality of ground electrode terminals 51 are connected by one short-line 41. Note that a ground line (not shown) connected to the short-line 41 is led out via a coupling portion (between the adjoining transmitting and receiving portions 60) of the adjoining US elements 20C or is led out via a piece of through-wiring.

[0070] The US unit 30C and the US endoscope 2C have effects which the US unit 30B and the like have.

<Fifth Embodiment>

[0071] A US unit 30D according to a fifth embodiment and a US endoscope 2D having the US unit 30D will be described below. Since the US unit 30D and the US endoscope 2D are similar to the US unit 30 and the US endoscope 2, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0072] As shown in Fig. 13, in a US element 20D of the US unit 30D, a surface where a signal electrode terminal 52 is disposed and a surface where a ground electrode terminal 51 is disposed are lower than a surface of a transmitting and receiving portion 60. A height of the surface of the transmitting and receiving portion 60 is higher than a maximum height of a signal line 42 and a maximum height of a ground line 53 (not shown). That is, a silicon substrate 11D as a base is stepped at end portions such that, even if the signal line 42 is connected to the signal electrode terminal 52, a short-line 41 and the ground line 53 are connected to the ground electrode terminal 51, the height of each of the components does not exceed the height of the transmitting and receiving portion 60.

[0073] The US unit 30D and the US endoscope 2D have effects which the US unit 30 and the like have. Additionally, in the US unit 30D with a plurality of US elements 20D disposed in a hollow cylindrical shape, a piece of wiring (wire) and the like do not protrude beyond the surface of the transmitting and receiving portion 60. Thus, the US unit 30D and a distal end portion 37 of the US endoscope 2D have smaller outer diameters.

<Sixth Embodiment>

[0074] A US unit 30E according to a sixth embodiment and a US endoscope 2E having the US unit 30E will be described below. Since the US unit 30E and the US endoscope 2E are similar to the US unit 30 and the US endoscope 2, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0075] As shown in Fig. 14, in a US element 20E of the US unit 30E, a transmitting and receiving portion 60 is disposed at a first principal surface 20SA, and a ground electrode terminal 51 and a signal electrode terminal 52 are disposed at a second principal surface 20SB. The ground electrode terminal 51 and an upper electrode 16 are connected via a piece 47 of through-wiring which pierces through a silicon substrate 11 as a base, and the signal electrode terminal 52 and a lower electrode 12 are connected via a piece 48 of through-wiring.

[0076] That is, in the US element 20E, the transmitting and receiving portion 60 is formed at the first principal surface 20SA of the base having the first principal surface 20SA and the second principal surface 20SB, and the signal electrode terminal 52 and the ground electrode terminal 51 are formed at the second principal surface

20SB. Note that a piece of wiring may be provided to extend to the second principal surface 20SB of the silicon substrate 11 by using a different wiring method, such as pieces of side face wiring, instead of the pieces 47 and 48 of through-wiring.

[0077] As shown in Figs. 15 and 16, in a US array 40E, the transmitting and receiving portion 60 is arranged substantially at a center of the first principal surface 20SA. The signal electrode terminals 52 disposed at the second principal surfaces 20SB are laid out alternately at end portions on opposite sides of the transmitting and receiving portions 60 disposed at the first principal surfaces 20SA to have a straight line shape. A plurality of ground electrode terminals 51 are laid out in a straight line shape in two rows closer to a center than the signal electrode terminals 52.

[0078] As in the US array 40 shown in Fig. 8, a plurality of signal lines 42 are each connected to the signal electrode terminal 52 of one US element 20E. Two short-lines 41 each connect the ground electrode terminals 51 of a plurality of US elements 20E and are each connected to a corresponding ground line 53 at one site.

[0079] Note that the signal lines 42 and the ground lines 53 are provided to extend to an inner side of the US array 40E so as not to protrude from end faces of the US array 40E.

[0080] The US unit 30E and the US endoscope 2E have effects which the US unit 30 and the like have and have even smaller outer diameters.

<Modifications of Sixth Embodiment>

[0081] US units 30F and 30G according to a modification 1 and a modification 2 of the sixth embodiment and US endoscopes 2F and 2G having the US units 30F and 30G will be described below. Since the US units 30F and 30G and the US endoscopes 2F and 2G are similar to the US unit 30E and the US endoscope 2E, respectively, identical components are denoted by identical reference numerals, and a description of the components will be omitted.

[0082] As shown in Fig. 17, in a US element 20F of the US unit 30F, a transmitting and receiving portion 60 and a signal electrode terminal 52 are disposed at a first principal surface 20SA, and a ground electrode terminal 51 is disposed at a second principal surface 20SB.

[0083] A plurality of US elements 20F are coupled in a state where the US elements 20F are alternately rotated by 180° along a longer side direction. Therefore, the signal electrode terminals 52 connected to signal lines 42 are arranged alternately at end portions on the first principal surface 20SA side. The ground electrode terminals 51 connected to short-lines 41 are arranged alternately at both end portions on the second principal surface 20SB side to have a straight line shape.

[0084] The US unit 30F and the US endoscope 2F have effects which the US unit 30E and the like have and are even shorter.

[0085] As shown in Fig. 18, in a US element 20G of the US unit 30G, a transmitting and receiving portion 60 is disposed substantially at a center portion of a first principal surface 20SA, and a ground electrode terminal 51 and a signal electrode terminal 52 are disposed at a second principal surface 20SB. The signal electrode terminal 52 here is disposed substantially at a center portion of the second principal surface 20SB.

[0086] A plurality of US elements 20G are coupled in a state where the US elements 20G are alternately rotated by 180° along a longer side direction. Therefore, the signal electrode terminals 52 connected to signal lines 42 are arranged alternately at end portions on the second principal surface 20SB side. The ground electrode terminals 51 connected to a short-line 41 are arranged in a straight line shape at a center portion on the second principal surface 20SB side. Thus, all the ground electrode terminals 51 can be connected by the one short-line 41.

[0087] The US unit 30G and the US endoscope 2G have effects which the US unit 30E and the like have and are even shorter.

[0088] As has been described above, at least one of a signal electrode terminal and a ground electrode terminal and a transmitting and receiving portion may be disposed at a first principal surface of an ultrasound element.

[0089] The present invention is not limited to the above-described embodiments or modifications. Various changes, alterations, and the like can be made without departing from spirit of the present invention.

[0090] The present application is filed claiming priority from Japanese Patent Application No. 2011-148593 filed in Japan on July 4, 2011. The above-described disclosure is incorporated in the description, the claims, and the drawings of the present application.

Claims

1. An ultrasound unit comprising:

an ultrasound array that has a plurality of ultrasound elements, in each of which a transmitting and receiving portion, a signal electrode terminal, and a ground electrode terminal are disposed, longer sides of the plurality of ultrasound elements being coupled;

one or more short-lines that are connected to a plurality of the ground electrode terminals;
a ground line that is connected to the short-line; and

a plurality of signal lines, each of which is connected to one of the signal electrode terminals, wherein the transmitting and receiving portion has a signal electrode for transmitting and receiving ultrasound and a ground electrode, the signal electrode is connected to the signal electrode terminal, and the ground electrode is con-

nected to the ground electrode terminal, and adjoining ultrasound elements of the ultrasound elements are coupled such that the signal electrode terminals are arranged alternately on opposite sides in a longer side direction of the transmitting and receiving portions that are rectangular.

2. The ultrasound unit according to claim 1, wherein the plurality of ground electrode terminals connected to one of the short-lines are laid out in a straight line shape.

3. The ultrasound unit according to claim 2, wherein the plurality of ultrasound elements bend in a convex shape or a radial shape in a coupling direction.

4. The ultrasound unit according to claim 3, wherein at least one of the signal electrode terminal and the ground electrode terminal, and the transmitting and receiving portion are disposed at a first principal surface of the ultrasound element.

5. The ultrasound unit according to claim 4, wherein the transmitting and receiving portion, the signal electrode terminal, and the ground electrode terminal are disposed at the first principal surface of the ultrasound element.

6. The ultrasound unit according to claim 5, wherein a plurality of ultrasound elements identical in a form in which the transmitting and receiving portion, the signal electrode terminal, and the ground electrode terminal are arranged are coupled in a state where the ultrasound elements are alternately rotated by 180° along the longer side direction.

7. The ultrasound unit according to claim 6, wherein a plurality of ultrasound cells are disposed at the transmitting and receiving portion, each of the ultrasound cells has a signal electrode portion and a ground electrode portion that are arranged to face each other across a cavity, a plurality of the signal electrode portions constitute the signal electrode, and a plurality of the ground electrode portions constitute the ground electrode.

8. The ultrasound unit according to claim 5, wherein the plurality of ultrasound elements are coupled such that shorter sides are positioned in a zigzag manner at either end face of the ultrasound array to form a plurality of notch portions, and the signal line is provided to extend to a second principal surface side via the notch portion.

9. The ultrasound unit according to claim 8, wherein a plurality of ultrasound elements identical in a form in which the transmitting and receiving portion, the sig-

nal electrode terminal, and the ground electrode terminal are arranged are coupled in a state where the ultrasound elements are alternately rotated by 180° along the longer side direction.

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10. The ultrasound unit according to claim 9, wherein a plurality of ultrasound cells are disposed at the transmitting and receiving portion, each of the ultrasound cells has a signal electrode portion and a ground electrode portion that are arranged to face each other across a cavity, a plurality of the signal electrode portions constitute the signal electrode, and a plurality of the ground electrode portions constitute the ground electrode.
11. The ultrasound unit according to claim 5, wherein a height of a surface of the transmitting and receiving portion is higher than a maximum height of the signal line and a maximum height of the ground line.
12. The ultrasound unit according to claim 11, wherein a plurality of ultrasound elements identical in a form in which the transmitting and receiving portion, the signal electrode terminal, and the ground electrode terminal are arranged are coupled in a state where the ultrasound elements are alternately rotated by 180° along the longer side direction.
13. The ultrasound unit according to claim 12, wherein a plurality of ultrasound cells are disposed at the transmitting and receiving portion, each of the ultrasound cells has a signal electrode portion and a ground electrode portion that are arranged to face each other across a cavity, a plurality of the signal electrode portions constitute the signal electrode, and a plurality of the ground electrode portions constitute the ground electrode.
14. An ultrasound endoscope comprising an ultrasound unit according to claim 3.

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FIG.1

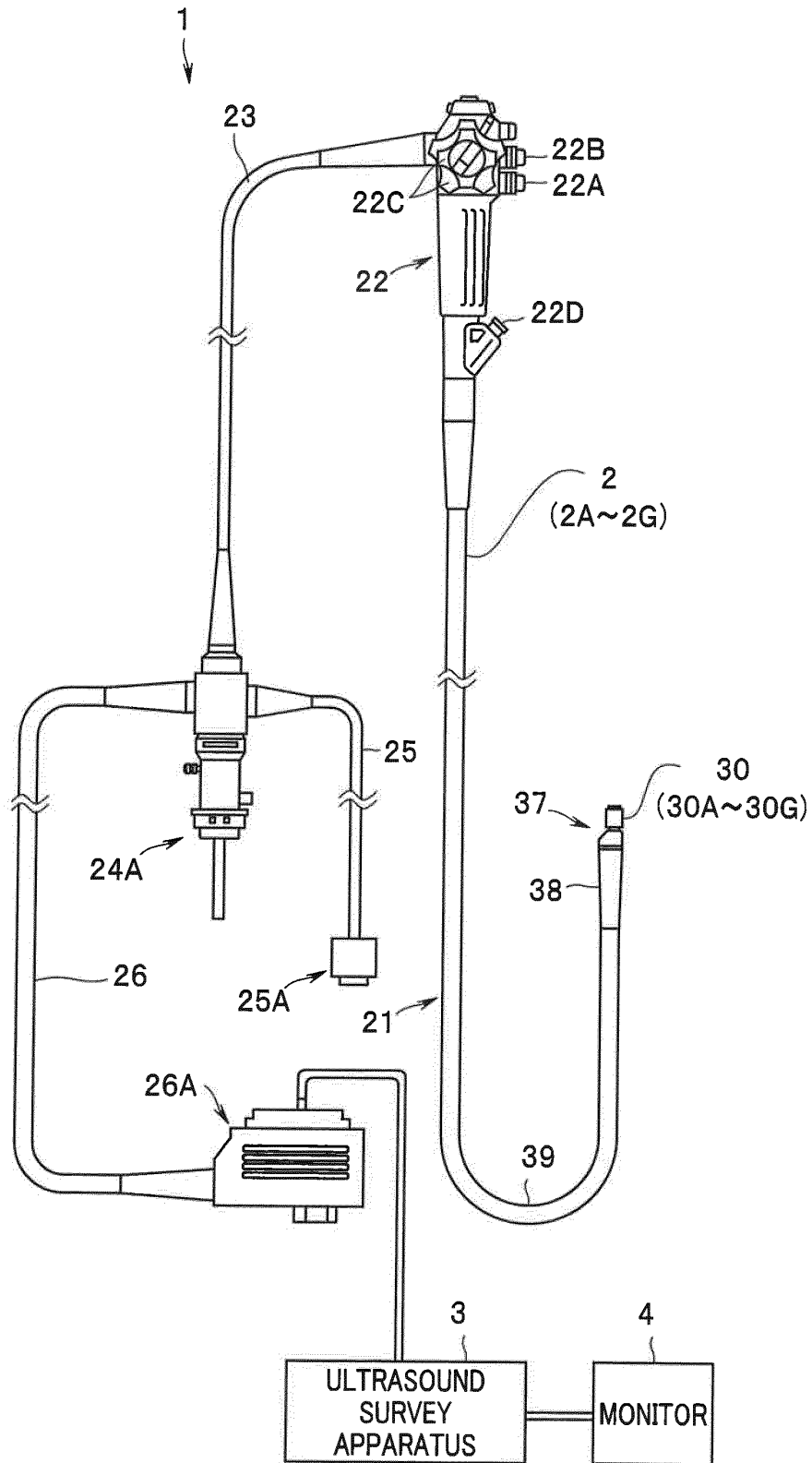


FIG.2

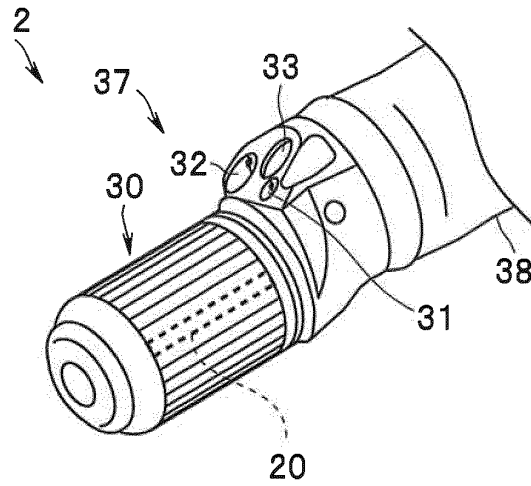


FIG.3

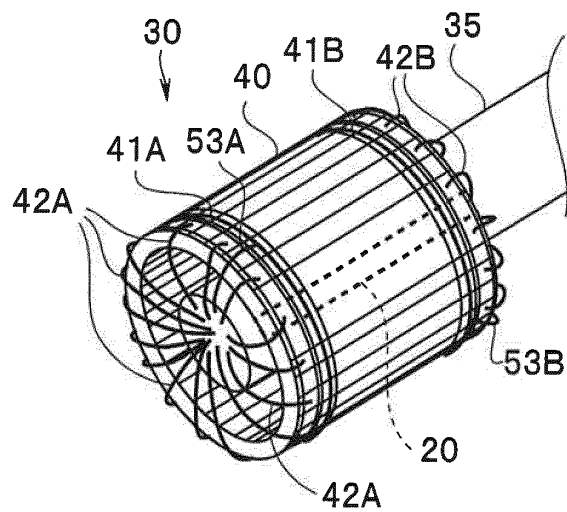


FIG.4

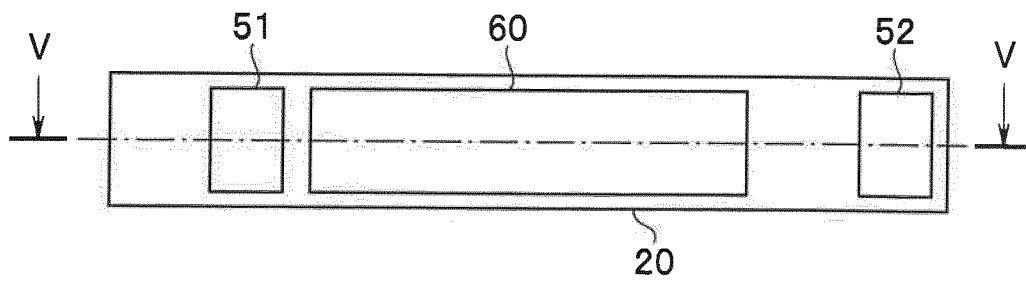


FIG.5

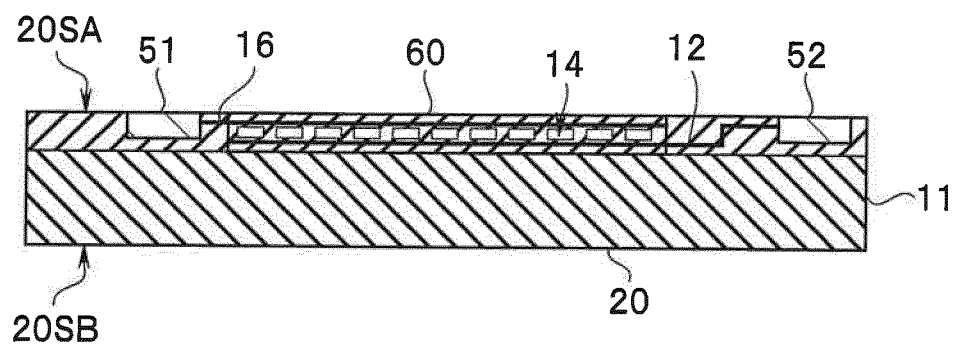


FIG.6

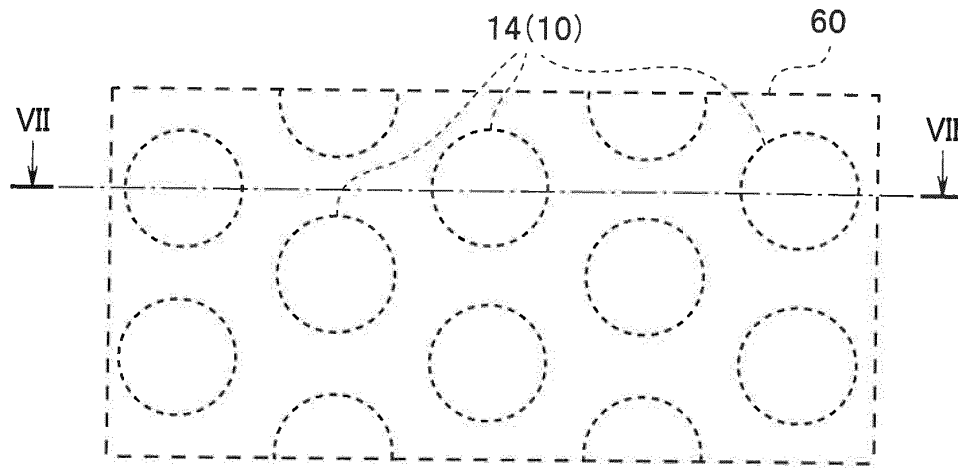


FIG.7

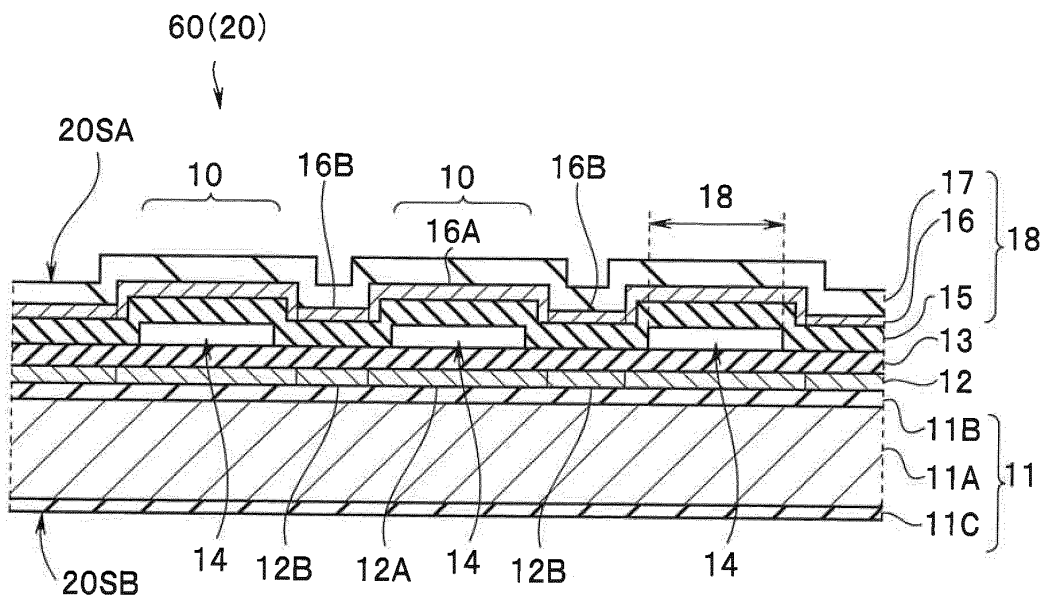


FIG.8

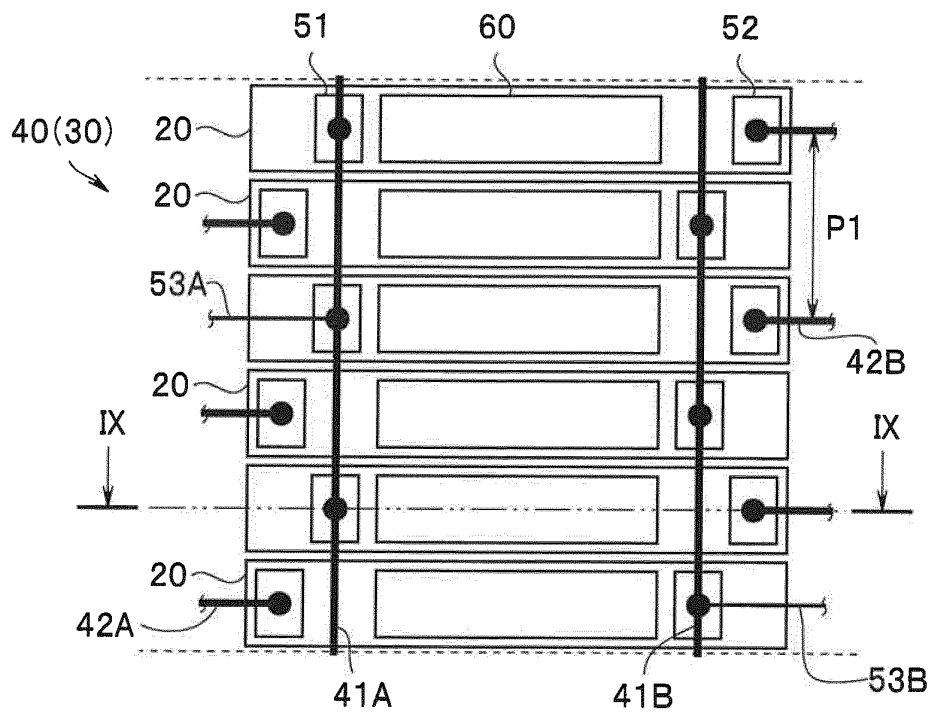


FIG.9

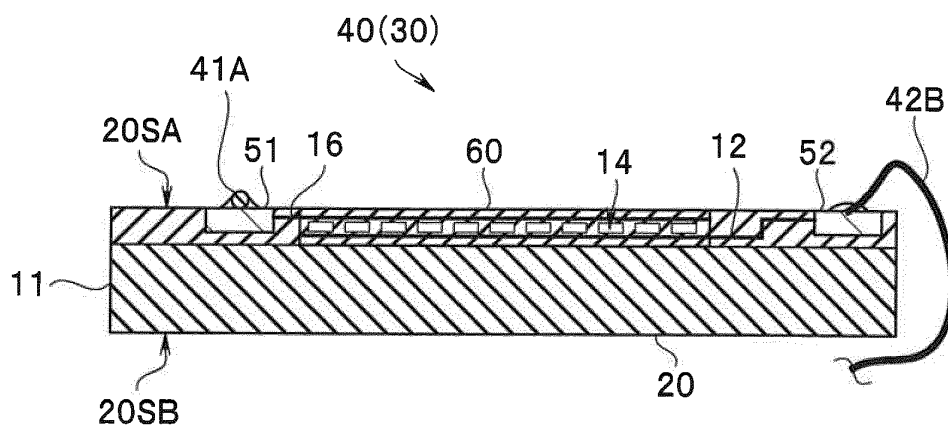


FIG.10

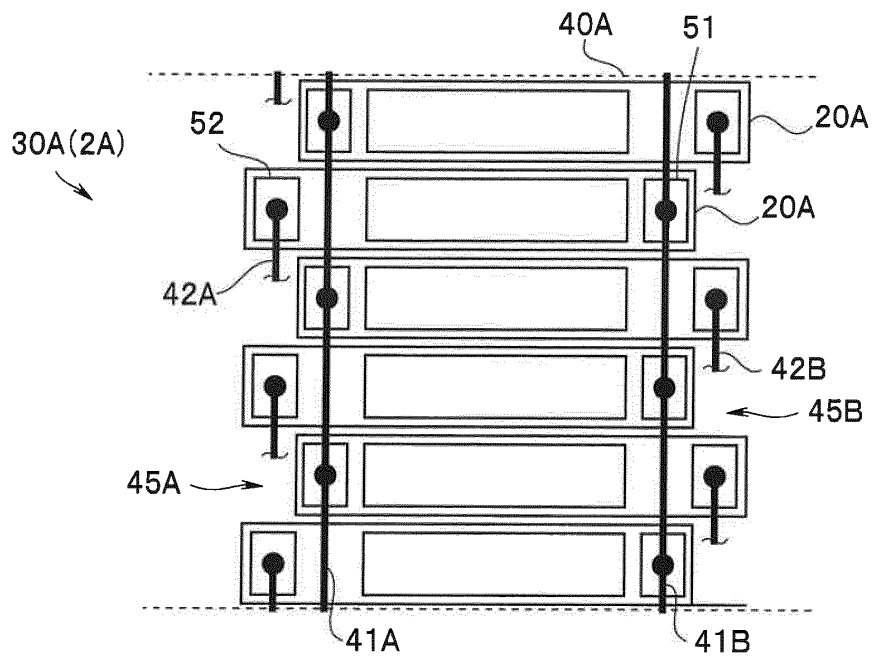


FIG.11

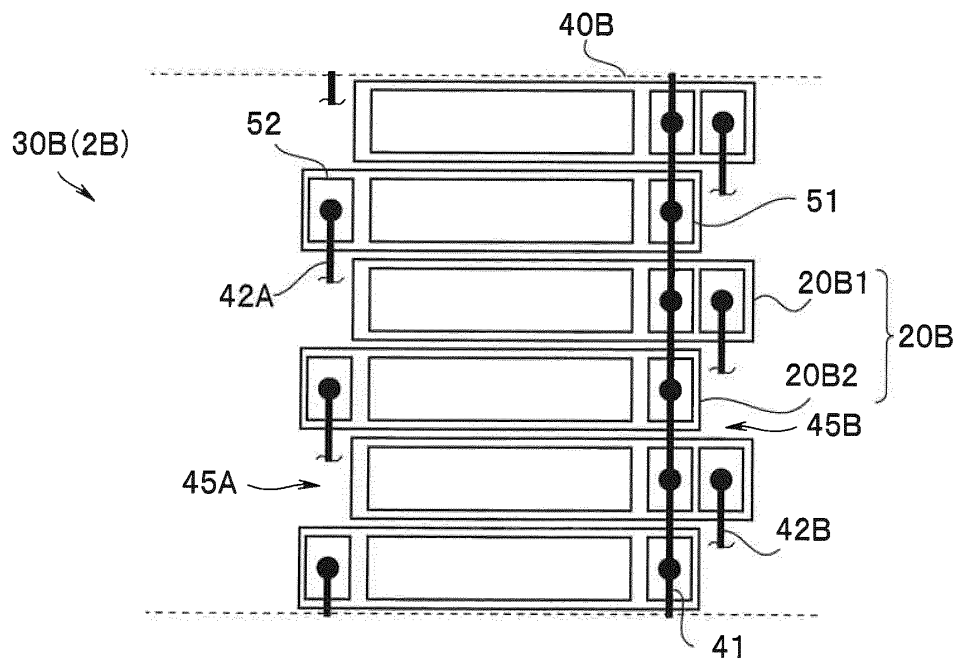


FIG.12

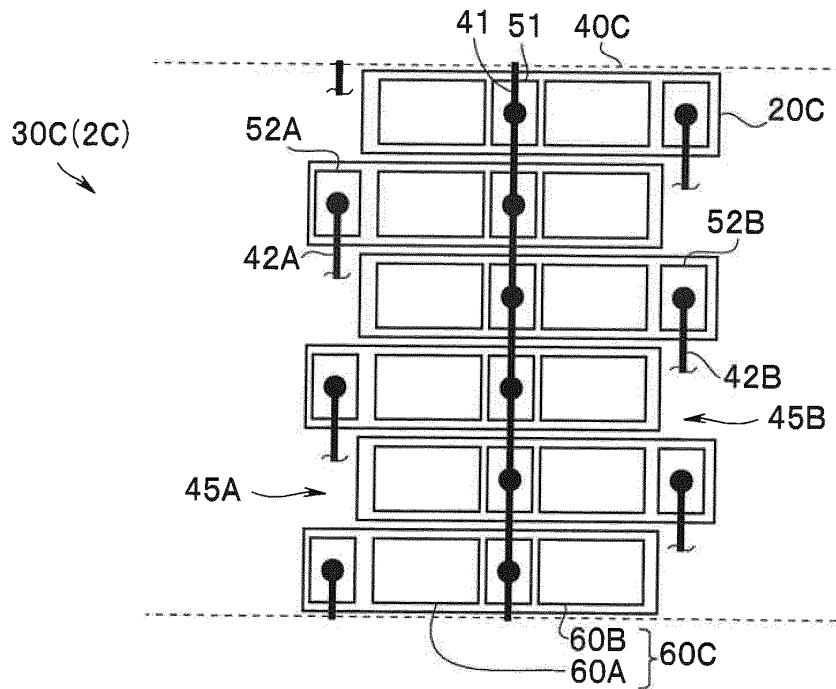


FIG.13

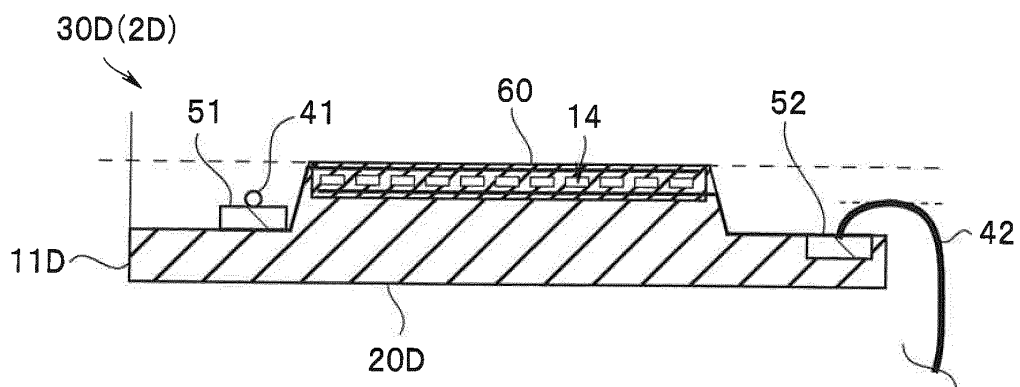


FIG.14

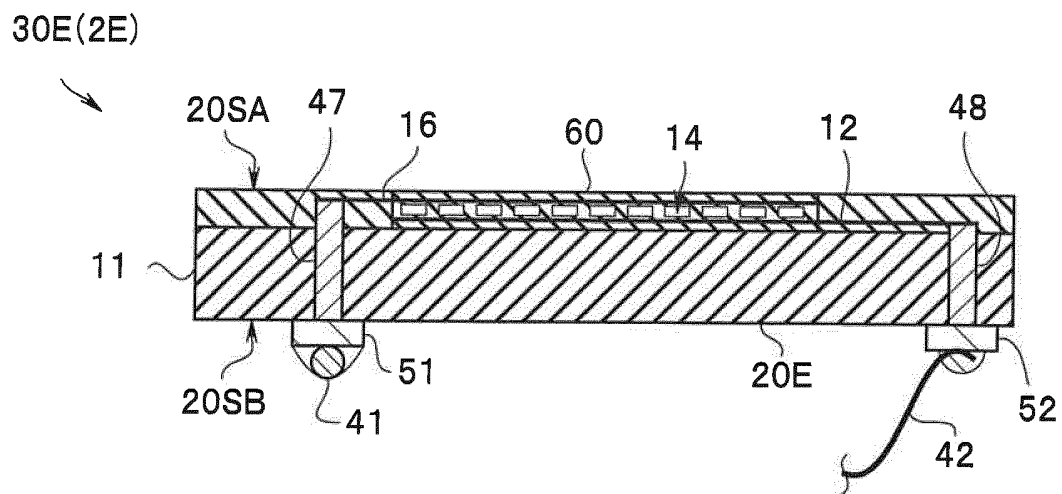


FIG.15

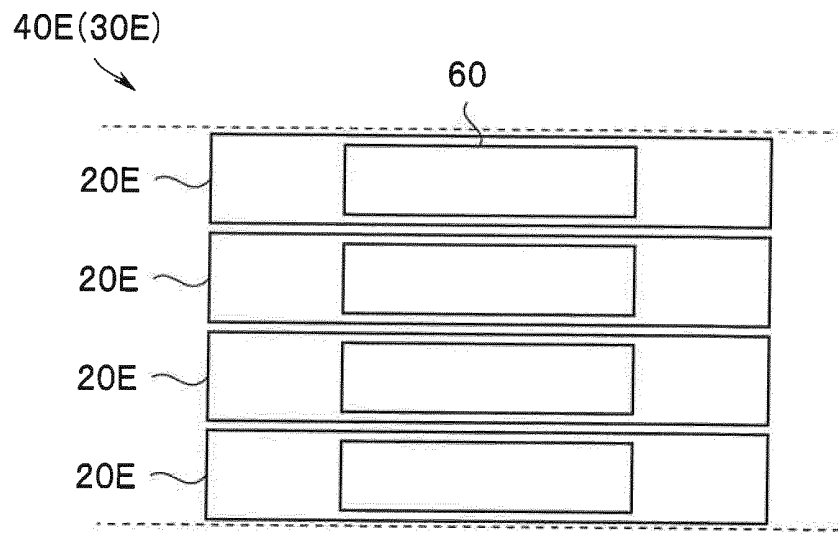


FIG.16

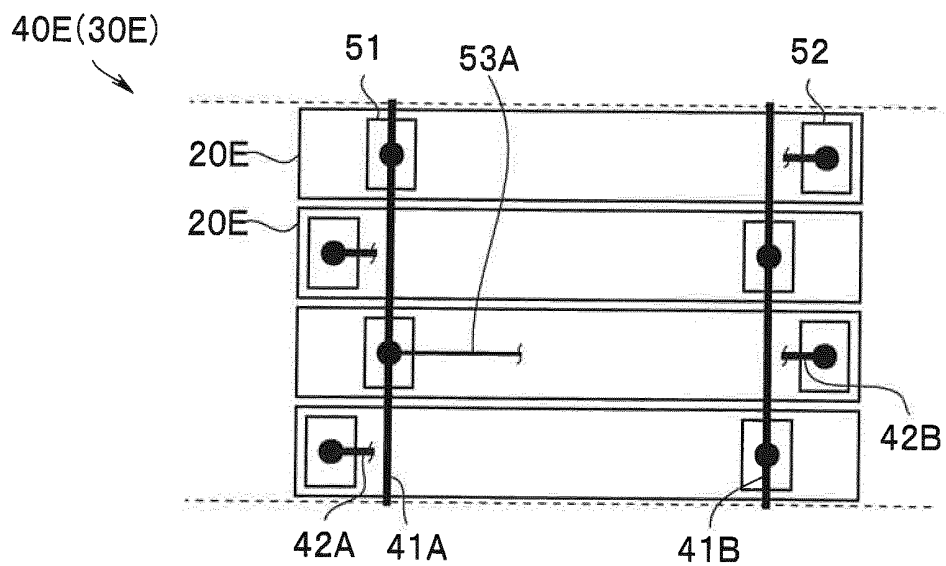


FIG.17

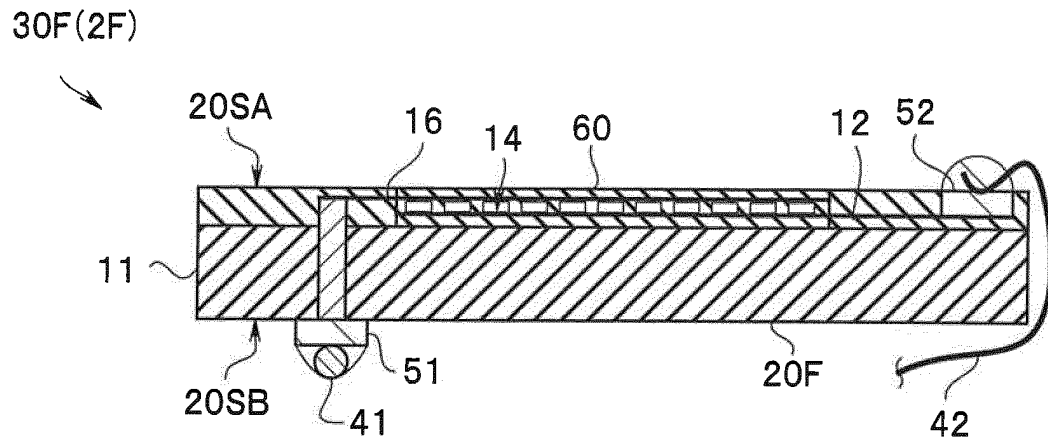
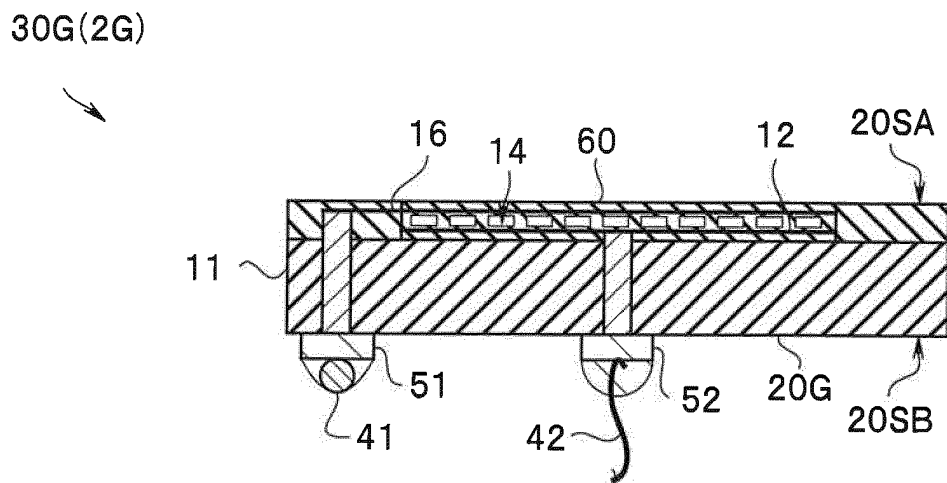


FIG.18



INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2012/065464

A. CLASSIFICATION OF SUBJECT MATTER

A61B8/12(2006.01) i

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B8/12

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Jitsuyo Shinan Koho	1922-1996	Jitsuyo Shinan Toroku Koho	1996-2012
Kokai Jitsuyo Shinan Koho	1971-2012	Toroku Jitsuyo Shinan Koho	1994-2012

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	JP 62-192651 A (Fujitsu Ltd.), 24 August 1987 (24.08.1987), page 1, lower right column to page 2, upper left column; fig. 3 (Family: none)	1-4
X	JP 64-27400 A (Nihon Dempa Kogyo Co., Ltd.), 30 January 1989 (30.01.1989), page 2, upper left column, lines 17 to 19; page 2, lower right column, line 5 to page 3, upper left column, line 12; fig. 1 (Family: none)	1-4

☒ Further documents are listed in the continuation of Box C.☐ See patent family annex.

* Special categories of cited documents:

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"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"I" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search
30 August, 2012 (30.08.12)Date of mailing of the international search report
11 September, 2012 (11.09.12)Name and mailing address of the ISA/
Japanese Patent Office

Authorized officer

Facsimile No.

Telephone No.

INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP2012/065464

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	JP 52-11926 A (Koden Electronics Co., Ltd.), 29 January 1977 (29.01.1977), page 2, upper right column, lines 12 to 15; fig. 5 (Family: none)	1-14
A	JP 55-103840 A (Matsushita Electric Industrial Co., Ltd.), 08 August 1980 (08.08.1980), page 2, upper right column, lines 16 to 20; fig. 1 to 4 (Family: none)	1-14
A	Giosue Caliano et al, Design, fabrication and characterization of a capacitive micromachined ultrasonic probe for medical imaging, IEEE TRANSACTIONS ON ULTRASONICS, FERROELECTRICS, AND FREQUENCY CONTROL, 2005.12, vol.52, no.12, pp.2259-2269	1-14
X Y	JP 2009-55475 A (Olympus Medical Systems Corp.), 12 March 2009 (12.03.2009), paragraphs [0013], [0018] to [0023], [0026] to [0027], [0035], [0113]; fig. 1 to 5 & US 8047995 B2 & EP 2030698 A1 & DE 602008002869 D	1-3, 14 4-13
Y	WO 2008/114582 A1 (Hitachi Medical Corp.), 25 September 2008 (25.09.2008), paragraph [0033]; fig. 5 & US 2010/0179430 A1 & EP 2130495 A1 & CN 101636112 A	4-13
Y	WO 2009/139400 A1 (Hitachi Medical Corp.), 19 November 2009 (19.11.2009), paragraphs [0054], [0107] to [0108]; fig. 5, 13 & US 2011/0071396 A1 & EP 2289419 A1 & CN 102026581 A	4-13
Y	JP 63-260299 A (Hitachi, Ltd.), 27 October 1988 (27.10.1988), page 2, upper left column, 3rd line from the bottom to page 2, upper right column, 3rd line from the bottom; fig. 1 (Family: none)	8-10
Y	JP 2005-304692 A (Toshiba Corp.), 04 November 2005 (04.11.2005), paragraphs [0079] to [0083]; fig. 11 (Family: none)	11-13

Form PCT/ISA/210 (continuation of second sheet) (July 2009)

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- JP 4377787 B [0005]
- JP 2011148593 A [0090]

专利名称(译)	超声波单元和超声波内窥镜		
公开(公告)号	EP2730230A1	公开(公告)日	2014-05-14
申请号	EP2012807399	申请日	2012-06-18
[标]申请(专利权)人(译)	奥林巴斯株式会社		
申请(专利权)人(译)	OLYMPUS CORPORATION		
当前申请(专利权)人(译)	OLYMPUS CORPORATION		
[标]发明人	INUI SATOSHI MATSUMOTO KAZUYA YOSHIZAWA FUKASHI IWAISAKO HIROSHI		
发明人	INUI SATOSHI MATSUMOTO KAZUYA YOSHIZAWA FUKASHI IWAISAKO HIROSHI		
IPC分类号	A61B8/12 B06B1/02		
CPC分类号	A61B8/12 A61B8/445 A61B8/4494 B06B1/0292 B06B1/0633 A61B8/461		
优先权	2011148593 2011-07-04 JP		
其他公开文献	EP2730230A4 EP2730230B1		
外部链接	Espacenet		

摘要(译)

超声单元30包括具有多个超声元件20的超声阵列40，每个超声元件20具有矩形的第一主表面，其中发送和接收部分60，信号电极端子52和接地电极端子51是沿长边方向排列，超声波元件20的长边连接，连接到多个接地电极端子51的一条或多条短线41，连接到短线41的地线43，多个信号线42，每个信号线42连接到信号电极端子52中的一个，并且超声元件20的相邻超声元件被耦合，使得信号电极端子52交替地布置在长边的相对侧上发送和接收部分60的方向是矩形的。

