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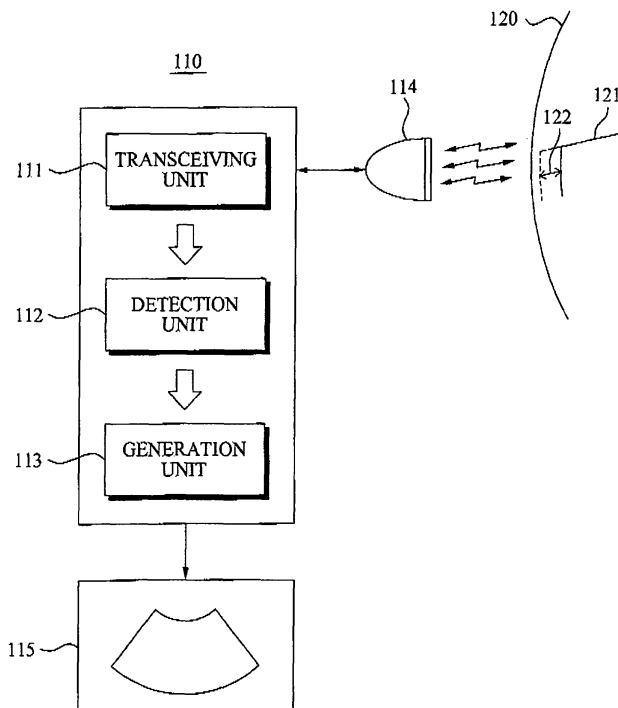
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(54) **Ultrasound system and method providing acoustic radiation force impulse imaging with high frame rate**

(57) An ultrasound method and system are provided. The ultrasound system (110) may transmit, to a target tissue (121), a pushing ultrasound signal for generating of a displacement (122), using a probe (114), receive a response signal from the target tissue in correspondence

to a tracking ultrasound signal transmitted via the probe, detect (112) displacement information associated with the target tissue using the response signal, and generate (113) the acoustic radiation force impulse image based on the displacement information.

FIG. 1



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Description

BACKGROUND

Field of the Invention

[0001] Embodiments of the present invention relate to an ultrasound system and method, and more particular, to an ultrasound system and method for providing an acoustic radiation force impulse image.

Description of the Related Art

[0002] An ultrasound system denotes a system that may emit ultrasound signals from the body surface of a subject to a selected interior portion of the body and provide images associated with blood flow or a section of soft tissue using information associated with reflected ultrasound signals. The ultrasound system is generally small and inexpensive, and also provides a display in real time. In addition, the ultrasound system has no absorbed dose such as with X rays and the like, and thus is highly stable. The ultrasound system is being widely used together with other image diagnostic apparatuses such as an X-ray diagnostic apparatus, a computerized tomography (CT) scanner, a magnetic resonance image (MRI) apparatus, a nuclear medicine diagnostic apparatus, and the like. In particular, the ultrasound system may display an interior body image in real time and thus is being variously used.

[0003] A human tissue has a characteristic of elasticity among various types of characteristics. The elasticity indicates a transformation level of the tissue with respect to a given unit force. As the elasticity increases, the transformation level may decrease. Conversely, as the elasticity decreases, the transformation level may increase. The elasticity may be a unique characteristic of the tissue. That the elasticity of the tissue has changed may mean that a physical property of the tissue has changed. For example, a cancer tissue generally has the elasticity by three times greater than a normal tissue. Such tissue generation may not be observed using a general ultrasound image. Accordingly, when the elasticity of the tissue is observed using ultrasound, it is possible to discern the cancer tissue from the normal tissue.

SUMMARY

[0004] According to an aspect of the present invention, there is provided an ultrasound method of providing an acoustic radiation force impulse image, the method including: transmitting, to a target tissue, a pushing ultrasound signal for generating of a displacement, using a probe; receiving a response signal from the target tissue in correspondence to a tracking ultrasound signal transmitted via the probe; detecting displacement information associated with the target tissue using the response signal; and generating the acoustic radiation force impulse

image based on the displacement information.

[0005] Here, the transmitting of the pushing ultrasound signal may include simultaneously transmitting the pushing ultrasound signal along a plurality of scan lines that are spaced apart from each other by a predetermined distance.

[0006] Also, the transmitting of the pushing ultrasound signal may include sequentially transmitting the pushing ultrasound signal with respect to a plurality of focal points along a scan line. Also, a frequency of the pushing ultrasound signal may be variable according to each of the focal points.

[0007] Also, the pushing ultrasound signal may be transmitted with respect to different focal points for each of the scan lines. Also, a frequency of the pushing ultrasound signal may be variable according to each of the different focal points.

[0008] Also, the probe may include two-dimensionally arranged transducers and the transducers may be classified into a plurality of sections. While the pushing ultrasound signal is being transmitted using a transducer included in a first section among the plurality of sections, the tracking ultrasound signal may be transmitted using a transducer included in a second section among the plurality of sections.

[0009] Also, the method may further include transmitting a control command to a cooling device associated with the target tissue in correspondence to transmitting of the pushing ultrasound signal.

[0010] According to another aspect of the present invention, there is provided an ultrasound system for providing an acoustic radiation force impulse image, the system including: a transceiving unit to transmit, to a target tissue, a pushing ultrasound signal for generating of a displacement, using a probe, and to receive a response signal from the target tissue in correspondence to a tracking ultrasound signal transmitted via the probe; a detection unit to detect displacement information associated with the target tissue using the response signal; and a generation unit to generate the acoustic radiation force impulse image based on the displacement information.

[0011] According to embodiments of the present invention, there may be provided an ultrasound system and method for providing an acoustic radiation force impulse image that may apply a pushing ultrasound signal along a plurality of scan lines and thereby improve a frame rate.

[0012] Also, according to embodiments of the present invention, there may be provided an ultrasound system and method for providing an acoustic radiation force impulse image that may apply a pushing ultrasound signal with respect to a plurality of focal points for each single scan line and thereby prevent overheating of a target tissue and may also improve a frame rate.

[0013] Also, according to embodiments of the present invention, there may be provided an ultrasound system and method for providing an acoustic radiation force impulse image that may simultaneously apply a pushing

ultrasound signal and a tracking ultrasound signal using different transducers and thereby more effectively obtain an acoustic radiation force impulse image.

[0014] Also, according to embodiments of the present invention, there may be provided an ultrasound system and method for providing an acoustic radiation force impulse image that may prevent overheating of a target tissue via a cooling device and thereby prevent a degeneration and a necrosis of the target tissue.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015] These and/or other aspects, features, and advantages of the invention will become apparent and more readily appreciated from the following description of exemplary embodiments, taken in conjunction with the accompanying drawings of which:

- FIG. 1 is a block diagram illustrating an ultrasound system for providing an acoustic radiation force impulse image according to an embodiment of the present invention;
- FIG. 2 is a flowchart illustrating an ultrasound method of providing an acoustic radiation force impulse image according to an embodiment of the present invention;
- FIG. 3 illustrates an example of transmitting a pushing ultrasound signal along a plurality of scan lines according to an embodiment of the present invention;
- FIG. 4 illustrates an example of transmitting a pushing ultrasound signal with respect to a plurality of focal points according to an embodiment of the present invention; and
- FIG. 5 illustrates an example of transmitting a different ultrasound signal for each transducer section according to an embodiment of the present invention.

DETAILED DESCRIPTION

[0016] Reference will now be made in detail to exemplary embodiments of the present invention, examples of which are illustrated in the accompanying drawings, wherein like reference numerals refer to the like elements throughout. Exemplary embodiments are described below to explain the present invention by referring to the figures.

[0017] FIG 1 is a block diagram illustrating an ultrasound system 110 for providing an acoustic radiation force impulse image according to an embodiment of the present invention.

[0018] As shown in FIG. 1, the ultrasound system 110 may receive a response signal in correspondence to a tracking ultrasound signal that is transmitted to a subject 120 via a probe 114. The response signal denotes a signal that is transmitted or reflected from the subject 120 by the tracking ultrasound signal. Also, the ultrasound

system 110 may generate ultrasound image data using the response signal, generate an ultrasound image from the ultrasound image data, and display the ultrasound image via an internal or external display device 115. Here, the ultrasound image may be displayed in either a two-dimensional (2D) form or a three-dimensional (3D) form. Also, the subject 120 may be a human body. The probe 114 may include transducers that transmit and receive the tracking ultrasound signal.

[0019] The ultrasound system 110 may transmit a pushing ultrasound signal to the subject 120 via the probe 120. In this case, the pushing ultrasound signal may cause a displacement 122 in a target tissue 121 of the subject 120. The pushing ultrasound signal may be transmitted to the subject 120 prior to transmitting of the tracking ultrasound signal and reception of the response signal.

[0020] The ultrasound system 110 may detect displacement information associated with the target tissue 121 using the response signal and generate the acoustic radiation force impulse image based on the displacement information. The displacement information may include a displacement level of the target tissue 121 that is caused by the pushing ultrasound signal.

[0021] The acoustic radiation force impulse image may indicate an elasticity level of the target tissue 121. A user may determine a state of the target tissue 121 based on the elasticity level of the target tissue 121. For example, the user may detect a tissue such as a wen having an elasticity less than a general tissue and may also detect a tissue degeneration such as a cancer having an elasticity greater than the general tissue, using the acoustic radiation force impulse image.

[0022] As described above, the ultrasound system 110 may provide the acoustic radiation force impulse image of the target tissue 121 together with the general ultrasound image.

[0023] The ultrasound system 110 may include a transceiving unit 111, a detection unit 112, and a generation unit 113. Here, the transceiving unit 111 may transmit, to the target tissue 121, a pushing ultrasound signal for generating of a displacement using the probe 114 and may receive a response signal from the target tissue 11 in correspondence to a tracking ultrasound signal transmitted via the probe 114. The detection unit 112 may detect displacement information associated with the target tissue 121 using the response signal. The generation unit 113 may generate the acoustic radiation force impulse image based on the displacement information. Also, although not shown in FIG 1, the ultrasound system 110 may further include a cooling device to decrease a temperature of the target tissue 121. The transceiving unit 111 may transmit a control command to the cooling device in correspondence to transmitting of the pushing ultrasound signal.

[0024] Hereinafter, an operating method of the ultrasound system 110 constructed as above will be further described in detail with reference to FIGS. 2 through 5.

[0025] FIG. 2 is a flowchart illustrating an ultrasound method of providing an acoustic radiation force impulse image according to an embodiment of the present invention.

[0026] As shown in FIG 2, the ultrasound method of providing the acoustic radiation force impulse image may be performed via operations S201 through S204. Here, operations S201 and S202 may be performed by the transceiving unit 111. Operation S203 may be performed by the detection unit 112. Operation S204 may be performed by the generation unit 113.

[0027] In operation S201, the transceiving unit 111 may transmit, to a target tissue, a pushing ultrasound signal for generating of a displacement using a probe. Here, the pushing ultrasound signal may induce a displacement of the target tissue. Specifically, the target tissue may be moved by the pushing ultrasound signal. This movement may induce the displacement. The displacement of the target tissue may be in inverse proportion to an elasticity of the target tissue. A recovering speed of a tissue may be in proportion to a viscoelasticity of the target tissue.

[0028] Generally, a short and strong sound wave may cause a greater displacement in comparison to a long and weak sound wave. Accordingly, examples of the pushing ultrasound signal may include an ultrasound signal that has a single pulse and a great amplitude. Since a maximum output of the ultrasound signal of the ultrasound system 110 is pre-determined, the transceiving unit 111 may generate the pushing ultrasound signal by extending the ultrasound signal of the maximum output as long as possible. Also, according to an embodiment of the present invention, the transceiving unit 111, may generate the pushing ultrasound signal using a sufficiently long color Doppler pulse signal with a great amplitude.

[0029] In operation S202, the transceiving unit 111 may receive a response signal from the target tissue in correspondence to a tracking ultrasound signal transmitted via the probe. Here, the tracking ultrasound signal may be used to measure a level of the displacement of the target tissue. The response signal may include information associated with the level of the displacement. For example, the tracking ultrasound signal may include a B mode ultrasound signal. The tracking ultrasound signal may be transmitted to a region of interest (ROI) including the target tissue. The response signal may be reflected from the ROI and thereby be received.

[0030] According to an embodiment of the present invention, the transceiving unit 111 may simultaneously transmit the pushing ultrasound signal along a plurality of scan lines that are spaced apart from each other by a predetermined distance.

[0031] FIG 3 illustrates an example of transmitting a pushing ultrasound signal along a plurality of scan lines according to an embodiment of the present invention.

[0032] As shown in a block 301, the transceiving unit 111 may transmit the pushing ultrasound signal to a target tissue via a single scan line. Also, as shown in a block

302, the transceiving unit 111 may simultaneously transmit the pushing ultrasound signal along the plurality of scan lines that are spaced apart from each other by a predetermined distance. As described above, the transceiving unit 111 may measure a displacement of the target tissue at the plurality of scan lines at one time by simultaneously transmitting the pushing ultrasound signals via the plurality of scan lines. Also, since the transceiving unit 111 may transmit the pushing ultrasound signal via the plurality of scan lines that are spaced apart from each other by the predetermined distance, it is possible to distribute a temperature rise of the target tissue and thereby prevent overheating or damage of the target tissue.

[0033] Also, the transceiving unit 111 may transmit the tracking ultrasound signal to the target tissue along the plurality of scan lines and receive a response signal that is reflected from the target tissue in correspondence to transmitting of the tracking ultrasound signal.

[0034] According to an embodiment of the present invention, the transceiving unit 111 may sequentially transmit the pushing ultrasound signal to a plurality of focal points along a scan line.

[0035] FIG. 4 illustrates an example of transmitting a pushing ultrasound signal with respect to a plurality of focal points according to an embodiment of the present invention.

[0036] As shown in a block 401, the transceiving unit 111 may sequentially transmit the pushing ultrasound signal with respect to the plurality of focal points along a scan line. For example, the transceiving unit 111 may sequentially transmit the pushing ultrasound signal with respect to the focal points from A to I along a single scan line. Here, a frequency of the pushing ultrasound signal may be variable according to each of the focal points. For example, the transceiving unit 111 may transmit a relatively low frequency of pushing ultrasound signal with respect to a focal point with a relatively deep depth and thereby make the pushing ultrasound signal reaching a deep target tissue be less attenuated. Generally, the attenuation may incur more frequently as the frequency of the pushing ultrasound signal is higher and the depth of the focal point is deeper. Also, the transceiving unit 111 may transmit the tracking ultrasound signal with respect to the plurality of focal points along the scan line and receive a response signal reflected from the target tissue in correspondence to transmitting of the tracking ultrasound signal.

[0037] According to an embodiment of the present invention, when transmitting the pushing ultrasound signal to the target tissue via a plurality of scan lines, the transceiving unit 111 may simultaneously transmit the pushing ultrasound signal with respect to different focal points for each of the scan lines.

[0038] For example, as shown in a block 402, the transceiving unit 111 may apply the pushing ultrasound signal in a focal point order of A, B, and C via a first scan line, apply the pushing ultrasound signal in a focal point order

of B, C, and A via a second scan line, and apply the pushing ultrasound signal in a focal point order of C, A, and B via a third scan line at the same time. Also, a frequency of the pushing ultrasound signal may be variable according to each of the different focal points. Displacement information associated with each of the different focal points may be simultaneously detected. Also, the transceiving unit 111 may simultaneously transmit the tracking ultrasound signal with respect to the different focal points and receive a response signal reflected from the target tissue in correspondence to transmitting of the tracking ultrasound signal.

[0039] According to an embodiment of the present invention, when transmitting, to a target tissue, a pushing ultrasound signal for generating of a displacement and receiving a response signal from the target tissue in correspondence to transmitting of the tracking ultrasound signal, the transceiving unit 111 may use a probe including two-dimensionally arranged transducers. Here, the transducers may be classified into a plurality of sections. While transmitting the pushing ultrasound signal using a transducer included in a first section among the plurality of sections, the transceiving unit 111 may transmit the tracking ultrasound signal using a transducer included in a second section among the plurality of sections.

[0040] FIG. 5 illustrates an example of transmitting a different ultrasound signal for each transducer section according to an embodiment of the present invention.

[0041] Referring to FIG 5, the transceiving unit 111 may transmit a pushing ultrasound signal using a transducer 511 included in a first section among a plurality of two-dimensionally arranged transducers 510 and simultaneously transmit a tracking ultrasound signal using a transducer 510 included in a second section. Also, while transmitting the pushing ultrasound signal using the transducer 511 of the first section, the transceiving unit 111 may receive a response signal using the transducer 512 of the second section. Also, while transmitting the pushing ultrasound signal to a first target tissue, a first ROI, or a first focal point using the transducer 511 of the first section, the transceiving unit 511 may transmit the pushing ultrasound signal to a second target tissue, a second ROI, or a second focal point using the transducer 512 of the second section.

[0042] According to an embodiment of the present invention, the transceiving unit 111 may use transducers, included in a particular section among the two-dimensionally arranged transducers 510 in order to generate a constant B mode ultrasound image. For example, the transceiving unit 111 may use an array corresponding to a bottom line among the arranged transducers 510 in order to generate the constant B mode ultrasound image. Specifically, the transceiving unit 111 may use transducers, included in a particular section, to transmit a constant tracking ultrasound signal and receive a response signal in correspondence thereto.

[0043] As described above, the transceiving unit 111 may allocate a different role to the transducers 510 for

each section and thereby making it possible to more effectively obtain an acoustic radiation force impulse image.

[0044] Referring again to FIG. 2, in operation S203, the detection unit 112 may detect displacement information associated with the target tissue using the response signal. Here, the response signal may include displacement information associated with the target tissue.

[0045] Specifically, the detection unit 112 may perform an envelope detection process that detects the magnitude of the response signal based on the response signal to thereby form ultrasound image data. Specifically, the detection unit 112 may form the ultrasound image data based on location information associated with a plurality of points existing in each scan line and data that is obtained from each of the points to thereby form ultrasound image data. Here, the ultrasound image data may include coordinates on an XY coordinate system at each point, angle information associated with each scan line with respect to a vertical scan line, data obtained at each point, and the like. Also, the detection unit 112 may compare ultrasound image data before and after a displacement of the target tissue occurs due to the applied pushing ultrasound signal and thereby may detect the displacement information.

[0046] In operation S204, the generation unit 113 may generate an acoustic radiation force impulse image based on the displacement information.

[0047] For example, the generation unit 113 may generate ultrasound image data associated with the target tissue or the ROI based on the response signal and generate a B mode ultrasound image using the ultrasound image data. Also, the generation unit 113 may generate the acoustic radiation force impulse image by overlapping the displacement information associated with the target tissue and the B mode ultrasound image.

[0048] Although not shown in FIG. 2, the ultrasound system 110 may further perform transmitting a control command to a cooling device associated with the target tissue in correspondence to transmitting of the pushing ultrasound signal. Through this, the ultrasound system 110 may control a temperature rise of the target tissue caused by the pushing ultrasound signal. In particular, the ultrasound system 110 may operate the cooling device positioned on the epidermis of the target tissue, while transmitting the pushing ultrasound signal to the transducers of the probe.

[0049] The ultrasound method for providing the acoustic radiation force impulse image according to the above-described exemplary embodiments of the present invention may be recorded in computer-readable media including program instructions to implement various operations embodied by a computer. The media may also include, alone or in combination with the program instructions, data files, data structures, and the like. Examples of computer-readable media include magnetic media such as hard disks, floppy disks, and magnetic tape; optical media such as CD ROM disks and DVDs; magneto-optical

media such as floptical disks; and hardware devices that are specially configured to store and perform program instructions, such as read-only memory (ROM), random access memory (RAM), flash memory, and the like. Examples of program instructions include both machine code, such as produced by a compiler, and files containing higher level code that may be executed by the computer using an interpreter. The described hardware devices may be configured to act as one or more software modules in order to perform the operations of the above-described exemplary embodiments of the present invention, or vice versa.

[0050] Although a few exemplary embodiments of the present invention have been shown and described, the present invention is not limited to the described exemplary embodiments. Instead, it would be appreciated by those skilled in the art that changes may be made to these exemplary embodiments without departing from the principles and spirit of the invention, the scope of which is defined by the claims and their equivalents.

Claims

1. An ultrasound method of providing an acoustic radiation force impulse image, the method comprising:
 - transmitting, to a target tissue, a pushing ultrasound signal for generating of a displacement, using a probe;
 - receiving a response signal from the target tissue in correspondence to a tracking ultrasound signal transmitted via the probe;
 - detecting displacement information associated with the target tissue using the response signal; and
 - generating the acoustic radiation force impulse image based on the displacement information.
2. The method of claim 1, wherein the transmitting of the pushing ultrasound signal comprises simultaneously transmitting the pushing ultrasound signal along a plurality of scan lines that are spaced apart from each other by a predetermined distance.
3. The method of claim 1, wherein the transmitting of the pushing ultrasound signal comprises sequentially transmitting the pushing ultrasound signal with respect to a plurality of focal points along a scan line.
4. The method of claim 3, wherein a frequency of the pushing ultrasound signal is variable according to each of the focal points.
5. The method of claim 2, wherein the pushing ultrasound signal is transmitted with respect to different focal points for each of the scan lines.
6. The method of claim 5, wherein a frequency of the pushing ultrasound signal is variable according to each of the different focal points.
7. The method of claim 1, wherein the probe includes two-dimensionally arranged transducers, the transducers are classified into a plurality of sections, and while the pushing ultrasound signal is being transmitted using a transducer included in a first section among the plurality of sections, the tracking ultrasound signal is transmitted using a transducer included in a second section among the plurality of sections.
8. The method of claim 1, further comprising:
 - transmitting a control command to a cooling device associated with the target tissue in correspondence to transmitting of the pushing ultrasound signal.
9. A computer-readable recording medium storing a program for implementing the method of claim 1.
10. An ultrasound system for providing an acoustic radiation force impulse image, the system comprising:
 - a transceiving unit to transmit, to a target tissue, a pushing ultrasound signal for generating of a displacement, using a probe, and to receive a response signal from the target tissue in correspondence to a tracking ultrasound signal transmitted via the probe;
 - a detection unit to detect displacement information associated with the target tissue using the response signal; and
 - a generation unit to generate the acoustic radiation force impulse image based on the displacement information.
11. The system of claim 10, wherein the transceiving unit simultaneously transmits the pushing ultrasound signal along a plurality of scan lines that are spaced apart from each other by a predetermined distance.
12. The system of claim 10, wherein the transceiving unit sequentially transmits the pushing ultrasound signal with respect to a plurality of focal points along a scan line.
13. The system of claim 10, wherein the probe includes two-dimensionally arranged transducers, the transducers are classified into a plurality of sections, and while the pushing ultrasound signal is being transmitted using a transducer included in a first section among the plurality of sections, the tracking ultrasound signal is transmitted using a transducer included in a second section among the plurality of

sections.

14. The system of claim 10, further comprising:

a cooling device to decrease a temperature of the target tissue, 5

wherein the transceiving unit transmits a control command to the cooling device in correspondence to transmitting of the pushing ultrasound signal. 10

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FIG. 1

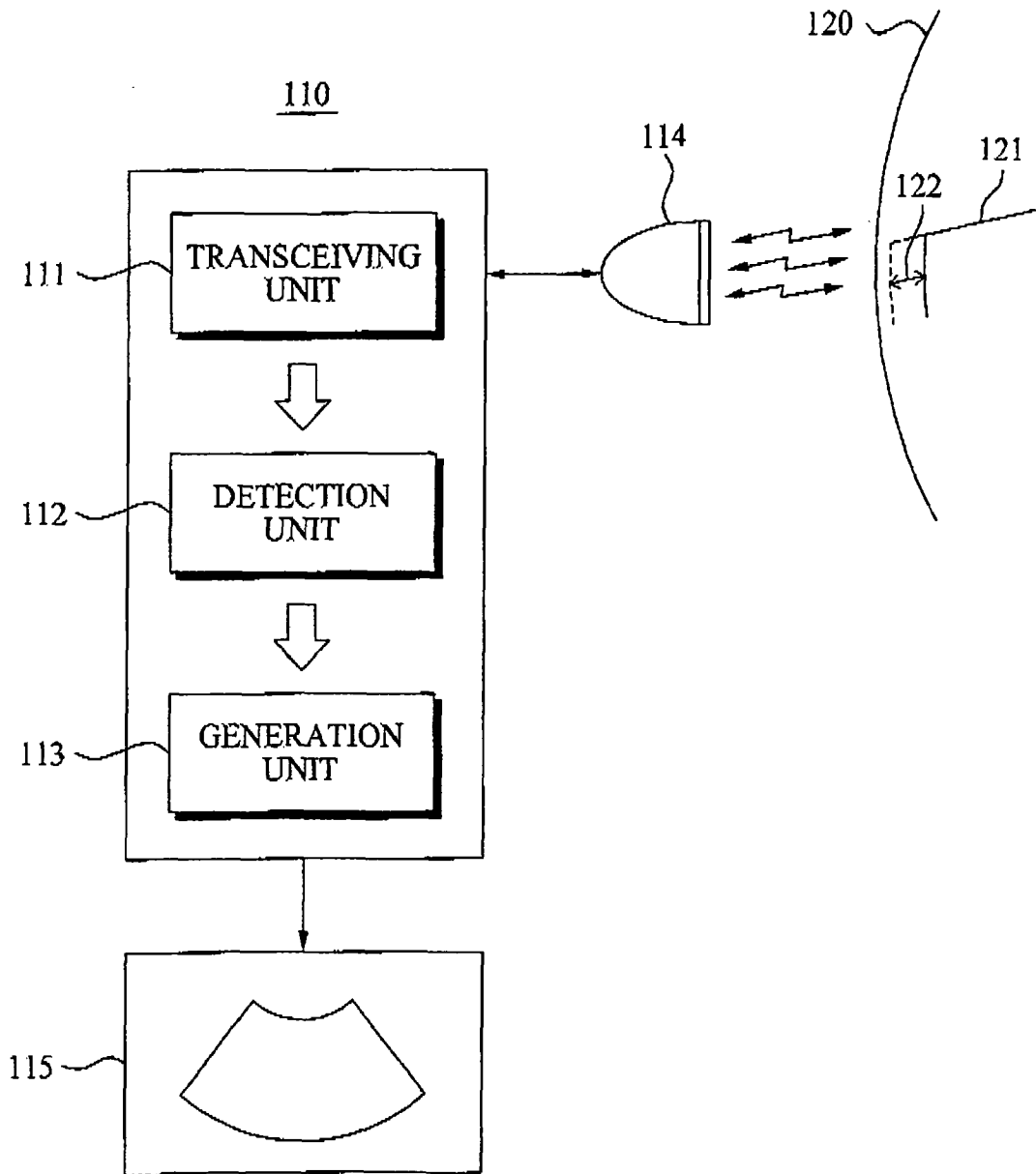


FIG. 2

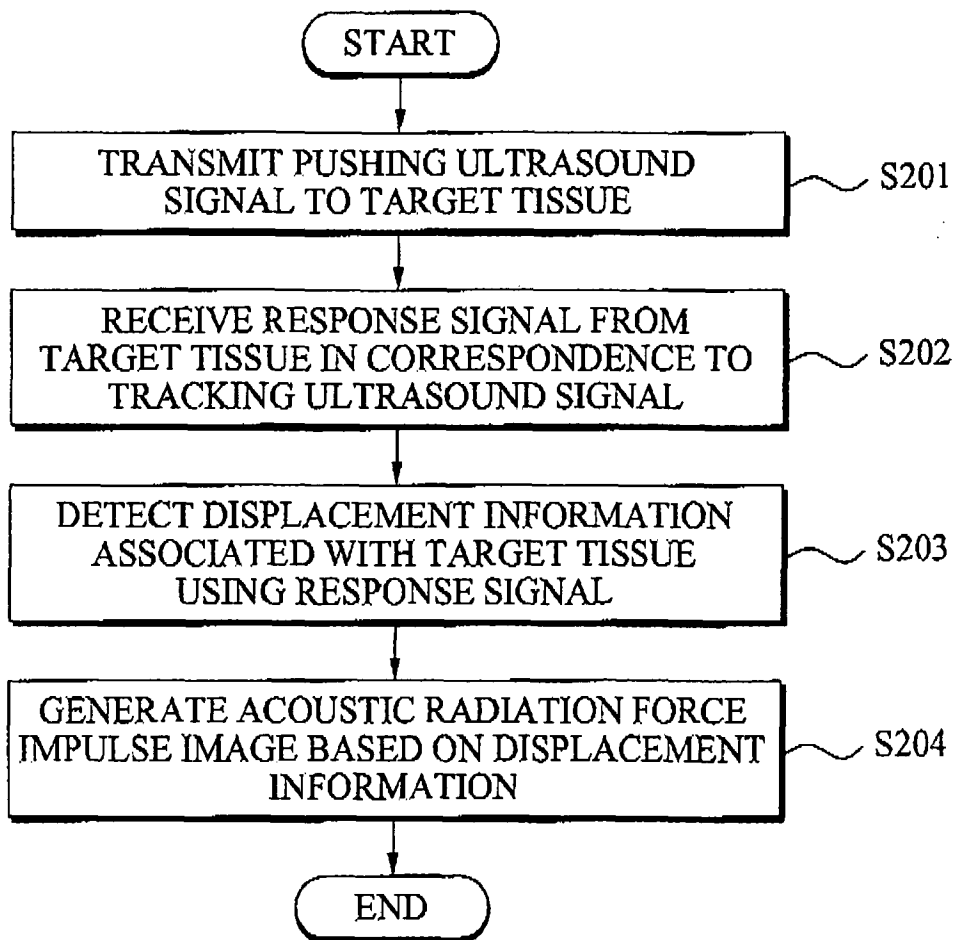


FIG. 3

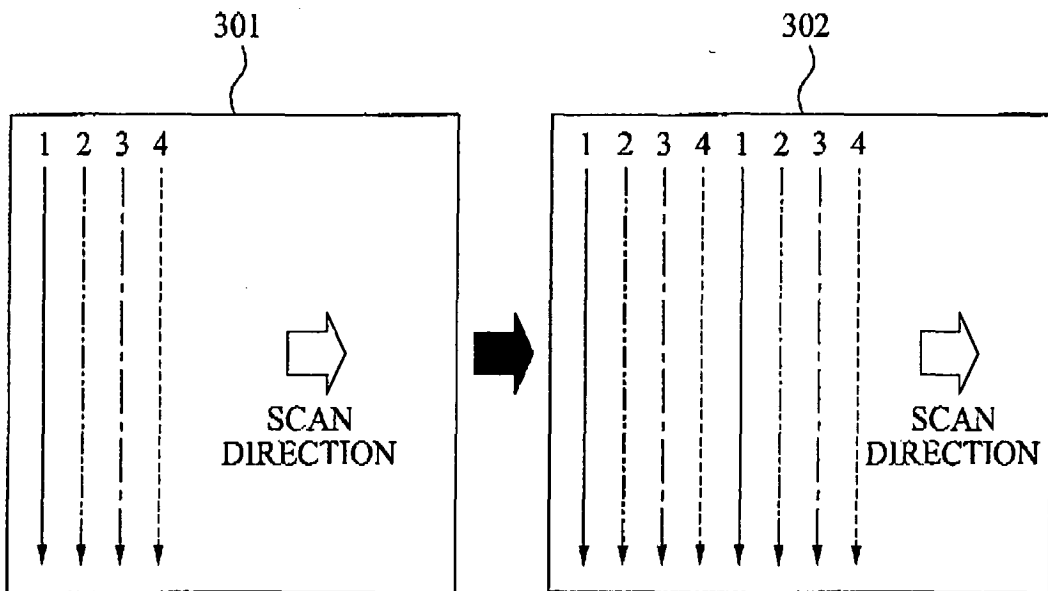


FIG. 4

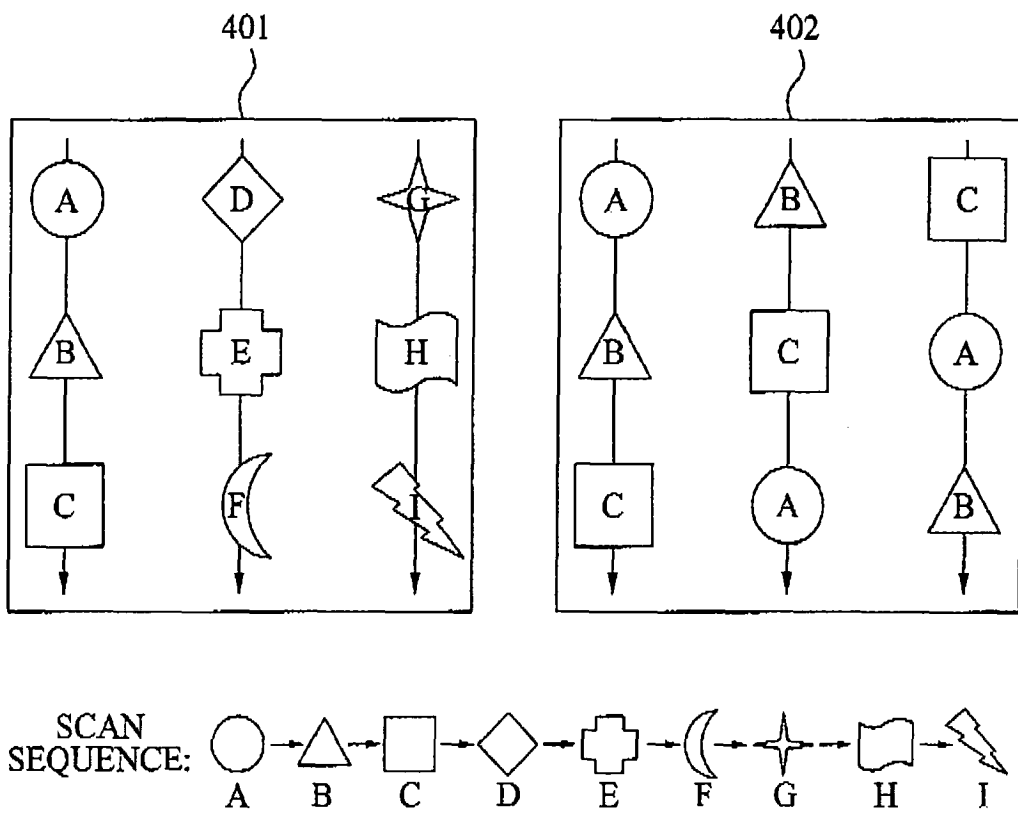
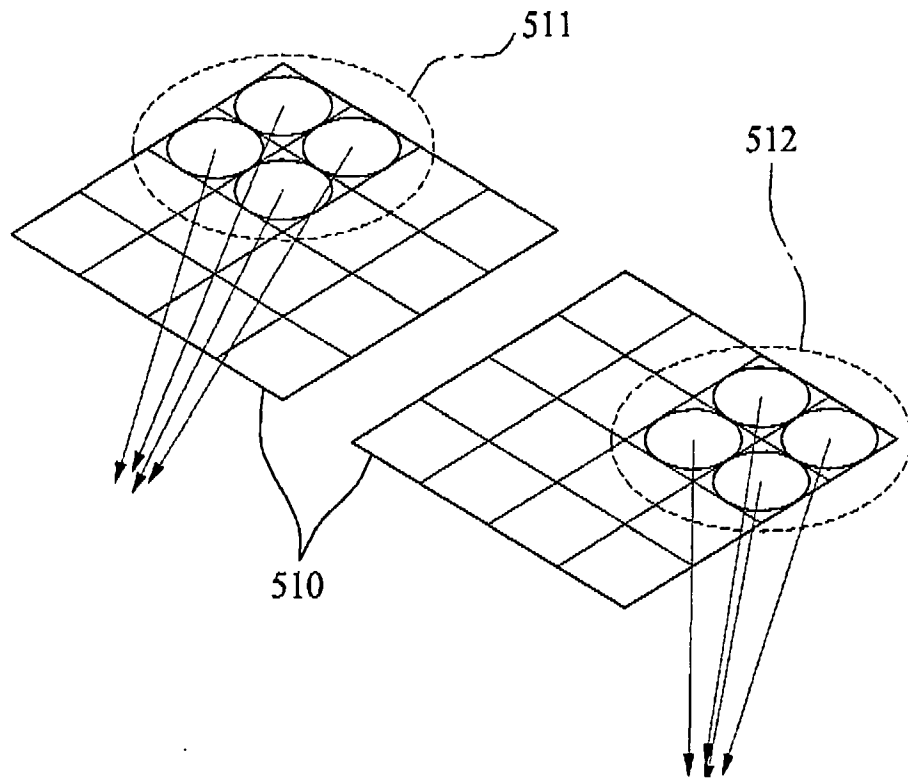


FIG. 5





EUROPEAN SEARCH REPORT

Application Number
EP 09 00 5620

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 2005/215899 A1 (TRAHEY GREGG E [US] ET AL) 29 September 2005 (2005-09-29) * paragraph [0039] - paragraph [0092]; figures 1-6 *	1-14	INV. A61B8/08
X	US 2004/068184 A1 (TRAHEY GREGG E [US] ET AL) 8 April 2004 (2004-04-08) * paragraph [0028] - paragraph [0049]; figures *	1-3,9-12	
X	BERCOFF J ET AL: "SUPERSONIC SHEAR IMAGING: A NEW TECHNIQUE FOR SOFT TISSUE ELASTICITY MAPPING" IEEE TRANSACTIONS ON ULTRASONICS, FERROELECTRICS AND FREQUENCY CONTROL, IEEE, US, vol. 51, no. 4, 1 April 2004 (2004-04-01), pages 396-409, XP001218171 ISSN: 0885-3010 * the whole document *	1,9-10	
X	WO 02/43564 A2 (ALLEZ PHYSIONIX LTD [CA]; UNIV WASHINGTON [US]) 6 June 2002 (2002-06-06) * page 33, line 11 - page 36, line 32; figures 2,3,4 *	1-2,5, 9-11	
A	WO 2006/042201 A1 (GUIDED THERAPY SYSTEMS LLC [US]; BARTHE PETER G [US]; SLAYTON MICHAEL) 20 April 2006 (2006-04-20) * page 25, line 6 - page 26, line 15; figures 4a,4b,11 *	8,14	
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 17 March 2010	Examiner Rosenblatt, Thomas
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

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EPO FORM 1503 03.02 (P04C01)

ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.

EP 09 00 5620

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report. The members are as contained in the European Patent Office EDP file on
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17-03-2010

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2005215899 A1	29-09-2005	NONE	
US 2004068184 A1	08-04-2004	NONE	
WO 0243564 A2	06-06-2002	AU 3936002 A	11-06-2002
		CA 2428872 A1	06-06-2002
		EP 1345527 A2	24-09-2003
		JP 2004520870 T	15-07-2004
		JP 2008279274 A	20-11-2008
WO 2006042201 A1	20-04-2006	CA 2583522 A1	20-04-2006
		EP 1855759 A1	21-11-2007
		JP 2008515559 T	15-05-2008
		KR 20070106972 A	06-11-2007
		US 2006241442 A1	26-10-2006
		US 2006122508 A1	08-06-2006
		US 2006089632 A1	27-04-2006
		US 2009182231 A1	16-07-2009

专利名称(译)	超声系统和方法提供具有高帧速率的声辐射力脉冲成像		
公开(公告)号	EP2186482A1	公开(公告)日	2010-05-19
申请号	EP2009005620	申请日	2009-04-22
申请(专利权)人(译)	MEDISON CO. , LTD.		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD.		
[标]发明人	JOO JONGHO KIM JONG SIK		
发明人	JOO, JONGHO KIM, JONG-SIK		
IPC分类号	A61B8/08		
CPC分类号	A61B8/08 A61B5/0048 A61B8/485 G01S7/52022 G01S7/52036 G01S7/52042 G01S7/52085 G01S15/8927		
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外部链接	Espacenet		

摘要(译)

提供了一种超声方法和系统。超声系统 (110) 可以使用探针 (114) 向目标组织 (121) 发送用于产生位移 (122) 的推动超声信号，从跟踪对应的目标组织接收响应信号。通过探头传输的超声信号，使用响应信号检测 (112) 与目标组织相关联的位移信息，并基于位移信息生成 (113) 声辐射力脉冲图像。

FIG. 1

