



(11) **EP 2 281 509 A1**

(12) **EUROPEAN PATENT APPLICATION**

(43) Date of publication:
09.02.2011 Bulletin 2011/06

(51) Int Cl.:
A61B 8/08 (2006.01)

(21) Application number: **10159227.7**

(22) Date of filing: **07.04.2010**

(84) Designated Contracting States:
AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO SE SI SK SM TR
Designated Extension States:
AL BA ME RS

(72) Inventor: **Lee, Kwang Hee**
135-851, Seoul (KR)

(74) Representative: **Schmid, Wolfgang**
Lorenz & Kollegen
Patentanwälte Partnerschaftsgesellschaft
Alte Ulmer Strasse 2
89522 Heidenheim (DE)

(30) Priority: **30.07.2009 KR 20090069867**

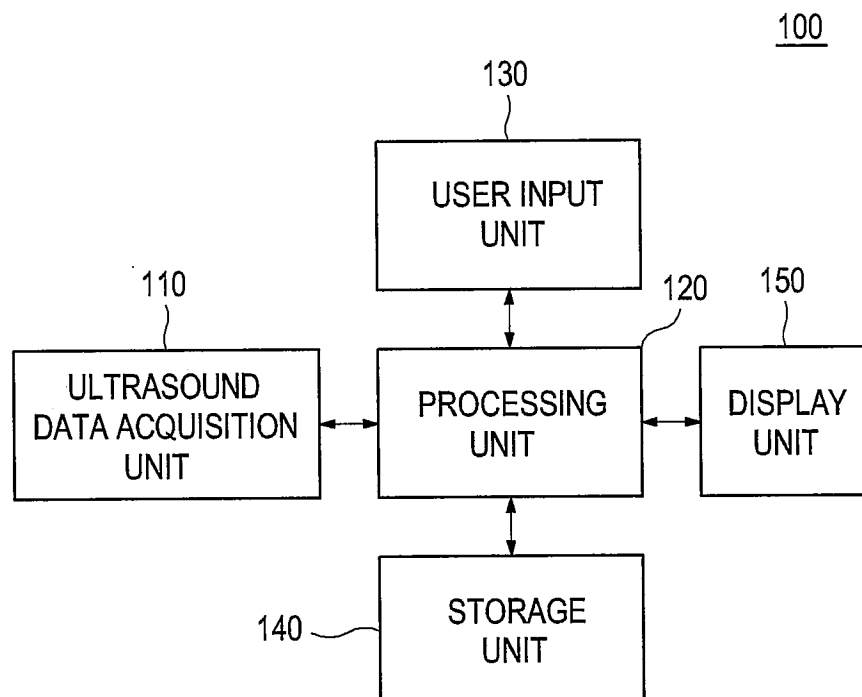
(71) Applicant: **MEDISON CO., LTD.**
Kangwon-do 250-870 (KR)

(54) **Setting a Sagittal View in an Ultrasound System**

(57) Embodiments for providing a plurality of slice images are disclosed. In one embodiment, by way of non-limiting example, an ultrasound system comprises: an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object

to thereby output ultrasound data; and a processing unit configured to form volume data based on the ultrasound data, set a reference slice, a reference point and a window on the volume data based on input information of a user and set a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus on the volume data.

FIG. 1



EP 2 281 509 A1

Description

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] The present application claims priority from Korean Patent Application No. 10-2009-0069867 filed on July 30, 2009, the entire subject matter of which is incorporated herein by reference.

TECHNICAL FIELD

[0002] The present disclosure generally relates to ultrasound systems, and more particularly to setting a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus in an ultrasound system.

BACKGROUND

[0003] An ultrasound system has become an important and popular diagnostic tool since it has a wide range of applications. Specifically, due to its non-invasive and non-destructive nature, the ultrasound system has been extensively used in the medical profession. Modern high-performance ultrasound systems and techniques are commonly used to produce two or three-dimensional diagnostic images of internal features of an object (e.g., human organs).

[0004] The ultrasound system transmits and receives ultrasound signals to and from a target object (e.g., a fetus) to thereby form a 2D (two-dimensional) ultrasound image of the fetus. Also, when a user sets a sagittal view for measuring a thickness of a nuchal translucency (NT) of the fetus based on the 2D ultrasound image, the ultrasound system may check a chromosomal abnormality of the fetus by measuring the thickness of the NT based on the sagittal view. However, it may be difficult to precisely set the sagittal view on volume data. Thus, there is a problem in that the thickness of the NT may not be measured exactly.

SUMMARY

[0005] Embodiments for providing a plurality of slice images in an ultrasound system are disclosed herein. In one embodiment, by way of non-limiting example, an ultrasound system comprises: an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object to thereby output ultrasound data; and a processing unit configured to form volume data based on the ultrasound data, the processing unit being configured to set a reference slice, a reference point and a window on the volume data based on input information of a user, and the processing unit being further configured to set a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus on the volume data.

[0006] In another embodiment, there is provided a method of setting a sagittal view, comprising: a) trans-

mitting and receiving ultrasound signals to and from a target object to thereby output ultrasound data; b) forming volume data based on the ultrasound data; c) setting a reference slice, a reference point and a window on the volume data based on input information of a user; and d) setting a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus on the volume data based on the reference slice, the reference point and the window.

[0007] The Summary is provided to introduce a selection of concepts in a simplified form that are further described below in the Detailed Description. This Summary is not intended to identify key or essential features of the claimed subject matter, nor is it intended to be used in determining the scope of the claimed subject matter.

BRIEF DESCRIPTION OF THE DRAWINGS

[0008]

Figure 1 is a block diagram showing an illustrative embodiment of an ultrasound system.

Figure 2 is a block diagram showing an illustrative embodiment of an ultrasound data acquisition unit.

Figure 3 is a schematic diagram showing an example of acquiring ultrasound data corresponding to a plurality of frames.

Figure 4 is a block diagram showing an illustrative embodiment of a processing unit.

Figure 5 is a schematic diagram showing an example of volume data.

Figure 6 is a schematic diagram showing an example of a reference slice, a reference point and a window set on the volume data.

Figure 7 is a schematic diagram showing an example of an ultrasound image, the reference point and the window.

DETAILED DESCRIPTION

40

[0009] A detailed description may be provided with reference to the accompanying drawings. One of ordinary skill in the art may realize that the following description is illustrative only and is not in any way limiting. Other embodiments of the present invention may readily suggest themselves to such skilled persons having the benefit of this disclosure.

45

[0010] Referring to Figure 1, an ultrasound system 100 in accordance with an illustrative embodiment is shown. As depicted therein, the ultrasound system 100 may include an ultrasound data acquisition unit 110. The ultrasound data acquisition unit 110 may be operable to transmit and receive ultrasound signals to and from a target object (e.g., a fetus) to thereby output ultrasound data. The ultrasound data acquisition unit 110 may include a transmit (Tx) signal generating section 111, as shown in Figure 2.

55

[0011] Figure 2 is a block diagram showing an illustrative

tive embodiment of the ultrasound data acquisition unit 110. Referring to Figure 2, the Tx signal generating section 111 may be operable to generate Tx signals. The Tx signal generating section 111 may generate the Tx signals at every predetermined time to thereby form a plurality of Tx signals for obtaining each of frames F_i ($1 \leq i \leq N$) representing the target object, as shown in Figure 3.

[0012] Figure 3 is a schematic diagram showing an example of acquiring ultrasound data corresponding to a plurality of frames F_i ($1 \leq i \leq N$). The plurality of frames F_i ($1 \leq i \leq N$) may represent sectional planes of the target object (not shown).

[0013] Referring back to Figure 2, the ultrasound data acquisition unit 110 may further include an ultrasound probe 112 containing a plurality of elements for reciprocally converting between ultrasound signals and electrical signals. The ultrasound probe 112 may be operable to transmit ultrasound signals into the target object in response to the Tx signals. The ultrasound probe 112 may further receive echo signals reflected from the target object to thereby output received signals. The received signals may be analog signals. The ultrasound probe 112 may include a three-dimensional mechanical probe, a two-dimensional array probe or the like. However, the ultrasound probe 112 may not be limited thereto.

[0014] The ultrasound data acquisition unit 110 may further include a beam former 113. The beam former 113 may be operable to convert the received signals into digital signals. The beam former 113 may further apply delays to the digital signals in consideration of distances between the elements and focal points to thereby output digital receive-focused signals.

[0015] The ultrasound data acquisition unit 110 may further include an ultrasound data forming section 114. The ultrasound data forming section 114 may be operable to form ultrasound data corresponding to each of the frames F_i ($1 \leq i \leq N$) based on the digital receive-focused signals. The ultrasound data forming unit 114 may be further operable to perform various signal processing (e.g., gain adjustment) to the digital receive-focused signals.

[0016] Referring back to Figure 1, the ultrasound system 100 may further include a processing unit 120, which may be coupled to the ultrasound data acquisition unit 110. Figure 4 is a block diagram showing an illustrative embodiment of the processing unit 120. Referring to Figure 4, the processing unit 120 may include a volume data forming section 121, a reference slice setting section 122, a reference point setting section 123, a window setting section 124, a sagittal view setting section 125, an image forming section 126 and a nuchal translucency (NT) thickness measuring section 127.

[0017] The volume data forming section 121 may synthesize the ultrasound data corresponding to the frames F_i ($1 \leq i \leq N$) to thereby form volume data including the frames F_i ($1 \leq i \leq N$), as shown in Figure 5. Figure 5 is a schematic diagram showing an example of volume data 210. The volume data 210 may include a plurality of vox-

els having brightness values. In Figure 5, reference numerals 221 to 223 represent an A plane, a B plane and a C plane. The A plane 221, the B plane 222 and the C plane 223 may be mutually orthogonal. Also, in Figure 5, the axial direction may be a Tx direction of the ultrasound signals, the lateral direction may be a longitudinal direction of the transducer and the elevation direction may be a swing direction of the transducer, i.e., a depth direction of a 3D (three-dimensional) ultrasound image.

[0018] The reference slice setting section 122 may set a reference slice 230 on the volume data 210 based on input information provided from a user input unit 130, as shown in Figure 6. Figure 6 is a schematic diagram showing an example of a reference slice 230, a reference point 240 and a window 250, which are set on the volume data 210. In one embodiment, the reference slice 230 in Figure 6 may be the B plane 222 as shown in Figure 5. However, the reference slice 230 may not be limited thereto.

[0019] Referring back to Figure 4, the reference point setting section 123 may set a reference point 240 on the reference slice 230 based on the input information provided from the user input unit 130, as shown in Figure 6.

[0020] The window setting section 124 may be operable to set a window 250 to encompass the reference point 240 on the reference slice 230 as shown in Figure 6. In one embodiment, the window 250 may be a rectangular window having a predetermined size. However, the window 250 may not be limited thereto.

[0021] The sagittal view setting section 125 may set a sagittal view on the volume data 210 based on the reference slice 230, the reference point 240 and the window 250. The sagittal view may be a slice for measuring a thickness of the NT of a fetus. However, the sagittal view may not be limited thereto.

[0022] In one embodiment, the sagittal view setting section 125 may be operable to detect brightness values of pixels within the window 250 set on the reference slice 230. The sagittal view setting section 125 may be further operable to calculate a reference value based on the brightness values. The reference value may be a mean value of the brightness values or a sum value of the brightness values. However, the reference value may not be limited thereto. The sagittal view setting section 125 may further move the reference slice 230, the reference point 240 and the window 250 to the lateral direction by predetermined intervals within the volume data 210 to thereby calculate the reference values. Positions of the moved reference slice 230 and the calculated reference values may be stored in a storage unit 140. The sagittal view setting section 125 may be further operable to compare the calculated reference values to thereby detect a maximum reference value. The sagittal view setting section 125 may also move the reference slice 230, the reference point 240 and the window 250 to a position corresponding to the maximum reference value. The sagittal view setting section 125 may further rotate the reference slice 230 and the window 250 to the axial direction by predetermined angles with respect to the reference point 240 to

thereby calculate the reference values. Positions of the rotated reference slice 230 and the calculated reference values may be stored in a storage unit 140. The sagittal view setting section 125 may be further operable to compare the calculated reference values to thereby detect a maximum reference value. The sagittal view setting section 125 may be further operable to rotate the reference slice 230 and the window 250 to a position corresponding to the maximum reference value. The sagittal view setting section 125 may rotate the reference slice 230 and the window 250 to the elevation direction by predetermined angles with respect to the reference point 240 to thereby calculate the reference values. The sagittal view setting section 125 may be further operable to compare the calculated reference values to thereby detect a maximum reference value. The sagittal view setting section 125 may rotate the reference slice 230 and the window 250 to a position corresponding to the maximum reference value. Thus, the sagittal view setting section 125 may set the sagittal view on the volume data 210 based on the reference slice 230. The sagittal view may include the reference point 240 and the window 250. For example, the sagittal view setting section 125 may be operable to set the reference slice 230 as the sagittal view on the volume data 210.

[0023] While the sagittal view setting section 125 may set the mean value of the brightness values or the sum value of the brightness values as the reference value in the foregoing embodiment, the sagittal view setting section 125 may further calculate a gradient magnitude and an orientation for each of the pixels within the window 250, form a histogram between the gradient magnitudes and the orientations, detect a peak in the histogram and set the detected peak as the reference value.

[0024] Also, while the sagittal view setting section 125 may move the reference slice 230 to the lateral direction and rotate the reference slice 230 to the axial direction and the elevation direction in the foregoing embodiment, the sagittal view setting section 125 may further move and rotate the reference slice 230 to arbitrary directions.

[0025] Further, while the sagittal view setting section 125 may rotate the reference slice 230 with respect to the reference point 240 in the foregoing embodiment, the sagittal view setting section 125 may further rotate the volume data 210 with respect to the reference point 240.

[0026] The image forming section 126 may form a 2D (two-dimensional) ultrasound image 310 corresponding to the sagittal view based on the volume data 210 as shown in Figure 7. Figure 7 is a schematic diagram showing an example of the ultrasound image 310, the reference point 240 and the window 250. The 2D ultrasound image 310 may be a brightness mode image. The image forming section 126 may be further operable to render the volume data 210 to thereby form a 3D (three-dimensional) ultrasound image (not shown).

[0027] The NT thickness measuring section 127 may be configured to set the reference point 240 and the window 250 on the 2D ultrasound image 310 based on the

sagittal view. The NT thickness measuring section 127 may be further configured to detect a contour of the NT 320 within the window 250. The contour may be detected by using an edge mask such as Sobel, Prewitt, Robert, Canny mask or the like. The contour may be detected based on the differences between eigenvalues using structure tensors. The NT thickness measuring section 127 may measure a thickness of the NT based on the detected contour to thereby output measurement information. The methods of measuring the thickness of the NT based on the contour are well known in the art. Thus, they have not been described in detail so as not to unnecessarily obscure the present invention.

[0028] Referring back to Figure 1, the ultrasound system 100 may further include the user input unit 130. The user input unit 130 may be operable to receive input information of a user. In one embodiment, the input information may include first input information for setting the reference slice on the volume data and second input information for setting the reference point on the NT of the reference slice. The user input unit 130 may include a control panel, a mouse, a keyboard or the like. However, the user input unit 130 may not be limited thereto.

[0029] The ultrasound system 100 may further include the storage unit 140. The storage unit 140 may store the positions of the reference slice 230 and the reference values. The storage unit 140 may further store the volume data 210.

[0030] The ultrasound system may further include a display unit 150. The display unit 150 may display the 2D ultrasound image, the 3D ultrasound image and the measurement information.

[0031] Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the spirit and scope of the principles of this disclosure. More particularly, numerous variations and modifications are possible in the component parts and/or arrangements of the subject combination arrangement within the scope of the disclosure, the drawings and the appended claims. In addition to variations and modifications in the component parts and/or arrangements, alternative uses will also be apparent to those skilled in the art.

Claims

1. An ultrasound system, comprising:

an ultrasound data acquisition unit configured to transmit and receive ultrasound signals to and from a target object to thereby output ultrasound data; and
a processing unit placed in communication with the ultrasound data acquisition unit and being configured to form volume data based on the

- ultrasound data, set a reference slice, a reference point and a window on the volume data based on input information of a user, and set a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus on the volume data.
- 5
2. The ultrasound system of Claim 1, further comprising a user input unit placed in communication with the processing unit and being configured to receive the input information.
- 10
3. The ultrasound system of Claim 1, wherein the input information comprises:
- 15
- a first input information for setting the reference slice on the volume data; and
a second input information for setting the reference point on the reference slice.
- 20
4. The ultrasound system of Claim 1, wherein the processing unit comprises:
- 25
- a volume data forming section configured to form the volume data based on the ultrasound data;
a reference slice setting section configured to set the reference slice on the volume data based on the input information;
a reference point setting section configured to set the reference point on the reference slice based on the input information;
a window setting section configured to set the window to encompass the reference point on the reference slice; and
a sagittal view setting section configured to set the sagittal view on the volume data based on the reference slice, the reference point and the window.
- 30
- 35
- 40
5. The ultrasound system of Claim 4, wherein the sagittal view setting section is configured to:
- 45
- move the reference slice, the reference point and the window to a first direction by predetermined intervals to thereby calculate first reference values;
detect a maximum first reference value from the first reference values;
move the reference slice, the reference point and the window to a position corresponding to the maximum first reference value;
rotate the reference slice and the window by predetermined angles with respect to the reference point to thereby calculate second reference values;
50
- 55
- detect a maximum second reference value from the second reference values; and
- rotate the reference slice and the window to a position corresponding to the maximum second reference value to thereby set the sagittal view on the volume data.
6. The ultrasound system of Claim 5, wherein the sagittal view setting section is configured to detect brightness values of pixels within the window, calculate a mean value of the brightness values and set the mean value as the first or second reference value.
7. The ultrasound system of Claim 5, wherein the sagittal view setting section is configured to detect brightness values of pixels within the window, calculate a sum value of the brightness values and set the sum value as the first or second reference value.
8. The ultrasound system of Claim 5, wherein the sagittal view setting section is configured to calculate a gradient magnitude and an orientation for pixels within the window, form a histogram between the gradient magnitude and the orientation, detect a peak in the histogram and set the detected peak as the first or second reference value.
9. The ultrasound system of Claim 4, wherein the processing unit further comprises:
- an image forming section configured to form an ultrasound image corresponding to the sagittal view based on the volume data; and
a NT thickness measuring section configured to detect a contour of the NT within the window at the ultrasound image and measure thickness of the NT based on the detected contour.
10. A method of setting a sagittal view, comprising:
- a) transmitting and receiving ultrasound signals to and from a target object to thereby output ultrasound data;
b) forming volume data based on the ultrasound data;
c) setting a reference slice, a reference point and a window on the volume data based on input information of a user; and
d) setting a sagittal view for measuring a thickness of a nuchal translucency (NT) of a fetus on the volume data based on the reference slice, the reference point and the window.
11. The method of Claim 10, wherein the input information comprises:
- first input information for setting the reference slice on the volume data; and
second input information for setting the refer-

ence point on the reference slice.

12. The method of Claim 10, wherein the step c) comprises:

5

setting the reference slice on the volume data based on the input information;
 setting the reference point on the reference slice based on the input information; and
 setting the window to encompass the reference point on the reference slice.

10

13. The method of Claim 10, wherein the step d) comprises:

15

d1) moving the reference slice, the reference point and the window to a first direction by predetermined intervals to thereby calculate first reference value;
 d2) detecting a maximum first reference value from the first reference values;
 d3) moving the reference slice, the reference point and the window to a position corresponding to the maximum first reference value;
 d4) rotating the reference slice and the window to a second direction by predetermined angles with respect to the reference point to thereby calculate second reference value;
 d5) detecting a maximum second reference value from the second reference values; and
 d6) rotating the reference slice and the window to a position corresponding to the maximum second reference value to thereby set the sagittal view on the volume data.

20

25

30

35

14. The method of Claim 13, wherein the first or second reference value is set based on one of a mean value of brightness values of pixels within the window, a sum value of brightness values of pixels within the window and a peak in a histogram between a gradient magnitude and an orientation for each of pixels within the window.

40

15. The method of Claim 10, further comprising the steps of:

45

e) forming an ultrasound image corresponding to the sagittal view based on the volume data;
 f) detecting a contour of the NT within the window at the ultrasound image; and
 g) measuring thickness of the NT based on the detected contour.

50

55

FIG. 1

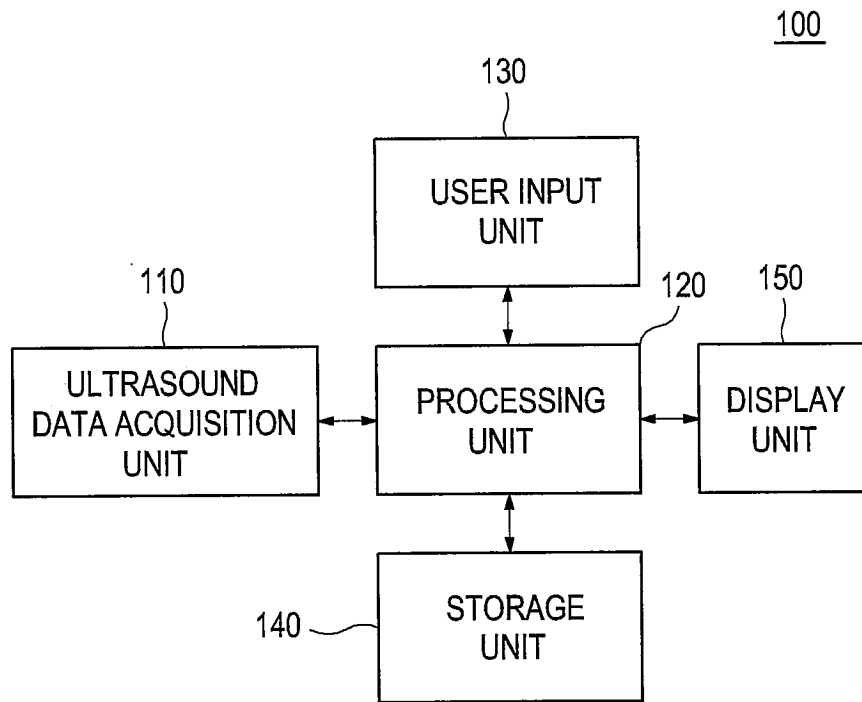


FIG. 2

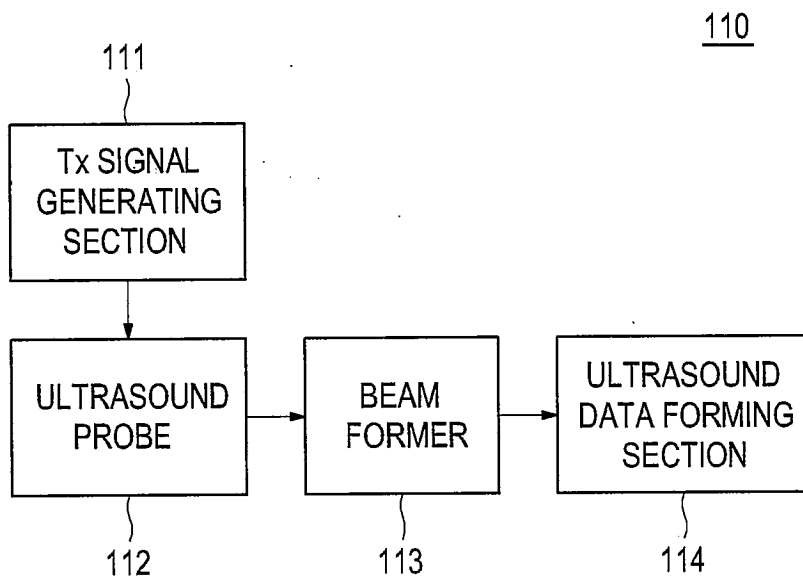


FIG. 3

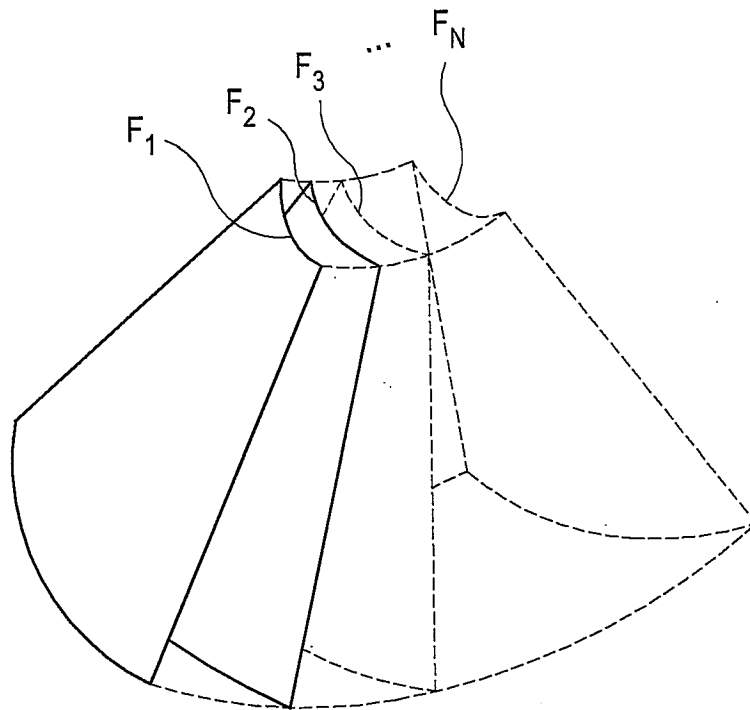


FIG. 4

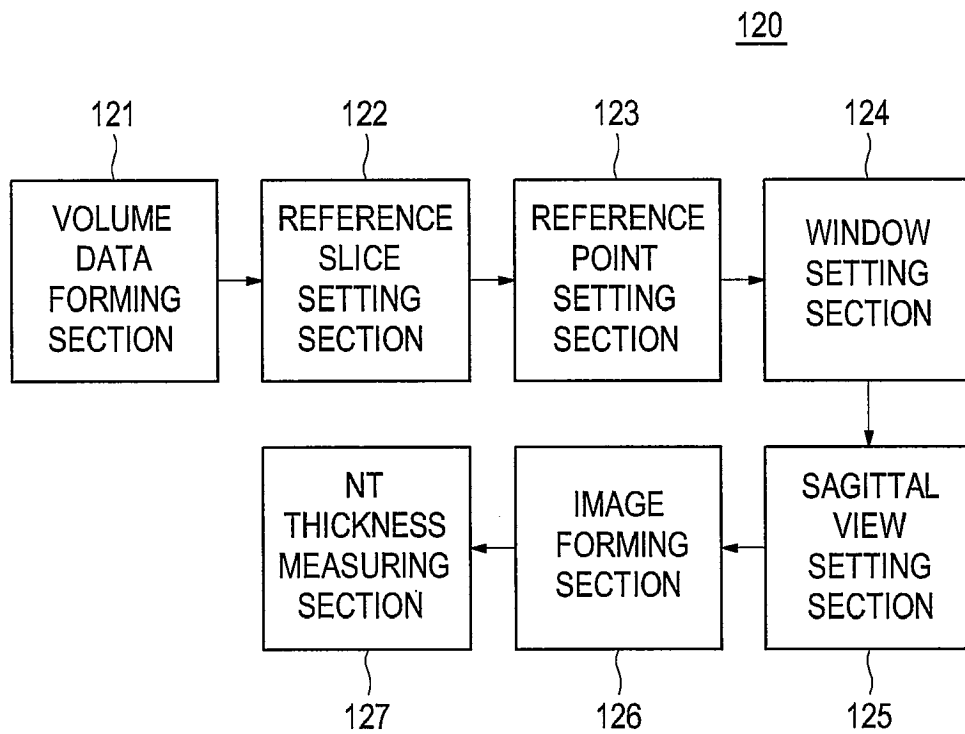


FIG. 5

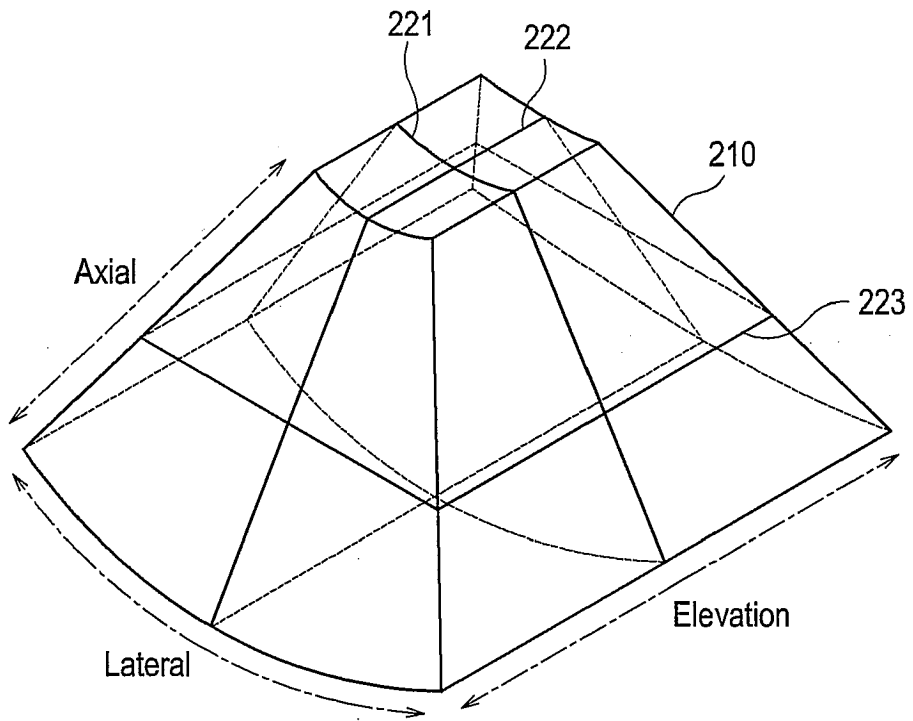


FIG. 6

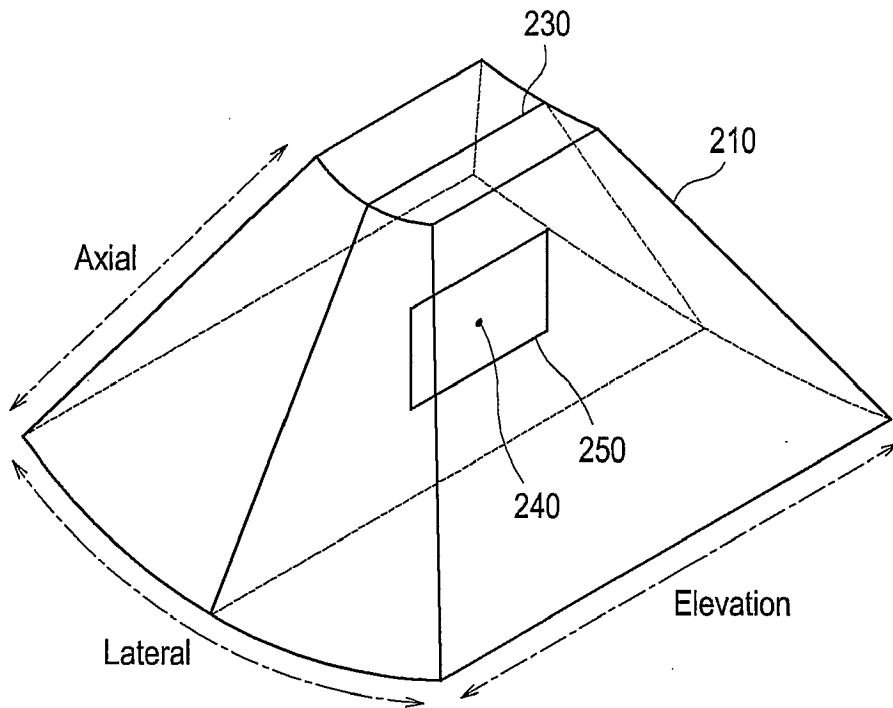
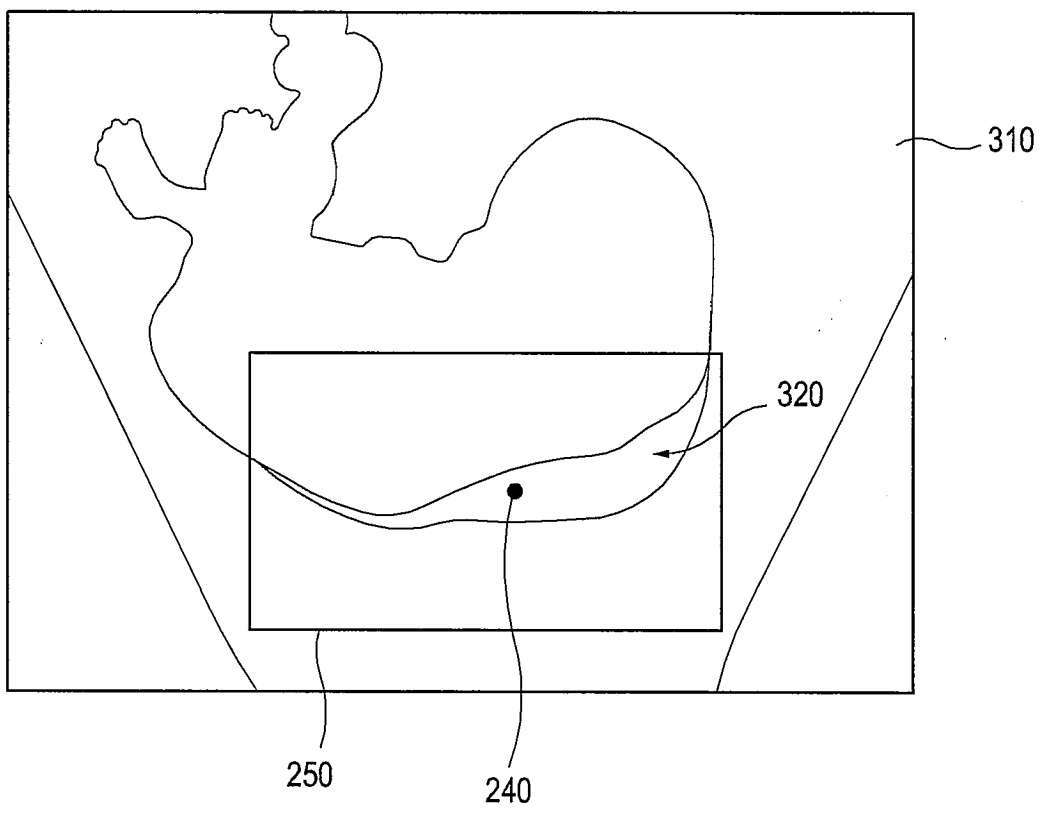


FIG. 7





EUROPEAN SEARCH REPORT

Application Number
EP 10 15 9227

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	EP 1 923 839 A1 (ALOKA CO LTD [JP]) 21 May 2008 (2008-05-21)	1-4, 9-12,15	INV. A61B8/08
Y	* paragraphs [0020] - [0021] * * paragraph [0028] - paragraph [0036] * * figures 2-12 *	5-8,13, 14	
X	US 6 102 861 A (AVILA RICARDO SCOTT [US] ET AL) 15 August 2000 (2000-08-15)	1-4, 9-12,15	TECHNICAL FIELDS SEARCHED (IPC)
A	* column 2, line 19 - line 33 * * column 6, line 24 - column 8, line 44 *	5-8,13, 14	
X	Andrew D. Hull, Gina James, Dolores H. Pretorius: "Detection of Jarcho-Levin syndrome at 12 weeks' gestation by nuchal translucency screening and three dimensional ultrasound", Prenatal Diagnosis, vol. 21 11 May 2001 (2001-05-11), pages 390-394, XP002612156, Retrieved from the Internet: URL:http://onlinelibrary.wiley.com/doi/10. 1002/pd.67/abstract [retrieved on 2010-11-30] * * page 390 right col. * * Figure 3 * *	1-4, 9-12,15	A61B G06T G06F G01S
Y	EP 1 470 784 A2 (ALOKA CO LTD [JP]) 27 October 2004 (2004-10-27)	5-8,13, 14	
A	* paragraph [0037] - paragraph [0045] * ----- -/--	1,10	
The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 7 December 2010	Examiner Dydenko, Igor
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

6
EPO FORM 1503 03.02 (P04/C01)



EUROPEAN SEARCH REPORT

 Application Number
 EP 10 15 9227

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
A	A. S. Lev-Toaff, S. Ozhan, D. Pretorius, G. Bega, A. B. Kurtz, K. Kuhlman: "Three-dimensional multiplanar ultrasound for fetal gender assignment: value of the mid-sagittal plane", Ultrasound Obstet Gynecol, vol. 16 2000, pages 345-350, XP002612157, Retrieved from the Internet: URL:http://onlinelibrary.wiley.com/doi/10.1046/j.1469-0705.2000.00179.x/abstract [retrieved on 2010-11-30] * the whole document *	1,10	
A	Hui-Xiong Xu, Qing-Ping Zhang, Ming-De Lu, Xian-Tao Xiao: "Comparison of two-dimensional and three-dimensional sonography in evaluating fetal malformations", Journal of Clinical Ultrasound, vol. 30, no. 9 25 October 2002 (2002-10-25), pages 515-525, XP002612158, Retrieved from the Internet: URL:http://onlinelibrary.wiley.com/doi/10.1002/jcu.10109/abstract [retrieved on 2010-11-20] * page 516 - page 518 *	1,10	TECHNICAL FIELDS SEARCHED (IPC)
A	US 2007/081705 A1 (CARNEIRO GUSTAVO [US] ET AL) 12 April 2007 (2007-04-12) * paragraph [0039] - paragraph [0044] * * paragraph [0057] - paragraph [0066] * * figure 2 *	1,4-8, 10,13,14	
The present search report has been drawn up for all claims			
6	Place of search The Hague	Date of completion of the search 7 December 2010	Examiner Dydenko, Igor
CATEGORY OF CITED DOCUMENTS X: particularly relevant if taken alone Y: particularly relevant if combined with another document of the same category A: technological background O: non-written disclosure P: intermediate document		T: theory or principle underlying the invention E: earlier patent document, but published on, or after the filing date D: document cited in the application L: document cited for other reasons &: member of the same patent family, corresponding document	

EPO FORM 1503 03-82 (P04C01)



EUROPEAN SEARCH REPORT

Application Number
EP 10 15 9227

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
A	WO 00/58754 A1 (GEN ELECTRIC [US]) 5 October 2000 (2000-10-05) * page 8 - page 13 * * figures 3, 4, 5, 8, 10 * -----	1,10	
A	US 2009/074280 A1 (LU XIAO GUANG [US] ET AL) 19 March 2009 (2009-03-19) * the whole document * -----	1,10	
A	YU-BU LEE ET AL: "Automated Ultrasonic Measurement of Fetal Nuchal Translucency Using Dynamic Programming", 1 January 2006 (2006-01-01), PROGRESS IN PATTERN RECOGNITION, IMAGE ANALYSIS AND APPLICATIONS LECTURE NOTES IN COMPUTER SCIENCE;;LNCS, SPRINGER, BERLIN, DE, PAGE(S) 157 - 167, XP019045806, ISBN: 978-3-540-46556-0 * the whole document * -----	4-8,10,13,14	
			TECHNICAL FIELDS SEARCHED (IPC)
The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 7 December 2010	Examiner Dydenko, Igor
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

6
EPO FORM 1503 03.82 (P04C01)

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 10 15 9227

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report. The members are as contained in the European Patent Office EDP file on The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

07-12-2010

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
EP 1923839 A1	21-05-2008	US 2008114244 A1	15-05-2008
US 6102861 A	15-08-2000	EP 1046929 A2	25-10-2000
		JP 4536869 B2	01-09-2010
		JP 2000325346 A	28-11-2000
EP 1470784 A2	27-10-2004	JP 3802508 B2	26-07-2006
		JP 2004313651 A	11-11-2004
		US 2004210138 A1	21-10-2004
US 2007081705 A1	12-04-2007	NONE	
WO 0058754 A1	05-10-2000	CN 1297534 A	30-05-2001
		EP 1084424 A1	21-03-2001
		US 6413219 B1	02-07-2002
US 2009074280 A1	19-03-2009	DE 102008046861 A1	14-05-2009
		JP 2009072593 A	09-04-2009
		KR 20090029673 A	23-03-2009

REFERENCES CITED IN THE DESCRIPTION

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

Patent documents cited in the description

- KR 1020090069867 [0001]

专利名称(译)	在超声系统中设置矢状面视图		
公开(公告)号	EP2281509A1	公开(公告)日	2011-02-09
申请号	EP2010159227	申请日	2010-04-07
申请(专利权)人(译)	MEDISON CO. , LTD.		
当前申请(专利权)人(译)	MEDISON CO. , LTD.		
[标]发明人	LEE KWANG HEE		
发明人	LEE, KWANG HEE		
IPC分类号	A61B8/08		
CPC分类号	A61B8/0858 A61B8/467 A61B8/469 A61B8/483 A61B8/523		
代理机构(译)	SCHMID , WOLFGANG		
优先权	1020090069867 2009-07-30 KR		
其他公开文献	EP2281509B1		
外部链接	Espacenet		

摘要(译)

公开了用于提供多个切片图像的实施例。在一个实施例中，作为非限制性示例，超声系统包括：超声数据获取单元，被配置为向目标对象发送超声信号和从目标对象接收超声信号，从而输出超声数据；处理单元，被配置为基于超声数据形成体数据，基于用户的输入信息在体数据上设置参考切片，参考点和窗口，并设置用于测量颈部半透明的厚度的矢状视图（NT）体积数据上的胎儿。

FIG. 1

