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(54) **Ultrasound system and method for adaptively performing clutter filtering**

Ultraschallsystem und -Verfahren für adaptive Clutter Filterung

Système à ultrasons et procédé à filtrage adaptif d'échos parasites

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Description

TECHNICAL FIELD

[0001] The present disclosure generally relates to ultrasound systems, and more particularly to an ultrasound system and method for adaptively performing clutter filtering.

BACKGROUND

[0002] An ultrasound system has become an important and popular diagnostic tool since it has a wide range of applications. Specifically, due to its non-invasive and non-destructive nature, the ultrasound system has been extensively used in the medical profession. Modern high-performance ultrasound systems and techniques are commonly used to produce two or three-dimensional diagnostic images of internal features of an object (e.g., human organs).

[0003] As is known in the art, the ultrasound system may provide ultrasound images of various modes including a brightness mode (B mode) image representing reflection coefficients of the ultrasound signals reflected from the target object with a 2D (two-dimensional) image, a Doppler mode (D mode) image representing speed of a moving object with spectral Doppler by using a Doppler effect, a color Doppler mode (C mode) image representing speed of a moving object with colors by using the Doppler effect, and an elastic mode (E mode) image representing mechanical characteristics of tissues object before and after applying a pressure thereto. In particular, the ultrasound system may transmit and receive ultrasound signals to and from the target object to thereby form Doppler signals. The ultrasound system may further form the C mode image representing the speed of the moving object with the colors based on the Doppler signals.

[0004] The Doppler signal may include a low frequency signal (so-called clutter signal) due to the motion of a tissue such as a blood vessel wall, a cardiac wall, a heart valve and the like. The clutter signal may have amplitude, which is over 100 times than that of a pure Doppler signal indicative of velocities of the blood flow. The clutter signal may be an obstacle to accurately detect speed of the blood flow. Thus, it is required to remove the clutter signal from the Doppler signal to accurately detect the speed of the blood flow.

[0005] A clutter downmixing has been used to remove the clutter signals. The downmixing may be carried out by estimating a center frequency of the clutter signals and by performing the downmixing (frequency shift), which shifts the center frequency of the clutter signals to 0, upon the Doppler signals based on the center frequency. Thereafter, the downmixed clutter signals, which are shifted to a DC component, may be removed by using the conventional clutter filtering methods.

[0006] The clutter signals may have a speed compo-

nent when a tissue exists within the target object, wherein the tissue moves at a constant speed. However, the clutter signals may have two speed components when tissues exist within the target object, wherein the tissues comprise a tissue that does not move within the target object and a tissue that moves at the constant speed. Thus, it may be difficult to accurately perform the downmixing, which shifts the center of the clutter signals to 0, by using the conventional clutter downmixing methods. Further, the clutter signals may have a plurality of speed components when a tissue exists within the target object, wherein the tissue moves at a lower speed than a predetermined speed (e.g., minimum speed of blood flow). As such, it may be difficult to accurately perform the downmixing, which shifts the center of the clutter signals to 0, by using the conventional clutter downmixing methods.

[0007] XP011437503 "Clutter rejection filters in color flow imaging: a theoretical approach" by Hans Torp refers to a general class of linear clutter rejection filters covering the commonly used filter types including FIR/IIR filters with linear initialization as well as regression filters, where the clutter component is estimated by least square fitting.

[0008] XP031000887 "A Novel Clutter Rejection Filters Applied to Wideband Blood Flow Velocity Estimation" by Xiaotao Wang et al. refers to color flow imaging in the diagnosis of many vascular diseases, especially cardiovascular disease. This document proposes a novel scheme to clutter rejection using parameter estimation methods based on the two-dimensional correlation function model and the conventional down mixing.

[0009] EP 0 481 691 A1 discloses an ultrasonic diagnostic system for measuring fluid flow velocities through Doppler techniques which eliminates the effects of tissue motion from fluid flow velocity information. Doppler information signals are discriminated to determine the presence of signal components resulting from moving tissue, which signal components are located at frequencies of a Doppler spectrum other than the predetermined frequency location of stationary tissue signals.

[0010] US 5,226,420 refers to an ultrasonic color flow information processing system receiving ultrasonic Doppler information signals which are used to develop a map of color flow display information of fluid flow. The system processes the Doppler information through autoregressive spectral estimation, which models the Doppler information as the output of an all-pole filter driven by white noise.

[0011] In EP 1 548 462 A1 an ultrasonic Doppler diagnostic equipment is described which includes a Doppler signal detection device which executes a filtering process for a plurality of reception signals obtained in time series at unequal intervals from a predetermined position within a patient by a transmission/reception device, thereby to detect Doppler signals based on a mobile object.

[0012] XP011180988 "Arc tangent Demodulation With DC Offset Compensation in Quadrature Doppler Radar Receiver Systems" by Byung-Kwon Park et al. refers to

direct-conversion microwave Doppler radar which can be used to detect cardiopulmonary activity at a distance.

SUMMARY

[0013] According to the present disclosure, there is disclosed an ultrasound system and method for adaptively performing a clutter filtering upon a plurality of ultrasound data in consideration of the speed of tissues (e.g., blood vessel wall) existing within a target object.

[0014] In one embodiment, an ultrasound system comprises the features of claim 1.

[0015] In another embodiment, there is provided a method of performing a clutter filtering, comprising the features of claim 9.

BRIEF DESCRIPTION OF THE DRAWINGS

[0016]

Figure 1 is a block diagram showing an illustrative embodiment of an ultrasound system.

Figure 2 is a schematic diagram showing an example of a brightness mode image and a region of interest (ROI).

Figure 3 is a block diagram showing an illustrative embodiment of an ultrasound data acquisition unit.

Figure 4 is a block diagram showing an illustrative embodiment of a processing unit.

Figure 5 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to a tissue on the complex plane, wherein the tissue moves at constant speed within the target object.

Figure 6 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to tissues on the complex plane, wherein the tissues comprise a tissue that does not move within the target object and a tissue that moves at constant speed within the target object.

Figure 7 is a schematic diagram showing an example of locating a plurality of ultrasound data corresponding to a tissue on the complex plane, wherein the tissue moves at a lower speed than a predetermined speed within the target object.

Figure 8 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to the tissue and the blood flow on the complex plane, wherein the tissue moves at the constant speed within the target object.

Figure 9 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to the tissues and the blood flow on the complex plane, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed.

Figure 10 is a schematic diagram showing an example of locating the plurality ultrasound data corre-

sponding to the tissue and the blood flow, wherein the tissue moves at a low speed within the target object.

Figure 11 is a schematic diagram showing an example of performing a circle fitting upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the constant speed within the target object.

Figure 12 is a schematic diagram showing an example of performing the circle fitting upon the plurality of ultrasound data corresponding to the tissues and the blood flow, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed within the target object.

Figure 13 is a schematic diagram showing an example of performing the circle fitting upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the low speed within the target object.

Figure 14 is a schematic diagram showing an example of performing a downmixing upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the constant speed.

Figure 15 is a schematic diagram showing an example of performing the downmixing upon the plurality of ultrasound data corresponding to the tissues and the blood flow, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed within the target object.

Figure 16 is a schematic diagram showing an example of performing the downmixing upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the low speed within the target object.

DETAILED DESCRIPTION

[0017] A detailed description is provided with reference to the accompanying drawings. One of ordinary skill in the art may realize that the following description is illustrative only and is not in any way limiting. Other embodiments of the present invention may readily suggest themselves to such skilled persons having the benefit of this disclosure. As used herein, the term "Doppler mode" comprises a color Doppler mode.

[0018] Figure 1 is a block diagram showing an illustrative embodiment of an ultrasound system. Referring to Figure 1, the ultrasound system 100 may include a user input unit 110, an ultrasound data acquisition unit 120, a processing unit 130, a storage unit 140 and a display unit 150.

[0019] The user input unit 110 is configured to receive input information from a user. In one embodiment, the input information may include position and size information of a region of interest (ROI) 220, which may be set

on a brightness mode image 210, as shown in Figure 2. The ROI 220 may include a color box. Also, at least one of scan-lines may be comprised within the ROI 220. The user input unit 110 may include a control panel, a keyboard, a mouse and the like.

[0020] The ultrasound data acquisition unit 120 is configured to transmit and receive ultrasound signals to and from a target object to thereby acquire ultrasound data corresponding to the ROI (i.e., color box). The ultrasound data acquisition unit 120 will be described with reference to Figure 3.

[0021] Figure 3 is a block diagram showing an illustrative embodiment of the ultrasound data acquisition unit. Referring to Figure 3, the ultrasound data acquisition unit 120 includes a transmit (Tx) signal generating section 121, an ultrasound probe 122 comprising a plurality of transducer elements (not shown), a beam former 123 and an ultrasound data forming section 124.

[0022] The Tx signal generating section 121 is configured to generate Tx signals in consideration of focal points and positions of the transducer elements. The Tx signals may be signals for acquiring a Doppler mode image. The Tx signal generating section 121 may generate a plurality of Tx signals based on a predetermined ensemble number. The ensemble number represents the number of transmitting and receiving the ultrasound signals in order to acquire Doppler signals corresponding to a scan-line.

[0023] The ultrasound probe 122 is configured to convert the Tx signals provided from the Tx signal generating section 121 into the ultrasound signals. The ultrasound probe 122 may further transmit the ultrasound signals into the target object, and receive ultrasound echo signals reflected from the target object to thereby form received signals, which may be analog signals. The ultrasound probe 122 may include a linear array probe, a convex array probe and the like.

[0024] The beam former 123 is configured to convert the received signals provided from the ultrasound probe 122 into digital signals. The beam former 123 may further receive-focus the digital signals in consideration of the focal points and the positions of the transducer elements to thereby form receive-focused signals.

[0025] The ultrasound data forming section 124 is configured to form the ultrasound data based on the receive-focused signals provided from the beam former 123. According to the invention, the ultrasound data may include IQ (in-phase/quadrature) data (i.e., ensemble data) for acquiring the Doppler signals. The ultrasound data forming section 124 forms a plurality of ultrasound data corresponding to the ensemble number based on the receive-focused signals sequentially provided from the beam former 123.

[0026] Referring back to Figure 1, the processing unit 130 is coupled to the user input unit 110 and the ultrasound data acquisition unit 120. The processing unit 130 is configured to adaptively perform clutter filtering upon the ultrasound data provided from the ultrasound data

acquisition unit 120. The processing unit 120 may further form the Doppler mode image based on the clutter-filtered ultrasound data. The processing unit 130 will be described in detail with reference to Figure 4.

[0027] Figure 4 is a block diagram showing an illustrative embodiment of the processing unit. Referring to Figure 4, the processing unit 130 includes a data processing section 131, a circle fitting section 132, a center point detecting section 133, a determining section 134, a filtering section 135 and an image forming section 136.

[0028] The data processing section 131 is configured to analyze the plurality of ultrasound data (i.e., ensemble data) provided from the ultrasound data acquisition unit 120 to thereby locate each of the plurality of ultrasound data on a complex plane.

[0029] Generally, the ultrasound data (i.e., ensemble data) corresponding to the ROI may be located on the complex plane in various shapes according to speeds of a tissue (e.g., vessel wall), blood flow and the like, which exist within the target object.

[0030] Figure 5 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to a tissue on the complex plane, wherein the tissue moves at a constant speed within the target object. Referring to Figure 5, when the tissue moves at the constant speed within the target object, a plurality of ultrasound data e1 to e12 acquired from the tissue are located on a circumference with a center point at an origin O of the complex plane. In addition, the plurality of ultrasound data e1 to e12 are located on the circumference at constant interval θ .

[0031] Figure 6 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to tissues on the complex plane, wherein the tissues comprise a tissue that does not move within the target object and another tissue that moves at constant speed within the target object. Referring to Figure 6, when the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed within the target object, a plurality of ultrasound data e1 to e12 acquired from the tissues may be located on a circumference with a speed component (i.e., DC component) of the tissue that does not move within the target object as a center point C apart from the origin O of the complex plane. In addition, the plurality of ultrasound data e1 to e12 are located on the circumference at the constant interval θ .

[0032] Figure 7 is a schematic diagram showing an example of locating a plurality of ultrasound data corresponding to a tissue on the complex plane, wherein the tissue moves at a lower speed (hereinafter, "a low speed") than a predetermined speed within the target object. Referring to Figure 7, when the tissue moves at the low speed within the target object, the ultrasound data e1 to e3 acquired from the tissue are located on a circumference C11, the ultrasound data e4 to e6 acquired from the tissue are located on a circumference C12, the ultrasound data e7 to e9 acquired from the tissue are

located on a circumference CI3, and the ultrasound data e10 to e12 acquired from the tissue are located on a circumference CI4. Center points C31 to C34 of the circumferences CI1 to CI4 are not located on the origin O of the complex plane, and may move slowly.

[0033] Examples of locating the plurality of ultrasound data, which correspond to the tissue and the blood flow that exist within the target object, on the complex plane in consideration of speeds of the tissue and the blood flow will be described in view of Figures 8 to 10.

[0034] Figure 8 is a schematic diagram showing an example of locating the plurality of ultrasound data, which correspond to the tissue and the blood flow, on the complex plane, wherein the tissue moves at the constant speed within the target object. The data processing section 131 is configured to analyze the plurality of ultrasound data e1 to e12 acquired from the tissue and the blood flow. The data processing section 131 may further locate the plurality of ultrasound data e1 to e12, which overlap speed components (shown by dotted lines) corresponding to the tissue with speed components (shown by lines) corresponding to the blood flow, on the complex plane as shown in Figure 8. The plurality of ultrasound data e1 to e12 are located on the complex plane with the center point at the origin O of the complex plane. In one embodiment, the overlap may represent sum of phases.

[0035] Figure 9 is a schematic diagram showing an example of locating the plurality of ultrasound data corresponding to the tissues and the blood flow on the complex plane, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed. The data processing section 131 is configured to analyze the plurality of ultrasound data e1 to e12 acquired from the tissues and the blood flow. The data processing section 131 may further locate the plurality of ultrasound data e1 to e12, which overlap speed components (shown by dotted lines) corresponding to the tissue with speed components (shown by lines) corresponding to the blood flow, on the complex plane as shown in Figure 9. The plurality of ultrasound data are located on the complex plane with the speed component (i.e., DC component) of the tissue that does not move within the target object as the center point C apart from the origin O of the complex plane.

[0036] Figure 10 is a schematic diagram showing an example of locating the plurality ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at a low speed within the target object. The data processing section 131 is configured to analyze the plurality of ultrasound data e1 to e12 acquired from the tissue and the blood flow. The data processing section 131 may further locate the plurality of ultrasound data e1 to e12, which overlap speed components (shown by dotted lines) corresponding to the tissue with speed components (shown by lines) corresponding to the blood flow, on the complex plane with the center points C31 to C34 as shown in Figure 10.

[0037] Referring back to Figure 4, the circle fitting sec-

tion 132 is configured to form a plurality of ultrasound data group based on the plurality of ultrasound data located on the complex plane by the data processing section 131. Each of the ultrasound data groups may include a predetermined number of ultrasound data. The circle fitting section 132 may further perform a circle fitting upon each of the ultrasound data groups. The methods of performing the circle fitting are well known in the art. For example, the circle fitting may include RANSAC circle fitting, a least-square circle fitting, an S-parameter circle fitting and the like.

[0038] Examples of performing the circle fitting upon the plurality of ultrasound data located on the complex plane in consideration of the speeds of the tissue and the blood flow, which exist within the target object, will be described in view of Figures 11 to 13.

[0039] Figure 11 is a schematic diagram showing an example of performing the circle fitting upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the constant speed within the target object. The circle fitting section 132 is configured to group the plurality of ultrasound data e1 to e12 located on the complex plane as shown in Figure 8 into the plurality of ultrasound data group G11 to G14 as shown in Figure 11. Each of the ultrasound data group G11 to G14 may include three ultrasound data. That is, a first ultrasound data group G 11 may include ultrasound data e1 to e3, a second ultrasound data group G12 may include ultrasound data e4 to e6, a third ultrasound data group G13 may include ultrasound data e7 to e9 and a fourth ultrasound data group G14 may include ultrasound data e10 to e12. The circle fitting section 132 may further perform the circle fitting upon the ultrasound data corresponding to each of the ultrasound data group G11 to G14 to thereby set circumferences CF11 to CF14 corresponding to each of the ultrasound data group as shown in Figure 11.

[0040] Figure 12 is a schematic diagram showing an example of performing the circle fitting upon the plurality of ultrasound data corresponding to the tissues and the blood flow, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed within the target object. The circle fitting section 132 is configured to group the plurality of ultrasound data e1 to e12 located on the complex plane as shown in Figure 9 into a plurality of ultrasound data groups G21 to G24 as shown in Figure 12. Each of the ultrasound data groups G21 to G24 may include three ultrasound data. That is, a first ultrasound data group G21 may include the ultrasound data e1 to e3, a second ultrasound data group G22 may include the ultrasound data e4 to e6, a third ultrasound data group G23 may include the ultrasound data e7 to e9, and the fourth ultrasound data group G24 may include the ultrasound data e10 to e12. The circle fitting section 132 may further perform the circle fitting upon the ultrasound data corresponding to each of the ultrasound data groups G21 to G24 to thereby set circumferences CF21 to CF24 corre-

sponding to each of the ultrasound data groups G21 to G24 as shown in Figure 12.

[0041] Figure 13 is a schematic diagram showing an example of performing the circle fitting upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the low speed within the target object. The circle fitting section 132 is configured to group the plurality of ultrasound data e1 to e12 located on the complex plane as shown in Figure 10 into a plurality of ultrasound data groups G31 to G34 as shown in Figure 13. Each of the ultrasound data groups G31 to G34 may include three ultrasound data. That is, a first ultrasound data may include the ultrasound data e1 to e3, a second ultrasound data may include the ultrasound data e4 to e6, a third ultrasound data may include the ultrasound data e7 to e9, and a fourth ultrasound data may include the ultrasound data e10 to e12. The circle fitting section 132 may further perform the circle fitting upon the ultrasound data corresponding to each of the ultrasound data groups G31 to G34 to thereby set circumferences CF31 to CF34 corresponding to each of the ultrasound data groups G31 to G34 as shown in Figure 13.

[0042] Referring back to Figure 4, the center point detecting section 133 is configured to detect center points of the circumferences corresponding to the plurality of ultrasound data groups based on the circumferences set by the circle fitting section 132. As one example, the center point detecting section 133 may detect center points C11 to C14 of each of the circumferences CF11 to CF14 corresponding to the plurality of ultrasound data groups G11 to G14 as shown in Figure 11. As another example, the center point detecting section 133 may detect center points C21 to C24 of each of the circumferences CF21 to CF24 corresponding to the plurality of ultrasound data groups G21 to G24 as shown in Figure 12. As yet another example, the center point detecting section 133 may detect center points C31 to C34 of each of the circumferences CF31 to CF34 corresponding to the plurality of ultrasound data groups G31 to G34 as shown in Figure 13. The methods of detecting the center points are well known in the art. Thus, they have not been described in detail so as not to unnecessarily obscure the present disclosure.

[0043] The determining section 134 is configured to analyze the plurality of center points detected by the center point detecting section 133. The determining section 134 may further determine whether the plurality of the center points are located on the same position and whether located on the origin of the complex plane to thereby form determination information.

[0044] As one example, the determining section 134 may be configured to analyze the center points C11 to C14 corresponding to the plurality of circumferences CF11 to CF14 as shown in Figure 11. The determining section 134 may further determine whether the plurality of center points C1 to C14 are located on the same position and whether located on the origin of the complex plane.

If it is determined that the plurality of center points C11 to C14 are located on the same position and located on the origin of the complex plane, then the determining section 134 may form first determination information. The first determination information may be the information representing that the plurality of center points C11 to C14 are located on the same position and located on the origin of the complex plane. That is, the first determination information may be information representing that the tissue and the blood flow exist within the target object, wherein the tissue moves at the constant speed.

[0045] As another example, the determining section 134 may be configured to analyze the center points C21 to C24 corresponding to the plurality of circumferences CF21 to CF24 as shown in Figure 12. The determining section 134 may further determine whether the plurality of center points C21 to C24 are located on the same position and whether located on the origin of the complex plane. If it is determined that the plurality of center points C21 to C24 are located on the same position but not located on the origin of the complex plane, then the determining section 134 may form second determination information. The second determination information may be the information representing that the plurality of center points C21 to C24 are located on the same position but not located on the origin of the complex plane. That is, the second determination information may be the information representing that the tissues and the blood flow exist within the target object, wherein the tissues comprise the tissue that does not move and the tissue that moves at the constant speed.

[0046] As yet another example, the determining section 134 may be configured to analyze the center points C31 to C34 corresponding to the plurality of the circumferences CF31 to CF34 shown in Figure 13. The determining section 134 may further determine whether the plurality of center points C31 to C34 are located on the same position and whether located on the origin of the complex plane. If it is determined that the plurality of center points C31 to C34 are neither located on the same position nor on the origin of the complex plane, then the determining section 134 may form third determination information. The third determination information may be the information representing that the plurality of center points C31 to C34 are neither located on the same position nor on the origin of the complex plane. That is, the third determination information may be the information representing that the tissue and the blood flow exist within the target object, wherein the tissue moves at the low speed.

[0047] The filtering section 135 is configured to perform a downmixing and a clutter filtering upon the plurality of ultrasound data based on the determination information provided from the determining section 134.

[0048] Examples of performing the downmixing and the clutter filtering upon the plurality of ultrasound data will be described with reference to Figures 14 to 16.

[0049] Figure 14 is a schematic diagram showing an

example of performing the downmixing upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the constant speed. The filtering section 135 is configured to perform the downmixing, which rotates each of the plurality of ultrasound data e1 to e12 into a real axis of the complex plane with the center point at the origin O of the complex plane based on the first determination information provided from the determining section 134, upon the plurality of ultrasound data e1 to e12 as shown in Figure 14. More particularly, the filtering section 135 may perform the downmixing, which performs a phase shift (0°) upon the ultrasound data e1 based on the first determination information. The filtering section 135 may further perform the downmixing, which performs a phase shift ($-\theta$) upon the ultrasound data e2 based on the first determination information. The filtering section 135 may further perform the downmixing, which performs a phase shift ($-\theta$) upon the ultrasound data e3 based on the first determination information. The filtering section 135 may further perform the downmixing on the ultrasound data e4 to e12 as described above. As to performing the downmixing upon each of the plurality of ultrasound data, the speed components corresponding to clutter signals moves to DC component. The filtering section 135 may further perform the clutter filtering upon the downmixed ultrasound data to thereby filter the speed components (i.e., DC component) corresponding to the clutter signals from the downmixed ultrasound data.

[0050] Figure 15 is a schematic diagram showing an example of performing the downmixing upon the plurality of ultrasound data corresponding to the tissues and the blood flow, wherein the tissues comprise the tissue that does not move within the target object and the tissue that moves at the constant speed within the target object. The filtering section 135 is configured to perform the downmixing upon each of the plurality of ultrasound data e1 to e12 based on the second determination information provided from the determining section 134 as shown in Figure 15. More particularly, the filtering section 135 may move the center points of the circumferences corresponding to the ultrasound data e1 to e12 to the origin O of the complex plane based on the second determination information. The filtering section 135 may further perform the downmixing, which rotates each of the plurality of ultrasound data e1 to e12 into the real axis based on the origin O of the complex plane as described above. That is, the filtering section 135 may perform the downmixing, which performs a phase shift (0°) on the ultrasound data e1 based on the second determination information. The filtering section 135 may further perform the downmixing, which performs a phase shift ($-\theta$) on the ultrasound data e2 based on the second determination information. The filtering section 135 may further perform the downmixing, which performs a phase shift ($-\theta$) on the ultrasound data e3 based on the second determination information. The filtering section 135 may further perform the downmixing on the ultrasound data e4 to e12

as described above. As to performing the downmixing upon each of the plurality of ultrasound data, the speed components corresponding to clutter signals move to DC component. The filtering section 135 may further perform the clutter filtering upon the downmixed ultrasound data to thereby filter the speed components (i.e., DC component) corresponding to the clutter signals from the plurality of the ultrasound data.

[0051] It was explained in the above embodiment that the filtering section 135 may move the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane, and perform the downmixing on each of the ultrasound data. However, the filtering section 135 may further set any ultrasound data (e.g., first ultrasound data e1) among the plurality of ultrasound data e1 to e12 as a reference ultrasound data, perform the downmixing, which rotates each of the ultrasound data into the reference ultrasound data, upon the plurality of ultrasound data, and move the center points of the circumferences to the origin of the complex plane.

[0052] Figure 16 is a schematic diagram showing an example of performing the downmixing upon the plurality of ultrasound data corresponding to the tissue and the blood flow, wherein the tissue moves at the low speed within the target object. The filtering section 135 is configured to perform the downmixing upon each of the ultrasound data e1 to e12 based on the third determination information provided from the determining section 134 as shown in Figure 16. More particularly, the filtering section 135 may move the center points of the plurality of circumferences corresponding to the plurality of ultrasound data e1 to e12 to the origin O of the complex plane based on the third determination information. The filtering section 135 may further perform the downmixing that rotates each of the ultrasound data e1 to e12 into the real axis of the complex plane based on the origin O of the complex plane as described above. As to performing the downmixing on each of the ultrasound data, the speed components corresponding to clutter signals move to the DC component. The filtering section 135 may further perform the clutter filtering on the plurality of ultrasound data to thereby filter the speed components (i.e., DC component) corresponding to the clutter signals from the plurality of the ultrasound data.

[0053] Referring back to Figure 4, the image forming section 136 is configured to form a Doppler mode image based on the plurality of ultrasound image downmixed and clutter-filtered by the filtering section 135.

[0054] Referring back to Figure 1, the storage unit 140 may store the plurality of ultrasound data acquired from the ultrasound data acquisition unit 110. The storage unit 140 may further store the plurality of ultrasound data filtered by the processing unit 130. The display unit 150 may display the Doppler mode image formed by the processing unit 130.

[0055] As an example, while only the processing unit 130 may perform the circle fitting, the downmixing and

the clutter filtering upon the plurality of ultrasound data acquired from the ultrasound data acquisition unit 120, the processing unit 130 may further perform the circle fitting, the downmixing and the clutter filtering on a plurality of ultrasound data provided from external devices (e.g., a personal computer, a storage medium, etc.) which connect to the ultrasound system.

Claims

1. An ultrasound system, comprising:

an ultrasound data acquisition (120) unit configured to transmit and receive ultrasound signals to and from a target object to thereby output a plurality of ultrasound data for obtaining a color Doppler mode image, wherein the target object includes at least one of a tissue and a blood flow; and

a processing unit (130) placed in communication with the ultrasound data acquisition unit and being configured to locate the plurality of ultrasound data on a complex plane, the processing unit being further configured to perform a circle fitting upon the plurality of ultrasound data located on the complex plane and perform a downmixing and a clutter filtering upon the circle-fitted ultrasound data in consideration of speed of the tissue, wherein the ultrasound data comprise IQ (in-phase/quadrature) data, wherein the processing unit (130) comprises:

a data processing section (131) configured to analyze the plurality of ultrasound data to thereby locate the plurality of ultrasound data on the complex plane;

a circle fitting section (132) configured to perform the circle fitting upon the plurality of ultrasound data to thereby set circumferences corresponding to the plurality of ultrasound data;

a center point detecting section (133) configured to detect center points of the circumferences;

a determining section (134) configured to analyze the detected center points and determine whether the detected center points are located on a same position and located on an origin of the complex plane to thereby form determination information; and

a filtering section (135) configured to perform the downmixing and the clutter filtering upon the plurality of ultrasound data based on the determination information.

2. The ultrasound system of Claim 1, wherein the circle

fitting section (132) is configured to:

group the plurality of ultrasound data located on the complex plane into a plurality of ultrasound data groups, wherein each of the plurality of ultrasound data groups comprises a predetermined number of ultrasound data; and perform the circle fitting upon each of the plurality of ultrasound data groups to thereby set the circumferences corresponding to the plurality of ultrasound data groups.

3. The ultrasound system of Claim 2, wherein the center point detecting section (133) is configured to detect the center points of the circumferences corresponding to the plurality of ultrasound data groups.

4. The ultrasound system of Claim 1, wherein the determination information comprises:

first determination information representing that the detected center points are located on the same position and located on the origin of the complex plane;

second determination information representing that the detected center points are located on the same position but not located on the origin of the complex plane; and

third determination information representing that the detected center points are neither located on the same position nor on the origin of the complex plane.

5. The ultrasound system of Claim 4, wherein the filtering section (135) is configured to:

perform the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane with the center point at the origin of the complex plane based on the first determination information; and perform the clutter filtering upon the downmixed ultrasound data.

6. The ultrasound system of Claim 4, wherein the filtering section (135) is configured to:

move the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane based on the second determination information; perform the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane based on the origin of the complex plane; and perform the clutter filtering on the downmixed ultrasound data.

7. The ultrasound system of Claim 4, wherein the filtering section (135) is configured to:

set any ultrasound data among the plurality of ultrasound data as a reference ultrasound data based on the second determination information; perform the downmixing for rotating each of the plurality of ultrasound data into the reference ultrasound data based on the center points of the circumferences; and move the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane.

8. The ultrasound system of Claim 4, wherein the filtering section (135) is configured to:

move the center points of the circumferences corresponding to the plurality of ultrasound data into the origin of the complex plane based on the third determination information; perform the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane based on the origin of the complex plane; and perform the clutter filtering upon the downmixed ultrasound data.

9. A method of performing a clutter filtering, comprising:

a) acquiring a plurality of ultrasound data corresponding to a target object including at least one of a tissue and a blood flow, wherein the plurality of ultrasound data are ultrasound data for obtaining a color Doppler mode image; b) locating each of the plurality of ultrasound data on a complex plane; c) performing a circle fitting on the plurality of ultrasound data located on the complex plane to thereby set the circumferences corresponding to the plurality of ultrasound data; and d) performing a downmixing and a clutter filtering on the circle-fitted ultrasound data in consideration of speed of the tissue,

wherein the ultrasound data comprise IQ (in-phase/quadrature) data, wherein the step d) comprises:

d1) detecting the center points corresponding to the circumferences; d2) analyzing the detected center points, determining whether the detected center points are located on a same position and located on origin of the complex plane to thereby form determination information; and d3) performing the downmixing and the clutter filtering upon the plurality of ultrasound data

based on the determination information.

10. The method of claim 9 wherein the step c) comprises:

grouping the plurality of ultrasound data located on the complex plane into a plurality of ultrasound data groups, wherein each of the plurality of ultrasound data groups comprises a predetermined number of ultrasound data; and performing the circle fitting upon each of the plurality of ultrasound data groups to thereby set the circumferences corresponding to the plurality of ultrasound data groups.

11. The method of Claim 10, wherein the determination information comprises:

first determination information representing that the detected center points are located on the same position and located on the origin of the complex plane; second determination information representing that the detected center points are located on the same position but not located on the origin of the complex plane; and third determination information representing that the detected center points are neither located on the same position nor on the origin of the complex plane.

12. The method of Claim 11, wherein the step d3) comprises:

performing the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane with the center point at the origin of the complex plane based on the first determination information; and performing the clutter filtering upon the downmixed ultrasound data.

13. The method of Claim 11, wherein the step d3) comprises:

moving the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane based on the second determination information; performing the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane based on the origin of the complex plane; and performing the clutter filtering upon the downmixed ultrasound data.

14. The method of Claim 11, wherein the step d3) comprises:

setting any ultrasound data among the plurality of ultrasound data as a reference ultrasound data based on the second determination information;

performing the downmixing for rotating each of the plurality of ultrasound data into the reference ultrasound data based on the center points of the circumferences; and
moving the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane.

15. The method of Claim 11, wherein the step d3) comprises:

moving the center points of the circumferences corresponding to the plurality of ultrasound data to the origin of the complex plane based on the third determination information;
performing the downmixing for rotating each of the plurality of ultrasound data into a real axis of the complex plane based on the origin of the complex plane; and
performing the clutter filtering on the downmixed ultrasound data.

Patentansprüche

1. Ultraschallsystem, welches folgendes aufweist:

Eine Ultraschalldatenerlangungseinheit (120), die dafür vorgesehen ist, Ultraschallsignale zu einem Zielobjekt zu übertragen und von demselben zu empfangen, um dadurch eine Vielzahl von Ultraschalldaten zur Erlangung eines Farb-/Dopplermodus-Bild auszugeben, wobei das Zielobjekt wenigstens eines eines Gewebes und einer Blutströmung aufweist; und
eine Verarbeitungseinheit (130), die in Verbindung mit der Ultraschalldatenerlangungseinheit angeordnet und dafür vorgesehen ist, die Vielzahl von Ultraschalldaten auf einer komplexen Ebene anzuordnen, wobei die Verarbeitungseinheit des Weiteren dafür vorgesehen ist, eine Kreisanpassung bzw. ein Kreisfitting an der Vielzahl von auf der komplexen Ebene angeordneten Ultraschalldaten durchzuführen und ein Abwärtsmischen bzw. ein Downmixing und ein Störfiltern bzw. Clutterfiltern an den kreisgefilterten Ultraschalldaten unter Beachtung der Geschwindigkeit des Gewebes durchzuführen, wobei die Ultraschalldaten IQ (In-Phasen/Quadratur) - Daten aufweisen,
wobei die Verarbeitungseinheit (130) folgendes aufweist:

einen Datenverarbeitungsabschnitt (131), der dafür vorgesehen ist, die Vielzahl von Ultraschalldaten zu analysieren, um dadurch die Vielzahl von Ultraschalldaten auf der komplexen Ebene anzuordnen;
einen Kreisanpassungsabschnitt (132), der dafür vorgesehen ist, die Kreisanpassung an der Vielzahl von Ultraschalldaten durchzuführen, um dadurch die der Vielzahl von Ultraschalldaten entsprechende Umkreise bzw. Ausdehnungen festzulegen;
einen Mittelpunktdetektierabschnitt (133), der dafür vorgesehen ist, Mittelpunkte der Umkreise zu detektieren;
einen Ermittlungsabschnitt (134), der dafür vorgesehen ist, die detektierten Mittelpunkte zu analysieren und zu ermitteln, ob die detektierten Mittelpunkte auf derselben Position und auf einem Ursprung der komplexen Ebene angeordnet sind, um dadurch Ermittlungsinformationen zu bilden;
einen Filterabschnitt (135), der dafür vorgesehen ist, das Downmixing und das Clutterfiltern an der Vielzahl von Ultraschalldaten basierend auf den Ermittlungsinformationen durchzuführen.

2. Ultraschallsystem nach Anspruch 1, wobei der Kreisanpassungsabschnitt (132) für folgendes vorgesehen ist:

Gruppieren der Vielzahl von Ultraschalldaten, die auf der komplexen Ebene angeordnet sind, in eine Vielzahl von Ultraschalldatengruppen, wobei jede der Vielzahl von Ultraschalldatengruppen eine bestimmte Anzahl an Ultraschalldaten aufweist; und
Durchführen der Kreisanpassung an jeder der Vielzahl von Ultraschalldatengruppen, um dadurch die der Vielzahl von Ultraschalldatengruppen entsprechenden Umkreise festzulegen.

3. Ultraschallsystem nach Anspruch 2, wobei der Mittelpunktdetektierabschnitt (133) dafür vorgesehen ist, die Mittelpunkte der der Vielzahl von Ultraschalldatengruppen entsprechenden Umkreise zu detektieren.

4. Ultraschallsystem nach Anspruch 1, wobei die Ermittlungsinformationen folgendes aufweisen:

Erste Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte auf derselben Position und auf dem Ursprung der komplexen Ebene angeordnet sind;
Zweite Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte auf derselben Position, jedoch nicht auf dem Ur-

- sprung der komplexen Ebene angeordnet sind;
und
Dritte Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte weder auf derselben Position noch auf dem Ursprung der komplexen Ebene angeordnet sind.
5. Ultraschallsystem nach Anspruch 4, wobei der Filterabschnitt (135) für folgendes vorgesehen ist:
- 10 Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene mit den Mittelpunkt auf dem Ursprung der komplexen Ebene basierend auf dem ersten Ermittlungsinformationen; und
15 Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.
6. Ultraschallsystem nach Anspruch 4, wobei der Filterabschnitt (135) für folgendes vorgesehen ist:
- 20 Bewegen der Mittelpunkte der des Vielzahl von Ultraschalldaten entsprechenden Umkreise auf den Ursprung der komplexen Ebene basierend auf den zweiten Ermittlungsinformationen;
25 Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene basierend auf dem Ursprung der komplexen Ebene; und
30 Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.
7. Ultraschallsystem nach Anspruch 4, wobei der Filterabschnitt (135) für folgendes vorgesehen ist:
- 35 Festlegen von beliebigen Ultraschalldaten unter der Vielzahl von Ultraschalldaten als Referenzultraschalldaten basierend auf den zweiten Ermittlungsinformationen;
40 Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in die Referenzultraschalldaten basierend auf den Mittelpunkten der Umkreise; und
45 Bewegen der Mittelpunkte der des Vielzahl von Ultraschalldaten entsprechenden Umkreise auf den Ursprung der komplexen Ebene.
8. Ultraschallsystem nach Anspruch 4, wobei der Filterabschnitt (135) für folgendes vorgesehen ist:
- 50 Bewegen der Mittelpunkte der der Vielzahl von Ultraschalldaten entsprechenden Umkreise in den Ursprung der komplexen Ebene basierend auf den dritten Ermittlungsinformationen;
55 Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene basierend auf dem Ursprung der komplexen Ebene; und
Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.
9. Verfahren zum Durchführen eines Störfilters bzw. Clutterfilterns, welches folgendes aufweist:
- a) Erlangen einer Vielzahl von Ultraschalldaten, die einen Zielobjekt entsprechen, das wenigstens eines eines Gewebes und einer Blutströmung aufweist, wobei die Vielzahl der Ultraschalldaten Ultraschalldaten zum Erlangen eines Farb-/Dopplermodus-Bilds sind;
b) Anordnen jeder der Vielzahl von Ultraschalldaten auf einer komplexen Ebene;
c) Durchführen einer Kreisanpassung bzw. eines Kreisfittings an der Vielzahl von auf der komplexen Ebene angeordneten Ultraschalldaten, um dadurch die der Vielzahl von Ultraschalldaten entsprechenden Umkreise festzulegen; und
d) Durchführen eines Abwärtsmischen bzw. eines Downmixings und eines Störfilters bzw. Clutterfilterns an den kreisgefitteten Ultraschalldaten unter Beachtung der Geschwindigkeit des Gewebes,
- wobei die Ultraschalldaten IQ (In-Phasen/Quadratur)-Daten aufweisen, wobei der Schritt d) folgendes aufweist:
- d1) Detektieren der Mittelpunkte, die den Umkreisen entsprechen;
d2) Analysieren der detektierten Mittelpunkte, ermitteln, ob die detektierten Mittelpunkte auf derselben Position und auf einem Ursprung der komplexen Ebene angeordnet sind, um dadurch Ermittlungsinformationen zu bilden; und
d3) Durchführen des Downmixings und des Clutterfilterns an der Vielzahl von Ultraschalldaten basierend auf den Ermittlungsinformationen.
10. Verfahren nach Anspruch 9, wobei der Schritt c) folgendes aufweist:
- Gruppieren der Vielzahl von Ultraschalldaten, die auf der komplexen Ebene angeordnet sind, in eine Vielzahl von Ultraschalldatengruppen, wobei jede der Vielzahl von Ultraschalldatengruppen eine bestimmte Anzahl an Ultraschalldaten aufweist; und
Durchführen der Kreisanpassung an jeder der Vielzahl von Ultraschalldatengruppen, um dadurch die der Vielzahl von Ultraschalldatengruppen entsprechenden Umkreise festzulegen.
11. Verfahren nach Anspruch 10, wobei die Ermittlungsinformationen folgendes aufweisen:

Erste Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte auf derselben Position und auf dem Ursprung der komplexen Ebene angeordnet sind;

Zweite Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte auf derselben Position, jedoch nicht auf dem Ursprung der komplexen Ebene angeordnet sind; und

Dritte Ermittlungsinformationen, die repräsentieren, dass die detektierten Mittelpunkte weder auf derselben Position noch auf dem Ursprung der komplexen Ebene angeordnet sind.

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Bewegen der Mittelpunkte der der Vielzahl von Ultraschalldaten entsprechenden Umkreise in den Ursprung der komplexen Ebene basierend auf den dritten Ermittlungsinformationen;

Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene basierend auf dem Ursprung der komplexen Ebene; und
Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.

Revendications

12. Verfahren nach Anspruch 11, wobei der Schritt d3) folgendes aufweist:

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Durchführen des Downmixings zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene mit dem Mittelpunkt auf dem Ursprung der komplexen Ebene basierend auf den ersten Ermittlungsinformationen; und

Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.

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13. Verfahren nach Anspruch 11, wobei der Schritt d3) folgendes aufweist:

Bewegen der Mittelpunkte der der Vielzahl von Ultraschalldaten entsprechenden Umkreise auf den Ursprung der komplexen Ebene basierend auf den zweiten Ermittlungsinformationen;

Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in eine reale Achse der komplexen Ebene basierend auf dem Ursprung der komplexen Ebene; und
Durchführen des Clutterfilterns an den downgemixten Ultraschalldaten.

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14. Verfahren nach Anspruch 11, wobei der Schritt d3) folgendes aufweist:

Festlegen von beliebigen Ultraschalldaten unter der Vielzahl von Ultraschalldaten als Referenzultraschalldaten basierend auf den zweiten Ermittlungsinformationen;

Durchführen des Downmixens zum Rotieren jeder der Vielzahl von Ultraschalldaten in die Referenzultraschalldaten basierend auf den Mittelpunkten der Umkreise; und

Bewegen der Mittelpunkte der der Vielzahl von Ultraschalldaten entsprechenden Umkreise auf den Ursprung der komplexen Ebene.

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15. Verfahren nach Anspruch 11, wobei der Schritt d3) folgendes aufweist:

1. Système ultrasonique comportant :

une unité d'acquisition de données ultrasoniques (120) configurée pour transmettre et recevoir des signaux ultrasoniques vers un objet cible pour émettre une pluralité de données ultrasoniques pour obtenir une image Doppler en couleurs, dans lequel l'objet cible comporte au moins un tissu ou un flux sanguin; et

une unité de traitement (130) placée en communication avec l'unité d'acquisition de données ultrasoniques et étant configurée pour localiser la pluralité de données ultrasoniques sur un plan complexe, l'unité de traitement étant par ailleurs configurée pour obtenir un cercle correspondant avec la pluralité de données ultrasoniques localisées sur le plan complexe et effectuer un mixage réducteur et un filtrage des amas sur les données ultrasoniques contenues dans le cercle en tenant compte de la vitesse du tissu ;
dans lequel les données ultrasoniques comportent des données I/Q (en-phase/quadrature), dans lequel l'unité de traitement (130) comprend :

une section de traitement de données (131) configurée pour analyser la pluralité de données ultrasoniques afin de localiser, de ce fait, la pluralité de données ultrasoniques sur le plan complexe ;

une section de détermination de cercle (132) configurée pour effectuer une détermination de cercle sur la pluralité de données ultrasoniques afin de fixer les circonférences correspondant à la pluralité de données ultrasoniques ;

une section de détection de point central (133) configurée pour détecter les points centraux des circonférences ;

une section de détermination (134) configurée pour analyser les points centraux détectés et déterminer si ces points centraux sont ou non localisés dans la même position et disposés sur l'origine du plan complexe

- afin de déterminer par ce moyen des informations ;
et
une section de filtrage (135) configurée pour effectuer le mixage réducteur et le filtrage des amas sur la pluralité de données ultrasoniques basés sur la détermination des informations.
2. Système ultrasonique selon la revendication 1, dans lequel la section de détermination de cercle (132) est en outre configurée pour :
- grouper la pluralité de données ultrasoniques localisées sur le plan complexe en une pluralité de groupes de données ultrasoniques, dans lequel la pluralité de groupes de données ultrasoniques comprend un nombre prédéterminé de données ultrasoniques ; et
effectuer la détermination de cercle respectivement de chaque groupe de pluralités de données ultrasoniques correspondant à la pluralité de groupes de données ultrasoniques.
3. Système ultrasonique selon la revendication 2, dans lequel la section de détection de point central (133) est configurée pour détecter les points centraux des circonférences correspondant à la pluralité de groupes de données ultrasoniques.
4. Système ultrasonique selon la revendication 1, dans lequel l'information de détermination d'informations comprend :
- une première détermination d'informations qui montre que les points centraux détectés sont localisés dans la même position et sont localisés sur l'origine du plan complexe ;
une seconde détermination d'informations qui montre que les points centraux détectés sont localisés dans la même position, mais non localisés sur l'origine du plan complexe ;
une troisième détermination d'informations qui montre que les points centraux détectés ne sont localisés ni dans la même position ni sur l'origine du plan complexe.
5. Système ultrasonique selon la revendication 4, dans lequel la section de filtrage (135) est configurée pour :
- effectuer le mixage réducteur afin de mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe avec le point central à l'origine du plan complexe basé sur la première détermination d'informations ; et
effectuer le filtrage des amas sur les données
- ultrasoniques mixées réduites.
6. Système ultrasonique selon la revendication 4, dans lequel la section de filtrage (135) est configurée pour :
- déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe sur la base de la seconde détermination d'informations ;
effectuer le mixage réducteur afin de mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe avec le point central à l'origine du plan complexe ; et
effectuer le filtrage des amas sur les données ultrasoniques mixées réduites.
7. Système ultrasonique selon la revendication 4, dans lequel la section de filtrage (135) est configurée pour :
- fixer chaque donnée ultrasoniques parmi la pluralité de données ultrasoniques comme une référence de données ultrasoniques sur la seconde détermination d'informations ; et
effectuer le mixage réducteur pour mettre en rotation chacune de la pluralité de données ultrasoniques dans la référence de données ultrasoniques sur la base des points centraux des circonférences ; et
déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe.
8. Système ultrasonique selon la revendication 4, dans lequel la section de filtrage (135) est configurée pour :
- déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe sur la base de la troisième détermination d'informations ;
effectuer le mixage réducteur pour mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe sur la base de l'origine du plan complexe ; et
effectuer le filtrage des amas sur les données ultrasoniques mixées.
9. Procédé pour effectuer le filtrage des amas comprenant :
- a) l'acquisition d'une pluralité de données ultrasoniques correspondant à un objet cible comportant au moins un tissu et un flux sanguin, dans lequel la pluralité de données ultrasoniques sont des données ultrasoniques destinées

à obtenir une image Doppler en couleurs;
 b) la localisation de chacune des données ultrasoniques sur un plan complexe ;
 c) la création d'un cercle correspondant à la pluralité des données ultrasoniques, et ainsi, la fixation des circonférences correspondant à la pluralité de données ultrasoniques;
 d) la réalisation d'un mixage réducteur et d'un filtrage des amas sur les données ultrasoniques fixées dans les cercles en considération de la vitesse du tissu ;

dans lequel dans lequel les données ultrasoniques comportent des données I/Q(en-phase/quadrature), dans lequel l'étape d) comprend :

d1) la détection des points centraux correspondants aux circonférences ;
 d2) l'analyse des points centraux détectés, la détermination si les points centraux détectés sont ou non localisés dans la même position et disposés sur l'origine du plan complexe afin de déterminer par ce moyen des informations ; et
 d3) le mixage réducteur et le filtrage des amas sur la pluralité de données ultrasoniques sur le plan complexe basés sur la détermination des informations.

10. Procédé selon la revendication 9, dans lequel l'étape c) comprend :

le groupage de la pluralité de données ultrasoniques localisées sur le plan complexe en une pluralité de groupes de données ultrasoniques, dans lequel chacun des groupes de données ultrasoniques comprend un nombre prédéterminé de données ultrasoniques ; et
 la définition de cercles correspondant à la pluralité de groupes de données ultrasoniques et de ce fait fixer les circonférences correspondant à la pluralité de groupes de données ultrasoniques,

11. Procédé selon la revendication 10, dans lequel la détermination des informations comprend :

une première détermination d'informations qui montre que les points centraux détectés sont localisés dans la même position et sont localisés sur l'origine du plan complexe ;
 une seconde détermination d'informations qui montre que les points centraux détectés sont localisés dans la même position mais pas sur l'origine du plan complexe ; et
 une troisième détermination d'informations qui montre que les points centraux détectés ne sont localisés ni dans la même position ni sur l'origine du plan complexe.

12. Procédé selon la revendication 11, dans lequel l'étape d3) consiste à :

effectuer le mixage réducteur afin de mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe avec le point central à l'origine du plan complexe basé sur la première détermination d'informations ; et
 effectuer le filtrage des amas sur les données ultrasoniques mixées.

13. Procédé selon la revendication 11, dans lequel l'étape d3) consiste à :

déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe sur la base de la seconde détermination d'informations ;
 effectuer le mixage réducteur afin de mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe avec le point central à l'origine du plan complexe ; et
 effectuer le filtrage des amas sur les données ultrasoniques mixées.

14. Procédé selon la revendication 11, dans lequel l'étape d3) consiste à :

fixer chaque donnée ultrasoniques parmi la pluralité de données ultrasoniques comme une référence de données ultrasoniques sur la seconde détermination d'informations ; et
 effectuer le mixage réducteur pour mettre en rotation chacune de la pluralité de données ultrasoniques dans la référence de données ultrasoniques sur la base des points centraux des circonférences ; et
 déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe

15. Procédé selon la revendication 11, dans lequel l'étape d3) consiste à :

déplacer les points centraux des circonférences correspondant à la pluralité de données ultrasoniques à l'origine du plan complexe sur la base de la troisième détermination d'informations ;
 effectuer le mixage réducteur pour mettre en rotation chacune de la pluralité de données ultrasoniques selon un axe réel du plan complexe sur la base de l'origine du plan complexe ; et
 effectuer le filtrage des amas sur les données ultrasoniques mixées.

FIG. 1

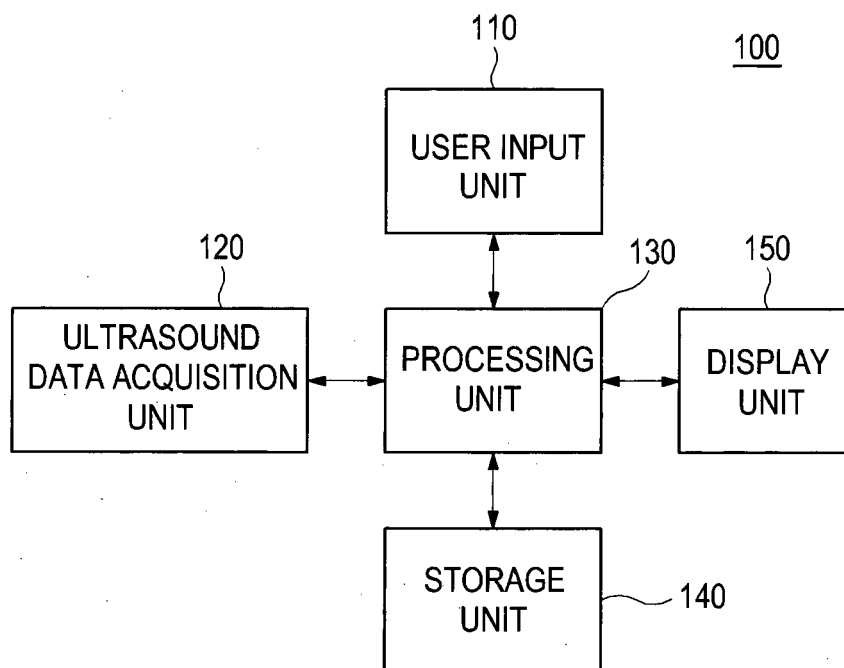


FIG. 2

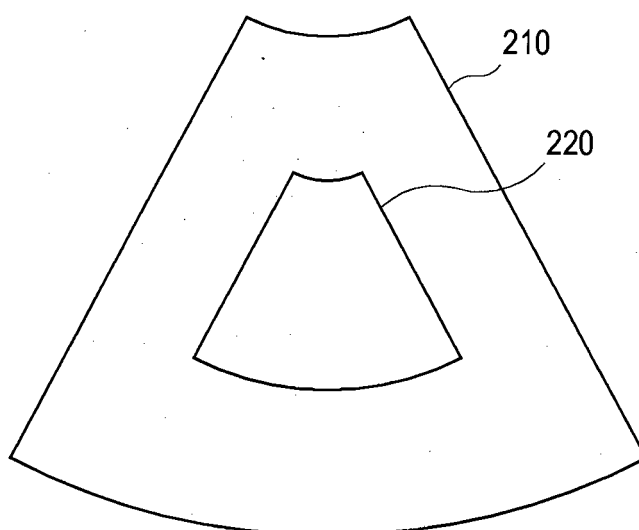


FIG. 3

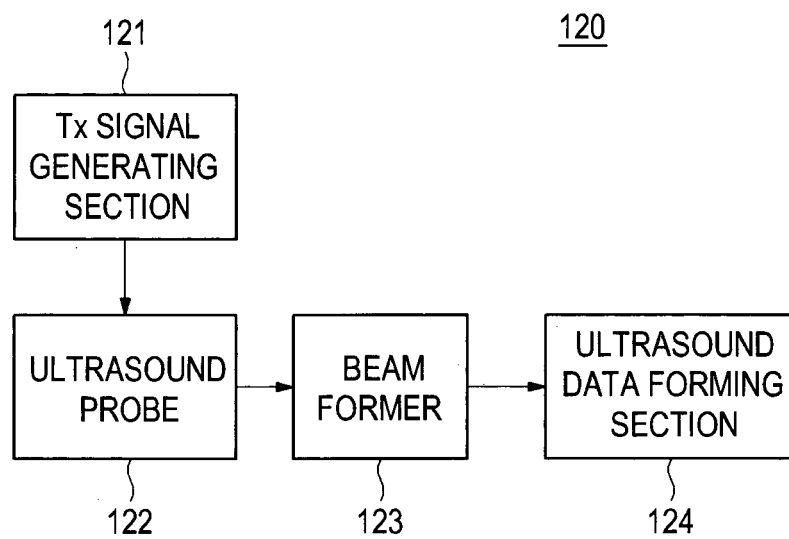


FIG. 4

130

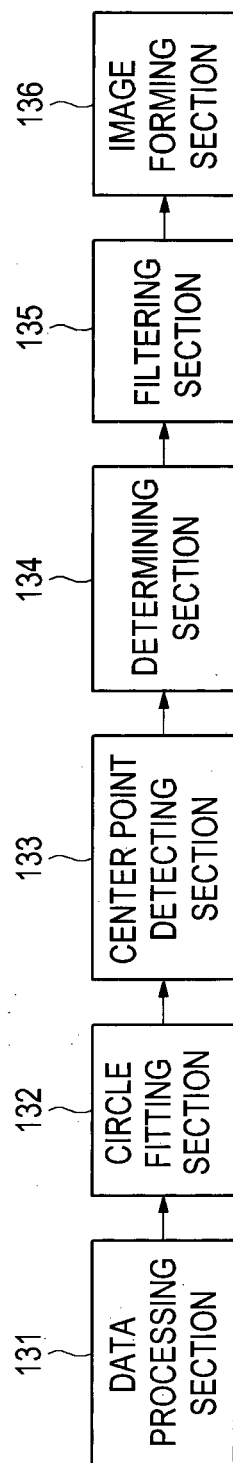


FIG. 5

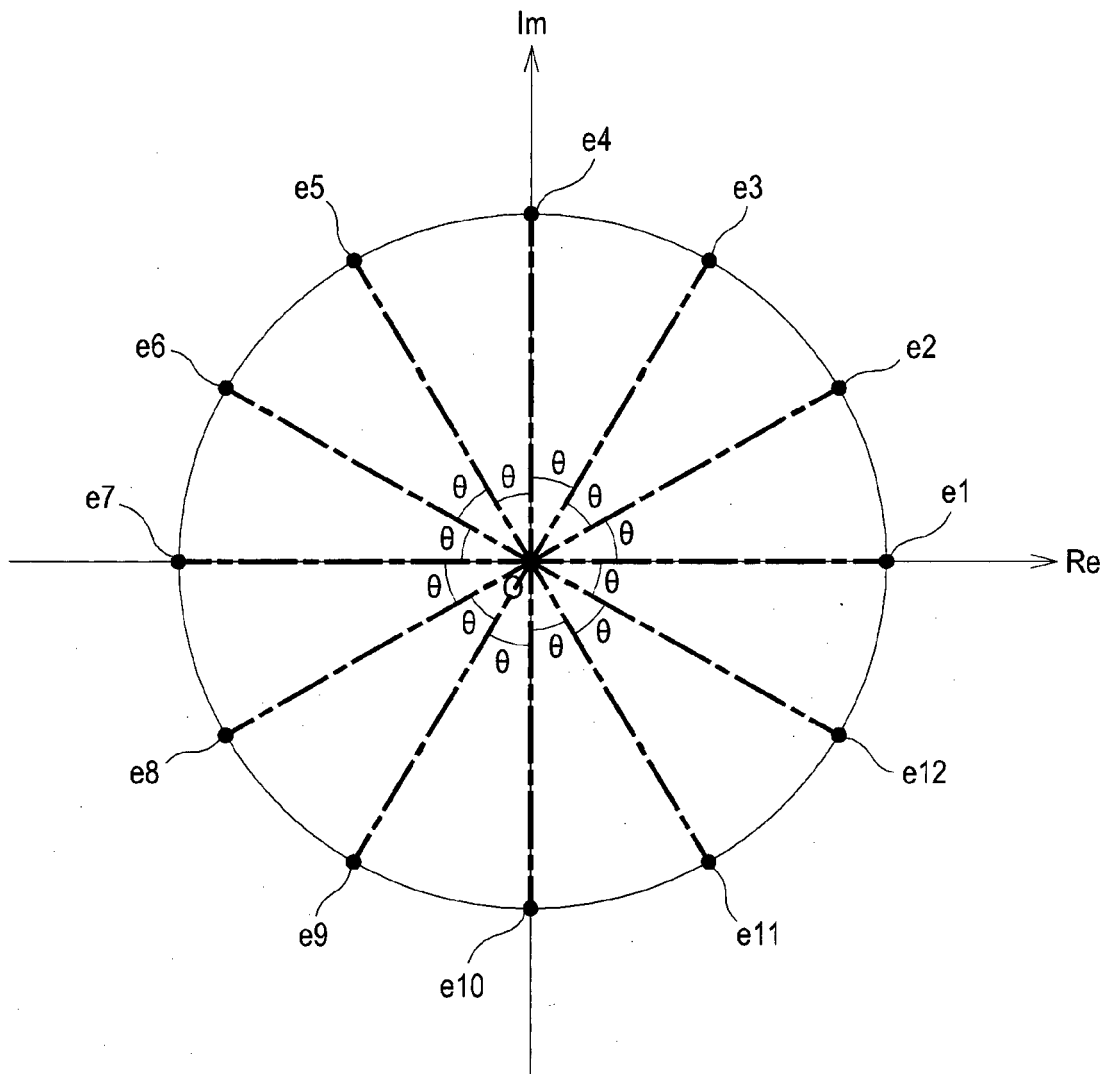


FIG. 6

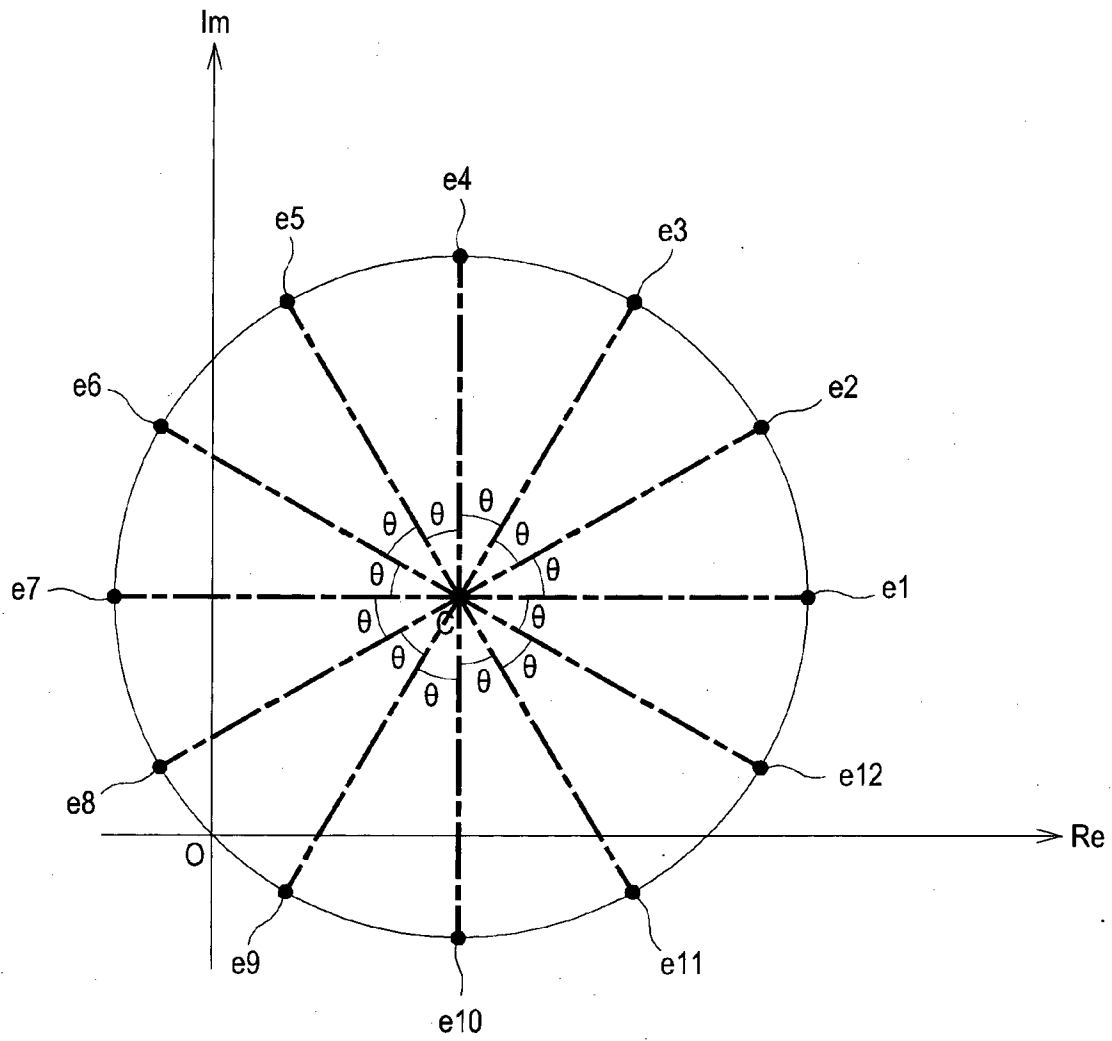


FIG. 7

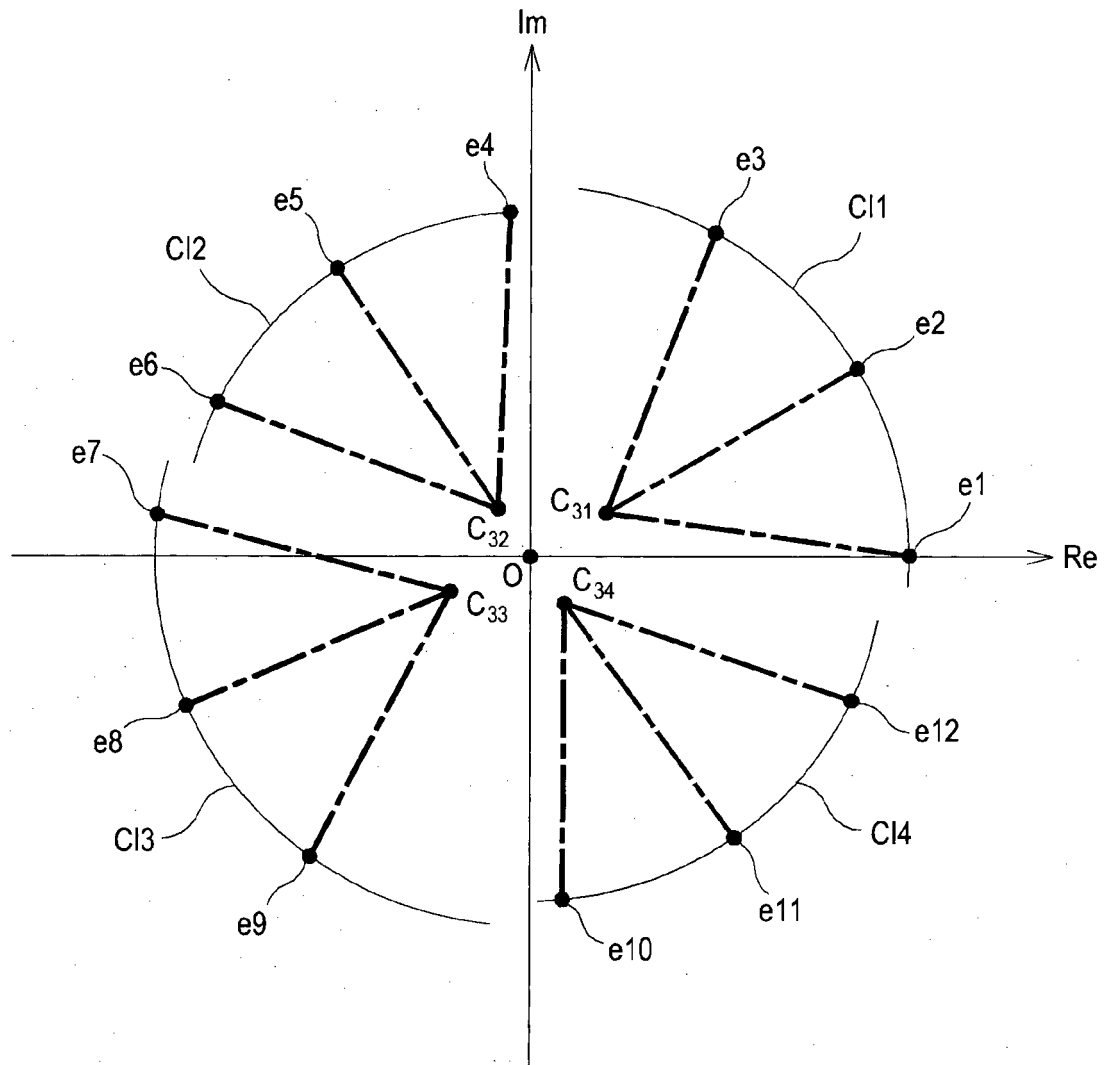


FIG. 8

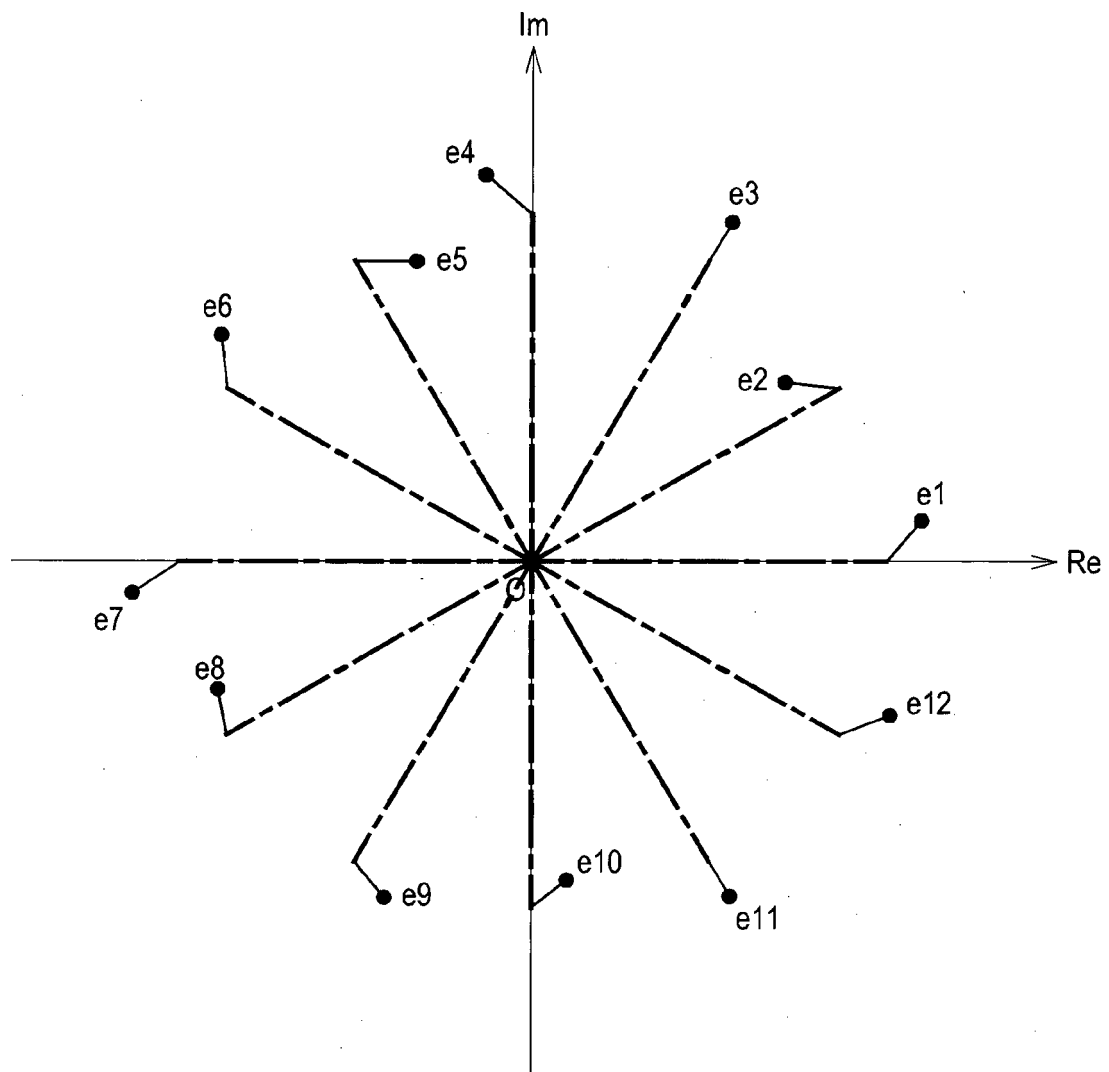


FIG. 9

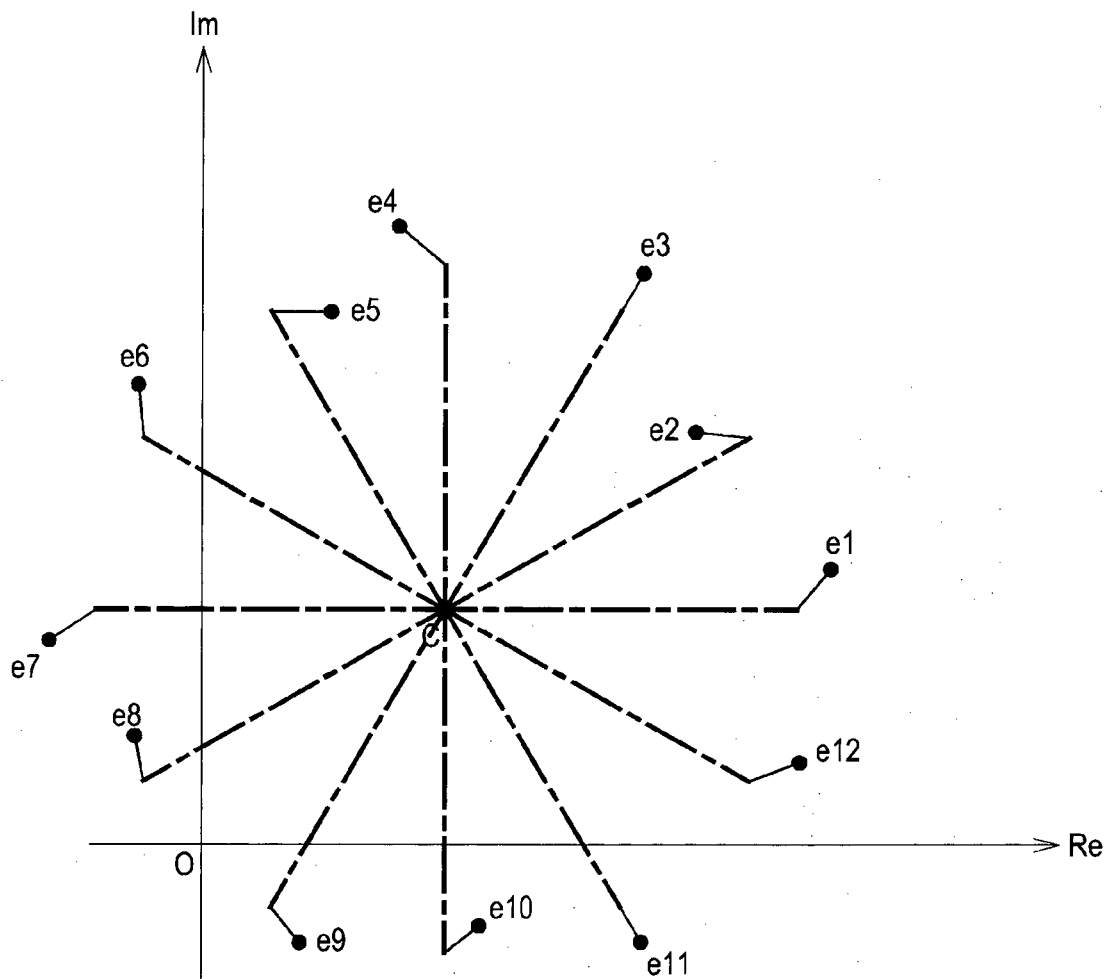


FIG. 10

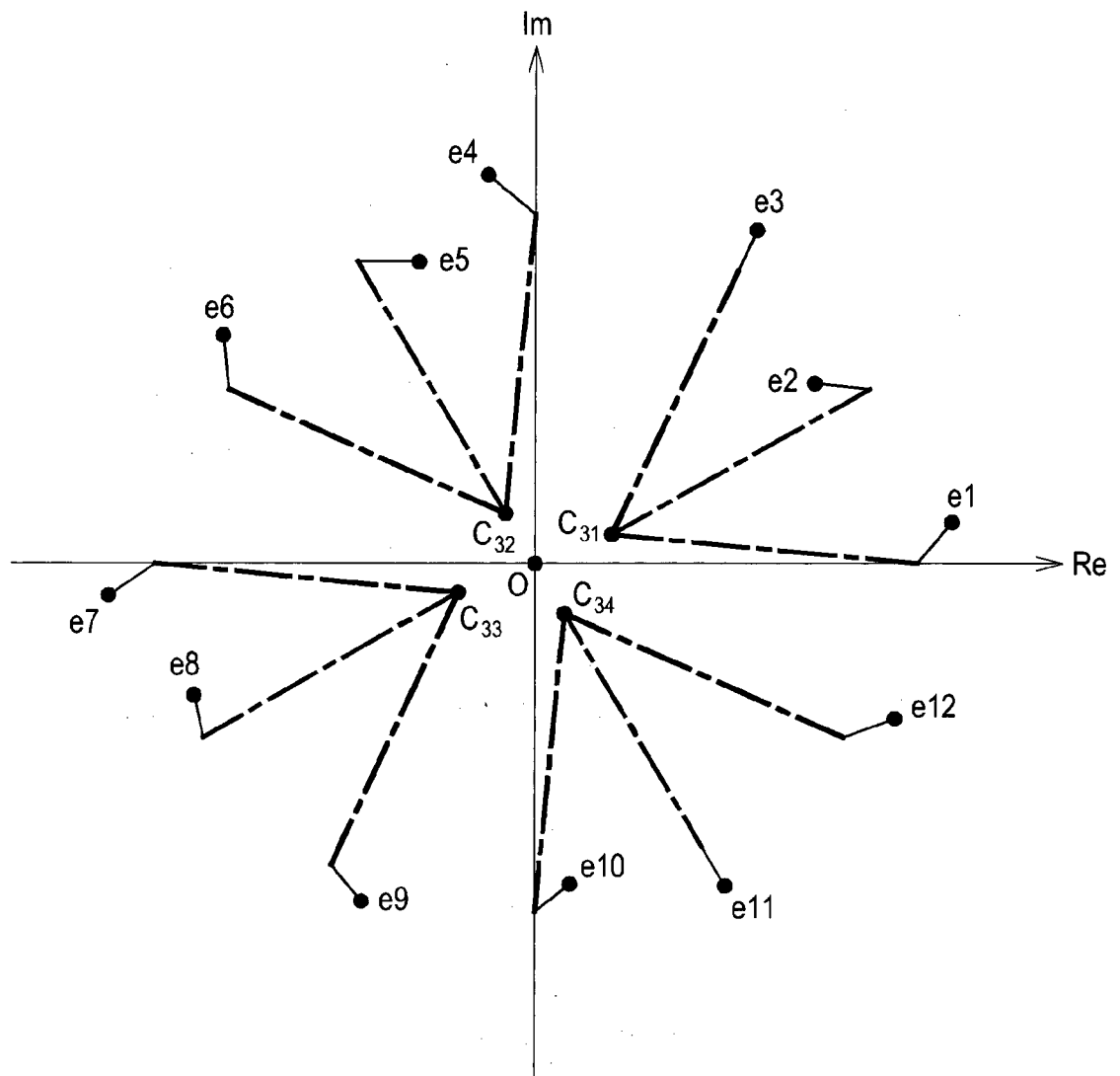


FIG. 11

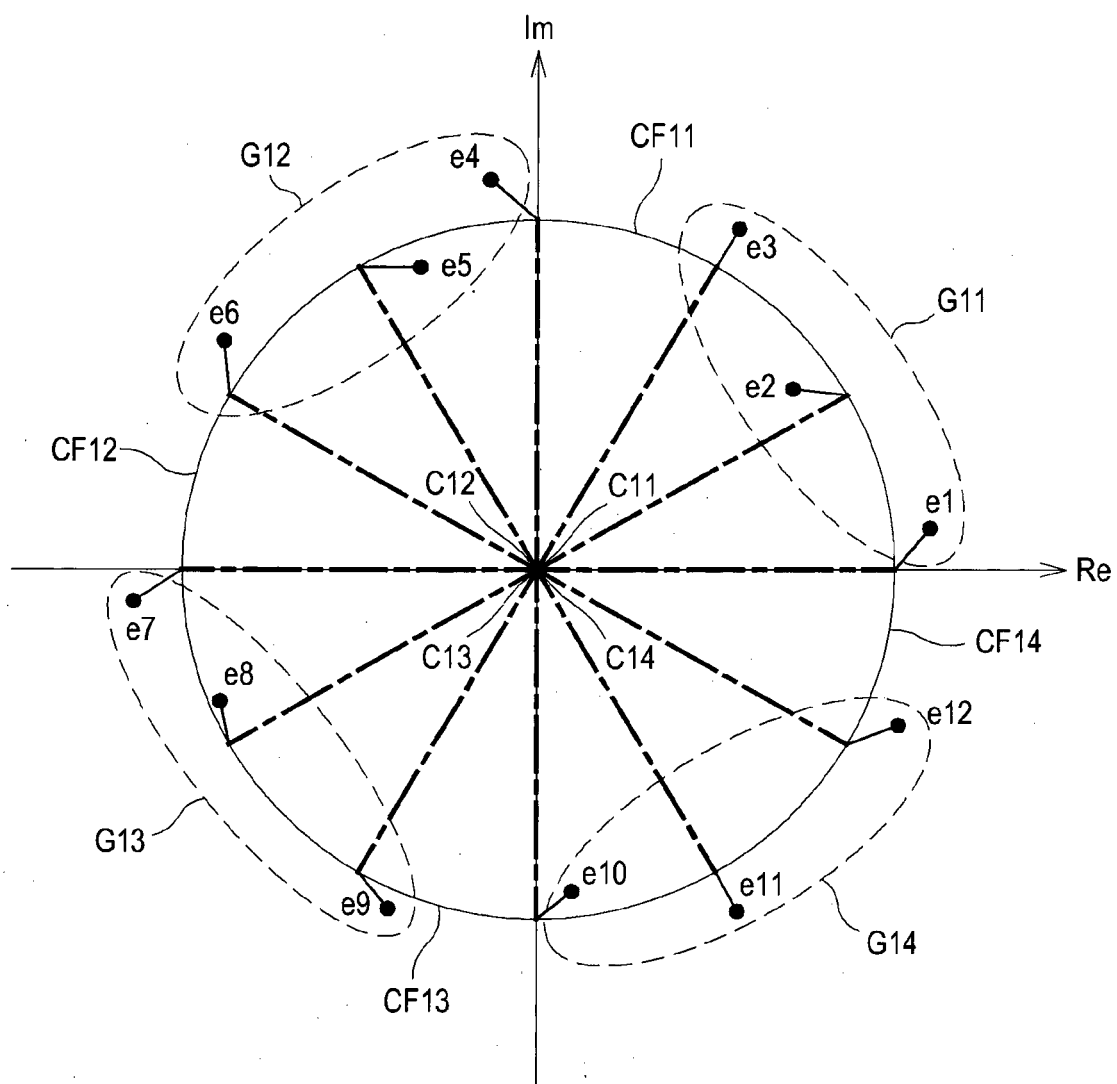


FIG. 12

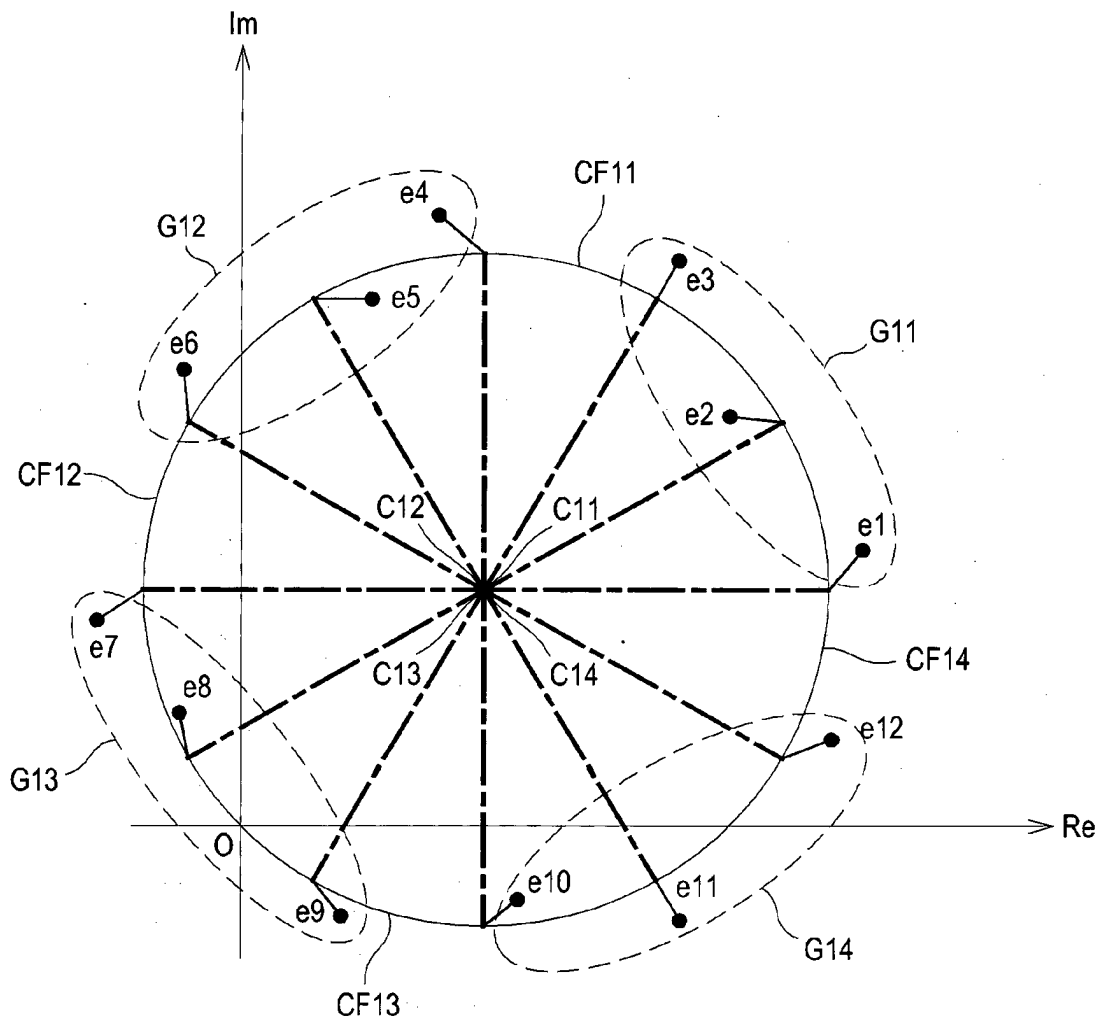


FIG. 13

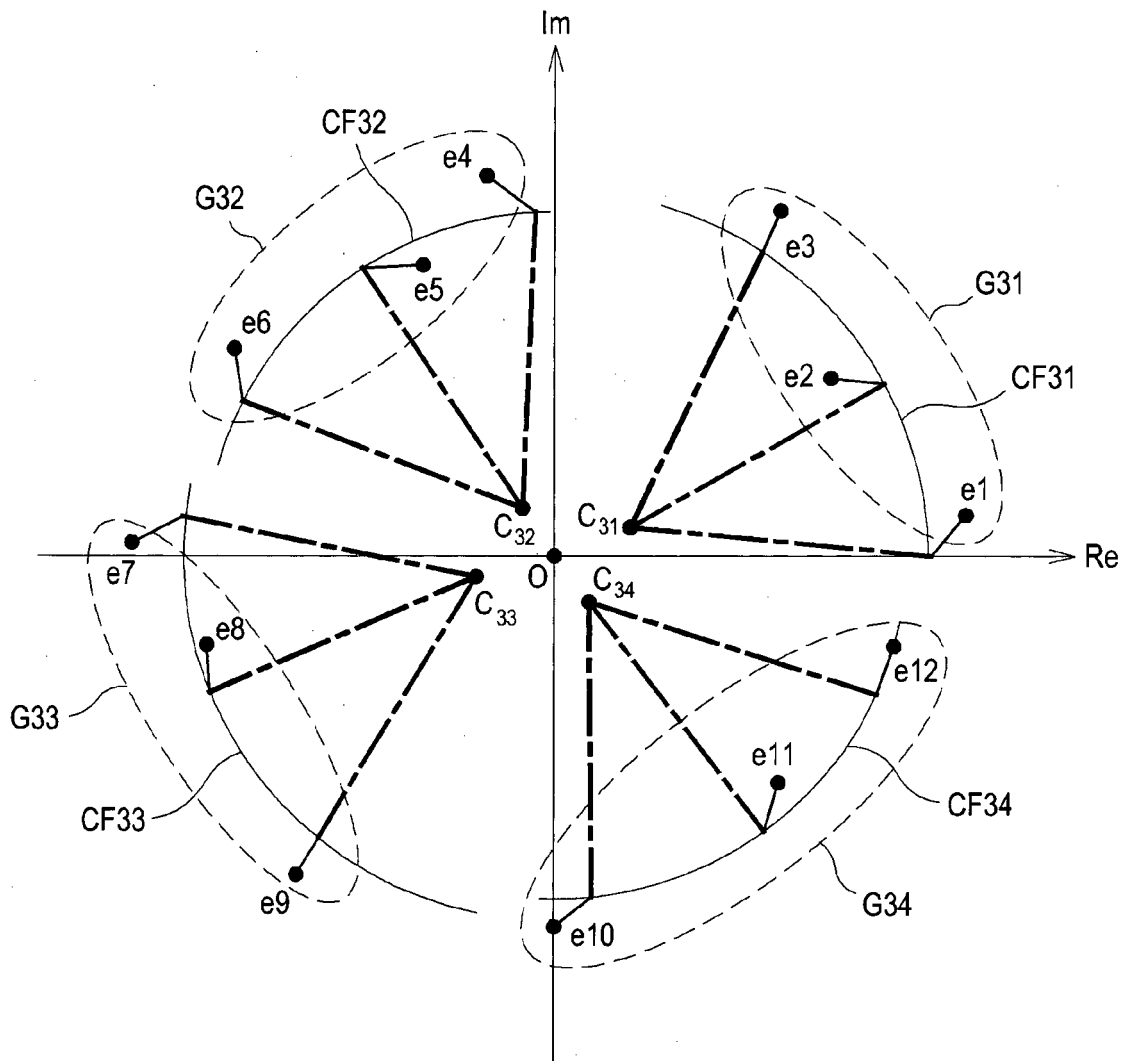


FIG. 14

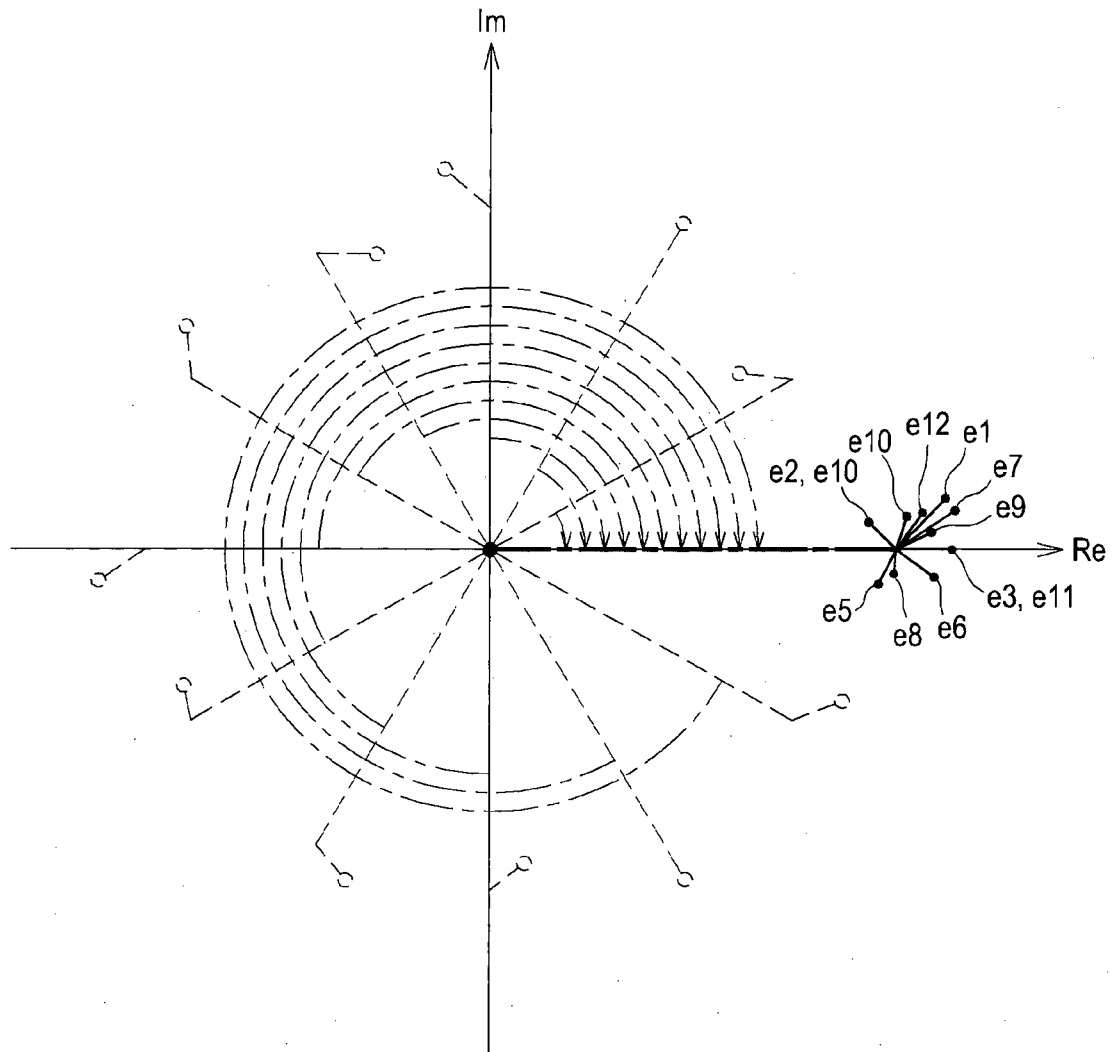
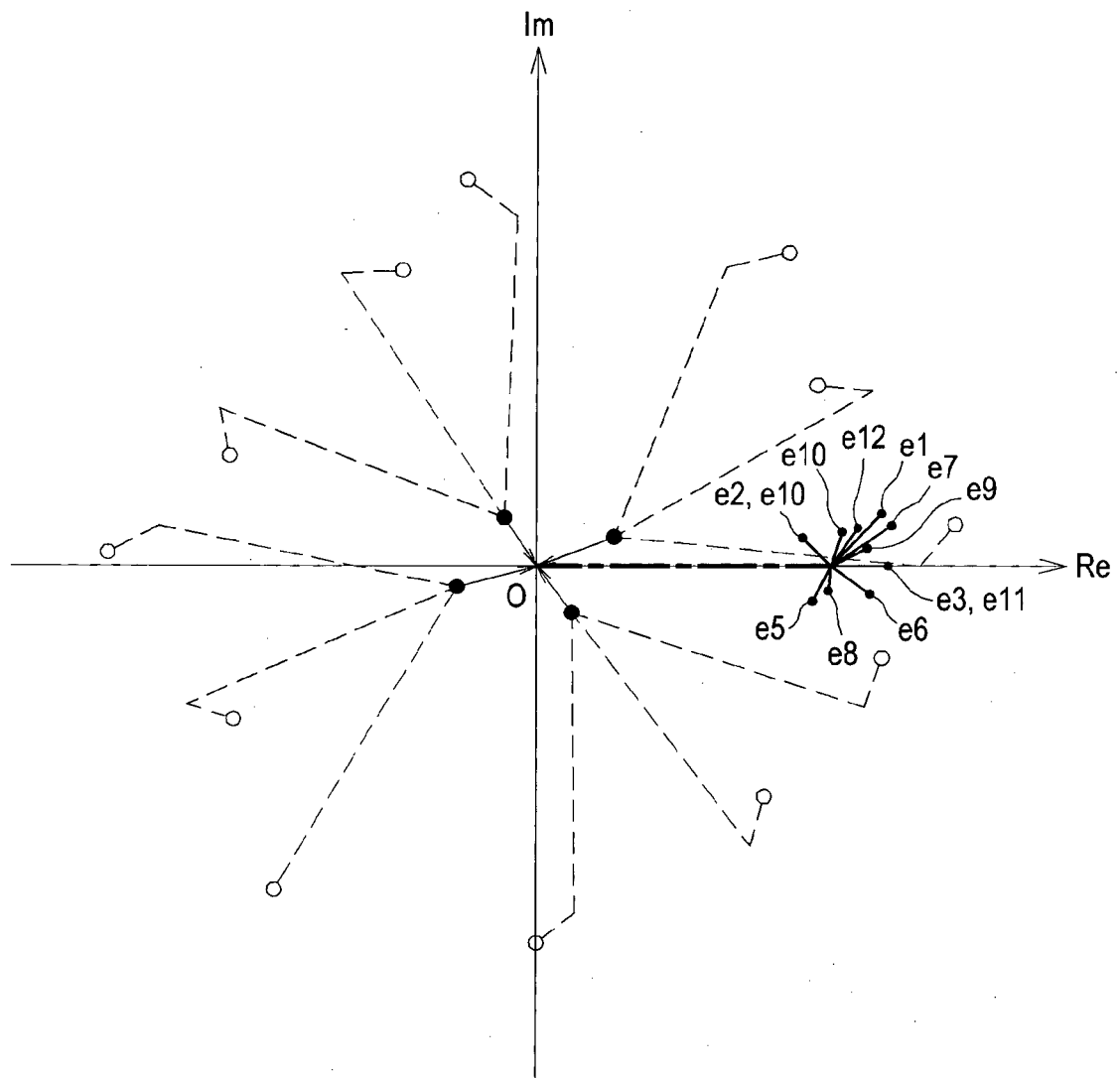


FIG. 16



REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- EP 0481691 A1 [0009]
- US 5226420 A [0010]
- EP 1548462 A1 [0011]

Non-patent literature cited in the description

- **BYUNG-KWON PARK.** *Arctangent Demodulation With DC Offset Compensation in Quadrature Doppler Radar Receiver Systems* [0012]

专利名称(译)	用于自适应地执行杂波滤波的超声系统和方法		
公开(公告)号	EP2248468B1	公开(公告)日	2014-07-02
申请号	EP2010160837	申请日	2010-04-23
申请(专利权)人(译)	MEDISON CO. , LTD.		
当前申请(专利权)人(译)	三星MEDISON CO. , LTD.		
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发明人	BAE, MOO HO KIM, TAE YUN		
IPC分类号	A61B8/00 G01S15/89		
CPC分类号	G01S15/8981 A61B8/488		
代理机构(译)	SCHMID , WOLFGANG		
优先权	1020090038060 2009-04-30 KR 1020100034064 2010-04-14 KR		
其他公开文献	EP2248468A3 EP2248468A2		
外部链接	Espacenet		

摘要(译)

公开了自适应地执行杂波滤波的实施例。在一个实施例中，作为非限制性示例，超声系统包括：超声数据获取单元，被配置为向目标对象发送超声信号和从目标对象接收超声信号，从而输出多个超声数据以获得彩色多普勒模式图像，其中，目标物体包括组织和血流中的至少一种；处理单元，与超声数据采集单元通信，用于将多个超声数据定位在复平面上，处理单元还用于对位于复平面上的多个超声数据进行圆拟合并且考虑到组织的速度对圆拟合的超声数据执行缩混和杂波滤波。

