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(54) **ACTIVE DISTRIBUTION OF HIGH-VOLTAGE POWER FOR ULTRASOUND TRANSDUCERS**

AKTIVE VERTEILUNG VON HOCHSPANNUNGSLEISTUNG FÜR ULTRASCHALLWANDLER

DISTRIBUTION ACTIVE D'ÉNERGIE HAUTE TENSION POUR TRANSDUCTEURS
ULTRASONORES

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(56) References cited:

EP-A1- 2 711 092

EP-A2- 1 445 624

WO-A2-2013/179179

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Description

[0001] This invention relates to medical diagnostic ultrasonic imaging and, in particular, to powering ultrasonic transducer probes.

[0002] Ultrasound transducer probes, such as those used for 3D imaging, can have transmit circuitry located in the probe and coupled to the transducer array (sensor) which excites the transducer elements with energy from power supplies located in ultrasound system. For some imaging modalities, such as shear-wave elastography or PW Doppler, and for probes used for therapeutic applications, the front-end circuitry can require higher electrical currents than the system power supplies are capable of supplying. An attempt by a probe to draw these high currents can result in a decline of the voltage level of the high-voltage supply which provides drive voltage to the front-end and the transducer, which in turn results in a drop in the acoustic pressure of the transmitted ultrasound, which degrades imaging and therapeutic effect. One approach to compensating for this problem is a passive approach, which is to couple a large capacitance to the high voltage supply line. International patent publication WO 2013/179179 describes the use of a large capacitor bank (100 μ F to >1000 μ F) coupled to the probe's high voltage supply line and located in either the ultrasound system mainframe, the transducer's system connector, and/or in the probe case. When the probe begins to draw excessive current during a transmit phase, the charge stored in the capacitor bank supplements that from the power supply, maintaining the desired voltage level.

[0003] This approach is not without its drawbacks, however, which involve the placement of a physically sizeable capacitor bank. When it is desired to locate the capacitor bank in the probe itself, the amount of space available is limited for ergonomic reasons and possibly also the probe's application, e.g., a TEE probe which needs to fit in the esophagus. When it is desired to locate the capacitor bank in the transducer's connector, the physical size of the capacitor bank is better accommodated, but the electrical resistance of the transducer cable becomes a constraining factor. For example, if the imaging modality can tolerate a 1 volt decline during a transmit pulse that requires 5A, the cable resistance needs to be less than 0.2 Ω . If a typical two-meter long cable for a 3D transducer probe distributes transmit power through a pair of conductors with a resistance of 2 ohms, the voltage drop caused by the cable is ten times that of an acceptable decline. This could be overcome by increasing the number of or diameter of the cable conductors, but this would make the cable less flexible, more expensive, and require the development of a new cable. It can also increase the size of the wire connectors at the ends of the cable.

[0004] The EP 1 445 624 A2 describes a ultrasonic diagnostic apparatus for the purpose of reducing the size and power consumption of a power source. This ultra-

sonic diagnostic apparatus comprises a charge pump circuits connected to a transmitter power source. A regulator in the transmitter power source drives the charge pump circuit to generate a positive bias voltage +HV2 higher than a positive voltage +HV1 generated by the transmitter power source. The regulator in the transmitter power source also drives the charge pump circuit to generate a negative bias voltage -HV2 lower than a negative voltage -HV1 generated by the transmitter power source.

[0005] The EP 2 711 092 A1 provides a transformer-free ultrasonic generator for generating ultrasound, preferably for a hand-held device to fix a body on a substrate by ultrasonic welding. The ultrasonic generator comprises: a power amplifier for amplifying an electrical power supply signal; and a pulse generator for generating a pulsed control signal for controlling pulsed power amplifier such that power amplifier generates a pulsed drive signal as an amplified electric signal supply for driving an ultrasonic transducer.

[0006] Accordingly it is desirable to solve the high-current voltage drop problem without compromising other aspects of the ultrasound system and probe.

[0007] In some aspects, the present invention includes ultrasound imaging systems including an active supply provides power to the array transducer in an ultrasound probe. For example, the ultrasound imaging systems can include an ultrasonic transducer located in a probe enclosure, an active supply, having an input coupled to a high voltage supply and an output coupled to the ultrasonic transducer, and a voltage feedback line coupled between the ultrasonic transducer and the active supply. The active supply can be configured to adjust an output voltage supplied to the ultrasonic transducer based on a feedback voltage from the voltage feedback line.

[0008] In certain aspects, the active supply, which supplies energy to the probe through conductors in the transducer cable, may be located a various places in the imaging system, such as in an ultrasound system mainframe, the transducer probe itself, or in the transducer probe's connector.

[0009] According to the present invention, the active high voltage supply is coupled to a capacitor bank, which is charged to a higher voltage. The capacitor bank can discharge by tens of volts during operation, but the active supply maintains the voltage at the transducer front end within a higher range that is acceptable for imaging. The active supply receives feedback from a point closer to the sensor in the signal path and an error amplifier compares the feedback signal to a reference either generated on the connector or provided by the ultrasound system. In response to the error amplifier output, the active supply changes its output to compensate for the change in the load presented by the front end sensor. The capacitor bank stores enough charge for the active supply to provide the current needed by the sensor throughout the duration of the transmit excitation. The voltage of the capacitor bank can be high enough for the active supply to maintain the desired voltage at the transducer through

the transmit interval. The use of the active supply allows use of the capacitor bank on the order of hundreds of microfarads instead of thousands as in the passive case, because its voltage decline can be many more volts than the voltage at the transducer front-end.

[0010] In the drawings:

FIGURE 1 is a schematic diagram of an ultrasound system constructed in accordance with the principles of the present invention.

FIGURE 2 illustrates a probe with its cable and connector for an ultrasound system mainframe.

FIGURES 3a and 3b illustrate schematic implementations of the present invention for positive and negative supply voltages.

FIGURE 4 illustrates voltage and current levels during a transmit pulse at different points in an implementation of the present invention.

FIGURE 5 is a schematic diagram of an active supply constructed in accordance with the principles of the present invention.

FIGURE 6 is a block diagram of the supply of probe power using multiple active supplies.

FIGURE 7 is a block diagram of another implementation of the supply of probe power using multiple active supplies.

[0011] Referring first to FIGURE 1, an ultrasound imaging system constructed in accordance with the principles of the present invention is shown in block diagram form. An ultrasound probe enclosure 10 is provided which is to be held by its handle section 8 with its distal end 6 against the body of a patient to image the anatomy below the point of contact. An array transducer inside the distal end 6 of the probe enclosure transmits focused pulses or waves along directions referred to as beam directions over a two or three dimensional region of the body. This region is shown as a sector-shaped plane 12 in FIGURE 1. Transmission is accomplished by applying high voltage pulses or waveforms to elements of the array transducer by transmitters located in the probe or an ultrasound system mainframe, to which the probe can be connected by a cable 24 or wirelessly. Echoes are returned from tissue, blood and structures along the beam directions in response to each transmission and the echoes are processed by beamforming with a system beamformer 14 to form coherent echo signals from the ultrasound signals received by elements of the array transducer. Some or all of the beamforming may also be performed by a microbeamformer ASIC located in the probe and coupled to the array transducer. After the received signals have been fully beamformed they are coupled to a signal processor 16 which performs functions such as decimation, filtering, harmonic separation, and signal compounding. The processed signals are coupled to an image processor 18 which forms them into images by processes such as amplitude or Doppler detection and scan conversion. The formed images are displayed on

an image display 20.

[0012] The system includes a power supply 22 which provides a number of voltages used to energize the various components of the ultrasound system. The power supply 22 can be coupled to an active supply 40 as described further herein and can provide a high voltage (e.g., ~100v) for use by the transmitter circuits to stimulate the transducer elements to transmit pulses or waves for imaging or therapy. The high voltage can be applied to transmitters in the system mainframe and/or transmitters in the probe 10.

[0013] In some aspects, an ultrasound system mainframe is included in the system and is operable with a number of different types of probes for different diagnostic applications. For this purpose the system mainframe can include one or more connectors to which probes may be connected. FIGURE 2 illustrates a probe 10 with a connector 30 at the proximal end of the cable 24. Strain reliefs 26 prevent excessive flexing at the ends of the cable where it is attached to the probe and probe connector. The probe connector 30 comprises a case which contains a multipin plug to which the conductors of the cable are connected. The plug is indicated at 36. To attach the probe to the system mainframe, the plug 36 is plugged into a mating connector on the ultrasound system and a lock handle 34 is turned to securely attach it to the system.

[0014] As previously mentioned, the demands on the high voltage supply when driving the transducer elements in some applications can cause the voltage to be drawn down during high transmit current demands. The decline in the supply voltage will provide a lower than desired voltage level at the probe sensor, which in turn will produce transmit signals of less than the desired acoustic pressure. The use of capacitor banks to supplement the high voltage supply during these transmit intervals faces the limitations described above. In accordance with the principles of the present invention, an active supply 40 is used to provide a high voltage to the sensor as illustrated in FIGURES 3a and 3b. An active approach for supplying transmit energy can achieve the same supply voltage performance as the passive capacitor bank approach, but with less capacitance (e.g., about 90% less capacitance) and, as a result, a much smaller space requirement in the probe or system. Thus, an active supply and its capacitance can readily fit in several parts of an ultrasound system, including the probe, the system mainframe, and most conventional probe connectors. Furthermore, the active approach can use existing transducer cable designs. FIGURE 3a shows a simplified block diagram of an active supply for a transmitter in a transducer probe 10. In this implementation the active supply 40 is located in the transducer connector 30 and supplies energy through conductors in the transducer cable 24. The active high voltage supply 40 is powered by a high voltage (+HV IN) from the power supply 22, which is applied to a capacitor C1 at the input of the active supply. The power supply charges the capacitor C1 to the high supply volt-

age. The capacitor C1 can discharge by tens of volts during operation, but the active supply maintains the voltage at the probe's front end sensor 50 within a tighter range that is acceptable for imaging and therapy. The active supply receives feedback from the sensor along a voltage feedback line, and compares the feedback voltage in the circuitry to a reference voltage either generated in the connector 30 or provided by the ultrasound system mainframe. One example of how the active supply compares the feedback voltage is explained with respect to the circuit in FIGURE 5 below. In response to a change in the feedback signal, the active supply varies its output to compensate for the change in the load presented by the sensor. The capacitor C1 stores enough charge for the active supply 40 to provide the current needed by the sensor 50 and its bypass capacitance 52 for the duration of the transmit excitation period. The voltage at the capacitor C1 only needs to be high enough for the active supply to maintain the voltage at the sensor through the transmit interval. The capacitor C1 can be on the order of hundreds of microfarads instead of thousands as in the passive case, because it can drop by many more volts than the actively controlled voltage at the sensor front-end.

[0015] It should be noted that the active supply can provide either a positive or a negative high voltage and that the sensor load can source or sink current. A sensor (e.g., a voltage sensing device) may utilize one or both polarities of high voltage. FIGURE 3b schematically illustrates the same arrangement as FIGURE 3a but for a sensor requiring a negative (-HV) drive voltage. A negative high voltage is applied to the capacitor C1 at the input to the active supply 40, and the current flow is in the opposite sense as indicated by the direction of the arrow in the symbol for the sensor 50.

[0016] FIGURE 4 illustrates exemplary waveforms at points in the circuit of FIGURE 3b during the supply of a high negative transmit voltage. In this example the input to the active supply 40 is -77V, the voltage at the sensor 50 is maintained to within 1V of -60V during a transmit interval of less than one millisecond, during which 5 amps (A) is drawn by the sensor. The capacitor C1 has a value of 300 μ F and the voltage at the input to the active supply drops by 10V, from -77V to -67V as shown by curve 60. Negative feedback from the sense conductor of the cable 24 forces the active supply 40 to decrease the voltage at the connector end of the supply conductor of the cable 24 to compensate for the voltage drop over the cable when the sensor sinks 5A into the cable. This is shown by curve 62, where the nominal -60V is changed to -62.5V to account for the cable's voltage drop. Curve 64 shows the voltage change at the sensor, which is from -60V to -59V, an acceptable one volt decline, which occurs when the sensor is drawing 5A as shown by curve 66. The capability of sinking 5A at -60V during the transmit interval is something that the typical ultrasound system power supply cannot do with this performance.

[0017] An exemplary schematic for an active supply of

the present invention having the performance illustrated in FIGURE 4 is shown in FIGURE 5. The active supply in this example is implemented as a high voltage linear regulator. It will be understood that switching supplies can also be used. The linear regulator as shown receives negative feedback from the sensor 50 at terminal FB, which enables it to maintain an approximately constant voltage at the feedback point, as the load and its input voltage vary. Since the high voltage supply -HV coupled to the input terminal IN of the linear regulator cannot sink 5A, the negative voltage on the capacitor C1 will rise towards 0V during the load (transmit) interval.

[0018] The regulator compensates for the change in load and its input voltage variation by varying the drain to source resistance of its NMOS pass transistor M1. A feedback network consisting of resistors R1 and R2 sets the voltage to be produced for the supply conductor(s) at the output terminal OUT to be approximately equal to a reference voltage Ref. supplied by the ultrasound system, multiplied by -1. Transistors Q1 and Q2 form an operational transconductance amplifier. The current output of Q1 drives the gate of the pass transistor M1 to a voltage which is set by resistor R4, thereby controlling the resistance between the input voltage to the regulator and the supply conductor(s). If the amount of current that the load sinks into the supply increases, the voltage at the regulator output increases, which decreases the base-emitter voltage of transistor Q2. This causes the collector-emitter current of transistor Q2 to decrease and collector-emitter current of transistor Q1 to increase, which raises the gate-source voltage of pass transistor M1. The increased gate-source voltage lowers the drain-source resistance of pass transistor M1, which is in series with the input supply to the regulator and its output, resulting in a lower output voltage.

[0019] Similarly, if the sensor load decreases, the voltage at the regulator output will decrease, which increases the bias of Q2 and results in an increase in the conductivity of Q2 and a decrease in the conductivity of Q1. This decreases the gate drive of the pass transistor, which raises its drain-source resistance and increases the output voltage of the regulator. The same mechanism causes the drain-source resistance of the pass transistor M1 to decrease as the input voltage to the regulator decreases; and increase as the input voltage increases when the high voltage system recharges the capacitor C1. Hence, the linear regulator holds the voltage at a set voltage as the load and its input voltage vary.

[0020] There is a discharge circuit in series with the ultrasound system and the linear regulator. The discharge circuit protects the ultrasound system from being back-driven by capacitor C1 when the negative high voltage supply is raised towards 0v. The discharge circuit also prevents a shock hazard which could occur if the capacitor C1 were directly connected to the probe connector 30. Diodes D1 and D2 become reverse-biased when -HV is increased by the system, or disconnected. The Q3 transistor then develops a positive bias on its

base and drives the base of transistor Q4, which causes Q4 to discharge the capacitor C1 through R7 and transistor Q4.

[0021] In order to image with transducer excitations of different voltages, an implementation of the present invention can employ multiple active supplies 40 and switches 44a, b, and c to change the actively controlled high voltages for the transducer when the excitation voltage changes. This is illustrated in FIGURE 6. The illustrated switching arrangement switches both the supply conductor and the sense line connections. The active supplies 40 are shown with a single capacitor C1. FIGURE 7 shows the same multiple excitation voltage implementation, but with different charge storage capacitors C1 for the different active supplies 40. Switches 42a, b and c selectively couple the system high voltage HV to the capacitors C1.

Claims

1. An ultrasound imaging system, comprising:

an ultrasonic transducer located in a probe enclosure (10);
 an active supply (40), having an input coupled to a high voltage supply and an output coupled to the ultrasonic transducer;
 a capacitor (C1) coupled to the input of the active supply (40); and
 a voltage feedback line coupled to the ultrasonic transducer and to the active supply (40),
 wherein the active supply (40) is configured to adjust an output voltage supplied to the ultrasonic transducer based on a feedback voltage from the voltage feedback line.

2. The ultrasound imaging system of Claim 1, comprising a reference voltage source coupled to the active supply (40).

3. The ultrasound imaging system of Claim 1, comprising a probe connector (30) coupled to an end of a probe cable (24) coupled to the probe enclosure (10), wherein the active supply (40) is located in the probe connector (30).

4. The ultrasound imaging system of Claim 3, wherein the capacitor (C1) is located in the probe connector (30) .

5. The ultrasound imaging system of Claim 4, wherein the probe cable (24) comprises a high voltage supply conductor coupled between the active supply (40) and the ultrasonic transducer, wherein the voltage feedback line is located in the probe cable (24), and wherein the high voltage supply is located in an ultrasound system mainframe.

6. The ultrasound imaging system of Claim 1, wherein the active supply (40) comprises an operational transconductance amplifier configured to adjust the output voltage supplied to the ultrasonic transducer based on the feedback voltage from the voltage feedback line.

7. The ultrasound imaging system of Claim 6, comprising a pass transistor (M1) configured to control conduction between the capacitor (C1) and the active supply output.

8. The ultrasound imaging system of Claim 1, comprising a transmitter coupled to the ultrasonic transducer, wherein the active supply (40) is coupled to provide high voltage to the transmitter.

9. The ultrasound imaging system of Claim 1, wherein the active supply (40) is located in the probe enclosure (10).

10. The ultrasound imaging system of Claim 1, wherein the active supply (40) is located in an ultrasound system mainframe.

11. The ultrasound imaging system of Claim 1, wherein the active supply (40) further comprises a discharge circuit, coupled to the capacitor, to discharge the capacitor when the probe is disconnected from the system mainframe.

12. The ultrasound imaging system of Claim 1, wherein the active supply (40) is configured to output a first high voltage to the ultrasonic transducer; and the system further comprises: a second active supply (40) having an input coupled to the high voltage supply and an output coupled to the ultrasonic transducer such that the active supply (40) is configured to provide a second high voltage to the ultrasonic transducer.

13. The ultrasound imaging system of Claim 12, further comprising a switch (42a, 42b, 42c) coupled between the high voltage supply and the input to each active supply (40) .

14. The ultrasound imaging system of Claim 12, further comprising a switch located between the output of each active supply (40) and the ultrasonic transducer, and a switch located between a feedback input of each active supply (40) and the ultrasonic transducer.

Patentansprüche

1. Ultraschallbildgebungssystem, umfassend:

- einen Ultraschallwandler, der sich in einem Sondengehäuse (10) befindet;
 eine aktive Zuführung (40), die einen mit einer Hochspannungszuführung gekoppelten Eingang und einen mit dem Ultraschallwandler gekoppelten Ausgang aufweist;
 einen Kondensator (C1), der mit dem Eingang der aktiven Zuführung (40) gekoppelt ist; und
 eine Spannungsrückmeldungsleitung, die mit dem Ultraschallwandler und der aktiven Zuführung (40) gekoppelt ist,
 wobei die aktive Zuführung (40) konfiguriert ist, um eine dem Ultraschallwandler zugeführte Ausgangsspannung basierend auf einer Rückmeldungsspannung von der Spannungsrückmeldungsleitung anzupassen.
2. Ultraschallbildgebungssystem nach Anspruch 1, umfassend eine mit der aktiven Zuführung (40) gekoppelte Referenzspannungsquelle.
 3. Ultraschallbildgebungssystem nach Anspruch 1, umfassend einen Sondenanschluss (30), der mit einem Ende eines mit dem Sondengehäuse (10) gekoppelten Sondenkabels (24) gekoppelt ist, wobei sich die aktive Zuführung (40) in dem Sondenanschluss (30) befindet.
 4. Ultraschallbildgebungssystem nach Anspruch 3, wobei sich der Kondensator (C1) in dem Sondenanschluss (30) befindet.
 5. Ultraschallbildgebungssystem nach Anspruch 4, wobei das Sondenkabel (24) einen zwischen die aktive Zuführung (40) und den Ultraschallwandler gekoppelten Hochspannungszuführungsleiter umfasst, wobei sich die Spannungsrückmeldungsleitung in dem Sondenkabel (24) befindet und wobei sich die Hochspannungszuführung in einem Ultraschallsystem-Mainframe befindet.
 6. Ultraschallbildgebungssystem nach Anspruch 1, wobei die aktive Zuführung (40) einen Transkonduktanzverstärker umfasst, der konfiguriert ist, um die dem Ultraschallwandler zugeführte Ausgangsspannung basierend auf der Rückmeldungsspannung von der Spannungsrückmeldungsleitung anzupassen.
 7. Ultraschallbildgebungssystem nach Anspruch 6, umfassend einen Durchgangstransistor (M1), der konfiguriert ist, um die Leitung zwischen dem Kondensator (C1) und dem aktiven Zuführungsausgang zu steuern.
 8. Ultraschallbildgebungssystem nach Anspruch 1, umfassend einen mit dem Ultraschallwandler gekoppelten Sender,
- wobei die aktive Zuführung (40) gekoppelt ist, um Hochspannung an den Sender bereitzustellen.
9. Ultraschallbildgebungssystem nach Anspruch 1, wobei sich die aktive Zuführung (40) in dem Sondengehäuse (10) befindet.
 10. Ultraschallbildgebungssystem nach Anspruch 1, wobei sich die aktive Zuführung (40) in einem Ultraschallsystem-Mainframe befindet.
 11. Ultraschallbildgebungssystem nach Anspruch 1, wobei die aktive Zuführung (40) weiter eine mit dem Kondensator gekoppelte Entladungsschaltung umfasst, um den Kondensator zu entladen, wenn die Sonde von dem System-Mainframe getrennt wird.
 12. Ultraschallbildgebungssystem nach Anspruch 1, wobei die aktive Zuführung (40) konfiguriert ist, um eine erste Hochspannung an den Ultraschallwandler auszugeben; und das System weiter umfasst:
 eine zweite aktive Zuführung (40), die einen mit der Hochspannungszuführung gekoppelten Eingang und einen mit dem Ultraschallwandler gekoppelten Ausgang aufweist, sodass die aktive Zuführung (40) konfiguriert ist, um eine zweite Hochspannung an den Ultraschallwandler bereitzustellen.
 13. Ultraschallbildgebungssystem nach Anspruch 12, weiter umfassend einen zwischen der Hochspannungszuführung und dem Eingang zu jeder aktiven Zuführung (40) gekoppelten Schalter (42a, 42b, 42c).
 14. Ultraschallbildgebungssystem nach Anspruch 12, weiter umfassend einen zwischen dem Ausgang jeder aktiven Zuführung (40) und dem Ultraschallwandler befindlichen Schalter und einen zwischen einem Rückmeldungseingang jeder aktiven Zuführung (40) und dem Ultraschallwandler befindlichen Schalter.

Revendications

1. Système d'imagerie ultrasonore, comprenant :
 un transducteur ultrasonore situé dans un boîtier de sonde (10) ;
 une alimentation active (40), ayant une entrée couplée à une alimentation de haute tension et une sortie couplée au transducteur ultrasonore ;
 un condensateur (C1) couplé à l'entrée de l'alimentation active (40) ; et
 une ligne de rétroaction de tension couplée au transducteur ultrasonore et à l'alimentation active (40),
 dans lequel l'alimentation active (40) est confi-

- gurée pour ajuster une tension de sortie fournie au transducteur ultrasonore sur la base d'une tension de rétroaction à partir de la ligne de rétroaction de tension.
2. Système d'imagerie ultrasonore selon la revendication 1, comprenant une source de tension de référence couplée à l'alimentation active (40). 5
 3. Système d'imagerie ultrasonore selon la revendication 1, comprenant un connecteur de sonde (30) couplé à une extrémité d'un câble de sonde (24) couplé au boîtier de sonde (10), dans lequel l'alimentation active (40) est située dans le connecteur de sonde (30). 10 15
 4. Système d'imagerie ultrasonore selon la revendication 3, dans lequel le condensateur (C1) est situé dans le connecteur de sonde (30). 20
 5. Système d'imagerie ultrasonore selon la revendication 4, dans lequel le câble de sonde (24) comprend un conducteur d'alimentation de haute tension couplé entre l'alimentation active (40) et le transducteur ultrasonore, dans lequel la ligne de rétroaction de tension est située dans le câble de sonde (24), et dans lequel l'alimentation de haute tension est située dans une structure centrale de système ultrasonore. 25
 6. Système d'imagerie ultrasonore selon la revendication 1, dans lequel l'alimentation active (40) comprend un amplificateur opérationnel de transconductance configuré pour ajuster la tension de sortie fournie au transducteur ultrasonore sur la base de la tension de rétroaction à partir de la ligne de rétroaction de tension. 30 35
 7. Système d'imagerie ultrasonore selon la revendication 6, comprenant un transistor de chute (M1) configuré pour réguler la conduction entre le condensateur (C1) et la sortie de l'alimentation active. 40
 8. Système d'imagerie ultrasonore selon la revendication 1, comprenant un transmetteur couplé au transducteur ultrasonore, dans lequel l'alimentation active (40) est couplée pour délivrer une haute tension au transmetteur. 45
 9. Système d'imagerie ultrasonore selon la revendication 1, dans lequel l'alimentation active (40) est située dans le boîtier de sonde (10). 50
 10. Système d'imagerie ultrasonore selon la revendication 1, dans lequel l'alimentation active (40) est située dans une structure centrale de système ultrasonore. 55
 11. Système d'imagerie ultrasonore selon la revendication 1, dans lequel l'alimentation active (40) comprend en outre un circuit de décharge, couplé au condensateur, pour décharger le condensateur lorsque la sonde est déconnectée de la structure principale du système.
 12. Système d'imagerie ultrasonore selon la revendication 1, dans lequel l'alimentation active (40) est configuré pour délivrer en sortie une première haute tension au transducteur ultrasonore ; et le système comprend en outre : une seconde alimentation active (40) ayant une entrée couplée à l'alimentation de haute tension et une sortie couplée au transducteur ultrasonore de telle manière que l'alimentation active (40) est configurée pour délivrer une seconde haute tension au transducteur ultrasonore.
 13. Système d'imagerie ultrasonore selon la revendication 12, comprenant en outre un commutateur (42a, 42b, 42c) couplé entre l'alimentation de haute tension et l'entrée à chaque alimentation active (40).
 14. Système d'imagerie ultrasonore selon la revendication 12, comprenant en outre un commutateur situé entre la sortie de chaque alimentation active (40) et le transducteur ultrasonore, et un commutateur situé entre une entrée de rétroaction de chaque alimentation active (40) et le transducteur ultrasonore.

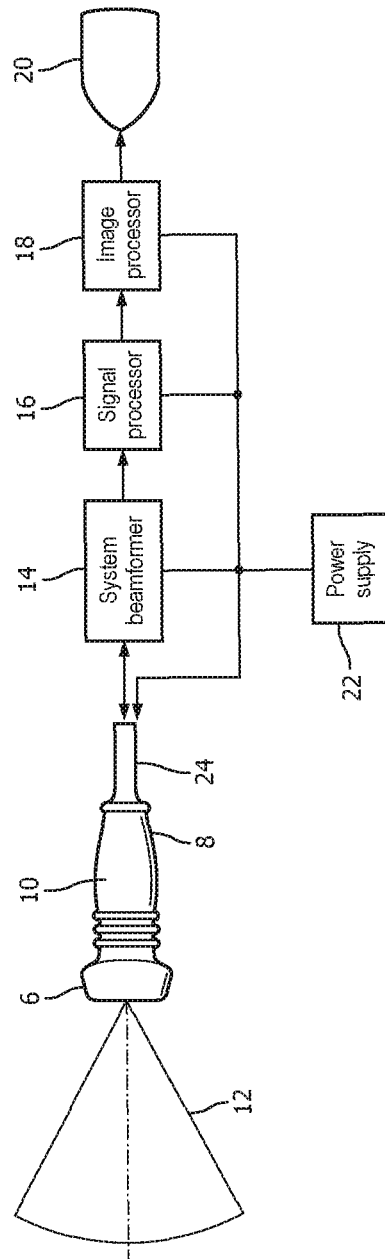


FIG. 1

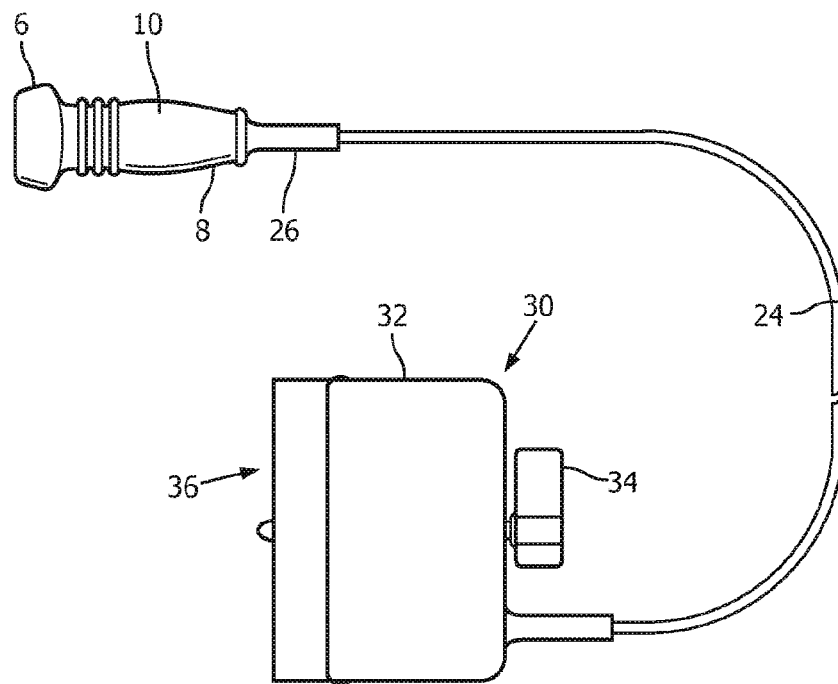


FIG. 2

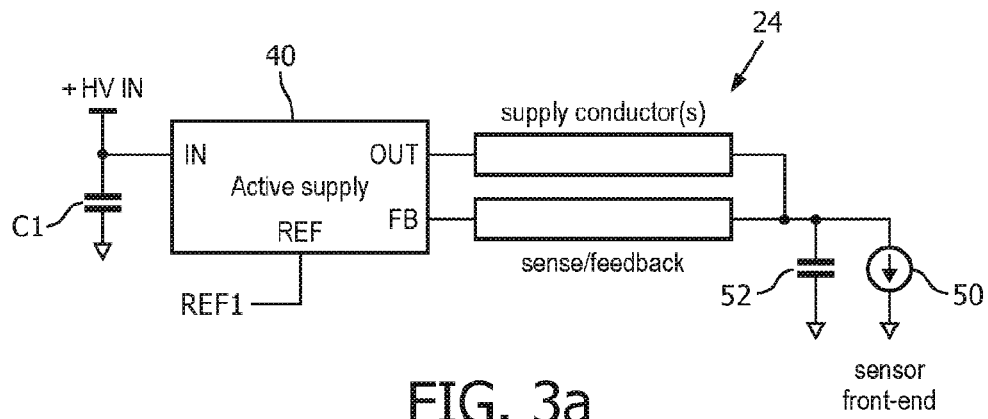


FIG. 3a

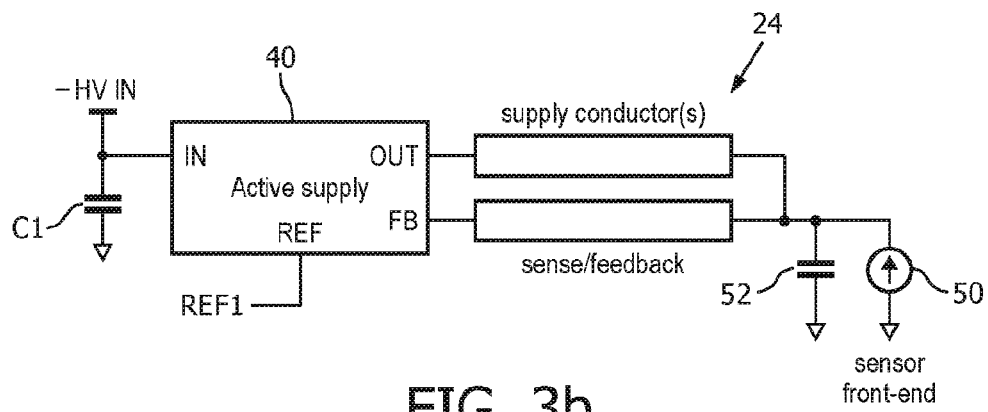
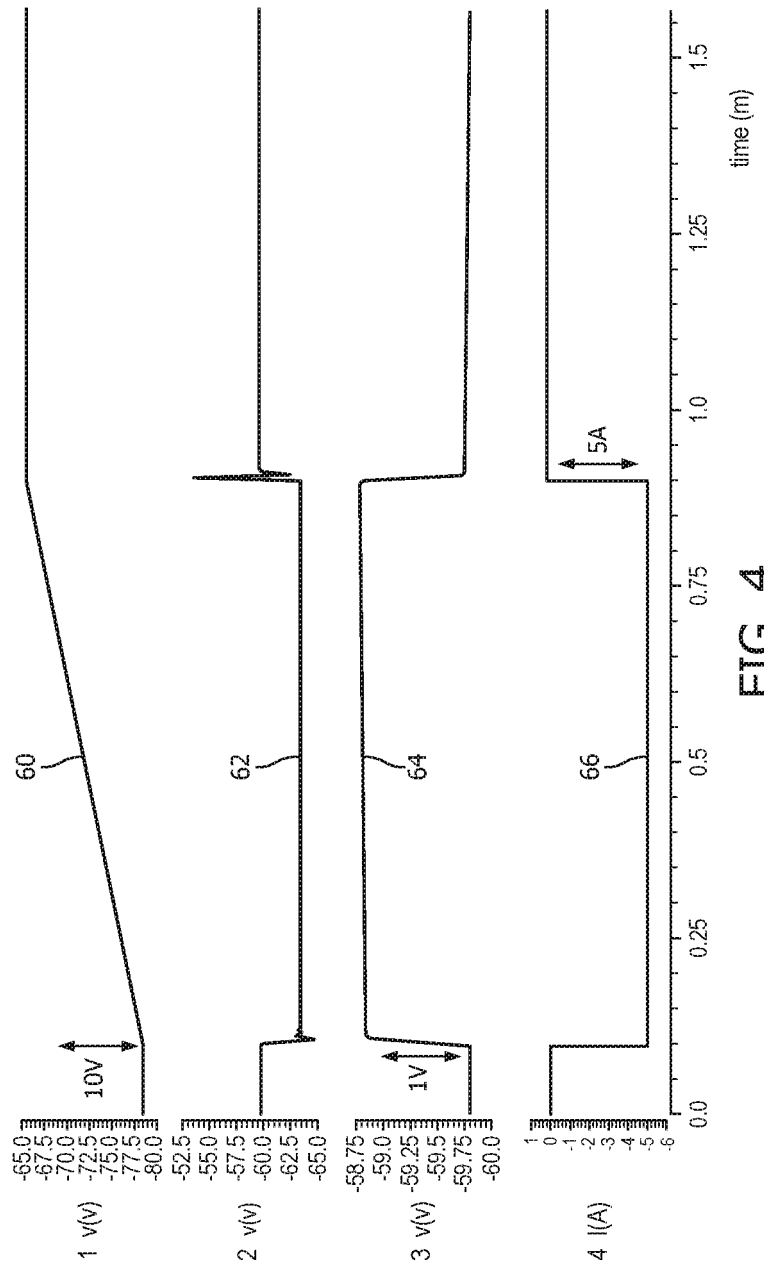


FIG. 3b



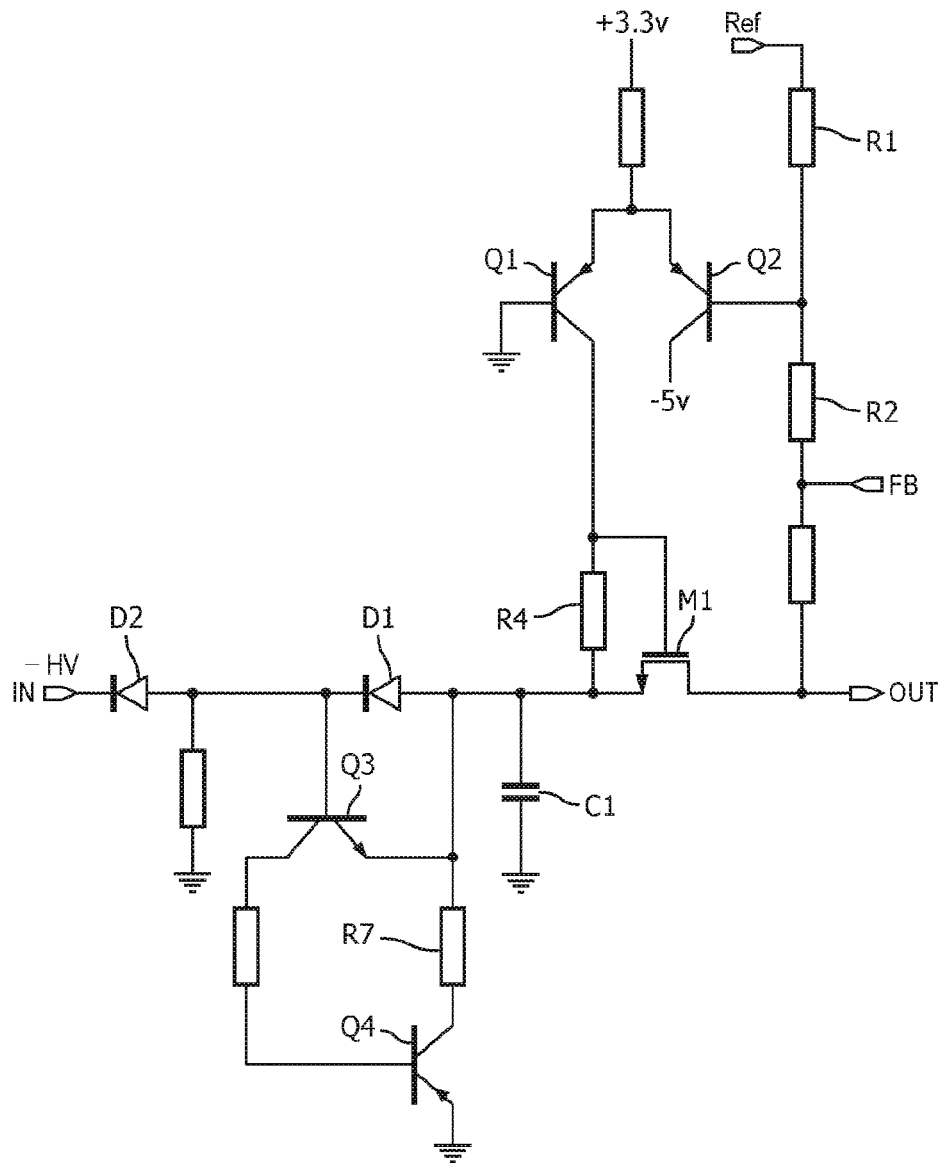


FIG. 5

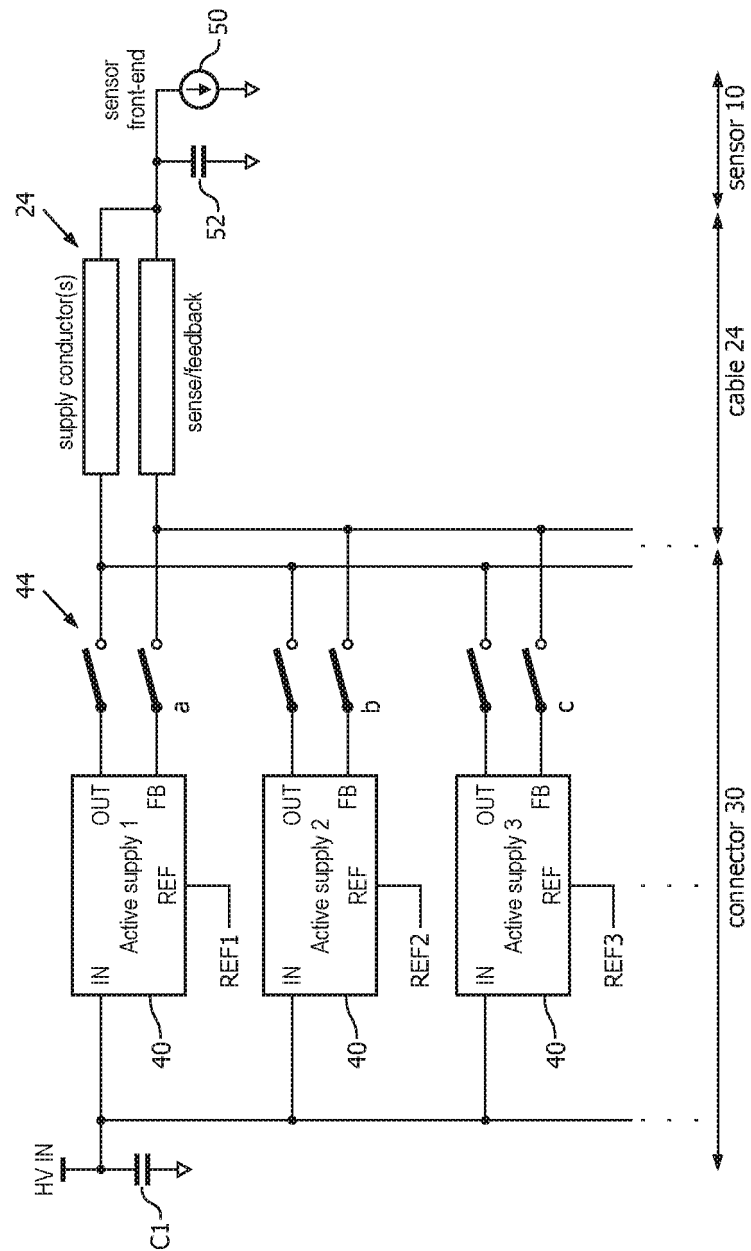
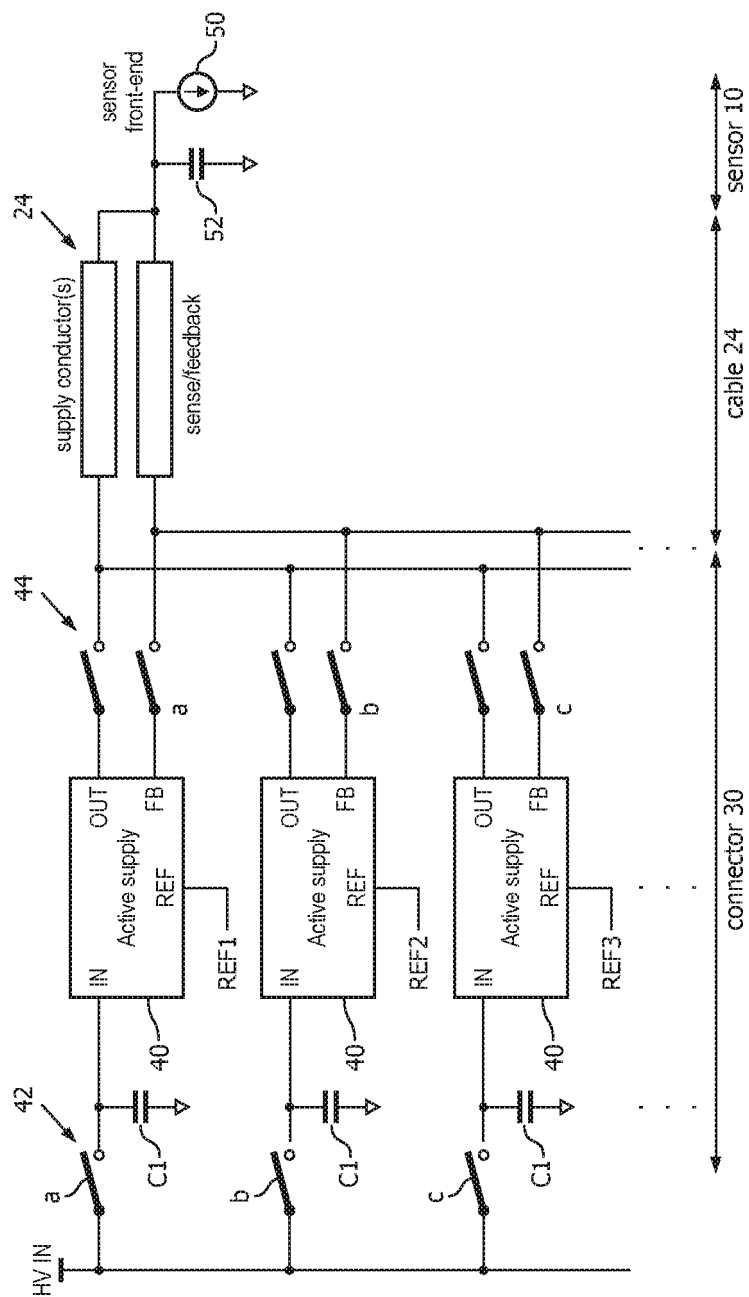


FIG. 6

7. ^{xi} **FIG**

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- WO 2013179179 A [0002]
- EP 1445624 A2 [0004]
- EP 2711092 A1 [0005]

专利名称(译)	超声传感器的高压性能的有源分布		
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[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
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代理机构(译)	飞利浦知识产权及标准		
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其他公开文献	EP3370622A1 EP3370622B8		
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摘要(译)

超声换能器探头的换能器的高压驱动器由有源电源提供，该有源电源通过反馈监视提供给换能器的高压，并在高压传输期间通过将电荷从电容器耦合到电容器来响应电压下降。探头的高压电源线，从而防止高压急剧下降。优选地，有源电源和电容器位于探针连接器外壳中。

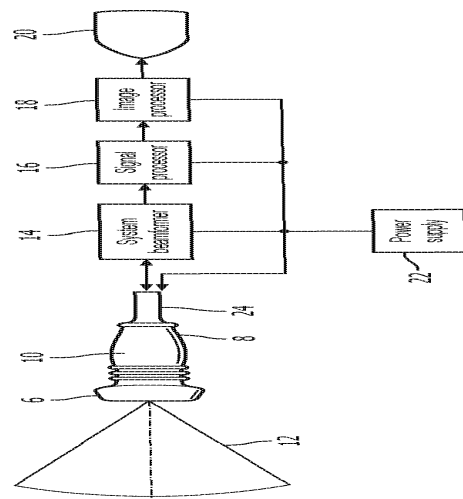


FIG. 1