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(54) **SYSTEMS AND METHODS FOR PROVIDING ULTRASOUND GUIDANCE TO TARGET
STRUCTURES WITHIN A BODY**

SYSTEME UND VERFAHREN ZUR BEREITSTELLUNG VON ULTRASCHALLFÜHRUNG ZU
ZIELSTRUKTUREN INNERHALB EINES KÖRPERS

SYSTÈMES ET PROCÉDÉS DE FOURNITURE DE GUIDAGE ULTRASONORE POUR CIBLER DES
STRUCTURES À L'INTÉRIEUR D'UN CORPS

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Description

FIELD OF THE INVENTION

[0001] This invention relates generally to ultrasound probes and, more particularly, to an ultrasound probe having guidance light sources and methods of directing an instrument from a surface to a target structure beneath the surface.

BACKGROUND

[0002] Ultrasound is a medical imaging tool that, in certain implementations, permits health care practitioners to locate and visualize internal bodily structures, such as blood vessels and internal organs. When these internal structures need to be accessed, ultrasound is sometimes used to direct an instrument toward the target structure. For example, ultrasound may be used for to assist with venous line placement, arterial line placement, biopsy, drainage, ablation, or other interventions.

[0003] Unfortunately, despite the improvements in ultrasound technology, as well as training and operator skills, it is still difficult to reliably and continuously direct the instrument to the target structure without complications. While an improvement over unguided approaches, current ultrasound probes are still limited in the guidance that they provide.

[0004] It should be appreciated that there is a need for an ultrasound probe that enables health care practitioners to safely perform procedures involving internal bodily structures with greater ease and accuracy and fewer complications. The probe should reliably and continuously direct an instrument from a surface to a target structure beneath the surface. The present invention fulfills these needs and provides further related advantages.

BRIEF SUMMARY OF THE INVENTION

[0005] The present invention is embodied in an ultrasonic probe, which includes a housing, a first ultrasonic transducer array, a second ultrasonic transducer array, a first light source, and a second light source. The first ultrasonic transducer array is coupled to the housing and configured to emit a first planar ultrasonic beam in a first direction within a first plane. The second ultrasonic transducer array is coupled to the housing and configured to emit a second planar ultrasonic beam in the first direction within a second plane, which is substantially perpendicular to the first plane. The first light source is coupled to the housing and configured to project a first light line substantially within the first plane. The second light source is coupled to the housing and configured to project a second light line within a third plane, which is substantially perpendicular to the first plane and intersects the second plane at an oblique angle. The first light line intersects and is substantially perpendicular to the second light line.

[0006] In one embodiment, the ultrasound probe is embodied in a handheld device. In another embodiment, the

first and second ultrasonic transducer arrays are arranged in a T-shaped configuration.

[0007] In one embodiment, the first light source is a first laser and the second light source is a second laser. In another embodiment, the second laser is configured to project the second light line within the third plane at a projection angle, wherein the projection angle is less than 90°. In an additional embodiment, a stepper motor coupled to the second laser. In a further embodiment, the stepper motor is configured to rotate the second laser and thereby adjust the projection angle, wherein the adjusted projection angle is less than 90°. In yet another embodiment, a position of the second laser relative to the first laser is adjustable.

[0008] In one embodiment, the ultrasound probe further includes a control panel. In another embodiment, the control panel includes a touch screen. In a further embodiment, the ultrasound probe includes a screen coupled to the ultrasound probe and configured to display both a first image from the first ultrasonic transducer array and a second image from the second ultrasonic transducer array. In an additional embodiment, the screen is configured to display a centerline. In another embodiment, the centerline corresponds to a center of the second ultrasonic transducer array. In yet another embodiment, the centerline corresponds to a point of intersection between the first ultrasonic transducer array and the second ultrasonic transducer array.

[0009] In one embodiment, the ultrasound probe further comprises a sterile cover coupled to the ultrasonic probe. In another embodiment, the sterile cover comprises a rigid, optically transparent material configured to be positioned over the first and second light source. In a further embodiment, the sterile cover further comprises a flexible bag coupled to the rigid, optically transparent material.

[0010] The present invention is also embodied in a method of directing an instrument from a surface to a target structure beneath the surface. In one embodiment, the method includes emitting a first planar ultrasonic beam in a first direction within a first plane, emitting a second planar ultrasonic beam in the first direction within a second plane, projecting a first light line substantially within the first plane, projecting a second light line within a third plane, aligning an end of the instrument with a point of entry, aligning a length of the instrument with both a guide path and an angle of entry, and guiding the instrument through the point of entry toward the target structure beneath the surface, while substantially maintaining alignment of the length of the instrument with both the guide path and the angle of entry. The second plane and the third plane are both substantially perpendicular to the first plane. The third plane intersects the second plane at an oblique angle and defines the angle of entry for the instrument. The first light line defines the guide path for the instrument. The second light line intersects and is substantially perpendicular to the first light line,

and a point of intersection between the first light line and the second light line defines the point of entry for the instrument.

[0011] In one embodiment, the method includes displaying both a first image from the first planar ultrasonic beam and a second image from the second planar ultrasonic beam. In a further embodiment, the second image includes a centerline. In another embodiment, the centerline corresponds to a center of the second planar ultrasonic beam. In yet another embodiment, the centerline corresponds to a point of intersection between the first planar ultrasonic beam and the second planar ultrasonic beam.

[0012] In one embodiment, the method includes aligning the second planar ultrasonic beam over the target structure such that the centerline of the second image is substantially centered over the image of the target structure. In another embodiment, the method includes aligning the first planar ultrasonic beam over the target structure such that the target structure is visible in the first image while the centerline of the second image is substantially centered over the target structure.

[0013] In another embodiment, the method includes selecting the target structure on the first or second image. In a further embodiment, the method includes selecting a desired angle of entry. In an additional embodiment, the method includes selecting a desired point of entry on the first image. In yet another embodiment, the method includes selecting both a desired point of entry on the first image and a desired angle of entry.

[0014] In one embodiment, the method includes determining both a vertical and a horizontal distance between the target structure and a light source projecting the second light line. In one embodiment, the method includes calculating a projection angle of the light source required to project the second light line within the third plane such that the third plane is substantially incident a point of intersection between the second plane and the target structure. The projection angle is defined by the equation $\alpha = \arctan(y/x)$, where α is the projection angle, y is the vertical distance between the target structure and the light source, and x is the horizontal distance between the target structure and the light source. In another embodiment, the method includes rotating the light source so as to project the second light line within the third plane substantially at the calculated projection angle.

[0015] In one embodiment, the method includes calculating a position of the light source required to project the second light line within the third plane such that the third plane is substantially incident a point of intersection between the second plane and the target structure. The position is determined from an equation $\tan \alpha = y/x$, where α is a projection angle of the light source, y is the vertical distance between the target structure and the light source, and x is the horizontal distance between the target structure and the light source. In another embodiment, the method includes moving the light source substantially to the calculated position.

[0016] In one embodiment, the method includes the step of calculating both a projection angle and a position of the light source required to project the second light line within the third plane such that the third plane is substantially incident a point of intersection between the second plane and the target structure. The projection angle and position are determined from an equation $\tan \alpha = y/x$, where α is the projection angle, y is the vertical distance between the target structure and the light source, and x is the horizontal distance between the target structure and the light source. In another embodiment, the method includes rotating the light source so as to project the second light line within the third plane substantially at the calculated projection angle, and moving the light source substantially to the calculated position.

[0017] From the Japanese patent application publication JP 2009045427 A a blood vessel imaging apparatus is known for guiding a needle, including a plurality of ultrasonic transducers and a light source.

[0018] The invention's objects are achieved by the features in claim 1 and a method of operating the same. Advantageous further embodiments are claimed in the dependent claims.

[0019] Other features and advantages of the invention should become apparent from the following description of the preferred embodiments, taken in conjunction with the accompanying drawings, which illustrate, by way of example, the principles of the invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0020]

Figure 1 is a top-left perspective view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 2 is a front elevational view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 3 is a top plan view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 4 is a left elevational view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 5 is a bottom-left perspective view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 6 is a bottom plan view of an ultrasound probe in accordance with one embodiment of the present invention.

Figure 7 is a top-left perspective view of an ultra-

sound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a surface.

Figure 8 is a front-right perspective view of an ultrasound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a target structure beneath a surface.

Figure 9 is a left-back perspective view of an ultrasound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a target structure beneath a surface.

Figure 10 is a left side elevational view of an ultrasound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a target structure beneath a surface at a first angle.

Figure 11 is a left side elevational view of an ultrasound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a target structure beneath a surface at a second angle.

Figure 12 is a top plan view of an ultrasound probe in use in accordance with one embodiment of the present invention, the ultrasound probe directing an instrument toward a surface.

Figure 13 is a left side elevational view of an ultrasound probe in accordance with one embodiment of the present invention, showing the ultrasound probe on a surface in relation to a target structure.

Figure 14 is a view of an ultrasound probe and a screen in use to direct an instrument toward a target structure beneath a surface in accordance with one embodiment of the present invention.

Figure 15 is a front elevational view of an ultrasound probe with a sterile cover in accordance with one embodiment of the present invention.

Figure 16 is a left elevational view of an ultrasound probe with a sterile cover in accordance with one embodiment of the present invention.

Figure 17 is a front elevational view of an ultrasound probe and folded sterile cover, in accordance with one embodiment of the present invention, with the sides of the folded sterile cover being shown in cross-section to reveal the folds.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0021] With reference now to Figures 1-6 of the illustrative drawings, there is shown an ultrasound probe 100 in accordance with embodiments of the invention. In one embodiment, the ultrasound probe includes a housing 105, a first ultrasonic transducer array 110, a second ultrasonic transducer array 115, a first light source 120, and a second light source 125.

[0022] In one embodiment, the first ultrasonic transducer array 110 and the second ultrasonic transducer array 115 are enclosed within the housing 105, either directly or indirectly, and are substantially perpendicular to each other. In an additional embodiment, the ultrasonic transducer arrays are arranged in a T-shaped configuration. In a further embodiment, the ultrasonic transducer arrays can be configured in a biplane linear, multiplane, or 3D configuration. In another embodiment, the ultrasonic transducer arrays are configured as linear sequential arrays, linear phased arrays, or curved sequential arrays.

[0023] The first light source 120 and the second light source 125 are coupled to the housing 105. Each of the light sources may be a laser or any other light source capable of emitting a light line within a plane.

[0024] With reference to Figures 7-13, the first ultrasonic transducer array 110 is configured to emit a first planar ultrasonic beam 111 in a first direction 113 within a first plane 112. The second ultrasonic transducer array 115 is configured to emit a second planar ultrasonic beam 116 in the first direction within a second plane 117. The second plane is substantially perpendicular to the first plane. In one embodiment, the first and second planar ultrasonic beams may be swept ultrasonic beams.

[0025] The first light source 120 is configured to project a first light line 121 substantially within the first plane. The second light source 125 is configured to project a second light line 126 within a third plane 127. The third plane is substantially perpendicular to the first plane and intersects the second plane at an oblique angle 128. The first light line intersects and is substantially perpendicular to the second light line.

[0026] The ultrasonic transducer arrays 110, 115 permit a user to visualize a target structure 20 beneath a surface 10. For example, the ultrasound probe 100 may be placed on a patient's skin so as to emit the planar ultrasonic beams 111, 116 through the skin toward a vein beneath the skin. As is well understood by a person of ordinary skill in the art, the transducer arrays are configured to collect reflected ultrasound waves and convert those sound waves into signals that can be used to produce images of the area beneath the transducer arrays.

[0027] With reference to Figure 14, in one embodiment, a screen 150 is coupled to the ultrasound probe 100 and configured to display both a first image 151 from the first ultrasonic transducer array 110 and a second image 152 from the second ultrasonic transducer array

115. In an additional embodiment, the screen is configured to display a centerline 153. In one embodiment, the centerline corresponds to a center 118 (Figures 5 and 6) of the second ultrasonic transducer array. In another embodiment, the centerline corresponds to a point of intersection between the first ultrasonic transducer array and the second ultrasonic transducer array. The screen may be coupled to the ultrasound probe directly or indirectly. For example, the screen may be coupled to the ultrasound probe via a WiFi radio, Bluetooth, Ethernet, USB, or other wired or wireless connection means.

[0028] Because the first and second ultrasound transducer arrays 110 and 115 are configured to emit planar ultrasonic beams 111, 116 in the same direction and within orthogonal planes, the ultrasound probe 100 can be positioned on the surface 10 to provide simultaneous, longitudinal and transverse images of the target structure beneath the surface. In one embodiment, the longitudinal image is the first image 151, which is produced by the first ultrasonic transducer array 110, and the transverse image is the second image 152, which is produced by the second ultrasonic transducer array 115.

[0029] In use, this arrangement can permit a user to visualize the target structure 20 and the position of an instrument 30, such as a needle, in relation to the target structure. More particularly, the first and second images 151, 152 and the optional centerline 153 can be used to facilitate locating the target structure and following the instrument as it travels beneath the surface toward the target structure.

[0030] For example, it can be difficult to obtain and maintain a longitudinal image of small arteries and nerves while it is relatively easy to obtain and maintain a transverse image of these small structures. The combination of the two images allows an operator to use the transverse image as a tool to adjust the position of the ultrasound probe so as to maintain a substantial length of the small artery or nerve within the longitudinal image. More particularly, the operator can adjust the position of the ultrasound probe 100 over the target structure 20 such that the centerline 153 of the transverse image is substantially centered over the target structure. Because, in one embodiment, the centerline corresponds to a point of intersection between the first ultrasonic transducer array 110 and the second ultrasonic transducer array 115, at least part of the target structure should be visible within the longitudinal image closest to the transverse image. To finish alignment, the operator can pivot the ultrasound probe so that a substantial length of the target structure is visible within the longitudinal image.

[0031] With the ultrasound probe 100 so aligned over the target structure 20, the first and second light lines 121, 126 can be used as visual guides to direct the instrument 30 from the surface 10 to the target structure 20 beneath the surface. For example, when the first planar ultrasonic beam 111 is aligned with the target structure, the first light line 121 defines a guide path 121 for the instrument because it is substantially within the first

plane 112 of the first planar ultrasonic beam.

[0032] Similarly, the third plane 127 can be configured to define an angle of entry 129 for the instrument 30, and the intersection 130 between the second light line 126 and the first light line 121 can define a point of entry 130 for the instrument. As discussed above, the second light line is projected within the third plane, which intersects the second plane 117 of the second planar ultrasonic beam 116 at an oblique angle 128. If the third plane intersects the second plane substantially at the point where the second plane intersects the target structure 20, the third plane will define an angle of entry for the instrument 129.

[0033] With the ultrasonic probe so positioned and configured, the operator can align an end of the instrument 30 with the point of entry 130, align a length of the instrument with both the guide path 121 and the angle of entry 129, and guide the instrument through the point of entry toward the target structure 20 beneath the surface 10 while substantially maintaining alignment of the length of the instrument with both the guide path and the angle of entry. In this way, the ultrasound probe 100 can be used to direct an instrument from the surface to the target structure beneath the surface such that the instrument reaches the target structure substantially at the intersection of the first and second planar ultrasonic beams 111, 116.

[0034] Of course, with different target structures at different depths beneath the surface (e.g., Figures 10 and 11), the third plane 127 may need to be adjusted so that it intersects the second plane 117 substantially at the point where the second plane intersects the target structure 20. Accordingly, in some embodiments, the second light source 125 may be rotated or moved, relative to the first light source 120, so as to modify the location or orientation of the third plane and the second light line 126 within that plane.

[0035] With reference again to Figures 7-13, in one embodiment, the second light source 125 is configured to project the second light line 126 within the third plane 127 at a projection angle 129, wherein the projection angle is less than 90°. In an additional embodiment, a stepper motor (not shown) is coupled to the second light source. The stepper motor may be coupled to the second light source directly or indirectly. With particular reference to Figures 10 and 11, in a further embodiment, the stepper motor is configured to rotate the second light source and thereby adjust the projection angle, wherein the adjusted projection angle is less than 90°.

[0036] With reference to Figure 13, the projection angle 129 (or angle of entry), is defined by the equation $\alpha = \arctan(y/x)$, where α is the projection angle, y is the vertical distance 135 between the target structure 20 and the second light source 125, and x is the horizontal distance 140 between the target structure and the second light source.

[0037] In yet another embodiment, a position of the second light source 125, relative to the first light source 120, is adjustable. For example, the a position of the sec-

ond light source may be adjustable, relative to the first light source, in a horizontal direction, a vertical direction, or both, so that the third plane 127 intersects the second plane 117 substantially at the point where the second plane intersects the target structure 20. In such a case, the position of the second light source is defined by the equation $\tan \alpha = y/x$, where α is the projection angle 129 of the second light source, y is the vertical distance 135 between the target structure and the second light source, and x is the horizontal distance 140 between the target structure and the second light source.

[0038] With reference again to Figure 2, in one embodiment, the ultrasound probe 100 further includes a control panel 160, which may optionally comprise a touchscreen. In some embodiments, the control panel includes a power button, a button to record the ultrasound images, and a button to record a video of the real-time images being generated by the ultrasound probe. In another embodiment, the image power and contrast can be adjusted, as well as the depth and angle of the target structure.

[0039] In a further embodiment, the control panel can include presets for different procedures or individuals. These presets can be modified by individuals and stored for future recall and use. For example, one operator may prefer to access a radial artery at 30° , while another operator may prefer a steeper angle, such as 45° . In such a case, the operators would select their preferred projection angle and set this as a preset value for future procedures.

[0040] With reference to Figures 15-17, in one embodiment, the ultrasound probe 100 further comprises a sterile cover 165 coupled to the ultrasonic probe 100. In another embodiment, an ultrasound gel can be used with the sterile probe cover 165 to optimize ultrasound transmission and optimize image quality with minimum ultrasound power. In an additional embodiment, the sterile cover 165 comprises a rigid, optically transparent material 165', such as a hard plastic, configured to be positioned over the first light source 120 and second light source 125. This rigid, optically transparent material can cover the light sources while minimizing light distortion and attenuation. As such, the rigid, optically transparent material 165' provides for a sterile environment while maintaining the desired relationship between the light lines and the planar ultrasonic beams. In an additional embodiment, the sterile cover 165 is secured to the ultrasound probe 100 by one or more attachment points 166, which may be provided on the ultrasound probe, the cover, or both.

[0041] With particular reference to Figure 17, in one embodiment, the sterile cover 165 further comprises a flexible bag 167 coupled to at least one piece of rigid, optically transparent material 165'. In one embodiment, the rigid material 165' is heat sealed onto the flexible bag 167. The melted portion of the flexible bag will form over the rigid material a melted layer, which will not wrinkle or cause light distortion and attenuation when the light passes through it.

[0042] The flexible bag 167 can be folded over itself to create multiple fold channels 170. Figure 17 depicts a folded flexible bag 167, in accordance with one embodiment, with the sides of the bag being shown in cross-section to reveal the fold channels 170. The rigid material 165' is visible on the front side of the center pocket 171. In one embodiment, the flexible bag further includes a guide portion 168, which extends across the top of the folded flexible bag 167, from a periphery of the flexible bag, into the center pocket 171. In an additional embodiment, the guide portion is opaque and, therefore, obscures all but the bottom of the center pocket 171 when viewed from above. Accordingly, the guide portion 168 can be configured to form a funnel leading to the center pocket 171. In this way, the guide portion facilitates placement of the ultrasonic probe 100 into the proper fold channel (i.e., center pocket 171). In yet another embodiment, the guide portion 168 further includes one or more tabs 169, which a user may pull to unfold the flexible bag 167 and draw it over the ultrasonic probe and its cable 172.

[0043] In use, an operator would add ultrasound gel to the center pocket 171, place the ultrasonic probe 100 into the center pocket, align the rigid, optically transparent members 165' over the first and second light sources 120, 125, attach the rigid members 165' to the ultrasonic probe at the attachment points 166, and pull the tabs 169 to draw the flexible bag 167 over the ultrasonic probe.

[0044] In another embodiment, the ultrasound probe further includes a sterile screen protector (not shown), which can permit an operator to interact with the ultrasound probe under sterile conditions. In one embodiment, the screen protector can be held in place by a vacuum system (not shown), which maintains and supports the screen protector in place and stretches it to enable the use of optional touch screen features. The vacuum system can be activated when the cover is placed on the screen and comes in contact with a sensor therein.

[0045] In a further embodiment, a reflective needle with depth guide is provided as the instrument 30. Ultrasound reflectivity of the needle can be enhanced to improve visualization of the needle as it approaches the target structure 20. In another embodiment, a surface of the needle includes ultrasound reflectors. In an additional embodiment, the needle is etched at regular intervals. These markings can be used to indicate the depth of the needle beneath the surface.

[0046] With reference again to Figures 7-14, the present invention is also embodied in a method of directing an instrument 30 from a surface 10 to a target structure 20 beneath the surface. In one embodiment, the method includes the steps of emitting a first planar ultrasonic beam 111 in a first direction 113 within a first plane 112, emitting a second planar ultrasonic beam 116 in the first direction within a second plane 117, projecting a first light line 121 substantially within the first plane, projecting a second light line 126 within a third plane 127, aligning an end of the instrument with a point of entry 130, aligning a length of the instrument with both a guide path 121 and

an angle of entry 129, and guiding the instrument through the point of entry toward the target structure beneath the surface, while substantially maintaining alignment of the length of the instrument with both the guide path and the angle of entry. The second plane and the third plane are both substantially perpendicular to the first plane. The third plane intersects the second plane at an oblique angle 128 and also defines the angle of entry for the instrument. The first light line defines the guide path for the instrument. The second light line intersects and is substantially perpendicular to the first light line, and a point of intersection 130 between the first light line and the second light line defines the point of entry for the instrument.

[0047] With particular reference to Figure 14, in one embodiment, the method includes displaying both a first image 151 from the first planar ultrasonic beam 111 and a second image 152 from the second planar ultrasonic beam 116. In another embodiment, the second image includes a centerline 153. In a further embodiment, the centerline corresponds to a center 118 of the second planar ultrasonic beam. In yet another embodiment, the centerline corresponds to a point of intersection between the first planar ultrasonic beam and the second planar ultrasonic beam.

[0048] In one embodiment, the method includes aligning the second planar ultrasonic beam 116 over the target structure 20 such that the centerline 153 of the second image 152 is substantially centered over the target structure. In another embodiment, the method includes aligning the first planar ultrasonic beam 111 over the target structure such that the target structure is visible in the first image 151 while the centerline of the second image is substantially centered over the target structure.

[0049] In another embodiment, the method includes selecting the target structure 20 on the first or second image 151, 152. For example, the target structure can be either automatically or manually identified and a touch screen can be used to select the best path from the surface 10 to the target structure. In a further embodiment, the method includes selecting a desired angle of entry 129. In an additional embodiment, the method includes selecting a desired point of entry 130 on the first image 151. In yet another embodiment, the method includes selecting both a desired point of entry on the first image and a desired angle of entry.

[0050] With reference to Figure 13, in one embodiment, the method includes determining both a vertical 135 and a horizontal distance 140 between the target structure 20 and a light source 125 projecting the second light line 126. In another embodiment, the method includes calculating a projection angle 129 of the light source required to project the second light line within the third plane 127 such that the third plane is substantially incident a point of intersection between the second plane 117 and the target structure. The projection angle is defined by the equation $\alpha = \arctan(y/x)$, where α is the projection angle, y is the vertical distance 135 between the

target structure and the light source, and x is the horizontal distance 140 between the target structure and the light source. In another embodiment, the method includes rotating the light source so as to project the second light line within the third plane substantially at the calculated projection angle.

[0051] In one embodiment, the method includes calculating a position of the light source 125 required to project the second light line 126 within the third plane 127 such that the third plane is substantially incident a point of intersection between the second plane 117 and the target structure 20. The position is determined from an equation $\tan \alpha = y/x$, where α is a projection angle of the light source, y is the vertical distance 135 between the target structure and the light source, and x is the horizontal distance 140 between the target structure and the light source. In another embodiment, the method includes moving the light source substantially to the calculated position.

[0052] In one embodiment, the method includes the step of calculating both a projection angle 129 and a position of the light source 125 required to project the second light line 126 within the third plane 127 such that the third plane is substantially incident a point of intersection between the second plane 117 and the target structure 20. The projection angle and position are determined from an equation $\tan \alpha = y/x$, where α is the projection angle, y is the vertical distance 135 between the target structure and the light source, and x is the horizontal distance 140 between the target structure and the light source. In another embodiment, the method includes rotating the light source so as to project the second light line within the third plane substantially at the calculated projection angle, and moving the light source substantially to the calculated position.

[0053] It should be appreciated from the foregoing description that the present invention provides an ultrasound probe that enables health care practitioners to safely perform procedures involving internal bodily structures with greater ease and accuracy and fewer complications. The ultrasound probe can be used to reliably and continuously direct an instrument from a surface to a target structure beneath the surface.

[0054] Specific methods, devices, and materials are described, although any methods and materials similar or equivalent to those described can be used in the practice or testing of the present embodiment. Unless defined otherwise, all technical and scientific terms used herein have the same meanings as commonly understood by one of ordinary skill in the art to which this embodiment belongs.

[0055] Without further elaboration, it is believed that one skilled in the art, using the proceeding description, can make and use the present invention to the fullest extent. The invention has been described in detail with reference only to the presently preferred embodiments. Persons skilled in the art will appreciate that various modifications can be made without departing from the inven-

tion defined only by the following claims.

Claims

1. An ultrasonic probe (100) comprising:

a housing (105);
a first ultrasonic transducer array (110) coupled to the housing (105) and configured to emit a first planar ultrasonic beam (111) in a first direction (113) within a first plane (112);
a second ultrasonic transducer array (115) coupled to the housing (105) and configured to emit a second planar ultrasonic beam (116) in the first direction (113) within a second plane (117), which is substantially perpendicular to the first plane (112); and
a first light source (120) coupled to the housing (105) and configured to project a first light line (121) substantially within the first plane (112);
characterized by

a second light source (125) coupled to the housing (105) and configured to project a second light line (126) within a third plane (127), which is substantially perpendicular to the first plane (112) and intersects the second plane (117) at an oblique angle (128);
wherein the first light line (121) intersects and is substantially perpendicular to the second light line (126).

2. The ultrasonic probe of claim 1, wherein the first light source (120) is a first laser and the second light source (125) is a second laser.

3. The ultrasonic probe of claim 2, wherein the first and second ultrasonic transducer arrays are arranged in a T-shaped configuration.

4. The ultrasonic probe of claim 2, further comprising a screen (150) coupled to the ultrasonic probe (100) and configured to display both a first image (151) from the first ultrasonic transducer array (110) and a second image (152) from the second ultrasonic transducer array (115).

5. The ultrasonic probe of claim 4, wherein the screen (150) is configured to display a centerline (153); and wherein the centerline (153) corresponds to a center (118) of the second ultrasonic transducer array (115).

6. The ultrasonic probe of claim 2, wherein the second laser is configured to project the second light line (126) within the third plane (127) at a projection angle

(129), wherein the projection angle (129) is less than 90°.

7. The ultrasonic probe of claim 6, further comprising a stepper motor coupled to the second laser; and wherein the stepper motor is configured to rotate the second laser and thereby adjust the projection angle, (129) wherein the adjusted projection angle is less than 90°.

8. The ultrasonic probe of claim 6, wherein a position of the second laser relative to the first laser is adjustable.

9. The ultrasonic probe of claim 8, further comprising a sterile cover (165) coupled to the ultrasonic probe (100), wherein the sterile cover (165) comprises a rigid, optically transparent material (165') configured to be positioned over the first and second light source.

10. The ultrasonic probe of claim 9, wherein the sterile cover (165) further comprises a flexible bag (167) coupled to the rigid, optically transparent material (165').

Patentansprüche

1. Eine Ultraschallsonde (100), mit:

einem Gehäuse (105);
einer ersten Gruppe von Ultraschallsendern (110), welche mit dem Gehäuse (105) verbunden ist und zum Senden eines ersten planaren Ultraschallstrahls (111) in eine erste Richtung (113) innerhalb einer ersten Ebene (112) ausgebildet ist;
einer zweiten Gruppe von Ultraschallsendern (115), welche mit dem Gehäuse (105) verbunden ist und zum Senden eines zweiten planaren Ultraschallstrahls (116) in der ersten Richtung (113) innerhalb einer zweiten Ebene (117) ausgebildet ist, die sich im Wesentlichen senkrecht zu der ersten Ebene (112) erstreckt; und
einer ersten Lichtquelle (120), welche mit dem Gehäuse (105) verbunden ist und dazu ausgebildet ist, eine erste Lichtlinie (121) zu projizieren, welche sich im Wesentlichen in der ersten Ebene (112) erstreckt;
gekennzeichnet durch

eine zweite Lichtquelle (125), welche mit dem Gehäuse (105) verbunden ist und dazu ausgebildet ist, eine zweite Lichtlinie (126) innerhalb einer dritten Ebene (127) zu projizieren, welche sich im Wesentlichen senkrecht zu der ersten Ebene (112) erstreckt

und sich im wesentlichen senkrecht mit der zweiten Ebene (117) in einem Neigungswinkel (128) überschneidet; wobei sich die erste Lichtlinie (121) im Wesentlichen senkrecht mit der zweiten Lichtlinie (126) überschneidet.

2. Die Ultraschallsonde nach Anspruch 1, wobei die erste Lichtquelle (120) ein erster Laser und die zweite Lichtquelle (125) ein zweiter Laser ist.
3. Die Ultraschallsonde nach Anspruch 2, wobei die erste und die zweite Gruppe von Ultraschallsendern in einer T-förmigen Konfiguration zueinander angeordnet sind.
4. Die Ultraschallsonde nach Anspruch 2, weiter versehen mit einem Bildschirm (150), welcher mit der Ultraschallsonde (100) verbunden ist und derart konfiguriert ist, sowohl ein erstes Bild (151) von der ersten Gruppe von Ultraschallsendern (110) als auch ein zweites Bild (152) von der zweiten Gruppe von Ultraschallsendern (115) zu zeigen.
5. Die Ultraschallsonde nach Anspruch 4, wobei der Bildschirm (150) dazu konfiguriert ist, eine Mittellinie (153) anzuzeigen; und wobei die Mittellinie (153) einer Mitte (118) der zweiten Gruppe von Ultraschallsendern (115) entspricht.
6. Die Ultraschallsonde nach Anspruch 2, wobei der zweite Laser dazu konfiguriert ist, eine zweite Lichtlinie (126) innerhalb der dritten Ebene (127) in einem solchen Projektionswinkel (129) zu projizieren, dass dieser Projektionswinkel (129) weniger als 90° beträgt.
7. Die Ultraschallsonde nach Anspruch 6, weiter versehen mit einem Schrittmotor, welcher mit dem zweiten Laser verbunden ist; und wobei der Schrittmotor dazu konfiguriert ist, den zweiten Laser zu drehen und so den Projektionswinkel (129) einzustellen, wobei der eingestellte Projektionswinkel weniger als 90° beträgt.
8. Die Ultraschallsonde nach Anspruch 6, wobei die Position des zweiten Lasers relativ zu dem ersten Laser einstellbar ist.
9. Die Ultraschallsonde nach Anspruch 8, weiter versehen mit einer sterilen Abdeckung (165), welches mit der Ultraschallsonde (100) verbunden ist, wobei die sterile Abdeckung (165) ein steifes, optisch transparentes Material (165') aufweist, welches dazu ausgebildet ist, über der ersten und der zweiten Lichtquelle angeordnet zu sein.
10. Die Ultraschallsonde nach Anspruch 9, wobei die

sterile Abdeckung (165) weiter versehen ist mit einer flexiblen Tasche (167), welche mit dem steifen, optisch transparenten Material (165') verbunden ist.

Revendications

1. Sonde ultrasonore (100) comprenant :

un boîtier (105) ;
un premier réseau de transducteurs ultrasonores (110) couplé au boîtier (105) et configuré pour émettre un premier faisceau ultrasonore plan (111) dans une première direction (113) dans un premier plan (112) ;
un second réseau de transducteurs ultrasonores (115) couplé au boîtier (105) et configuré pour émettre un second faisceau ultrasonore plan (116) dans la première direction (113) dans un deuxième plan (117), qui est sensiblement perpendiculaire au premier plan (112) ; et
une première source de lumière (120) couplée au boîtier (105) et configurée pour projeter une première ligne de lumière (121) sensiblement dans le premier plan (112) ;
caractérisée par

une seconde source de lumière (125) couplée au boîtier (105) et configurée pour projeter une seconde ligne de lumière (126) dans un troisième plan (127), qui est sensiblement perpendiculaire au premier plan (112) et recoupe le deuxième plan (117) selon un angle oblique (128) ;
dans lequel la première ligne de lumière (121) recoupe et est sensiblement perpendiculaire à la seconde ligne de lumière (126).

2. Sonde ultrasonore selon la revendication 1, dans laquelle la première source de lumière (120) est un premier laser et la seconde source de lumière (125) est un second laser.
3. Sonde ultrasonore selon la revendication 2, dans laquelle les premier et second réseaux de transducteurs ultrasonores sont agencés dans une configuration en forme de T.
4. Sonde ultrasonore selon la revendication 2, comprenant en outre un écran (150) couplé à la sonde ultrasonore (100) et configuré pour afficher à la fois une première image (151) provenant du premier réseau de transducteurs ultrasonores (110) et une seconde image (152) provenant du second réseau de transducteurs ultrasonores (115).
5. Sonde ultrasonore selon la revendication 4, dans la-

quelle l'écran (150) est configuré pour afficher une ligne centrale (153) ; et
 dans lequel la ligne centrale (153) correspond à un centre (118) du second réseau de transducteurs ultrasonores (115).

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6. Sonde ultrasonore selon la revendication 2, dans laquelle le second laser est configuré pour projeter la seconde ligne de lumière (126) dans le troisième plan (127) selon un angle de projection (129), dans laquelle l'angle de projection (129) est inférieur à 90°. 10
7. Sonde ultrasonore selon la revendication 6, comprenant en outre un moteur pas à pas couplé au second laser ; et 15
 dans laquelle le moteur pas à pas est configuré pour faire tourner le second laser et ainsi ajuster l'angle de projection (129), dans laquelle l'angle de projection ajusté est inférieur à 90°. 20
8. Sonde ultrasonore selon la revendication 6, dans laquelle une position du second laser par rapport au premier laser est ajustable. 25
9. Sonde ultrasonore selon la revendication 8, comprenant en outre un couvercle stérile (165) couplé à la sonde ultrasonore (100), dans laquelle le couvercle stérile (165) comprend un matériau rigide optiquement transparent (165') configuré pour être positionné au-dessus des première et seconde sources de lumière. 30
10. Sonde ultrasonore selon la revendication 9, dans laquelle le couvercle stérile (165) comprend en outre une poche flexible (167) couplée au matériau rigide optiquement transparent (165'). 35

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FIG. 1

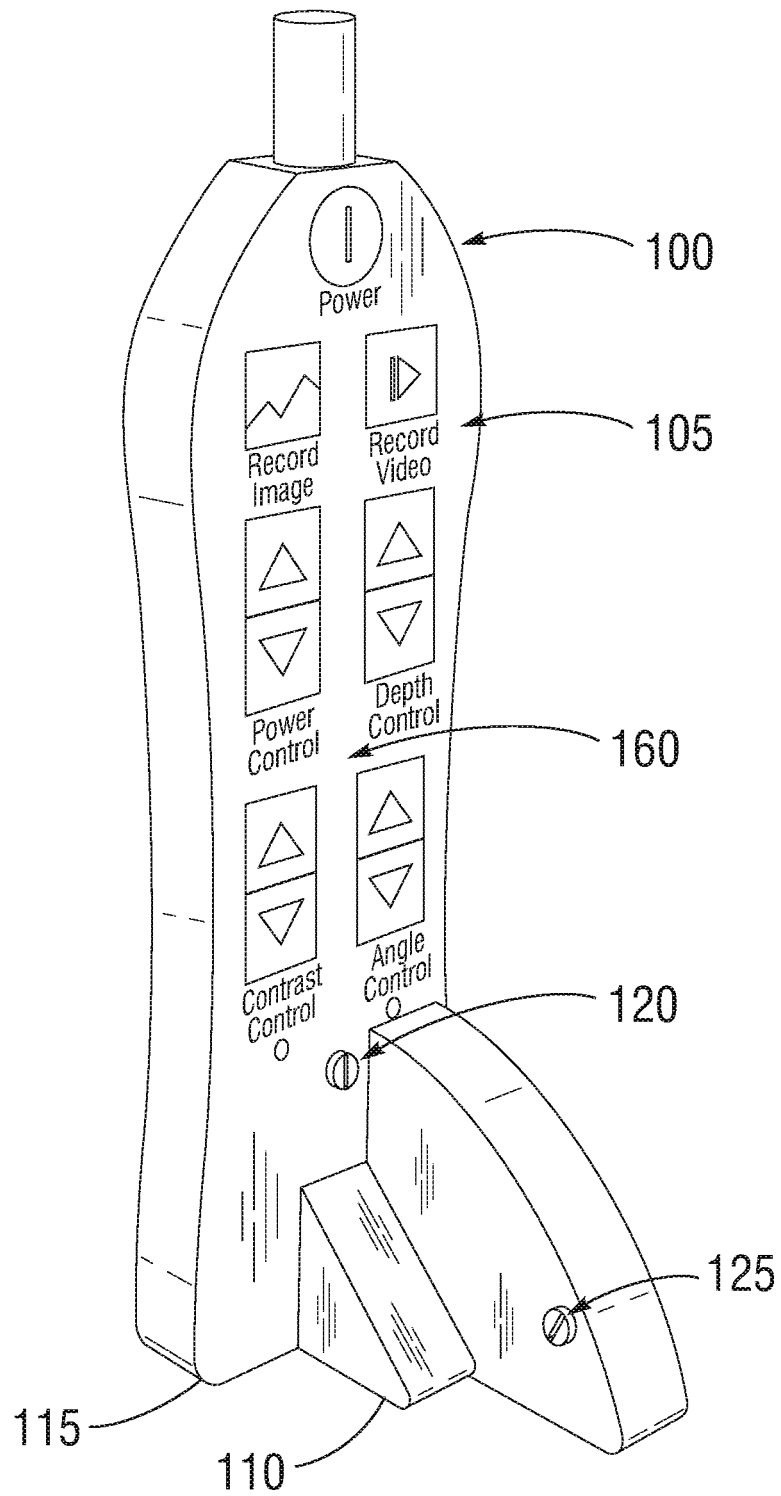


FIG. 2

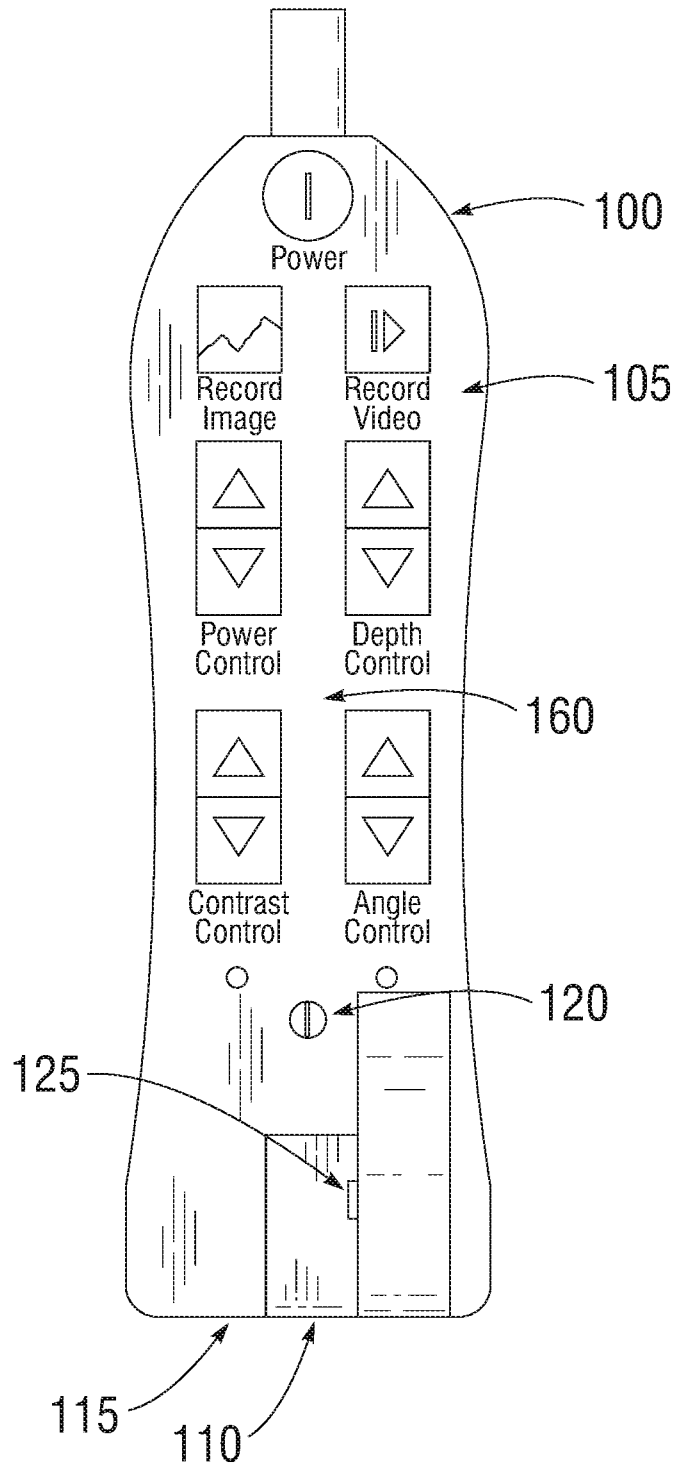


FIG. 3

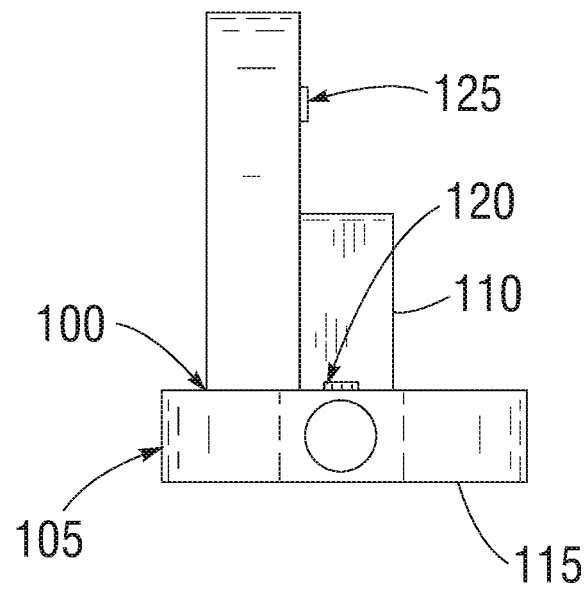


FIG. 4

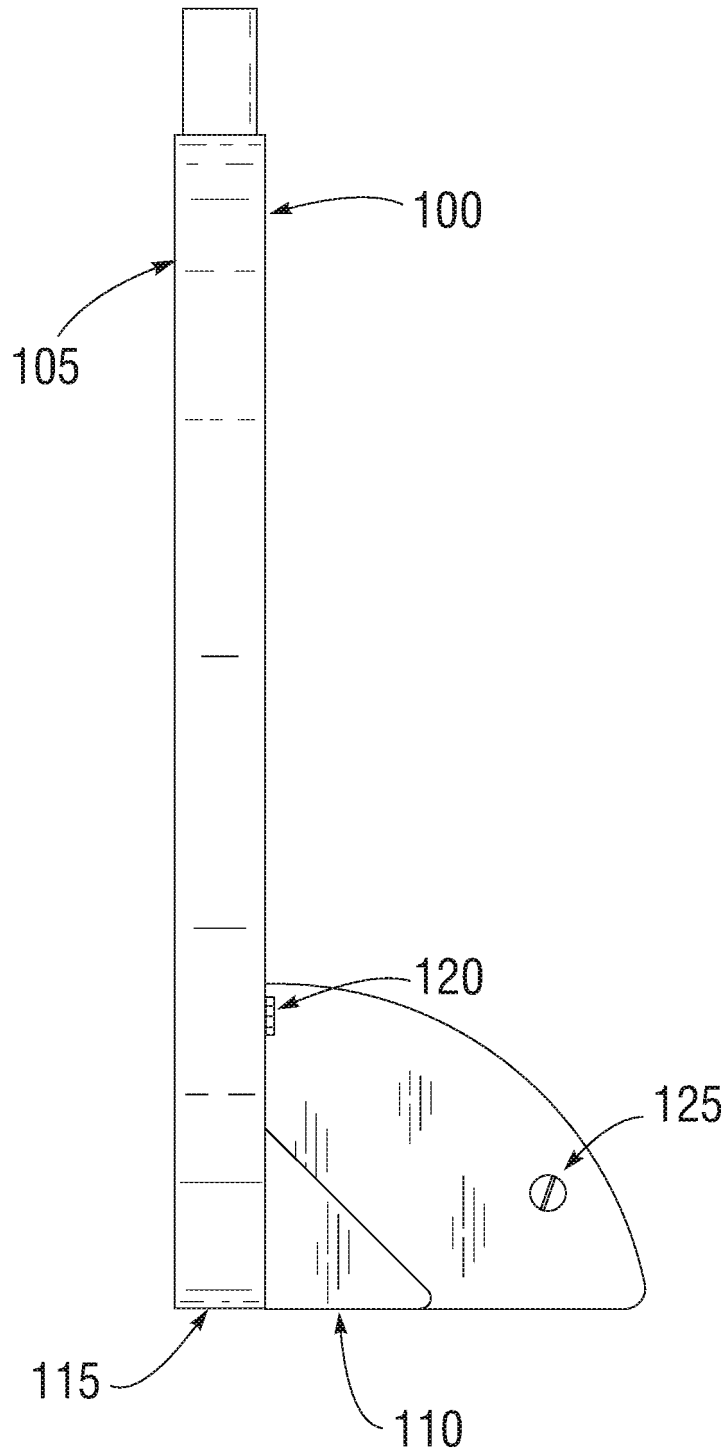


FIG. 5

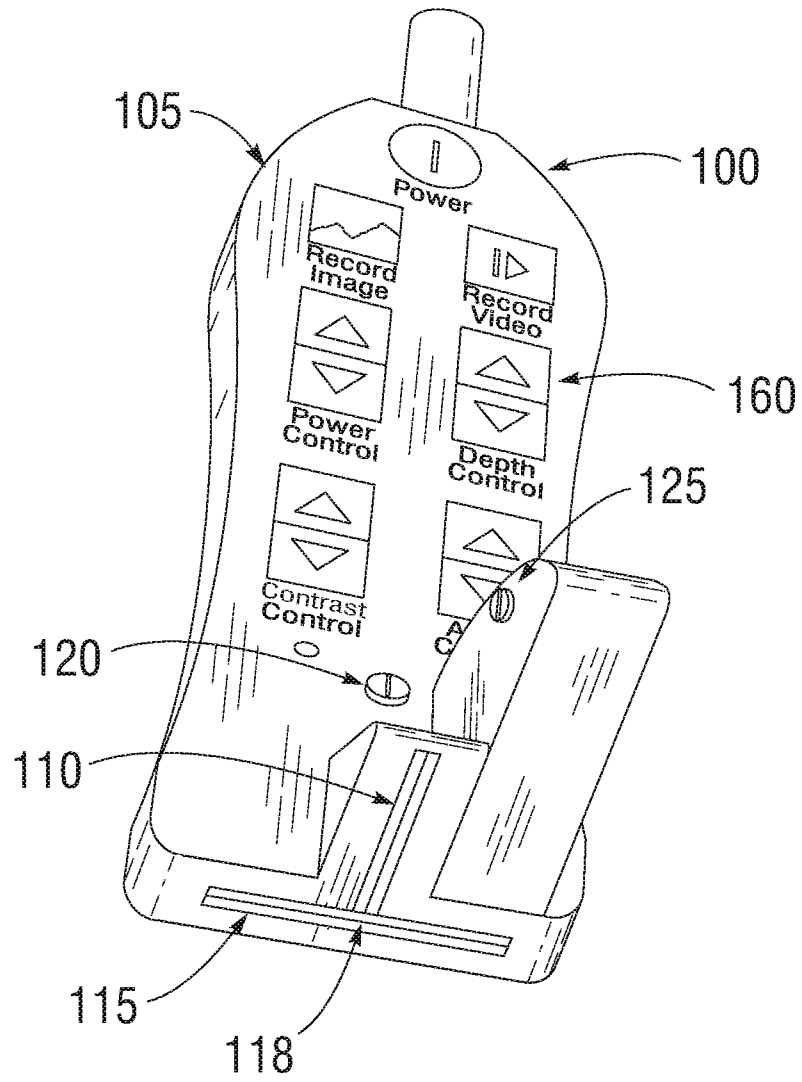


FIG. 6

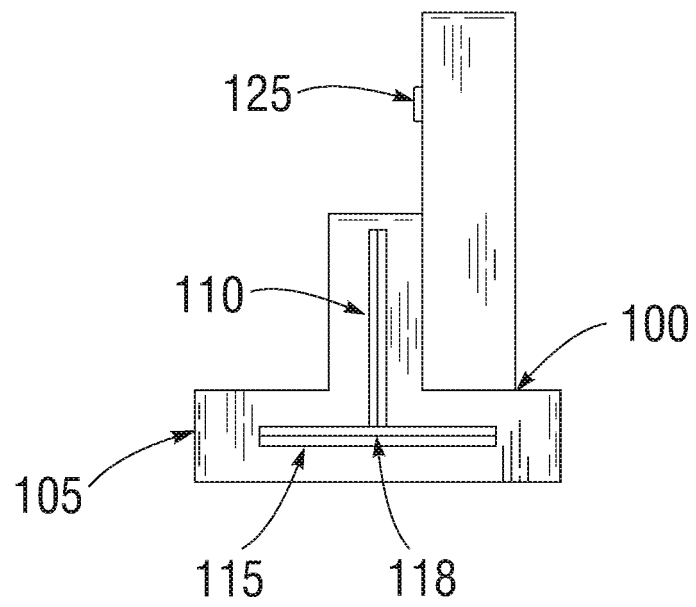


FIG. 7

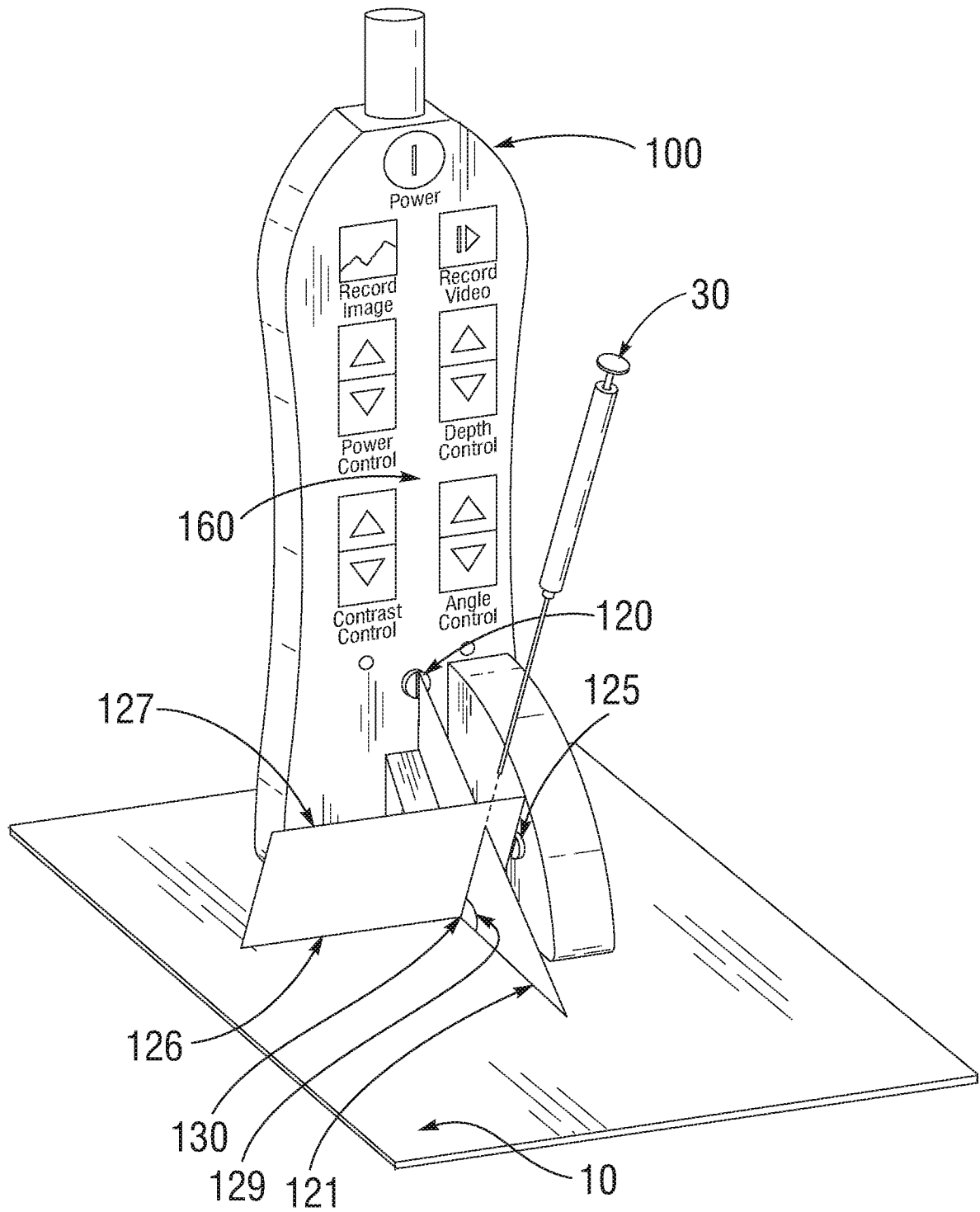


FIG. 8

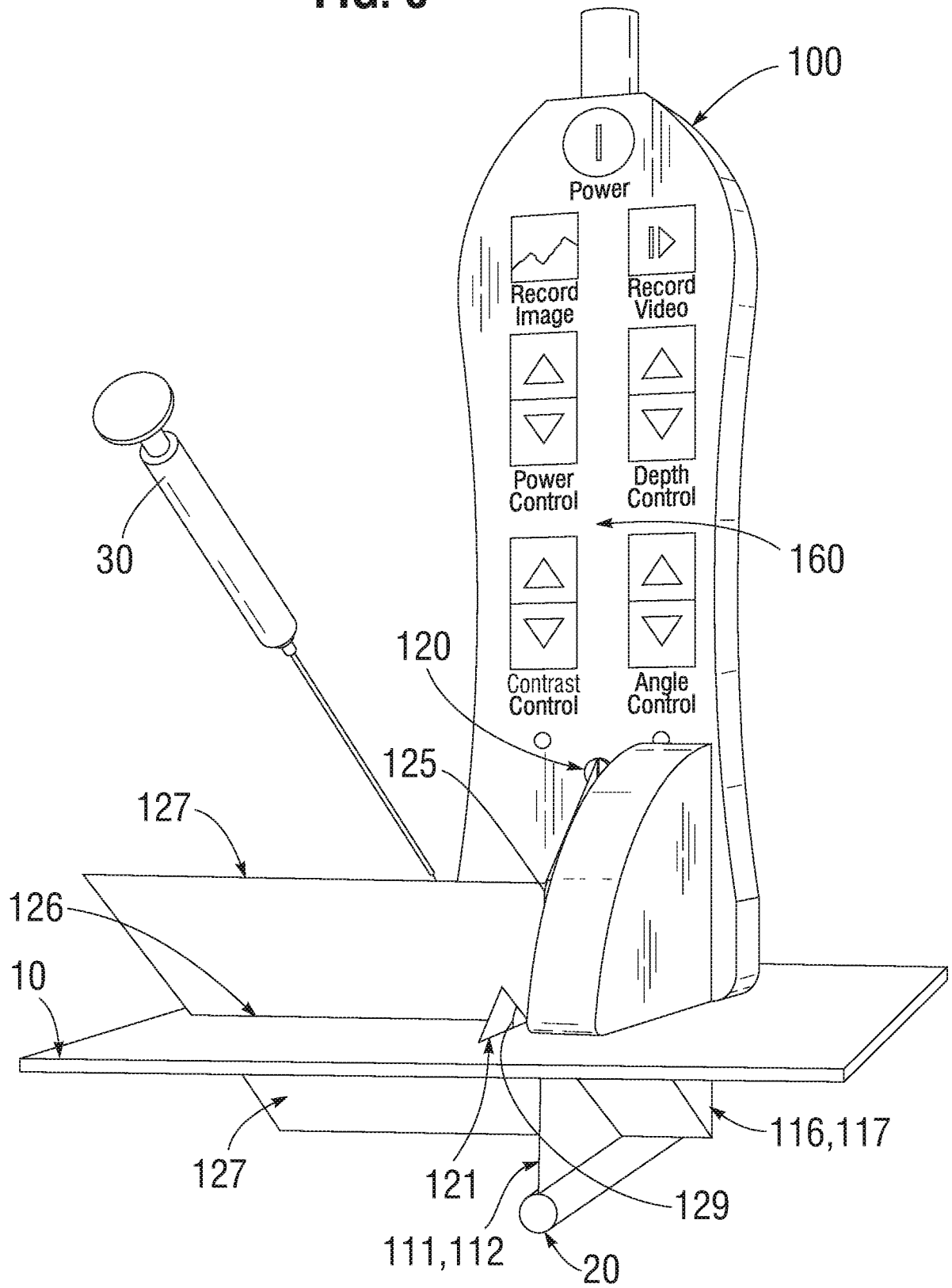


FIG. 9

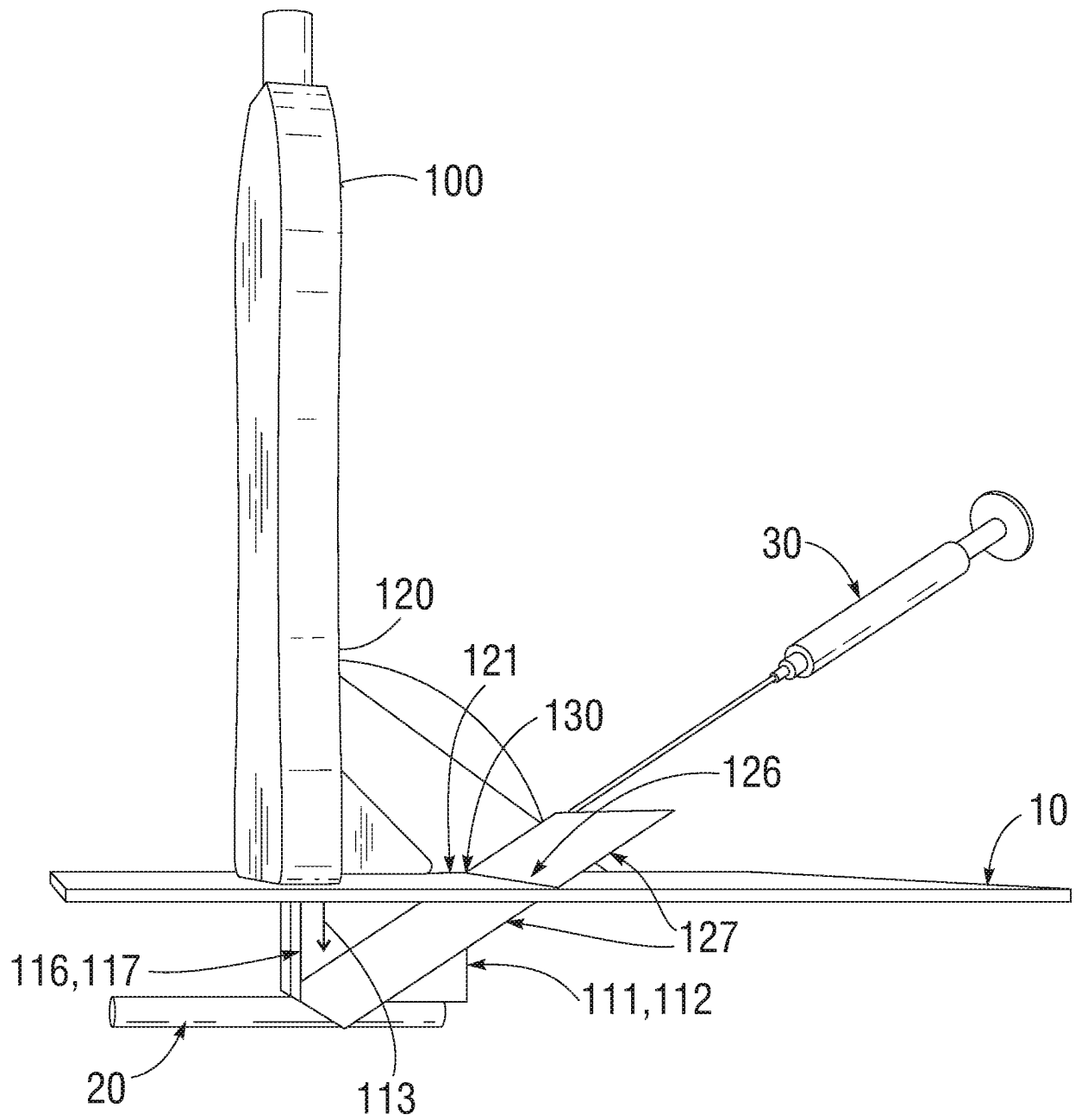


FIG. 10

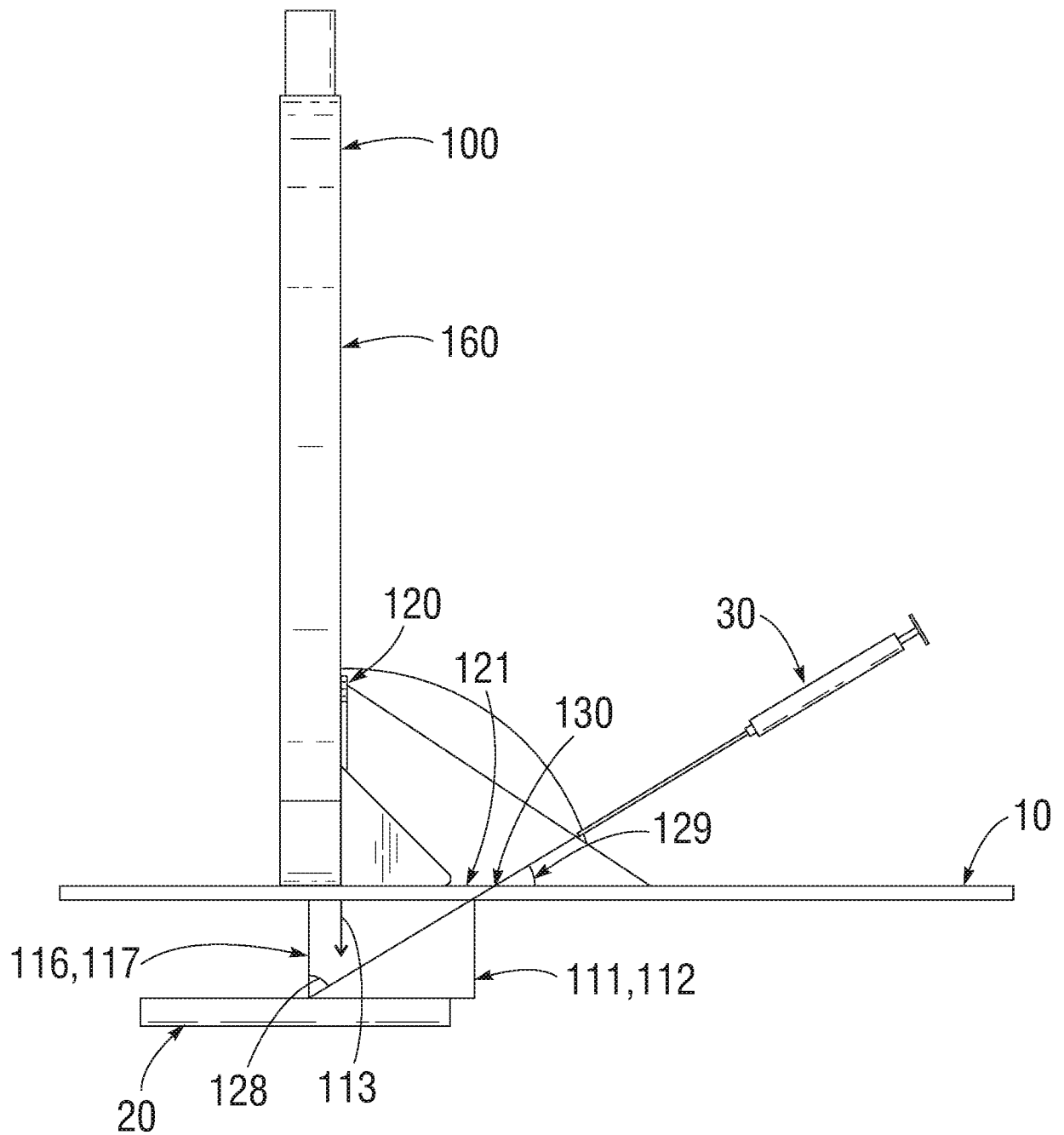


FIG. 11

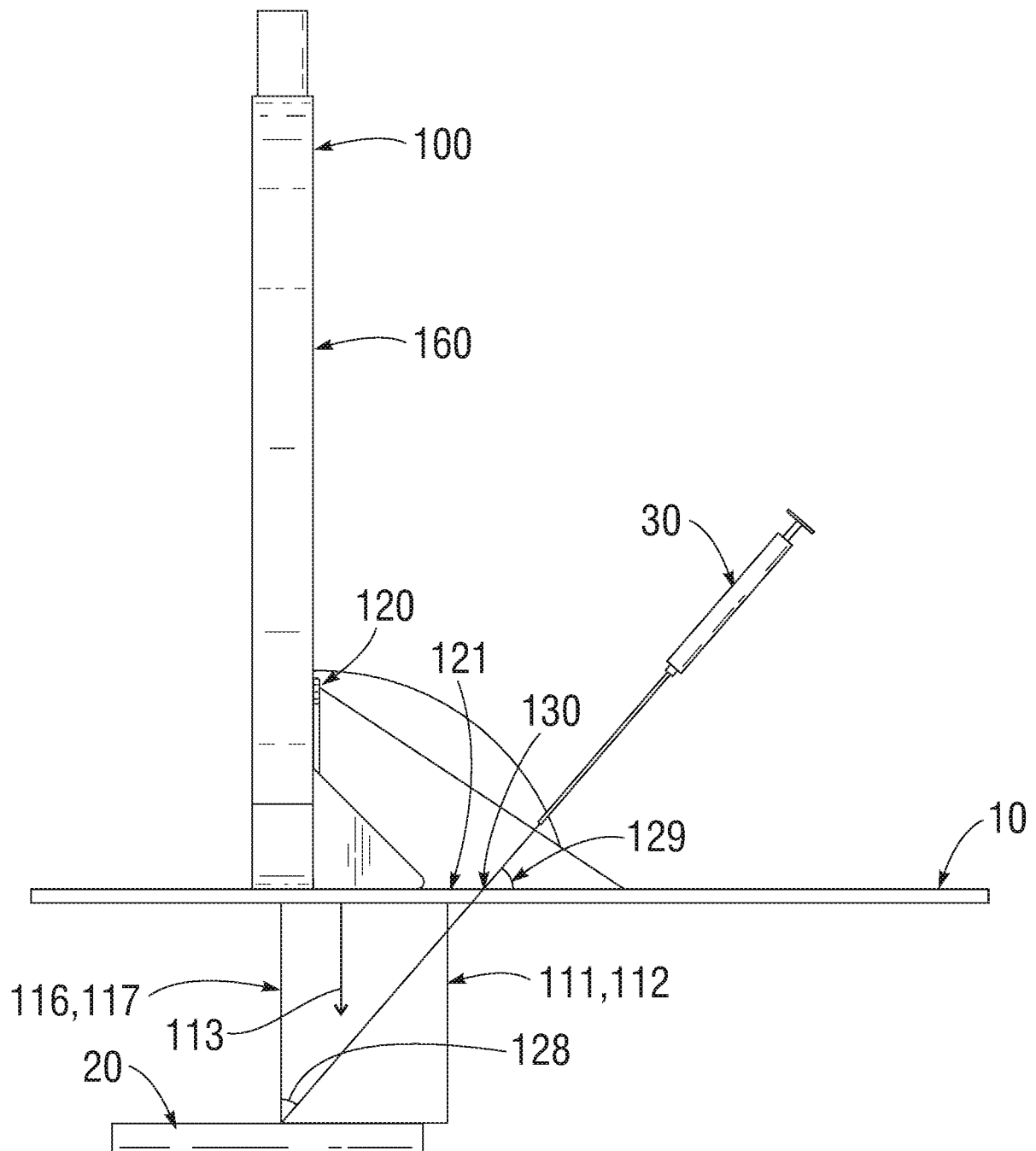


FIG. 12

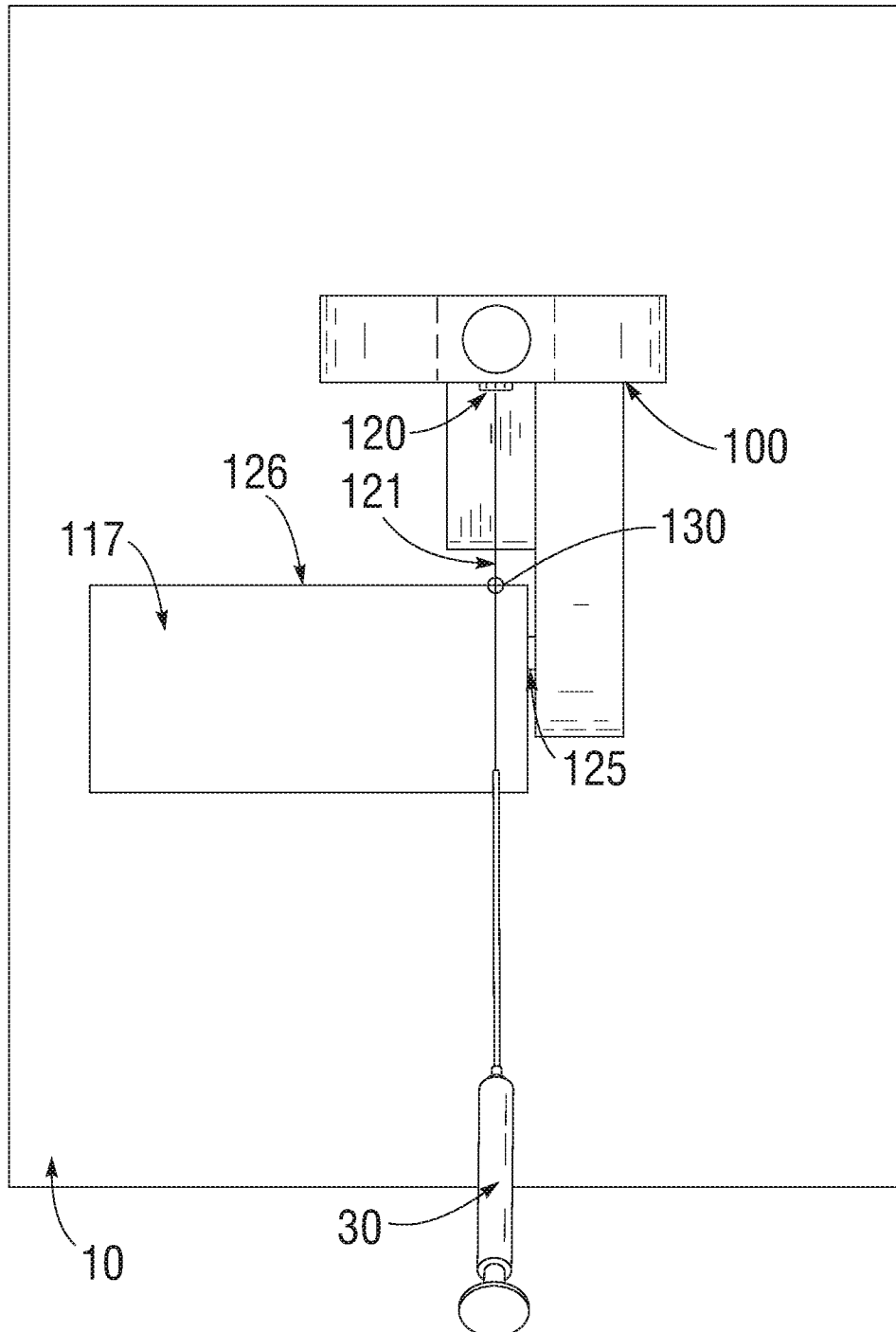


FIG. 13

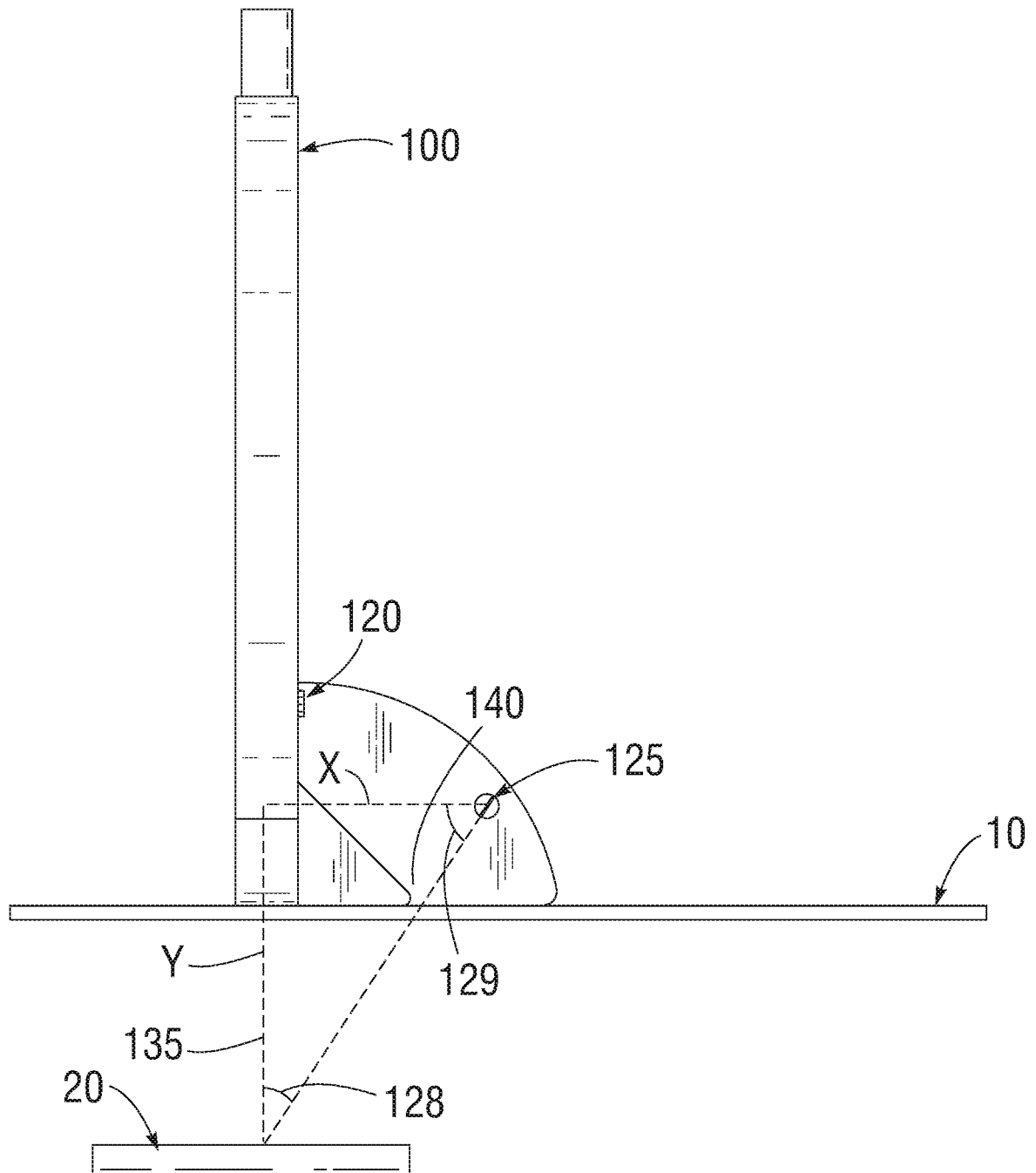


FIG. 14

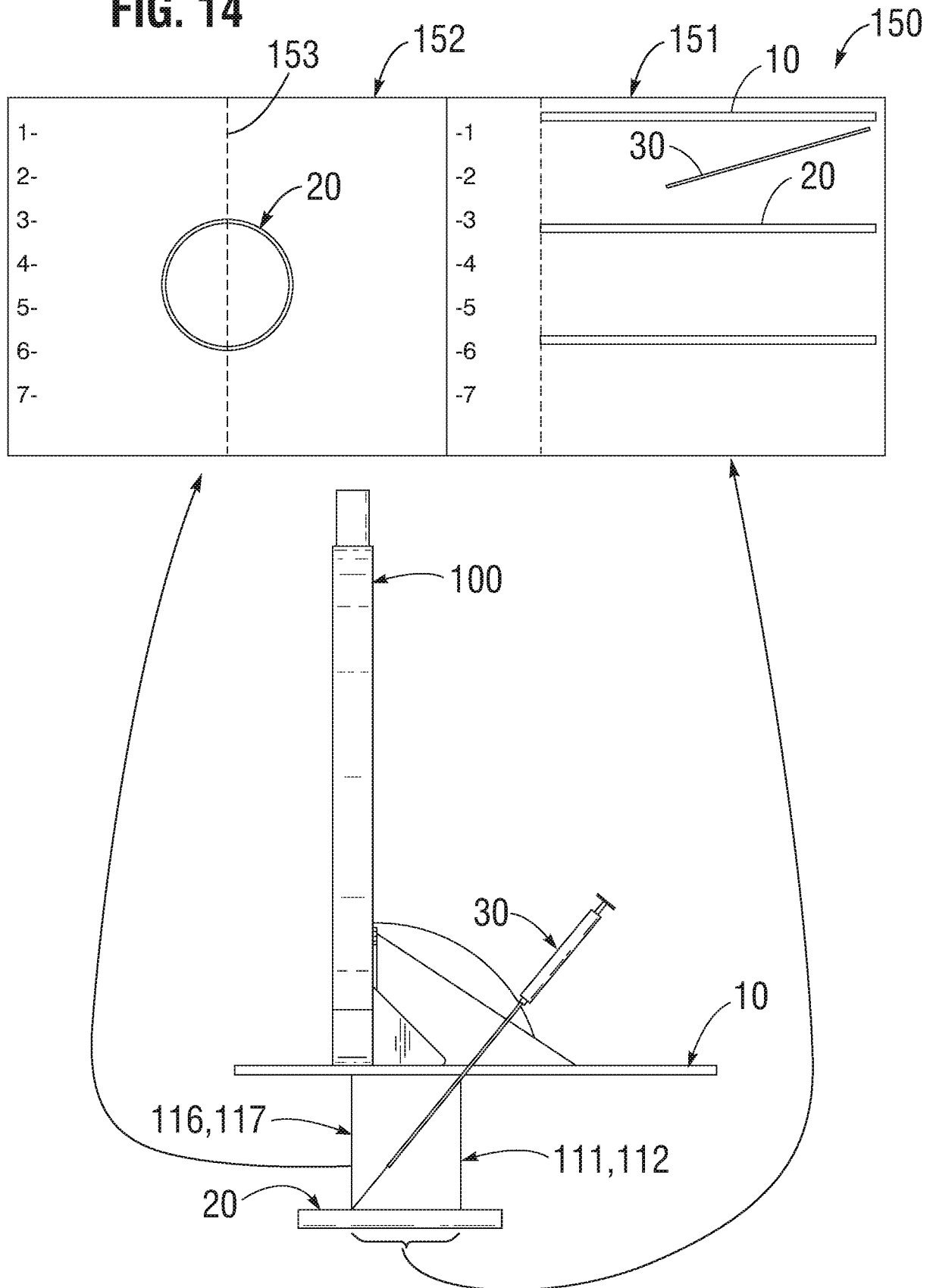


FIG. 15

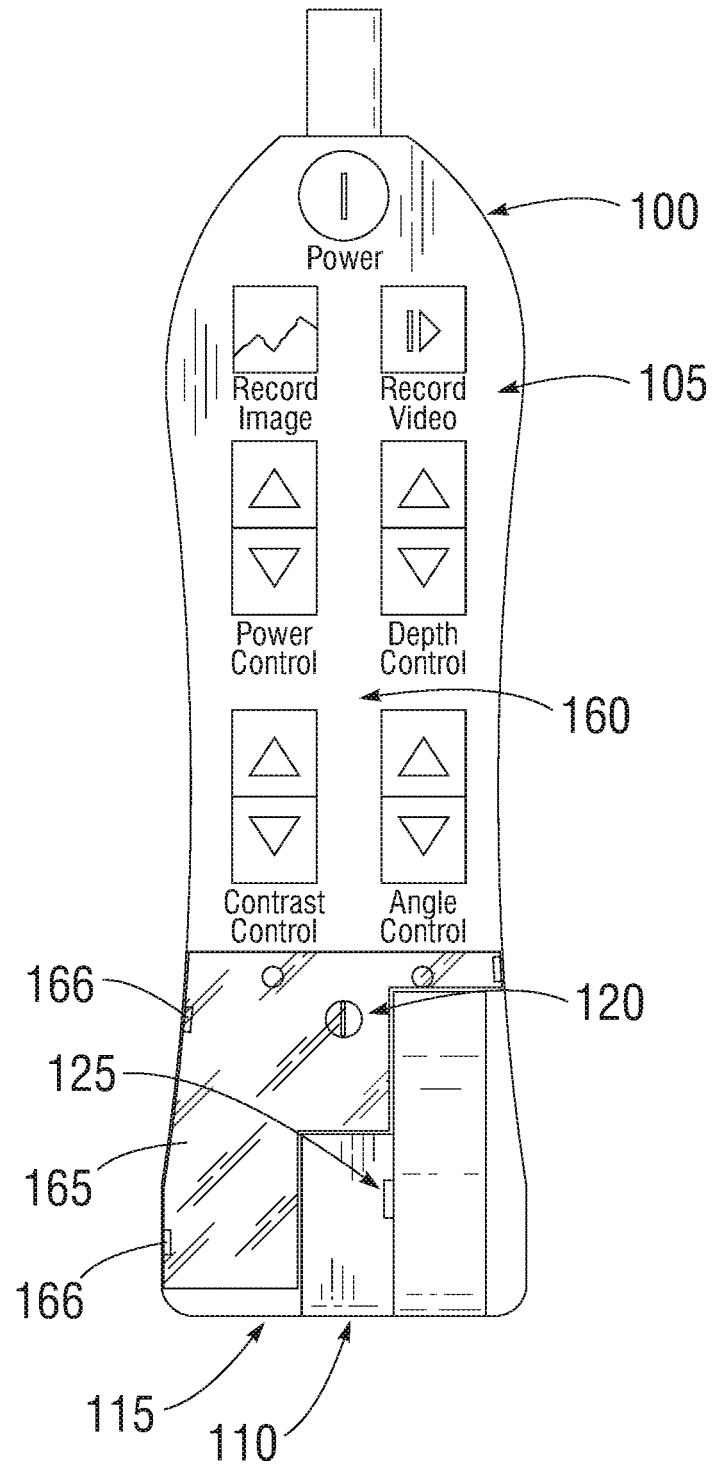


FIG. 16

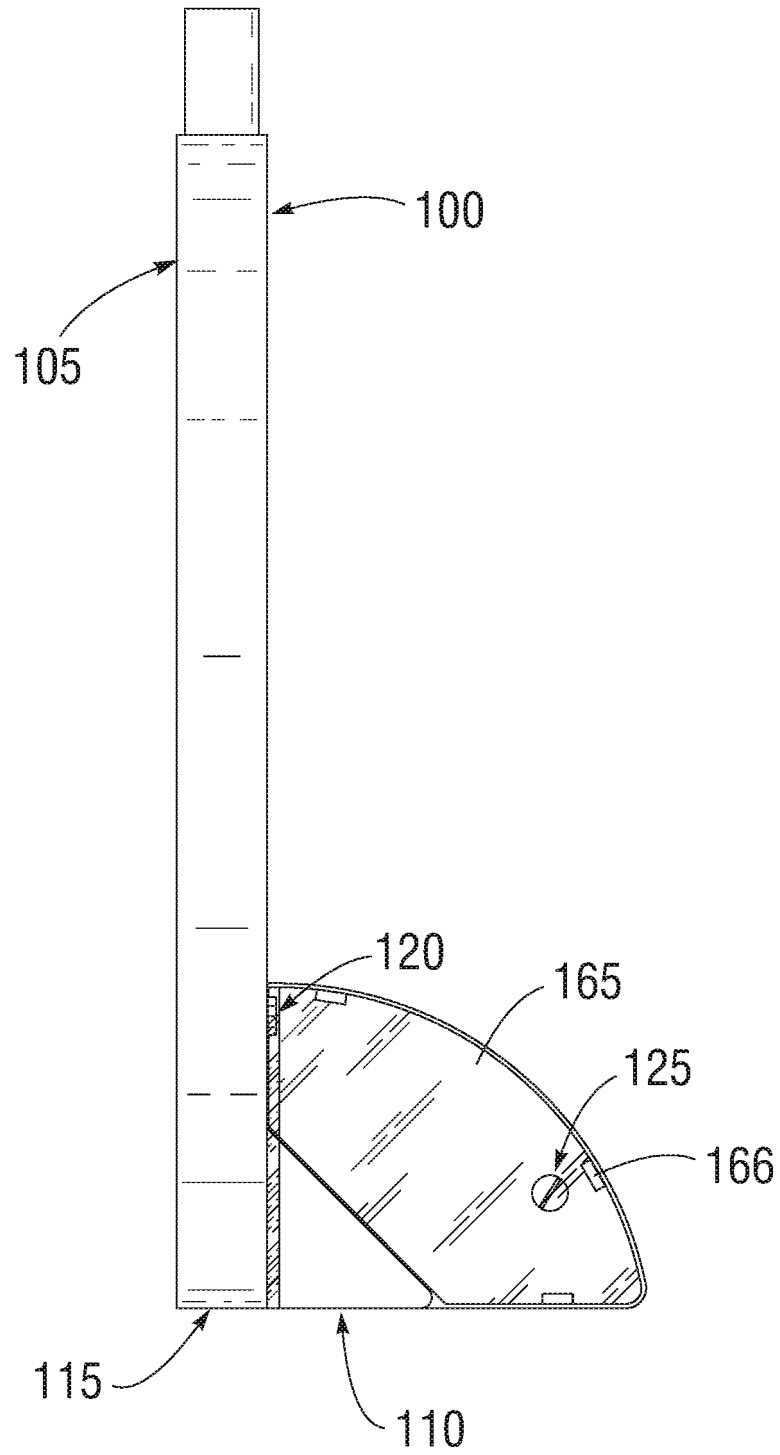
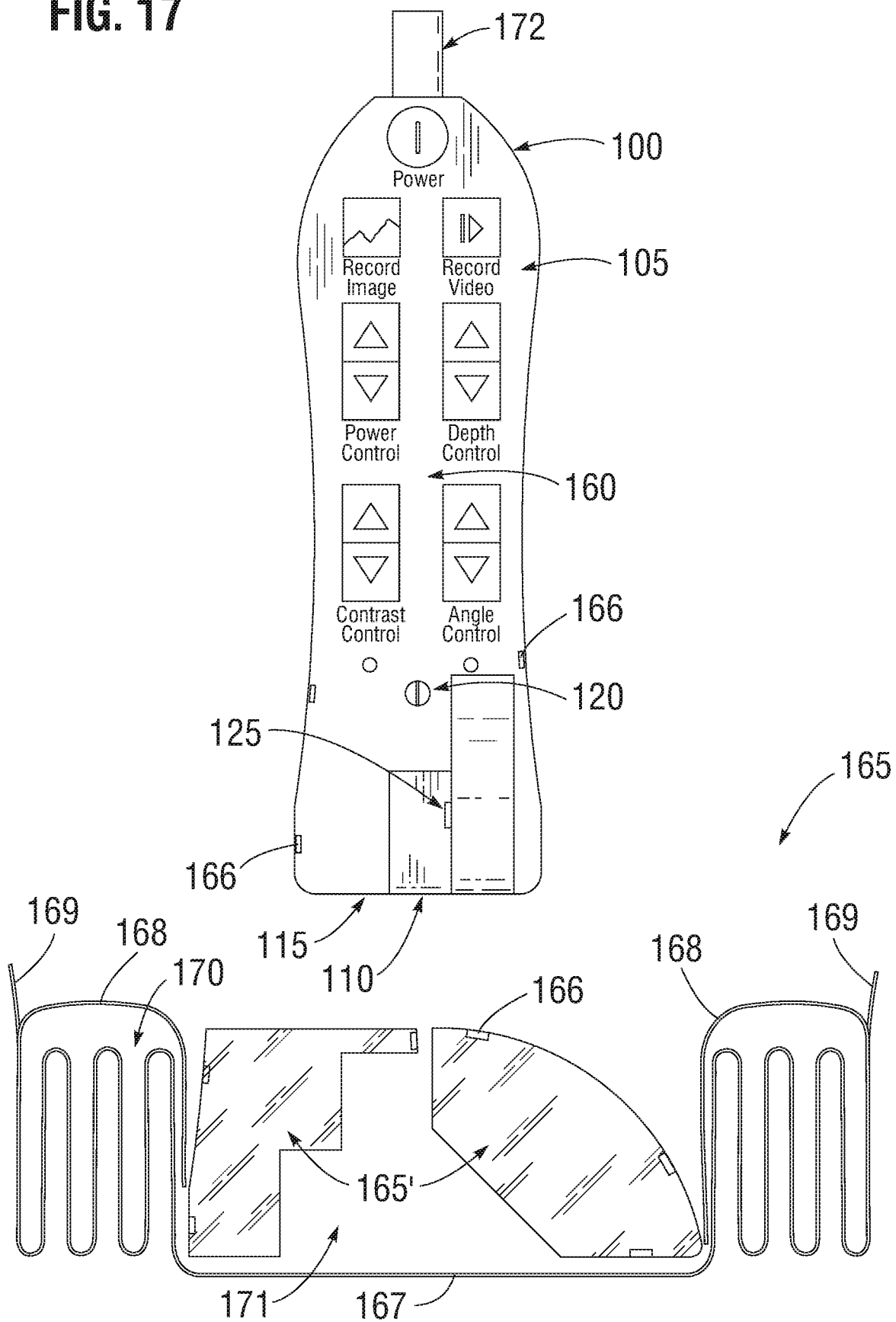


FIG. 17



REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- JP 2009045427 A [0017]

专利名称(译)	系统和方法，用于为身体内的目标结构提供超声引导		
公开(公告)号	EP3344146B1	公开(公告)日	2020-05-06
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[标]申请(专利权)人(译)	BULJUBASIC NEDA		
申请(专利权)人(译)	BULJUBASIC , NEDA		
当前申请(专利权)人(译)	BULJUBASIC , NEDA		
[标]发明人	BULJUBASIC NEDA		
发明人	BULJUBASIC, NEDA		
IPC分类号	A61B8/00 G01S15/89 A61M5/42 A61B8/08 A61B5/15 A61B90/00 A61M25/01 A61B18/20		
CPC分类号	A61B5/15003 A61B5/150748 A61B8/0841 A61B8/4209 A61B8/4455 A61B8/4477 A61B8/4494 A61B8/463 A61B8/467 A61B8/483 A61B8/54 A61B17/3403 A61B46/10 A61B90/13 A61B2017/3413 A61B2018/2025 A61B2090/0811 A61B2090/378 A61M5/427 A61M25/01 G01S15/899		
优先权	62/212586 2015-08-31 US		
其他公开文献	EP3344146A1 EP3344146A4		
外部链接	Espacenet		

摘要(译)

一种超声探头，包括壳体，第一超声换能器阵列，第二超声换能器阵列，第一光源和第二光源。所述第一超声换能器阵列耦合到所述壳体，并且被配置为在第一平面内沿第一方向发射第一平面超声束。第二超声换能器阵列耦合到壳体，并且被配置为在基本垂直于第一平面的第二平面内沿第一方向发射第二平面超声束。所述第一光源耦合到所述壳体并且被配置为将第一光线大致投射在所述第一平面内。第二光源耦合到壳体并且被配置为在第三平面内投射第二光线，该第三平面基本垂直于第一平面并且以倾斜角度与第二平面相交。第一光线与第二光线相交并基本垂直。

