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(54) **LOW POWER PORTABLE ULTRASONIC DIAGNOSTIC INSTRUMENT**

TRAGBARES INSTRUMENT FÜR ULTRASCHALLDIAGNOSTIK MIT NIEDRIGEM
LEISTUNGSBEDARF

INSTRUMENT DE DIAGNOSTIC A ULTRASON, PORTATIF ET A FAIBLE CONSOMMATION

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(56) References cited:
US-A- 5 483 656 **US-A- 5 817 024**
US-A- 5 865 749

- **JUIN-JET HWANG ET AL INSTITUTE OF ELECTRICAL AND ELECTRONICS ENGINEERS: "Portable ultrasound device for battlefield trauma" 1998 IEEE ULTRASONICS SYMPOSIUM PROCEEDINGS. SENDAI, MIYAGI, JP, OCT. 5 - 8, 1998, IEEE ULTRASONICS SYMPOSIUM PROCEEDINGS, NEW YORK, NY : IEEE, US, vol. VOL.2, 5 October 1998 (1998-10-05), pages 1663-1667, XP002148417 ISBN: 0-7803-4096-5**

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Description

BACKGROUND OF THE INVENTION

[0001] This invention relates generally to medical ultrasonic diagnostic systems, and more particularly the invention relates to a portable ultrasonic diagnostic instrument which operates at low power.

[0002] Modern ultrasonic diagnostic systems are large, complex instruments. Today's premium ultrasound systems, while mounted in carts for portability, continue to weigh several hundred pounds. In the past, ultrasound systems such as the ADR 4000 ultrasound system produced by Advanced Technology Laboratories, Inc., were smaller desktop units about the size of a personal computer. However, such instruments lacked many of the advanced features of today's premium ultrasound systems such as color Doppler imaging and three dimensional display capabilities. As ultrasound systems have become more sophisticated they have also become bulkier.

[0003] Disclosed in US Patent No. 5,722,412 is a diagnostic ultrasound instrument which exhibits many of the features of a premium ultrasound system in a hand-held unit. The instrument can be produced as a single unit or, in a preferred embodiment, the instrument is a two part unit: one including a transducer beamformer and image processor and the other including a display and power source for both units. In such a configuration the transducer/processor unit can be manipulated with one hand while a cable between the two units enables the video to be shown on the display unit while the latter unit is held or positioned for optimal viewing of the ultrasound image. The cable also provides energy for the transducer/processor unit from the display.

[0004] In a preferred embodiment the ultrasound system from the transducer to the video output is fabricated on four types of application specific integrated circuits (ASICs): a transmit/receive ASIC which is connected to the elements of an array transducer, a front end ASIC which performs and controls transmit and receive beamforming, a digital signal processing ASIC which provides processing of the ultrasound signals such as filtering, and a back end ASIC which receives processed ultrasound signals and produces ultrasound image data. The image can be displayed on either a standard monitor or on a liquid crystal display (LCD). The elements of the unit including the ASICs can be fabricated on a single printed circuit board, thus eliminating the problems conventionally posed by connectors and cables. This sophisticated ultrasound instrument can be manufactured as a hand held unit weighing less than five pounds (2.3kg).

[0005] A limiting factor in portable ultrasonic diagnostic instruments is the power required for operation. Typically at least 35 watts of power are required for a digital beamforming instrument whereas an analog beamforming instrument requires a minimum of 15 watts of power. The digital beamformer is more precise in performance, but

the analog to digital and digital to analog signal conversions require considerably more power than the analog beamformer which requires no conversion and relies on phase modulation in beamforming.

[0006] The article by Juin-Jet Hwang et al entitled "Portable ultrasound device for battlefield trauma" published in the Ultrasonics Symposium Proceedings of the IEEE which took place on October 5-8 1998 and published in Volume 2, pages 1663-1667 discloses that a hand-held portable ultrasound device may have an extended battery life by disabling hardware which is not in active use in various usage modes.

[0007] The present invention is directed to providing a portable ultrasonic diagnostic instrument, either digital, analog or hybrid, with reduced power in operation.

SUMMARY OF THE INVENTION

[0008] According to the present invention there is provided a portable ultrasonic diagnostic instrument and a method of operating a portable ultrasonic diagnostic instrument as claimed in the appended claims.

[0009] In accordance with the invention a portable ultrasonic diagnostic instrument is provided which includes an array transducer, a beamformer for delaying and combining echo signals received by elements of the array transducer, signal processing and imaging circuitry for processing the echo signals, and a display for the processed echo signals, wherein the instrument operates on no more than 25 watts of electrical power. In one embodiment with an analog beamformer, the instrument operates on no more than 10 watts of power.

[0010] More particularly, the portable ultrasonic diagnostic instrument operates from battery power, and power control is provided for limiting power consumption in the instrument to 25 watts for a digital beamformer instrument or 10 watts for an analog beamformer instrument. Before operation of the instrument, various modes of operation are evaluated for required circuit functions, and other circuit functions are powered down or turned-off to conserve power. For example, B mode scanning does not require color power angiography and this function is turned-off. Similarly, sampling at a lower rate allows the analog to digital function to operate at a lower frequency thus reducing power consumption. In a sleep mode, the monitor display intensity can be diminished. Further, during operation of the instrument, current from the battery source to the instrument components is monitored, and when the current reaches a first selected power limit, first functions in the instrument are altered to thereby reduce power consumption. For example, that function can be - the display of processed signals, and the display can be shifted in mode from active scanning to a mode selected from freeze and sleep which require less power. Additionally, un-needed functional blocks such as color display and 3D display of processed signals can be turned off. In a digital beamformer instrument, considerable power is expended in the analog to digital

conversion of signals from the ultrasound transducers, and power can be conserved by reducing the clock frequency to the analog to digital converters. Similarly, the clock frequency to the digital signal processor of the instrument can be reduced with attendant power savings. Thus, power reduction can be effected before instrument operation and/or during operation.

[0011] Furthermore, current from the battery source is monitored during instrument operation and first functions in the instrument operation are altered when the power consumption has reached a first power limit, and additional functions when monitored current reaches a second power limit whereby instrument operation is altered in steps. An ultimate threshold can be reached wherein the instrument operation is terminated entirely until troubleshooting of the instrument for possible failure is completed.

[0012] The invention and objects and features thereof will be more readily apparent from the following detailed description and appended claims when taken with the drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013]

Fig. 1 is a functional block diagram of a portable ultrasonic diagnostic instrument including a power monitor and control in accordance with the invention. Fig. 2 is a graphic illustrating operation of the power monitor in Fig. 1.

Fig. 3 is a more detailed functional block diagram of an ultrasonic diagnostic instrument having a digital beamformer and a power monitor in accordance with the invention.

DETAILED DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS

[0014] Fig. 1 is a functional block diagram of a portable ultrasonic diagnostic instrument in which the present invention is employed. Ultrasound transducers 1 generate ultrasonic waves shown generally at 2 and receive reflections of the ultrasonic waves. Wave generation and echo signal processing is accomplished by a beamformer circuit 3 which interfaces with the transducers 1. Signals from the beamformer circuit 3 are then passed to a signal processor 4, and the processed signals are then used to control a display 5. Electric power for the components of the instrument is provided by a battery source 6 which includes a power monitor and control in accordance with the present invention.

[0015] Heretofore, portable ultrasonic diagnostic instruments have been available but have operated at power levels exceeding 35 watts. The present invention limits power consumption to 25 watts for a digital beamformer instrument and 10 watts for an analog beamformer instrument. The digital beamformer instrument has im-

proved fidelity when compared with the analog beamformer, but the analog to digital conversion circuits and amplifiers require considerably more power than does an analog beamformer. For example, a transducer array with 100 elements and analog to digital circuits can expend 64 milliwatts per element or 6.4 watts total just for the analog to digital conversion. Additionally, a time gain control (TGC) amplifier also expends approximately 64 milliwatts per transducer which is an additional 6.4 watts.

[0016] In accordance with the invention, selected circuit functions are powered down or turned-off depending on the operating mode of the instrument. For example, for B mode scanning, the Color Power Angio circuitry is turned-off. For Scan/Transmit without Wide Aperture, the Synthetic Aperture function is not needed and is turned-off. Similarly, if a rough image is sufficient during an operating mode, the Frequency Compounding function is not needed. Two dimensional (2D) mode of operation does not require any 3D processing. Low frequency cardiac imaging permits a reduction in Front End (FE) clock frequency and possibly a reduced frequency for the entire signal path. Analog to Digital conversion speed can be reduced and thus save power when data sampling frequency is reduced.

[0017] Accordingly, power is saved by selective use of instrument circuitry depending on mode of operation of the instrument.

[0018] Fig. 2 is a graph illustrating operation of the power monitor and control in power source 6 of Fig. 1. The graph illustrates power along the coordinate and time along the abscissa. In this example it is assumed that power consumption is to be limited to 15-20 watts during normal operation and in no event to exceed 25 watts of power. A first power limit is defined at 15 watts, a second power limit is defined at 20 watts, and a third power limit is defined at 25 watts. Assume that during instrument operation power consumption rises from 10 watts to 15 watts at Point A on the graph. In accordance with one embodiment of the invention the power monitor and control 6 in Fig. 1 alters first functions in the instrument, as described above, and additionally during operation. For example, when the power reaches Point A (15 watts) function and operating speed can be further reduced in order to reduce power consumption. The first functions can include mode of operation of display 5 with the display switched from active scanning to a freeze mode. Since the display is one of the larger consumers of electrical power, the switch of display mode can limit further increases in power consumption. However, assuming power consumption continues to rise from 15 watts (Point A) to 20 watts (Point B), the power monitor and control will then alter second functions in the instrument operation to further limit power consumption. These alterations can include reducing clock frequency to the digital signal processor and clock frequency to analog to digital circuitry in the beamformer.

[0019] Fig. 3 is a more detailed functional block diagram of an ultrasonic diagnostic instrument having a dig-

ital beamform and further illustrates functions in the instrument which can be altered by the power monitor and control. The instrument is described in more detail in U.S. Patent No. 5,722,412.

[0020] In this instrument a transducer array 10 is used for its solid state, electronic control capabilities, variable aperture, image performance and reliability. Either a flat or curved linear array can be used. In a preferred embodiment the array is a curved array, which affords a broad sector scanning field. While the preferred embodiment provides sufficient delay capability to both steer and focus a flat array such as a phased array, the geometric curvature of the curved array reduces the delay requirements on the beamformer. The elements of the array are connected to a transmit/receive ASIC 20 which drives the transducer elements and receives echoes received by the elements. The transmit/receive ASIC 20 also controls the transmit and receive apertures of the array 10 and the gain of the received echo signals. The transmit/receive ASIC is preferably located within inches of the transducer elements, preferably in the same enclosure, and just behind the transducer.

[0021] Echoes received by the transmit/receive ASIC 20 are provided to the adjacent front end ASIC 30, which beamforms the echoes from the individual transducer elements into scanline signals. The front end ASIC 30 also controls the transmit waveform, timing, aperture and focusing. In the illustrated embodiment the front end ASIC 30 provides timing signals for the other ASICs, time gain control, and monitors and controls the power applied to the transducer array, thereby controlling the acoustic energy which is applied to the patient and minimizing power consumption of the unit. A memory device 32 is connected to the front end ASIC 30, which stores data used by the beamformer.

[0022] Beamformer scanline signals are coupled from the front end ASIC 30 to the adjacent digital signal processing ASIC 40. The digital signal processing ASIC 40 filters the scanline signals and in the preferred embodiment also provides several advanced features including synthetic aperture formation, frequency compounding, Doppler processing such as power Doppler (color power angio) processing, and speckle reduction.

[0023] The ultrasound B mode and Doppler information is then coupled to the adjacent back end ASIC 50 for scan conversion and the production of video output signals. A memory device 42 is coupled to the back end ASIC 50 to provide storage used in three dimensional power Doppler (3D CPA) imaging. The back end ASIC also adds alphanumeric information to the display such as the time, date, and patient identification. A graphics processor overlays the ultrasound image with information such as depth and focus markers and cursors. Frames of ultrasonic images are stored in a video memory 54 coupled to the back end ASIC 50, enabling them to be recalled and replayed in a live Cineloop® realtime sequence. Video information is available at a video output in several formats, including NTSC and PAL televi-

sion formats and RGB drive signals for an LCD display 60 or a video monitor.

[0024] The back end ASIC 50 also includes the central processor for the ultrasound system, a RISC (reduced instruction set controller) processor. The RISC processor is coupled to the front end and digital signal processing ASICs to control and synchronize the processing and control functions throughout the hand-held unit. A program memory 52 is coupled to the back end ASIC 50 to store program data which is used by the RISC processor to operate and control the unit. The back end ASIC 50 is also coupled to a data port configured as a PCMCIA interface 56. This interface allows other modules and functions to be attached to the hand-held ultrasound unit. The interface 56 can connect to a modem or communications link to transmit and receive ultrasound information from remote locations. The interface can also accept other data storage devices to add new functionality to the unit, such as an ultrasound information analysis package.

[0025] The RISC processor is also coupled to the user control 70 of the unit to accept user inputs to direct and control the operations of the hand-held ultrasound system.

[0026] Power for the hand-held ultrasound system in a preferred embodiment is provided by a rechargeable battery. Battery power is conserved and applied to the components of the unit from a power subsystem 80. The power subsystem 80 includes a DC converter to convert the low battery voltage to a higher voltage which is applied to the transmit/receive ASIC 20 to drive the elements of the transducer array 10.

[0027] The power monitor and control in unit 80 operates in accordance with the description with reference to Fig. 2 and controls the operating mode of the LCD display 60 and video circuitry in unit 50 along with the clock frequency of the RISC processor in unit 50 and the clock frequencies of the VCA and ADC units in beamformer circuitry 30. The color power and geography function unit and 3D signal processing of DSP unit 40 are similarly controlled by the power monitor and control.

[0028] In Fig. 3, power consumption is controlled by power monitor and control block 80 and master clock control 90 which are both controlled by the RISC processor in block 50. The overall signal path depicted in Fig. 3 contains various functional blocks such as the analog to digital converters (ADC) 34 in block 30, the color power angio processor 44 in block 40, and the frequency compounding processor 46 in block 40. Each such functional block may be turned off individually by the power monitor and control circuit 80. As an example, when the ultrasound system is imaging in B-mode only, the color power angio block 44 is not needed and is turned off.

[0029] In addition to controlling whether functional blocks are on or off, power monitor and control block 80 controls the bias current supplied to ADC block 34. Lower frequency operation typically requires less bias current. Similarly, voltage and current supplied to transmit/receive block 20 is controlled as appropriate. As an exam-

ple, superficial imaging typically will require less transmitted power than deep abdominal imaging.

[0030] Power monitor and control block 80 also controls power to LCD display 60, and in particular to the backlight associated with the LCD display. The display may be provided with less current (dimmed) to conserve power.

[0031] In terms of overall system operation, the system may be in one of several power conservation modes at any particular time. For example, a full operation mode may draw the most power, while a "freeze" mode that allows review of stored images but not active scanning would draw less power. A sleep mode where the display and most other functions are disabled would draw even less power, while a power-off mode would draw no power. Power monitor and control block 80 controls transitions between these states based on algorithms executed by the RISC processor contained in block 50.

[0032] In the preferred embodiment, many of the functional blocks described are embedded in Application Specific Integrated Circuits (ASICs) 20, 30, 40, and 50 in Fig. 1. The choice of which functions to integrate on each ASIC relates to power consumption. For example, the integration of ADC blocks 34 and delay and sum blocks 36 and 38 are integrated in the same ASIC to conserve power. Separation of these elements would require higher current driver circuitry for communication between blocks.

[0033] The use of power monitor and control functions in a portable ultrasonic diagnostic instrument limits power consumption and enables an instrument operating within a limited power range. While the invention has been described with reference to specific embodiments the description illustrative of the invention and is not to be construed as limiting the invention. Various modifications and applications may occur to those skilled in the art without departing from the scope of the invention as defined by the appended claims.

Claims

1. A method of operating a portable ultrasonic diagnostic instrument having ultrasound transducers (1) for transmitting and receiving ultrasonic waves, beamforming circuitry (3) for focusing transmitted and received waves and a battery source (6) of electrical current for the circuitry, the method comprising the steps of monitoring power and altering first circuitry functions when the monitored power reaches a predetermined first power limit, the first circuitry functions that are altered depending on the mode of operation of the instrument; and altering second functions in instrument operation when the monitored power reaches a predetermined second power limit; the altering steps having the effect of reducing power consumption.
2. The method as defined by claim 1 wherein the instrument further includes signal processing circuitry (4), imaging circuitry for controlling a display of processed signals, and a display (5) and wherein the first functions and second functions are selected from display operation, colour signal processing, 3D signal processing, clock frequency for analog to digital signal conversion and clock frequency for data processing.
3. The method as defined by claim 2 wherein the step of altering the first circuitry functions includes altering display of processed signals.
4. The method as defined by claim 3 wherein the display of processed signals is shifted in mode from active scanning to a mode selected from freeze and sleep.
5. A portable ultrasonic diagnostic instrument comprising:
 - a) ultrasound transducers (1) for transmitting and receiving ultrasonic waves,
 - b) beamforming circuitry (3) for focusing transmitted and received waves,
 - c) a display (5),
 - d) battery power (6), and
 - e) power control (6) for limiting power consumption in the instrument not to exceed 25 watts, wherein said power control alters one or more first functions of said portable ultrasonic diagnostic instrument when power consumption reaches a predetermined first power limit and said power control alters second functions in instrument operation when power consumption reaches a predetermined second power limit.
6. The portable ultrasonic diagnostic instrument as defined by claim 5 wherein the beamforming circuitry (3) is digital.
7. The portable ultrasonic diagnostic instrument as defined by claim 6 wherein the power control (6) reduces clock frequency to analog to digital converter circuitry in the beamforming circuitry (3) when power consumption exceeds one of said first and second power limits.
8. The portable ultrasonic diagnostic instrument as defined by claim 7 and further including:
 - f) signal processing circuitry (4) for processing electrical signals from received waves,
 - g) imaging circuitry for controlling a display of processed signals, and
 - h) a display (5).

9. The portable ultrasonic diagnostic instrument as defined by claim 5 wherein the power control (6) blocks color display and 3D display of processed signals.
10. The portable ultrasonic diagnostic instrument as defined by claim 9 wherein the power control (6) alters display of processed signals.
11. The portable ultrasonic diagnostic instrument as defined by claim 10 wherein the display of processed signals is shifted in mode from active scanning to a mode selected from freeze and sleep.
12. The portable ultrasonic diagnostic instrument as defined by claim 5 wherein the beamforming circuitry (3) is analog and the power control (6) limits power consumption to 10 watts.
13. The portable ultrasonic diagnostic instrument as defined by claim 5, wherein the first and second functions are selected from display operation, color signal processing, 3D signal processing, clock frequency for analog to digital conversion, and clock frequency for data processing.

Patentansprüche

1. Verfahren zum Betreiben eines tragbaren Ultraschall Diagnoseinstruments mit Ultraschallwandlern (1) zum Senden und Empfangen von Ultraschallwellen, einer Strahlformungsschaltungsanordnung (3) zum Fokussieren gesendeter und empfangener Wellen und einer Batteriequelle (6) eines elektrischen Stroms für die Schaltungsanordnung, wobei das Verfahren die Schritte umfasst des Überwachens von Leistung und des Änderns von ersten Schaltungsanordnungsfunktionen, wenn die überwachte Leistung einen vorbestimmten ersten Leistungsgrenzwert erreicht, wobei die ersten Schaltungsanordnungsfunktionen, die geändert werden, vom Betriebsmodus des Instruments abhängen; und Ändern von zweiten Funktionen beim Betrieb des Instruments, wenn die überwachte Leistung einen vorbestimmten zweiten Leistungsgrenzwert erreicht; wobei die Änderungsschritte den Effekt der Verringerung des Leistungsverbrauchs haben.
2. Verfahren nach Anspruch 1, wobei das Instrument ferner eine Signalverarbeitungsschaltungsanordnung (4), eine Bildgebungsschaltungsanordnung zum Steuern einer Anzeige von verarbeiteten Signalen und eine Anzeige (5) umfasst und wobei die ersten Funktionen und zweiten Funktionen aus Anzeigebetrieb, Farbsignalverarbeitung, 3D-Signalverarbeitung, Taktfrequenz für Analog-Digital-Signalumsetzung und Taktfrequenz für Datenverarbeitung ausgewählt sind.

3. Verfahren nach Anspruch 2, wobei der Schritt des Änderns der ersten Schaltungsanordnungsfunktionen das Ändern der Anzeige von verarbeiteten Signalen beinhaltet.
4. Verfahren nach Anspruch 3, wobei die Anzeige verarbeiteter Signale aus dem Modus des aktiven Abtastens in einen Modus ausgewählt aus Einfrier- und Ruhemodus umgeschaltet wird.
5. Tragbares Ultraschall Diagnoseinstrument umfassend:
 - a) Ultraschallwandler (1) zum Senden und Empfangen von Ultraschallwellen,
 - b) eine Strahlformungsschaltungsanordnung (3) zum Fokussieren gesendeter und empfangener Wellen,
 - c) eine Anzeige (5),
 - d) Batterieleistung (6) und
 - e) eine Leistungssteuerung (6) zum Begrenzen des Leistungsverbrauchs im Instrument auf nicht mehr als 25 Watt, wobei die Leistungssteuerung eine oder mehrere erste Funktionen des tragbaren Ultraschall Diagnoseinstruments ändert, wenn der Leistungsverbrauch einen vorbestimmten ersten Leistungsgrenzwert erreicht, und die Leistungssteuerung zweite Funktionen beim Betrieb des Instruments ändert, wenn der Leistungsverbrauch einen vorbestimmten zweiten Leistungsgrenzwert erreicht.
6. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 5, wobei die Strahlformungsschaltungsanordnung (3) digital ist.
7. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 6, wobei die Leistungssteuerung (6) die Taktfrequenz für die Analog-Digital-Umsetzungsschaltungsanordnung in der Strahlformungsschaltungsanordnung (3) verringert, wenn der Leistungsverbrauch einen der ersten und zweiten Leistungsgrenzwerte überschreitet.
8. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 7, ferner umfassend:
 - f) eine Signalverarbeitungsschaltungsanordnung (4) zum Verarbeiten elektrischer Signale von empfangenen Wellen,
 - g) eine Bildgebungsschaltungsanordnung zum Steuern einer Anzeige verarbeiteter Signale, und
 - h) eine Anzeige (5).
9. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 5, wobei die Leistungssteuerung (6) eine Farbanzeige und 3D-Anzeige verarbeiteter Signale

blockiert.

10. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 9, wobei die Leistungssteuerung (6) die Anzeige verarbeiteter Signale ändert.
11. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 10, wobei die Anzeige verarbeiteter Signale aus dem Modus des aktiven Abtastens in einen Modus ausgewählt aus Einfrier- und Ruhemodus umgeschaltet wird.
12. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 5, wobei die Strahlformungsschaltungsanordnung (3) analog ist und die Leistungssteuerung (6) den Leistungsverbrauch auf 10 Watt begrenzt.
13. Tragbares Ultraschall Diagnoseinstrument nach Anspruch 5, wobei die ersten und zweiten Funktionen aus Anzeigebetrieb, Farbsignalverarbeitung, 3D-Sigrtalverarbeitung, Taktfrequenz für Analog-Digital-Umsetzung und Taktfrequenz für Datenverarbeitung ausgewählt sind.

Revendications

1. Procédé pour faire fonctionner un instrument portable de diagnostic par ultrasons ayant des transducteurs (1) d'ultrasons pour l'émission et la réception d'ondes ultrasonores, un circuit (3) de mise en forme de faisceau pour focaliser des ondes émises et reçues et une source (6) de courant électrique à batterie pour le circuit, le procédé comprenant les étapes de contrôle de puissance et de modification de premières fonctions du circuit lorsque la puissance contrôlée atteint une première limite prédéterminée de puissance, les premières fonctions du circuit qui sont modifiées dépendant du mode de fonctionnement de l'instrument, et de modifications de secondes fonctions pendant le fonctionnement de l'instrument lorsque la puissance contrôlée atteint une seconde limite de puissance prédéterminée ; les étapes de modifications ayant pour effet de réduire la consommation d'énergie.
2. Procédé selon la revendication 1, dans lequel l'instrument comprend en outre un circuit (4) de traitement de signaux, un circuit de formation d'image destiné à commander un affichage de signaux traités, et un afficheur (5), et dans lequel les premières fonctions et les secondes fonctions sont sélectionnées à partir d'une opération d'affichage, d'un traitement de signaux de couleur, d'un traitement de signaux 3D, d'une fréquence d'horloge pour une conversion de signaux analogiques en signaux numériques et une fréquence d'horloge pour un traitement de données.

3. Procédé selon la revendication 2, dans lequel l'étape de modification des premières fonctions de circuit comprend une modification de l'affichage de signaux traités.

4. Procédé selon la revendication 3, dans lequel l'affichage de signaux traités est modifié d'un mode à balayage actif en un mode sélectionné entre un fi-geage et une veille.

5. Instrument portable de diagnostic par ultrasons comportant :

- a) des transducteurs (1) à ultrasons pour l'émission et la réception d'ondes ultrasonores,
- b) un circuit (3) de mise en forme de faisceau pour focaliser des ondes émises et reçues,
- c) un afficheur (5),
- d) une alimentation (6) en énergie à batterie, et
- e) une commande de puissance (6) pour limiter la puissance consommée dans l'instrument afin qu'elle ne dépasse pas 25 watts, dans lequel ladite commande de puissance modifie une ou plusieurs premières fonctions dudit instrument portable de diagnostic par ultrasons lorsque la puissance consommée atteint une première limite de puissance prédéterminée et ladite commande de puissance modifie des secondes fonctions pendant le fonctionnement de l'instrument lorsque la puissance consommée atteint une seconde limite de puissance prédéterminée.

6. Instrument portable de diagnostic par ultrasons selon la revendication 5, dans lequel le circuit (3) de mise en forme de faisceau est numérique.

7. Instrument portable de diagnostic par ultrasons selon la revendication 6, dans lequel la commande (6) de puissance réduit la fréquence d'horloge pour un circuit de convertisseur analogique-numérique dans le circuit (3) de mise en forme de faisceau lorsque la puissance consommée dépasse lesdites première et seconde limites de puissance.

8. Instrument portable de diagnostic par ultrasons selon la revendication 7, et comprenant en outre :

- f) un circuit (4) de traitement de signaux pour le traitement de signaux électriques provenant d'ondes reçues,
- g) un circuit de formation d'image pour la commande d'un affichage de signaux traités, et
- h) un afficheur (5).

9. Instrument portable de diagnostic par ultrasons selon la revendication 5, dans lequel la commande de puissance (6) bloque un affichage en couleurs et un

affichage 3D de signaux traités.

- 10.** Instrument portable de diagnostic par ultrasons selon la revendication 9, dans lequel la commande de puissance (6) modifie l'affichage de signaux traités. 5
- 11.** Instrument portable de diagnostic par ultrasons selon la revendication 10, dans lequel l'affichage de signaux traités est modifié d'un mode à balayage actif à un mode sélectionné entre un figeage et une veille. 10
- 12.** Instrument portable de diagnostic par ultrasons selon la revendication 5, dans lequel le circuit (3) de mise en forme de faisceau est analogique et la commande (6) de puissance limite la puissance consommée à 10 watts. 15
- 13.** Instrument portable de diagnostic par ultrasons selon la revendication 5, dans lequel les premières et secondes fonctions sont sélectionnées parmi une opération d'affichage, un traitement de signaux de couleurs, un traitement de signaux 3D, une fréquence d'horloge pour une conversion analogique à numérique, et une fréquence d'horloge pour un traitement de données. 20 25

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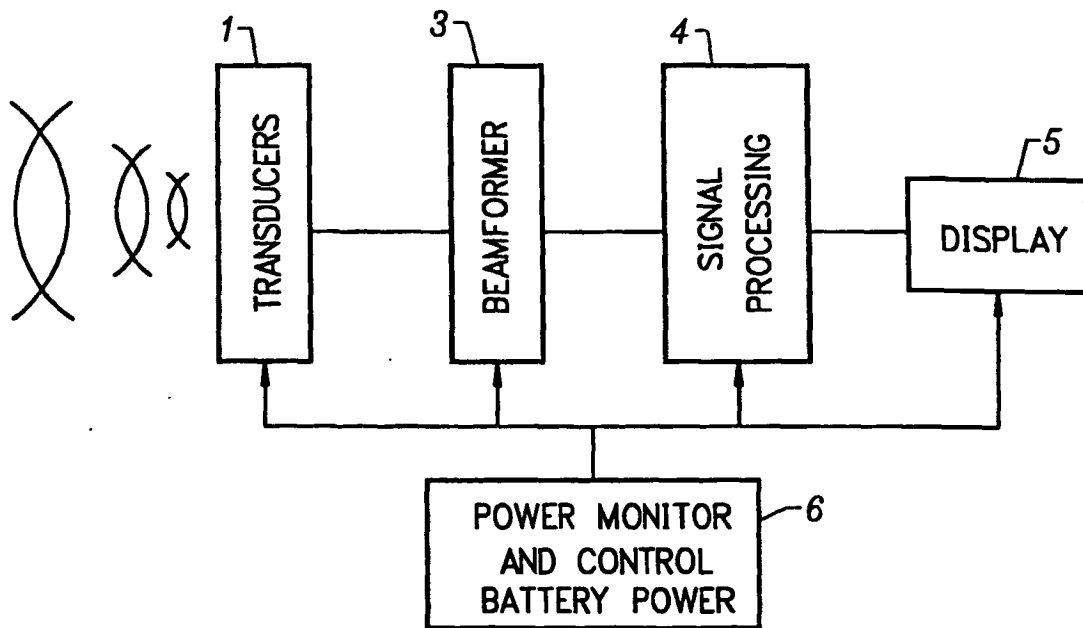


FIG. 1

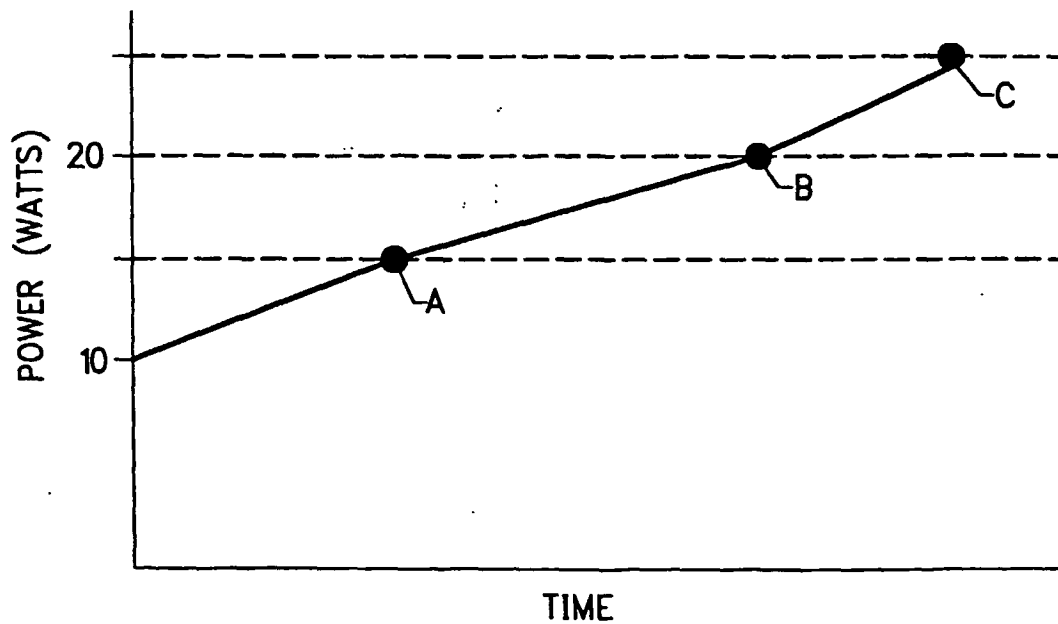


FIG. 2

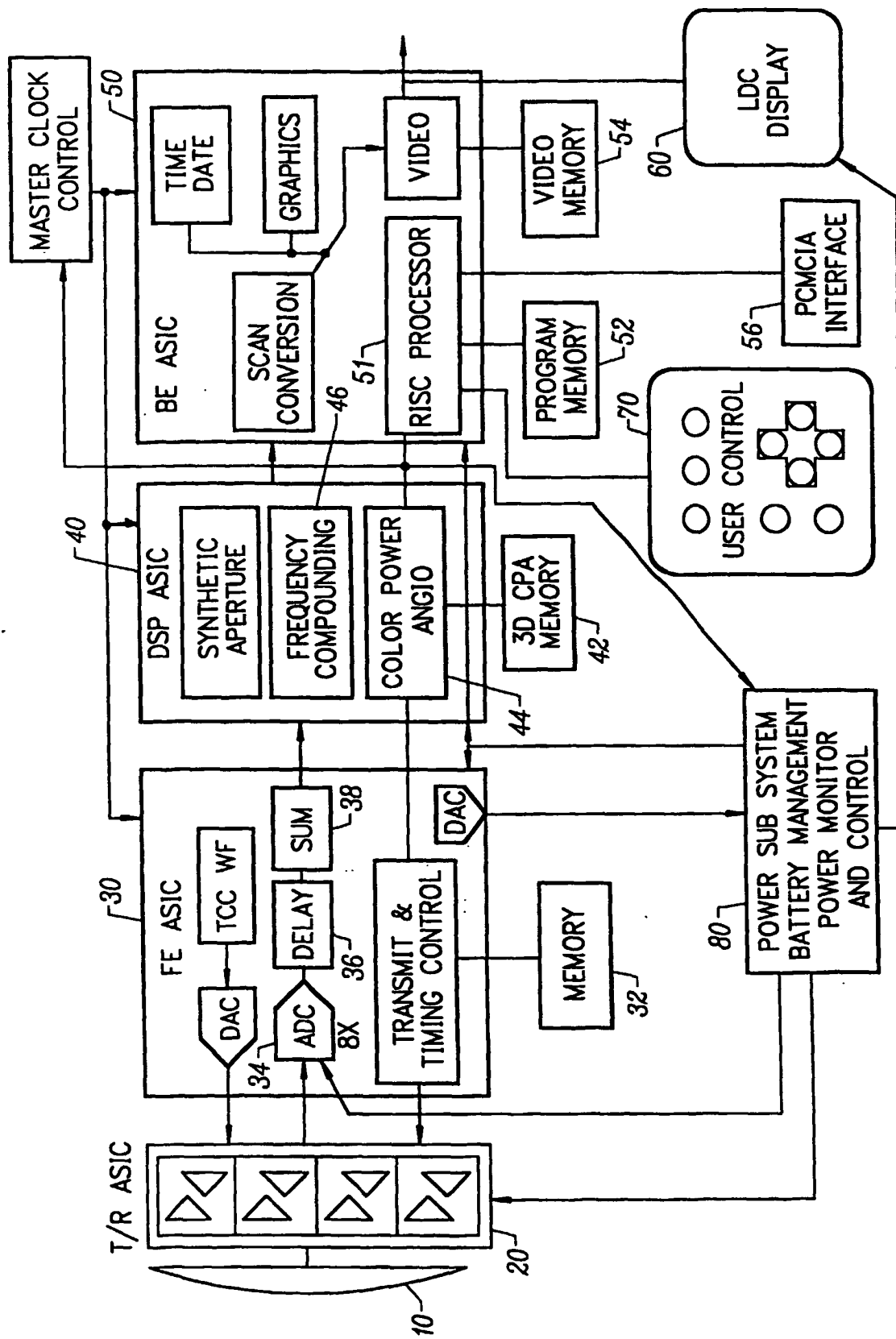


FIG. 3

专利名称(译)	低功耗便携式超声诊断仪		
公开(公告)号	EP1180971A4	公开(公告)日	2004-03-31
申请号	EP2000932064	申请日	2000-05-04
[标]申请(专利权)人(译)	索诺塞特公司		
申请(专利权)人(译)	SONOSITE INC.		
当前申请(专利权)人(译)	SONOSITE INC.		
[标]发明人	HWANG JUIN JET COUGHLIN JUSTIN M DHATT DAVIN JONES GEOFFREY LITTLE BLAKE W		
发明人	HWANG, JUIN-JET COUGHLIN, JUSTIN, M. DHATT, DAVIN JONES, GEOFFREY LITTLE, BLAKE, W.		
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优先权	09/564299 2000-05-03 US 60/132558 1999-05-05 US		
其他公开文献	EP1180971B1 EP1180971A1		
外部链接	Espacenet		

摘要(译)

便携式超声诊断仪器包括阵列换能器，波束形成器，信号处理和成像电路，以及用于处理的回波信号的显示器，其工作电压不超过25瓦。电路功能可以根据仪器的操作模式选择参加，从而降低功耗。此外，功率监视器和控制可以监视来自电池电源的电流，并且当功耗达到预定水平时，功率监视器和控制进一步改变仪器中的一个或多个功能单元，包括显示操作模式，时钟频率。用于模数转换和信号处理，颜色信号处理和3D信号处理。可以针对两个或更多个预定水平来监视功耗，其中根据已经达到的功耗水平来改变仪器功能单元或操作模式。在具有模拟波束形成器的仪器中，功耗可以被限制为10瓦，而在数字波束形成器中，功耗可以被限制为不超过25瓦。