

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
23 December 2009 (23.12.2009)

(10) International Publication Number  
**WO 2009/154298 A1**

- (51) **International Patent Classification:**  
A61B 5/00 (2006.01) A61B 8/14 (2006.01)
- (21) **International Application Number:**  
PCT/JP2009/061434
- (22) **International Filing Date:**  
17 June 2009 (17.06.2009)
- (25) **Filing Language:** English
- (26) **Publication Language:** English
- (30) **Priority Data:**  
2008-159314 18 June 2008 (18.06.2008) JP  
2009-136365 5 June 2009 (05.06.2009) JP
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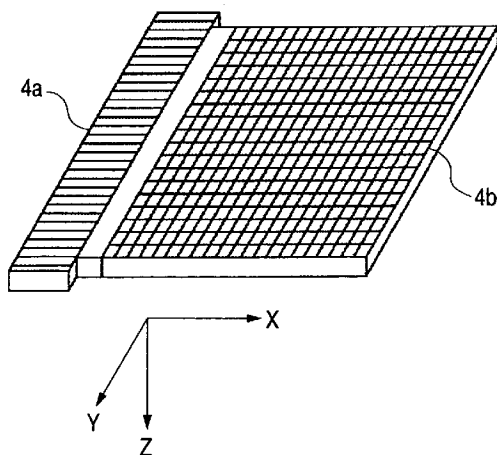
(81) **Designated States (unless otherwise indicated, for every kind of national protection available):** AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IS, KE, KG, KM, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PE, PG, PH, PL, PT, RO, RS, RU, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

(84) **Designated States (unless otherwise indicated, for every kind of regional protection available):** ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

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(54) **Title:** ULTRASONIC PROBE, AND PHOTOACOUSTIC-ULTRASONIC SYSTEM AND INSPECTION OBJECT IMAGING APPARATUS INCLUDING THE ULTRASONIC PROBE

FIG. 1B



(57) **Abstract:** Provided are an ultrasonic probe capable of forming an image without degradation even when the frequency band of a photoacoustic wave and the frequency band of an ultrasonic wave used in ultrasonography are separated from each other, and an inspection object imaging apparatus including the ultrasonic probe. The ultrasonic probe includes a first array device capable of transmitting and receiving an ultrasonic wave; and a second array device capable of receiving a photoacoustic wave. The first array device includes plural electromechanical transducers arranged in a direction perpendicular to a scanning direction, the second array device includes plural electromechanical transducers arranged in a two-dimensional manner, and the first array device and the second array device are provided on the same plane and in the scanning direction.

WO 2009/154298 A1

**Published:**

— with international search report (Art. 21(3))

— before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments (Rule 48.2(h))

## DESCRIPTION

ULTRASONIC PROBE, AND PHOTOACOUSTIC-ULTRASONIC SYSTEM AND  
INSPECTION OBJECT IMAGING APPARATUS INCLUDING THE  
5 ULTRASONIC PROBE

## TECHNICAL FIELD

The present invention relates to an ultrasonic probe  
for transmitting and receiving an ultrasonic wave and for  
10 receiving a photoacoustic wave, and to a photoacoustic-  
ultrasonic system and an inspection object imaging  
apparatus including the ultrasonic probe.

## BACKGROUND ART

15 A conventional tomographic imaging apparatus which  
obtains a tomographic image using an ultrasonic wave  
includes: a probe for transmitting an ultrasonic wave to a  
sample and receiving the reflected ultrasonic wave; a  
transmitting portion for supplying an ultrasonic signal to  
20 the probe; a receiving portion for receiving the reflected  
wave; and a unit for converting the received reflected wave  
signal into a luminance signal for visualization. When a  
time-series tomographic image acquired by the apparatus is  
used, it is possible to observe an inside of a sample. In  
25 the apparatus according to one mode, a unit for performing  
scanning of a probe two-dimensionally scans a sample with  
an ultrasonic wave to obtain a three-dimensional image.

Meanwhile, in examining an inspection object, apparatuses which display not only a morphologic image but also a functional image have progressively been developed in recent years. As one of such apparatuses as described  
5 above, there is an apparatus which utilizes a photoacoustic spectroscopy. In the photoacoustic spectroscopy, visible light, near-infrared light, or mid-infrared light each having a predetermined wavelength is applied to the inspection object. Then, a specific substance inside the  
10 inspection object absorbs energy of the applied light, and as a result of the absorption, an elastic wave (photoacoustic wave) is generated and detected. In this manner, concentration of the specific substance is quantitatively measured. The specific substance inside the  
15 inspection object is, for example, glucose or hemoglobin contained in blood. A technology of acquiring a photoacoustic image through the photoacoustic spectroscopy is disclosed in, for example, Japanese Patent Application Laid-Open No. 2001-507952. The technology is referred to  
20 as a photoacoustic tomography (PAT).

In addition, Japanese Patent Application Laid-Open No. 2005-021380 discloses a method of reconstructing both a photoacoustic image and a normal ultrasonic echo image using a one-dimensionally-arranged electromechanical  
25 transducer which is common to the both images; and a structure in which a lighting system using a glass fiber is provided between one-dimensionally-arranged

electromechanical transducers. According to Japanese Patent Application Laid-Open No. 2005-021380, the ultrasonic echo image and the photoacoustic image are simultaneously acquired, thereby displaying a morphologic image and a functional image. In this case, a common probe is used to transmit and receive an ultrasonic wave for forming the ultrasonic echo image and to receive a photoacoustic wave for forming the photoacoustic image.

It should be noted herein that an elastic wave generated by the photoacoustic spectroscopy (photoacoustic imaging method) is referred to as a photoacoustic wave, and a sonic wave which is transmitted and received in a normal pulse echo method is referred to as an ultrasonic wave.

The frequency band of a photoacoustic wave used in the photoacoustic spectroscopy is generally lower than the frequency band of an ultrasonic wave used in ultrasonography. For example, the frequency band of the photoacoustic wave is distributed within a range of 200 KHz to 2 MHz with 1 MHz being a center frequency. The distribution of the frequency band of the photoacoustic wave is lower than a center frequency of 3.5 MHz of the ultrasonic wave used in ultrasonography. According to Japanese Patent Application Laid-Open No. 2005-021380, the common probe is used to receive the photoacoustic wave and the ultrasonic wave used in ultrasonography.

However, as described in Japanese Patent Application Laid-Open No. 2005-021380, when the common probe is used to

receive the photoacoustic wave and the ultrasonic wave which have frequency bands different from each other, there arises a problem that spatial resolution is deteriorated in the ultrasonic image. In order to solve the above-mentioned problem, a harmonic imaging method is used in Japanese Patent Application Laid-Open No. 2005-021380. However, a signal contained in a harmonic component is attenuated more than a signal contained in a fundamental component, and hence there is a fear that sensitivity may be decreased.

In a case where the frequency band of the photoacoustic wave and the frequency band of the ultrasonic wave are remarkably separated from each other (for example, the center frequency band of the photoacoustic wave is approximately 1 MHz and the center frequency band of the ultrasonic wave is approximately 10 MHz), the above-mentioned problem becomes more remarkable when the common probe is used to receive the waves as described in Japanese Patent Application Laid-Open No. 2005-021380.

Moreover, with regard to a photoacoustic-ultrasonic system including an ultrasonic probe and an optical system, the following problem arises. Specifically, according to Japanese Patent Application Laid-Open No. 2005-021380, for generation of a photoacoustic wave, a laser light is introduced using an optical fiber. However, in order to generate the photoacoustic wave, an extremely strong laser light is required, which may adversely affect the fiber.

Particularly, when a sample is thick so that light is attenuated to a large degree, the above-mentioned problem becomes more serious.

According to an experiment conducted by the inventors of the present invention using a dummy inspection object, it was found that, in order to generate a photoacoustic wave strong enough to detect a sample having a thickness exceeding the order of "cm", the intensity of the laser light introduced into the optical fiber exceeds several tens  $\text{kJ}/\text{cm}^2$ , which increases a burden on the optical fiber. Therefore, the optical fiber may not be selected as the optical system for detecting a sample having a certain volume.

#### 15 DISCLOSURE OF THE INVENTION

An object of the present invention is to provide an ultrasonic probe capable of forming an image without degradation even when a frequency band of a photoacoustic wave and a frequency band of an ultrasonic wave used in ultrasonography are separated from each other, and an inspection object imaging apparatus including the ultrasonic probe.

Another object of the present invention is to provide a photoacoustic-ultrasonic system including the ultrasonic probe and an optical system, which is capable of applying pulse light having a strong light intensity for detecting a sufficient photoacoustic wave.

In view of the above-mentioned objects, the present invention provides an ultrasonic probe, comprising: a first array device capable of transmitting and receiving an ultrasonic wave; and a second array device capable of receiving a photoacoustic wave, wherein the first array device includes plural electromechanical transducers arranged in a first direction; the second array device includes plural electromechanical transducers arranged two-dimensionally; and the first array device and the second array device are provided on the same plane and in a second direction perpendicular to the first direction.

The present invention also provides a photoacoustic-ultrasonic system, comprising: an optical system for introducing light emitted from a light source into an inspection object; and the ultrasonic probe, wherein the optical system is provided in an interspace between the first array device and the second array device.

The present invention also provides an inspection object imaging apparatus, comprising: a light source for generating pulse light; the ultrasonic probe; and a system control unit for controlling the light source and the ultrasonic probe to form an image. The system control unit forms an image based on morphologic information inside an inspection object by using the first array device and forms an image based on functional information inside the inspection object by using the light source and the second array device.

According to the present invention, there can be provided an ultrasonic probe capable of forming an image without degradation even when the frequency band of the photoacoustic wave and the frequency band of the ultrasonic wave used in ultrasonography are separated from each other, and an inspection object imaging apparatus including the ultrasonic probe.

Other features and advantages of the present invention will be apparent from the following description taken in conjunction with the accompanying drawings, in which like reference characters designate the same or similar parts throughout the figures thereof.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1A is a view illustrating an ultrasonic probe according to an embodiment of the present invention;

FIG. 1B is a view illustrating an arrangement of an ultrasonic transducer and a photoacoustic transducer which form a transducer used in the ultrasonic probe according to the embodiment of the present invention;

FIG. 2 is a diagram illustrating a configuration of an inspection object imaging apparatus including the ultrasonic probe according to the embodiment of the present invention;

FIG. 3 is a diagram for describing a signal collection method using the ultrasonic probe according to the embodiment of the present invention;

FIG. 4 is a diagram illustrating a beam shape of the ultrasonic transducer according to the present invention;

FIG. 5 is a diagram illustrating a beam shape of the ultrasonic transducer in a height direction thereof according to the present invention;

FIG. 6 is a graph illustrating a relation between the ultrasonic probe and a beam thickness of the ultrasonic transducer in the height direction according to the present invention;

FIG. 7A is a perspective view illustrating a photoacoustic-ultrasonic system including an ultrasonic probe and an optical system according to another embodiment of the present invention; and

FIG. 7B is a cross-sectional view of the photoacoustic-ultrasonic system, which illustrates incidence of light.

#### BEST MODE FOR CARRYING OUT THE INVENTION

Preferred embodiments of the present invention are now described in detail in accordance with the accompanying drawings.

Hereinafter, the present invention is described in more detail with reference to the accompanying drawings. It should be noted that the same components are denoted by the same reference symbol in general, and description thereof is omitted.

*First Embodiment: Ultrasonic Probe and Inspection Object*

*Imaging Apparatus*

An ultrasonic probe according to this embodiment includes a first array device capable of transmitting and receiving an ultrasonic wave; and a second array device  
5 capable of receiving a photoacoustic wave. The first array device includes plural electromechanical transducers arranged in a first direction. The second array device includes plural electromechanical transducers arranged two-dimensionally. The first array device and the second array  
10 device are provided on the same plane and in a second direction. In the present invention, the "same plane" is not necessarily required to be strictly the same plane as long as the plane can be regarded as substantially the same plane. In the definition of "substantially the same plane",  
15 it is acceptable that the plane on which the array devices are provided includes irregularities within a range of processing accuracy and includes inclination or level difference as long as the contact condition between an inspection object and the array device is not adversely  
20 affected. Even when irregularities or the like are intentionally provided on a surface of the plane in order to reduce contact resistance with the inspection object, similarly to the above-mentioned case, the irregularities or the like are acceptable as long as the contact condition  
25 between the inspection object and the array device is not adversely affected.

In the ultrasonic probe and an inspection object

imaging apparatus including the ultrasonic probe according to this embodiment, the second direction is typically a scanning direction and the first direction is typically a direction perpendicular to the scanning direction.

5           The ultrasonic probe and the inspection object imaging apparatus including the ultrasonic probe according to this embodiment may acquire an image of the inspection object even in a rest state without scanning the first array device and the second array device.

10           Hereinafter, description is specifically made with reference to the accompanying drawings. FIGS. 1A and 1B are structural views of the ultrasonic probe according to the present invention. FIG. 1A is a schematic view and FIG. 1B is an enlarged view illustrating a transducer portion.

15           The ultrasonic probe includes a probe case 30, a cable 31, and a transducer 4. The transducer 4 is comprised of an ultrasonic transducer 4a which is the first array device capable of transmitting and receiving an ultrasonic wave; and a photoacoustic transducer 4b which is the second array

20           device capable of receiving a photoacoustic wave. A one-dimensional (linear) array is employed for the ultrasonic transducer 4a while a two-dimensional array is employed for the photoacoustic transducer 4b.

          The ultrasonic transducer 4a is used for revealing

25           morphologic information of the inside of the inspection object, and therefore is a transducer capable of transmitting and receiving an ultrasonic wave higher in

frequency than a photoacoustic wave received by the photoacoustic transducer 4b which acquires functional information. Here, the frequency band of the ultrasonic transducer 4a is 7 to 12 MHz as a typical value. The  
5 "morphologic information" is information which is based on a morphology of the inside of the inspection object and obtained by a normal pulse echo method.

On the other hand, the photoacoustic transducer 4b is used for revealing functional information of the inside of  
10 the inspection object, and therefore is a transducer capable of receiving an ultrasonic wave (photoacoustic wave) lower in frequency than an ultrasonic wave transmitted and received by the ultrasonic transducer 4a which acquires morphologic information. Here, the  
15 frequency band of the photoacoustic transducer 4b is 1 to 4 MHz as a typical value. The "functional information" is information which is obtained by a photoacoustic spectroscopy (photoacoustic imaging method) and relates to concentration of a specific substance inside the inspection  
20 object, such as glucose or hemoglobin contained in blood.

The reason why the one-dimensional array is employed for the ultrasonic transducer 4a is as follows. The ultrasonic transducer 4a transmits and receives an ultrasonic wave having a relatively high frequency, and  
25 hence the device density thereof needs to be made high. For example, the number of transducer arrays is as large as 128 to 256 even in the one-dimensional array. Therefore,

when the two-dimensional array is employed for the ultrasonic transducer 4a, it is not appropriate in terms of costs.

The main reason why the two-dimensional array is employed for the photoacoustic transducer 4b is that light utilization efficiency is regarded as important. Specifically, when photoacoustic waves generated by one irradiation with laser light are received by two-dimensionally-arranged devices, larger number of photoacoustic waves can be received compared with a case where the devices are one-dimensionally arranged. The photoacoustic wave is generally lower in frequency than an ultrasonic echo, and hence the device density can be suppressed to be small. Accordingly, the two-dimensional array has a small influence on costs. The number of transducer arrays in one line is approximately 10 to 50.

The ultrasonic transducer 4a includes the plural electromechanical transducers. The electromechanical transducer is a device which conducts mutual conversion between an electrical signal and a mechanical vibration (ultrasonic wave), and, for example, a piezoelectric device is used therefor. The plural electromechanical transducers are arranged in a direction (first direction) perpendicular to the scanning direction.

The photoacoustic transducer 4b is a device in which the electromechanical transducers are two-dimensionally arranged. Examples of the electromechanical transducer

include a transducer using a piezoelectric phenomenon, a  
transducer using optical resonance, and a transducer using  
a change in capacity. Any detector may be employed as the  
electromechanical transducer as long as the detector can  
5 detect an acoustic wave. In a case where sizes of  
detection targets vary widely, bands of generated  
photoacoustic waves are also widened, and hence a required  
transducer favorably has a wide detection band. In  
consideration of the above-mentioned aspect, an  
10 electrostatic capacity type ultrasonic transducer, which  
has actively been studied in recent years, is one of most  
suitable transducers for the object of the present  
invention. Alternatively, when a device in which plural  
transducers having different detection bands are combined  
15 is employed, the same effect can be expected.

The ultrasonic probe according to this embodiment is  
manufactured in the following manner. First, the  
ultrasonic transducer 4a (one-dimensional array transducer)  
and the photoacoustic transducer 4b (two-dimensional array  
20 transducer) are manufactured by a method similar to the  
conventional method. The method includes cutting out a  
piezoelectric transducer; fixing the transducer to a  
backing material; dicing the transducer; bonding an  
acoustic matching layer; and leading out a wiring portion.  
25 In addition, an acoustic lens is attached to the ultrasonic  
transducer.

The ultrasonic transducer and the photoacoustic

transducer are arranged with a space therebetween, and then fixed by molding. After that, the ultrasonic transducer and the photoacoustic transducer are fit into a housing, whereby the ultrasonic probe is completed.

5           The acoustic matching layer, the backing, and the wiring are provided on an upper surface and a lower surface of each of the transducers, and the acoustic lens is provided on the upper surface of the ultrasonic transducer. Those components are omitted in FIGS. 1A and 1B.

10           The ultrasonic transducer 4a and the photoacoustic transducer 4b have a positional relation in which the ultrasonic transducer 4a is provided in parallel to any one of four sides of the photoacoustic transducer 4b which is two-dimensionally arrayed. In this embodiment, the two  
15           array devices are housed in one probe case 30. Alternatively, a probe case that houses the ultrasonic transducer 4a and a probe case that houses the photoacoustic transducer 4b may be provided to form one  
20           probe as a whole. In this case, the two array devices are only required to be on the same plane and may be located with a certain space therebetween.

          FIG. 2 is a block diagram illustrating an inspection object imaging apparatus using the ultrasonic probe according to this embodiment. In order to transmit an  
25           ultrasonic wave from the ultrasonic transducer 4a, an ultrasonic signal is generated through a system control unit 1, a transmission beam former 2, and a transmission

amplifier 3, and then a voltage is applied to the ultrasonic transducer 4a. The transmitted ultrasonic wave is reflected on an inspection object 14 and received by the ultrasonic transducer 4a. The received ultrasonic signal, each of the signals of the respective devices in the ultrasonic probe, is subjected to phasing addition through a reception amplifier 5 and a reception beam former 6. The reception beam former 6 performs analog-digital conversion, delay, and weighting control. Then, the ultrasonic signal is detected and converted into a luminance signal by an ultrasonic signal processing unit 10, and is accumulated in an image memory within an image processing unit 11.

On the other hand, a photoacoustic wave is detected in the following manner. A light source 13 irradiates the inspection object 14 with pulse laser light. The pulse laser light is emitted by transmitting a drive signal from the system control unit 1 to the light source 13. When the inspection object 14 is irradiated with the pulse laser light, a detection target inside the inspection object 14, such as hemoglobin, absorbs energy of the laser light. The temperature of the detection target rises in accordance with the amount of the absorbed energy. As a result of the temperature rise, the detection target momentarily expands to generate an elastic wave (photoacoustic wave). The generated photoacoustic wave is received by the photoacoustic transducer 4b, passes through a reception amplifier 7 and an analog-digital converter 8, and then is

subjected to an image reconstruction processing by a photoacoustic signal processing unit 9. The reconstructed photoacoustic signal is accumulated as a luminance signal in the image memory within the image processing unit 11.

5 Then, the image processing unit 11 superimposes the accumulated ultrasonic signals on the accumulated photoacoustic signals followed by image display by an image display unit 12.

Next, a method of acquiring three-dimensional signals of an ultrasonic signal and a photoacoustic signal with the use of the ultrasonic probe according to this embodiment is described. As described above, the one-dimensional array is employed for the ultrasonic transducer and the two-dimensional array is employed for the photoacoustic transducer, and hence, in order to acquire volume data with the use of the ultrasonic probe according to this embodiment, scanning is performed with the ultrasonic probe.

FIG. 3 is a conceptual diagram of scanning performed with the ultrasonic probe according to this embodiment, and illustrates scanning areas 20a, 20b, and 20c. In the scanning, the ultrasonic probe is moved in the second direction (X direction of FIG. 3) in which the ultrasonic transducer 4a and the photoacoustic transducer 4b are arranged. When the scanning of the scanning area 20a is finished, the ultrasonic probe is moved in a longitudinal direction (Y direction of FIG. 3) by a stripe width of the scanning area and then is moved over the scanning area 20b

in the opposite direction. The above-mentioned scanning is repeatedly performed, whereby signals of an entire inspection area are acquired.

The following three patterns of methods are conceivable for the scanning: (a) a method in which a photoacoustic signal is acquired during a stage suspension period and an ultrasonic signal is acquired during a stage moving period; (b) a method in which a photoacoustic signal and an ultrasonic signal are both acquired during the stage suspension period; and (c) a method in which a photoacoustic signal and an ultrasonic signal are both acquired during the stage moving period. The same signals can be acquired by any one of the above-mentioned methods.

First, in the method (a) in which the photoacoustic signal is acquired during the stage suspension period and the ultrasonic signal is acquired during the stage moving period, the pulse laser is irradiated during the stage suspension period to acquire the photoacoustic signal. After that, the ultrasonic signals are continuously transmitted and received during the stage moving period, and a process of acquiring a slice image at each position is repeated. In this case, for example, the length of the photoacoustic transducer 4b in the scanning direction (X direction) is taken as one step width, and one set of pulse laser irradiation, photoacoustic signal detection and moving by one-step width is repeated. When the transducer 4 is moved by the one-step width, the ultrasonic wave is

acquired using the ultrasonic transducer 4a. The step width of the transducer 4 may be determined based on a range in which the photoacoustic transducer 4b can detect the photoacoustic wave. In other words, in a case where a range in the X direction in which the photoacoustic transducer 4b can detect a photoacoustic wave is narrow, the step width of the transducer 4 is made narrow.

Next, in the method (b) in which the photoacoustic signal and the ultrasonic signal are both acquired during the stage suspension period, the pulse laser is first irradiated during the stage suspension period to acquire the photoacoustic signal. After that, the ultrasonic signals are transmitted and received, and a slice image is acquired. Those procedures may be performed in the opposite order. After the stage is moved, the same process is repeated. In this method, the amount of one stage moving corresponds to that of such an extent that the volume data can be created from the slice image generated by the ultrasonic signal, that is, that of the same order of resolution of the slice image. In this method, when the information on the inspection object can be obtained only by acquiring the image information at one position, the image can be obtained while the stage is suspended without being moved.

In the method (c) in which the photoacoustic signal and the ultrasonic signal are both acquired during the stage moving period, the pulse laser irradiation, the

photoacoustic signal acquisition, and the transmission and reception of the ultrasonic signal are performed during the stage moving period. In this case, the pulse laser is emitted at an operating frequency of ten to several tens hertz, and the transmission and reception of the ultrasonic signal are performed at an operating frequency on the order of kilohertz. Therefore, each data is acquired with a duty ratio therebetween of approximately 100.

As described above, the stripe width (length in Y direction) of the scanning by the transducer 4 is equal to the width of the photoacoustic transducer 4b (two-dimensional array) which is the photoacoustic probe. This is because luminance signals within the volume area are calculated based on the photoacoustic signals at all positions when an image is reconstructed from the photoacoustic signals. Specifically, in a case where the stripe width is thicker than the width of the photoacoustic transducer 4b, there is a portion which is not inspected. Conversely, in a case where the width of the photoacoustic transducer 4b is thicker than the stripe width, there are devices which are not used. Accordingly, an optimum condition for each width is such that the stripe width and the width of the photoacoustic transducer 4b are made equal to each other.

On the other hand, when the ultrasonic transducer 4a which is the ultrasonic probe acquires the ultrasonic signal in the stripe, the length of the one-dimensional

array of the ultrasonic transducer 4a needs to be made longer than the stripe width.

With reference to FIG. 4, a linear scanning of an ultrasonic beam by the ultrasonic transducer 4a is described. FIG. 4 is a diagram illustrating the ultrasonic transducer 4a viewed from the scanning direction (X direction) of the transducer 4. In general, one transmission and one reception of an ultrasonic beam 21 are performed by multiple devices. Therefore, a beam center 22 in a Z direction of FIG. 4 inevitably lies inside with respect to an end surface of the probe. Accordingly, an ultrasonic image obtained by the ultrasonic transducer 4a in a beam scanning direction 23 (Y direction) is narrower than the array width of the ultrasonic transducer 4a by an aperture width used for the beam transmission and reception. Therefore, when the scanning is performed using a linear probe having the same width as the stripe width, there is a portion in which signals are not acquired between the stripes.

When the aperture for the beam transmission and reception is made smaller or when a particular method such as steering is used, imaging is possible also on the end surface of the probe. However, in a case of using those methods, methods of forming a beam are different between the center of the probe and the end surface thereof, which causes nonuniformity in the resolution and image quality.

Therefore, in this embodiment, the array length of

the ultrasonic transducer 4a is made longer than the stripe width, whereby loss of the ultrasonic signals between the stripes can be avoided.

In view of the above, in the transducer 4 according to this embodiment, the length of the ultrasonic transducer 4a in the direction perpendicular to the scanning direction may be set to be longer than the length of the photoacoustic transducer 4b in the direction perpendicular to the scanning direction. The length of the ultrasonic transducer 4a in the direction perpendicular to the scanning direction may be made longer at respective longitudinal ends thereof by one half the length (aperture width) of the device used for transmitting and receiving an ultrasonic wave. As a result, when the increased lengths of the respective longitudinal ends are added, the total length of the ultrasonic transducer 4a becomes longer by a length equal to the aperture width. In general, the aperture of an ultrasonic beam is formed of several tens of devices, and hence the array length of the ultrasonic transducer 4a may be set to be longer than the stripe width by a length corresponding to several tens of devices.

FIG. 5 illustrates a state in which a beam generated by the ultrasonic transducer 4a is focused in a depth direction of the inspection object. The ultrasonic transducer 4a for transmitting and receiving an ultrasonic signal includes an acoustic lens 25 on an entire surface thereof in order to focus a beam also in a height direction

thereof (Z direction). Similarly to the above-mentioned lateral direction beam, an ultrasonic beam is focused while following a locus 24 of FIG. 5. However, a range of acquiring an ultrasonic signal has a certain distance from immediately below the probe, and hence it is difficult to prevent the ultrasonic beam from spreading. The spreading of the ultrasonic beam in this case depends on focus conditions and lens conditions, and may be substantially equal to the height of the probe or may be wider than the height of the probe.

FIG. 6 illustrates a form of the beam generated by the ultrasonic transducer 4a. As illustrated in FIG. 6, the width of the beam generated by the ultrasonic transducer 4a exceeds the width of the ultrasonic transducer 4a in a shallower portion and a deeper portion in the depth direction of the inspection object.

Meanwhile, according to the present invention, the photoacoustic transducer 4b is provided in a portion close to the ultrasonic transducer 4a. Therefore, there is a fear that an interference (crosstalk) between the ultrasonic wave from the ultrasonic transducer 4a and the photoacoustic wave detected by the photoacoustic transducer 4b may be generated. Accordingly, in this embodiment of the present invention, an interspace is provided between the ultrasonic transducer 4a and the photoacoustic transducer 4b, whereby the crosstalk can be prevented. The size of the interspace depends on the width of the

ultrasonic transducer 4a, the focus conditions, and the like. For example, a calculation reveals that there is no problem when the ultrasonic transducer 4a and the photoacoustic transducer 4b are separated from each other in the scanning direction by a distance corresponding to 20% or more of the length of the ultrasonic transducer 4a in the scanning direction.

With the use of the ultrasonic probe described above, all ultrasonic signals and photoacoustic signals can be acquired within the scanning range. In the mode described above, the one-dimensional array probe is employed for acquiring the ultrasonic signal, but the present invention is not limited thereto. Probes generally referred to as 1.25-dimensional array probe, 1.5-dimensional array probe, and 1.75-dimensional array probe, in which devices are further divided in a direction orthogonal to the array direction, may be employed.

The 1.25-dimensional array probe, in which the devices are divided into an odd number of parts in the direction orthogonal to the array direction, has an aperture control function by switching the other devices than a central device. The 1.5-dimensional array probe, in which the devices are divided in the direction orthogonal to the array direction as in the case of the 1.25-dimensional array probe, is capable of independently controlling a central device and symmetrical devices. The 1.75-dimensional array probe, in which the devices are

divided in the direction orthogonal to the array direction as in the case of the 1.25-dimensional array probe, is capable of independently controlling all devices in the direction orthogonal to the array direction. Each of the  
5 1.25-dimensional, 1.5-dimensional, and 1.75-dimensional array probes is mounted for improving focusing and steering functions in the direction orthogonal to the array direction, and the same effect can be obtained by the above-mentioned array probes as in the case where the one-  
10 dimensional array probe is employed.

In the mode described above, the one-dimensional array probe is employed for acquiring the ultrasonic signal and the two-dimensional array probe is employed for acquiring the photoacoustic signal. However, the one-  
15 dimensional array probe may be employed for acquiring both the ultrasonic signal and the photoacoustic signal. In this case, for the relationship of the array lengths of the probes, similarly to the above-mentioned mode, the array length of an array probe for acquiring the ultrasonic  
20 signal is set to be longer than the array length of an array probe for acquiring the photoacoustic signal, thereby obtaining the same effect.

*Second Embodiment: Photoacoustic-ultrasonic System*

Next, a photoacoustic-ultrasonic system in which an  
25 optical system is combined with an ultrasonic probe is described. FIG. 7A is a perspective view illustrating the photoacoustic-ultrasonic system including the ultrasonic

probe and the optical system according to this embodiment.

A first probe for transmitting and receiving an ultrasonic wave includes a probe case 30a, a cable 31a, and a transducer 4a. A second probe for receiving a photoacoustic wave includes a probe case 30b, a cable 31b, and a transducer 4b. The transducer 4a is a first array device capable of transmitting and receiving the ultrasonic wave. The transducer 4b is a second array device capable of receiving the photoacoustic wave. A one-dimensional (linear) array is employed for the ultrasonic transducer 4a while a two-dimensional array is employed for the photoacoustic transducer 4b.

An optical prism 32a is provided in an interspace between the ultrasonic transducer 4a and the photoacoustic transducer 4b. The optical prism 32a serves as an optical system for introducing pulse light emitted from a light source into an inspection object. An optical prism 32b may similarly be provided on a side of the second probe, which is opposite to the optical prism 32a, so as to guide light from both sides of the photoacoustic-ultrasonic system. This is because a target region may need to be irradiated as uniformly as possible due to the fact that the intensity of the generated photoacoustic wave largely depends on an irradiation intensity of laser.

FIG. 7B is a cross-sectional view of the photoacoustic-ultrasonic system according to this embodiment, which illustrates incidence of light. The

light enters a sample as indicated by a broken line of FIG. 7B. The light from the light source (not shown) is first guided in a direction perpendicular to a plane on which the two array devices 4a and 4b are provided. The traveling  
5 direction of the guided light is changed by the optical prisms 32a and 32b, whereby the light is emitted toward below the second array device 4b.

The optical prism 32a is provided between the two probes in this manner. Accordingly, even in a case where  
10 the two-dimensional array device 4b is used, light can be effectively applied to the photoacoustic transducer 4b which detects the photoacoustic wave. In addition, the two array devices 4a and 4b naturally need to be spaced apart from each other, and hence the crosstalk described in the  
15 first embodiment can be prevented.

The space between the two array devices 4a and 4b is described. It is understood that, in order to realize uniform irradiation as described above, the thickness of an optical path needs to be a half or more of the width of the  
20 photoacoustic transducer 4b for each side irrespective of an irradiation angle of laser. Therefore, an interspace having a size equal to at least a half of the width of the photoacoustic transducer 4b needs to be provided between the ultrasonic transducer 4a and the photoacoustic  
25 transducer 4b. In other words, the two array devices 4a and 4b may be separated from each other in the second direction by a distance corresponding to 50% or more of the

length of the second array device in the second direction.

A method of manufacturing the photoacoustic-ultrasonic system according to this embodiment is the same as that of the first embodiment, and hence the description thereof is omitted.

In the mode described above, the optical prisms are provided on both sides of the second probe. However, when optical prisms are provided so as to surround a probe, a more favorable irradiation amount distribution can be obtained.

*Example*

Hereinafter, in this example, a case where the probe according to the present invention is used for a mammary examination is specifically described. In the mammary examination, it is sufficient that an ultrasonic signal and a photoacoustic signal for up to a depth of 4 cm are acquired. The probe used in this case is the probe of FIGS. 1A and 1B which is used in the description above.

A laser light intensity allowable to be applied to a human body is  $100 \text{ mJ/cm}^2$ , and hence a range in which a sufficient photoacoustic signal can be acquired is 4 cm in depth and 4 cm in width. Accordingly, one side of a photoacoustic probe was set to 4 cm. Accordingly, one side of the photoacoustic probe was set to 4 cm. The device pitch was set to 2 mm in consideration of probe sensitivity and a frequency of 1 MHz to be used, whereby a two-dimensional array probe including 400 devices was formed.

An electrostatic capacity type ultrasonic transducer having a band width of 130% was used as the two-dimensional array probe because the two-dimensional array probe is required to detect targets having various sizes.

5           On the other hand, with regard to an ultrasonic probe, beam forming was performed with a 32-device aperture in order to sufficiently converge beams. Therefore, the ultrasonic probe is longer than the photoacoustic probe by 16 devices on each of the left and right sides. The total  
10           number of devices was set to 192, the device pitch was set to 0.25 mm, the center frequency was set to 10 MHz, and the array length was set to 48 mm. Further, an acoustic lens which is formed on a surface of the ultrasonic probe had a radius of R8. The beam formed under the above-mentioned  
15           conditions spreads to 7 mm in the vicinities of the ultrasonic probe and the vicinities of a depth of 4 cm, and hence an interspace between the ultrasonic probe and the photoacoustic probe was set to 1 mm.

          Considering that the mamma is scanned using the  
20           above-mentioned probes, five strips each having a size of 4 cm × 20 cm were formed because the scanning region is 20 cm × 20 cm and the stripe width is 4 cm. The scanning with the probes was performed in a step-and-repeat manner. Laser was applied while the probes were suspended, and the  
25           photoacoustic signal was acquired by the two-dimensional array probe. Then, while the probes were moving, the ultrasonic signal was acquired by the one-dimensional array

probe, and an ultrasonic image of each slice surface was generated and stored as volume data after being subjected to an interpolation processing.

After the scanning of an entire target surface is finished, the image is reconstructed using the photoacoustic signal. A photoacoustic image generated by the reconstruction is accumulated as volume data and superimposed on the ultrasonic image. The resultant image is displayed on a screen. The photoacoustic signal and the ultrasonic signal can be superimposed on each other by the above-mentioned method, with the result that information containing a morphologic image and a functional image can be provided to a user.

In this example, the 32-device aperture for an ultrasonic beam was adopted. When the size of the aperture is changed according to required beam resolution or a required beam forming method, the same effect can also be obtained.

The photoacoustic-ultrasonic system illustrated in FIGS. 7A and 7B can also be used for the mammary examination. In this case, the interspace between the ultrasonic probe and the photoacoustic probe needs to be at least 1.4 mm. On the other hand, in consideration of an incidence angle of 45 degrees and 2 cm which is one half the length of one side of the photoacoustic probe of 4 cm, the necessary thickness of a prism is 2.83 cm, and hence the space between the probes was set to 2.83 cm.

The present invention is not limited to the above embodiments and various changes and modifications can be made within the spirit and scope of the present invention. Therefore to apprise the public of the scope of the present invention, the following claims are made.

This application claims the benefit of Japanese Patent Applications No. 2008-159314, filed June 18, 2008, and No. 2009-136365, filed June 5, 2009, which are hereby incorporated by reference herein in their entirety.

## CLAIMS

1. An ultrasonic probe, comprising:

a first array device capable of transmitting and receiving an ultrasonic wave; and

5 a second array device capable of receiving a photoacoustic wave,

wherein the first array device includes a plurality of electromechanical transducers arranged in a first direction; the second array device includes a plurality of electromechanical transducers arranged in a two-dimensional  
10 manner; and

the first array device and the second array device are provided on the same plane and in a second direction perpendicular to the first direction.

15 2. An ultrasonic probe according to Claim 1, wherein the length of the first array device in the first direction is longer than the length of the second array device in the first direction.

20 3. An ultrasonic probe according to Claim 1 or 2, wherein the first array device and the second array device are separated from each other in the second direction by a distance corresponding to 20% or more of the length of the first array device in the second direction.

25 4. An ultrasonic probe according to Claim 1 or 2, wherein the first array device and the second array device are separated from each other in the second direction by a distance corresponding to 50% of the length of the second

array device in the second direction.

5. An ultrasonic probe according to any one of Claims 1 to 4, wherein the second direction corresponds to a scanning direction in which the first array device and  
5 the second array device are scanned.

6. An ultrasonic probe according to any one of Claims 1 to 5, wherein the second array device comprises an electrostatic capacity type ultrasonic transducer.

7. A photoacoustic-ultrasonic system, comprising:  
10 an optical system for introducing light emitted from a light source into an inspection object; and  
the ultrasonic probe according to any one of Claims 1 to 6,  
wherein the optical system is provided in an  
15 interspace between the first array device and the second array device.

8. A photoacoustic-ultrasonic system according to Claim 7, wherein the optical system is provided so that light guided between a first probe including the first  
20 array device and a second probe including the second array device in a direction perpendicular to the plane is emitted from the interspace between the first array device and the second array device toward below the second array device.

9. A photoacoustic-ultrasonic system according to  
25 Claim 8, wherein the optical system is provided so that light is guided from both sides of the second probe.

10. An inspection object imaging apparatus,

comprising:

a light source for generating pulse light;

the ultrasonic probe according to any one of Claims 1  
to 6; and

5 a system control unit for controlling the light  
source and the ultrasonic probe to form an image,

wherein the system control unit forms an image based  
on morphologic information of the inside of an inspection  
object by using the first array device and forms an image  
10 based on functional information of the inside of the  
inspection object by using the light source and the second  
array device.

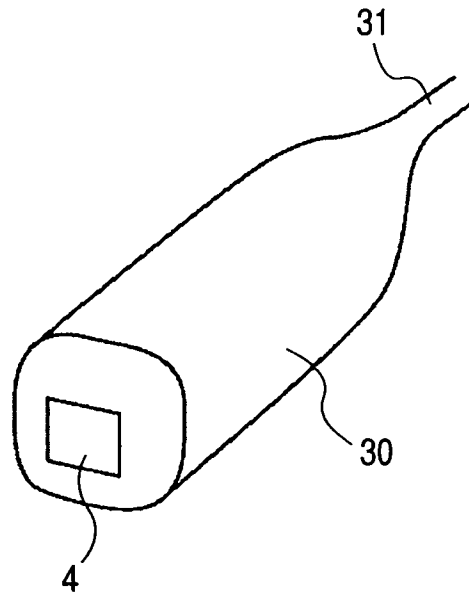
11. An inspection object imaging apparatus according  
to Claim 10, wherein the first array device transmits and  
15 receives an ultrasonic wave having a frequency higher than  
the frequency of an ultrasonic wave received by the second  
array device.

12. An inspection object imaging apparatus according  
to Claim 10,

20 wherein the first array device transmits and receives  
an ultrasonic wave having a frequency of 7 to 12 MHz; and

wherein the second array device receives an  
ultrasonic wave having a frequency of 1 to 4 MHz.

**FIG. 1A**



**FIG. 1B**

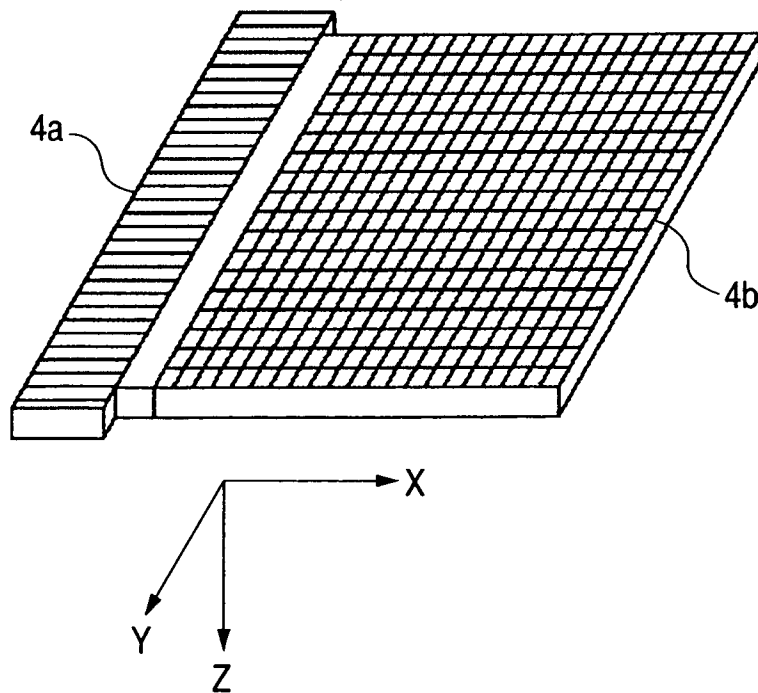


FIG. 2

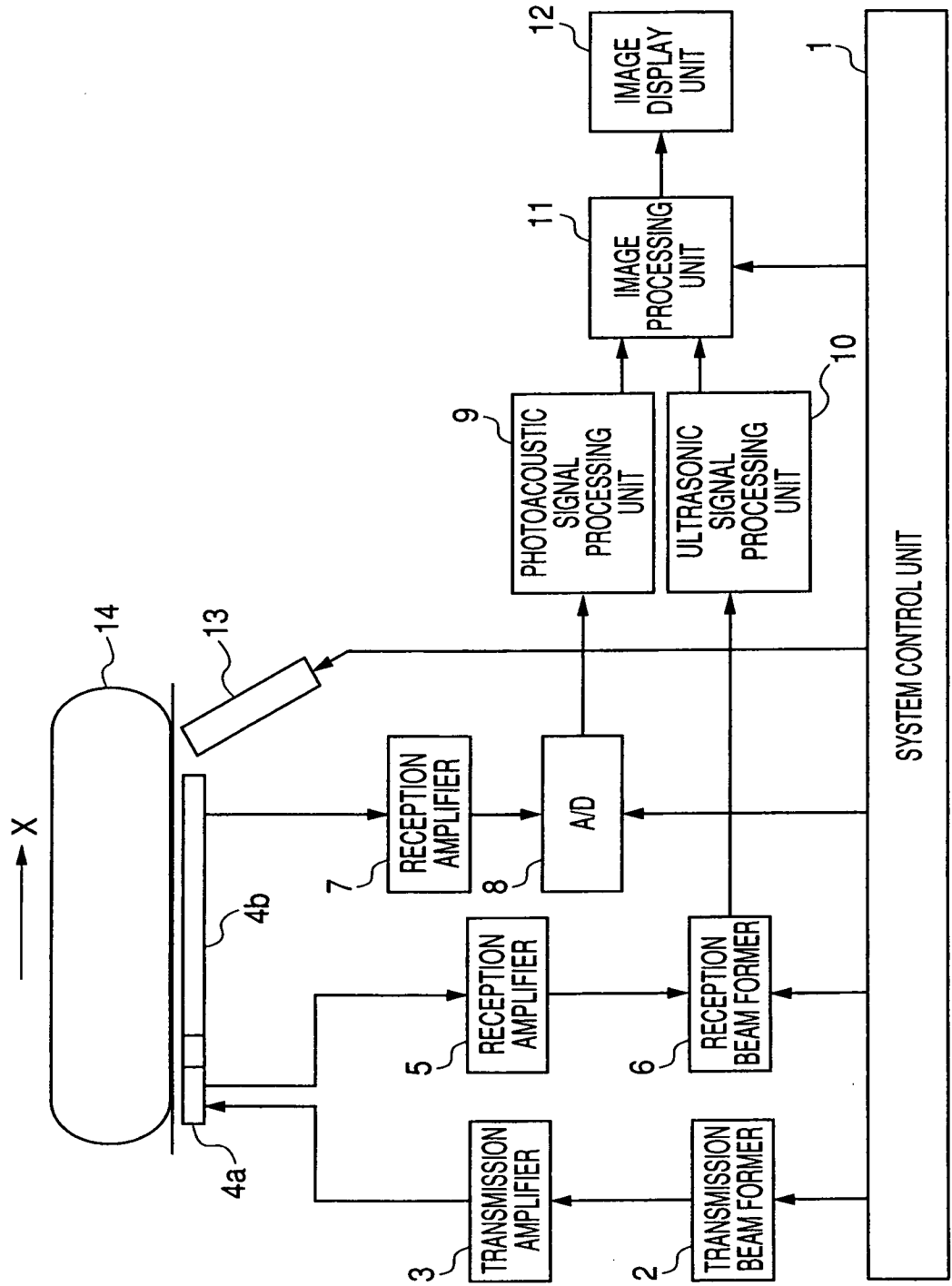


FIG. 3

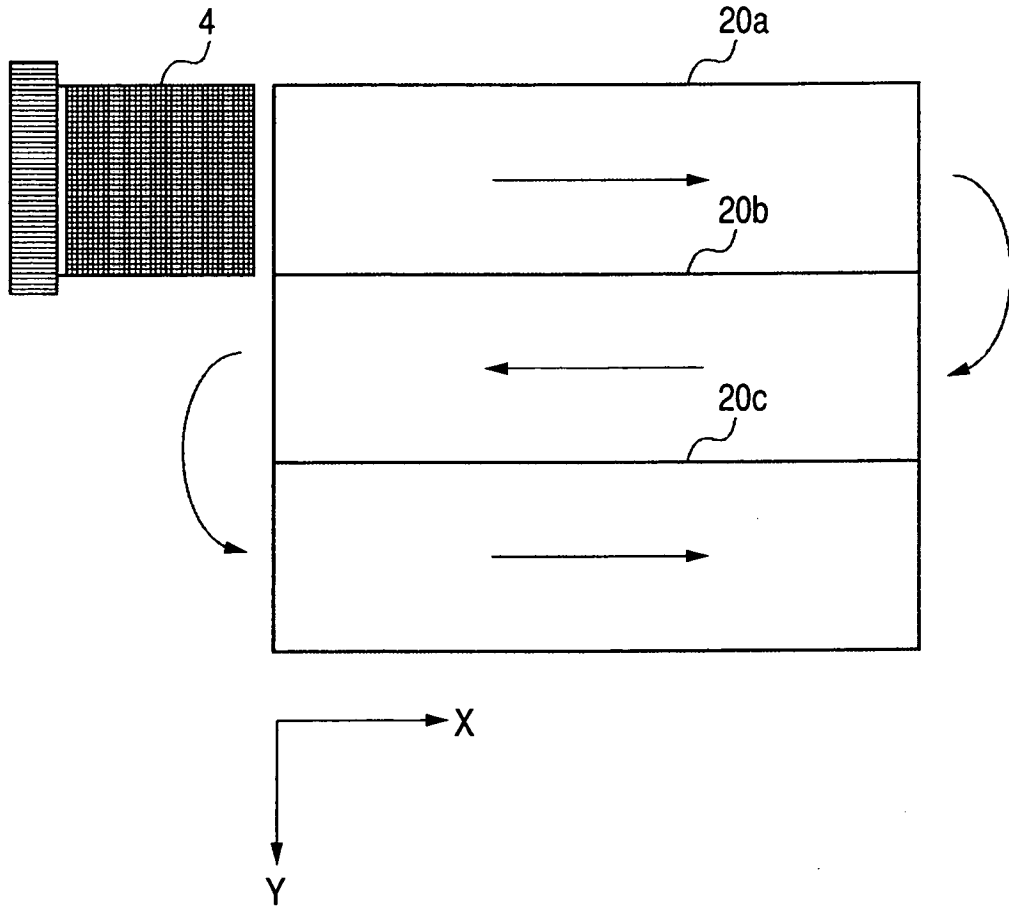


FIG. 4

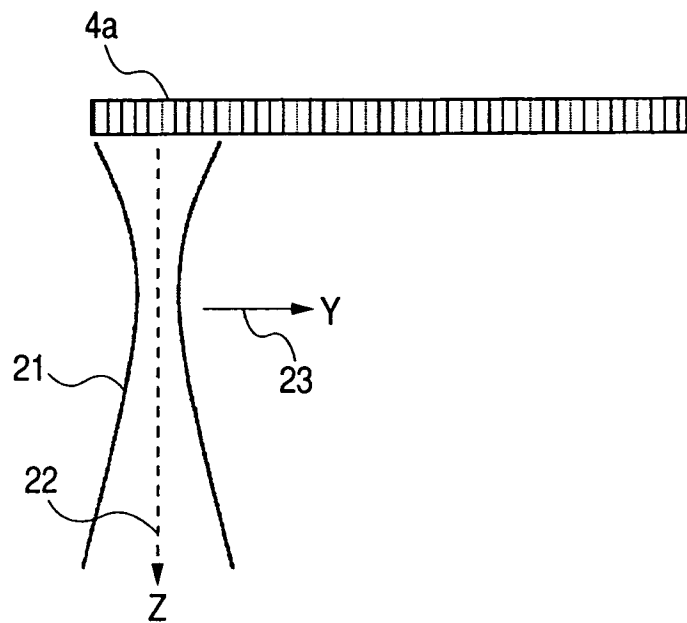


FIG. 5

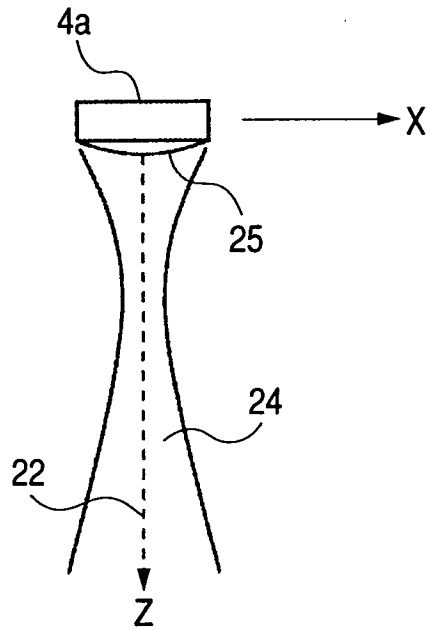
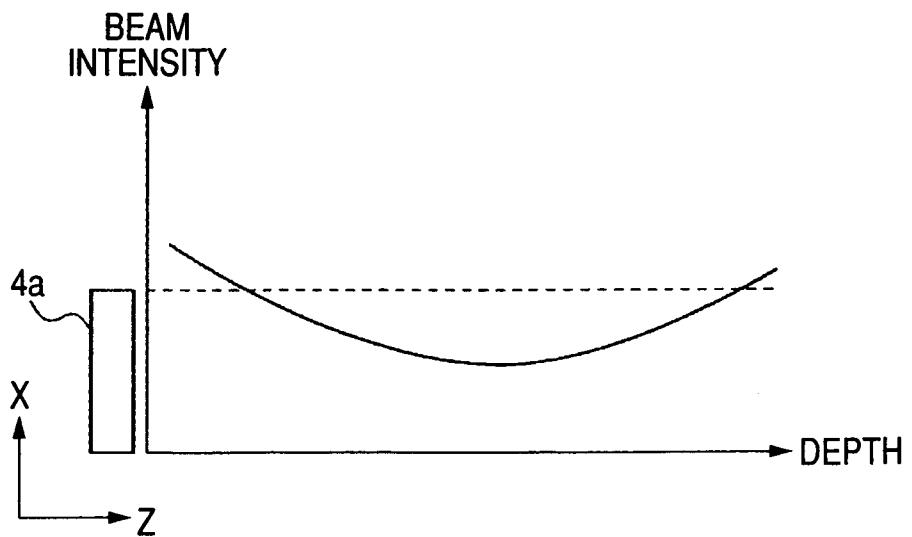
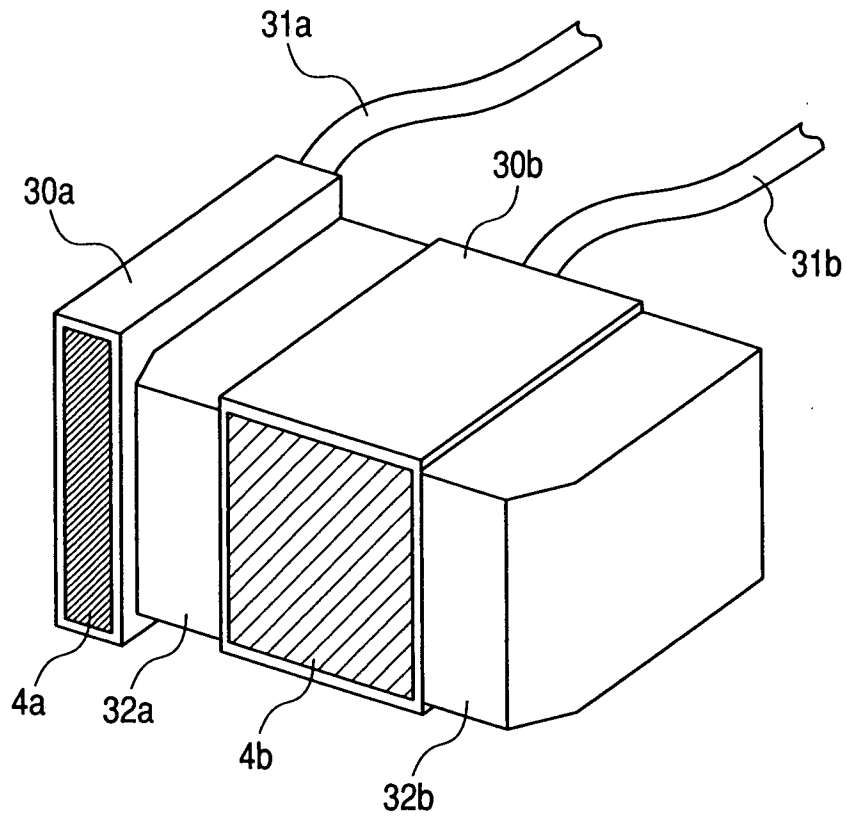


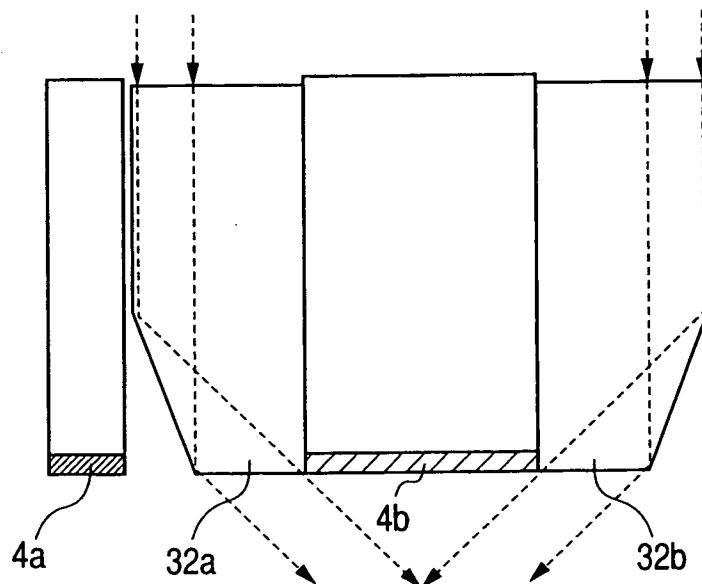
FIG. 6



**FIG. 7A**



**FIG. 7B**



**INTERNATIONAL SEARCH REPORT**

International application No  
PCT/JP2009/061434

**A. CLASSIFICATION OF SUBJECT MATTER**  
INV. A61B5/00 A61B8/14

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**  
Minimum documentation searched (classification system followed by classification symbols)  
A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)  
EPO-Internal, WPI Data

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 831 601 A (BREIMESSER FRITZ [DE] ET AL) 16 May 1989 (1989-05-16)	1-6
Y	column 2, lines 10-48 column 3, lines 21-59 figure 1	7-12
Y	WO 2007/148239 A (KONINKL PHILIPS ELECTRONICS NV [NL]; BURCHER MICHAEL [US]) 27 December 2007 (2007-12-27) page 2, line 21 - page 3, line 5 page 4, lines 9-22 page 10, lines 12-17 claim 23	7-12

Further documents are listed in the continuation of Box C.  See patent family annex.

- \* Special categories of cited documents :
- \*A\* document defining the general state of the art which is not considered to be of particular relevance
  - \*E\* earlier document but published on or after the international filing date
  - \*L\* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
  - \*O\* document referring to an oral disclosure, use, exhibition or other means
  - \*P\* document published prior to the international filing date but later than the priority date claimed
  - \*T\* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
  - \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
  - \*Y\* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
  - \*8\* document member of the same patent family

Date of the actual completion of the international search <b>20 October 2009</b>	Date of mailing of the international search report <b>06/11/2009</b>
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Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040. Fax: (+31-70) 340-3016	Authorized officer <b>Völlinger, Martin</b>
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## INTERNATIONAL SEARCH REPORT

International application No

PCT/JP2009/061434

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	<p>US 2005/004458 A1 (KANAYAMA SHOICHI [JP] ET AL) 6 January 2005 (2005-01-06)  cited in the application  paragraph [0003]  paragraph [0058]  paragraph [0073]  paragraphs [0122], [0123]  paragraphs [0135] - [0137]  figures 1,3A</p>	1,7,10
A	<p>US 2005/187471 A1 (KANAYAMA SHOICHI [JP] ET AL) 25 August 2005 (2005-08-25)  paragraph [0027]  paragraph [0050]  paragraphs [0061], [0062]  paragraphs [0073], [0074]  figures 1,3,4A,5</p>	1,7,10
A	<p>FRENZ M ET AL: "Combined Ultrasound and Optoacoustic System for Real-Time High-Contrast Vascular Imaging in Vivo" IEEE TRANSACTIONS ON MEDICAL IMAGING, IEEE SERVICE CENTER, PISCATAWAY, NJ, US, vol. 24, no. 4, 1 April 2005 (2005-04-01), pages 436-440, XP011129441  ISSN: 0278-0062  page 437, left-hand column, last paragraph - right-hand column, paragraph 3  figure 1</p>	1,7,10
A	<p>KOZHUSHKO VICTOR ET AL: "Focused array transducer for two-dimensional optoacoustic tomography" JOURNAL OF THE ACOUSTICAL SOCIETY OF AMERICA, AIP / ACOUSTICAL SOCIETY OF AMERICA, MELVILLE, NY, US, vol. 116, no. 3, 1 September 2004 (2004-09-01), pages 1498-1506, XP012072498  ISSN: 0001-4966  page 1498, left-hand column, paragraph 3 - right-hand column, paragraph 2  page 1502, left-hand column  figures 1,5</p>	1,7,10

## INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/JP2009/061434

Patent document cited in search report.		Publication date	Patent family member(s)	Publication date
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WO 2007148239	A	27-12-2007	CN 101472520 A EP 2034878 A2 US 2009187099 A1	01-07-2009 18-03-2009 23-07-2009
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专利名称(译)	超声波探头，光声 - 超声波系统和包括超声波探头的检查对象成像设备		
公开(公告)号	<a href="#">EP2303103A1</a>	公开(公告)日	2011-04-06
申请号	EP2009766746	申请日	2009-06-17
[标]申请(专利权)人(译)	佳能株式会社		
申请(专利权)人(译)	佳能株式会社		
当前申请(专利权)人(译)	佳能株式会社		
[标]发明人	SOMEDA YASUHIRO SAITO KEISHI ASAO YASUFUMI NAKAGAWA KATSUMI ICHIHARA SHIGERU		
发明人	SOMEDA, YASUHIRO SAITO, KEISHI ASAO, YASUFUMI NAKAGAWA, KATSUMI ICHIHARA, SHIGERU		
IPC分类号	A61B5/00 A61B8/14		
CPC分类号	A61B5/0035 A61B5/0095 A61B8/0825 A61B8/14 A61B8/483 A61B8/5238 A61B8/145 A61B8/4416 A61B8/4444 A61B8/4494		
代理机构(译)	TBK专利		
优先权	2008159314 2008-06-18 JP 2009136365 2009-06-05 JP		
外部链接	<a href="#">Espacenet</a>		

#### 摘要(译)

本发明提供一种即使在超声波中使用的光声波的频带和超声波的频带彼此分离时也能够在不劣化的情况下形成图像的超声波探头，以及包括该超声波探头的检查对象成像装置。超声波探头包括能够发送和接收超声波的第一阵列装置;以及能够接收光声波的阵列装置。第一阵列装置包括沿垂直于扫描方向的方向排列的多个机电变换器，第二阵列装置包括以二维方式排列的多个机电变换器，第一阵列装置和第二阵列装置设置在同一平面上并在扫描方向。