



US 20180296101A1

(19) **United States**

(12) **Patent Application Publication**
KUBO

(10) **Pub. No.: US 2018/0296101 A1**

(43) **Pub. Date: Oct. 18, 2018**

(54) **ELECTRONIC BLOOD PRESSURE MONITOR**

Publication Classification

(71) Applicant: **OMRON HEALTHCARE CO., LTD.**,
Muko-shi (JP)

(51) **Int. Cl.**
A61B 5/0225 (2006.01)
A61B 5/00 (2006.01)

(72) Inventor: **Takeshi KUBO**, Kyoto (JP)

(52) **U.S. Cl.**
CPC *A61B 5/0225* (2013.01); *A61B 2560/0475*
(2013.01); *A61B 5/4806* (2013.01); *A61B*
5/7221 (2013.01)

(21) Appl. No.: **16/015,257**

(57) **ABSTRACT**

(22) Filed: **Jun. 22, 2018**

An electronic blood pressure monitor of the present invention includes a blood pressure measurement cuff that is to be worn on a measurement site of a measurement subject. The electronic blood pressure monitor includes a blood pressure measurement unit that measures a blood pressure value of the measurement subject using the cuff. The electronic blood pressure monitor includes an external compression detection unit that detects whether or not there was external compression on the cuff during blood pressure measurement performed by the blood pressure measurement unit.

Related U.S. Application Data

(63) Continuation of application No. PCT/JP2016/079314, filed on Oct. 3, 2016.

Foreign Application Priority Data

(30) Dec. 28, 2015 (JP) 2015-257066

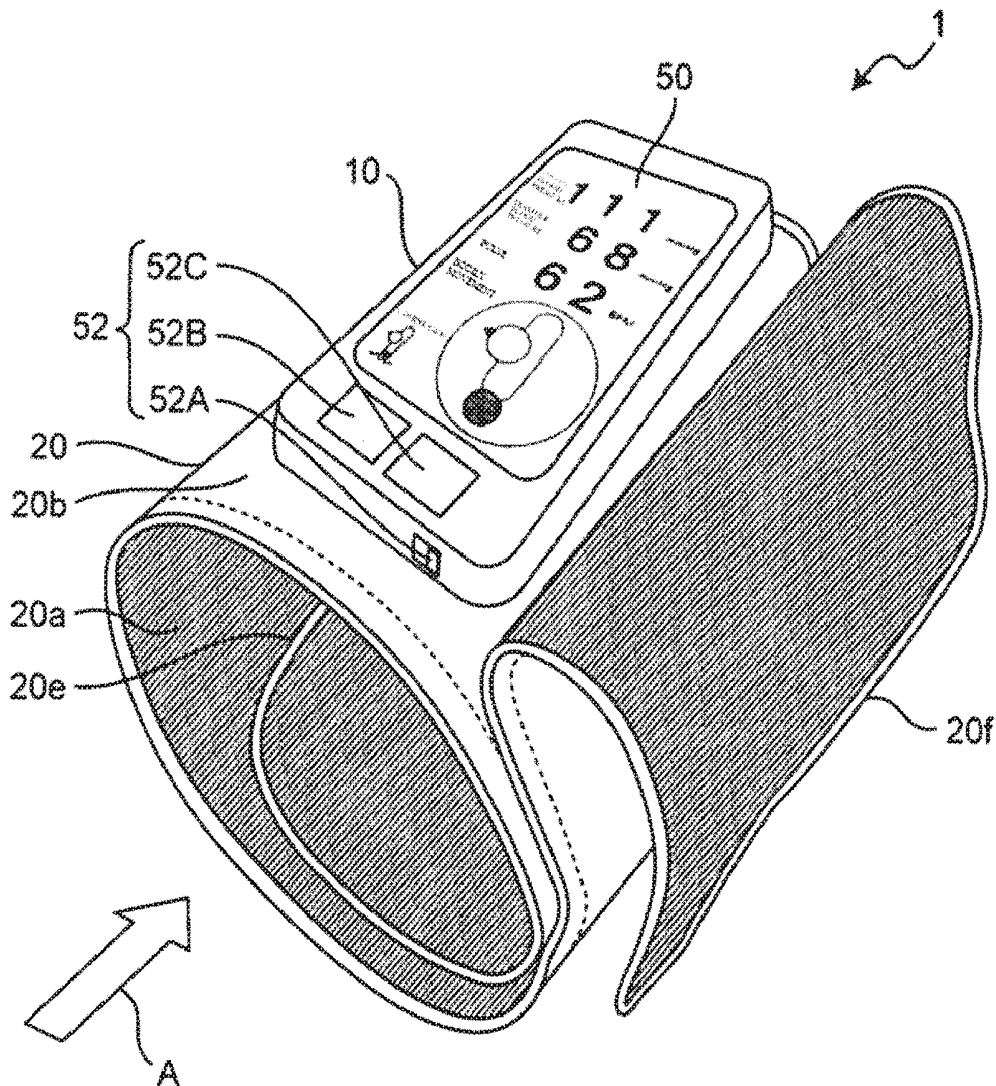


FIG. 1

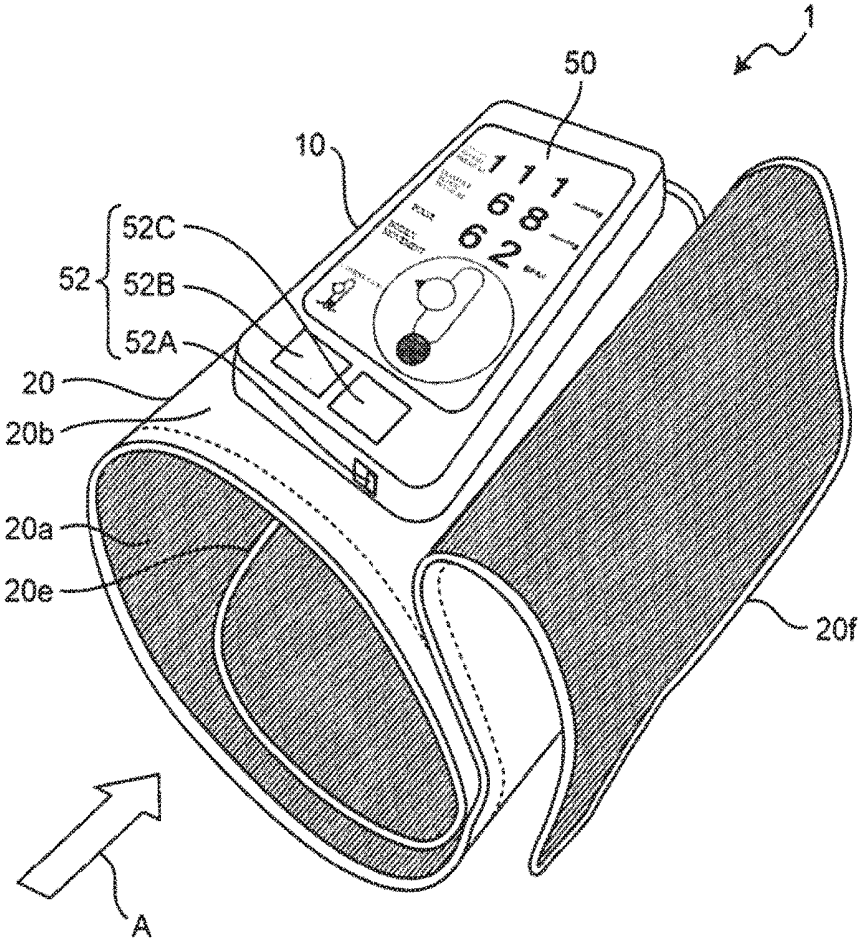


FIG. 2

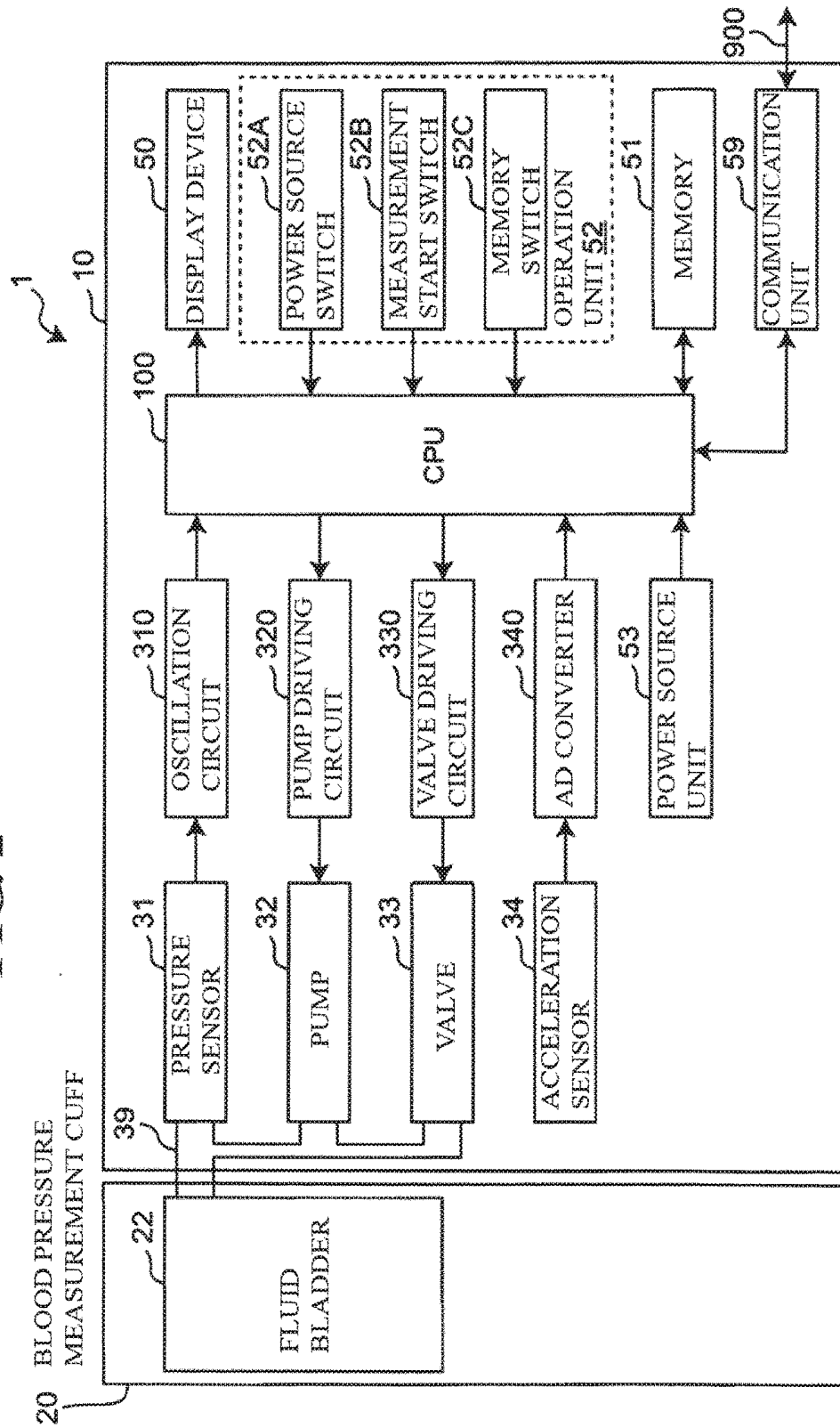


FIG. 3

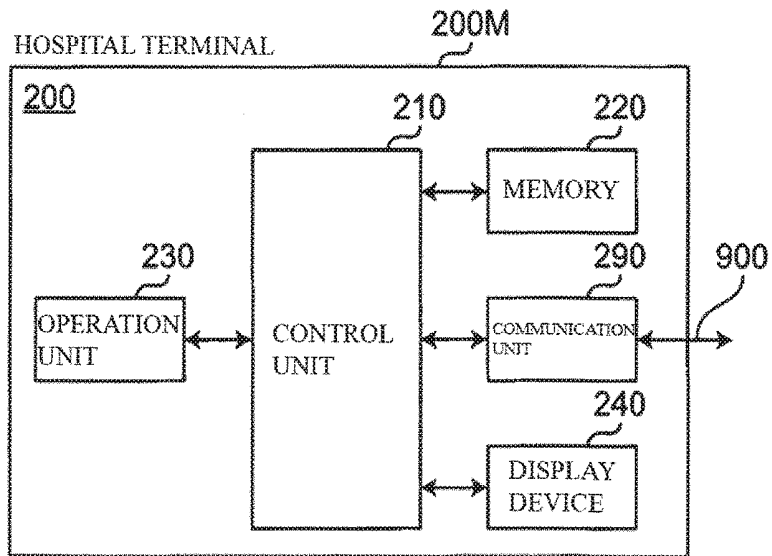


FIG. 4A

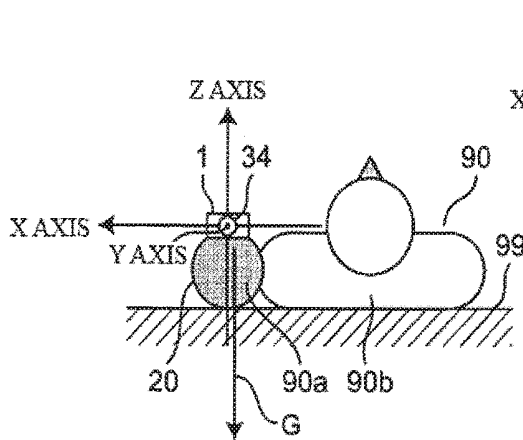


FIG. 4B

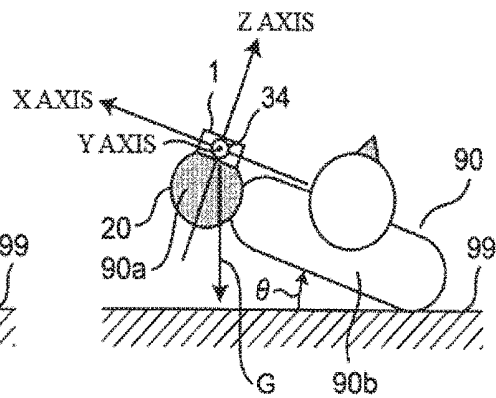


FIG. 5

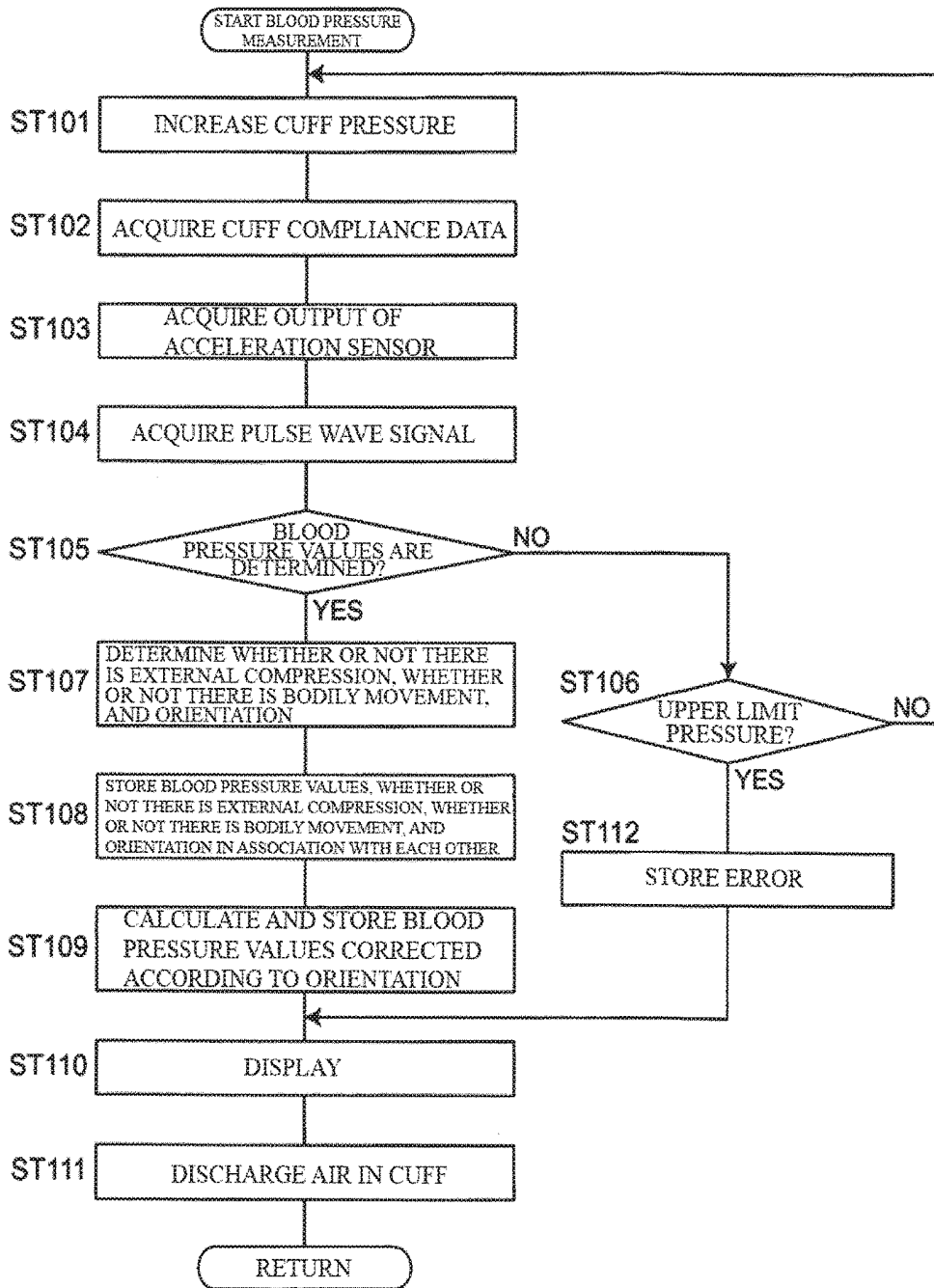


FIG. 6A

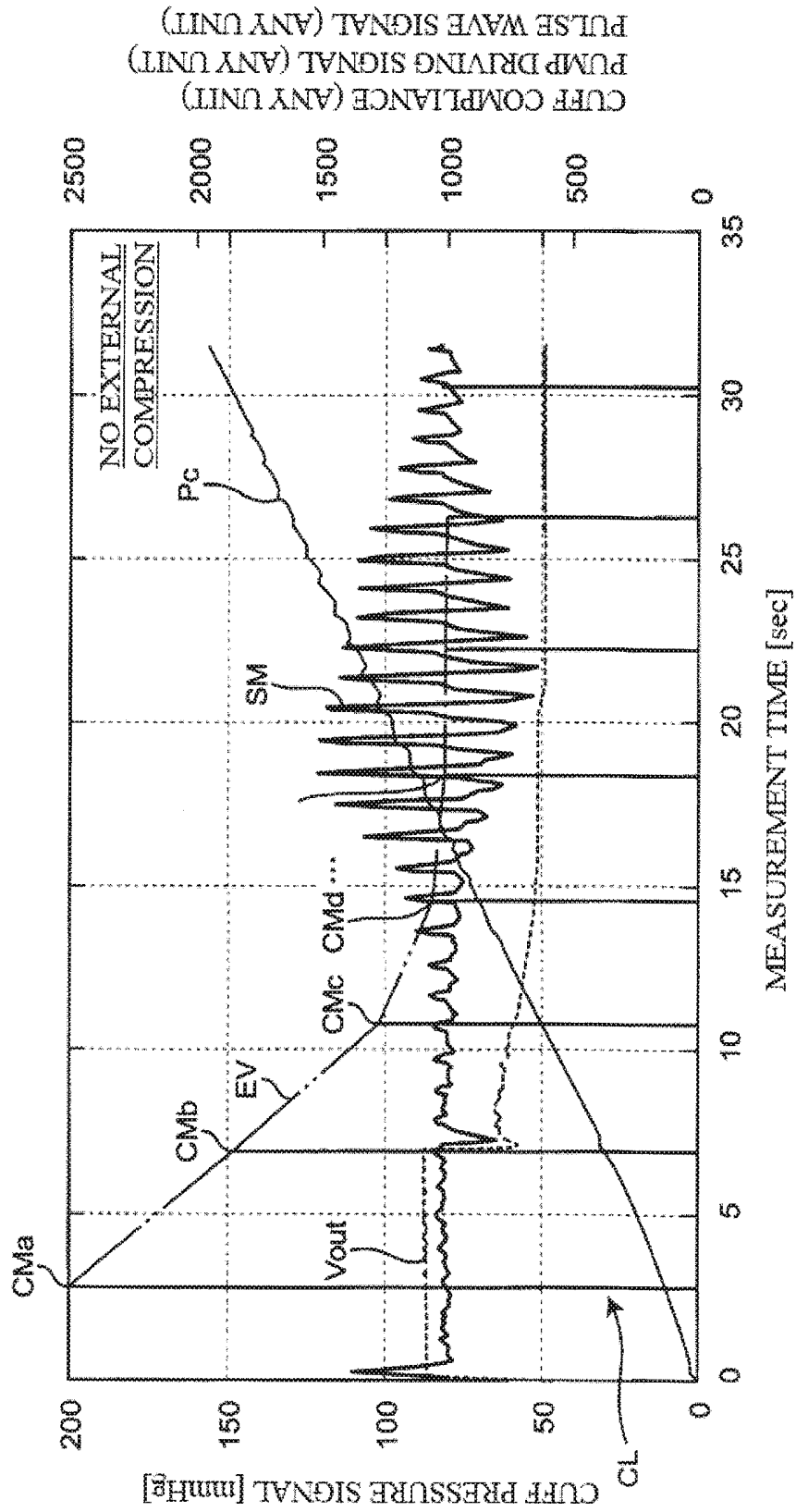


FIG. 6B

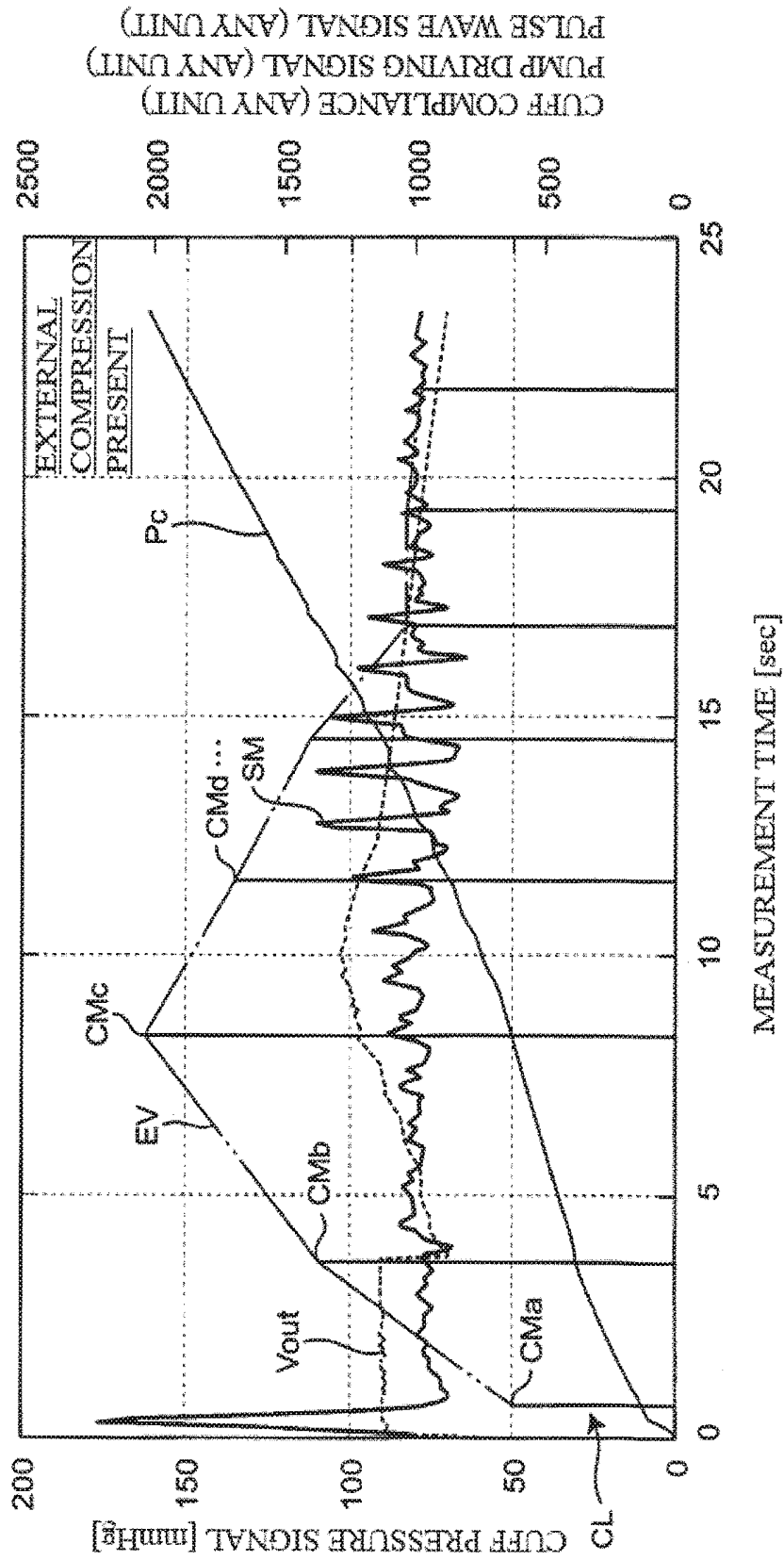


FIG 7

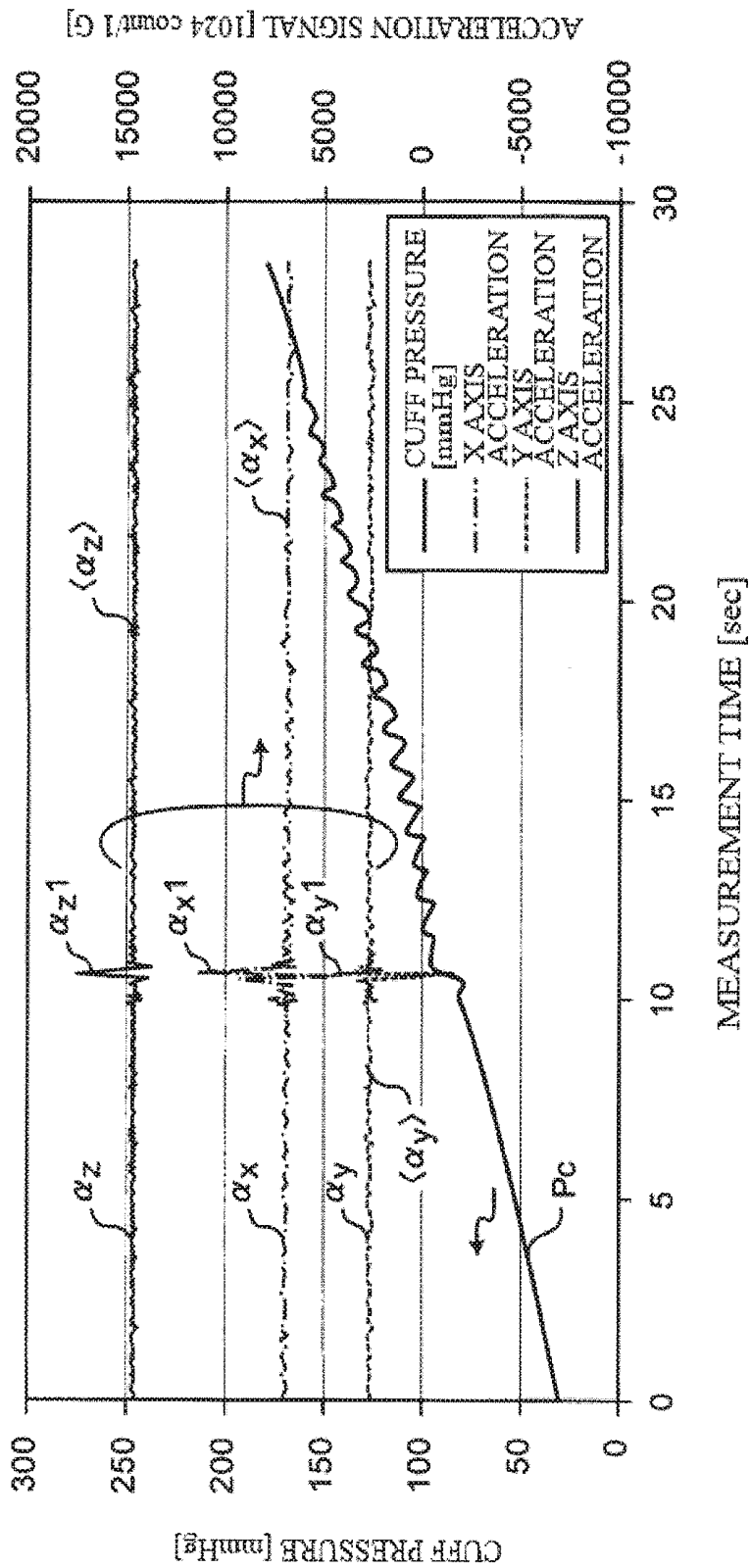


FIG. 8A

		SUPINE POSITION (0 DEGREES)			
TORSO ANGLE	A-1				
	ARM POSITION				
		BODY-LATERAL	BODY-SIDE SEPARATED	ON-CHEST	HURRAH
XZ COORDINATES					
XY COORDINATES					

FIG. 8B

BETWEEN SUPINE POSITION AND RIGHT SIDE POSITION (20 DEGREES)	
	<div style="display: flex; justify-content: space-around;"> <div style="text-align: center;"> <p>B-1</p> </div> <div style="text-align: center;"> <p>B-2</p> </div> <div style="text-align: center;"> <p>B-3</p> </div> <div style="text-align: center;"> <p>B-4</p> </div> </div>
TORSO ANGLE	
	<div style="display: flex; justify-content: space-around;"> <div style="text-align: center;"> <p>B-1</p> </div> <div style="text-align: center;"> <p>B-2</p> </div> <div style="text-align: center;"> <p>B-3</p> </div> <div style="text-align: center;"> <p>B-4</p> </div> </div>
ARM POSITION	
	<div style="display: flex; justify-content: space-around;"> <div style="text-align: center;"> <p>BACK-SIDE</p> </div> <div style="text-align: center;"> <p>BODY-LATERAL</p> </div> <div style="text-align: center;"> <p>CHEST-SIDE</p> </div> <div style="text-align: center;"> <p>HURRAH</p> </div> </div>
XZ COORDINATES	
	<div style="display: flex; justify-content: space-around;"> <div style="text-align: center;"> <p>BACK-SIDE</p> </div> <div style="text-align: center;"> <p>BODY-LATERAL</p> </div> <div style="text-align: center;"> <p>CHEST-SIDE</p> </div> <div style="text-align: center;"> <p>HURRAH</p> </div> </div>
XY COORDINATES	

FIG. 8C

		RIGHT SIDE POSITION (90 DEGREES)			
		C-1	C-2	C-3	C-4
TORSO ANGLE					
ARM POSITION					
		BACK-SIDE	BODY-LATERAL	CHEST-SIDE	HURRAH
XZ COORDINATES					
XY COORDINATES					

FIG. 8D

BETWEEN RIGHT SIDE POSITION AND PRONE POSITION (160 DEGREES)				
TORSO ANGLE	<p>D-1</p>	<p>D-2</p>	<p>D-3</p>	<p>D-4</p>
ARM POSITION				
XZ COORDINATES	<p>BACK-SIDE</p>	<p>BODY-LATERAL</p>	<p>CHEST-SIDE</p>	<p>HURRAH</p>
XY COORDINATES				

FIG. 8E

		PRONE POSITION (180 DEGREES)				
TORSO ANGLE	E-1	<p>90b 90a 20 90 90h</p>	E-2	<p>90a 20 90h 10</p>	E-3	<p>90b 10 90h 20 90a</p>
	ARM POSITION	<p>90a 90b 90h</p>	<p>90a 90b 90h</p>	<p>90a 90b 90h</p>		
		BODY-LATERAL	BODY-SIDE SEPARATED	HURRAH		
XZ COORDINATES		<p>z 1 -1 0 x axz</p>	<p>z 1 -1 0 x axz</p>	<p>z 1 -1 0 x axz</p>		
XY COORDINATES		<p>y 1 -1 0 x axy</p>	<p>y 1 -1 0 x axy</p>	<p>y 1 -1 0 x axy</p>		

FIG. 8F

BETWEEN PRONE POSITION AND LEFT SIDE POSITION (200 DEGREES)							
TORSO ANGLE	<table border="1"> <tr> <td>F-1</td> <td>90a 20 90b 20 90h 10</td> <td>F-2</td> <td>90a 20 90b 20 90h 10</td> <td>F-3</td> <td>90a 20 90b 20 90h 10</td> </tr> </table>	F-1	90a 20 90b 20 90h 10	F-2	90a 20 90b 20 90h 10	F-3	90a 20 90b 20 90h 10
F-1	90a 20 90b 20 90h 10	F-2	90a 20 90b 20 90h 10	F-3	90a 20 90b 20 90h 10		
ARM POSITION	<table border="1"> <tr> <td>90</td> <td>90a 90b 90h</td> <td>90a</td> <td>90b 90h</td> <td>90a</td> <td>90b 90h</td> </tr> </table>	90	90a 90b 90h	90a	90b 90h	90a	90b 90h
90	90a 90b 90h	90a	90b 90h	90a	90b 90h		
	BODY-LATERAL	BODY-SIDE SEPARATED	HURRAH				
XZ COORDINATES							
XY COORDINATES							

FIG. 8G

LEFT SIDE POSITION (270 DEGREES)			
TORSO ANGLE	<p>G-1 90h 90b 90a 10 20 90</p>	<p>G-2 90h 90b 90a 10 20 90</p>	<p>G-3 90h 90b 90a 10 20 90</p>
ARM POSITION	<p>90a 90b 90h</p>	<p>90a 90b 90h</p>	<p>90a 90b 90h</p>
	CHEST-FRONT SEPARATED	BODY-LATERAL	HURRAH
XZ COORDINATES	<p>z 1 0 1 x -1 -1</p>	<p>z 1 0 1 x -1 -1</p>	<p>z 1 0 1 x -1 -1</p>
XY COORDINATES	<p>y 1 0 1 x -1 -1</p>	<p>y 1 0 1 x -1 -1</p>	<p>y 1 0 1 x -1 -1</p>

FIG. 8H

BETWEEN LEFT SIDE POSITION AND SPINE POSITION (340 DEGREES)			
	H-1	90h	90
TORSO ANGLE	H-2	90h	90h
	H-3	90h	90h
ARM POSITION			
	CHEST-FRONT	BODY-LATERAL	HURRAH
XZ COORDINATES			
XY COORDINATES			

FIG. 9B

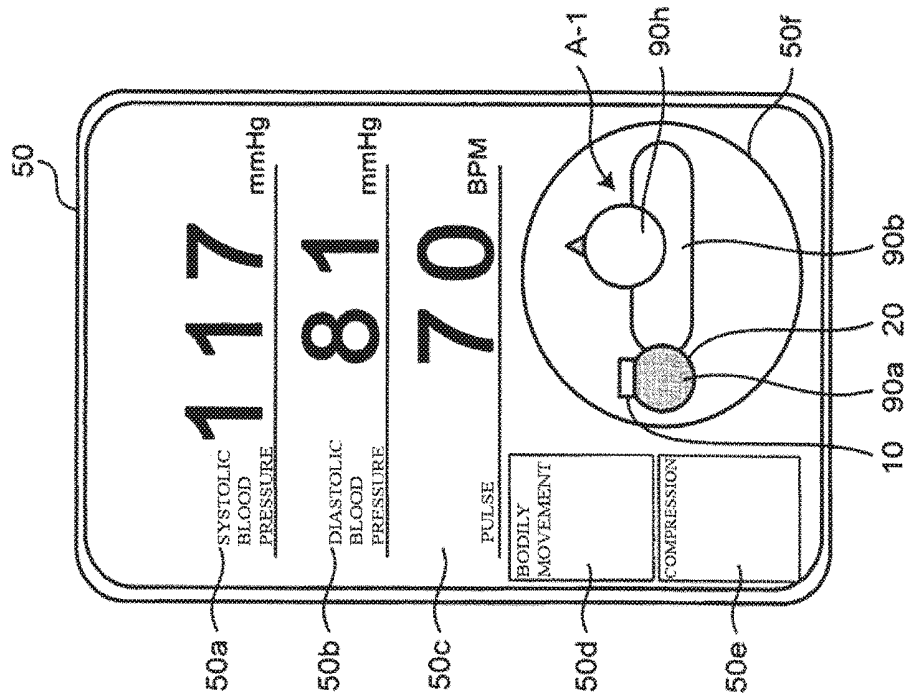


FIG. 9A

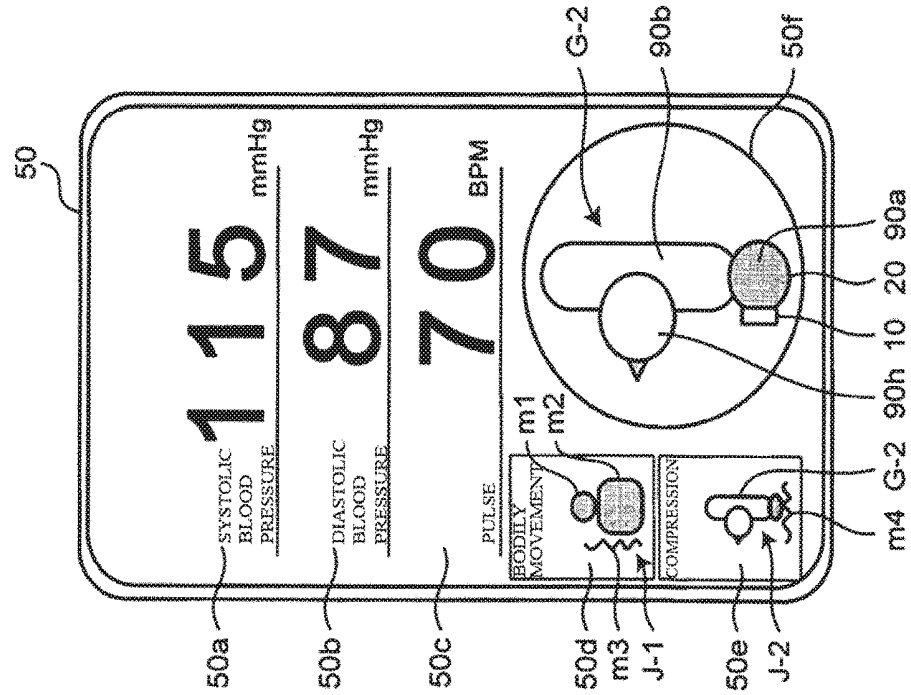


FIG. 10B

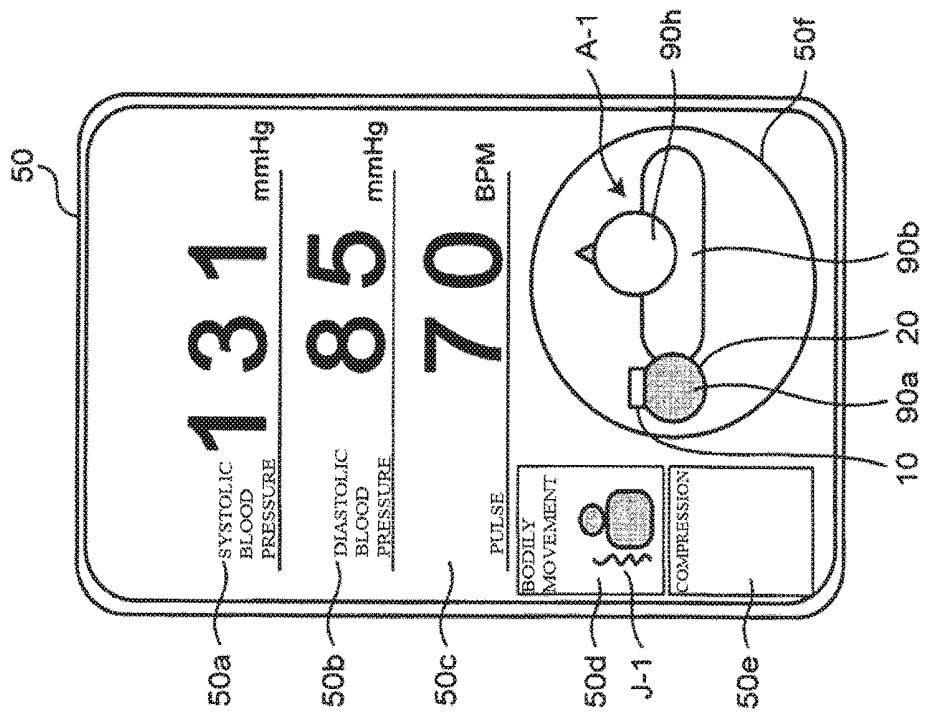


FIG. 10A

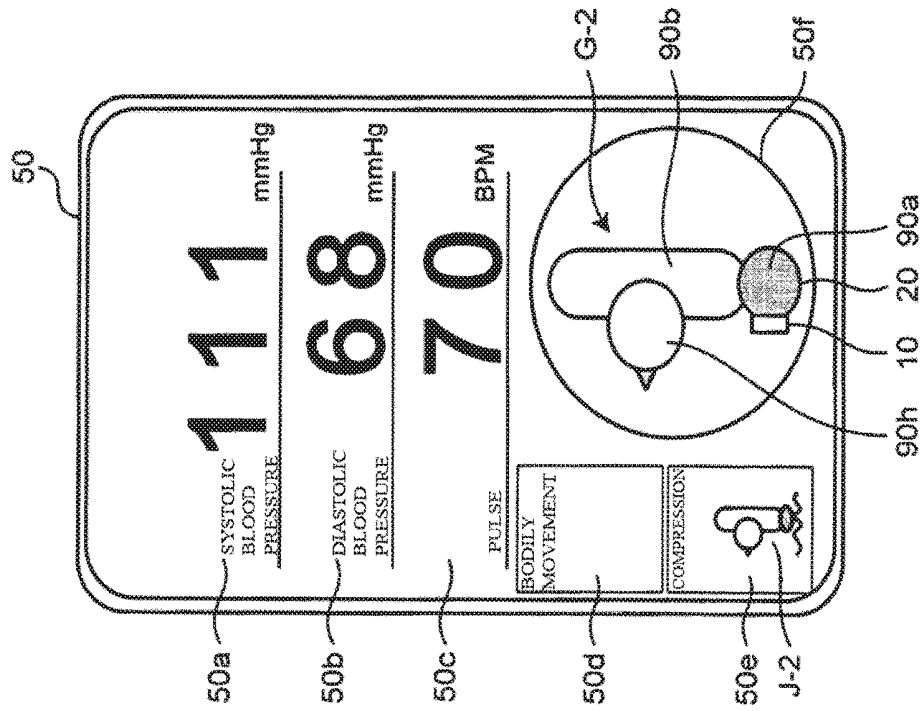


FIG. 11

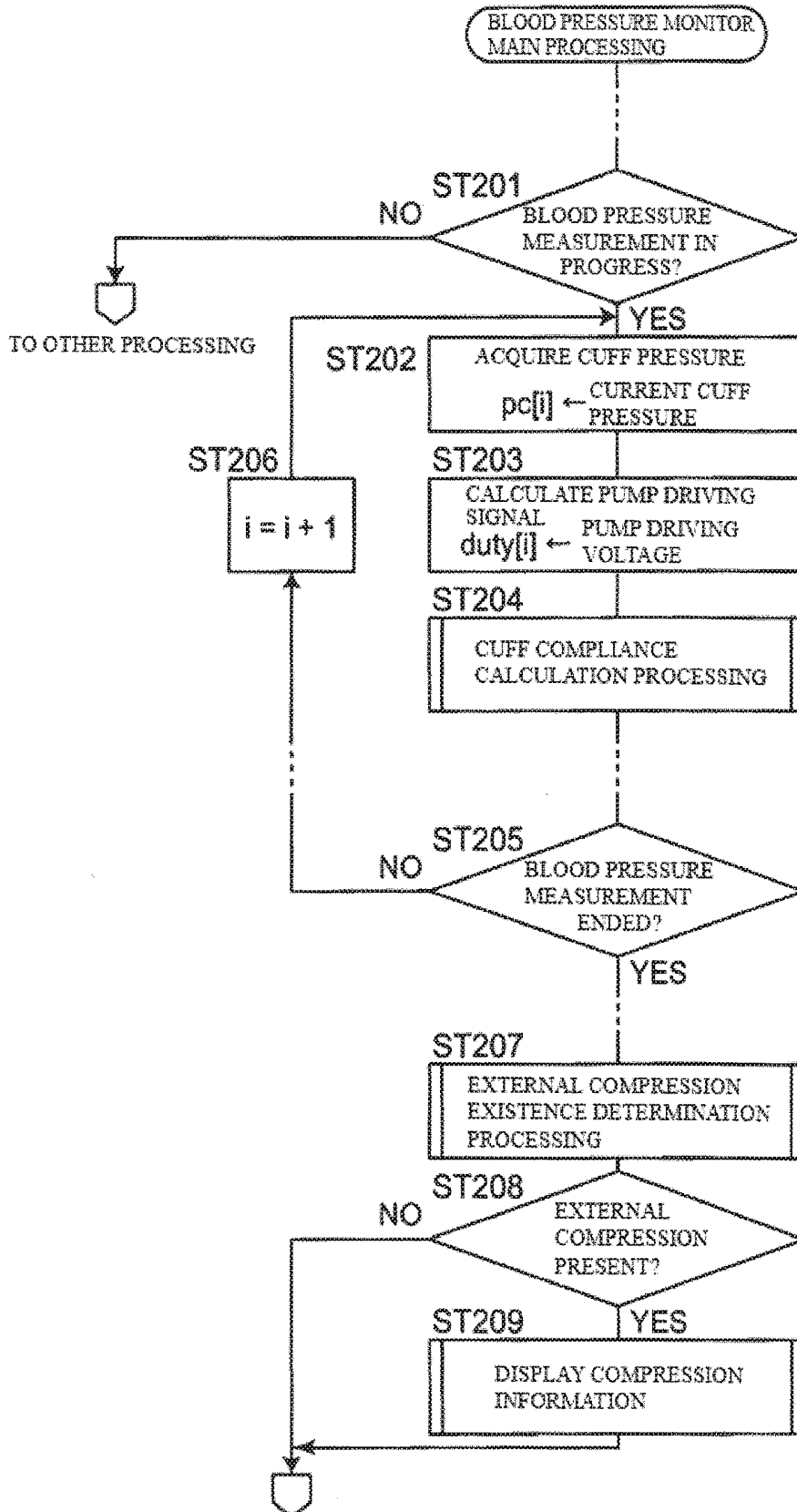


FIG. 12

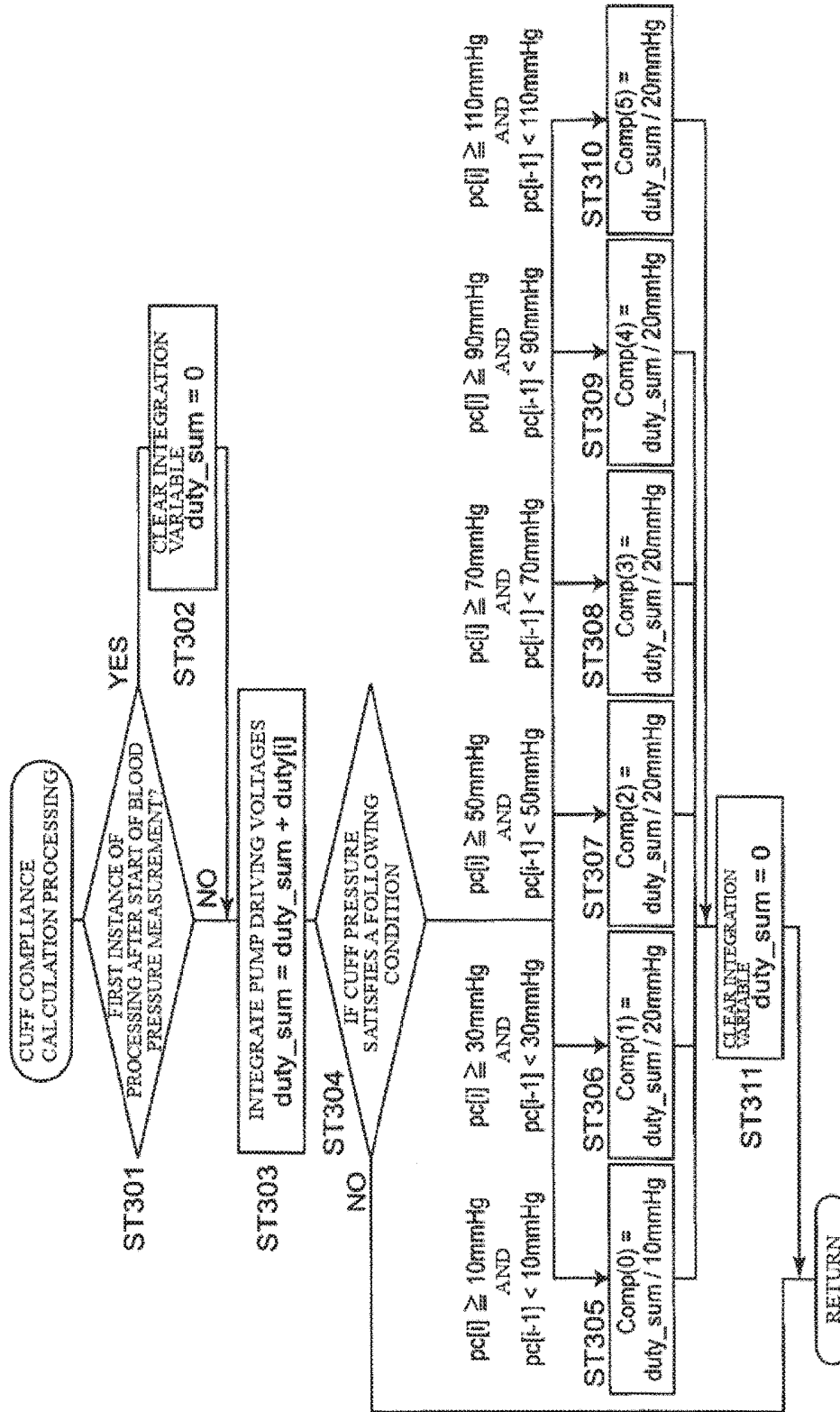


FIG. 13

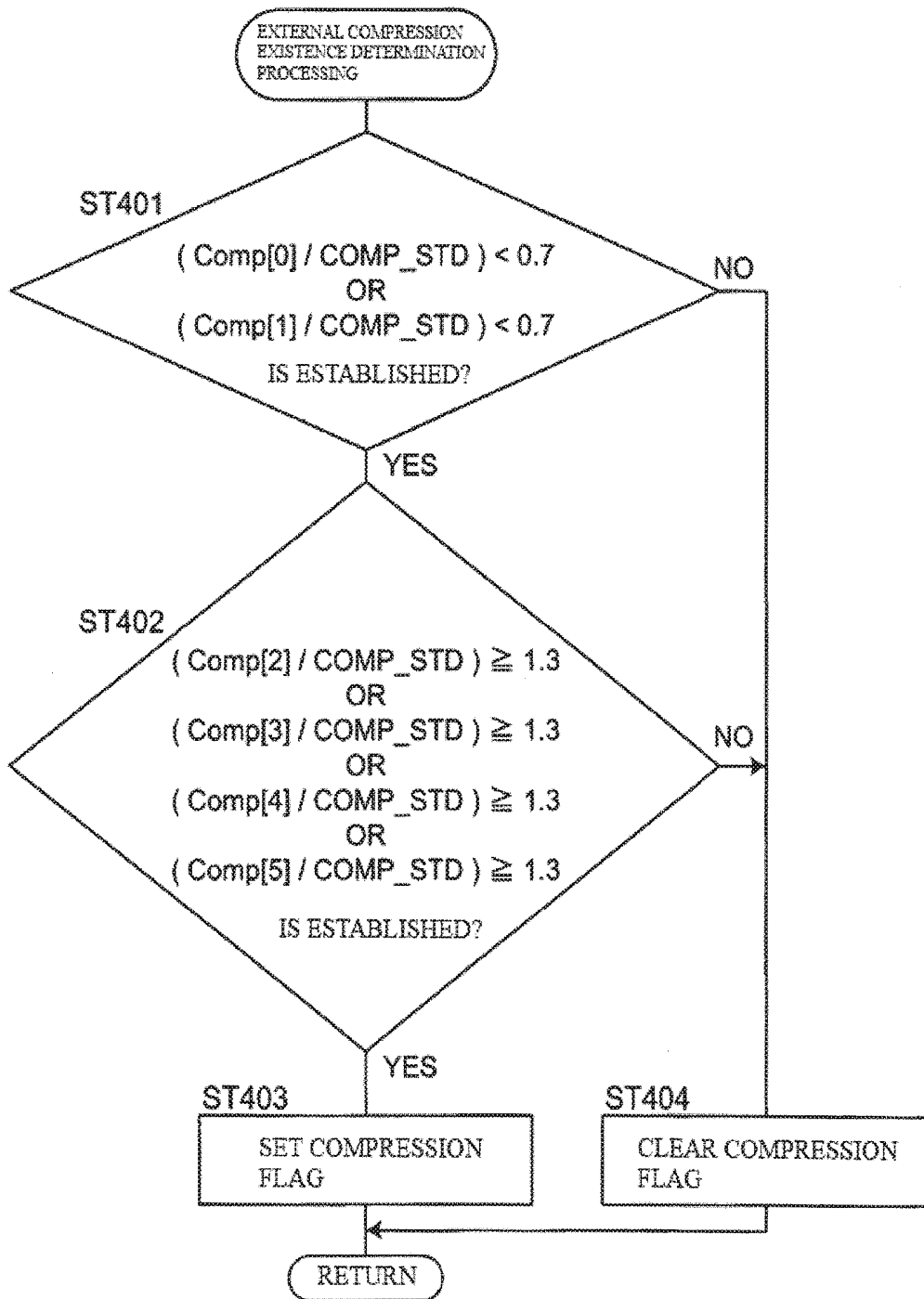


FIG. 14A

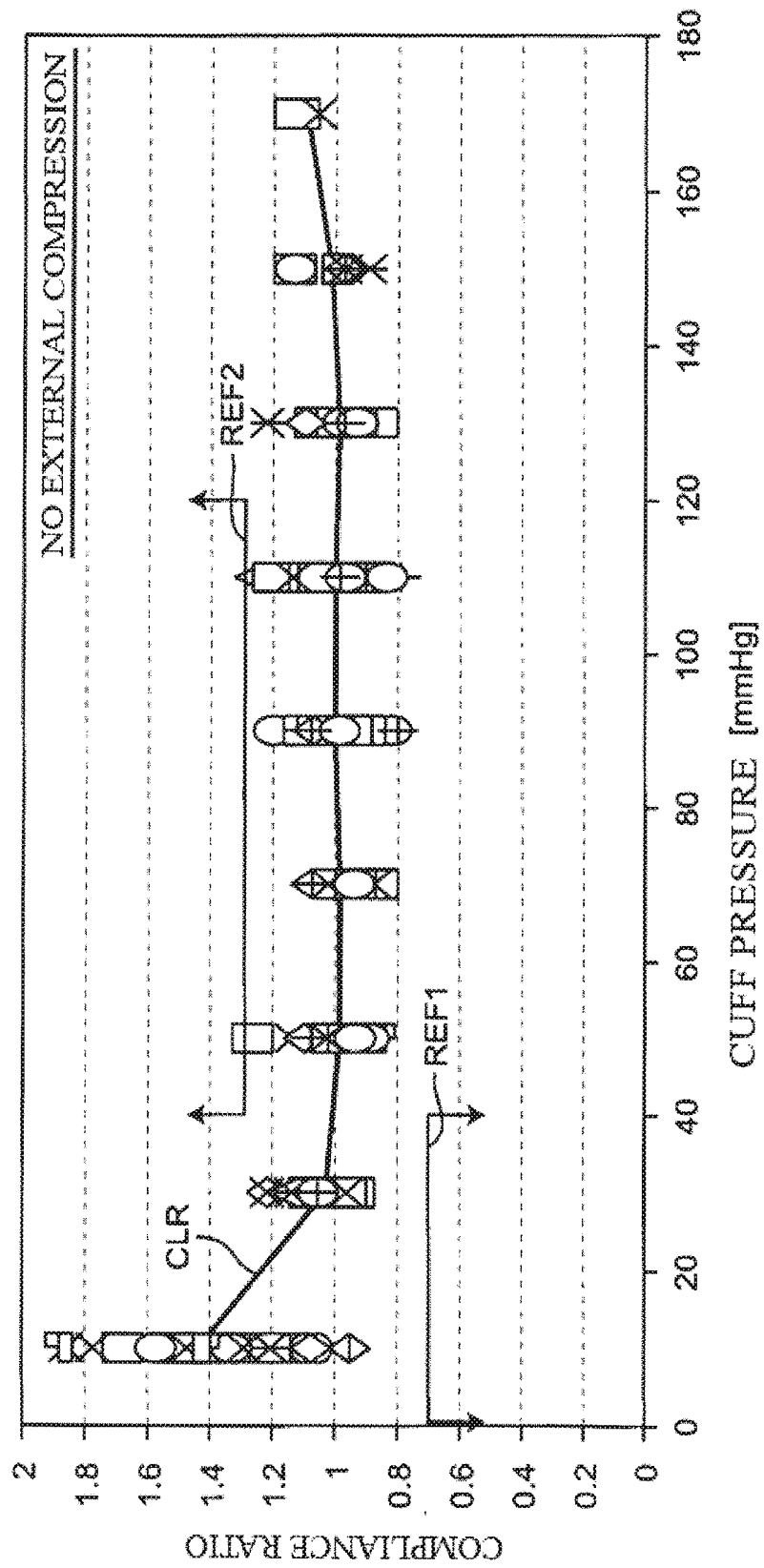


FIG. 14B

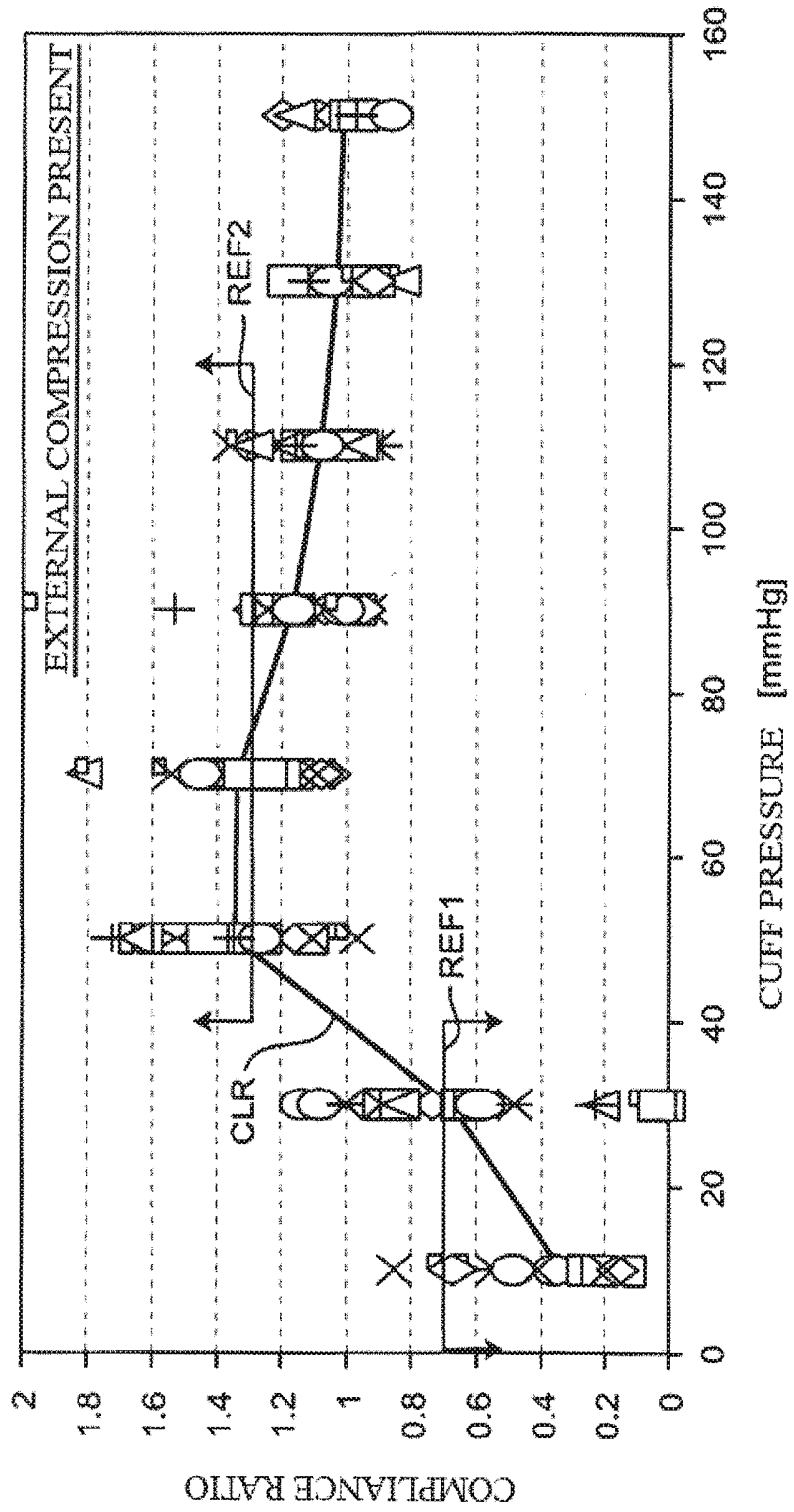
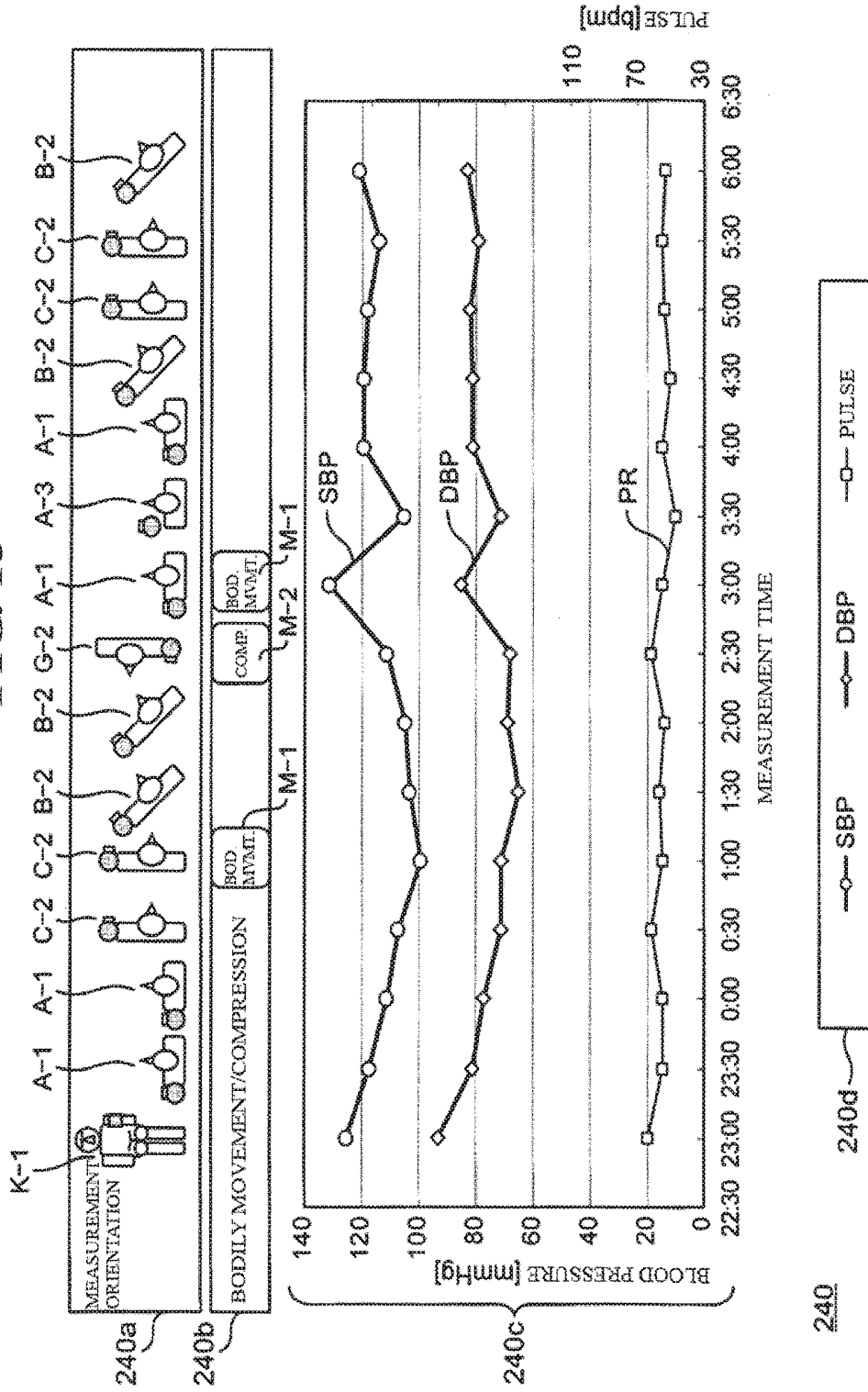


FIG. 15



240

240d

FIG. 16

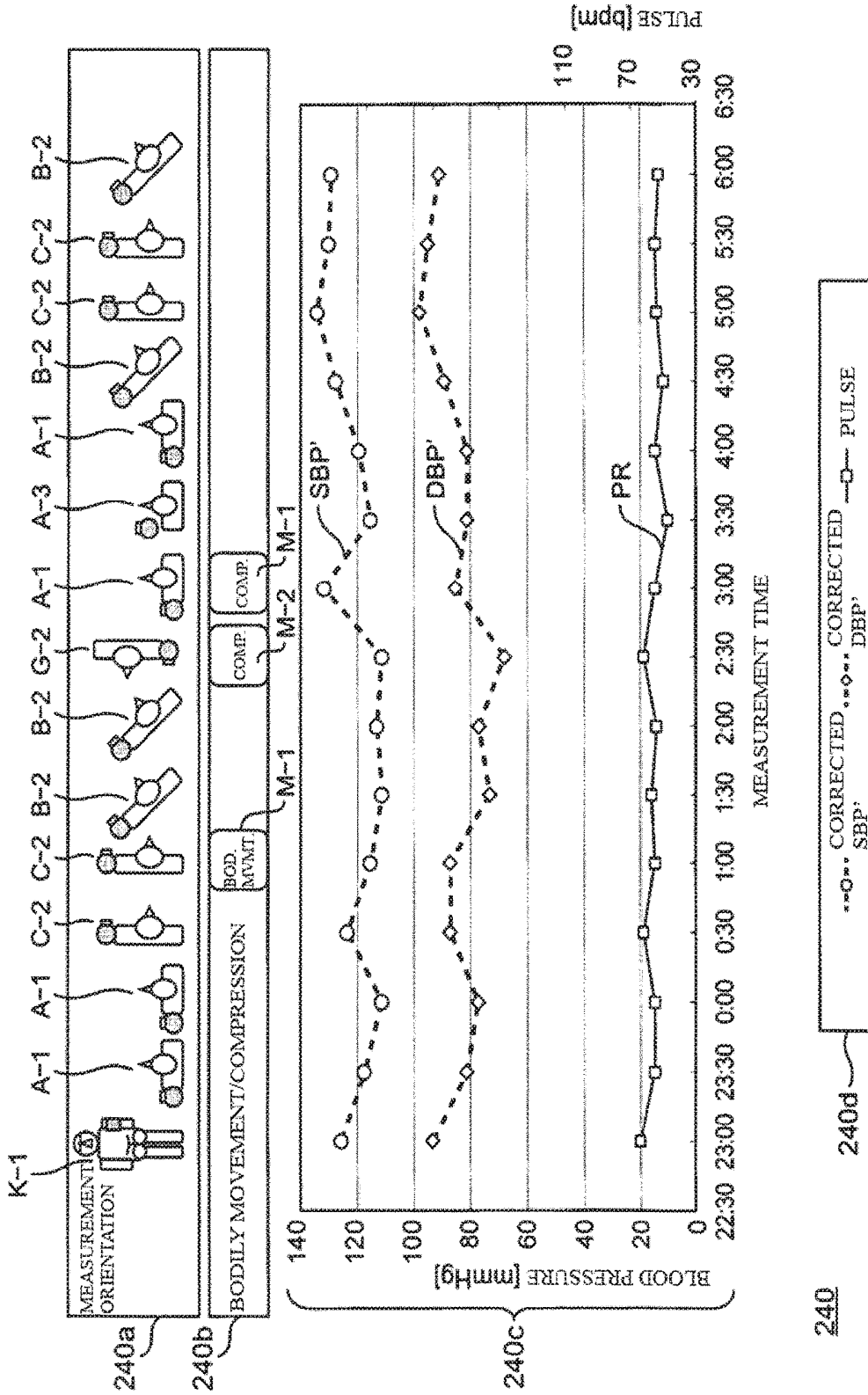
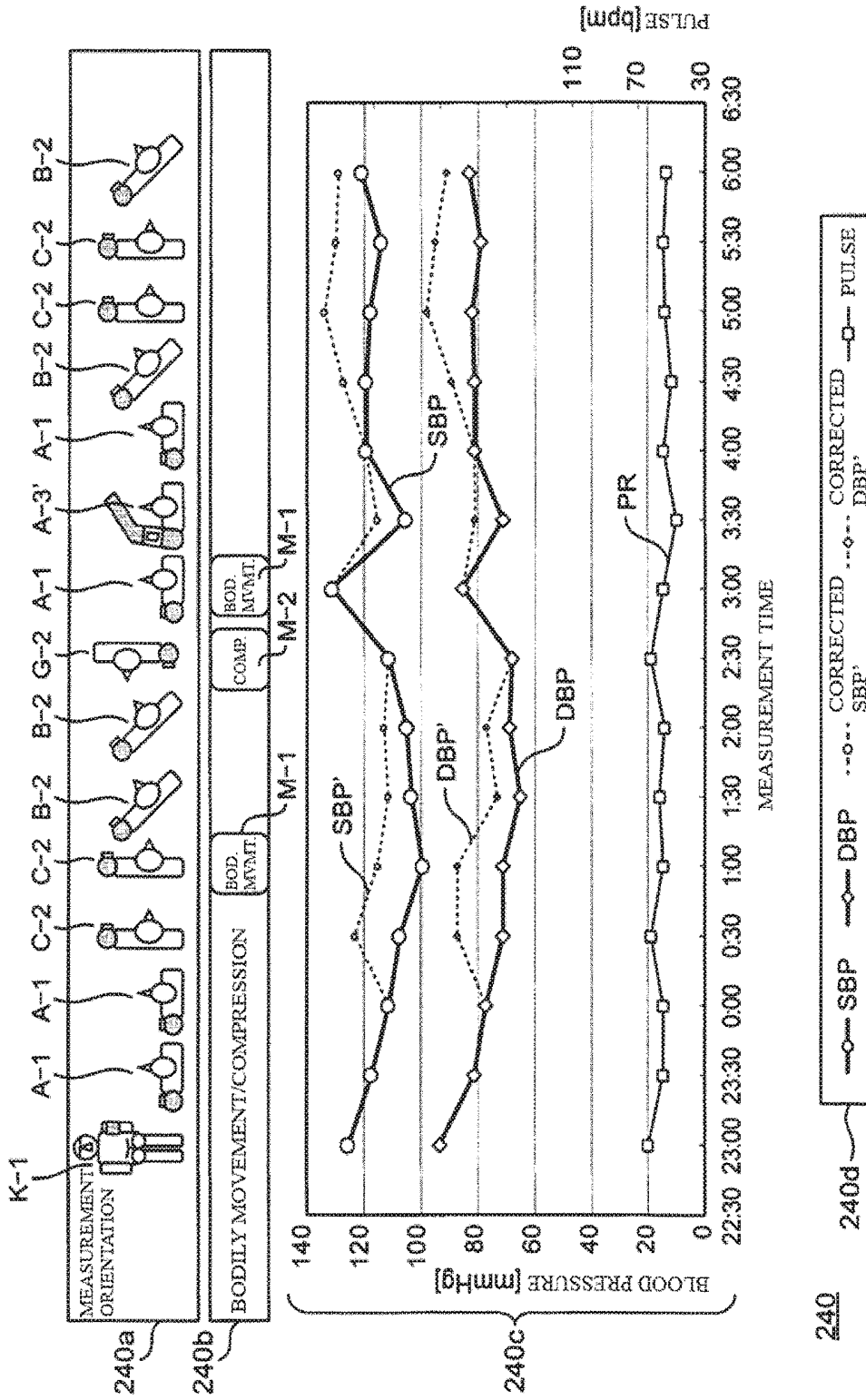


FIG. 17



ELECTRONIC BLOOD PRESSURE MONITOR

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This is a continuation application of International Application No. PCT/JP2016/079314, with an International filing date of Oct. 3, 2016, which claims priority of Japanese Patent Application No. 2015-257066 filed on Dec. 28, 2015, the entire content of which is hereby incorporated by reference.

TECHNICAL FIELD

[0002] The present invention relates to an electronic blood pressure monitor, and more specifically relates to an electronic blood pressure monitor that includes a cuff worn on a measurement site of a measurement subject, and that increases the pressure of the cuff by supplying a fluid thereto to compress the measurement site and perform blood pressure measurement.

BACKGROUND ART

[0003] Conventionally, as this type of electronic blood pressure monitor, as disclosed in Patent Document 1 (JP 2008-188197A) for example, an electronic blood pressure monitor is known in which, upon being started up, air is supplied to a cuff, pressure increase is started, and based on the extent of the increase in the pressure in the cuff, it is determined whether or not the cuff is being worn appropriately on a measurement site such as an upper arm.

SUMMARY OF INVENTION

[0004] Incidentally, in recent years, the importance of measuring night-time blood pressure for treatment of hypertension has been receiving attention. In night-time blood pressure measurement, blood pressure measurement is generally performed automatically using a timer setting during a sleep period of the measurement subject, and therefore the measurement subject cannot consciously correct his or her orientation during blood pressure measurement. For this reason, blood pressure values obtained in various orientations can be recorded. For example, if the measurement subject, who is lying on a bed surface, places the cuff, which is worn on the upper arm (measurement site), under his or her torso, the cuff will be compressed from the outside (the torso and the bed surface), and therefore there is a possibility that the recorded blood pressure value will be influenced. Accordingly, it is convenient if a user (includes a medical professional such as a doctor or a nurse, for example, in addition to the measurement subject; the same applies in the following description) can later check whether or not there was compression from the outside (external compression) on the cuff during blood pressure measurement.

[0005] However, as far as the applicants of the present application know, an electronic blood pressure monitor according to which a user can check whether or not there was external compression on a cuff during blood pressure measurement has not conventionally existed.

[0006] In view of this, the present invention aims to provide a blood pressure monitor according to which a user can check whether or not there was external compression on the cuff during blood pressure measurement.

[0007] In order to solve the above-described problem, the electronic blood pressure monitor of this disclosure includes:

[0008] a blood pressure measurement cuff configured to be worn on a measurement site of a measurement subject;

[0009] a blood pressure measurement unit configured to measure a blood pressure value of the measurement subject using the cuff; and

[0010] an external compression detection unit configured to detect whether or not there was external compression on the cuff during the blood pressure measurement performed by the blood pressure measurement unit, wherein in each predetermined pressure segment, the external compression detection unit calculates a cuff compliance, which is an amount of air that is to be pumped into the cuff and is needed to increase pressure in the cuff per unit pressure, as the pressure of the cuff is increased by the blood pressure measurement unit during blood pressure measurement, and the external compression detection unit determines whether or not there is external compression on the cuff based on a change indicated by the cuff compliance in each pressure segment.

[0011] In the present specification, “during blood pressure measurement” does not indicate the entire period in which the blood pressure measurement cuff is worn for night-time blood pressure measurement and the like, for example, but indicates a timing during which the blood pressure values of the measurement subject are measured by actually increasing or reducing the pressure of the above-described blood pressure measurement cuff.

[0012] Also, “external compression” indicates compression from the outside of the external circumferential surface of the blood pressure monitor that is wrapped around the measurement site. In other words, “external compression” does not encompass compression from the measurement site (inner circumferential surface side of the cuff) around which the blood pressure measurement cuff is wrapped. Typically, external compression occurs when the measurement subject lying on the bed surface places the cuff worn on the measurement site under the torso in the case of night-time blood pressure measurement. Note that “bed surface” widely indicates a surface on which a measurement subject can lie, such as an upper surface of a bed or futon. The torso of the measurement subject may be wearing clothes.

BRIEF DESCRIPTION OF DRAWINGS

[0013] The present invention will become more fully understood from the detailed description given hereinbelow and the accompanying drawings which are given by way of illustration only, and thus are not limitative of the present invention, and wherein:

[0014] FIG. 1 is a schematic view showing an exterior of a blood pressure monitor in which the cuff and the main body are integrated, and in which a blood pressure related information display apparatus according to an embodiment of the invention is included.

[0015] FIG. 2 is a diagram showing a block configuration of the blood pressure monitor.

[0016] FIG. 3 is a diagram showing a block configuration of a hospital terminal that can communicate with the blood pressure monitor via a network.

[0017] FIG. 4A is a diagram showing a state in which the measurement subject wears the blood pressure monitor on a left upper arm serving as a measurement site and is in a

supine orientation (supine position) on a bed surface. FIG. 4B is a diagram showing a state in which the measurement subject has changed the torso angle with respect to the bed surface from the state of FIG. 4A.

[0018] FIG. 5 is a diagram showing an overall operation flow of the blood pressure monitor.

[0019] FIG. 6A is a diagram illustrating a cuff pressure signal, a pulse wave signal, a pump driving signal, and a cuff compliance during blood pressure measurement (pressure increase process) in the case where there is no external compression on the cuff of the blood pressure monitor.

[0020] FIG. 6B is a diagram illustrating a cuff pressure signal, a pulse wave signal, a pump driving signal, and a cuff compliance during blood pressure measurement (pressure increase process) in the case where there is external compression on the cuff of the blood pressure monitor (here, a case in which the cuff is placed under the torso of the measurement subject).

[0021] FIG. 7 is a diagram illustrating the output of an acceleration sensor built in the main body, during blood pressure measurement performed by the blood pressure monitor.

[0022] FIG. 8A is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0023] FIG. 8B is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0024] FIG. 8C is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0025] FIG. 8D is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0026] FIG. 8E is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0027] FIG. 8F is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0028] FIG. 8G is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0029] FIG. 8H is a diagram showing a correspondence relationship between the orientation (torso angle and arm position) of the measurement subject during blood pressure measurement and the outputs (XZ coordinates and XY coordinates) of the acceleration sensor.

[0030] FIGS. 9A and 9B are diagrams illustrating images to be displayed on a display device of the blood pressure monitor.

[0031] FIGS. 10A and 10B are diagrams illustrating images to be displayed on the display device of the blood pressure monitor.

[0032] FIG. 11 is a diagram showing portions of the overall operation flow (portions relating to detection of external compression) of FIG. 5.

[0033] FIG. 12 is a diagram showing a specific flow of cuff compliance calculation processing shown in FIG. 11.

[0034] FIG. 13 is a diagram showing a specific flow of cuff pressure existence detection processing shown in FIG. 11.

[0035] FIG. 14A is a diagram showing a change in the compliance ratio accompanying a change in the cuff pressure during blood pressure measurement (pressure increase process) in the case where there is no external compression on the cuff.

[0036] FIG. 14B is a diagram showing a change in the compliance ratio accompanying a change in the cuff pressure during blood pressure measurement (pressure increase process) in the case where there is external compression on the cuff (here, in the case where the cuff is placed under the torso of the measurement subject).

[0037] FIG. 15 is a diagram illustrating an image to be displayed on the display device of the hospital terminal.

[0038] FIG. 16 is a diagram illustrating another image to be displayed on the display device of the hospital terminal.

[0039] FIG. 17 is a diagram illustrating yet another image to be displayed on the display device of the hospital terminal.

DESCRIPTION OF EMBODIMENTS

Configuration of Blood Pressure Monitor

[0040] FIG. 1 shows an exterior of an electronic blood pressure monitor (indicated overall by reference numeral 1) according to an embodiment of the invention.

[0041] The blood pressure monitor 1 mainly includes a blood pressure measurement cuff 20 that is to be wrapped around a measurement site of a measurement subject, and a main body 10 that is integrally attached to the cuff 20.

[0042] The cuff 20 has a shape that is elongated so as to wrap around the measurement site along the circumferential direction, and includes a band-shaped inner cloth 20a that is to come into contact with the measurement site, and an outer cloth 20b that opposes the inner cloth 20a. The inner cloth 20a and the outer cloth 20b are formed into a bladder shape by having their peripheral edges sewn together. The cuff 20 contains a fluid bladder 22 (see FIG. 2) for compressing a measurement site.

[0043] In order to form a surface fastener, the surface (inner circumferential surface that is to come into contact with the measurement site) of the inner cloth 20a is provided with many minute hooks (not shown). On the other hand, many minute loops (not shown) that engage with the above-described hooks are formed on the surface (outer circumferential surface) of the outer cloth 20b.

[0044] The main body 10 is integrally attached to a site between one end (end portion that is to serve as the inner circumferential end when worn) 20e and another end (end portion that is to serve as the outer circumferential end when worn) 20f with respect to the lengthwise direction (circumferential direction) of the cuff 20.

[0045] When the blood pressure monitor 1 is worn on the left upper arm 90a (see FIG. 4A) serving as the measurement site, the left upper arm 90a is arranged in the orientation indicated by the arrow A in FIG. 1 and the cuff 20 is arranged along with the main body 10 on the front surface of the left upper arm 90a. Next, the cuff 20 is wrapped in the form of a left-handed spiral as viewed by the measurement subject. Then, the corresponding surface of the inner cloth 20a is pressed onto and fixed to a site near the inner circumferential end 20e compared to the main body 10 of the outer cloth 20b. The extra portion near the other end 20f in the lengthwise direction (circumferential direction) of the cuff 20 is folded over so as to prevent the main body 10 from being hidden.

[0046] FIG. 2 shows a schematic block configuration of the cuff 20 and the main body 10 of the blood pressure monitor 1. The blood pressure monitor 1 includes a CPU (Central Processing Unit) 100 serving as a control unit, a display device 50, an operation unit 52, a memory 51 serving as a storage unit, a communication unit 59, a power source unit 53, a pump 32, a valve 33, a pressure sensor 31, and an acceleration sensor 34, all of which are mounted in the main body 10. Furthermore, the main body 10 includes an oscillation circuit 310 that converts the output from the pressure sensor 31 into a frequency, a pump driving circuit 320 that drives the pump 32, a valve driving circuit 330 that drives the valve 33, and an AD converter 340 that performs AD (Analog to Digital) conversion on the output from the acceleration sensor 34, all of which are mounted in the main body 10.

[0047] In this example, the display device 50 is composed of an LCD (Liquid Crystal Display) and displays information relating to blood pressure, such as a blood pressure measurement result, in accordance with a control signal from the CPU 100.

[0048] The operation unit 52 includes a power source switch 52A for turning on and off the power source of the main body 10, a measurement start switch 52B for receiving an instruction to start blood pressure measurement, and a memory switch 52C for calling a blood pressure measurement result stored in the memory. The switches 52A, 52B, and 52C input operation signals corresponding to instructions performed by a user to the CPU 100.

[0049] As shown in FIG. 1, the display device 50 and the operation unit 52 are provided on the front surface (upper surface in FIG. 1) or the side surface of the main body 10.

[0050] The memory 51 shown in FIG. 2 stores data of programs for controlling the blood pressure monitor 1, data to be used to control the blood pressure monitor 1, setting data for setting various functions of the blood pressure monitor 1, data of measurement results of blood pressure values, data indicating whether or not there is later-described external compression on the cuff 20, whether or not there is bodily movement of a measurement subject, and the orientation of the measurement subject, and the like. Also, the memory 51 is used as a work memory or the like for when a program is executed.

[0051] In accordance with a program for controlling the blood pressure monitor 1 that is stored in the memory 51, the CPU 100 performs control for driving the pump 32 and the valve 33 according to the operation signal from the operation unit 52. Also, based on a signal from the pressure sensor 31, the CPU 100 performs control for calculating the blood pressure values and control for detecting whether or not

there is external compression on the cuff 20. Furthermore, based on the output of the acceleration sensor 34, the CPU 100 performs control for detecting whether or not there is bodily movement of the measurement subject and the orientation of the measurement subject. These controls will be described in detail later.

[0052] The communication unit 59 is controlled by the CPU 100 to transfer predetermined information to an external apparatus via the network 900, and to receive information from the external apparatus via the network 900 and transfer it to the CPU 100. Communication via the network 900 may be performed wirelessly or using a wire. In this embodiment, the network 900 is the Internet, but there is no limitation to this, and it is also possible to use another type of network such as an in-hospital LAN (Local Area Network), or one-to-one communication using a USB cable or the like.

[0053] The power source unit 53 supplies power to the units, namely the CPU 100, the pressure sensor 31, the pump 32, the valve 33, the acceleration sensor 34, the display device 50, the memory 51, the communication unit 59, the oscillation circuit 310, the pump driving circuit 320, the valve driving circuit 330, and the AD converter 340.

[0054] The pump 32, the valve 33, and the pressure sensor 31 are connected to the fluid bladder 22 contained in the cuff 20 via a common air tube 39 serving as a tube system. The pump 32 supplies air to the fluid bladder 22 through the air tube 39 in order to increase the pressure (cuff pressure) in the fluid bladder 22 contained in the cuff 20. The valve 33 is a solenoid valve that is controlled so as to open and close through application of a current, and is used to control the cuff pressure by discharging the air in the air bladder 22 through the air tube 39 or sealing the air in the air bladder 22. The pump driving circuit 320 drives the pump 32 based on the control signal provided by the CPU 100. The valve driving circuit 330 opens and closes the valve 33 based on the control signal provided from the CPU 100.

[0055] In this example, the pressure sensor 31 is a piezoresistance pressure sensor that detects the pressure of the cuff 20 (fluid bladder 22) through the air tube 39, and in this example, the pressure sensor 31 detects a pressure obtained with reference to atmospheric pressure (with atmospheric pressure being set to zero) and outputs the detected pressure as a cuff pressure signal P_c in a time series. The oscillation circuit 310 oscillates based on an electricity signal value that is based on a change in the electric resistance caused by a piezoresistance effect from the pressure sensor 31, and outputs a frequency signal having a frequency corresponding to the electricity signal value of the pressure sensor 31 to the CPU 100.

[0056] In this example, the output of the pressure sensor 31 is used to calculate the blood pressure values (includes systolic blood pressure and diastolic blood pressure; the same applies in the description hereinafter) of the measurement subject 90 through an oscillometric method. In addition to this, the output of the pressure sensor 31 is used to determine whether or not there is external compression on the cuff 20 by calculating the cuff compliance (amount of air needed to change the cuff pressure by a unit pressure 1 mmHg). Typically, in the case of night-time blood pressure measurement, external compression occurs when the cuff 20 and the left upper arm 90a serving as the measurement site

are placed under the torso of the measurement subject who is lying down, and are compressed by the torso and the bed surface.

[0057] The acceleration sensor **34** is composed of a tri-axial acceleration sensor that is integrally built into the main body **10**. The acceleration sensor **34** outputs an acceleration signal indicating acceleration in three mutually orthogonal directions of the main body **10** and accordingly, of the cuff **20** integrally attached to the main body **10**, to the CPU **100** via the AD converter **340**.

[0058] In this example, as shown in FIG. 4A, an XYZ orthogonal coordinate system is set with the position of the acceleration sensor **34** in the main body **10** serving as the origin. The Z axis is set facing outward orthogonally to the front surface of the main body **10**. The Y axis is set in an orientation facing from the knee to the shoulder along the left upper arm **90a** of the measurement subject **90** in a state in which the blood pressure monitor **1** is worn on the left upper arm **90a** serving as the measurement site as described above. Also, the X axis is set orthogonally to the Y axis and the Z axis (the X axis faces approximately leftward as viewed by the measurement subject **90**, but this depends on the orientation of the measurement subject **90** as well). Note that in FIG. 4A, the measurement subject **90** is in a supine orientation (supine position) on the bed surface **99**, but in actuality, especially in the case of night-time blood pressure measurement, the measurement subject **90** can be in various orientations. For example, as shown in FIG. 4B, the measurement subject can be in an orientation in which the angle θ of the torso is changed with respect to the bed surface **99**.

[0059] In this example, the output of the acceleration sensor **34** is used to detect whether or not there is bodily movement of the measurement subject **90**. In addition, the output of the acceleration sensor **34** is used to detect the orientation of the measurement subject **90** according to the direction (e.g., in FIGS. 4A and 4B, the directions of the gravity acceleration vectors G with respect to the XYZ orthogonal coordinate system are different) of a gravity acceleration vector G with respect to the above-described XYZ orthogonal coordinate system.

Method of Detecting External Compression

[0060] FIG. 6A shows a cuff pressure signal P_c , a pulse wave signal SM , a pump driving signal V_{out} , and a cuff compliance CL during blood pressure measurement (pressure increase process) in the case where there is no external compression on the cuff **20**. On the other hand, FIG. 6B shows a cuff pressure signal P_c , a pulse wave signal SM , a pump driving signal V_{out} , and a cuff compliance CL during blood pressure measurement (pressure increase process) in the case where there is external compression on the cuff **20** (here, a case in which the cuff **20** is placed under the torso of the measurement subject **90**). The cuff pressure signal P_c indicates the pressure of the cuff **20** (fluid bladder **22**) that is detected via the air tube **39** and the oscillation circuit **310** by the pressure sensor **31**. The pulse wave signal SM indicates a signal extracted through a filter (not shown) as a fluctuation component of the cuff pressure signal P_c (the pulse wave signal SM is used to calculate the blood pressure values through an oscillometric method). The pump driving signal V_{out} indicates a square wave signal (pulse width modulation signal) output from the CPU **100** to the pump driving circuit **320** in order to increase the pressure of the cuff **20**. The cuff compliance CL is obtained as values

(calculated for each predetermined pressure segment) CM_a , CM_b , CM_c , CM_d , . . . , which are obtained by integrating the duty of the pump driving signal V_{out} over time. In order to facilitate understanding, in FIGS. 6A and 6B, an envelope EV is added to the sequence formed by the values CM_a , CM_b , CM_c , CM_d , . . . of the cuff compliance CL .

[0061] As can be understood from FIG. 6A, if there is no external compression on the cuff **20**, air is supplied to the cuff **20**, and the cuff compliance CL gradually decreases and is saturated as pressure increase from the low pressure range (0 mmHg to less than 40 mmHg) to the high pressure range (over 120 mmHg) is performed. The reason for this is because if there is no external compression on the cuff **20**, the volume of the cuff easily expands in the low pressure region (0 mmHg to less than 40 mmHg), and therefore a large amount of air is needed to raise the cuff pressure, but the volume of the cuff **20** is substantially less likely to increase when the tensile force of the cuff **20** increases due to the cuff pressure rising by a certain degree. On the other hand, as can be understood from FIG. 6B, if there is external compression on the cuff **20**, the cuff compliance CL has a maximum value in the pressure increase process. In this case, in the low pressure region (0 mmHg to less than 40 mmHg), the volume of the cuff **20** increases due to the cuff **20** pressing back on the torso of the measurement subject **90**. Accordingly, the cuff compliance CL changes gradually from a low value (varies due to the influence of the tensile force of wrapping the cuff around the measurement site) to a high value. On the other hand, in the high pressure region (over 120 mmHg), the torso is pushed away by the top of the cuff **20** due to the inflation of the cuff **20**, and therefore the cuff compliance CL gradually decreases and is saturated, similarly to the case shown in FIG. 6A (the case in which there is no external compression). As a result, in the intermediate range (40 mmHg or more, 120 mmHg or less), the cuff compliance CL has a maximum value accompanying the rising of the cuff pressure.

[0062] Accordingly, it is possible to detect whether or not there is external compression on the cuff **20** according to whether or not the cuff compliance CL has a maximum value in the intermediate pressure range (40 mmHg or more and 120 mmHg or less) in the pressure increase process.

Method of Detecting Bodily Movement

[0063] FIG. 7 illustrates the outputs (acceleration signals) of the acceleration sensor **34** during blood pressure measurement. During blood pressure measurement, and especially during night-time blood pressure measurement, the measurement subject **90** is essentially in a resting state, and therefore an output α_x in the X-axis direction of the acceleration sensor **34**, an output α_y in the Y-axis direction, and an output α_z in the Z-axis direction have approximately constant values. However, if the measurement subject **90** temporarily moves by turning over or the like, the outputs α_x , α_y , and α_z change as indicated by $\alpha_{x,1}$, $\alpha_{y,1}$, and $\alpha_{z,1}$.

[0064] In this example, the CPU **100** functions as a bodily movement detection unit, and during blood pressure measurement, obtains average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, and $\langle \alpha_z \rangle$ of the outputs α_x , α_y , and α_z of the acceleration sensor **34** in each unit period (e.g., one second or several seconds). Furthermore, the CPU **100** obtains fluctuation amounts $(\alpha_x - \langle \alpha_x \rangle)$, $(\alpha_y - \langle \alpha_y \rangle)$, and $(\alpha_z - \langle \alpha_z \rangle)$ by which the acceleration outputs α_x , α_y , and α_z of the times in the unit period

fluctuate with respect to the average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, and $\langle \alpha_z \rangle$. Also, when the square root of the sum of squares of these fluctuation amounts

$$\{(\alpha_x - \langle \alpha_x \rangle)^2 + (\alpha_y - \langle \alpha_y \rangle)^2 + (\alpha_z - \langle \alpha_z \rangle)^2\}^{1/2}$$

exceeds a predetermined threshold (denoted as $\Delta\alpha$), it is determined that there is bodily movement. On the other hand, if the square root of the sum of the squares is less than or equal to the threshold $\Delta\alpha$, it is determined that there is no bodily movement.

[0065] Accordingly, it is possible to detect whether or not there is bodily movement of the measurement subject **90** based on changes in the outputs of the acceleration sensor **34**.

Method of Detecting Orientation

[0066] FIGS. **8A** to **8H** show correspondence relationships between the orientation (torso angle and arm position) of the measurement subject **90** during blood pressure measurement and the normalized outputs (XZ coordinates and XY coordinates) of the acceleration sensor **34**.

[0067] Specifically, FIGS. **8A** to **8H** show eight types of “torso angles” as torso patterns in the first rows (top rows). “Torso angle” means the angle (indicated by reference numeral θ in FIG. **4B**) by which the flat torso **90b** is rotated about a center (approximately matches the spine) in a view along the body height direction (in this example, in a view from head to feet) of a person lying on a bed surface. In FIG. **8A**, the torso **90b** is in the supine position and the torso angle is 0 degrees. In FIG. **8B**, the torso **90b** is between the supine position and the right side position, and the torso angle is 20 degrees. In FIG. **8C**, the torso **90b** is in the right side position and the torso angle is 90 degrees. In FIG. **8D**, the torso **90b** is between the right side position and the prone position, and the torso angle is 160 degrees. In FIG. **8E**, the torso **90b** is in the prone position and the torso angle is 180 degrees. In FIG. **8F**, the torso **90b** is between the prone position and the left side position, and the torso angle is 200 degrees. In FIG. **8G**, the torso **90b** is in the left side position and the torso angle is 270 degrees. In FIG. **8H**, the torso **90b** is between the left side position and the supine position, and the torso angle is 340 degrees.

[0068] Also, in FIGS. **8A** to **8H**, the second rows each show four or three types of representative arm positions serving as arm patterns corresponding to arm positions that are varied with respect to a person’s torso. In FIG. **8A**, in the first column (leftmost column), the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, in the second column, the left upper arm **90a** is at a “body-side separated” position of being separated laterally from the torso **90b**, in the third column, the left upper arm **90a** is at an “on-chest” position of being placed on the torso **90b**, and in the fourth column (rightmost column), the left upper arm **90a** is in a “hurrah” position of being raised toward the head. In FIGS. **8B**, **8C**, and **8D**, in the first columns (leftmost columns), the left upper arm **90a** is at a “back-side” position of being rotated rearward of the torso **90b**, in the second columns, the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, in the third columns, the left upper arm **90a** is at a “chest-side” position of being rotated frontward of the torso **90b**, and in the fourth columns (rightmost columns), the left upper arm **90a** is at a “hurrah” position of being raised toward the head. In FIG. **8E**, in the first column

(leftmost column), the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, in the second column, the left upper arm **90a** is at a “body-side separated” position of being separated laterally from the torso **90b**, and in the third column, (rightmost column), the left upper arm **90a** is in a “hurrah” position of being raised toward the head. In FIG. **8F**, in the first column (leftmost column), the left upper arm **90a** is at a “back-side” position of being rotated rearward of the torso **90b**, in the second column, the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, and in the third column (rightmost column), the left upper arm **90a** is at a position of being rotated frontward of the torso **90b**. In FIG. **8G**, in the first column (leftmost column), the left upper arm **90a** is at a “chest-front separated” position of being separated frontward from the torso **90b**, in the second column, the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, and in the third column (rightmost column), the left upper arm **90a** is at a “hurrah” position of being raised toward the head. Also, in FIG. **8H**, in the first column (leftmost column), the left upper arm **90a** is at a “chest-front” position of being rotated frontward from the torso **90b**, in the second column, the left upper arm **90a** is at a “body-lateral” position of extending along the lateral side of the torso **90b**, and in the third column (rightmost column), the left upper arm **90a** is at a “hurrah” position of being raised toward the head.

[0069] The orientations of the measurement subject **90** during blood pressure measurement (in particular, during night-time blood pressure measurement) are specified using combinations of the “torso angles” in the first rows (top rows) and the “arm positions” in the second rows corresponding thereto in FIGS. **8A** to **8H**.

[0070] In the third rows and the fourth rows (bottom rows) in FIGS. **8A** to **8H**, the normalized (normalized to 1) outputs of the acceleration sensor **34** in cases where the measurement subject **90** is in orientations specified using combinations of the “torso angles” in the first rows and the “arm positions” in the second rows are indicated in XZ coordinate planes and XY coordinate planes. Here, the measurement subject **90** is substantially in a resting state, and the outputs (the above-described average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, and $\langle \alpha_z \rangle$) of the acceleration sensor **34** correspond to the direction of the gravity acceleration vector **G** corresponding to the XYZ orthogonal coordinate system set in the main body **10**.

[0071] For example, if the measurement subject **90** is in an orientation specified using a combination in which the “torso angle” is 0 degrees and the “arm position” is “body-lateral” in the first column (leftmost column) of FIG. **8A**, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $X=0$ and $Z=1$ in the XZ coordinate plane in the third row, and as point a_{xy} where $X=0$ and $Y=0$ in the XY coordinate plane in the fourth row. Also, when the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 0 degrees and the “arm position” is “body-side separated” in the second column of FIG. **8A**, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $-1 < X < 0$ and $0 < Z < 1$ (second quadrant) in the XZ coordinate plane in the third row, and as point a_{xy} where $-1 < X < 0$ and $Y=0$ in the XY coordinate plane in the fourth row. When the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 0 degrees and the “arm position” is “on-chest” in the third column of FIG.

8A, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $0 < X < 1$ and $0 < Z < 1$ (first quadrant) in the XZ coordinate plane in the third row, and as point a_{xy} where $0 < X < 1$ and $-1 < Y < 0$ (fourth quadrant) are satisfied in the XY coordinate plane in the fourth row. When the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 0 degrees and the “arm position” is “hurrah” in the fourth column (rightmost column) of FIG. **8A**, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $-1 < X < 0$ and $-1 < Z < 0$ (third quadrant) in the XZ coordinate plane in the third row, and as point a_{xy} where $-1 < X < 0$ and $-1 < Y < 0$ (third quadrant) in the XY coordinate plane in the fourth row.

[0072] Also, for example, if the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 270 degrees and the “arm position” is “chest-front separated” in the first column (leftmost column) in FIG. **8G**, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $X = -1$ and $Z = 0$ in the XZ coordinate plane in the third row, and as point a_{xy} where $X = -1$ and $Y = 0$ in the XY coordinate plane in the fourth row. Also, if the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 270 degrees and the “arm position” is “body-lateral” in the second column in FIG. **8G**, the normalized outputs of the acceleration sensor **34** are detected as point a_{xz} where $X = -1$ and $Z = 0$ in the XZ coordinate plane in the third row, and as point a_{xy} where $X = -1$ and $Y = 0$ in the XY coordinate plane in the fourth row. If the measurement subject **90** is in an orientation specified using the combination in which the “torso angle” is 270 degrees and the “arm position” is “hurrah” in the third column (rightmost column) in FIG. **8G**, the normalized output of the acceleration sensor **34** is detected as point a_{xz} where $0 < X < 1$ and $0 < Z < 1$ (first quadrant) in the XZ coordinate plane in the third row, and as point a_{xy} where $0 < X < 1$ and $Y = 0$ in the XY coordinate plane in the fourth row.

[0073] As can be understood from the examples above, in FIGS. **8A** to **8H**, when the measurement subject **90** is in an orientation specified using a combination of a “torso angle” in a first row and an “arm position” in a second row, the orientation and the normalized output (combination of XZ coordinates and XY coordinates) of the acceleration sensor **34** are in a one-to-one correspondence. Accordingly, if the normalized outputs (combination of the XZ coordinates and the XY coordinates) of the acceleration sensor **34** are specified, the orientation of the measurement subject **90**, that is, the combination of the “torso angle” and the “arm position” is specified. In other words, the orientation of the measurement subject **90** is determined. In this example, the CPU **100** functions as an orientation detection unit and determines the orientation of the measurement subject **90** based on the outputs (the above-described average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, and $\langle \alpha_z \rangle$ are desirable) of the acceleration sensor **34**. Accordingly, the orientation of the measurement subject can be detected easily.

[0074] With the blood pressure monitor **1**, in order to express the orientation of the measurement subject **90** specified based on the output of the acceleration sensor **34**, illustrations A-1 to A-4 shown in the first row in FIG. **8A**, illustrations B-1 to B-4 shown in the first row in FIG. **8B**, illustrations C-1 to C-4 shown in the first row in FIG. **8C**, illustrations D-1 to D-4 shown in the first row in FIG. **8D**,

illustrations E-1 to E-3 shown in the first row in FIG. **8E**, illustrations F-1 to F-3 shown in the first row in FIG. **8F**, illustrations G-1 to G-3 shown in the first row in FIG. **8G**, and illustrations H-1 to H-3 shown in the first row in FIG. **8H** are prepared in advance. These illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3 correspond to combinations obtained using the torso patterns and arm patterns as materials.

[0075] In these illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3, the torso **90b** of the measurement subject **90** is expressed as an elongated circle. In the approximate center in the long axis direction of the elongated circle indicating the torso **90b**, the head **90h** of the measurement subject **90** is indicated by a circle and a small triangle corresponding to the nose, in a state of being overlaid slightly shifted in the short axis direction. Also, the left upper arm **90a** around which the cuff **20** is wrapped is indicated by a circle on the left side of the elongated circle indicating the torso **90b**. The main body **10** attached integrally to the cuff **20** is indicated by a rectangle.

[0076] For example, in the illustration A-1 shown in FIG. **8A**, the elongated circle indicating the torso **90b** is extended in the horizontal direction so as to indicate that the torso angle is 0 degrees (supine position). The circle indicating the head **90h** of the measurement subject **90** is overlaid shifted upward of the elongated circle indicating the torso **90b** (note that up, down, left, and right in this paragraph indicate up, down, left, and right in FIG. **8A**). The circle indicating the left upper arm **90a** is adjacent to the left of the elongated circle indicating the torso **90b** so as to indicate “body-lateral”. The rectangle indicating the main body **10** is located on the upper portion of the circle indicating the left upper arm **90a** so as to indicate that the main body **10** is on the front surface of the left upper arm **90a**. In the illustration A-2, the circle indicating the left upper arm **90a** is separated from the elongated circle indicating the torso **90b** so as to indicate “body-side separated”. In the illustration A-3, the circle indicating the left upper arm **90a** is located above and to the left of the elongated circle indicating the torso **90b** so as to indicate “on-chest”. In the illustration A-4, the circle indicating the left upper arm **90a** is located above and to the left of the elongated circle indicating the torso **90b** and the rectangle indicating the main body **10** is located below the circle indicating the left upper arm **90a** so as to indicate “hurrah”. The other portions of the illustrations A-2 to A-4 are drawn in the same manner as those of the illustration A-1.

[0077] Also, for example, in the illustration G-1 shown in FIG. **8G**, the elongated circle indicating the torso **90b** is elongated in the vertical direction so as to indicate that the torso angle is 270 degrees (left side position). The circle indicating the head **90h** of the measurement subject **90** is overlaid shifted to the left of the elongated circle indicating the torso **90b** (note that up, down, left, and right in this paragraph indicate up, down, left, and right in FIG. **8G**). The circle indicating the left upper arm **90a** is separated from the elongated circle indicating the torso **90b** so as to indicate “chest-front separated”. The rectangle indicating the main body **10** is located on the left portion of the circle indicating the left upper arm **90a** so as to indicate that the main body **10** is on the front surface of the left upper arm **90a**. In the illustration G-2, the circle indicating the left upper arm **90a**

is adjacent to the bottom of the elongated circle indicating the torso **90b** so as to indicate “body-lateral”. In the illustration G-3, the circle indicating the left upper arm **90a** is located downward and to the left of the elongated circle indicating the torso **90b** and the rectangle indicating the main body **10** is located on the right portion of the circle indicating the left upper arm **90a** so as to indicate “hurray”. The other portions of the illustrations G-2 to G-3 are drawn in the same manner as those of the illustration G-1.

[0078] In this manner, the orientation of the measurement subject **90** can be schematically indicated using the illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3, that is, as a combination of a torso pattern indicating the “torso angle” and an arm pattern indicating the “arm position”.

[0079] With the blood pressure monitor **1**, the normalized outputs (XZ coordinates and XY coordinates) of the acceleration sensor **34** in the third rows and the fourth rows in FIGS. **8A** to **8H** and the illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3 in the first rows are stored in a one-to-one correspondence as an orientation table in the memory **51**. Thus, by preparing various illustrations indicating orientations of the measurement subject **90** in advance, image data including an illustration of an orientation of the measurement subject **90** can be created rapidly with simple processing during later-described display processing (step ST110 in FIG. **5**).

Overall Operation

[0080] FIG. **5** illustrates an overall operation flow of the blood pressure monitor **1**.

[0081] If the measurement start switch **52B** is pressed in a state in which the power source switch **52A** is on, or if a predetermined measurement timing is reached in the case of night-time blood pressure measurement, the blood pressure monitor **1** starts the blood pressure measurement. At the start of blood pressure measurement, the CPU **100** initializes a memory region for processing and outputs a control signal to the valve driving circuit **330**. Based on the control signal, the valve driving circuit **330** opens the valve **33** to discharge the air in the fluid bladder **22** of the cuff **20**. Next, control for adjusting the pressure sensor **31** to 0 mmHg is performed.

[0082] When the blood pressure measurement is started, first, the CPU **100** closes the valve **33** via the valve driving circuit **330**, and thereafter drives the pump **32** via the pump driving circuit **320** while monitoring the cuff pressure signal P_c using the pressure sensor **31** (and the air tube **39** and the oscillation circuit **310**), and thus performs control for sending air to the fluid bladder **22**. Accordingly, the fluid bladder **22** is inflated and the cuff pressure gradually increases (step ST101).

[0083] In the pressure increase process, in order to detect whether or not there is external compression on the cuff **20**, the CPU **100** integrates the pump driving signal V_{out} for the pump driving circuit **320** to acquire data indicating the cuff compliance CL , as illustrated in FIGS. **6A** and **6B** (step ST102).

[0084] Also, in the pressure increase process, in order to detect whether or not there is bodily movement of the measurement subject **90** and the orientation of the measurement subject **90**, the CPU **100** acquires the outputs of the acceleration sensor **34** (step ST **103**).

[0085] Also, in this example, in the pressure increase process, in order to calculate the blood pressure values, the CPU **100** acquires the pulse wave signal SM serving as a fluctuation component through a filter (not shown) from the cuff pressure signal P_c (step ST104).

[0086] Next, the CPU **100** functions as a blood pressure measurement unit and attempts calculation of the blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) and the pulse by applying a known algorithm through the oscillometric method based on the pulse wave signal SM acquired at this time point (step ST105).

[0087] At this time point, if the blood pressure values cannot yet be calculated due to insufficient data (NO in step ST105), the processing of steps ST101 to ST105 are repeated as long as the cuff pressure has not reached the upper limit pressure (in the interest of safety, the upper limit pressure is set in advance to 300 mmHg, for example) (NO in step ST106).

[0088] When the blood pressure values and pulse can be thus calculated (YES in step ST105), the processing advances to step ST107, and the CPU **100** detects whether or not there is external compression on the cuff **20**, whether or not there is bodily movement of the measurement subject **90**, and the orientation of the measurement subject **90**.

[0089] Here, the CPU **100** functions as an external compression detection unit and detects whether or not there is external compression on the cuff **20** based on whether or not the cuff compliance CL is at a maximum value in the pressure increase process. Specifically, when the cuff compliance CL decreases monotonically as illustrated in FIG. **6A** in the pressure increase process, it is determined that there is no external compression. On the other hand, when the cuff compliance CL has a maximum value as illustrated in FIG. **6B** in the pressure increase process, it is determined that there is external compression.

[0090] Also, the CPU **100** functions as a bodily movement detection unit and detects whether or not there is bodily movement of the measurement subject **90** based on changes in the output of the acceleration sensor **34**. Specifically, in each unit period (e.g., one second or multiple seconds) in the pressure increase process, the CPU **100** obtains the average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, and $\langle \alpha_z \rangle$ of the outputs α_x , α_y , and α_z of the acceleration sensor **34** illustrated in FIG. **7**. Then, when the square root of the sum of squares of the fluctuation amounts of the acceleration outputs α_x , α_y , and α_z in the unit period

$$\{(\alpha_x - \langle \alpha_x \rangle)^2 + (\alpha_y - \langle \alpha_y \rangle)^2 + (\alpha_z - \langle \alpha_z \rangle)^2\}^{1/2}$$

exceeds a predetermined threshold $\Delta\alpha$, it is determined that there is bodily movement. On the other hand, if the square root of the sum of the squares is less than or equal to the threshold $\Delta\alpha$, it is determined that there is no bodily movement.

[0091] Also, the CPU **100** functions as an orientation detection unit and detects the orientation of the measurement subject **90** based on the outputs (the above-described average values $\langle \alpha_x \rangle$, $\langle \alpha_y \rangle$, $\langle \alpha_z \rangle$) of the acceleration sensor **34** in the pressure increase process. Specifically, the CPU **100** determines whether or not the orientation of the measurement subject **90** corresponds to an orientation in an illustration in one of the first rows (top rows) in FIGS. **8A** to **8H** based on the correspondence relationship between the normalized outputs (XZ coordinates and XY coordinates) of the

acceleration sensor **34** in the third rows and fourth rows of FIGS. **8A** to **8H** and the illustrations **A-1** to **A-4**, **B-1** to **B-4**, **C-1** to **C-4**, **D-1** to **D-4**, **E-1** to **E-3**, **F-1** to **F-3**, **G-1** to **G-3**, and **H-1** to **H-3** in the first rows, which are stored in the orientation table in the memory **51**.

[0092] Next, in step **ST108** in FIG. **5**, the CPU **100** stores the measurement number, measurement time, measured blood pressure values (systolic blood pressure **SBP** and diastolic blood pressure **DBP**), pulse, whether or not there is external compression on the cuff **20**, whether or not there is bodily movement of the measurement subject **90**, and the orientation of the measurement subject **90**, in association with each other in the memory **51**.

[0093] Here, the data stored in the memory **51** is accumulated for each measurement of the blood pressure, as shown in the following data table (Table 1) for example. In this example, the night-time blood pressure measurement is performed every 30 seconds.

measured blood pressure values according to the obtained orientation of the measurement subject **90**.

[0096] As is known, the measured blood pressure values are shifted from the actual values (values in the case where the heart and the measurement site are at the same height level) according to an altitude difference between the heart and the measurement site (in this example, the left upper arm **90a**) of the measurement subject **90**. In view of this, a correction amount that is thought to be suitable due to experience is set in advance according to the obtained orientation of the measurement subject **90**, as shown in the “correction amount” column in “correction according to altitude difference” of the data table (Table 1). For example, with the orientation “**A-1**”, the heart and the left upper arm **90a** of the measurement subject **90** are at the same height level, and therefore the correction amount is set to 0 [mmHg]. With the orientation “**C-2**”, the left upper arm **90a** is at a higher level than the heart of the measurement subject

TABLE 1

Data table										
Measurement number	Measurement time	Systolic blood pressure SBP [mmHg]	Diastolic blood pressure DBP [mmHg]	Pulse [BPM]	External compression	Bodily movement	Orientation	Correction according to altitude difference		
								Correction amount [mmHg]	Systolic blood pressure SBP' [mmHg]	Diastolic blood pressure DBP' [mmHg]
0	23:00	125	93	64	0	0	K-1	0	125	93
1	23:30	117	81	55	0	0	A-1	0	117	81
2	0:00	111	77	55	0	0	A-1	0	111	77
3	0:30	107	71	62	0	0	C-2	16	123	87
4	1:00	99	71	55	0	1	C-2	16	115	87
5	1:30	103	65	57	0	0	B-2	8	111	73
6	2:00	105	69	54	0	0	B-2	8	113	77
7	2:30	111	68	62	1	0	G-2	0	111	68
8	3:00	131	85	55	0	1	A-1	0	131	85
9	3:30	105	71	47	0	0	A-3	10	115	81
10	4:00	119	81	55	0	0	A-1	0	119	81
11	4:30	119	81	50	0	0	B-2	8	127	89
12	5:00	118	82	54	0	0	C-2	16	134	98
13	5:30	114	79	55	0	0	C-2	16	130	95
14	6:00	121	83	53	0	0	B-2	8	129	91
...

[0094] Here, in the “external compression” column, “1” indicates that there is external compression and “0” indicates that there is no external compression. In the “bodily movement” column, “1” indicates that there is bodily movement and “0” indicates that there is no bodily movement. In the “orientation” column, the orientation of the measurement subject **90** is indicated by the reference sign specifying an illustration in a first row (top row) of FIGS. **8A** to **8H**. Note that the reference sign “**K-1**” in the “orientation” column indicates an orientation (e.g., an orientation corresponding to the first illustration **K-1** in later-described FIG. **15**) in which the measurement subject **90** is in a sitting position and the left upper arm **90a** serving as the measurement site naturally hangs downward. Although not shown in the third and fourth rows of FIGS. **8A** to **8H**, the orientation **K-1** is detected as the point at which $X=0$ and $Z=0$ in the XZ coordinate plane and is detected as the point at which $X=0$ and $Y=1$ in the XY coordinate plane. The “correction using altitude difference” column will be described later.

[0095] Next, in step **ST109** in FIG. **5**, the CPU **100** functions as a blood pressure correction unit and corrects the

90, and therefore the correction amount is set to 16 [mmHg]. Also, with the orientation “**B-2**”, the altitude difference between the heart and the left upper arm **90a** of the measurement subject **90** is at a level between that of the orientation “**A-1**” and that of the orientation “**C-2**”, and therefore the correction amount is set to 8 [mmHg].

[0097] Then, the CPU **100** adds the pre-set correction amount to the measured blood pressure value according to the obtained orientation of the measurement subject **90**. For example, if the obtained orientation is “**C-2**”, 16 [mmHg] is added as the correction amount when the measurement blood pressure values are systolic blood pressure $SBP=107$ [mmHg] and diastolic blood pressure $DBP=71$ [mmHg], for example. As a result, the corrected blood pressure values are systolic blood pressure $SBP'=123$ [mmHg] and diastolic blood pressure $DBP'=87$ [mmHg]. Also, if the obtained orientation is “**B-2**”, 8 [mmHg] is added as the correction amount when the measurement blood pressure values are systolic blood pressure $SBP=103$ [mmHg] and diastolic blood pressure $DBP=65$ [mmHg], for example. As a result, the corrected blood pressure values are systolic blood pres-

sure SBPⁱ=111 [mmHg] and diastolic blood pressure DBPⁱ=73 [mmHg]. Note that if the obtained orientation is “A-1”, the correction amount is 0 [mmHg], and therefore values that are the same as those of the systolic blood pressure SBP and the diastolic blood pressure DBP go in the “systolic blood pressure SBP” and “diastolic blood pressure DBP” columns of the data table (Table 1).

[0098] In this example, the CPU 100 additionally stores the correction amount corresponding to the orientation and the corrected blood pressure values (systolic blood pressure SBPⁱ and diastolic blood pressure DBPⁱ) in the data table (Table 1) in the memory 51 in association with the measurement number, the measurement time, the measured blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP), the pulse, whether or not there is external compression on the cuff 20, whether or not there is bodily movement of the measurement subject 90, and the orientation of the measurement subject 90.

[0099] Next, in step ST110 in FIG. 5, the CPU 100 refers to the data table (Table 1) in the memory 51, functions as a notification unit, and displays the blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) measured in this instance of measurement, the pulse, whether or not there is external compression on the cuff 20, whether or not there is bodily movement of the measurement subject 90, and the orientation of the measurement subject 90 on the display screen of the display device 50.

[0100] Finally, in step ST111 in FIG. 5, the CPU 100 performs control for opening the valve 33 via the valve driving circuit 330 and discharging the air in the fluid bladder 22 of the cuff 20.

[0101] Note that in the flow shown in FIG. 5, the acquisition of the cuff compliance data, the acquisition of the output of the acceleration sensor, the acquisition of the pulse wave signal, and the calculation of the blood pressure values are performed in the process of increasing the pressure of the cuff 20, but there is no limitation to this. The acquisition of the output of the acceleration sensor, the acquisition of the pulse wave signal, and the calculation of the blood pressure values may be performed in the pressure decrease process.

Example of Display in Blood Pressure Monitor Main Body

[0102] As shown in FIGS. 9A, 9B, 10A, and 10B, a “systolic blood pressure” region 50a for displaying the measured systolic blood pressure SBP as a numerical value, a “diastolic blood pressure” region 50b for displaying the measured diastolic blood pressure DBP as a numerical value, a “pulse” region 50c for displaying the pulse as a numerical value, a “bodily movement” region 50d for displaying whether or not there is bodily movement of the measurement subject as an illustration as bodily movement information, a “compression” region 50e for displaying whether or not there is external compression on the cuff 20 as an illustration as compression information, and an orientation region 50f for displaying the orientation of the measurement subject 90 as an illustration are set on the display screen of the display device 50. An illustration J-1 indicating that there is bodily movement is composed of a circle m1 indicating the head of the measurement subject 90, a rounded-corner rectangle (a rectangle with rounded corners) m2 indicating the torso of the measurement subject 90, and a waveform mark m3 indicating motion of the body. Also, the illustration J-2 indicating that there is external compression is obtained approximately by adding a waveform mark

m4 indicating the bed surface to the illustration G-2. The illustrations J-1 and J-2 are stored in advance in the memory 51. Note that when there is no bodily movement, the “bodily movement” region 50d is blank (empty) and when there is no external compression, the “compression” region 50e is blank (empty). The illustration corresponding to the content (reference numeral specifying the illustration) of the “orientation” column of the data table (Table 1) is selected from among the multiple illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3 in the first rows (top rows) in FIGS. 8A to 8H, and is displayed in the orientation region 50f. Accordingly, the image data including the illustration indicating the orientation of the measurement subject 90 can be rapidly created with simple processing.

[0103] In the example shown in FIG. 9A, a systolic blood pressure SBP of 115 mmHg, a diastolic blood pressure DBP of 87 mmHg, and a pulse of 70 BPM that were measured in this instance of measuring are displayed as numerical values in the “systolic blood pressure” region 50a, the “diastolic blood pressure” region 50b, and the “pulse” region 50c. Also, the fact that there is bodily movement is displayed as an illustration J-1 in the “bodily movement” region 50d. The fact that there is external compression is displayed as an illustration J-2 in the “compression” region 50e. Furthermore, the orientation of the measurement subject 90 is displayed as the illustration G-2 in the orientation region 50f.

[0104] In the example shown in FIG. 9B, a systolic blood pressure SBP of 117 mmHg, a diastolic blood pressure DBP of 81 mmHg, and a pulse of 70 BPM that were measured in the current instance of measurement are displayed as numerical values in the “systolic blood pressure” region 50a, the “diastolic blood pressure” region 50b, and the “pulse” region 50c, similarly to the example above. Also, the fact that there is no bodily movement is displayed as a blank in the “bodily movement” region 50d. The fact that there is no external compression is displayed as a blank in the “compression” region 50e. Furthermore, the orientation of the measurement subject 90 is displayed as an illustration A-1 in the orientation region 50f.

[0105] In the example shown in FIG. 10A, similarly to the example above, a systolic blood pressure SBP of 111 mmHg, a diastolic blood pressure DBP of 68 mmHg, and a pulse of 70 BPM that were measured in the current instance of measurement are displayed as numerical values in the “systolic blood pressure” region 50a, the “diastolic blood pressure” region 50b, and the “pulse” region 50c. Also, the fact that there is no bodily movement is displayed as a blank in the “bodily movement” region 50d. The fact that there is external compression is displayed as the illustration J-2 in the “compression” region 50e. Furthermore, the orientation of the measurement subject 90 is displayed as the illustration G-2 in the orientation region 50f.

[0106] In the example shown in FIG. 10B, similarly to the example above, a systolic blood pressure SBP of 131 mmHg, a diastolic blood pressure DBP of 85 mmHg, and a pulse of 70 BPM that were measured in the current instance of measurement are displayed as numerical values in the “systolic blood pressure” region 50a, the “diastolic blood pressure” region 50b, and the “pulse” region 50c. Also, the fact that there is bodily movement is displayed as the illustration J-1 in the “bodily movement” region 50d. The fact that there is no external compression is displayed as a blank in the “compression” region 50e. Furthermore, the

orientation of the measurement subject **90** is displayed as the illustration A-1 in the orientation region **50f**.

[0107] Accordingly, the user can find out the blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) and the value of the pulse that were measured in this instant of measurement by viewing the numerical values in the “systolic blood pressure” region **50a**, the “diastolic blood pressure” region **50b**, and the “pulse” region **50c** on the display screen of the display device **50**. In addition to this, by viewing the illustrations in the “bodily movement” region **50d**, the “compression” region **50e**, and the orientation region **50f**, the user can intuitively understand whether or not there is bodily movement of the measurement subject **90**, whether or not there is external compression on the cuff **20**, and the orientation of the measurement subject **90** during blood pressure measurement.

[0108] Note that in the pressure increase process shown in FIG. 5, if the cuff pressure reaches the upper limit value while the blood pressure values cannot be calculated (YES in step ST106), the fact that an error occurred is stored in the memory **51** in association with the measurement time (step ST112). In this example, “Error” is stored in the columns for the measured blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) in the data table (Table 1) in the memory **51**. Even if this error is present, it is desirable to store the detection results in the “external compression” column, the “bodily movement” column, and the “orientation” column of the data table (Table 1), if possible. The reason for this is that there is a possibility that the cause of the error is due to the external compression, bodily movement, or orientation. Also, in step ST110 in FIG. 5, “Error” is displayed as character strings in the “systolic blood pressure” region **50a** and the “diastolic blood pressure” region **50b** on the display screen of the display device **50** in this example, and illustrations indicating the detection results are displayed in the “bodily movement” region **50d**, the “compression” region **50e**, and the orientation region **50f**. In this type of case, the user can infer the cause of the error by viewing the illustrations in the “bodily movement” region **50d**, the “compression” region **50e**, and the orientation region **50f**.

Specific Method of Detecting External Compression

[0109] FIG. 14A shows change in a compliance ratio accompanying change in the cuff pressure during blood pressure measurement (pressure increase process) in the case where there is no external compression on the cuff **20**. On the other hand, FIG. 14B shows change in a cuff compliance ratio accompanying change in the cuff pressure during blood pressure measurement (pressure increase process) in the case where there is external compression on the cuff **20** (here, a case in which the cuff **20** is placed under the torso of the measurement subject **90**). Here, “compliance ratio” means the ratio between the cuff compliance calculated during blood pressure measurement and the cuff compliance (referred to as “reference cuff compliance”) measured once as a reference in a state in which there is no external compression on the cuff **20**. In other words, (compliance ratio)=(cuff compliance measured during blood pressure measurement)/(reference cuff compliance). Thus, the compliance ratio is used to more accurately determine whether or not there is external compression on the cuff **20**. In FIGS. 14A and 14B, the data of the compliance ratio

during multiple instances of blood pressure measurement is denoted by respective signs at the locations of cuff pressures 10 mmHg, 30 mmHg, 50 mmHg, 70 mmHg, 90 mmHg, 110 mmHg, 130 mmHg, 150 mmHg, Also, the average values of the data of the multiple instances are denoted as a line graph CLR.

[0110] As can be understood from FIG. 14A, if there is no external compression on the cuff **20**, the compliance ratio is approximately constant (except for the location of the cuff pressure 10 mmHg in the low pressure region). On the other hand, as can be understood from FIG. 14B, if there is external compression on the cuff **20**, the compliance ratio (graph CLR) has a maximum value in the intermediate pressure region (40 mmHg or more and 120 mmHg or less) in the pressure increase process. Also, as can be understood from FIGS. 14A and 14B, in both the case where there is no external compression on the cuff **20** and the case where there is external compression, there is significant variation in the compliance ratio in the low pressure region (0 mmHg to less than 40 mmHg). This is thought to be because the volume of the cuff **20** tends to not increase in some cases due not only to external compression but also to variation in the tensile force of wrapping the cuff **20** around the measurement site.

[0111] In view of this, in this example, taking these circumstances into consideration, it is determined that there is external compression on the cuff **20** only if, in the pressure increase process, the compliance ratio (CLR) is less than a first threshold REF1 (in this example, 0.7) in the low pressure region (0 mmHg to less than 40 mmHg) and the compliance ratio CLR is greater than or equal to a second threshold REF2 (in this example, 1.3) in the intermediate pressure region (40 mmHg or more and 120 mmHg or less). It is determined that there is no external compression in other cases, that is, if, in the pressure increase process, the compliance ratio CLR is greater than or equal to the first threshold REF1 (=0.7) in the low pressure region (0 mmHg to less than 40 mmHg), or the compliance ratio CLR is less than the second threshold REF2 (=1.3) in the intermediate pressure region (40 mmHg or more and 120 mmHg or less). Since REF1<REF2, this determination condition matches the condition of whether or not the compliance ratio has a maximum value in the intermediate pressure region (40 mmHg or more and 120 mmHg or less).

[0112] In order to determine whether or not there is external compression based on this determination condition, the CPU **100** functions as an external compression detection unit and executes the operation flow shown in FIGS. 11 to 13.

[0113] FIG. 11 shows portions of the overall operation flow (portions related to detection of external compression) in FIG. 5. That is, if blood pressure measurement is in progress (YES in step ST201 of FIG. 11), the cuff pressure is acquired and the current cuff pressure is set as pc[i] (step ST202). Here, i is an index indicating the number of instances of processing, and in the first instance, i=0. Next, calculation for a pump driving signal (duty) is performed, and the current pump driving voltage is set as duty[i] (step ST203). Next, cuff compliance calculation processing (FIG. 12) for obtaining a cuff compliance is performed (step ST204).

[0114] As shown in FIG. 12, in the cuff compliance calculation processing, if it is the first instance of processing after the start of blood pressure measurement (the start of pressure increase) (YES in step ST301 of FIG. 12), an

integration variable $duty_sum$ for indicating an integration value (integration value) of the pump driving voltage is cleared (set to $duty_sum=0$) (step ST302). Next, the current pump driving voltage $duty[i]$ is added to the integration variable $duty_sum$ (step ST303). If the current cuff pressure $pc[i]$ has not reached a predetermined value (10 mmHg at first) (NO in step ST304), the processing returns to the flow of FIG. 11 (NO in step ST205). Also, the index i indicating the number of instances of processing is incremented (increased by one) in step ST206 of FIG. 11, and the processing of steps ST202 and ST203 and steps ST301 to ST303 in FIG. 12 is repeated. When the current cuff pressure pc reaches 10 mmHg in step ST304 (when $pc[i] \geq 10$ mmHg and $pc[i-1] < 10$ mmHg), the cuff compliance at the cuff pressure 10 mmHg is obtained as $Comp(0)=duty_sum/10$ mmHg (step ST305). Then, the addition variable $duty_sum$ is cleared, and the processing returns to the flow of FIG. 11 (NO in step ST205). Then, the index i indicating the number of instances of processing is incremented in step ST206 of FIG. 11, and the processing of steps ST202 and ST203 and steps ST301 to ST303 of FIG. 12 is repeated. Then, when the current cuff pressure $pc[i]$ reaches 30 mmHg in step ST304 (when $pc[i] \geq 30$ mmHg and $pc[i-1] < 30$ mmHg), the cuff compliance at the cuff pressure 30 mmHg is obtained as $Comp(1)=duty_sum/20$ mmHg (step ST306). The processing is sequentially repeated in this manner, and when the current cuff pressure pc reaches 50 mmHg in step ST304 (when $pc[i] \geq 50$ mmHg and $pc[i-1] < 50$ mmHg), the cuff compliance at the cuff pressure 50 mmHg is obtained as $Comp(2)=duty_sum/20$ mmHg (step ST307). Also, when the current cuff pressure pc reaches 70 mmHg in step ST304 (when $pc[i] \geq 70$ mmHg and $pc[i-1] < 70$ mmHg), the cuff compliance at the cuff pressure 70 mmHg is obtained as $Comp(3)=duty_sum/20$ mmHg (step ST308). Also, when the current cuff pressure $pc[i]$ reaches 90 mmHg in step ST304 (when $pc[i] \geq 90$ mmHg and $pc[i-1] < 90$ mmHg), the cuff compliance at the cuff pressure 90 mmHg is obtained as $Comp(4)=duty_sum/20$ mmHg (step ST309). Also, when the current cuff pressure $pc[i]$ reaches 110 mmHg in step ST304 (when $pc[i] \geq 110$ mmHg and $pc[i-1] < 110$ mmHg), the cuff compliance at the cuff pressure 110 mmHg is obtained as $Comp(5)=duty_sum/20$ mmHg (step ST310). Then, the addition variable $duty_sum$ is cleared and the processing returns to the flow of FIG. 11.

[0115] If it is determined that the blood pressure measurement has ended in step ST205 of FIG. 11 (corresponds to step ST105 of FIG. 5) (YES in step ST205), external compression existence detection processing (FIG. 13) for determining whether or not there is external compression on the cuff 20 is performed (step ST207).

[0116] As shown in FIG. 13, in the external compression existence detection processing, an equation is used to determine whether or not the above-described determination condition has been satisfied. Note that for this determination, the CPU 100 functions in advance as a reference data acquisition unit, and in a state in which the cuff 20 is worn on a left upper arm 90a and there is no external compression, the CPU 100 increases the pressure in the cuff 20 and calculates the reference cuff compliance (reference signal COMP_STD) that is to serve as a reference at the times of the cuff pressures 10 mmHg, 30 mmHg, 50 mmHg, 70 mmHg, 90 mmHg, and 110 mmHg.

[0117] Also, it is determined that there is external pressure only in the case where, regarding the low pressure region (0 mmHg to less than 40 mmHg),

$$Comp(0)/COMP_STD < 0.7 \quad (Eq.0)$$

or

$$Comp(1)/COMP_STD < 0.7 \quad (Eq.1)$$

is established (YES in step S401) and, regarding the intermediate pressure region (40 mmHg or more and 120 mmHg or less),

$$Comp(2)/COMP_STD \geq 1.3 \quad (Eq.2)$$

or

$$Comp(3)/COMP_STD \geq 1.3 \quad (Eq.3)$$

or

$$Comp(4)/COMP_STD \geq 1.3 \quad (Eq.4)$$

or

$$Comp(5)/COMP_STD \geq 1.3 \quad (Eq.5)$$

is established (YES in step ST402). In this case, in step ST403, a compression flag indicating that there was external compression is set. Note that although COMP_STDs in Eq. 0 to Eq. 5 are indicated by the same reference signs for the sake of simplicity, they respectively indicate the reference cuff compliances at the times of the cuff pressures 10 mmHg, 30 mmHg, 50 mmHg, 70 mmHg, 90 mmHg, and 110 mmHg (the same applies also to Eq. 6 to Eq. 11, which will be described next).

[0118] On the other hand, it is determined that there is no external compression in the case where, regarding the low pressure region (0 mmHg to less than 40 mmHg),

$$Comp(0)/COMP_STD \geq 0.7 \quad (Eq.6)$$

or

$$Comp(1)/COMP_STD \geq 0.7 \quad (Eq.7)$$

is established (NO in step ST401), or, regarding the intermediate pressure region (40 mmHg or more and 120 mmHg or less),

$$Comp(2)/COMP_STD < 1.3 \quad (Eq.8)$$

or

$$Comp(3)/COMP_STD < 1.3 \quad (Eq.9)$$

or

$$Comp(4)/COMP_STD < 1.3 \quad (Eq.10)$$

or

$$Comp(5)/COMP_STD < 1.3 \quad (Eq.11)$$

is established (NO in step ST402). In this case, in step ST404, a no compression flag indicating that there was no external compression is set.

[0119] When the compression flag is set in step ST403, "1", which indicates that there is external compression in the current instance of blood pressure measurement, is stored in the "external compression" column of the above-described

data table (Table 1). On the other hand, when the no compression flag is set in step ST404, “0”, which indicates that there is no external compression in the current instance of blood pressure measurement, is stored in the “external compression” column of the data table (Table 1).

[0120] Thereafter, the processing returns to the flow of FIG. 11, and if there is external compression (YES in step ST208), compression information (e.g., the illustration J-2 shown in FIGS. 9A and 10B) indicating that there was external compression in the present instance of blood pressure measurement is displayed in step ST209 (corresponds to step ST110 of FIG. 5).

[0121] If it is determined whether or not there is external compression based on the above-described determination conditions in this way, it is possible to more accurately determine whether or not there is external compression on the cuff 20.

Example of Display on Hospital Terminal

[0122] FIG. 3 shows a block configuration of a hospital terminal 200 that can communicate with the blood pressure monitor 1 via a network 900. The hospital terminal 200 is composed of a commercially-available personal computer, includes a main body 200M, and includes a control unit 210 composed of a CPU, a memory 220 including a RAM (Random Access Memory) and a ROM (Read Only Memory), an operation unit 230 including a keyboard and a mouse, a display device 240 composed of an LCD, and a communication unit 290 for performing communication via the network 900, all of which are mounted in the main body 200M.

[0123] FIGS. 15 to 17 illustrate images displayed on the display screen of the display device 240 based on the image data received by the hospital terminal 200 from the blood pressure monitor 1 via the communication unit 290.

[0124] For example, as shown in FIG. 15, the “measurement orientation” region 240a indicating the orientation of the measurement subject 90 during blood pressure measurement, the “bodily movement/compression” region 240b indicating whether or not there is bodily movement of the measurement subject 90 or compression, a blood pressure/pulse region 240c indicating the measured blood pressure values or the corrected blood pressure values, and a legend region 240d indicating a legend of reference signs displayed on the blood pressure/pulse region 240c are set on the display screen of the display device 240.

[0125] In the “measurement orientation” region 240a, the illustrations K-1, A-1, C-2, . . . , which correspond to the reference numerals “K-1”, “A-1”, “C-2”, . . . stored in the above-described “orientation” column of the data table (Table 1) are displayed in alignment with the passage of time (measurement time shown on the horizontal axis in the blood pressure/pulse region 240c). By viewing the illustrations of the orientations displayed in the “measurement orientation” region 240a, a doctor serving as a user can intuitively understand the orientations of the measurement subject 90 during blood pressure measurement according to the passage of time. In the example shown in FIG. 15, it can be understood intuitively that the orientation of the measurement subject 90 changes from K-1 to A-1, A-1, C-2, C-2, B-2, B-2, G-2, A-1, A-3, A-1, B-2, C-2, C-2, and B-2 in the period of measurement times 23:00 to 6:00.

[0126] In the “bodily movement/compression” region 240b, the bodily movement information that is stored in the

“bodily movement” column of the data table (Table 1) and indicates that there is bodily movement is indicated by a mark M-1 at the positions in the horizontal direction corresponding to the measurement times when there was bodily movement. In addition, the compression information that is stored in the “external compression” column of the data table (Table 1) and indicates that there is external compression is indicated by a mark M-2 at the position on the horizontal axis corresponding to the measurement time when there was external compression. The mark M-1 is constituted by the words “BOD. MVMT.” being included in a rectangle with rounded corners. The mark M-2 is constituted by the word “COMP.” being included in a rectangle with rounded corners. By viewing the marks M-1 and M-2 displayed in the “bodily movement/compression” region 240b, a doctor serving as a user can intuitively understand that there was bodily movement of the measurement subject 90 and that there was external compression on the cuff 20 at a specific blood pressure measurement time. In the example shown in FIG. 15, it can be understood intuitively that there was bodily movement during blood pressure measurement at the blood pressure measurement times 1:00 and 3:00, and that there was external compression during blood pressure measurement at the blood pressure measurement time 2:30.

[0127] In the blood pressure/pulse region 240c, the measured blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) in the data table (Table 1) and the pulse value PR stored in the “pulse” column are displayed as line graphs in this example. By viewing these line graphs, a user can intuitively understand the passage of time of the blood pressure values and the pulse of the measurement subject 90. Also, by viewing both the illustrations of the orientations displayed in the “measurement orientation” region 240a and the line graph of the blood pressure values displayed in the blood pressure/pulse region 240c, the user can intuitively understand the influence that the orientation, bodily movement, and external compression have on the blood pressure value of the measurement subject 90.

[0128] Accordingly, for example, in the case of diagnosing the health state of the measurement subject 90, a doctor serving as a user can make a diagnosis giving consideration to the influence that the orientation, bodily movement, and external compression have on the blood pressure value of the measurement subject 90. Specifically, for example, if the orientation has a large influence on the blood pressure value of the measurement subject 90, the doctor can make a diagnosis based only on the blood pressure values measured at times when the measurement subject 90 was in a specific orientation (e.g., A-1). Also, if the bodily movement or the external compression has a large influence on the blood pressure value of the measurement subject 90, it is possible to ignore the blood pressure values measured when there is bodily movement and the blood pressure values measured when there is external compression, and to make a diagnosis based only on the blood pressure values measured when there is no bodily movement and no external compression.

[0129] As shown in FIG. 16, in the blood pressure/pulse region 240c, the corrected blood pressure values (systolic blood pressure SBP' and diastolic blood pressure DBP') in the data table (Table 1) may be displayed as line graphs instead of the measured blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) in the data table (Table 1). Accordingly, by viewing both the

illustrations of the orientations displayed in the “measurement orientation” region 240a and the line graph of the corrected blood pressure values displayed in the blood pressure/pulse region 240c, a doctor serving as a user can intuitively understand whether or not the blood pressure values of the measurement subject 90 have been appropriately corrected according to the orientations of the measurement subject 90 during blood pressure measurement.

[0130] Also, as shown in FIG. 17, the corrected blood pressure values (systolic blood pressure SBPⁱ and diastolic blood pressure DBPⁱ) in the data table (Table 1) may be displayed along with the measured blood pressure values (systolic blood pressure SBP and diastolic blood pressure DBP) in the data table (Table 1) as line graphs in the blood pressure/pulse region 240c. Accordingly, by viewing the illustrations of the orientations displayed in the “measurement orientation” region 240a and the line graphs of the uncorrected and corrected blood pressure values displayed in the blood pressure/pulse region 240c, a doctor serving as a user can more intuitively understand whether or not the blood pressure values of the measurement subject 90 were corrected appropriately according to the orientation of the measurement subject 90 during blood pressure measurement.

Modified Examples

[0131] In the example above, as shown in FIGS. 8A to 8H, the orientations of the measurement subject 90 are detected as combinations of eight types of “torso angles” and four or three types of “arm positions”. Furthermore, in correspondence to this, the orientations of the measurement subject 90 are indicated using the illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3, F-1 to F-3, G-1 to G-3, and H-1 to H-3, which are obtained by combining eight types of torso patterns and four or three types of arm patterns. However, there is no limitation to this, and for example, the torso angle may be detected roughly as four types, namely 0 degrees (supine position), 90 degrees (right side position), 180 degrees (prone position), and 270 degrees (left side position), and in correspondence to this, the torso angle may be displayed as four types of torso patterns.

[0132] Also, the “arm position” of the measurement subject 90 may be at a special arm position other than the four or three types of representative “arm positions” in FIGS. 8A to 8H. In this case, it is desirable that with regard to this special arm position, the points that are to be detected in the XZ coordinate plane in the third rows in FIGS. 8A to 8H and in the XY coordinate plane in the fourth rows are defined, and the arm pattern that indicates the special arm position is prepared. For example, as shown in the “measurement orientation” region 240a, at the measurement time 3:30 shown in FIG. 17, the torso angle of the measurement subject 90 is 0 degrees (supine position). In this case, the left upper arm 90a is in an arm position of being separated frontward with respect to the torso 90b of the measurement subject 90 (being extended approximately vertically upward). In response to this, it is desirable that the points that are to be detected in the XZ coordinate plane in the third row and in the XY coordinate plane in the fourth row in FIG. 8A are defined and the arm pattern indicating this arm position (in this example, illustration A-3') is prepared.

[0133] Also, in the example above, the orientation of the measurement subject 90 is indicated using the illustrations A-1 to A-4, B-1 to B-4, C-1 to C-4, D-1 to D-4, E-1 to E-3,

F-1 to F-3, G-1 to G-3, and H-1 to H-3 in the first rows (top rows) of FIGS. 8A to 8H. However, there is no limitation to this, and the orientation of the measurement subject 90 may be indicated using illustrations of another type, for example, the illustrations in the second rows of FIGS. 8A to 8H. The illustrations in the second rows in FIGS. 8A to 8H indicate schematic views of the orientations of the measurement subject 90 from above in the vertical direction. In the illustrations shown in the second rows, the head 90h of the measurement subject 90 is indicated by an oval, the torso 90b is indicated by a half-oval, and the left upper arm 90a is indicated by a rounded-corner rectangle. With this kind of illustration as well, the user can intuitively understand the orientations of the measurement subject 90 during blood pressure measurement according to the passage of time.

[0134] Also, with the blood pressure monitor 1, the cuff 20 and the main body 10 are constituted integrally, but there is no limitation to this. Instead, the cuff 20 and the main body 10 may be constituted separately, and may be connected via an elongated tube corresponding to the air tube 39. In this case, the acceleration sensor 34 is preferably mounted in (built in) the cuff 20 so as to be able to detect the orientation of the measurement subject 90.

[0135] As is described above, the electronic blood pressure monitor of this disclosure includes:

[0136] a blood pressure measurement cuff configured to be worn on a measurement site of a measurement subject;

[0137] a blood pressure measurement unit configured to measure a blood pressure value of the measurement subject using the cuff; and

[0138] an external compression detection unit configured to detect whether or not there was external compression on the cuff during the blood pressure measurement performed by the blood pressure measurement unit,

[0139] wherein in each predetermined pressure segment, the external compression detection unit calculates a cuff compliance, which is an amount of air that is to be pumped into the cuff and is needed to increase pressure in the cuff per unit pressure, as the pressure of the cuff is increased by the blood pressure measurement unit during blood pressure measurement, and

[0140] the external compression detection unit determines whether or not there is external compression on the cuff based on a change indicated by the cuff compliance in each pressure segment.

[0141] In the present specification, “during blood pressure measurement” does not indicate the entire period in which the blood pressure measurement cuff is worn for night-time blood pressure measurement and the like, for example, but indicates a timing during which the blood pressure values of the measurement subject are measured by actually increasing or reducing the pressure of the above-described blood pressure measurement cuff.

[0142] Also, “external compression” indicates compression from the outside of the external circumferential surface of the blood pressure monitor that is wrapped around the measurement site. In other words, “external compression” does not encompass compression from the measurement site (inner circumferential surface side of the cuff) around which the blood pressure measurement cuff is wrapped. Typically, external compression occurs when the measurement subject lying on the bed surface places the cuff worn on the measurement site under the torso in the case of night-time blood pressure measurement. Note that “bed surface” widely

indicates a surface on which a measurement subject can lie, such as an upper surface of a bed or futon. The torso of the measurement subject may be wearing clothes.

[0143] With the electronic blood pressure monitor of the present disclosure, in a state in which the cuff is worn on the measurement site of the measurement subject, a fluid is supplied to the cuff to increase the pressure, and thereby the measurement site is compressed, and the blood pressure measurement unit performs blood pressure measurement. According to this, the blood pressure value is obtained. Also, the external compression detection unit detects whether or not there was external compression on the cuff during the blood pressure measurement performed by the blood pressure measurement unit. Accordingly, the user can check whether or not there was external compression on the cuff during blood pressure measurement, based on the detection result. Moreover, in each predetermined pressure segment, the external compression detection unit calculates a cuff compliance, which is an amount of air that is to be pumped into the cuff and is needed to increase pressure in the cuff per unit pressure, as the pressure of the cuff is increased by the blood pressure measurement unit during blood pressure measurement, and the external compression detection unit determines whether or not there is external compression on the cuff based on a change indicated by the cuff compliance in each pressure segment. Accordingly, for example, if the cuff is wrapped tightly around the measurement site, it is possible to avoid a circumstance in which it is erroneously determined that there is external compression on the cuff due to the influence of the tension of the wrapping. Accordingly, it is possible to more accurately determine whether or not there is external compression on the cuff.

[0144] With an electronic blood pressure monitor of an embodiment, the external compression detection unit determines whether or not there is external compression on the cuff according to whether or not the cuff compliance has a maximum value with respect to pressure change of the cuff in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.

[0145] In the present specification, "cuff compliance" means the amount of air that is to be pumped into the cuff, and which is needed to increase the pressure, per unit pressure of the cuff. For example, milliliters/millimeters of mercury (ml/mmHg) are used as the units.

[0146] Also, the "intermediate pressure region" (40 mmHg or more and 120 mmHg or less) is a pressure region that is set based on experiments performed by the inventor of the present invention.

[0147] In general, if there is no external compression on the cuff, the cuff compliance gradually decreases and is saturated as the fluid is supplied to the cuff and the pressure is increased from the low pressure region (0 mmHg to less than 40 mmHg) to the high pressure region (more than 120 mmHg). The reason for this is as follows: the volume of the cuff easily increases in the low pressure region, and therefore a large amount of air is needed to increase the cuff pressure, but if the tensile force of the cuff increases due to the cuff pressure increasing by a certain extent, the volume of the cuff substantially stops increasing. On the other hand, if the measurement subject lying on the bed surface places the cuff worn on the measurement site under his or her torso, the cuff is compressed from the outside (the torso and the bed surface). In this case, in the low pressure region (0 mmHg to less than 40 mmHg), the volume of the cuff

increases due to the cuff pressing back against the torso of the measurement subject. Accordingly, the cuff compliance changes gradually from a low value (varies due to the influence of the tensile force of wrapping the cuff around the measurement site) to a high value. On the other hand, in the high pressure region (more than 120 mmHg), the torso is pressed by the upper portion of the cuff due to the inflation of the cuff, and therefore, similarly to the case in which there is no external compression, the cuff compliance gradually decreases and is saturated. As a result, in the intermediate range (40 mmHg or more, 120 mmHg or less), the cuff compliance has a maximum value accompanying the increase of the cuff pressure. In view of this, with the electronic blood pressure monitor of this embodiment, the external compression detection unit determines whether or not there is external compression on the cuff according to whether or not the cuff compliance has a maximum value with respect to the pressure change of the cuff in the intermediate pressure region (40 mmHg or more and 120 mmHg or less). Accordingly, it is possible to accurately determine whether or not there is external compression on the cuff.

[0148] An electronic blood pressure monitor of an embodiment includes

[0149] a reference data acquisition unit configured to increase pressure in the cuff and calculate a reference cuff compliance that is to serve as a reference, in a state in which the cuff is worn on the measurement site and there is no external compression,

[0150] wherein the external compression detection unit detects a compliance ratio between the cuff compliance calculated during blood pressure measurement and the reference cuff compliance, and

[0151] the external compression detection unit detects whether or not there is external compression on the cuff according to whether or not the compliance ratio has a maximum value with respect to the pressure change of the cuff in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.

[0152] In the present specification, "compliance ratio" means (cuff compliance calculated during blood pressure measurement)/(reference cuff compliance).

[0153] With the electronic blood pressure monitor of this embodiment, the pressure is increased and the reference data acquisition unit calculates the reference cuff compliance that is to serve as a reference in a state in which the cuff is worn on the measurement site and there is no external compression. The external compression detection unit detects the compliance ratio between the cuff compliance calculated during blood pressure measurement and the reference cuff compliance. Furthermore, the external compression detection unit detects whether or not there is external compression on the cuff according to whether or not the compliance ratio has a maximum value in the pressure change of the cuff in the intermediate pressure region, in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less. Accordingly, it is possible to more accurately determine whether or not there is external compression on the cuff.

[0154] With an electronic blood pressure monitor of an embodiment, the external compression detection unit determines that there is external compression on the cuff only when the compliance ratio is smaller than a predetermined threshold in a low pressure region in which the pressure of the cuff is less than 40 mmHg.

[0155] In the low pressure region, in which the pressure of the cuff is less than 40 mmHg, the volume of the cuff tends to not increase in some cases due not only to external compression but also to variation in the tensile force of wrapping the cuff around the measurement site. In this case, there is a possibility that it will be erroneously determined that there is external compression on the cuff. In view of this, with the electronic blood pressure monitor of this embodiment, the external compression detection unit determines that there is external compression on the cuff only when the compliance ratio is smaller than a predetermined threshold in a low pressure region in which the pressure of the cuff is less than 40 mmHg. Accordingly, if the cuff is wrapped tightly around the measurement site, it is possible to avoid a situation in which it is erroneously determined that there is external compression on the cuff due to the influence of the tensile force of the wrapping. Accordingly, it is possible to more accurately determine whether or not there is external compression on the cuff.

[0156] An electronic blood pressure monitor of an embodiment includes a storage unit configured to store compression information indicating a result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit.

[0157] With the blood pressure monitor of this embodiment, the storage unit stores the compression information indicating the result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit. The storage content of the storage unit is read out, whereby the user can check whether or not there was external compression on the cuff during blood pressure measurement.

[0158] An electronic blood pressure monitor of an embodiment includes a notification unit configured to perform notification of compression information indicating the result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit.

[0159] With the blood pressure monitor of this embodiment, the notification unit performs notification of the compression information indicating the result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit. According to the notification content of the notification unit, the user can find out whether or not there was external compression on the cuff during blood pressure measurement. Accordingly, for example, in the case of diagnosing the health state of the measurement subject, a doctor serving as a user can make a diagnosis giving consideration to the influence that the external compression has on the blood pressure value of the measurement subject. Specifically, for example, if the external compression has a large influence on the blood pressure values of the measurement subject **90**, the blood pressure values measured when there was external compression can be ignored, and diagnosis can be performed based on only the blood pressure values measured when there was no external compression.

[0160] Also, an electronic blood pressure monitor of an embodiment includes

[0161] a reference data acquisition unit configured to increase pressure in the cuff and calculate a reference cuff

compliance that is to serve as a reference, in a state in which the cuff is worn on the measurement site and there is no external compression,

[0162] wherein the external compression detection unit detects a compliance ratio between the cuff compliance calculated during blood pressure measurement and the reference cuff compliance, and

[0163] the external compression detection unit detects whether or not there is external compression on the cuff according to whether or not the compliance ratio is smaller than a predetermined first threshold in a low pressure region in which the pressure of the cuff is less than 40 mmHg and the compliance ratio is greater than or equal to a predetermined second threshold in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.

[0164] As is clear from the foregoing description, with the electronic blood pressure monitor of the present disclosure, a user can check whether or not there was external compression on a cuff during blood pressure measurement.

[0165] The above-described embodiments are exemplary and various modifications are possible without departing from the scope of the invention. The above-described multiple embodiments can be established separately, but combinations of the embodiments are also possible. Also, the various characteristics of the different embodiments can be established separately, but combinations of the characteristics in the different embodiments are also possible.

1. An electronic blood pressure monitor, comprising:
 - a blood pressure measurement cuff configured to be worn on a measurement site of a measurement subject;
 - a blood pressure measurement unit configured to measure a blood pressure value of the measurement subject using the cuff; and
 - an external compression detection unit configured to detect whether or not there was external compression on the cuff during the blood pressure measurement performed by the blood pressure measurement unit, wherein in each predetermined pressure segment, the external compression detection unit calculates a cuff compliance, which is an amount of air that is to be pumped into the cuff and is needed to increase pressure in the cuff per unit pressure, as the pressure of the cuff is increased by the blood pressure measurement unit during blood pressure measurement, and
 - the external compression detection unit determines whether or not there is external compression on the cuff based on a change indicated by the cuff compliance in each pressure segment.
2. The electronic blood pressure monitor according to claim 1, wherein
 - the external compression detection unit determines whether or not there is external compression on the cuff according to whether or not the cuff compliance has a maximum value with respect to pressure change of the cuff in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.
3. The electronic blood pressure monitor according to claim 1, comprising
 - a reference data acquisition unit configured to increase pressure in the cuff and calculate a reference cuff compliance that is to serve as a reference, in a state in

which the cuff is worn on the measurement site and there is no external compression, wherein the external compression detection unit detects a compliance ratio between the cuff compliance calculated during blood pressure measurement and the reference cuff compliance, and the external compression detection unit detects whether or not there is external compression on the cuff according to whether or not the compliance ratio has a maximum value with respect to the pressure change of the cuff in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.

4. The electronic blood pressure monitor according to claim 3,

wherein the external compression detection unit determines that there is external compression on the cuff only when the compliance ratio is smaller than a predetermined threshold in a low pressure region in which the pressure of the cuff is less than 40 mmHg.

5. The electronic blood pressure monitor according to claim 1, comprising

a storage unit configured to store compression information indicating a result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit.

6. The electronic blood pressure monitor according to claim 1, comprising

a notification unit configured to perform notification of compression information indicating the result of detection performed by the external compression detection unit, in association with the blood pressure value measured by the blood pressure measurement unit.

7. The electronic blood pressure monitor according to claim 1, comprising

a reference data acquisition unit configured to increase pressure in the cuff and calculate a reference cuff compliance that is to serve as a reference, in a state in which the cuff is worn on the measurement site and there is no external compression,

wherein the external compression detection unit detects a compliance ratio between the cuff compliance calculated during blood pressure measurement and the reference cuff compliance, and

the external compression detection unit detects whether or not there is external compression on the cuff according to whether or not the compliance ratio is smaller than a predetermined first threshold in a low pressure region in which the pressure of the cuff is less than 40 mmHg and the compliance ratio is greater than or equal to a predetermined second threshold in an intermediate pressure region in which the pressure of the cuff is 40 mmHg or more and 120 mmHg or less.

* * * * *

专利名称(译)	电子血压计		
公开(公告)号	US20180296101A1	公开(公告)日	2018-10-18
申请号	US16/015257	申请日	2018-06-22
[标]申请(专利权)人(译)	欧姆龙健康医疗事业株式会社		
申请(专利权)人(译)	欧姆龙保健CO., LTD.		
当前申请(专利权)人(译)	欧姆龙保健CO., LTD.		
[标]发明人	KUBO TAKESHI		
发明人	KUBO, TAKESHI		
IPC分类号	A61B5/0225 A61B5/00		
CPC分类号	A61B5/0225 A61B5/7221 A61B5/4806 A61B2560/0475 A61B5/02108 A61B5/022 A61B5/1116		
优先权	2015257066 2015-12-28 JP		
外部链接	Espacenet	USPTO	

摘要(译)

本发明的电子血压计包括血压测量袖带，该血压测量袖带将佩戴在测量对象的测量部位上。电子血压计包括血压测量单元，其使用袖带测量测量对象的血压值。电子血压计包括外部压缩检测单元，其检测在由血压测量单元执行的血压测量期间袖带上是否存在外部压缩。

