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(57) **ABSTRACT**

Examples of monolithic integrated emitter-detector array in a flexible substrate for biometric sensing and associated devices and methods are disclosed. One disclosed example device includes a flexible substrate; a first array of emitters embedded in the flexible substrate, the first array of emitters configured to emit first electromagnetic (EM) signals; a first array of detectors embedded in the flexible substrate, the first array of detectors configured to detect reflections of the first EM signals; a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters of the first array of emitters; and a first sensing circuit coupled to individual detectors of the first array of detectors, the first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors.

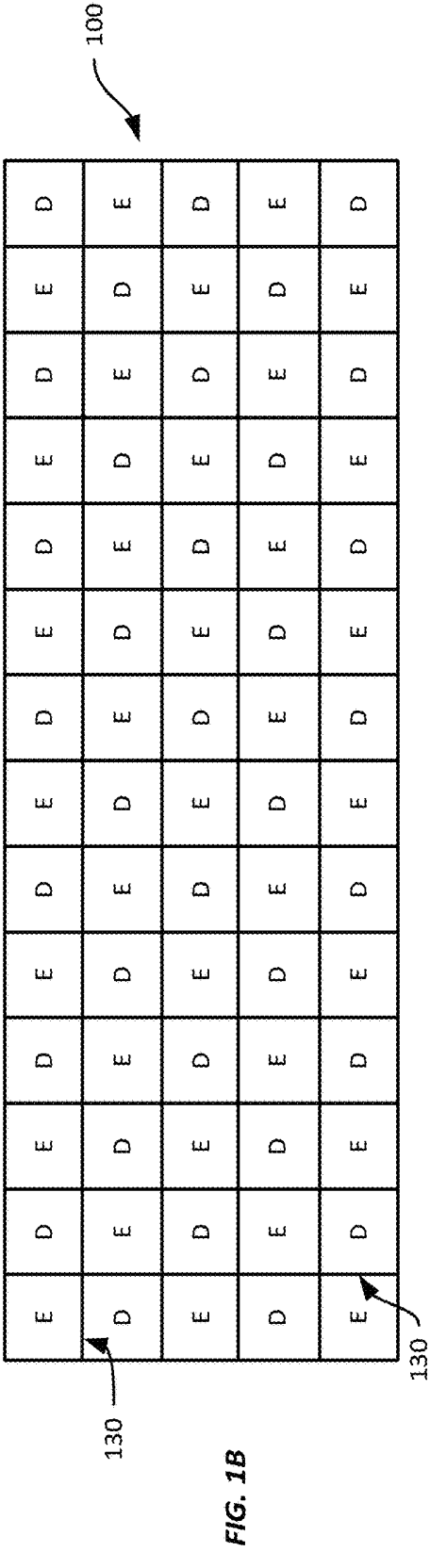
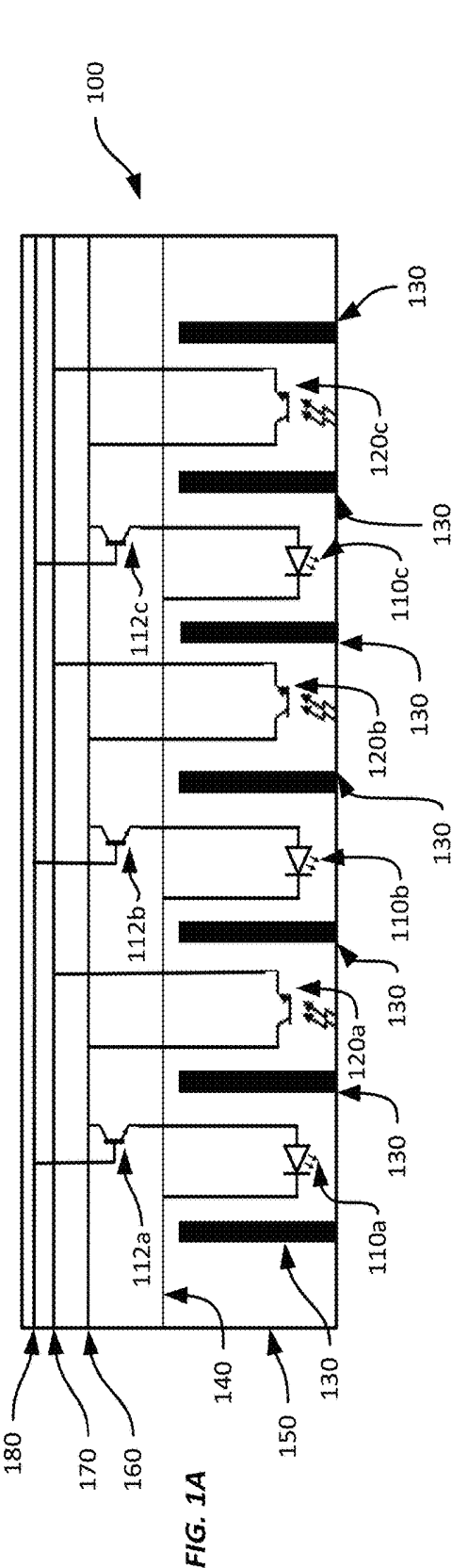
26 Claims, 5 Drawing Sheets

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 (2013.01); *A61B 5/14551* (2013.01); *A61B*
2560/0214 (2013.01); *A61B 2560/0475*
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2562/046 (2013.01); *A61B 2562/164* (2013.01)
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A61B 5/742; *A61B 5/6823*; *A61B*
5/6824; *A61B 5/7475*; *A61B 5/7278*;
A61B 5/6828

See application file for complete search history.

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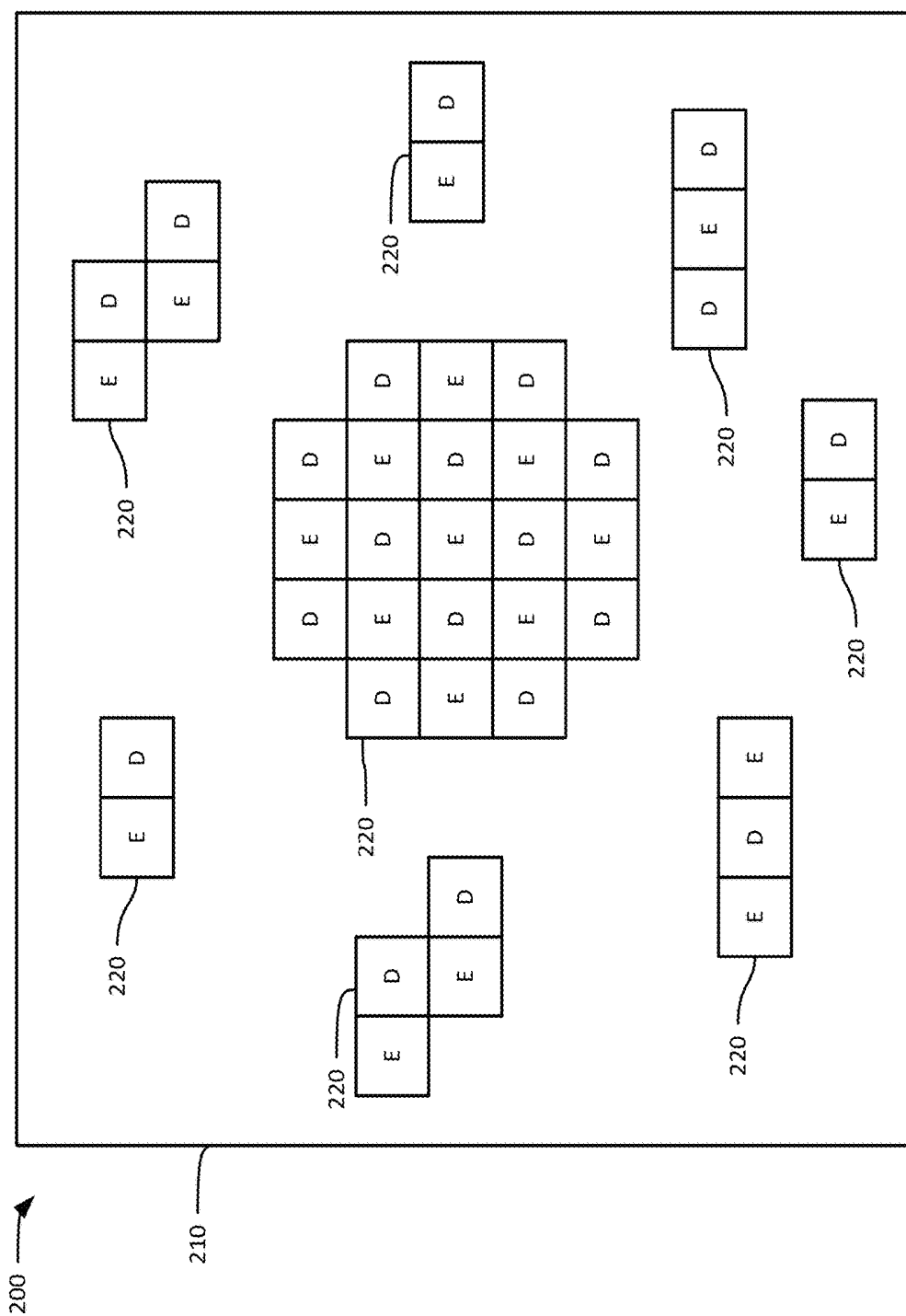


FIG. 2

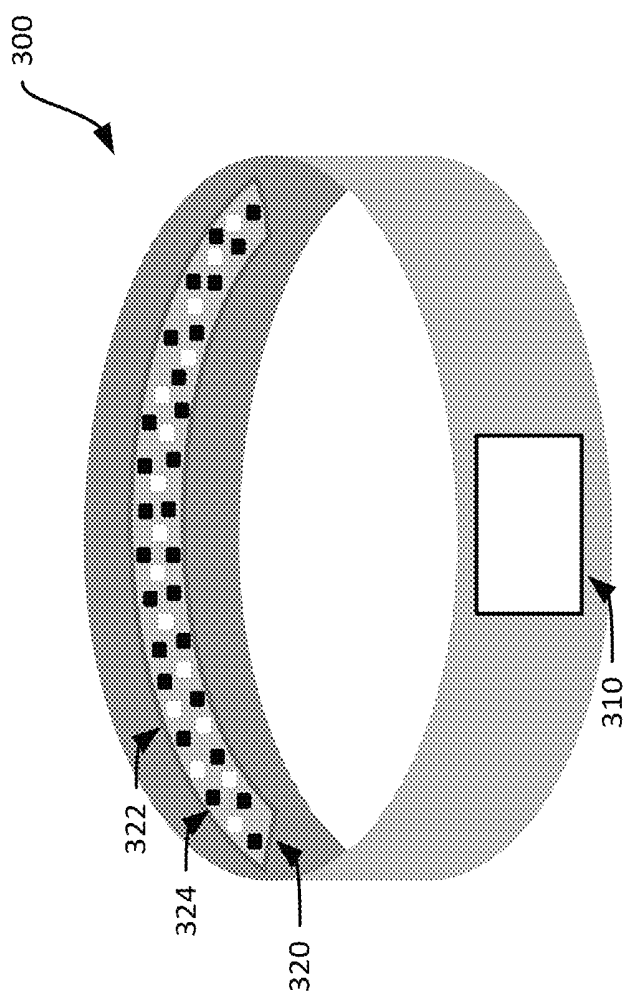
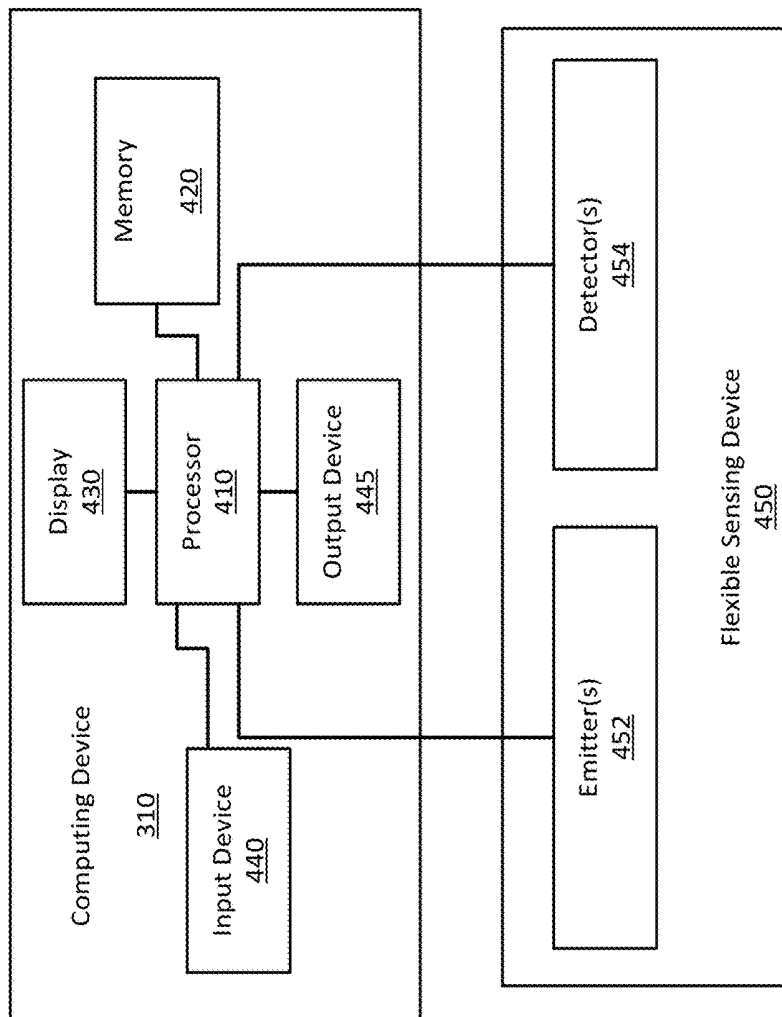


FIG. 3

**FIG. 4**

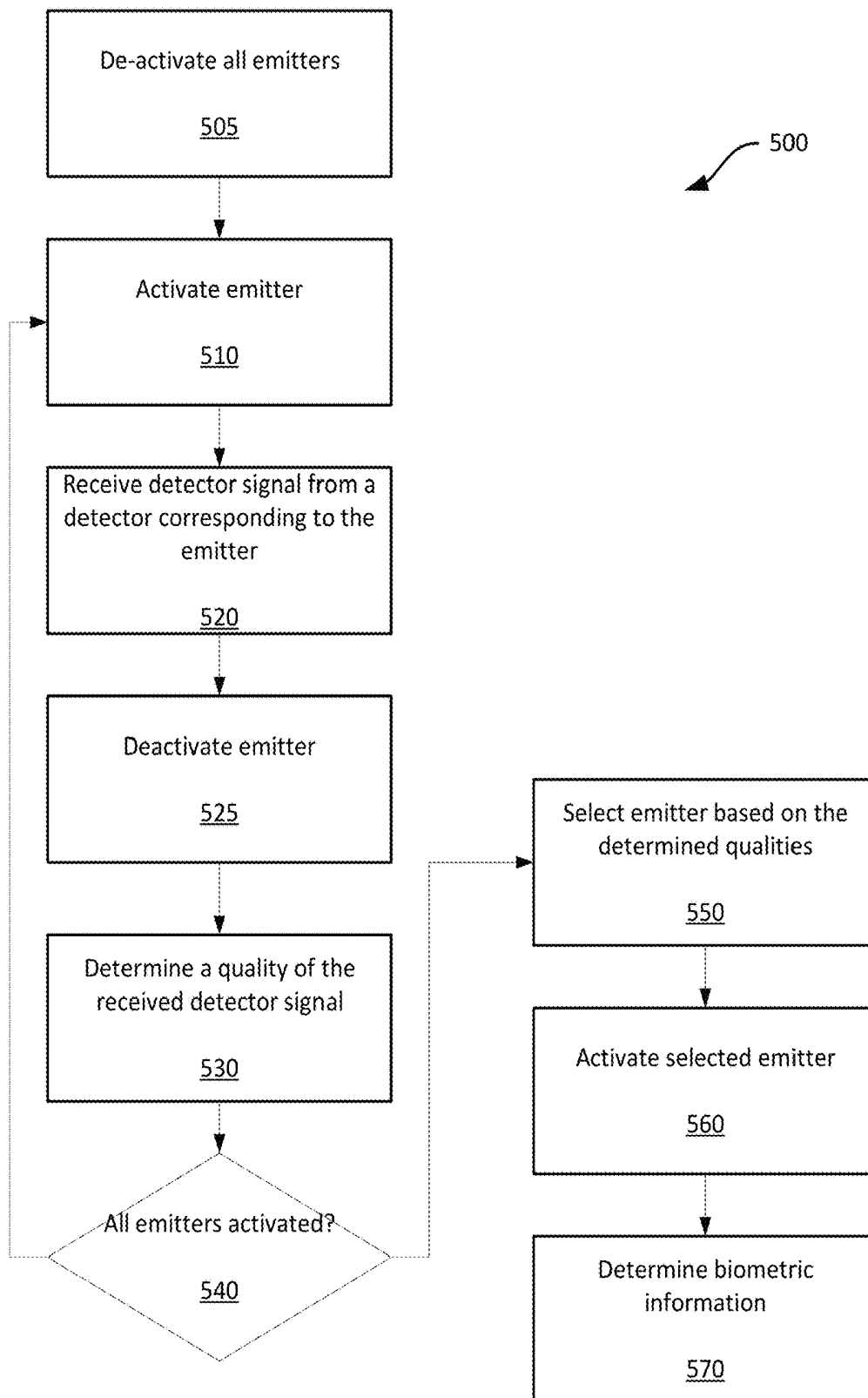


FIG. 5

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MONOLITHIC INTEGRATED EMITTER-DETECTOR ARRAY IN A FLEXIBLE SUBSTRATE FOR BIOMETRIC SENSING

BACKGROUND

It is often desirable for a user to be aware his/her bodily function measurements. Recently, many individuals wear small portable devices capable of measuring their heart rate (HR) and other physiological information. One of the techniques used by these devices to measure heart rate is photoplethysmography (PPG). Many of the small portable fitness devices are wearable electronics that are typically package in the form of a watch (e.g., smart watch), activity monitoring band (e.g., worn on the wrist), etc.

However, these devices typically have one or two light sources that illuminate light into the user's skin and one or two detectors to measure the reflected light in order to obtain the PPG measurement. In the everyday course of the user's activities, however, these wrist-worn devices are susceptible to rotation around the wrist (e.g., when a user is walking, etc.) Even a small rotation of the device around the user's wrist can cause decrease in accuracy by a factor of two. This is due to the amount of measured light because the arteries in the portion where a user typically wears a wrist-worn device are rather sparse. Thus, these wrist-worn devices may not always be able to obtain the most accurate PPG measurement due to having only a small number of light sources and detectors which may not always be located at the optimum location around the user's wrist due to rotations of the device around the user's wrist during the course of their everyday life.

BRIEF SUMMARY

Various examples are described for monolithic integrated emitter-detector array in a flexible substrate for biometric sensing. For example, one disclosed device includes a flexible substrate; a first array of emitters embedded in the flexible substrate, the first array of emitters configured to emit first electromagnetic (EM) signals; a first array of detectors embedded in the flexible substrate, the first array of detectors configured to detect reflections of the first EM signals; a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters of the first array of emitters; and a first sensing circuit coupled to individual detectors of the first array of detectors, the first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors.

In another example, one disclosed system includes a wearable housing; a processor and a non-transitory computer-readable medium disposed within the wearable housing, the processor in communication with the non-transitory computer-readable medium and configured to execute program code stored in the non-transitory computer-readable medium; a monolithic sensor in communication with the processor and configured to provide sensor signals to the processor, the sensor comprising: a flexible substrate; a first array of emitters embedded in the flexible substrate, the first array of emitters configured to emit first electromagnetic (EM) signals; a first array of detectors embedded in the flexible substrate, the first array of detectors configured to detect reflections of the first EM signals; a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters

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of the first array of emitters; and a first sensing circuit coupled to individual detectors of the first array of detectors, the first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors.

In a further example, one disclosed method includes for each emitter of an array of emitters embedded in a flexible substrate, each emitter configured to emit an electromagnetic (EM) signal: activating the emitter, receiving a detector signal from one or more detectors of an array of detectors corresponding to the activated emitter, the array of detectors embedded in the flexible substrate, and determining a quality of the received detector signal; selecting an emitter and corresponding detector having a high quality of the determined qualities; deactivating all emitters of the plurality of emitters; activating the selected emitter; and determining biometric information based at least in part on a detector signal received from the corresponding detector.

These illustrative examples are mentioned not to limit or define the scope of this disclosure, but rather to provide examples to aid understanding thereof. Illustrative examples are discussed in the Detailed Description, which provides further description. Advantages offered by various examples may be further understood by examining this specification

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings, which are incorporated into and constitute a part of this specification, illustrate one or more certain examples and, together with the description of the example, serve to explain the principles and implementations of the certain examples.

FIGS. 1A-2 show example flexible sensing devices including monolithic integrated emitter-detector arrays in a flexible substrate for biometric sensing;

FIG. 3 shows an example wearable device including flexible sensing device;

FIG. 4 shows an example computing device for biometric sensing using a flexible sensing device; and

FIG. 5 shows an example method for biometric sensing using a flexible sensing device.

DETAILED DESCRIPTION

Examples are described herein in the context of monolithic integrated emitter-detector arrays in a flexible substrate for biometric sensing. Those of ordinary skill in the art will realize that the following description is illustrative only and is not intended to be in any way limiting. Reference will now be made in detail to implementations of examples as illustrated in the accompanying drawings. The same reference indicators will be used throughout the drawings and the following description to refer to the same or like items.

In the interest of clarity, not all of the routine features of the examples described herein are shown and described. It will, of course, be appreciated that in the development of any such actual implementation, numerous implementation-specific decisions must be made in order to achieve the developer's specific goals, such as compliance with application- and business-related constraints, and that these specific goals will vary from one implementation to another and from one developer to another.

Illustrative Example of a Monolithic Integrated Emitter-Detector Array in a Flexible Substrate for Biometric Sensing

In one illustrative example, a sensor for sensing biometric information includes a flexible substrate, such a plastic

substrate. Such a substrate allows the sensor to wrap around, or otherwise conform, to a portion of a person's body, such as a wrist or arm. Embedded within the substrate are a number of emitters that emit light in one or more wavelengths. In addition, a number of detectors are also embedded within the substrate to detect light reflected off of the portion of the person's body.

In this example, the sensor is a part of a wearable device to be worn around a user's wrist. The emitters are embedded within the flexible substrate in a rectangular array to allow illumination of a large portion of the user's wrist. The detectors are also embedded within the flexible substrate in a rectangular array that corresponds with the array of emitters. Thus, when the emitters emit light, the light will reflect off of the user's wrist and be detected by one or more of the detectors.

The arrays of emitters and detectors are connected to a processor within the wearable device. The processor is able to selectively activate the emitters, individually or in groups, and then receive information from the detectors. However, because the wrist has a sparse layout of blood vessels near the surface of the skin, some of the emitters will not illuminate any blood vessels, or will only poorly illuminate a nearby blood vessel, and corresponding detectors will not detect useful biometric information. Thus, the processor attempts to optimize the use of the emitters and detectors to identify the emitters that result in the best quality detector readings, and discontinue activating the other emitters. To do so, the processor selectively activates emitters one at a time and obtains signals from one or more detectors. The processor evaluates each detector signal to determine whether the signal provides useful biometric information or not, and identifies the emitters that, when activated, resulted in the best biometric information. The processor then adjusts its configuration to use the identified emitters to obtain biometric information and to deactivate the other emitters. Over time, the processor may continue to evaluate the received biometric information and may re-optimize emitter selection over time. For example, if the wearable device moves on the user's wrist, different emitters may result in better biometric information. Thus, the processor may periodically re-optimize its emitter usage, or may do so when the quality of the detected biometric information drops below a threshold. Further, by deactivating one or more emitters, the wearable device may reduce its power consumption, thereby increasing its battery life.

This illustrative example is not intended to be in any way limiting, but instead is intended to provide an introduction to the subject matter of the present application. For example, the illustrative example above is described with respect to an autonomous car; however, the present application is not limited to such an environment, but may be used in any suitable environment. Other examples of monolithic integrated emitter-detector arrays in a flexible substrate for biometric sensing are described below.

Referring now to FIG. 1A, FIG. 1A shows a cross-section of an example monolithic integrated emitter-detector array in a flexible substrate for biometric sensing. In this example, the sensing device **100** has a flexible substrate **150** in which are embedded several emitters **110a-c** and several detectors **120a-c**, which are separated by optical shielding **130**. Each emitter **110a-c** is connected to a power source by a switch **112a-c**, which allows each emitter **110a-c** to be independently activated of the other emitters. In this example, a processor is connected to each switch **112a-c** and toggles a switch to activate the corresponding emitter(s). For example, each switch may be connected to the processor via a switch

matrix circuit to enable individual addressing of each switch. In some examples, pins on the processor may each be connected to a corresponding switch via an individual wire thus allowing one pin on the processor to change the state of the corresponding switch.

In different examples, the flexible substrate **150** may be a polymer material, such as a fluoropolymer/polyimide copolymer, an acrylic-based material, a polyester material, a polyimide material, a polyethylene naphthalate material, a polyetherimide material, a fluoropolymer, or a copolymer comprising two or more of the foregoing materials. In some examples, the substrate may have a single layer or may have more than one layers. Multiple layers of substrates of the same or different types may be bonded using suitable adhesives. In some examples, the flexible substrate **150** may have a thickness between approximately 12 to 127 microns (± 5 microns).

In this example, the switches **112a-c** comprise a transistor coupling a power source, provided by wire **160**, to a respective emitter **110a**, which, in this example, are each also coupled to an electrical ground **140**. The transistors are configured to operate in a saturation mode to gate power on or off to the respective emitter. For example, a signal may be provided to the switch via a scanning circuit **180**, which as described above may comprise a switch matrix or a discrete wire running from a processor to the switch. However, in some examples, the switches **112a-c** may allow for different settings to affect an intensity or type of signal emitted by the corresponding emitter **110a-c**. Further, while in this example each switch **112a-c** is coupled to only one emitter, in some examples, a switch **112a-c** may be coupled to and configured to activate/deactivate multiple emitters.

In this example, the emitters **110a-c** are light emitting diodes (LEDs) that emit red light in the visible spectrum when activated. However, other color LEDs may be employed, such as orange or green. For example, an orange LED may be advantageous for sensing biometric information on people having darker skin, while red LEDs may be more advantageous for sensing biometric information on people having lighter skin. In some examples, the emitters **100a-c** may emit electromagnetic (EM) signals in wavelengths outside the visible spectrum; however, for purposes of this description EM signals include visible light and infrared radiation. For example, the following table illustrates wavelengths, in nanometers (nm), of EM radiation that correspond to different colors of light and infrared radiation:

Color	Wavelength
Infrared	751-1,000,000 nm
Red	620-750 nm
Orange	591-620 nm
Yellow	571-590 nm
Green	496-560 nm
Blue	451-495 nm
Violet	380-450 nm

It should be understood, however, the ranges given above are not intended to be exact for all examples. For example, each color range may extend ± 10 nm or $\pm 2\%$ beyond what is recited in the table above.

In some examples, different types of emitters **110a-c** may be employed. For example, a first set of emitters may be configured to output red light, a second set of emitters may be configured to output orange light, and a third set of emitters may be configured to output green light. In one such example, each set of emitters may have a separate scanning

circuit, which may allow a processor to separately and independently activate or deactivate emitters of one kind or another. However, in some examples, all three sets of emitters may be coupled to the same scanning circuit. Further, it should be understood that while this example includes three sets of emitters configured to output specific EM signals, different numbers of emitters, sets of emitters, or EM signal configurations may be employed in different examples according to this disclosure.

In some examples, emitters may be selected based on a desired frequency of emitted EM signal. For example, red light or near infrared radiation may be desirable, such as for sensing a level of blood oxygen saturation. In some examples, green light may be desirable for sensing a pulse or a pulse rate. Further, in some examples, a sensing device may include different kinds of emitters, such as to allow sensing of different kinds of biometric information with a single sensing device.

The sensing device **100** also includes several detectors **120a-c**. The detectors **120a-c** are arranged to correspond with one or more emitters **110a-c**. In this example, the detectors **120a-c** comprise silicon photodiodes, however, other suitable detectors include photoresistors, photodiodes, amorphous silicon, and organic CMOS. The detectors **120a-c** are configured to detect EM signals emitted by one or more of the emitters **110a-c**. For example, based on the selection of emitters and the EM signals emitted by each, detectors **120a-c** should be selected to match such selected emitters. For example, if emitters that emit red light are selected, at least one detector should be selected that can detect red light and emit a detector signal indicating the detection of red light. Further, detectors **120a-c** should be located in sufficient proximity to corresponding emitters to allow the detector to detect reflected EM signals emitted by the emitters.

In this example, each of the detectors **120a-c** is configured to output one or more sensor signals in response to detecting an EM signal. In some examples, the detectors **120a-c** may output a saturation signal to that provides a binary indication of whether an EM signal was detected, e.g., either an EM signal was detected or not. In some examples, however, the detectors **120a-c** may output a signal indicating information about the detected EM signal, such as intensity or color. For example, a detector **120a** may be configured to detect orange light and may output an voltage or current based on the intensity of the detected EM signal, or the color of the detected signal.

As can be seen in this example, each detector **120a-c** is connected to a sensing circuit **170** that is configured to carry detector signals, such as to a processor or other device. In this example, each detector **120a-c** is connected to a discrete wire dedicated to the respective detector **120a-c**, however, in other examples each detector **120a-c** may be coupled to a wire matrix configured to provide row and column identification as well as a detector signal from the respective detector **120a-c**. In some examples, different types of detectors **120a-c** may be employed. For example, a first set of detectors may be configured to detect red light, a second set of detectors may be configured to detect orange light, and a third set of detectors may be configured to detect green light. In one such example, each set of detectors may have a separate sensing circuit, which may allow a processor to separately and independently receive detecting signals from one kind of detector or another. However, in some examples, all three sets of detectors may be coupled to the same sensing circuit. Further, it should be understood that while this example includes three sets of detectors configured to

detect specific EM signals, different numbers of detectors, sets of detectors, or EM signal configurations may be employed in different examples according to this disclosure.

In some examples, each detector, or groups of detectors, may be coupled to a sensing circuit by a switch. When the switch is activated, it may allow detector signals generated by the corresponding detector or detectors **120a-c** to travel onto the sensing circuit. Thus, like emitters **110a-c**, detectors **120a-c** may be individually activated or deactivated in a manner similar to that discussed above with respect to emitters. For example, the each detector switch may be connected to a switch matrix (or one of a plurality of switch matrices) to allow a processor to independently activate or deactivate one or more detectors.

Further, the emitters **110a-c** and detectors **120a-c** are fabricated to provide a monolithic emitter/detector strip in which the emitters **110a-c** and detectors **120a-c** are fabricated together into a flexible substrate. Advantages according to this disclosure may be realized in part based on the monolithic construction of an array of emitters, an array of detectors, or a combined array of emitters and detectors, rather than using individual emitters and detectors placed within a device.

As is shown in FIG. 1A, the detectors **120a-c** are isolated from the emitters **110a-c** by optical shielding **130**. In this example, the optical shielding **130** comprises an opaque plastic material; however, in some examples, other suitable materials may be used, such as an opaque polymer material, an opaque metallic material, or an opaque portion of the flexible substrate. The optical shielding **130** in this example is arranged and configured to reduce or eliminate direct transmission of EM signals from an emitter **110a-c** to a detector **120a-c**. Thus, in this example, the detectors **120a-c** and optical shielding **130** have been arranged to allow EM signals from one or more of the emitters **110a-c** to be reflected from a surface and reach one or more of the detectors **120a-c**, however, direct transmission from an emitter to a detector is prohibited by the optical shielding **130**. However, in some examples, optical shielding may allow for some reduced amount of EM signals to directly travel from an emitter to a detector, while also allowing reflected EM signals.

For example, referring to FIG. 1B, FIG. 1B shows a top-down view of an example monolithic integrated emitter-detector array in a flexible substrate for biometric sensing. FIG. 1B illustrates the arrangement of emitters and detectors of the example sensing device **100** shown in FIG. 1A. Emitters are denoted with an "E," while detectors are denoted with a "D." In this example, the emitters and detectors are arranged in a regular "checkerboard" pattern of alternating emitters and detectors in a rectangular pattern. In some examples, other regular patterns may be used, such as hexagonal patterns, triangular patterns, etc. Optical shielding **130** has been arranged in a grid pattern to optically isolate emitters from adjacent detectors. However, as discussed above, other arrangements of emitters, detectors, and optical shielding may be employed.

As shown in FIG. 1B, each emitter is adjacent to a plurality of detectors, and each detector is adjacent to a plurality of emitters. In this example, each emitter is configured to emit the same type of EM signals, e.g., green light, and each detector is configured to detect green light and output a detector signal indicating a detection of green light. However, as discussed above, some examples may employ multiple different types of emitters and detectors.

For example, referring to FIG. 2, FIG. 2 shows a top-down view of an example monolithic integrated emitter-

detector array in a flexible substrate for biometric sensing. In this example, emitters and detectors, denoted by “E” and “D” respectively, are embedded in a flexible substrate **210** and optically isolated from each other by optical shielding **220**. As can be seen, in this example, the arrangement of emitters and detectors is irregular. A number of emitters and detectors have been arranged in a group in the center of the flexible substrate **210**, however, a number of other pairs of emitters and detectors have been arranged in other locations in the flexible substrate **210**. In some examples, irregular arrangements of emitters and detectors may allow for detection of different biometric information, or may allow for movement of a device, e.g., a wearable device, incorporating the sensing device **200** on a person’s body while retaining the ability to sense biometric information. For example, a person may wear a wristband incorporating an example sensing device according to this disclosure. Throughout the day, the sensing device may change positions on the person’s wrist, but due to the arrangement of emitters and detectors on the sensing device, biometric information may still be sensed. FIG. 2 also illustrates that a single detector may be grouped with multiple emitters, or that multiple detectors may be grouped with a single emitter.

Referring now to FIG. 3, FIG. 3 shows an example wearable device **300** having an example flexible sensing device **320**. The example wearable device **300** includes a computing device **310** and a flexible sensing device **320**. In this example, the wearable device **300** is a wristband to be worn on a person’s wrist, but could be worn in other locations. The flexible sensing device **320** includes a flexible substrate with several embedded emitters **322** and detectors **324**, and optical shielding between the emitters and detectors. As discussed above, each of the emitters **322** is configured to emit EM signals, such as visible light or infrared radiation, and each of the detectors **324** is configured to detect EM signals of the kind emitted by one or more of the emitters **322**. The flexible sensing device **320** also includes one or more scanning circuits coupled to the emitters **322**, and one or more sensing circuits coupled to the detectors **324**. The flexible sensing device **320** also includes optical shielding arranged between the emitters **324** and detectors **322** to reduce or eliminate direct transmission of EM signals from an emitter to a detector.

In this example, the flexible sensing device **320** is disposed within a cavity formed in the wearable device **300** with an adhesive. In some examples, however, the flexible sensing device **320** may be attached to the wearable device **300** in another suitable fashion, such as using screws, rivets, or other fasteners.

The computing device **310** is communicatively coupled to the flexible sensing device **320** and configured to transmit signals to the flexible sensing device **320** to activate and deactivate emitters **322** and receive sensing signals from the detectors **324**. The computing device **310** is also configured to determine biometric information from the received signals from the detectors **324**. For example, the computing device **310** can determine a pulse rate of the person wearing the wearable device **300**, determine a level of oxygen saturation in the person’s bloodstream, or determine a level of glucose in the person’s bloodstream.

Referring now to FIG. 4, FIG. 4 shows an example computing device **310** suitable for use with a monolithic integrated emitter-detector array in a flexible substrate for biometric sensing. The example computing device **310** includes a processor **410**, a memory **420**, a display device **430**, an input device **440**, and an output device **445**, as well as a power source (not shown) such as a battery. The

processor **410** is communicatively coupled to the memory **420** and the display device **430**, and is configured to read and execute processor-executable instructions stored in the memory **420**. In this example, the display device **420** includes any suitable display device or display devices. For example, a display device **420** may be an LCD display, an LED display, or an OLED display. Further, in some examples, the display device **420** may be a touch-sensitive display device.

Suitable input devices **440** may include a physical manipulatable input device or manipulandum, such as one or more buttons, switches, dials, or sliders. Other input devices may include touch-sensitive input devices, such as capacitive touch sensors, pressure sensors, or strain gages. One or more such touch-sensitive input devices may include a touchscreen or may be disposed on any other surface of the example wearable device to receive user input. However, in some examples, the computing device **310** may not comprise any user input devices **440**, but may instead simply provide biometric information to the user.

The computing device **400** may also include one or more output devices **445**. Such devices may be configured to communicatively couple to another computing device, such as a medical monitoring device or to a data storage device. For example, the wearable device **300** may be coupled to a patient’s skin and connected to a medical computing device, e.g., computing device **310**, that monitors pulse rate, blood oxygen levels, blood glucose levels, or other biometric information, and also provides that information via the output device **445** to one or more other medical systems. The wearable device may thus function as a wearable sensing device coupled to an external processing device. In some examples, a user may connect another computing device to other computing device **310**, such as to download information from the computing device or to install updated software or settings. Suitable output devices **445** may include a USB interface, an Ethernet interface, an Apple lightning interface, a display interface, a wireless interface such as WiFi, Bluetooth, or near-field communication (NFC), or other suitable output device.

As can be seen in FIG. 4, the example computing device **310** is communicatively coupled to a one or more emitters **452** and one or more detectors **454** of an example flexible sensing device **450**, such as shown in FIGS. 1A-3 and described above. As discussed above, the computing device **310** is configured to activate and deactivate one or more of the emitters **452** and receive sensing signals from one or more of the detectors **454**. The computing device **310** is further configured to determine biometric information based on the received sensing signals.

In some examples, the computing device **310** is further configured to select an optimal set of emitters for use in obtaining detector signals. For example, depending on the placement of a flexible sensing device **450**, or inadvertent movement of the flexible sensing device **450**, different emitters may result in better quality detector signals. Thus, the computing device **310** may execute a process to select an optimal set of emitters, and not use other emitters. Such a process may allow for increased battery life as only the subset of optimal emitters may be used during normal operation.

To do so, in this example, the processor **410** selectively activates one or more emitters and obtain corresponding detector signals to identify an emitter or set of emitters that provides the best sensing information for determining biometric information. For example, and as will be discussed in more detail below, the processor **410** may selectively acti-

vate and deactivate each emitter individually in succession and analyze the received detector signals to determine a quality of the detector signals. After cycling through each emitter, the computing device **310** determines the best emitter or emitters and only uses the determined emitters for later activation to obtain detector signals. Over time, the processor **410** may re-perform such a process to update the determined emitters, such as to accommodate a different user, a change in position of the flexible sensing device **450**, or because a predetermined time has elapsed since a prior optimization process.

Referring now to FIG. 5, FIG. 5 shows an example method **500** for optimizing a monolithic integrated emitter-detector array in a flexible substrate for biometric sensing. The method **500** will be described with respect to the computing device shown in FIG. 4 and the flexible sensing device shown in FIGS. 1A-1B, however, any suitable flexible sensing device or computing device may be used. The example method **500** shown in FIG. 5 begins in block **505**.

At block **505**, the computing device **310** first deactivates all emitters. In some examples, a flexible sensing device may include multiple different types of emitters and detectors, e.g., having different colors of EM signals, as discussed above to sense different types of biometric information. In some examples of the method **500**, the computing device **310** may separately optimize the different types of emitters and detectors while continuing to operate other types of emitters and detectors normally. Thus, at block **505**, the computing device **310** may only deactivate a subset of the emitters, such as the emitters of a particular type, while continuing to use any or all of the remaining emitters normally.

At block **510**, the computing device **310** activates a first emitter. To activate an emitter, the processor **410** identifies all available emitters **110a-c** and determines which have not yet been activated as a part of the method **500**. The processor **410** then selects one of these emitters **120a** and transmits a signal to a switch **112a** corresponding to the emitter **120a**. In this example, the processor **410** selects individual emitters and activates only one; however, in other examples, the flexible sensing device **450** may include one or more scanning circuits having switches corresponding to multiple emitters. In one such example, the processor **410** may then activate and deactivate multiple emitters at a time using a single switch. Or, in some examples, the processor **410** may maintain in memory **420** a data structure indicating a correspondence of emitters and detectors. In one such example, the processor **410** may select detectors one at a time (or a group at a time) and activate all corresponding emitters for the selected detector or group of detectors. In another such example, the processor **410** may select detectors one at a time (or a group at a time), and only activate one corresponding emitter at a time, but step through the remaining corresponding emitters before selecting a new detector.

At block **520**, the processor **410** receives a detector signal from a detector corresponding to the activated emitter. In this example, one or more detectors may receive EM signals from the activated emitter. Because the detectors are optically shielded from the emitters, such received EM should mostly be due to reflections of emitted EM signals off of another object, such as a person's skin. As discussed above, a detector, in response to receiving one or more EM signals, generates and transmits a detector signal. The detector circuit carries the sensing signal to the processor **410**, which then receives the detector signal. In some examples, more than one detector may receive emitted EM signals and therefore, more than one detector may transmit a detector

signal in response to EM signals emitted by the activated emitter. In one such example, the processor **410** may receive such signals one at a time. For example, as discussed above, the processor **410** may selectively activate each detector to selectively receive detector signals from individual detectors. The processor **410**, in one such example, may selectively activate and deactivate, in succession, each detector for an activated emitter to attempt to receive detector signals from each detector. Such an example may allow a processor to determine a correspondence between an emitter and one or more detectors. For example, a correspondence may be determined between an emitter and any detector from which a detector signal is received, or from which a detector signal having a quality above a predetermined threshold is received. In some examples, a correspondence between emitters and detectors may be predetermined, thus detector signals may only be received from detectors predetermined to correspond to an activated emitter.

In some examples, detectors in the flexible sensing device **450** may comprise analog detectors that may provide a constant detector signal, such as a voltage, irrespective of any received EM signals. In one such example, the detector may change the voltage of the detector signal based on a strength of a received EM signal, such as an intensity of received light. Such a detector signal may fluctuate over time as the strength of the received EM signal changes over time, e.g., due to movement of the detector, movement of a surface reflecting EM signals from an emitter onto the detector, changes in conditions on a surface reflecting EM signals from an emitter onto the detector, a user's pulse, or other reasons. Such fluctuation may itself be a component of a detector signal, in some examples. For example, a processing device **410** may attempt to determine a pulse rate of a person. Thus, the processing device **410** may receive detector signals over a period of time. Such fluctuations may also include noise, such as due to inherent properties of the detector; EM signals penetrating optical shielding; characteristics of a person's skin; exposure of the detector to other light sources, e.g., sunlight; or movement of the detector. Thus, in some examples, a detector signal may not include an instantaneous or digital signal, but may instead be an analog signal having properties including magnitude, frequency, noise, or other properties.

At block **525**, the processor **410** deactivates the activated emitter or emitters.

At block **530**, the processor **410** determines a quality of the received detector signal. In this example, the detectors **460** are configured to output detector signals comprising analog voltages based on a strength of a received EM signal. Thus, for each received detector signal, the processor **410** determines a base voltage value for the detector and a magnitude of the received detector signal. In this example, the base voltage for the detector signal is based on a received detector signal during which no emitters are activated. The processor **410** determines a quality based on a difference between the magnitude of the received detector signal and the base voltage. The processor **410** then compares the difference to a predetermined threshold. For example a detector may be configured to output a voltage between 0 and 5 volts. The processor **410** has previously determined that the base voltage output by the detector is 0.3 volts, and a received detector signal has a magnitude of 3.7 volts. Thus, the processor **410** determines a difference of 3.4 volts, which is compared against a threshold. In this example, the predetermined threshold is 3.2 volts, thus the processor **410** determines that the received detector signal is a good detector signal. In some examples, multiple predetermined

thresholds may be used, and a quality of a detector signal may be increasingly high the more thresholds the received detector signal meets or exceeds.

In some examples, the processor **410** determines other qualities of the received detector signal. For example, the processor **410** may determine a signal-to-noise (SNR) ratio for a received detector signal. For example, rather than determining the difference between a base output voltage and a voltage of a received detector signal, the processor **410** may determine a ratio between the two voltages. In the example discussed above, the SNR may be computed as 3.7 volts divided 0.3 volts, which results in a SNR of 12.3. In some examples, a SNR may be calculated in decibels, such as by calculating the SNR as described above, calculating the base-10 logarithm of the SNR, and then multiplying that value by 10. Using the example values above, the SNR_{dB} is 10.91. In some examples, the determined SNR may be compared against a threshold or thresholds, as described above, or may be otherwise compared against detector signals received from other detectors. For example, after calculating an SNR_{dB}, the processor **410** may determine whether the received detector signal is in the top 10% of received sensor signals that exceed the threshold.

A quality of a received detector signal thus may be established as a SNR, such as a raw SNR or an SNR_{dB}. In some examples, a quality may be a binary or otherwise stepped value, such as based on whether the detector signal exceeds one or more threshold values.

Further, as discussed above, the processor **410** may receive detector signals from a plurality of detectors. Thus, in some examples, the processor **410** may determine a quality of a plurality of received detector signals for an activated emitter. The processor **410** determines the qualities of such received detector signals as discussed above.

The processor **410** then stores the determined quality or qualities in the memory **420**.

At block **540**, the processor **410** determines whether all emitters have been activated. If not, the method **500** returns to block **510**. Otherwise, the method proceeds to block **550**. However, as discussed above, only a subset of all emitters in a sensing device may be employed with respect to execution of the method **500**, thus, at block **540**, the processor **410** may determine whether all emitters within the relevant subset have been activated.

At block **550**, the processor **410** selects an emitter based on the determined qualities. For example, as discussed above, the processor **410**, for each emitter of a plurality of emitters, has determined qualities of received detector signals. Thus, the processor **410** may analyze the determined qualities to identify a highest or best quality detector signal of the determined qualities of all the received detector signals, and select the emitter associated with the highest quality detector signal. For example, an emitter associated with the highest SNR value for a detector signal may be selected. In some examples, however, the processor **410** may analyze the qualities of the detector signals to determine a sum of the qualities for each activated emitter and select the emitter resulting in the highest sum qualities. In some examples, other statistics may be employed.

For example, for each activated emitter, an average value, a range, a standard deviation, a variance, a median value, or other value may be determined to select an emitter. For example an emitter associated with lower peak qualities of received detector signals, but with a mean value above a threshold and a standard deviation below a second threshold may be selected. Such an emitter may be associated with high quality readings from multiple different detectors. In

some examples, emitters associated with a lowest range value, but highest peak value, may be selected. In some examples, emitters with a highest mean or median value may be selected. Still other values may be used to select an emitter.

In some examples, the processor **410** may select more than one emitter. For example, multiple emitters may result in high quality detector signals. For example, calculated SNR or SNR_{dB} values for detector signals may be above a threshold value for multiple emitters. In one such example, the processor **410** may select each of such emitters.

At block **560**, the processor **410** activates the selected emitter or emitters.

At block **570**, the processor determines biometric information, such as a pulse rate, blood oxygen saturation level, blood glucose level, or other biometric information based on received detector signals resulting from the activated selected emitters.

The method **500** of FIG. **5** may be repeated periodically, such as once per minute, to obtain high quality detector signals for determining biometric information. In some examples, the method **500** may be executed in succession, such as based on a flexible sensing device **450** having multiple different types of emitters and detectors. Thus, the method **500** may be executed sequentially, or in parallel, for each different type of emitter.

While the methods and systems herein are described in terms of software executing on various computing devices, the methods and systems may also be implemented as specifically-configured hardware, such as field-programmable gate array (FPGA) specifically to execute the various methods. For example, examples can be implemented in digital electronic circuitry, or in computer hardware, firmware, software, or in a combination thereof. In one example, a device may include a processor or processors. The processor comprises a computer-readable medium, such as a random access memory (RAM) coupled to the processor. The processor executes computer-executable program instructions stored in memory, such as executing one or more computer programs for editing an image. Such processors may comprise a microprocessor, a digital signal processor (DSP), an application-specific integrated circuit (ASIC), field programmable gate arrays (FPGAs), and state machines. Such processors may further comprise programmable electronic devices such as PLCs, programmable interrupt controllers (PICs), programmable logic devices (PLDs), programmable read-only memories (PROMs), electronically programmable read-only memories (EPROMs or EEPROMs), or other similar devices.

Such processors may comprise, or may be in communication with, media, for example computer-readable storage media, that may store instructions that, when executed by the processor, can cause the processor to perform the steps described herein as carried out, or assisted, by a processor. Examples of computer-readable media may include, but are not limited to, an electronic, optical, magnetic, or other storage device capable of providing a processor, such as the processor in a web server, with computer-readable instructions. Other examples of media comprise, but are not limited to, a floppy disk, CD-ROM, magnetic disk, memory chip, ROM, RAM, ASIC, configured processor, all optical media, all magnetic tape or other magnetic media, or any other medium from which a computer processor can read. The processor, and the processing, described may be in one or more structures, and may be dispersed through one or more

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structures. The processor may comprise code for carrying out one or more of the methods (or parts of methods) described herein.

The foregoing description of some examples has been presented only for the purpose of illustration and description and is not intended to be exhaustive or to limit the disclosure to the precise forms disclosed. Numerous modifications and adaptations thereof will be apparent to those skilled in the art without departing from the spirit and scope of the disclosure.

Reference herein to an example or implementation means that a particular feature, structure, operation, or other characteristic described in connection with the example may be included in at least one implementation of the disclosure. The disclosure is not restricted to the particular examples or implementations described as such. The appearance of the phrases “in one example,” “in an example,” “in one implementation,” or “in an implementation,” or variations of the same in various places in the specification does not necessarily refer to the same example or implementation. Any particular feature, structure, operation, or other characteristic described in this specification in relation to one example or implementation may be combined with other features, structures, operations, or other characteristics described in respect of any other example or implementation.

Use herein of the word “or” is intended to cover inclusive and exclusive OR conditions. In other words, A or B or C includes all of the following alternative combinations as appropriate for a particular usage: A alone; B alone; C alone; A and B only; A and C only; B and C only; and A and B and C.

What is claimed is:

1. A monolithic device for sensing biometric information comprising:

- a flexible substrate; and
- a monolithic array of emitters and detectors fabricated in the flexible substrate, the monolithic array comprising:
 - a first array of emitters configured to emit first electromagnetic (EM) signals;
 - a first array of detectors configured to detect reflections of the first EM signals;
 - a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters of the first array of emitters; and
 - a first sensing circuit coupled to individual detectors of the first array of detectors, the first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors.

2. The device of claim 1, wherein the first array of emitters comprises a light emitting diode (LED) or an organic LED (OLED).

3. The device of claim 1, wherein the first EM signals comprise red light, orange light, green light, or infrared radiation.

4. The device of claim 1, wherein the first array of detectors comprises a photodiode or a photoresistor.

5. The device of claim 1, further comprising a second array of emitters embedded in the flexible substrate, the second array of emitters configured to emit second electromagnetic (EM) signals, and wherein:

- the first array of detectors is further configured to detect reflections of the second EM signals, and
- the first scanning circuit is further coupled to the second array of emitters and further configured to selectively activate individual emitters of the second array of emitters.

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6. The device of claim 1, further comprising:

- a plurality of arrays of emitters,
- a plurality of arrays of detectors, wherein each array of detectors is arranged to correspond with at least one array of emitters.

7. The device of claim 1, wherein the emitters of the first array of emitters are arranged in a regular pattern.

8. The device of claim 7, wherein the regular pattern comprises a rectangular grid or a hexagonal grid.

9. The device of claim 1, wherein the emitters of the first array of emitters are arranged in an irregular pattern.

10. The device of claim 1, further comprising optical shielding between adjacent emitters and detectors of the monolithic array.

11. A system for sensing biometric information comprising:

- a wearable housing;
- a processor and a non-transitory computer-readable medium disposed within the wearable housing, the processor in communication with the non-transitory computer-readable medium and configured to execute program code stored in the non-transitory computer-readable medium;
- a flexible substrate;
- a monolithic sensor fabricated in the flexible substrate in communication with the processor and configured to provide sensor signals to the processor, the sensor comprising:
 - a first array of emitters configured to emit first electromagnetic (EM) signals;
 - a first array of detectors configured to detect reflections of the first EM signals;
 - a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters of the first array of emitters; and
 - a first sensing circuit coupled to individual detectors of the first array of detectors, the first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors.

12. The system of claim 11, further comprising a power source in communication with the processor, the non-transitory computer-readable medium, and the sensor.

13. The system of claim 11, wherein the first array of emitters comprises a light emitting diode (LED) or a silicon photodiode.

14. The system of claim 11, wherein the first EM signals comprises red light, orange light, green light, or infrared radiation.

15. The system of claim 11, wherein the first array of detectors comprises a photodiode or a photoresistor.

16. The system of claim 11, further comprising a second array of emitters embedded in the flexible substrate, the second array of emitters configured to emit second electromagnetic (EM) signals, and wherein:

- the first array of detectors is further configured to detect reflections of the second EM signals, and
- the first scanning circuit is further coupled to the second array of emitters and further configured to selectively activate individual emitters of the second array of emitters.

17. The system of claim 11, further comprising:

- a plurality of arrays of emitters,
- a plurality of arrays of detectors, wherein each array of detectors is arranged to correspond with at least one array of emitters.

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18. The system of claim 17, wherein emitters of the first array of emitters are arranged in a regular pattern.

19. The system of claim 18, wherein the regular pattern comprises a rectangular grid or a hexagonal grid.

20. The system of claim 17, wherein the emitters of the first array of emitters are arranged in an irregular pattern.

21. The system of claim 11, wherein the wearable housing is configured to be worn on a person's wrist, a person's forearm, a person's upper arm, a person's chest, or a person's leg.

22. The system of claim 11, wherein the processor is further configured to:

cause the first scanning circuit to selectively activate individual emitters of the first array of emitters;

determine biometric information based at least in part on a sensor signal received from the sensor.

23. The system of claim 22, wherein the biometric information comprises one or more of a pulse rate, a blood oxygen saturation level, or a blood glucose level.

24. A method of sensing biometric information using a monolithic sensor comprising:

providing a monolithic array of emitters and detectors fabricated in a flexible substrate, the monolithic array comprising: a first array of emitters, each emitter configured to emit an electromagnetic (EM) signal, a first array of detectors; a first scanning circuit coupled to the first array of emitters, the first scanning circuit configured to selectively activate individual emitters of the first array of emitters; and a first sensing circuit coupled to individual detectors of the first array of detectors, the

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first sensing circuit configured to receive a detection signal from at least one of the detectors of the first array of detectors;

for each emitter of the monolithic array:

activating the emitter,

receiving a detector signal from one or more detectors of the monolithic array corresponding to the activated emitter,

deactivating the activated emitter, and

determining a quality of the received detector signal;

selecting an emitter based on the determined qualities;

activating the selected emitter; and

determining biometric information based at least in part on a detector signal received from the corresponding detector.

25. The method of claim 24, wherein selecting the emitter comprises:

determining a signal-to-noise ratio (SNR) value of the received detector signal; and

responsive to determining that the SNR value exceeds a threshold SNR value, determining that the SNR value exceeds a threshold value and selecting the emitter associated with the SNR value.

26. The method of claim 24 wherein:

selecting the emitter comprises selecting a plurality of emitters, and

activating the selected emitter comprises activating each emitter of the selected plurality of emitters.

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专利名称(译)	用于生物识别传感的柔性基板中的单片集成发射器 - 探测器阵列		
公开(公告)号	US10271745	公开(公告)日	2019-04-30
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[标]申请(专利权)人(译)	高通股份有限公司		
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当前申请(专利权)人(译)	高通公司		
[标]发明人	GU SHIQUN NOWAK MATTHEW MICHAEL KASKOUN KENNETH DANTSKER EUGENE MARTIN RUSSEL ALLYN		
发明人	GU, SHIQUN NOWAK, MATTHEW MICHAEL KASKOUN, KENNETH DANTSKER, EUGENE MARTIN, RUSSEL ALLYN		
IPC分类号	A61B5/1455 A61B5/024 A61B5/145 A61B5/00		
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外部链接	Espacenet		

摘要(译)

公开了用于生物特征感测的柔性基板中的单片集成发射器 - 检测器阵列的示例以及相关联的装置和方法。一个公开的示例装置包括柔性基板;嵌入柔性基板中的第一发射器阵列, 第一发射器阵列配置成发射第一电磁 (EM) 信号;嵌入柔性基板中的第一检测器阵列, 第一检测器阵列配置成检测第一EM信号的反射;第一扫描电路, 耦合到第一发射器阵列, 第一扫描电路配置成选择性地激活第一发射器阵列的各个发射器;第一传感电路, 其耦合到第一检测器阵列的各个检测器, 第一传感电路配置成从第一检测器阵列的至少一个检测器接收检测信号。

