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- (54) **SINE SATURATION TRANSFORM**
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5,341,805 A	8/1994	Stavridi et al.
D353,195 S	12/1994	Savage et al.
D353,196 S	12/1994	Savage et al.
5,377,676 A	1/1995	Vari et al.
D359,546 S	6/1995	Savage et al.
5,431,170 A	7/1995	Mathews

(Continued)

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FOREIGN PATENT DOCUMENTS

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WO	WO 98/42250	10/1998
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(65) **Prior Publication Data**

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(Continued)

Related U.S. Application Data**OTHER PUBLICATIONS**

- (63) Continuation of application No. 11/417,914, filed on May 3, 2006, which is a continuation of application No. 11/048,232, filed on Feb. 1, 2005, which is a continuation of application No. 10/184,032, filed on Jun. 26, 2002, now Pat. No. 6,850,787.
- (60) Provisional application No. 60/302,438, filed on Jun. 29, 2001.
- (51) **Int. Cl.**
A61B 5/145 (2006.01)
- (52) **U.S. Cl.** **600/324; 600/323; 702/190**
- (58) **Field of Classification Search** **600/322, 600/323, 324; 702/189, 190**
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Office Action of Japanese Patent Application No. 2003-508244 dated Mar. 26, 2008 and English Translation of same in 35 pages.

(Continued)

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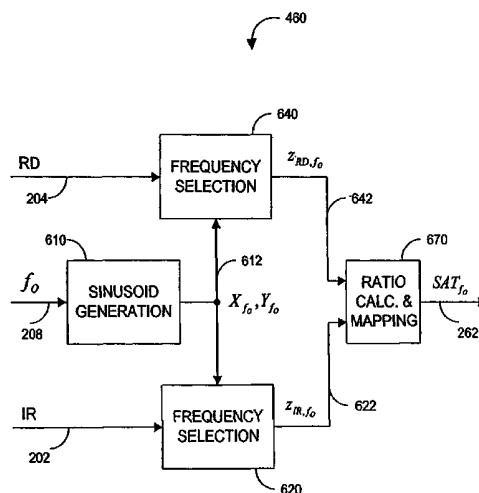
(57) **ABSTRACT**

A transform for determining a physiological measurement is disclosed. The transform determines a basis function index from a physiological signal obtained through a physiological sensor. A basis function waveform is generated based on basis function index. The basis function waveform is then used to determine an optimized basis function waveform. The optimized basis function waveform is used to calculate a physiological measurement.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,960,128 A	10/1990	Gordon et al.
4,964,408 A	10/1990	Hink et al.
5,041,187 A	8/1991	Hink et al.
5,069,213 A	12/1991	Polczynski
5,163,438 A	11/1992	Gordon et al.
5,337,744 A	8/1994	Branigan

14 Claims, 14 Drawing Sheets

U.S. PATENT DOCUMENTS					
D361,840 S	8/1995	Savage et al.	6,371,921 B1	4/2002	Caro et al.
D362,063 S	9/1995	Savage et al.	6,377,829 B1	4/2002	Al-Ali
5,452,717 A	9/1995	Branigan et al.	6,388,240 B2	5/2002	Schulz et al.
D363,120 S	10/1995	Savage et al.	6,397,091 B2	5/2002	Diab et al.
5,456,252 A	10/1995	Vari et al.	6,430,525 B1	8/2002	Weber et al.
5,482,036 A	1/1996	Diab et al.	6,463,311 B1	10/2002	Diab
5,490,505 A	2/1996	Diab et al.	6,470,199 B1	10/2002	Kopotic et al.
5,494,043 A	2/1996	O'Sullivan et al.	6,501,975 B2	12/2002	Diab et al.
5,533,511 A	7/1996	Kaspari et al.	6,505,059 B1	1/2003	Kollias et al.
5,561,275 A	10/1996	Savage et al.	6,515,273 B2	2/2003	Al-Ali
5,562,002 A	10/1996	Lalin	6,519,486 B1 *	2/2003	Edgar et al. 600/336
5,590,649 A	1/1997	Caro et al.	6,519,487 B1	2/2003	Parker
5,602,924 A	2/1997	Durand et al.	6,525,386 B1	2/2003	Mills et al.
5,632,272 A	5/1997	Diab et al.	6,526,300 B1	2/2003	Kiani et al.
5,638,816 A	6/1997	Kiani-Azarbayjany et al.	6,541,756 B2	4/2003	Schulz et al.
5,638,818 A	6/1997	Diab et al.	6,542,764 B1	4/2003	Al-Ali et al.
5,645,440 A	7/1997	Tobler et al.	6,580,086 B1	6/2003	Schulz et al.
5,685,299 A	11/1997	Diab et al.	6,584,336 B1	6/2003	Ali et al.
D393,830 S	4/1998	Tobler et al.	6,595,316 B2	7/2003	Cybulski et al.
5,743,262 A	4/1998	Lepper, Jr. et al.	6,597,932 B2	7/2003	Tian et al.
5,758,644 A	6/1998	Diab et al.	6,597,933 B2	7/2003	Kiani et al.
5,760,910 A	6/1998	Lepper, Jr. et al.	6,606,511 B1	8/2003	Ali et al.
5,769,785 A	6/1998	Diab et al.	6,632,181 B2	10/2003	Flaherty et al.
5,782,757 A	7/1998	Diab et al.	6,639,668 B1	10/2003	Trepagnier
5,785,659 A	7/1998	Caro et al.	6,640,116 B2	10/2003	Diab
5,791,347 A	8/1998	Flaherty et al.	6,643,530 B2	11/2003	Diab et al.
5,810,734 A	9/1998	Caro et al.	6,650,917 B2	11/2003	Diab et al.
5,823,950 A	10/1998	Diab et al.	6,654,624 B2	11/2003	Diab et al.
5,830,131 A	11/1998	Caro et al.	6,658,276 B2	12/2003	Kianl et al.
5,833,618 A	11/1998	Caro et al.	6,661,161 B1	12/2003	Lanzo et al.
5,853,364 A *	12/1998	Baker et al. 600/300	6,671,531 B2	12/2003	Al-Ali et al.
5,860,919 A	1/1999	Kiani-Azarbayjany et al.	6,678,543 B2	1/2004	Diab et al.
5,890,929 A	4/1999	Mills et al.	6,684,090 B2	1/2004	Ali et al.
5,904,654 A	5/1999	Wohltmann et al.	6,684,091 B2	1/2004	Parker
5,919,134 A	7/1999	Diab	6,697,656 B1	2/2004	Al-Ali
5,934,925 A	8/1999	Tobler et al.	6,697,657 B1	2/2004	Shehada et al.
5,940,182 A	8/1999	Lepper, Jr. et al.	6,697,658 B2	2/2004	Al-Ali
5,995,855 A	11/1999	Kiani et al.	RE38,476 E	3/2004	Diab et al.
5,997,343 A	12/1999	Mills et al.	6,699,194 B1	3/2004	Diab et al.
6,002,952 A	12/1999	Diab et al.	6,714,804 B2	3/2004	Al-Ali et al.
6,011,986 A	1/2000	Diab et al.	RE38,492 E	4/2004	Diab et al.
6,027,452 A	2/2000	Flaherty et al.	6,721,582 B2	4/2004	Trepagnier et al.
6,036,642 A	3/2000	Diab et al.	6,721,585 B1	4/2004	Parker
6,045,509 A	4/2000	Caro et al.	6,725,075 B2	4/2004	Al-Ali
6,067,462 A	5/2000	Diab et al.	6,728,560 B2	4/2004	Kollias et al.
6,081,735 A	6/2000	Diab et al.	6,735,459 B2	5/2004	Parker
6,088,607 A	7/2000	Diab et al.	6,745,060 B2	6/2004	Diab et al.
6,110,522 A	8/2000	Lepper, Jr. et al.	6,760,607 B2	7/2004	Al-Ali
6,124,597 A	9/2000	Shehada	6,770,028 B1	8/2004	Ali et al.
6,144,868 A	11/2000	Parker	6,771,994 B2	8/2004	Kiani et al.
6,151,516 A	11/2000	Kiani-Azarbayjany et al.	6,792,300 B1	9/2004	Diab et al.
6,152,754 A	11/2000	Gerhardt et al.	6,813,511 B2	11/2004	Diab et al.
6,157,850 A	12/2000	Diab et al.	6,816,741 B2	11/2004	Diab
6,165,005 A	12/2000	Mills et al.	6,822,564 B2	11/2004	Al-Ali
6,184,521 B1	2/2001	Coffin, IV et al.	6,826,419 B2	11/2004	Diab et al.
6,206,830 B1	3/2001	Diab et al.	6,830,711 B2	12/2004	Mills et al.
6,229,856 B1	5/2001	Diab et al.	6,850,787 B2	2/2005	Weber et al.
6,232,609 B1	5/2001	Snyder et al.	6,850,788 B2	2/2005	Al-Ali
6,236,872 B1	5/2001	Diab et al.	6,852,083 B2	2/2005	Caro et al.
6,241,683 B1	6/2001	Macklem et al.	6,861,639 B2	3/2005	Al-Ali
6,256,523 B1	7/2001	Diab et al.	6,898,452 B2	5/2005	Al-Ali et al.
6,263,222 B1	7/2001	Diab et al.	6,920,345 B2	7/2005	Al-Ali et al.
6,278,522 B1	8/2001	Lepper, Jr. et al.	6,931,268 B1	8/2005	Kiani-Azarbayjany et al.
6,280,213 B1	8/2001	Tobler et al.	6,934,570 B2	8/2005	Kiani et al.
6,285,896 B1	9/2001	Tobler et al.	6,939,305 B2	9/2005	Flaherty et al.
6,321,100 B1	11/2001	Parker	6,943,348 B1	9/2005	Coffin IV
6,334,065 B1	12/2001	Al-Ali et al.	6,950,687 B2	9/2005	Al-Ali
6,343,224 B1	1/2002	Parker	6,961,598 B2	11/2005	Diab
6,349,228 B1	2/2002	Kiani et al.	6,970,792 B1	11/2005	Diab
6,360,114 B1	3/2002	Diab et al.	6,979,812 B2	12/2005	Al-Ali
6,368,283 B1	4/2002	Xu et al.	6,985,764 B2	1/2006	Mason et al.
			6,993,371 B2	1/2006	Kiani et al.
			6,996,427 B2	2/2006	Ali et al.

6,999,904 B2 2/2006 Weber et al.
 7,003,338 B2 2/2006 Weber et al.
 7,003,339 B2 2/2006 Diab et al.
 7,015,451 B2 3/2006 Dalke et al.
 7,024,233 B2 4/2006 Ali et al.
 7,027,849 B2 4/2006 Al-Ali
 7,030,749 B2 4/2006 Al-Ali
 7,039,449 B2 5/2006 Al-Ali
 7,041,060 B2 5/2006 Flaherty et al.
 7,044,918 B2 5/2006 Diab
 7,067,893 B2 6/2006 Mills et al.
 7,096,052 B2 8/2006 Mason et al.
 7,096,054 B2 8/2006 Abdul-Hafiz et al.
 7,132,641 B2 11/2006 Schulz et al.
 7,142,901 B2 11/2006 Kiani et al.
 7,149,561 B2 12/2006 Diab
 7,186,966 B2 3/2007 Al-Ali
 7,190,261 B2 3/2007 Al-Ali
 7,215,984 B2 5/2007 Diab
 7,215,986 B2 5/2007 Diab
 7,221,971 B2 5/2007 Diab
 7,225,006 B2 5/2007 Al-Ali et al.
 7,225,007 B2 5/2007 Al-Ali
 RE39,672 E 6/2007 Shehada et al.
 7,239,905 B2 7/2007 Kiani-Azarbayjany et al.
 7,245,953 B1 7/2007 Parker
 7,254,431 B2 8/2007 Al-Ali
 7,254,433 B2 8/2007 Diab et al.
 7,254,434 B2 8/2007 Schulz et al.
 7,272,425 B2 9/2007 Al-Ali
 7,274,955 B2 9/2007 Kiani et al.

D554,263 S 10/2007 Al-Ali
 7,280,858 B2 10/2007 Al-Ali et al.
 7,289,835 B2 10/2007 Mansfield et al.
 7,292,883 B2 11/2007 De Felice et al.
 7,295,866 B2 11/2007 Al-Ali
 7,328,053 B1 2/2008 Diab et al.
 7,332,784 B2 2/2008 Mills et al.
 7,340,287 B2 3/2008 Mason et al.
 7,341,559 B2 3/2008 Schulz et al.
 7,343,186 B2 3/2008 Lamego et al.
 D566,282 S 4/2008 Al-Ali et al.
 7,355,512 B1 4/2008 Al-Ali
 7,371,981 B2 5/2008 Abdul-Hafiz
 7,373,193 B2 5/2008 Al-Ali et al.
 7,373,194 B2 5/2008 Weber et al.
 7,376,453 B1 5/2008 Diab et al.
 7,377,794 B2 5/2008 Al-Ali et al.
 7,377,899 B2 5/2008 Weber et al.
 7,383,070 B2 6/2008 Diab et al.

FOREIGN PATENT DOCUMENTS

WO WO 02/047582 A3 6/2002

OTHER PUBLICATIONS

PCT International Search Report, App. No. PCT/US 02/20674, App. Dates: Jun. 28, 2002, 5 pages.

Office Action of Japanese Patent Application No. 2003-508244 Dispatched on Mar. 26, 2008 and English Translation of same in 35 pages.

* cited by examiner

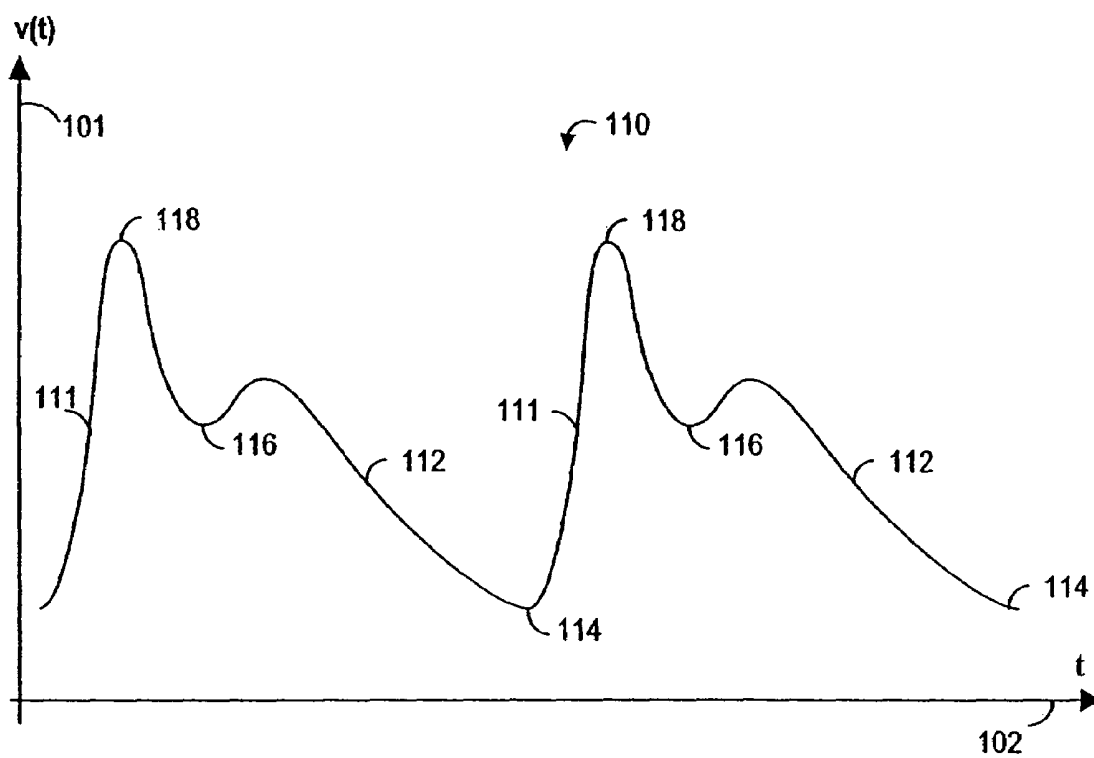


FIG. 1A

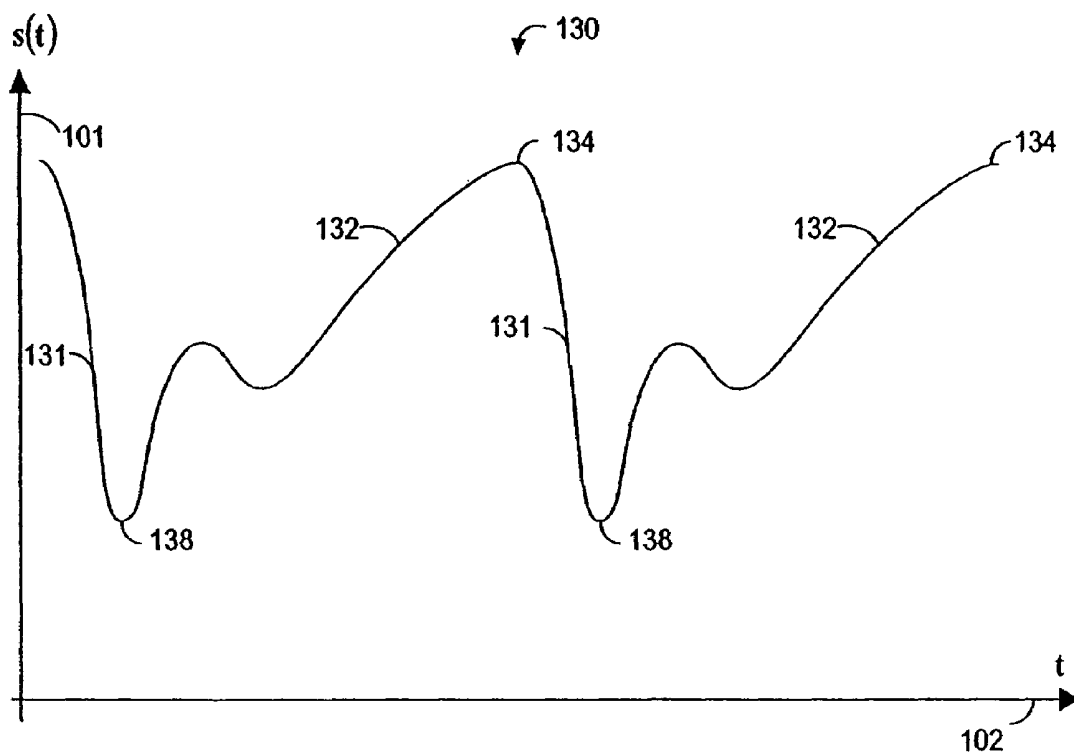


FIG. 1B

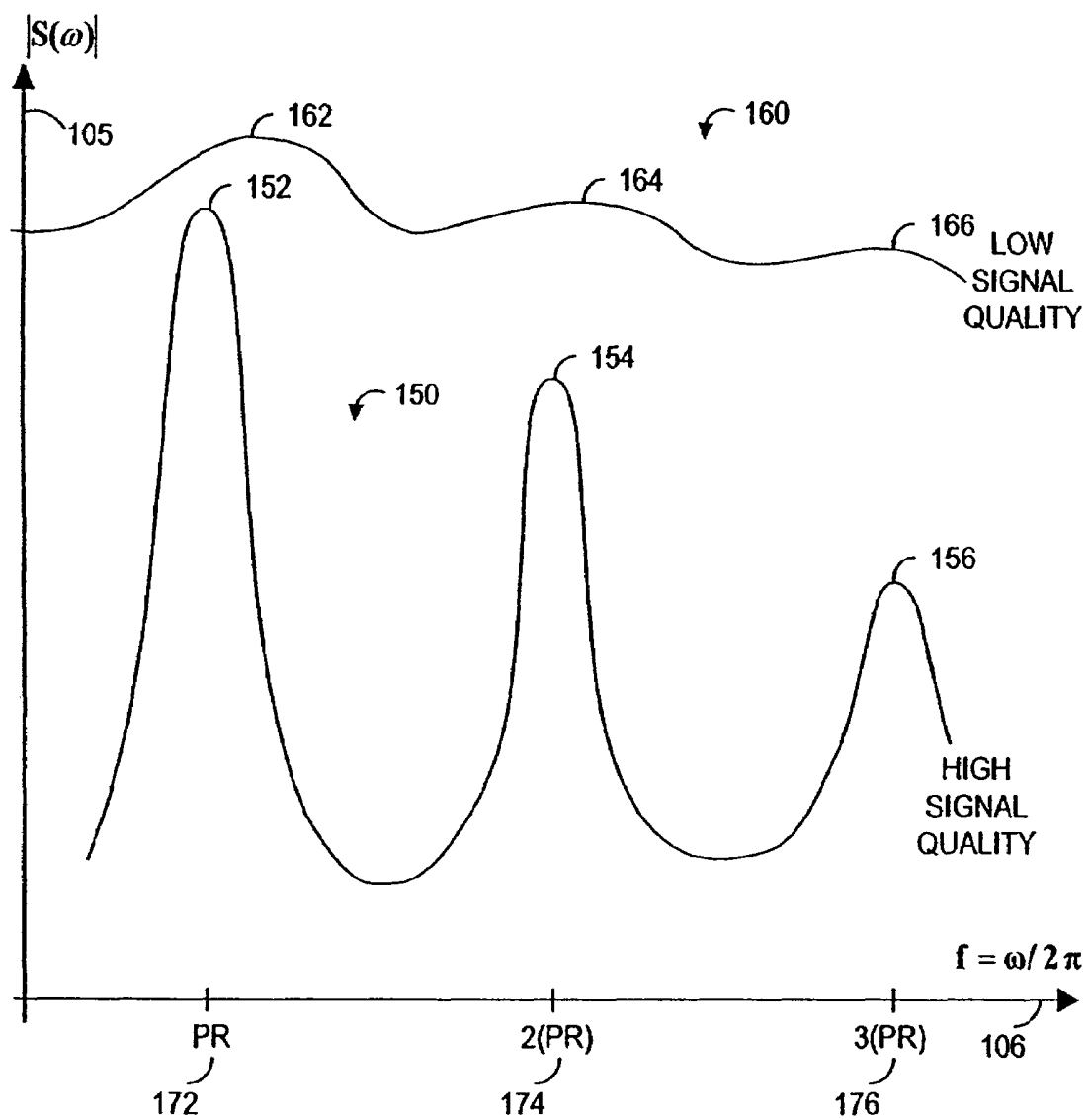


FIG. 1C

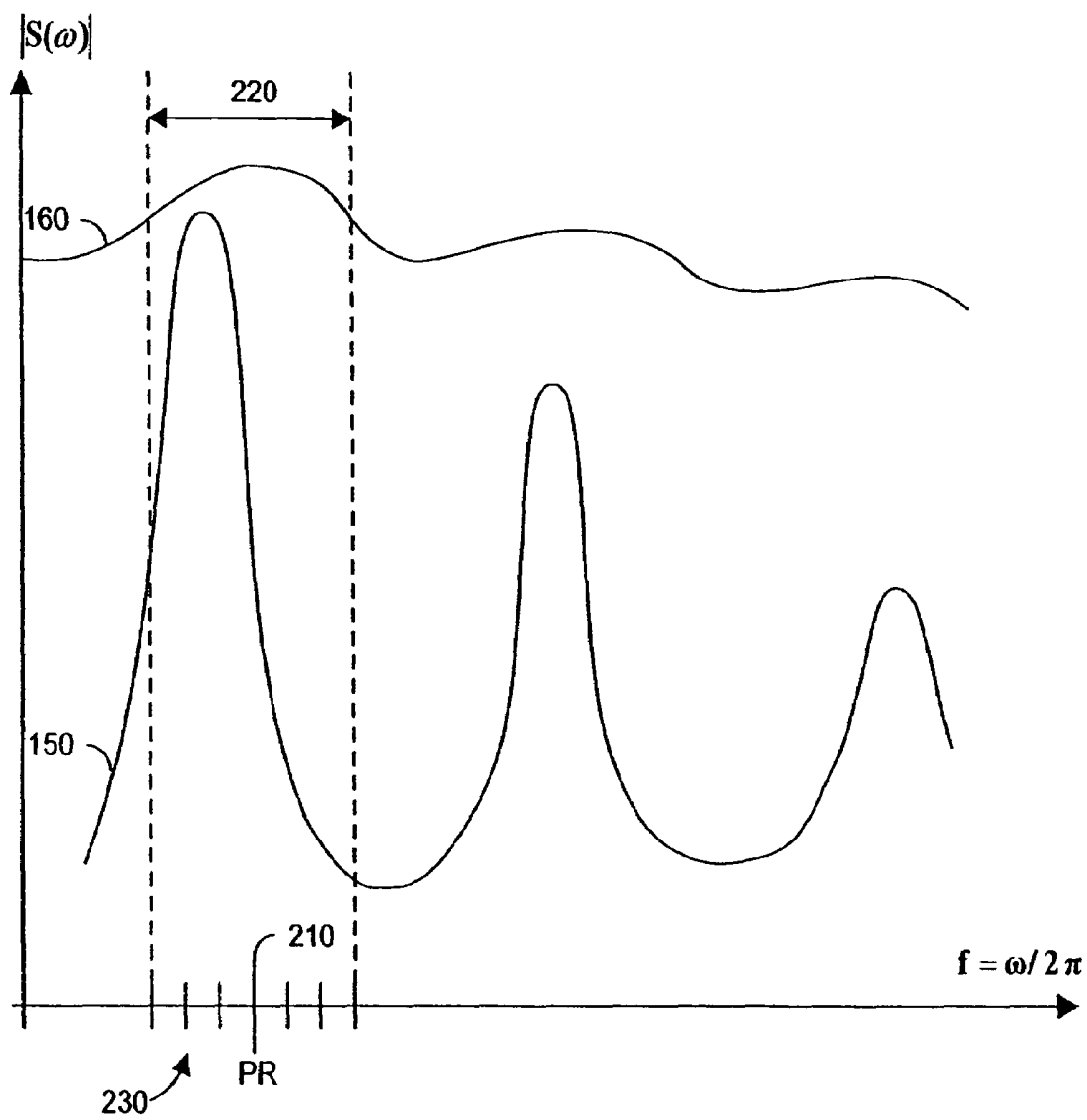


FIG. 2

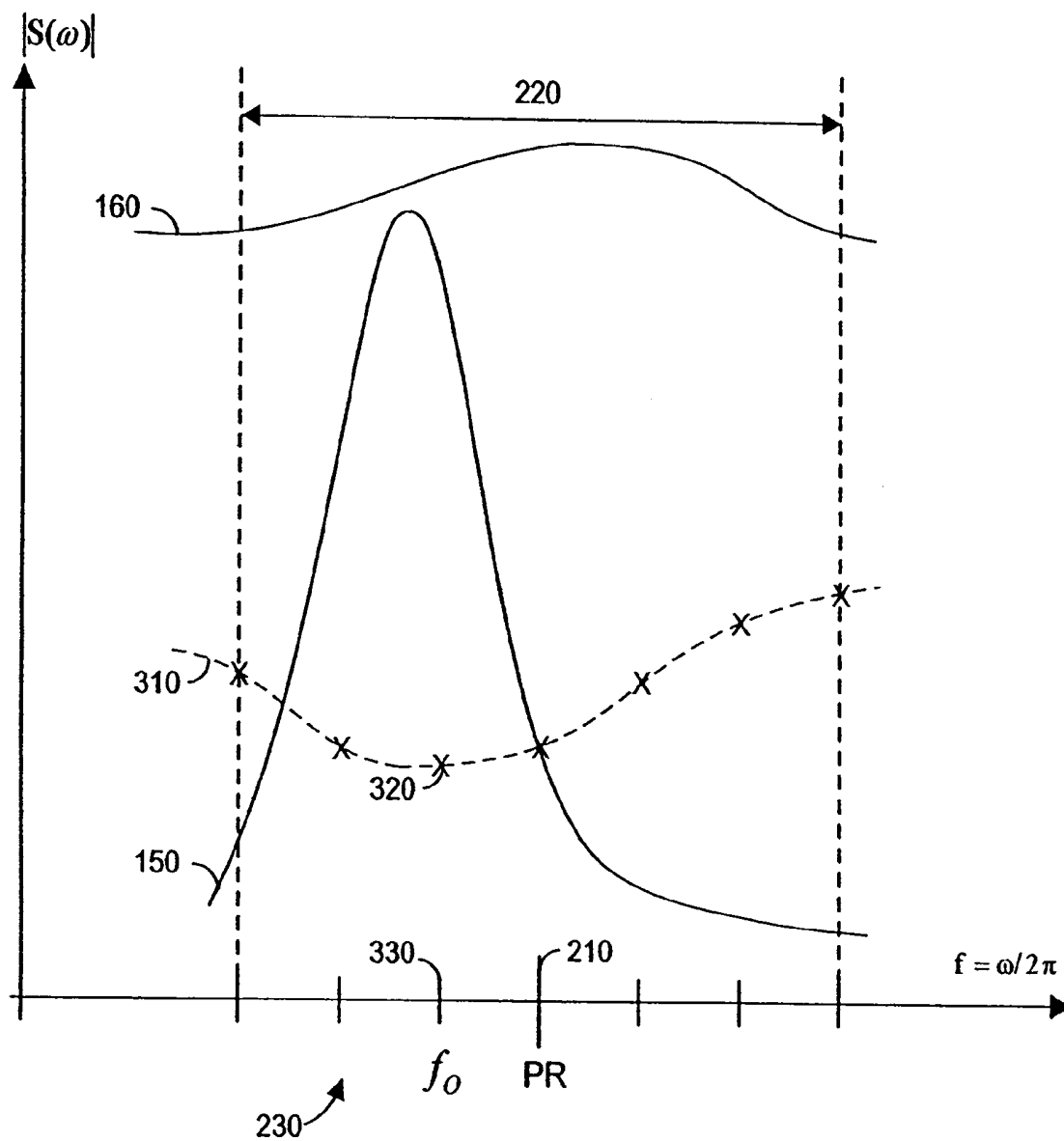


FIG. 3

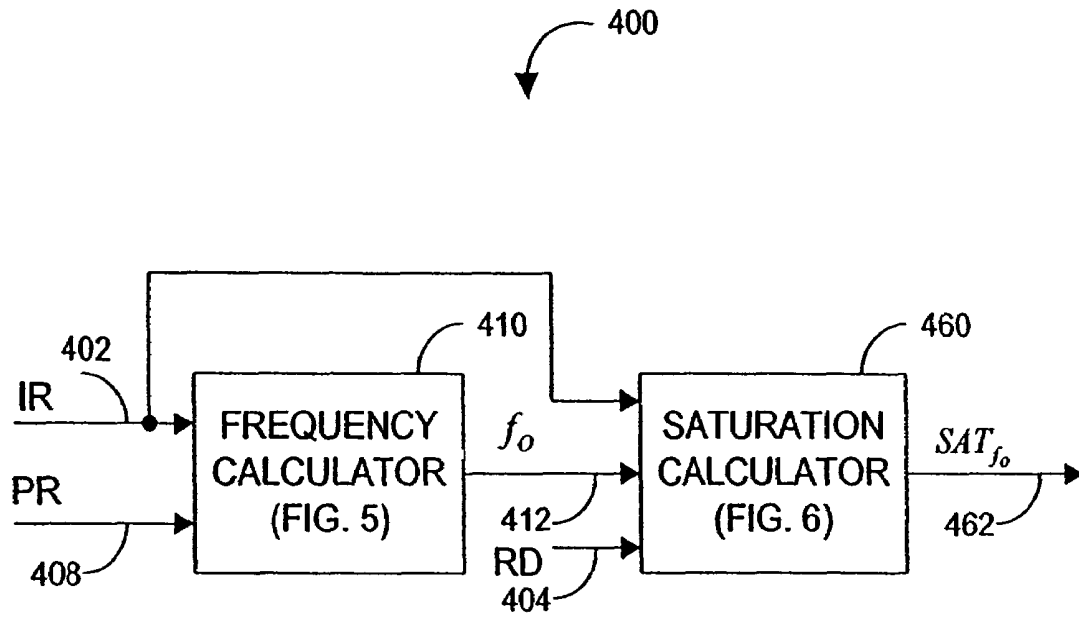


FIG. 4

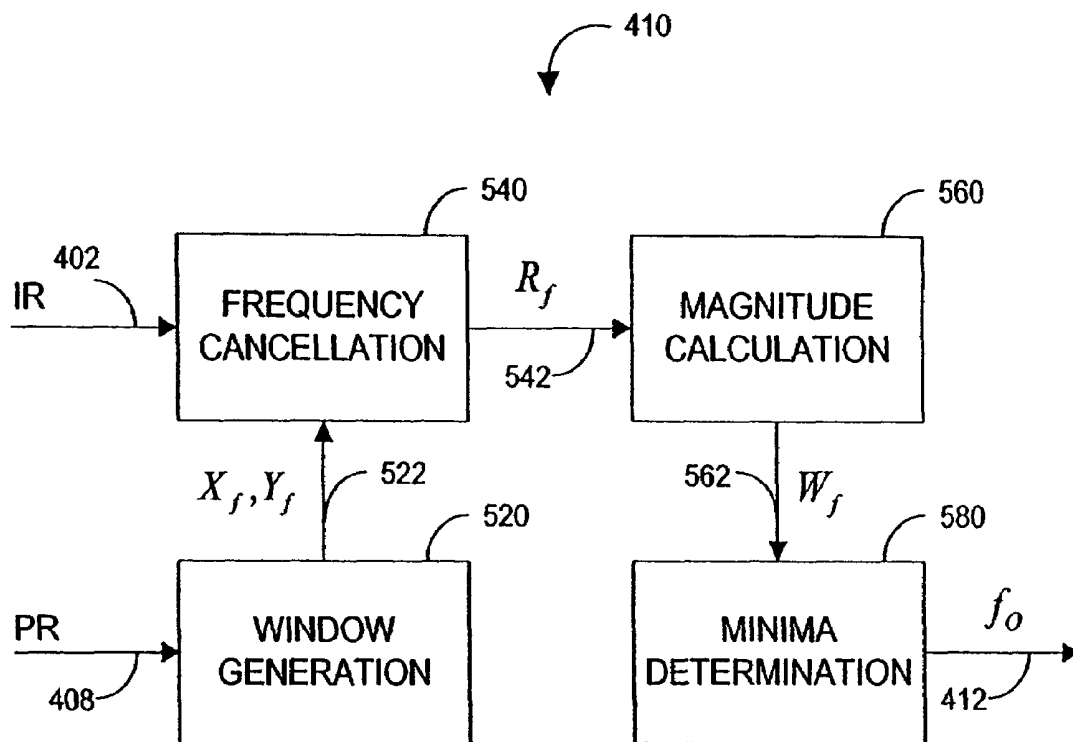


FIG. 5

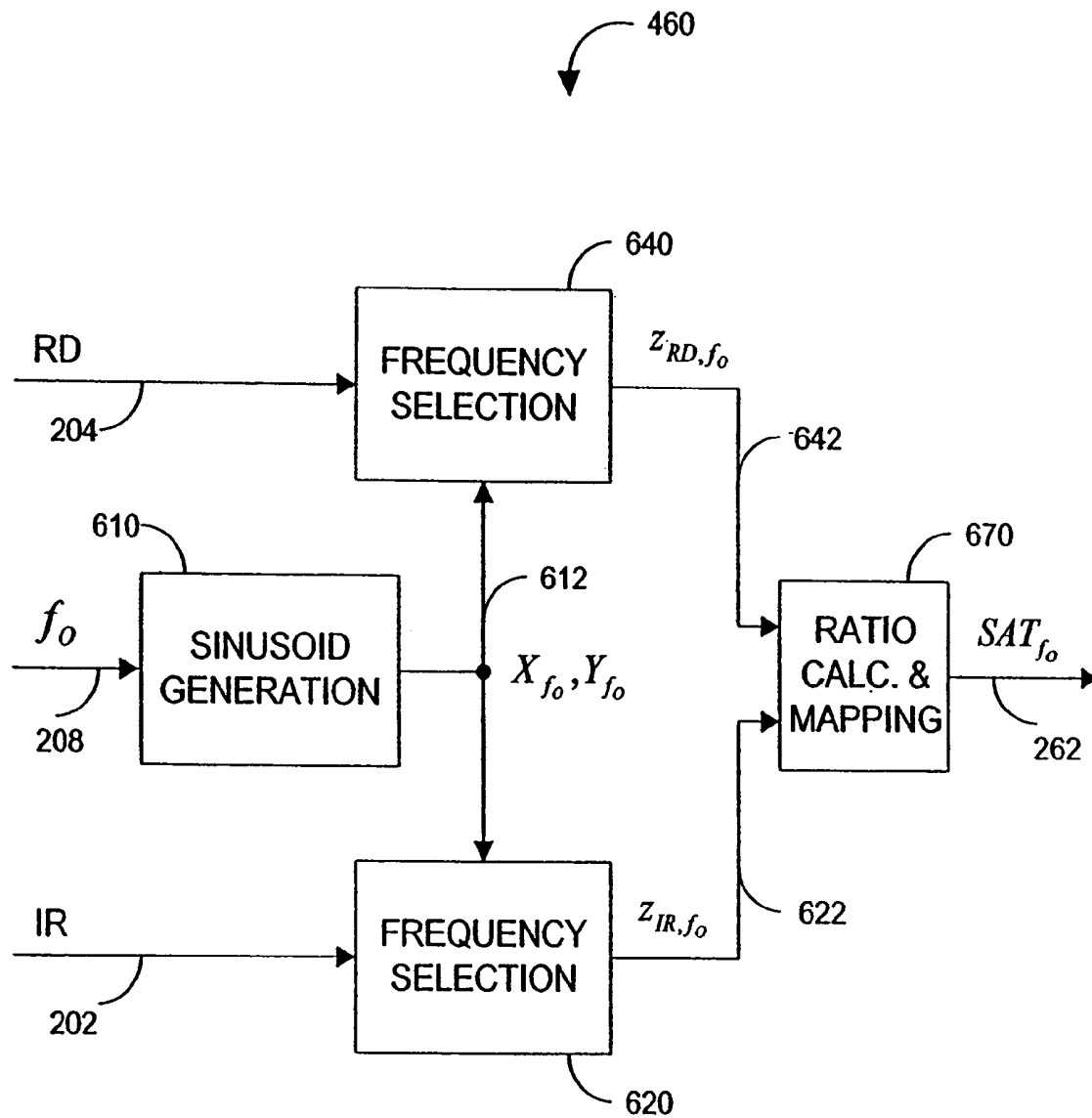


FIG. 6

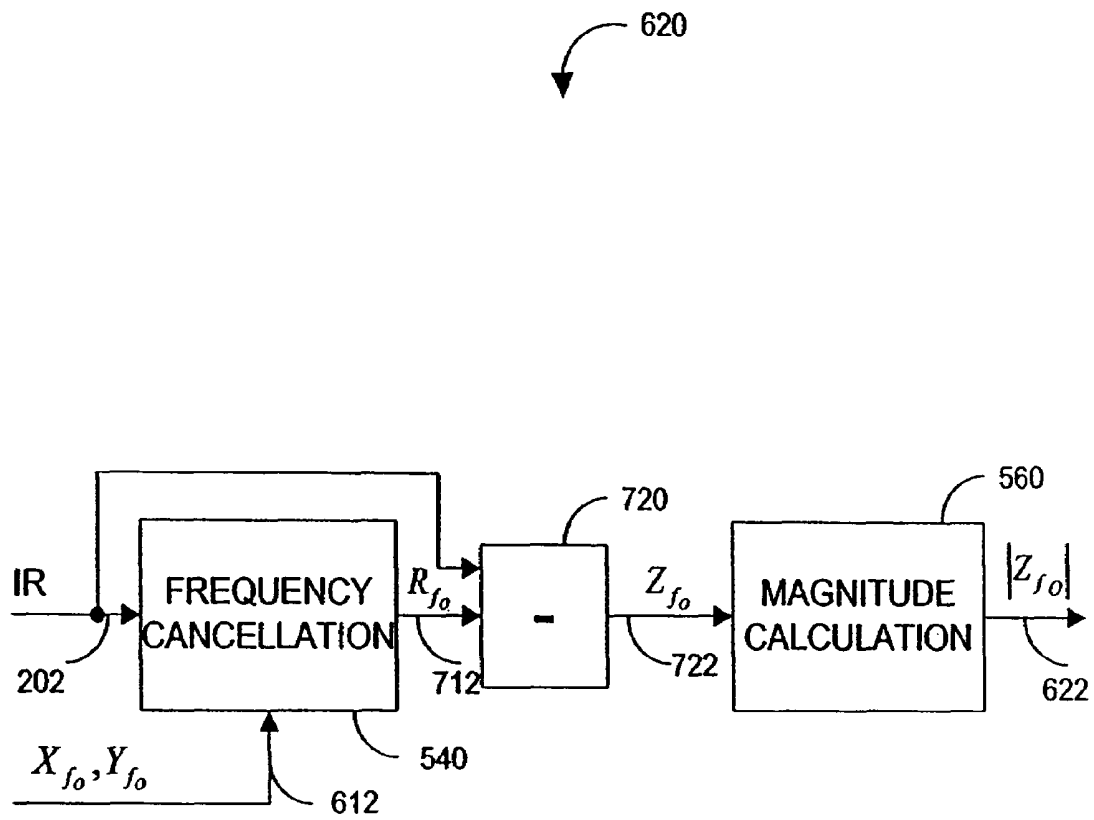


FIG. 7

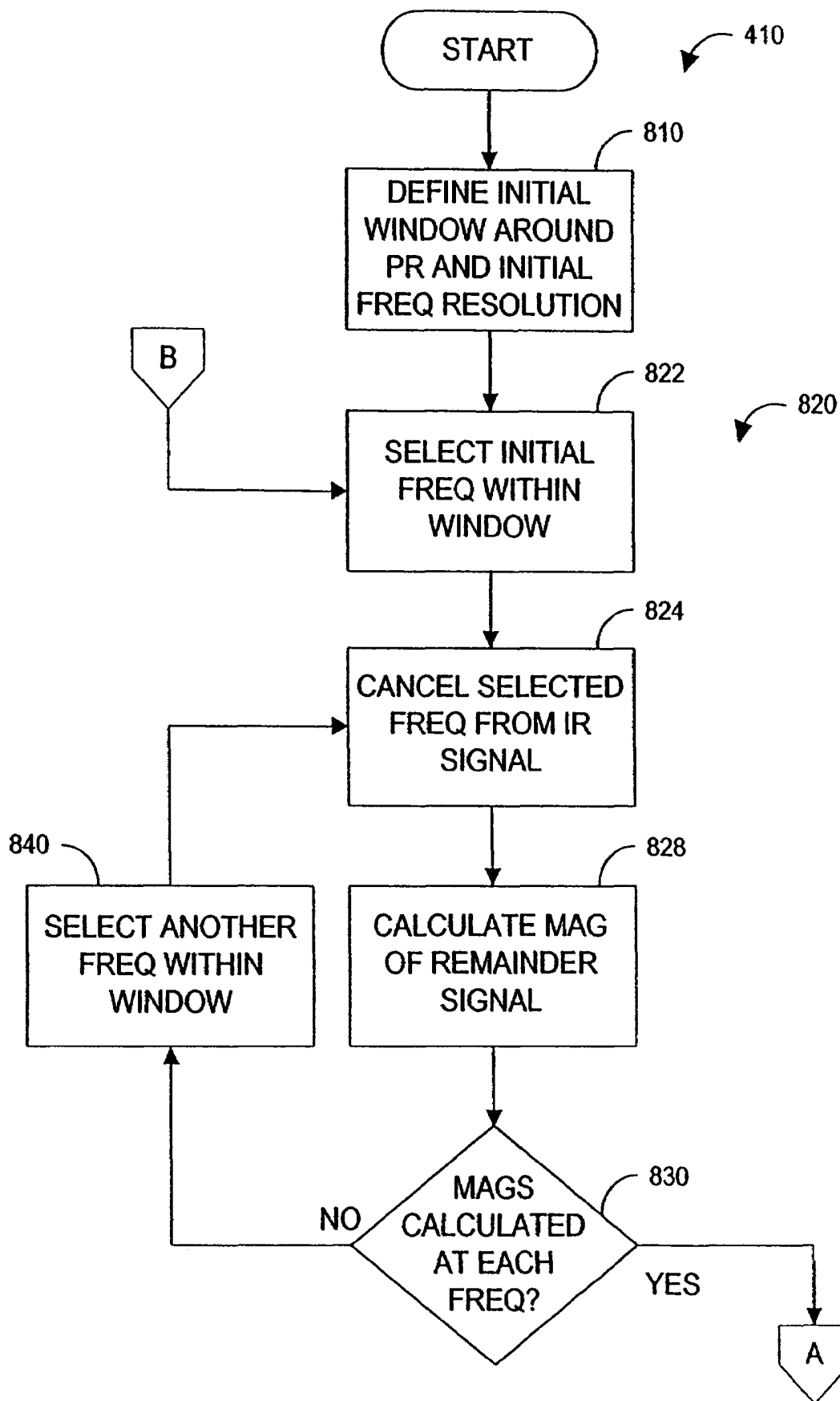


FIG. 8A

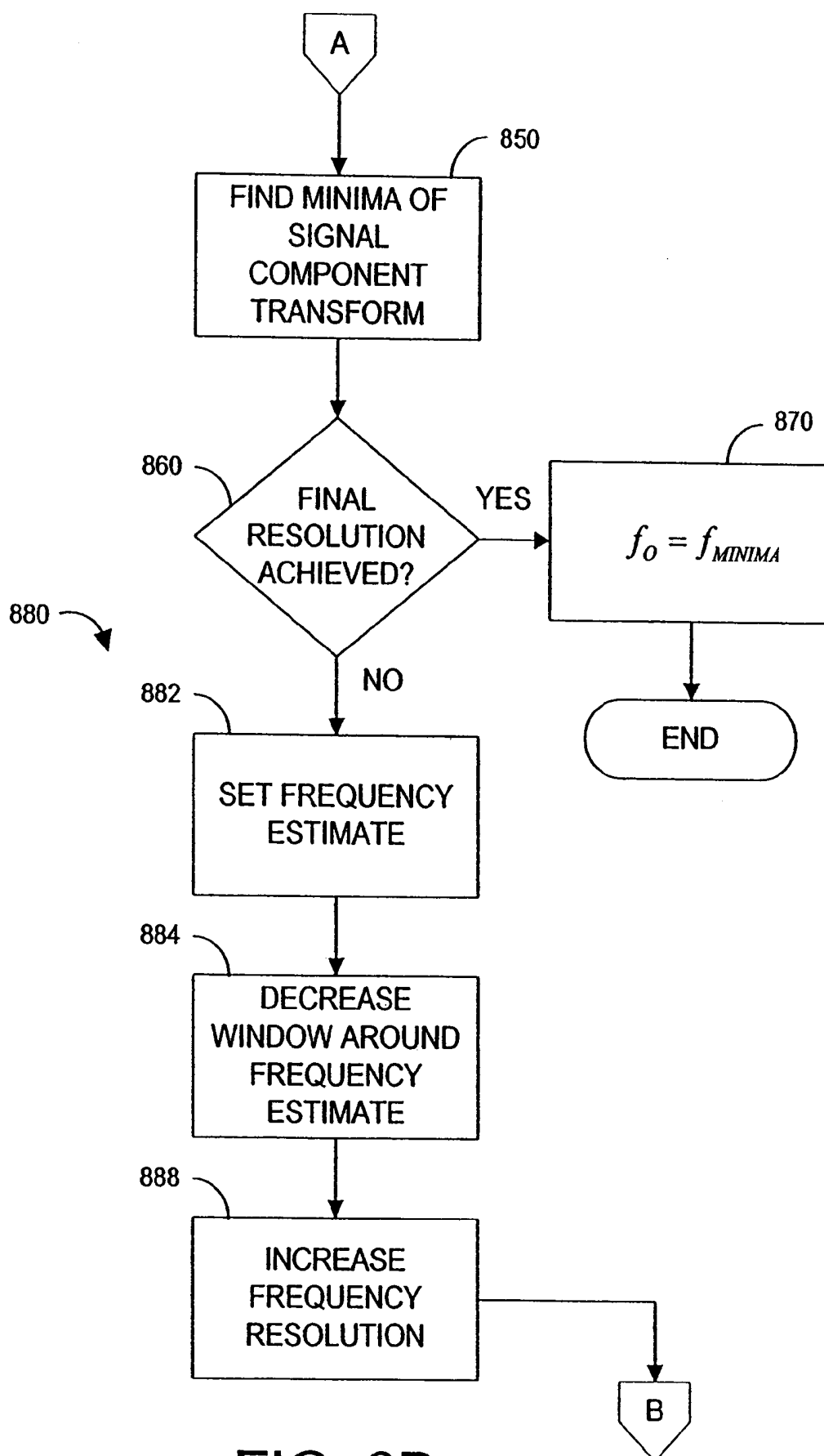


FIG. 8B

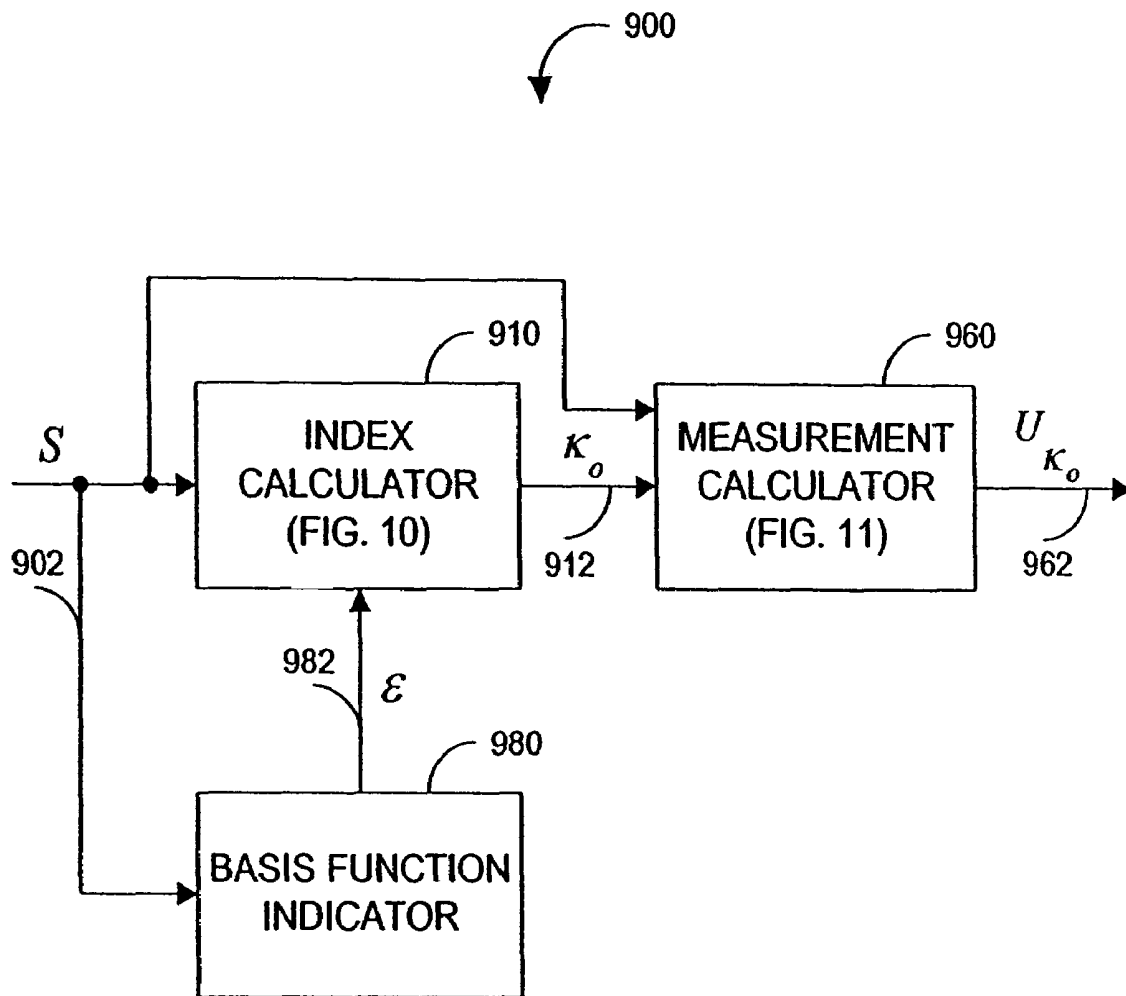


FIG. 9

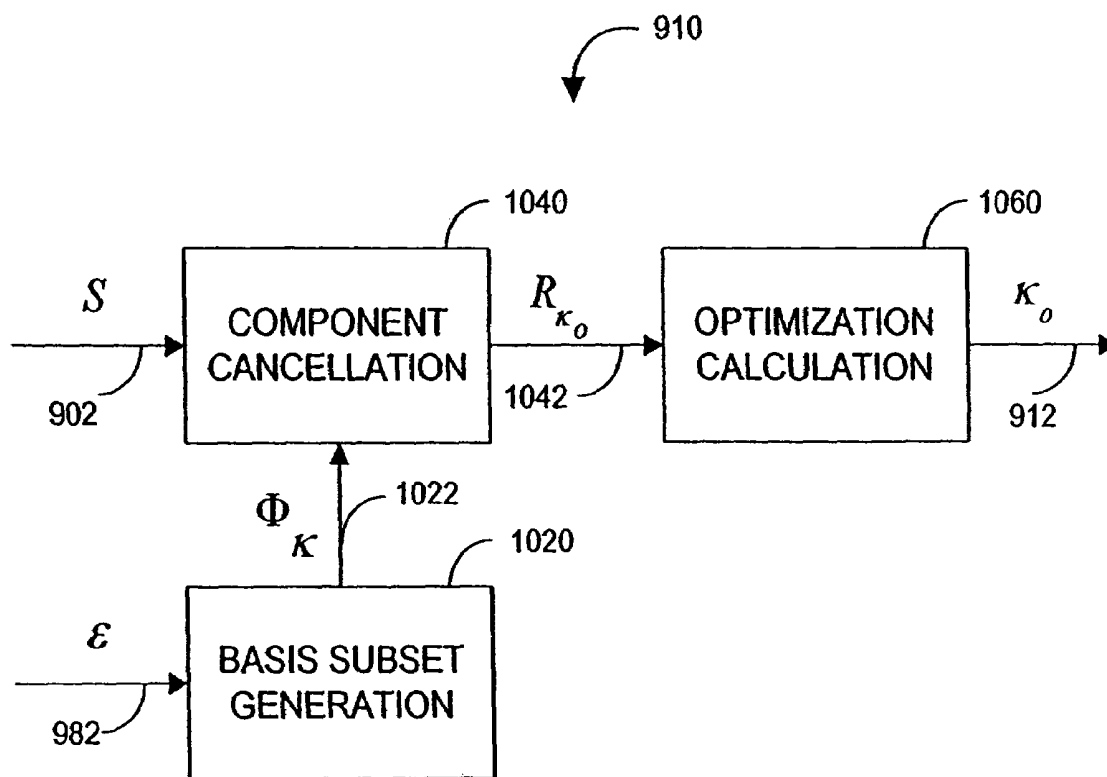


FIG. 10

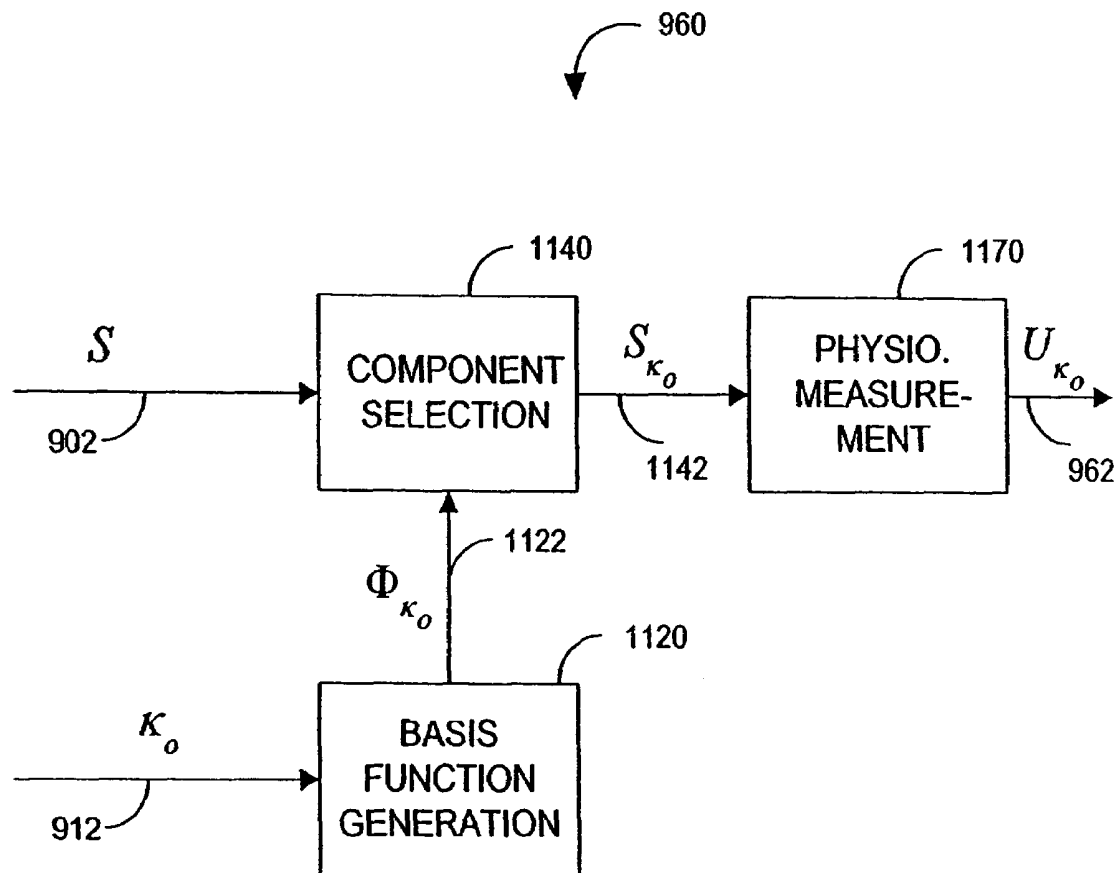


FIG. 11

SINE SATURATION TRANSFORM

PRIORITY CLAIM

The present application claims priority benefit under 35 U.S.C. § 120 to, and is a continuation of U.S. patent application Ser. No. 11/417,914, filed May 3, 2006, entitled "Sine Saturation Transform," which is a continuation of, U.S. patent application Ser. No. 11/048,232, filed Feb. 1, 2005, entitled "Signal Component Processor," which is a continuation of U.S. patent application Ser. No. 10/184,032, filed Jun. 26, 2002, entitled "Signal Component Processor," now U.S. Pat. No. 6,850,787, which claims priority benefit under 35 U.S.C. § 119(e) from U.S. Provisional Application No. 60/302,438, filed Jun. 29, 2001, entitled "Signal Component Processor." The present application also incorporates the foregoing disclosures herein by reference.

CROSS-REFERENCE TO RELATED APPLICATIONS

The following applications are currently pending: U.S. patent application Ser. No. 11/417,914, filed May 3, 2006, entitled "Sine Saturation Transform," and U.S. patent application Ser. No. 11/048,232, filed Feb. 1, 2005, entitled "Signal Component Processor."

BACKGROUND OF THE INVENTION

Early detection of low blood oxygen is critical in the medical field, for example in critical care and surgical applications, because an insufficient supply of oxygen can result in brain damage and death in a matter of minutes. Pulse oximetry is a widely accepted noninvasive procedure for measuring the oxygen saturation level of arterial blood, an indicator of oxygen supply. A pulse oximeter typically provides a numerical readout of the patient's oxygen saturation and pulse rate. A pulse oximetry system consists of a sensor attached to a patient, a monitor, and a cable connecting the sensor and monitor. Conventionally, a pulse oximetry sensor has both red (RD) and infrared (IR) light-emitting diode (LED) emitters and a photodiode detector. The pulse oximeter measurements are based upon the absorption by arterial blood of the two wavelengths emitted by the sensor. The pulse oximeter alternately activates the RD and IR sensor emitters and reads the resulting RD and IR sensor signals, i.e. the current generated by the photodiode in proportion to the detected RD and IR light intensity, in order to derive an arterial oxygen saturation value, as is well-known in the art. A pulse oximeter contains circuitry for controlling the sensor, processing the sensor signals and displaying the patient's oxygen saturation and pulse rate.

SUMMARY OF THE INVENTION

FIG. 1A illustrates a plethysmograph waveform **110**, which is a display of blood volume, shown along the ordinate **101**, over time, shown along the abscissa **102**. The shape of the plethysmograph waveform **110** is a function of heart stroke volume, pressure gradient, arterial elasticity and peripheral resistance. Ideally, the waveform **110** displays a short, steep inflow phase **111** during ventricular systole followed by a typically three to four times longer outflow phase **112** during diastole. A dicrotic notch **116** is generally attributed to closure of the aortic valve at the end of ventricular systole.

FIG. 1B illustrates a corresponding RD or IR sensor signal $s(t)$ **130**, such as described above. The typical plethysmograph waveform **110** (FIG. 1A), being a function of blood volume, also provides a light absorption profile. A pulse oximeter, however, does not directly detect light absorption and, hence, does not directly measure the plethysmograph waveform **110**. However, IR or RD sensor signals are 180° out-of-phase versions of the waveform **110**. That is, peak detected intensity **134** occurs at minimum absorption **114** and minimum detected intensity **138** occurs at maximum absorption **118**.

FIG. 1C illustrates the corresponding spectrum of $s(t)$, which is a display of signal spectral magnitude $|S(\omega)|$, shown along the ordinate **105**, versus frequency, shown along the abscissa **106**. The plethysmograph spectrum is depicted under both high signal quality **150** and low signal quality **160** conditions. Low signal quality can result when a pulse oximeter sensor signal is distorted by motion-artifact and noise. Signal processing technologies such as described in U.S. Pat. No. 5,632,272, assigned to the assignee of the present invention and incorporated by reference herein, allow pulse oximetry to function through patient motion and other low signal quality conditions.

Ideally, plethysmograph energy is concentrated at the pulse rate frequency **172** and associated harmonics **174**, **176**. Accordingly, motion-artifact and noise may be reduced and pulse oximetry measurements improved by filtering out sensor signal frequencies that are not related to the pulse rate. Under low signal quality conditions, however, the frequency spectrum is corrupted and the pulse rate fundamental **152** and harmonics **154**, **156** can be obscured or masked, resulting in errors in the computed pulse rate. In addition, a pulse rate, physiologically, is dynamic, potentially varying significantly between different measurement periods. Hence, maximum plethysmograph energy may not correspond to the computed pulse rate except under high signal quality conditions and stable pulse rates. Further, an oxygen saturation value calculated from an optical density ratio, such as a normalized red over infrared ratio, at the pulse rate frequency can be sensitive to computed pulse rate errors. In order to increase the robustness of oxygen saturation measurements, therefore, it is desirable to improve pulse rate based measurements by identifying sensor signal components that correspond to an optimization, such as maximum signal energy.

One aspect of a signal component processor comprises a physiological signal, a basis function index determined from the signal, a basis function waveform generated according to the index, a component derived from the sensor signal and the waveform, and a physiological measurement responsive to the component. In one embodiment, the component is responsive to the inner product of the sensor signal and the waveform. In another embodiment, the index is a frequency and the waveform is a sinusoid at the frequency. In that embodiment, the signal processor may further comprise a pulse rate estimate derived from the signal wherein the frequency is selected from a window including the pulse rate estimate. The physiological measurement may be an oxygen saturation value responsive to a magnitude of the component.

Another aspect of a signal component processor comprises a signal input, a basis function indicator derived from the signal input, a plurality of basis functions generated according to the indicator, a plurality of characteristics of the signal input corresponding to the basis functions and an optimization of the characteristics so as to identify at least one of said basis functions. In one embodiment, the indicator is a pulse rate estimate and the processor further comprises a window configured to include the pulse rate estimate, and a plurality

of frequencies selected from within the window. In another embodiment, the characteristic comprises a plurality of signal remainders corresponding to the basis functions and a plurality of magnitudes of the signal remainders. In that embodiment, the optimization comprises a minima of the magnitudes. In a further embodiment, the characteristic comprises a plurality of components corresponding to the basis functions and a plurality of magnitudes of the components. In this embodiment, the optimization comprises a maxima of the magnitudes.

An aspect of a signal component processing method comprises the steps of receiving a sensor signal, calculating an estimated pulse rate, determining an optimization of the sensor signal proximate the estimated pulse rate, defining a frequency corresponding to the optimization, and outputting a physiological measurement responsive to a component of the sensor signal at the frequency. In one embodiment the determining step comprises the substeps of transforming the sensor signal to a frequency spectrum encompassing the estimated pulse rate and detecting an extrema of the spectrum indicative of the frequency. The transforming step may comprise the substeps of defining a window including the estimated pulse rate, defining a plurality of selected frequencies within the window, canceling the selected frequencies, individually, from the sensor signal to generate a plurality of remainder signals and calculating a plurality of magnitudes of the remainder signals. The detecting step may comprise the substep of locating a minima of the magnitudes.

In another embodiment, the outputting step comprises the substeps of inputting a red (RD) portion and an infrared (IR) portion of the sensor signal, deriving a RD component of the RD portion and an IR component of the IR portion corresponding to the frequency and computing an oxygen saturation based upon a magnitude ratio of the RD component and the IR component. The deriving step may comprise the substeps of generating a sinusoidal waveform at the frequency and selecting the RD component and the IR component utilizing the waveform. The selecting step may comprise the substep of calculating the inner product between the waveform and the RD portion and the inner product between the waveform and the IR portion. The selecting step may comprise the substeps of canceling the waveform from the RD portion and the IR portion, leaving a RD remainder and an IR remainder, and subtracting the RD remainder from the RD portion and the IR remainder from the IR portion.

A further aspect of a signal component processor comprises a first calculator means for deriving an optimization frequency from a pulse rate estimate input and a sensor signal, and a second calculator means for deriving a physiological measurement responsive to a sensor signal component at the frequency. In one embodiment, the first calculator means comprises a signal component transform means for determining a plurality of signal values corresponding to a plurality of selected frequencies within a window including the pulse rate estimate, and a detection means for determining a particular one of the selected frequencies corresponding to an optimization of the sensor signal. The second calculator means may comprise a waveform means for generating a sinusoidal signal at the frequency, a frequency selection means for determining a component of the sensor signal from the sinusoidal signal and a calculator means for deriving a ratio responsive to the component.

BRIEF DESCRIPTION OF THE DRAWINGS

FIGS. 1A-C are graphical representations of a pulse oximetry sensor signal;

FIG. 1A is a typical plethysmograph illustrating blood volume versus time;

FIG. 1B is a pulse oximetry sensor signal illustrating detected light intensity versus time;

FIG. 1C is a pulse oximetry sensor signal spectrum illustrating both high signal quality and low signal quality conditions;

FIGS. 2-3 are magnitude versus frequency graphs for a pulse oximetry sensor signal illustrating an example of signal component processing;

FIG. 2 illustrates a frequency window around an estimated pulse rate; and

FIG. 3 illustrates an associated signal component transform;

FIGS. 4-7 are functional block diagrams of one embodiment of a signal component processor;

FIG. 4 is a top-level functional block diagram of a signal component processor;

FIG. 5 is a functional block diagram of a frequency calculator;

FIG. 6 is a functional block diagram of a saturation calculator; and

FIG. 7 is a functional block diagram of one embodiment of a frequency selection;

FIGS. 8A-B are flowcharts of an iterative embodiment of a frequency calculator; and

FIGS. 9-11 are functional block diagrams of another embodiment of a signal component processor;

FIG. 9 is a top-level functional block diagram of a signal component processor;

FIG. 10 is a functional block diagram of an index calculator; and

FIG. 11 is a functional block diagram of a measurement calculator.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIGS. 2 and 3 provide graphical illustration examples of signal component processing. Advantageously, signal component processing provides a direct method for the calculation of saturation based on pulse rate. For example, it is not necessary to compute a frequency transform, such as an FFT, which derives an entire frequency spectrum. Rather, signal component processing singles out specific signal components, as described in more detail below. Further, signal component processing advantageously provides a method of refinement for the calculation of saturation based on pulse rate.

FIG. 2 illustrates high and low signal quality sensor signal spectra **150**, **160** as described with respect to FIG. 1C, above. A frequency window **220** is created, including a pulse rate estimate **PR 210**. A pulse rate estimate can be calculated as disclosed in U.S. Pat. No. 6,002,952, entitled "Signal Processing Apparatus and Method," assigned to the assignee of the present invention and incorporated by reference herein. A search is conducted within this window **220** for a component frequency f_o at an optimization. In particular, selected frequencies **230**, which include **PR**, are defined within the window **220**. The components of a signal $s(t)$ at each of these frequencies **230** are then examined for an optimization indicative of an extrema of energy, power or other signal characteristic. In an alternative embodiment, the components of the signal $s(t)$ are examined for an optimization over a continuous range of frequencies within the window **220**.

FIG. 3 illustrates an expanded portion of the graph described with respect to FIG. 2, above. Superimposed on the

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high signal quality **150** and low signal quality **160** spectrums is a signal component transform **310**. In one embodiment, a signal component transform **310** is indicative of sensor signal energy and is calculated at selected signal frequencies **230** within the window **220**. A signal component transform **310** has an extrema **320** that indicates, in this embodiment, energy optimization at a particular one **330** of the selected frequencies **230**. The extrema **320** can be, for example, a maxima, minima or inflection point. In the embodiment illustrated, each point of the transform **310** is the magnitude of the signal remaining after canceling a sensor signal component at one of the selected frequencies. The extrema **320** is a minima, which indicates that canceling the corresponding frequency **330** removes the most signal energy. In an alternative embodiment, not illustrated, the transform **310** is calculated as the magnitude of signal components at each of the selected frequencies **230**. In that embodiment, the extrema is a maxima, which indicates the largest energy signal at the corresponding frequency. The result of a signal component transform **310** is identification of a frequency f_o **330** determined from the frequency of a signal component transform extrema **320**. Frequency f_o **330** is then used to calculate an oxygen saturation. A signal component transform and corresponding oxygen saturation calculations are described in additional detail with respect to FIGS. 4-8, below. Although signal component processing is described above with respect to identifying a particular frequency within a window including a pulse rate estimate PR, a similar procedure could be performed on 2PR, 3PR etc. resulting in the identification of multiple frequencies f_{o1} , f_{o2} , etc., which could be used for the calculation of oxygen saturation as well.

Advantageously, a signal component transform **310** is calculated over any set of selected frequencies, unrestricted by the number or spacing of these frequencies. In this manner, a signal component transform **310** differs from a FFT or other standard frequency transforms. For example, a FFT is limited to N evenly-distributed frequencies spaced at a resolution of f_s/N , where N is the number of signal samples and f_s is the sampling frequency. That is, for a FFT, a relatively high sampling rate or a relatively large record length or both are needed to achieve a relatively high resolution in frequency. Signal component processing, as described herein, is not so limited. Further, a signal component transform **310** is advantageously calculated only over a range of frequencies of interest. A FFT or similar frequency transformation may be computationally more burdensome than signal component processing, in part because such a transform is computed over all frequencies within a range determined by the sampling frequency, f_s .

FIGS. 4-7 illustrate one embodiment of a signal component processor. FIG. 4 is a top-level functional block diagram of a signal component processor **400**. The signal component processor **400** has a frequency calculator **410** and a saturation calculator **460**. The frequency calculator **410** has an IR signal input **402**, a pulse rate estimate signal PR input **408** and a component frequency f_o output **412**. The frequency calculator **410** performs a signal component transform based upon the PR input **408** and determines the f_o output **412**, as described with respect to FIGS. 2-3, above. The frequency calculator **410** is described in further detail with respect to FIG. 5, below.

In an alternative embodiment, the frequency calculator **410** determines f_o **412** based upon a RD signal input substituted for, or in addition to, the IR signal input **402**. Similarly, one of ordinary skill in the art will recognize that f_o can be determined by the frequency calculator **410** based upon one or more inputs responsive to a variety of sensor wavelengths.

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The saturation calculator **460** has an IR signal input **402**, a RD signal input **404**, a component frequency f_o input **412** and an oxygen saturation output, SAT_{f_o} **462**. The saturation calculator **460** determines values of the IR signal input **402** and the RD signal input **404** at the component frequency f_o **412** and computes a ratio of those values to determine SAT_{f_o} **462**, as described with respect to FIG. 6, below. The IR signal input **402** and RD signal input **404** can be expressed as:

$$IR = \begin{bmatrix} IR_0 \\ \vdots \\ IR_{N-1} \end{bmatrix}; \quad RD = \begin{bmatrix} RD_0 \\ \vdots \\ RD_{N-1} \end{bmatrix} \quad (1)$$

where N is the number of samples of each signal input.

FIG. 5 shows one embodiment of the frequency calculator **410**. In this particular embodiment, the frequency calculator functions are window generation **520**, frequency cancellation **540**, magnitude calculation **560** and minima determination **580**. Window generation **520**, frequency cancellation **540** and magnitude calculation **560** combine to create a signal component transform **310** (FIG. 3), as described with respect to FIG. 3, above. Minima determination **580** locates the signal component transform extrema **320** (FIG. 3), which identifies f_o **412**, also described with respect to FIG. 3, above.

As shown in FIG. 5, window generation **520** has a PR input **408** and defines a window **220** (FIG. 3) about PR **210** (FIG. 3) including a set of selected frequencies **230** (FIG. 3)

$$\{f_m; m = 0, \dots, M-1\}; \quad f = \begin{bmatrix} f_0 \\ \vdots \\ f_{M-1} \end{bmatrix} \quad (2)$$

where M is the number of selected frequencies **230** (FIG. 3) within the window **220** (FIG. 3). Window generation **520** has a sinusoidal output X_f, Y_f **522**, which is a set of sinusoidal waveforms $x_{n,f}, y_{n,f}$ each corresponding to one of the set of selected frequencies **230** (FIG. 3). Specifically

$$X_f = \begin{bmatrix} x_{0,f} \\ \vdots \\ x_{N-1,f} \end{bmatrix}; \quad Y_f = \begin{bmatrix} y_{0,f} \\ \vdots \\ y_{N-1,f} \end{bmatrix} \quad (3a)$$

$$x_{n,f} = \sin(2\pi f n); \quad y_{n,f} = \cos(2\pi f n) \quad (3b)$$

Also shown in FIG. 5, the frequency cancellation **540** has IR **402** and X_f, Y_f **522** inputs and a remainder output R_f **542**, which is a set of remainder signals $r_{n,f}$ each corresponding to one of the sinusoidal waveforms $x_{n,f}, y_{n,f}$. For each selected frequency f **230** (FIG. 3), frequency cancellation **540** cancels that frequency component from the input signal IR **402** to generate a remainder signal $r_{n,f}$. In particular, frequency cancellation **540** generates a remainder R_f **542**

$$R_f = \begin{bmatrix} r_{0,f} \\ \vdots \\ r_{N-1,f} \end{bmatrix} \quad (4a)$$

-continued

$$R_f = IR - \frac{IR \cdot X_f}{|X_f|^2} X_f - \frac{IR \cdot Y_f}{|Y_f|^2} Y_f \quad (4b)$$

Additionally, as shown in FIG. 5, the magnitude calculation 560 has a remainder input R_f 542 and generates a magnitude output W_f 562, where

$$W_f = |R_f| = \sqrt{\sum_{n=0}^{N-1} r_{n,f}^2} \quad (5)$$

Further shown in FIG. 5, the minima determination 580 has the magnitude values W_f 562 as inputs and generates a component frequency f_o output. Frequency f_o is the particular frequency associated with the minimum magnitude value

$$W_{f_o} = \min \{W_f\} \quad (6)$$

FIG. 6 shows that the saturation calculator 460 functions are sinusoid generation 610, frequency selection 620, 640 and ratio calculation 670. Sinusoid generation has a component frequency f_o input 208 and a sinusoidal waveform X_{f_o}, Y_{f_o} output 612, which has a frequency of f_o . Frequency selection 620, 640 has a sensor signal input, which is either an IR signal 202 or a RD signal 204 and a sinusoid waveform X_{f_o}, Y_{f_o} input 612. Frequency selection 620, 640 provides magnitude outputs Z_{IR,f_o} 622 and Z_{RD,f_o} 642 which are the frequency components of the IR 202 and RD 204 sensor signals at the f_o frequency. Specifically, from equation 3(a)

$$X_{f_o} = \begin{bmatrix} x_{0,f_o} \\ \vdots \\ x_{N-1,f_o} \end{bmatrix}; \quad Y_{f_o} = \begin{bmatrix} y_{0,f_o} \\ \vdots \\ y_{N-1,f_o} \end{bmatrix} \quad (7)$$

Then, referring to equation 1

$$Z_{IR,f_o} = \left| \frac{IR \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} + \frac{IR \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o} \right| \quad (8a)$$

$$= \sqrt{\frac{(IR \cdot X_{f_o})^2}{|X_{f_o}|^2} + \frac{(IR \cdot Y_{f_o})^2}{|Y_{f_o}|^2}}$$

$$Z_{RD,f_o} = \left| \frac{RD \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} + \frac{RD \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o} \right| \quad (8b)$$

$$= \sqrt{\frac{(RD \cdot X_{f_o})^2}{|X_{f_o}|^2} + \frac{(RD \cdot Y_{f_o})^2}{|Y_{f_o}|^2}}$$

For simplicity of illustration, EQS. 8a-b assume that the cross-product of X_{f_o} and Y_{f_o} is zero, although generally this is not the case. The ratio calculation and mapping 670 has Z_{IR,f_o} 622 and Z_{RD,f_o} 642 as inputs and provides SAT $_{f_o}$ 262 as an output. That is

$$SAT_{f_o} = g\{Z_{RD,f_o}/Z_{IR,f_o}\} \quad (9)$$

where g is a mapping of the red-over-IR ratio to oxygen saturation, which may be an empirically derived lookup table, for example.

FIG. 7 illustrates an alternative embodiment of frequency selection 620 (FIG. 6), as described above. In this embodiment, frequency cancellation 540 and magnitude calculation 560, as described with respect to FIG. 5, can also be used,

advantageously, to perform frequency selection. Specifically, frequency cancellation 540 has IR 202 and X_{f_o}, Y_{f_o} 612 as inputs and generates a remainder signal R_{f_o} 712 as an output, where

$$R_{f_o} = IR - \frac{IR \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} - \frac{IR \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o} \quad (10)$$

The remainder R_{f_o} 712 is subtracted 720 from IR 202 to yield

$$Z_{f_o} = IR - \left[\frac{IR \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} + \frac{IR \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o} \right] \quad (11)$$

$$= \frac{IR \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} + \frac{IR \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o}$$

where Z_{f_o} 722 is the component of IR 202 at the f_o frequency. The magnitude calculation 560 has Z_{f_o} 722 as an input and calculates

$$|Z_{f_o}| = \left| \frac{IR \cdot X_{f_o}}{|X_{f_o}|^2} X_{f_o} + \frac{IR \cdot Y_{f_o}}{|Y_{f_o}|^2} Y_{f_o} \right| \quad (12)$$

$$= \sqrt{\frac{(IR \cdot X_{f_o})^2}{|X_{f_o}|^2} + \frac{(IR \cdot Y_{f_o})^2}{|Y_{f_o}|^2}}$$

which is equivalent to equation 8a, above.

FIGS. 8A-B illustrate an iterative embodiment of the frequency calculator 410 (FIG. 4) described above. An iterative frequency calculator 410 has an initialization 810, a signal component transform 820, an extrema detection 850, a resolution decision 860 and a resolution refinement 880 and provides a component frequency f_o 870. Initialization 810 defines a window around the pulse rate estimate PR and a frequency resolution within that window.

As shown in FIG. 8A, a signal component transform 820 has an initial frequency selection 822, a frequency cancellation 824 and an magnitude calculation 828. A decision block 830 determines if the magnitude calculation 828 has been performed at each frequency within the window. If not, the loop of frequency cancellation 824 and magnitude calculation 828 is repeated for another selected frequency in the window. The frequency cancellation 824 removes a frequency component from the IR sensor signal, as described with respect to FIG. 5, above. The magnitude calculation 828 determines the magnitude of the remainder signal, also described with respect to FIG. 5, above. If the decision block 830 determines that the remainder signal magnitudes have been calculated at each of the selected frequencies, then the signal component transform loop 820 is exited to the steps described with respect to FIG. 8B.

As shown in FIG. 8B, the extrema detector 850 finds a minima of a signal component transform 820 and a resolution decision block 860 determines if the final frequency resolution of a signal component transform is achieved. If not, resolution refinement 880 is performed. If the final resolution is achieved, the component frequency output f_o is equated to the frequency of the minima 870, i.e. a signal component transform minima determined by the extrema detector 850.

Further shown in FIG. 8B, the resolution refinement 880 has a set frequency estimate 882, a window decrease 884 and a frequency resolution increase 888. Specifically, the fre-

quency estimate **882** is set to a signal component transform minima, as determined by the extrema detector **850**. The window decrease **884** defines a new and narrower window around the frequency estimate, and the frequency resolution increase **888** reduces the spacing of the selected frequencies within that window prior to the next iteration of a signal component transform **820**. In this manner, a signal component transform **820** and the resulting frequency estimate are refined to a higher resolution with each iteration of signal component transform **820**, extrema detection **850**, and resolution refinement **880**.

In a particular embodiment, the component calculation requires three iterations. A frequency resolution of 4 beats per minute or 4 BPM is used initially and a window of five or seven selected frequencies, including that of the initial pulse rate estimate PR, is defined. That is, a window of either 16 BPM or 24 BPM centered on PR is defined, and a signal component transform is computed for a set of 5 or 7 selected frequencies evenly spaced at 4 BPM. The result is a frequency estimate f_1 . Next, the frequency resolution is reduced from 4 BPM to 2 BPM and a 4 BPM window centered on f_1 is defined with three selected frequencies, i.e. $f_1 - 2$ BPM, f_1 , and $f_1 + 2$ BPM. The result is a higher resolution frequency estimate f_2 . On the final iteration, the frequency resolution is reduced to 1BPM and a 2 BPM window centered on f_2 is defined with three selected frequencies, i.e. $f_2 - 1$ BPM, f_2 , and $f_2 + 1$ BPM. The final result is the component frequency f_o determined by a signal component transform to within a 1BPM resolution. This component frequency f_o is then used to calculate the oxygen saturation, SAT_{f_o} , as described above.

The signal component processor has been described above with respect to pulse oximetry and oxygen saturation measurements based upon a frequency component that optimizes signal energy. The signal component processor, however, is applicable to other physiological measurements, such as blood glucose, carboxy-hemoglobin, respiration rate and blood pressure to name a few. Further, the signal component processor is generally applicable to identifying, selecting and processing any basis function signal components, of which single frequency components are one embodiment, as described in further detail with respect to FIG. 9, below.

FIGS. 9-11 illustrate another embodiment of a signal component processor **900**. As shown in FIG. 9, the processor **900** has an index calculator **910** and a measurement calculator **960**. The index calculator has a sensor signal input **S 902** and outputs a basis function index κ_o **912**, as described with respect to FIG. 10, below. The measurement calculator **960** inputs the basis function index κ_o **912** and outputs a physiological measurement U_{κ_o} **962**, as described with respect to FIG. 11, below. The processor **900** also has a basis function indicator **980**, which is responsive to the sensor signal input **S 902** and provides a parameter ϵ **982** that indicates a set of basis functions to be utilized by the index calculator **910**, as described with respect to FIG. 10, below.

As shown in FIG. 10, the functions of the index calculator **910** are basis subset generation **1020**, component cancellation **1040** and optimization calculation **1060**. The basis subset generation **1020** outputs a subset Φ_{κ} **1022** of basis function waveforms corresponding to a set of selected basis function indices κ . The basis functions can be any complete set of functions such that

$$S = \sum_{\kappa} a_{\kappa} \Phi_{\kappa} \quad (13)$$

For simplicity of illustration purposes, these basis functions are assumed to be orthogonal

$$\langle \vec{\Phi}_{\gamma}, \vec{\Phi}_{\eta} \rangle = 0; \gamma \neq \eta \quad (14)$$

where $\langle \rangle$ denotes an inner product. As such

$$a_{\kappa} = \langle S, \Phi_{\kappa} \rangle / \langle \Phi_{\kappa}, \Phi_{\kappa} \rangle \quad (15)$$

$$S_{\kappa} = a_{\kappa} \Phi_{\kappa} \quad (16)$$

In general, the basis functions may be non-orthogonal. The subset of basis functions generated is determined by an input parameter ϵ **982**. In the embodiment described with respect to FIG. 5, above, the basis functions are sinusoids, the indices are the sinusoid frequencies and the input parameter ϵ **982** is a pulse rate estimate that determines a frequency window.

As shown in FIG. 10, the component cancellation **1040** generates a remainder output R_{κ} **1042**, which is a set of remainder signals corresponding to the subset of basis function waveforms Φ_{κ} **1022**. For each basis function waveform generated, component cancellation removes the corresponding basis function component from the sensor signal **S 902** to generate a remainder signal. In an alternative embodiment, component cancellation **1040** is replaced with a component selection that generates a corresponding basis function component of the sensor signal **S 902** for each basis function generated. The optimization calculation **1060** generates a particular index κ_o **912** associated with an optimization of the remainders R_{κ} **1042** or, alternatively, an optimization of the selected basis function signal components.

As shown in FIG. 11, the functions of the measurement calculator **960** are basis function generation **1120**, component selection **1140**, and physiological measurement calculation **1170**. The component selection **1140** inputs the sensor signal **S 902** and a particular basis function waveform Φ_{κ_o} **1122** and outputs a sensor signal component S_{κ_o} **1142**. The physiological measurement **1170** inputs the sensor signal component S_{κ_o} **1142** and outputs the physiological measurement U_{κ_o} **962**, which is responsive to the sensor signal component S_{κ_o} **1142**. In the embodiment described with respect to FIG. 6, above, the basis functions Φ_{κ} are sinusoids and the index κ_o is a particular sinusoid frequency. The basis function generation **1120** creates sine and cosine waveforms at this frequency. The component selection **1140** selects corresponding frequency components of the sensor signal portions, RD and IR. Also, the physiological measurement **1170** computes an oxygen saturation based upon a magnitude ratio of these RD and IR frequency components.

The signal component processor has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

What is claimed is:

1. A method for filtering a physiological signal to improve a calculation of a pulse rate, the method comprising:
 - obtaining within a patient monitor a signal indicative of pulse rate information of a patient being monitored;
 - obtaining an initial frequency estimate of a pulse rate of the patient with a processor;

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combining at least one sinusoidal waveform with said signal to produce a predetermined response; and signal component processing the combined signal with the processor to determine said pulse rate.

2. The method of claim 1, comprising generating one or more sinusoidal waves as the at least one sinusoidal waveform.

3. The method of claim 2, comprising individually canceling the generated sinusoidal waves from the signal.

4. The method of claim 1, wherein said signal component processing includes determining a frequency corresponding to the sinusoidal waveform which produces an extrema.

5. The method of claim 1, comprising segmenting the signal into at least one pulse rate cycle.

6. The method of claim 4, wherein the extrema comprises a minima.

7. The method of claim 1, wherein said signal component processing includes determining an oxygen saturation.

8. A signal component processor capable of determining a pulse rate of a patient being monitored, the processor comprising:

at least one input capable of receiving a signal indicative of pulse rate information of a patient being monitored; and a frequency calculator configured to determine an initial frequency estimate of a pulse rate of the patient, config-

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ured to combine at least one sinusoidal waveform with said signal to produce a predetermined response, and configured to component process the combined signal to determine said pulse rate.

9. The processor of claim 8, wherein the frequency calculator is further configured to generate one or more sinusoidal waves as the at least one sinusoidal waveform.

10. The processor of claim 9, wherein the frequency calculator is further configured to individually cancel the generated sinusoidal waves from the signal.

11. The processor of claim 8, wherein the frequency calculator is further configured to determine a frequency corresponding to the sinusoidal waveform which produces an extrema.

12. The processor of claim 11, wherein the extrema comprises a minima.

13. The processor of claim 8, wherein the frequency calculator is further configured to segment the signal into at least one pulse rate cycle.

14. The processor of claim 8, comprising a saturation calculator configured to process said at least one input signal using said pulse rate to determine an oxygen saturation of the patient.

* * * * *

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摘要(译)

公开了一种用于确定生理测量的变换。变换根据通过生理传感器获得的生理信号确定基函数指数。基于基函数索引生成基函数波形。然后使用基函数波形来确定优化的基函数波形。优化的基函数波形用于计算生理测量。

