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(54) **ULTRASOUND MEDICAL SYSTEM**

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(56) **References Cited**

U.S. PATENT DOCUMENTS

3,168,659 A 2/1965 Bayre et al.
3,902,501 A 9/1975 Citron et al.
3,927,557 A 12/1975 Viertl
4,315,514 A 2/1982 Drewes et al.
4,323,077 A 4/1982 Smith

4,396,019 A 8/1983 Perry, Jr.
4,484,569 A 11/1984 Driller et al.
4,646,756 A 3/1987 Watnough et al.
4,748,985 A 6/1988 Nagasaki
4,757,820 A 7/1988 Itoh
4,765,331 A 8/1988 Petrucci et al.
4,787,394 A 11/1988 Ogura
4,798,215 A 1/1989 Turner
4,818,954 A 4/1989 Flachenecker et al.
4,844,080 A 7/1989 Frass et al.
4,858,613 A 8/1989 Fry et al.
4,932,414 A 6/1990 Coleman et al.
4,937,767 A 6/1990 Reuschel et al.
4,951,653 A 8/1990 Fry et al.
4,955,365 A 9/1990 Fry et al.
4,955,366 A 9/1990 Uchiyama et al.

(Continued)

FOREIGN PATENT DOCUMENTS

CN 1628615 6/2005

(Continued)

OTHER PUBLICATIONS

Chavrier et al., "Modeling of high-intensity focused ultrasound-in-
duced lesions in the presence of cavitation bubbles," J. Acoust. Soc.
Am. 108 (1), pp. 432-440 (Jul. 2000).

(Continued)

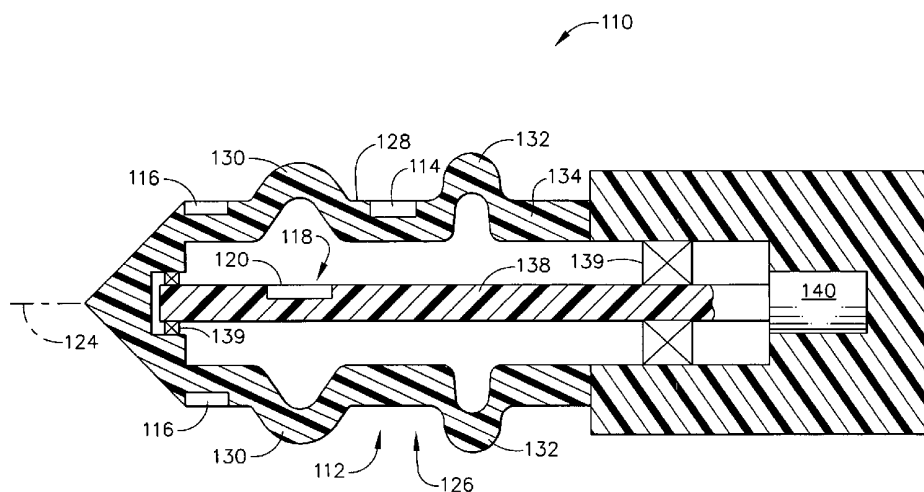
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Assistant Examiner — Vani Gupta

(57) **ABSTRACT**

An ultrasound medical system includes an ultrasound end
effector and at least one non-ultrasound tissue-property-meas-
uring sensor. The ultrasound end effector includes a medical
ultrasound transducer assembly having at least one medical-
treatment ultrasound transducer. The at-least-one non-ultra-
sound tissue-property-measuring sensor is supported by the
ultrasound end effector and is positionable in contact with
patient tissue.

13 Claims, 6 Drawing Sheets



U.S. PATENT DOCUMENTS					
4,960,107	A	10/1990	Aida et al.	5,649,547	A 7/1997 Ritchart et al.
4,960,109	A *	10/1990	Lele 600/549	5,657,760	A 8/1997 Ying et al.
4,984,575	A	1/1991	Uchiyama et al.	5,665,054	A 9/1997 Dory
4,986,275	A	1/1991	Ishida et al.	5,666,954	A 9/1997 Chapelon et al.
RE33,590	E	5/1991	Dory	5,676,692	A 10/1997 Sanghvi et al.
5,015,929	A	5/1991	Cathignol et al.	5,687,729	A 11/1997 Schaetzle
5,036,855	A	8/1991	Fry et al.	5,694,936	A 12/1997 Fujimoto et al.
5,054,470	A	10/1991	Fry et al.	5,697,897	A 12/1997 Buchholtz et al.
5,065,740	A	11/1991	Itoh	5,699,804	A 12/1997 Rattner
5,078,144	A	1/1992	Sekino et al.	5,703,922	A 12/1997 Rattner
5,080,101	A	1/1992	Dory	5,715,825	A 2/1998 Crowley
5,080,102	A	1/1992	Dory	5,720,287	A 2/1998 Chapelon et al.
5,095,907	A	3/1992	Kudo et al.	5,722,411	A 3/1998 Suzuki et al.
5,117,832	A	6/1992	Sanghvi et al.	5,728,062	A 3/1998 Briskeen
5,143,073	A	9/1992	Dory	5,733,315	A 3/1998 Burdette et al.
5,143,074	A	9/1992	Dory	5,735,280	A 4/1998 Sherman et al.
5,149,319	A	9/1992	Unger	5,735,796	A 4/1998 Granz et al.
5,150,711	A	9/1992	Dory	5,738,635	A 4/1998 Chapelon et al.
5,150,712	A	9/1992	Dory	5,743,862	A 4/1998 Izumi
5,158,070	A	10/1992	Dory	5,743,863	A 4/1998 Chapelon
5,158,071	A	10/1992	Umemura et al.	5,746,224	A 5/1998 Edwards
5,203,333	A	4/1993	Nomura	5,759,154	A 6/1998 Hoyns
5,209,221	A	5/1993	Riedlinger	5,759,162	A 6/1998 Oppelt et al.
5,238,007	A	8/1993	Giele et al.	5,762,066	A 6/1998 Law et al.
5,240,005	A	8/1993	Viebach	5,769,086	A 6/1998 Ritchart et al.
5,242,437	A	9/1993	Everett et al.	5,769,790	A 6/1998 Watkins et al.
5,295,484	A	3/1994	Marcus et al.	5,771,896	A 6/1998 Sliwa et al.
5,304,115	A	4/1994	Pflueger et al.	5,785,705	A 7/1998 Baker
5,305,731	A	4/1994	Buchholtz	5,788,636	A 8/1998 Curley
5,311,869	A	5/1994	Okazaki	5,800,379	A 9/1998 Edwards
5,348,017	A *	9/1994	Thornton et al. 600/467	5,800,429	A 9/1998 Edwards
5,354,258	A	10/1994	Dory	5,807,308	A 9/1998 Edwards
5,391,140	A	2/1995	Schaetzle et al.	5,817,021	A 10/1998 Reichenberger
5,391,197	A	2/1995	Burdette et al.	5,817,049	A 10/1998 Edwards
5,402,792	A	4/1995	Kimura	5,820,580	A 10/1998 Edwards et al.
5,409,002	A	4/1995	Pell	5,823,962	A 10/1998 Schaetzle et al.
5,413,550	A	5/1995	Castel	5,836,896	A 11/1998 Rosenschein
5,419,335	A	5/1995	Hartmann et al.	5,840,031	A 11/1998 Crowley
5,431,663	A	7/1995	Carter	5,842,994	A 12/1998 TenHoff et al.
5,435,304	A	7/1995	Oppelt et al.	5,860,974	A 1/1999 Abele
5,435,311	A	7/1995	Umemura et al.	5,873,828	A 2/1999 Fujio et al.
5,443,069	A	8/1995	Schaetzle	5,873,845	A 2/1999 Cline et al.
5,448,994	A	9/1995	Iinuma	5,873,902	A 2/1999 Sanghvi et al.
5,458,597	A	10/1995	Edwards et al.	5,876,399	A 3/1999 Chia et al.
5,465,724	A	11/1995	Sliwa et al.	5,882,302	A 3/1999 Driscoll, Jr. et al.
5,471,988	A	12/1995	Fujio et al.	5,895,356	A 4/1999 Andrus et al.
5,474,071	A	12/1995	Chapelon et al.	5,897,495	A 4/1999 Aida et al.
5,485,839	A	1/1996	Aida et al.	5,897,523	A 4/1999 Wright et al.
5,492,126	A	2/1996	Hennige et al.	5,925,044	A 7/1999 Hofmann et al.
5,500,012	A	3/1996	Brucker et al.	5,928,169	A 7/1999 Schatzle et al.
5,501,655	A	3/1996	Rolt et al.	5,931,848	A 8/1999 Saadat
5,514,085	A	5/1996	Yoon	5,938,600	A 8/1999 Van Vaals et al.
5,514,130	A	5/1996	Baker	5,938,608	A 8/1999 Bieger et al.
5,520,188	A	5/1996	Hennige et al.	5,938,659	A 8/1999 Tu et al.
5,522,869	A	6/1996	Burdette et al.	5,944,663	A 8/1999 Kuth et al.
5,524,620	A	6/1996	Rosenschein	5,964,755	A 10/1999 Edwards
5,526,815	A	6/1996	Granz et al.	5,979,453	A 11/1999 Savage et al.
5,526,822	A	6/1996	Burbank et al.	5,984,881	A 11/1999 Ishibashi et al.
5,540,656	A	7/1996	Pflueger et al.	5,984,882	A 11/1999 Rosenschein et al.
5,545,195	A	8/1996	Lennox et al.	5,993,389	A 11/1999 Driscoll, Jr. et al.
5,547,459	A	8/1996	Kaufman et al.	5,997,534	A 12/1999 Tu et al.
5,549,638	A	8/1996	Burdette	6,001,069	A 12/1999 Tachibana et al.
5,558,092	A	9/1996	Unger et al.	6,004,269	A 12/1999 Crowley et al.
5,569,241	A	10/1996	Edwards	6,007,499	A 12/1999 Martin et al.
5,571,088	A	11/1996	Lennox et al.	6,022,319	A 2/2000 Willard et al.
5,573,497	A	11/1996	Chapelon	6,024,718	A 2/2000 Chen et al.
5,575,288	A	11/1996	Sliwa et al.	6,024,740	A 2/2000 Lesh et al.
5,575,772	A	11/1996	Lennox	6,027,449	A 2/2000 Mazess et al.
5,575,789	A	11/1996	Bell et al.	6,033,397	A 3/2000 Laufer et al.
5,582,588	A	12/1996	Sakurai et al.	6,039,689	A 3/2000 Lizzi
5,588,432	A *	12/1996	Crowley 600/439	6,041,260	A * 3/2000 Stern et al. 607/98
5,590,657	A	1/1997	Cain et al.	6,042,556	A 3/2000 Beach et al.
5,601,526	A	2/1997	Chapelon et al.	6,050,943	A 4/2000 Slayton et al.
5,620,479	A	4/1997	Diederich	6,066,123	A 5/2000 Li et al.
5,624,382	A	4/1997	Oppelt et al.	6,071,238	A 6/2000 Chapelon et al.
5,628,743	A	5/1997	Cimino	6,071,239	A 6/2000 Cribbs et al.
5,630,837	A	5/1997	Crowley	6,083,159	A 7/2000 Driscoll, Jr. et al.
5,643,179	A	7/1997	Fujimoto	6,086,535	A 7/2000 Ishibashi et al.
				6,086,583	A 7/2000 Ouchi

6,088,613	A	7/2000	Unger	2003/0040698	A1	2/2003	Makin et al.
6,106,469	A	8/2000	Suzuki et al.	2003/0047582	A1	3/2003	Sonnenschein et al.
6,106,517	A	8/2000	Zupkas	2003/0073907	A1	4/2003	Taylor
6,112,123	A	8/2000	Kelleher et al.	2003/0109786	A1	6/2003	Irioka et al.
6,113,558	A	9/2000	Rosenschein et al.	2003/0120270	A1	6/2003	Acker
6,117,101	A	9/2000	Diederich et al.	2003/0144593	A1	7/2003	Whitmore et al.
6,135,963	A	10/2000	Haider	2003/0181900	A1	9/2003	Long
6,135,971	A	10/2000	Hutchinson et al.	2003/0212331	A1	11/2003	Fenton et al.
6,138,513	A	10/2000	Barabash et al.	2003/0212332	A1	11/2003	Fenton et al.
6,148,224	A	11/2000	Jensen	2003/0220568	A1	11/2003	Hansmann et al.
6,156,029	A	12/2000	Mueller	2003/0225331	A1	12/2003	Diederich et al.
6,171,248	B1	1/2001	Hossack et al.	2003/0229293	A1	12/2003	Hibner et al.
6,176,842	B1	1/2001	Tachibana et al.	2003/0233091	A1	12/2003	Wayne et al.
6,183,469	B1	2/2001	Thapliyal et al.	2004/0006336	A1	1/2004	Swanson
6,210,330	B1	4/2001	Tepper	2004/0030268	A1	2/2004	Weng et al.
6,216,704	B1	4/2001	Ingle et al.	2004/0143252	A1	7/2004	Hurst
6,217,576	B1	4/2001	Tu et al.	2004/0236375	A1	11/2004	Redding, Jr.
6,231,834	B1	5/2001	Unger et al.	2004/0254570	A1	12/2004	Hadjicostis et al.
6,352,532	B1	3/2002	Kramer et al.	2005/0015107	A1	1/2005	O'Brien
6,361,531	B1	3/2002	Hissong	2005/0085726	A1	4/2005	Lacoste et al.
6,371,903	B1	4/2002	Blanc et al.	2005/0137520	A1	6/2005	Rule et al.
6,379,320	B1	4/2002	Lafon et al.	2005/0228286	A1	10/2005	Messery et al.
6,394,949	B1	5/2002	Crowley et al.	2005/0234438	A1	10/2005	Mast et al.
6,425,867	B1	7/2002	Vaezy et al.	2005/0240123	A1	10/2005	Mast et al.
6,482,178	B1	11/2002	Andrews et al.	2005/0240124	A1	10/2005	Mast et al.
6,508,774	B1	1/2003	Acker et al.	2005/0240125	A1	10/2005	Makin et al.
6,512,957	B1	1/2003	Witte	2005/0256405	A1	11/2005	Makin et al.
6,521,211	B1	2/2003	Unger et al.	2005/0261586	A1	11/2005	Makin et al.
6,533,726	B1	3/2003	Lizzi et al.	2005/0261587	A1	11/2005	Makin et al.
6,546,934	B1	4/2003	Ingle et al.	2005/0261588	A1	11/2005	Makin et al.
6,547,788	B1 *	4/2003	Maguire et al. 606/41	2005/0267488	A1	12/2005	Hare et al.
6,575,956	B1	6/2003	Briskin et al.	2006/0052695	A1	3/2006	Adam
6,599,245	B1	7/2003	Ma et al.	2006/0052701	A1	3/2006	Carter et al.
6,602,251	B2	8/2003	Burbank et al.	2006/0173348	A1	8/2006	Wilser et al.
6,613,004	B1	9/2003	Vitek et al.	2006/0235306	A1	10/2006	Cotter et al.
6,618,620	B1	9/2003	Freundlich et al.	2007/0016184	A1	1/2007	Cropper et al.
6,626,855	B1	9/2003	Weng et al.	2007/0021691	A1	1/2007	Nita et al.
6,645,202	B1	11/2003	Pless et al.	2008/0058648	A1	3/2008	Novak et al.
6,669,638	B1	12/2003	Miller et al.	2008/0287837	A1	11/2008	Makin et al.
6,716,184	B2	4/2004	Vaezy et al.	2009/0198156	A1	8/2009	Mast et al.
6,719,694	B2	4/2004	Weng et al.				
6,740,082	B2	5/2004	Shaddock				
6,764,488	B1	7/2004	Burbank et al.				
6,770,070	B1	8/2004	Balbierz				
6,783,524	B2 *	8/2004	Anderson et al. 606/28				
6,887,239	B2	5/2005	Elstrom et al.				
6,902,536	B2	6/2005	Manna et al.				
6,921,371	B2	7/2005	Wilson				
6,936,024	B1	8/2005	Houser				
6,936,048	B2	8/2005	Hurst				
6,974,417	B2	12/2005	Lockwood et al.				
7,037,306	B2	5/2006	Podany et al.				
7,063,666	B2	6/2006	Weng et al.				
7,078,015	B2	7/2006	Unger				
7,247,141	B2	7/2007	Makin et al.				
7,473,250	B2	1/2009	Makin et al.				
7,494,467	B2	2/2009	Makin et al.				
7,695,436	B2	4/2010	Mast et al.				
2001/0007940	A1	7/2001	Tu et al.				
2001/0014805	A1	8/2001	Burbank et al.				
2001/0037073	A1	11/2001	White et al.				
2002/0065512	A1	5/2002	Fjield et al.				
2002/0068934	A1	6/2002	Edwards et al.				
2002/0072741	A1	6/2002	Sliwa et al.				
2002/0087081	A1	7/2002	Serrano et al.				
2002/0087083	A1	7/2002	Nix et al.				
2002/0111662	A1	8/2002	Iaizzo et al.				
2002/0147447	A1	10/2002	Long				
2002/0156470	A1	10/2002	Shaddock				
2002/0165579	A1	11/2002	Burbank et al.				
2002/0183742	A1	12/2002	Carmel et al.				
2002/0183771	A1	12/2002	Burbank et al.				
2002/0193781	A1	12/2002	Loeb				
2003/0004434	A1	1/2003	Greco et al.				
2003/0013960	A1	1/2003	Makin et al.				
2003/0013971	A1	1/2003	Makin et al.				
2003/0018266	A1	1/2003	Makin et al.				
2003/0018358	A1 *	1/2003	Saadat 606/232				
2003/0028111	A1	2/2003	Vaezy et al.				

FOREIGN PATENT DOCUMENTS

EP	1518498	3/2005
JP	01-288242	11/1989
JP	06-181923	7/1994
JP	10-14967	1/1998
WO	WO 01/45550	A2 6/2001

OTHER PUBLICATIONS

Watkin et al., "High-intensity focused ultrasound ablation of the kidney in a large animal model," J. Endourol., 11(3), 191, abstract (Jun. 1997).

Hill, C.R. et al., Lesion Development in Focused Ultrasound Surgery: A General Model, Ultrasound in Med. & Biol., 1994, pp. 259-269, vol. 20, No. 3, Elsevier Science Ltd, New York, USA.

Clare, M.C. et al., MRI Guided Focused Ultrasound Surgery (FUS) of uterine leiomyomas: A Feasibility Study, Workshop on MRI-Guided: Focused Ultrasound Surgery, 2002, Syllabus, International Society for Magnetic Resonance in Medicine.

Vaezy, S. et al., Treatment of Uterine Fibroid Tumors in a Nude Mouse Model Using High-Intensity Focused Ultrasound, Am J Obstet Gynecol, 2000, pp. 6-11, vol. 183, No. 1.

Cool-tip™ RF Radio Frequency Ablation System, web page from radionics.com.

Electrosurgical Devices, RF Generator and RITA Base Software, web pages from ritamedical.com.

Billard, et al., "Effects of Physical Parameters in High Temperature Ultrasound Hyperthermia," Ultrasound in Medicine and Biology, vol. 16, Issue 4, pp. 409-420 (1990).

Office Action, Chinese Application No. 200680032059.2 (6 pages) (Nov. 6, 2009).

Supplementary European Search Report, European Application No. 06787104.6 (8 pages) (Sep. 16, 2009).

* cited by examiner

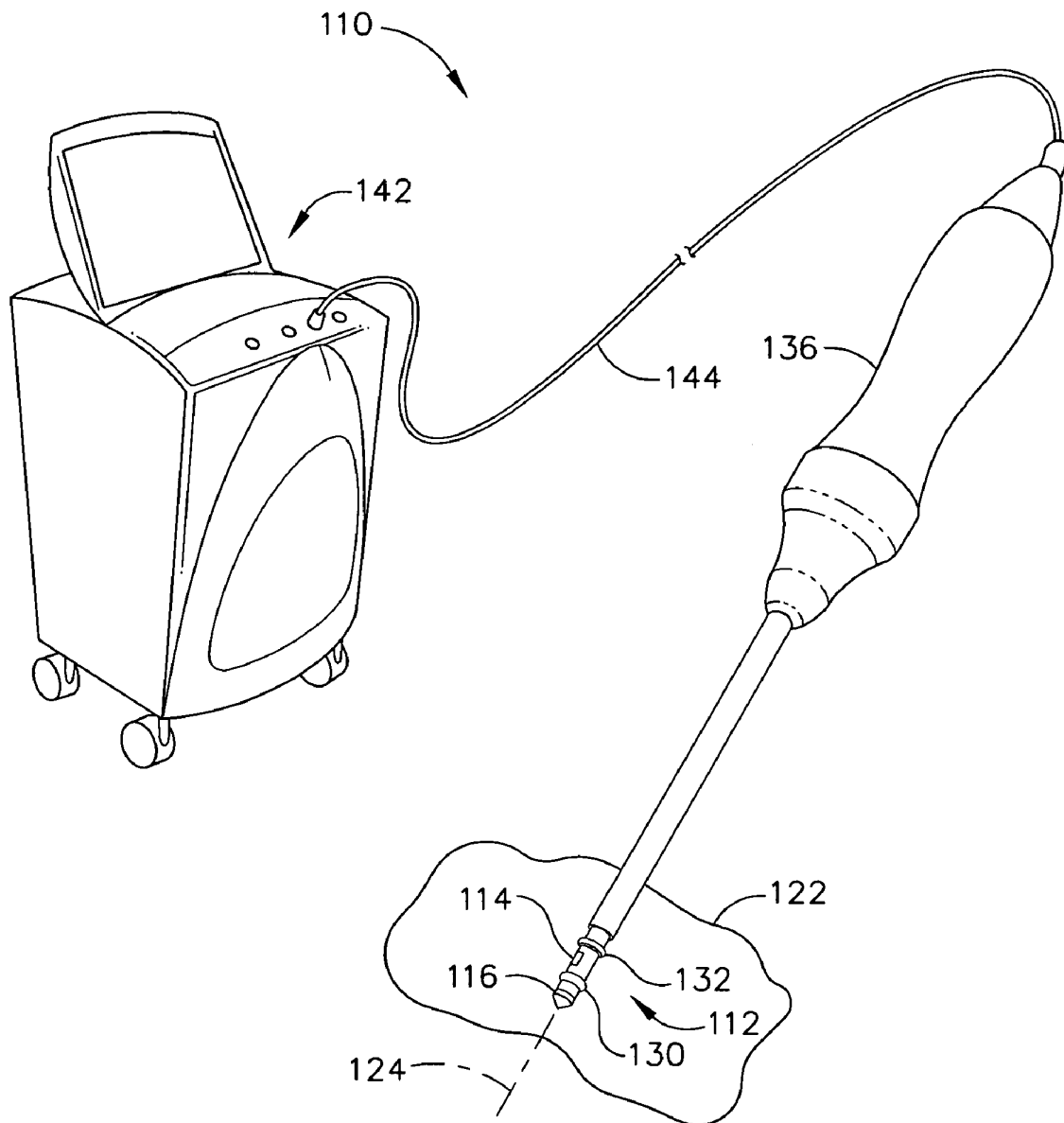


FIG. 1

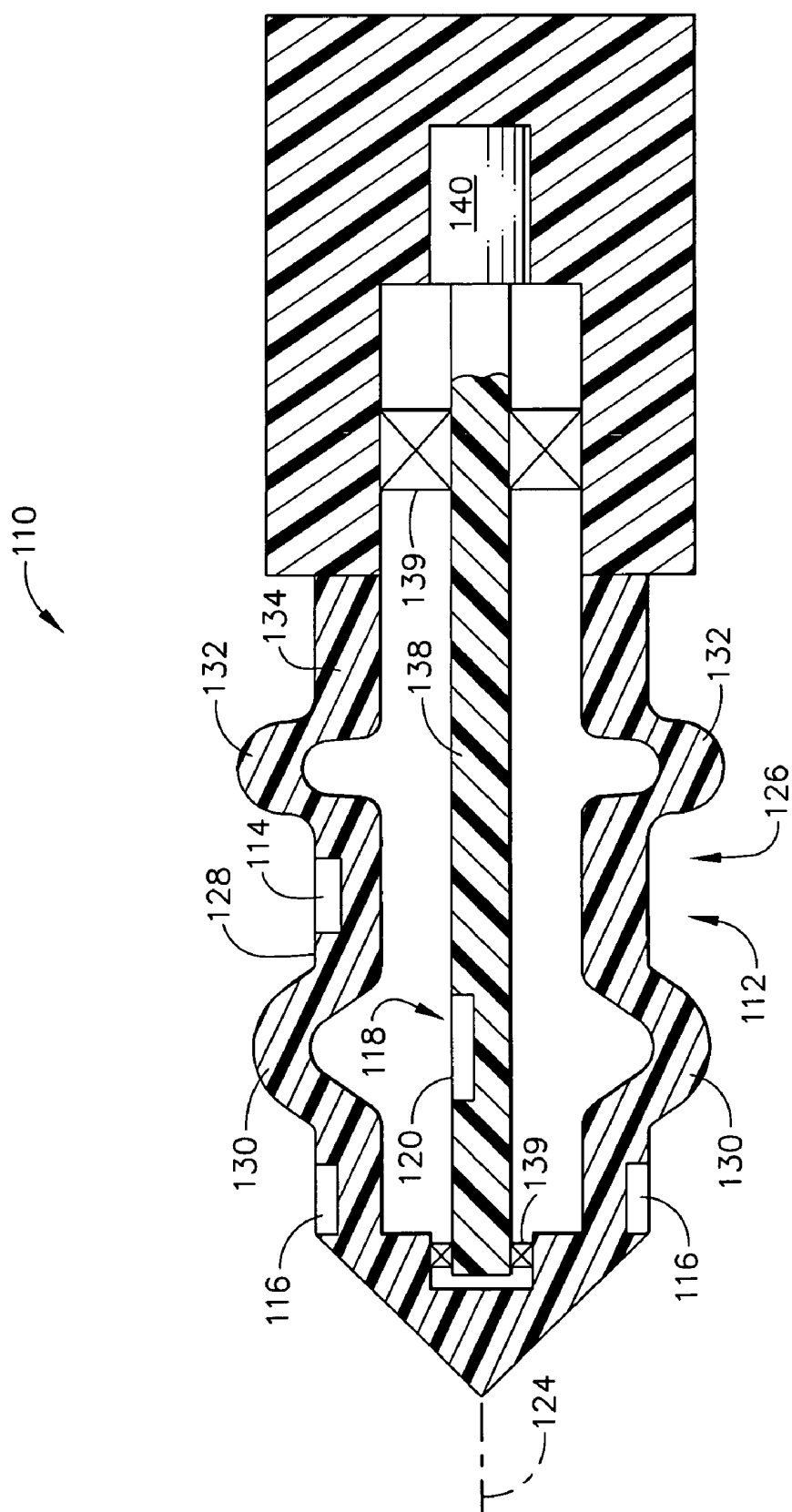


FIG. 2

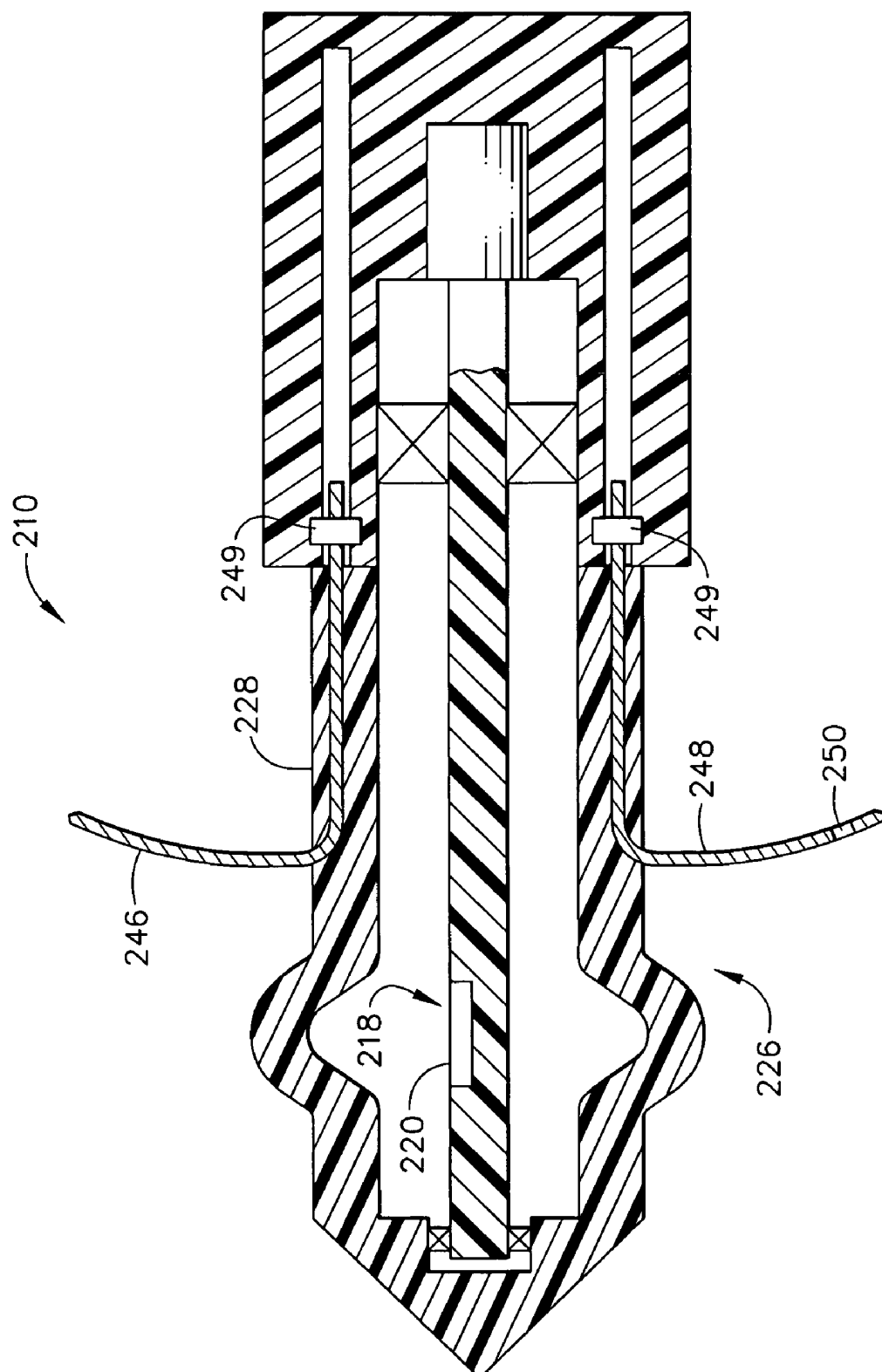


FIG. 3

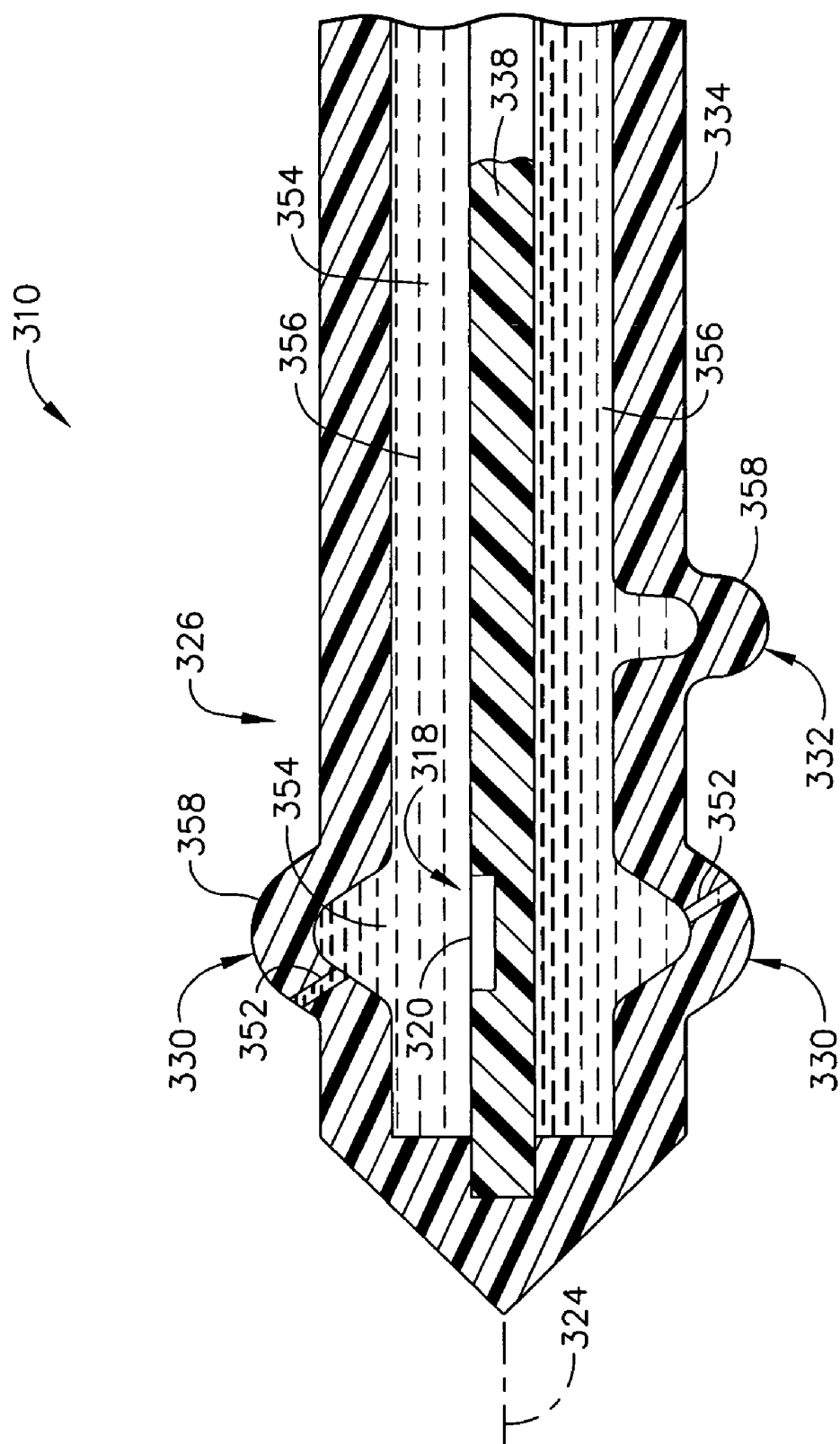


FIG. 4

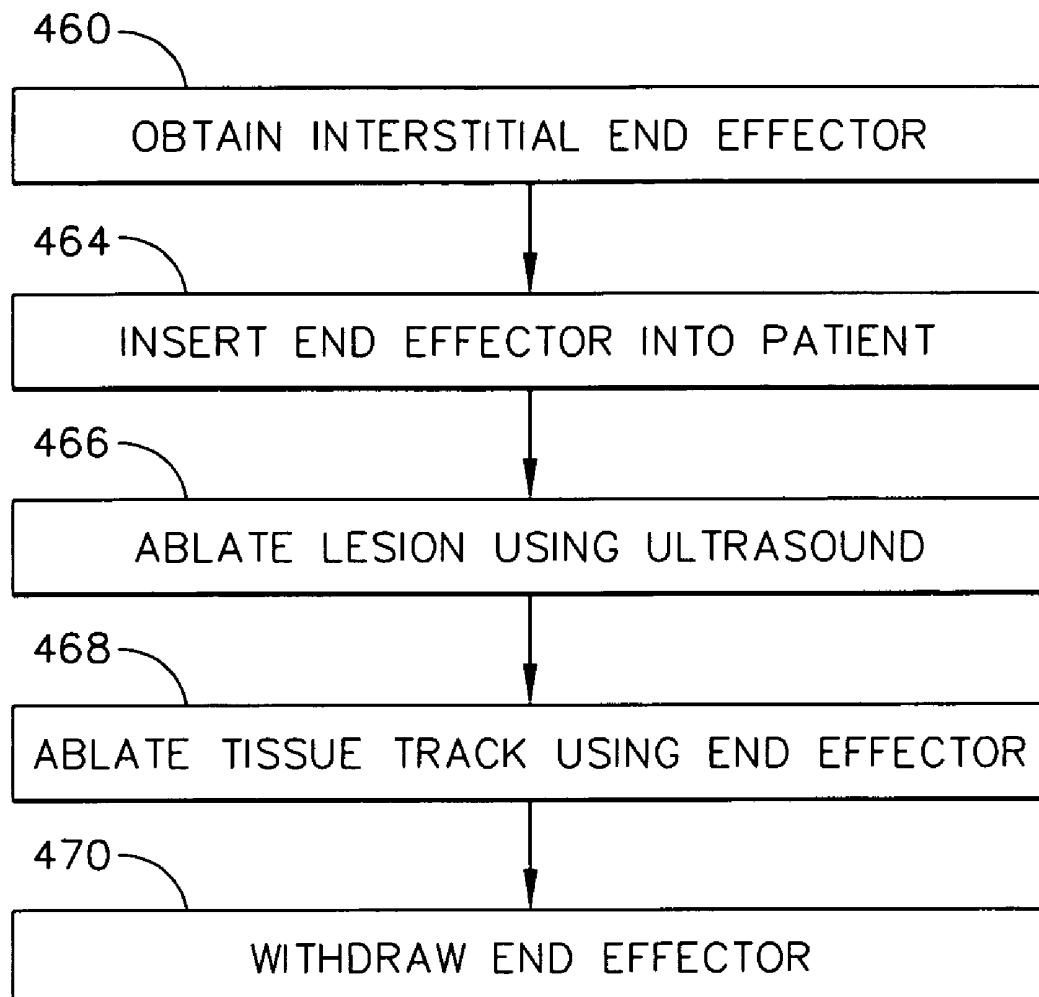


FIG. 5

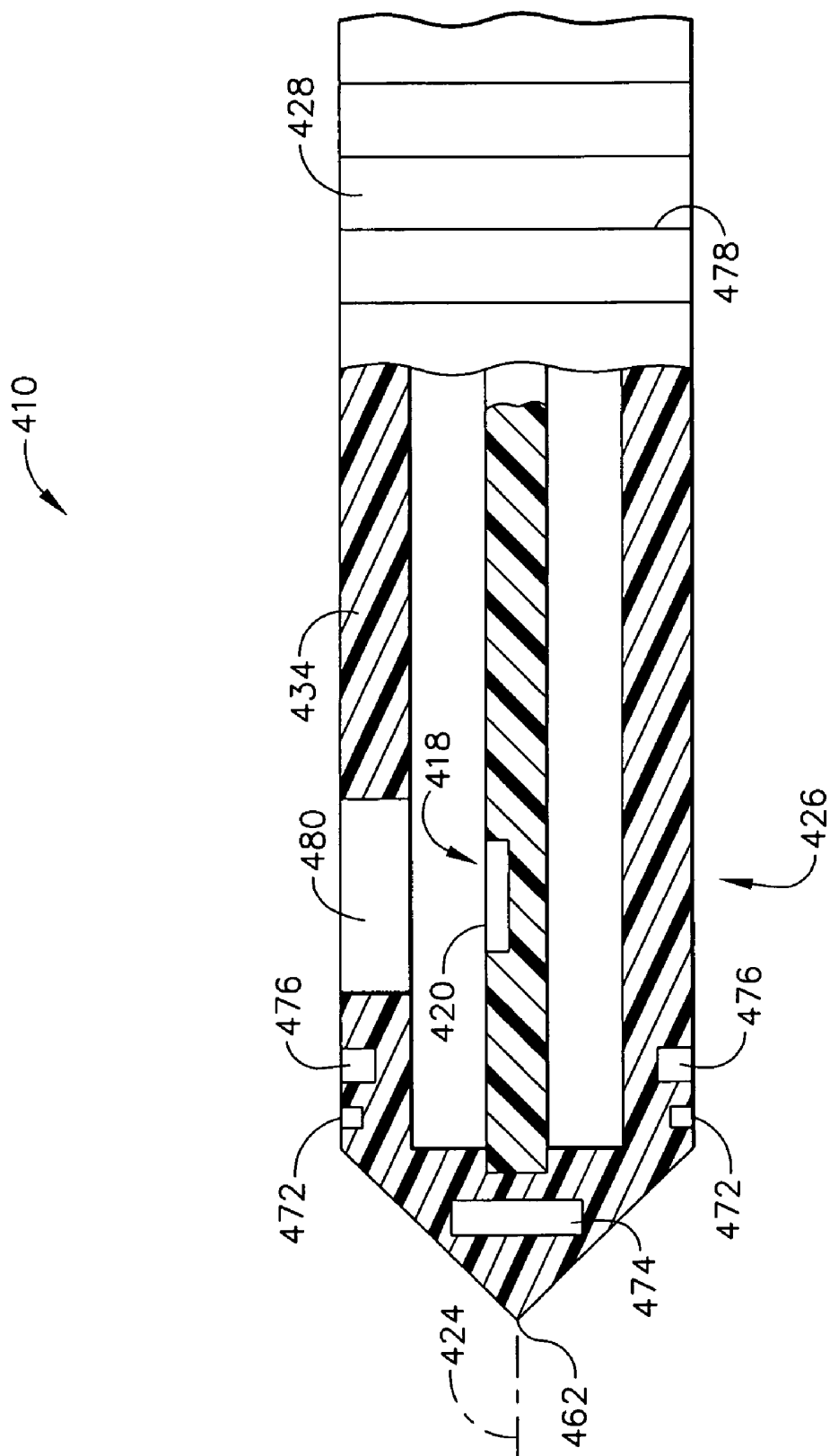


FIG. 6

ULTRASOUND MEDICAL SYSTEM

FIELD OF THE INVENTION

The present invention relates generally to ultrasound, and more particularly to ultrasound medical systems and methods.

BACKGROUND OF THE INVENTION

Known medical methods include using ultrasound imaging (at low power) of patients to identify patient tissue for medical treatment and include using ultrasound (at high power) to ablate identified patient tissue by heating the tissue.

Known ultrasound medical systems and methods include deploying an ultrasound end effector having an ultrasound transducer outside the body to break up kidney stones inside the body, endoscopically inserting an ultrasound end effector having an ultrasound transducer in the rectum to medically destroy prostate cancer, laparoscopically inserting an ultrasound end effector having an ultrasound transducer in the abdominal cavity to medically destroy a cancerous liver tumor, intravenously inserting a catheter ultrasound end effector having an ultrasound transducer into a vein in the arm and moving the catheter to the heart to medically destroy diseased heart tissue, and interstitially inserting a needle ultrasound end effector having an ultrasound transducer needle into the tongue to medically destroy tissue to reduce tongue volume to reduce snoring.

Rotatable ultrasound end effectors are known wherein an ultrasound transducer is non-rotatably attached to a shaft whose distal end is circumferentially and longitudinally surrounded by a sheath having a longitudinal axis and having an acoustic window. Water between the shaft and the sheath provides acoustic coupling between the ultrasound transducer and the acoustic window. The shaft is rotatable about the longitudinal axis with respect to the sheath. The sheath is non-rotatably attached to a handpiece.

Known medical systems and methods include deploying a radio-frequency (RF) end effector having an RF electrode to thermally ablate patient tissue and to take tissue electric impedance and tissue temperature measurements using electrodes integrated into the shaft or into a tine which also helps stabilize the RF end effector in patient tissue.

Still, scientists and engineers continue to seek improved ultrasound medical systems and methods.

SUMMARY OF THE INVENTION

An embodiment of the invention is an ultrasound medical system including an ultrasound end effector and including at least one non-ultrasound tissue-property-measuring sensor. The ultrasound end effector includes a medical ultrasound transducer assembly having at least one medical-treatment ultrasound transducer. The at-least-one non-ultrasound tissue-property-measuring sensor is supported by the ultrasound end effector and is positionable in contact with patient tissue.

Several benefits and advantages are obtained from one or more of the embodiments and methods of the invention. In one example, having a non-ultrasound tissue-property-measuring sensor (such as a tissue temperature sensor and/or a tissue electric impedance sensor) allows ultrasound tissue ablation with feedback from the sensor used to evaluate the tissue ablation and/or modify the ultrasound treatment.

The present invention has, without limitation, application in conventional interstitial, endoscopic, laparoscopic, and open surgical instrumentation as well as application in robotic-assisted surgery.

BRIEF DESCRIPTION OF THE FIGURES

FIG. 1 is a perspective view of a first embodiment of the present invention showing an ultrasound medical system which includes an end effector, a handpiece, and a controller;

FIG. 2 is a schematic cross-sectional view of a first embodiment of the end effector and the handpiece of the ultrasound medical system of FIG. 1 showing a medical ultrasound transducer assembly and two non-ultrasound tissue-property-measuring sensors;

FIG. 3 is a view, as in FIG. 2, but of a second embodiment of a handpiece and of an end effector having a medical ultrasound transducer assembly and two tines;

FIG. 4 is a view, as in FIG. 2, but of a third embodiment of an end effector having a medical ultrasound transducer assembly supported by a shaft and having a surrounding sheath, wherein the sheath includes two balloon portions;

FIG. 5 is a block diagram view of a method of the invention for ultrasonically treating a lesion in a patient; and

FIG. 6 is a schematic view, partially in cross-section, of a fourth embodiment of an end effector which has a medical-treatment ultrasound transducer and three end-effector-tissue-track ablation devices and which can be used in one employment of the method of FIG. 5.

DETAILED DESCRIPTION OF THE INVENTION

Before explaining the present invention in detail, it should be noted that the invention is not limited in its application or use to the details of construction and arrangement of parts and/or steps illustrated in the accompanying drawings and description. The illustrative embodiments and methods of the invention may be implemented or incorporated in other embodiments, methods, variations and modifications, and may be practiced or carried out in various ways. Furthermore, unless otherwise indicated, the terms and expressions employed herein have been chosen for the purpose of describing the illustrative embodiments and methods of the present invention for the convenience of the reader and are not for the purpose of limiting the invention.

It is understood that any one or more of the following-described embodiments, methods, examples, etc. can be combined with any one or more of the other following-described embodiments, methods, examples, etc.

Referring now to FIGS. 1-2 of the drawings, a first embodiment of the present invention is an ultrasound medical system 110 comprising an ultrasound end effector 112 and at least one non-ultrasound tissue-property-measuring sensor 114 and 116. The ultrasound end effector 112 includes a medical ultrasound transducer assembly 118 having at least one medical-treatment ultrasound transducer 120. The at-least-one non-ultrasound tissue-property-measuring sensor 114 and 116 is supported by the ultrasound end effector 112 and is disposable in contact with patient tissue 122.

It is noted that a medical-treatment ultrasound transducer includes a medical-treatment-only ultrasound transducer and a medical-imaging-and-treatment ultrasound transducer. In one arrangement, an ultrasound transducer has a single transducer element, and in another arrangement, an ultrasound transducer has a plurality (also called an array) of transducer elements. It is also noted that a medical ultrasound transducer assembly having at least one medical-treatment ultrasound transducer can also have at least one medical-imaging ultrasound transducer.

In one example of the embodiment of FIGS. 1-2, the ultrasound end effector 112 includes a longitudinal axis 124. In this example, the at-least-one non-ultrasound tissue-property-measuring sensor 114 and 116 includes a first non-ultrasound tissue-property-measuring sensor 114 and a second non-ultrasound tissue-property-measuring sensor 116. The

at-least-one medical-treatment ultrasound transducer **120** is disposed longitudinally between the first and second non-ultrasound tissue-property-measuring sensors **114** and **116**.

In one variation of the embodiment of FIGS. 1-2, the at-least-one non-ultrasound tissue-property-measuring sensor (e.g., **114**) measures tissue temperature. In one modification, the at-least-one non-ultrasound tissue-property-measuring sensor (e.g., **114**) is chosen from the group consisting of a thermistor, a thermocouple, and combinations thereof. In another variation, the at-least-one non-ultrasound tissue-property-measuring sensor (e.g., **116**) measures tissue electric impedance. In one modification, the at-least-one non-ultrasound tissue-property-measuring sensor (e.g., **116**) is chosen from the group consisting of a monopolar electrode, a bipolar electrode, and combinations thereof. It is noted that tissue temperature and/or tissue electric impedance is a measure of the degree of ultrasonic ablation of patient tissue, as can be appreciated by those skilled in the art.

In one construction of the embodiment of FIGS. 1-2, the ultrasound end effector **112** is an ultrasound interstitial end effector **126** which is interstitially insertable into patient tissue **122** and which has an exterior surface **128**. The at-least-one non-ultrasound tissue-property-measuring sensor **114** and **116** is attached to the ultrasound interstitial end effector **126** and is fixedly disposed substantially flush with the exterior surface **128**. In one arrangement, the exterior surface **128** includes at least one balloon portion **130** and **132** which is expandable and contractible and which is expandable against patient tissue **122** to provide at least some stabilization of the ultrasound interstitial end effector **126** with respect to patient tissue **122**. In one variation, the exterior surface **128** is the exterior surface of a sheath **134** and has first and second balloon portions **130** and **132**, wherein the first balloon portion **130** surrounds the medical ultrasound transducer assembly **118** and acts as an acoustic window, and wherein the second balloon portion **132** is longitudinally spaced apart from the medical ultrasound transducer assembly **118**. An acoustic coupling medium, such as water, is disposable between the medical ultrasound transducer assembly **118** and the first balloon portion **130** and has been omitted from FIG. 2 for clarity. In one modification, the first balloon portion **130** is omitted and the sheath **134** terminates before the medical ultrasound transducer assembly **118** which is exposed to patient tissue. In another modification, the second balloon portion **132** is omitted. In one employment, the at-least-one balloon portion **130** and **132** is contracted during tissue insertion and withdrawal of the ultrasound interstitial end effector **126**. Other constructions, arrangements, variations, and modifications are left to the artisan.

In one enablement of the embodiment of FIGS. 1-2, the ultrasound end effector **112** is an ultrasound interstitial end effector **126** which is interstitially insertable into patient tissue **122** and which has an exterior surface **128**. In this enablement, the at-least-one non-ultrasound tissue-property-measuring sensor **114** and **116** is deployable to extend away from the exterior surface into patient tissue **128** to provide at least some stabilization of the ultrasound interstitial end effector **126** with respect to patient tissue **122** and is retrievable to retract back toward the exterior surface **128**. In one arrangement, the at-least-one non-ultrasound tissue-property-measuring sensor **114** and **116** is storable inside the exterior surface.

In one implementation of the embodiment of FIGS. 1-2, the ultrasound medical system **110** also includes a handpiece **136** operatively connected to the ultrasound end effector **112**. The ultrasound end effector **112** has a longitudinal axis **124** and a shaft **138**, and the medical ultrasound transducer assembly **118** is supported by the shaft **138**. The shaft **138** is rotatable with respect to the handpiece **136** about the longitudinal axis **124** and is supported by bearings **139**. In one variation, a

motor **140** rotates the shaft **138**. In one arrangement, the ultrasound medical system **110** includes a controller **142** operatively connected to the handpiece **136** via a cable **144**.

A second embodiment of the present invention, shown in FIG. 3, is an ultrasound medical system **210** comprising an ultrasound end effector **226**. The ultrasound end effector **226** has an exterior surface **228**. The ultrasound end effector **226** includes a medical ultrasound transducer assembly **218** having at least one medical-treatment ultrasound transducer **220**, and includes at least one tine **246** and **248**. The at-least-one tine **246** and **248** is deployable to extend away from the exterior surface into patient tissue to provide at least some stabilization of the ultrasound end effector **226** with respect to patient tissue and is retrievable to retract back toward the exterior surface **228**.

In one example of the embodiment of FIG. 3, the ultrasound end effector **226** is insertable into a patient. In one variation, the ultrasound end effector **226** is an ultrasound interstitial end effector which is interstitially insertable into patient tissue. In other variations, the ultrasound end effector is insertable into a patient in an endoscopic, laparoscopic, and/or open surgical manner. In another example, the ultrasound end effector is disposable on the outside of a patient. Other examples and variations are left to the artisan.

In one enablement of the embodiment of FIG. 3, the at-least-one tine **246** and **248** includes a plurality of tines. In one example of the embodiment of FIG. 3, the at-least-one tine **246** and **248** is storable inside the exterior surface. It is noted that construction of deployable tines **246** and **248** in an ultrasound end effector **226** is within the level of skill of the artisan. In one arrangement, such deployment is accomplished using one or more of cables, levers, motors **249**, gearing, push rods and the like to move a tine partially out of, and back into, a lumen in the end effector. In one choice of materials, the tine comprises or consists essentially of Nitinol wire or nichrome wire.

In one employment of the embodiment of FIG. 3, the at-least-one tine (e.g., **246**) acts as an element chosen from the group consisting of an electrode, a thermistor, a thermocouple, an acoustic reflector, an acoustic absorber, an acoustic emitter, an acoustic receiver, a radio-frequency (RF) heater, a resistive heater, and combinations thereof. In another employment, the at-least-one tine (e.g., **248**) includes a component **250** chosen from the group consisting of an electrode, a thermistor, a thermocouple, an acoustic reflector, an acoustic absorber, an acoustic emitter, an acoustic receiver, a radio-frequency (RF) heater, a resistive heater, and combinations thereof.

The embodiment, examples, constructions, implementations, etc. of the embodiment of FIGS. 1-2 are equally applicable to the embodiment, constructions, implementations, etc. of FIG. 3. In one construction of the embodiment of FIG. 3, the exterior surface **228** is like the exterior surface **128** of a previously-illustrated and described construction of the embodiment of FIGS. 1-2 including at least one balloon portion which is expandable and contractible, and which is expandable against patient tissue to provide at least some stabilization of the ultrasound end effector with respect to patient tissue. In one implementation of the embodiment of FIG. 3, the ultrasound medical system **210** also includes, like a previously-illustrated and described implementation of the embodiment of FIGS. 1-2, a handpiece operatively connected to the ultrasound end effector, wherein the ultrasound end effector has a longitudinal axis and a shaft, wherein the medical ultrasound transducer assembly is supported by the shaft, and wherein the shaft is rotatable with respect to the handpiece about the longitudinal axis.

One method, using the embodiment of FIG. 3 and enablements, examples, employments, and constructions thereof, is for ultrasonically treating a lesion in a patient and includes

steps a) through f). Step a) includes obtaining the ultrasound medical system 210. Step b) includes inserting the ultrasound end effector 226 into patient tissue. Step c) includes deploying the plurality of tines 246 and 248 to extend away from the exterior surface 228 into the patient tissue. Step d) includes ultrasonically ablating the lesion using the at-least-one medical-treatment ultrasound transducer 220. Step e) includes retrieving the plurality of tines 246 and 248 to retract back toward the exterior surface and storing the plurality of tines 246 and 248 inside the exterior surface 228. Step f) includes withdrawing the ultrasound end effector 226 from the patient tissue. Another method also includes the step of employing the plurality of tines 246 and 248 to each act as the element or using each component 250. An additional method also includes the step of expanding the at-least-one balloon portion against patient tissue and contracting the at-least-one balloon portion.

A third embodiment of the present invention, shown in FIG. 4, is an ultrasound medical system 310 comprising an ultrasound end effector 326 including a shaft 338, a sheath 334, and a medical ultrasound transducer assembly 318. The medical ultrasound transducer assembly 318 is supported by the shaft 338 and has at least one medical-treatment ultrasound transducer 320. The sheath 334 surrounds the shaft 338. The sheath 334 includes at least one balloon portion 330 and 332 which is expandable against patient tissue to provide at least some stabilization of the ultrasound end effector 326 with respect to patient tissue.

In one example of the embodiment of FIG. 4, the ultrasound end effector 326 is insertable into a patient. In one variation, the ultrasound end effector 326 is an ultrasound interstitial end effector which is interstitially insertable into patient tissue. In other variations, the ultrasound end effector is insertable into a patient in an endoscopic, laparoscopic, and/or open surgical manner. In another example, the ultrasound end effector is disposable on the outside of a patient. Other examples and variations are left to the artisan.

In one construction of the embodiment of FIG. 3, the ultrasound end effector 326 has a longitudinal axis 324, and the at-least-one balloon portion (e.g., 330) acts as an acoustic window and is disposed to longitudinally overlap the at-least-one medical-treatment ultrasound transducer 320. In one variation of this construction, the at-least-one balloon portion (e.g., 330) includes at least one through hole 352. In one modification, the at-least-one balloon portion (e.g., 330) includes a plurality of through holes 352 creating a "weeping" balloon portion, wherein some of the acoustic coupling medium inside the sheath 334 extends and/or flows outside the sheath acoustic window providing improved acoustic coupling between the at-least-one medical-treatment ultrasound transducer 320 and patient tissue.

In one arrangement of the embodiment of FIG. 3, the at-least-one balloon portion (e.g., 330) includes at least one through hole 352 and the ultrasound end effector 326 is adapted to dispense a drug 354 through the at-least-one through hole 352 to patient tissue. In one variation, the drug 354 is carried in a liquid acoustic coupling medium 356, such as water, disposed between the medical ultrasound transducer assembly 318 and the at-least-one balloon portion 330 whose pressure is controlled (such as by a pump in a handpiece operatively connected to the ultrasound end effector) to expand and contract the at-least-one balloon portion 330. In one variation, the drug 354 is at least potentiated (i.e., has its medical effect increased and/or activated) by ultrasound emitted from the at-least-one medical-treatment ultrasound transducer 320.

In the same or another arrangement of the embodiment of FIG. 3, the ultrasound end effector 326 has a longitudinal axis 324, and the at-least-one balloon portion (e.g., 332) is disposed longitudinally apart from the at-least-one medical-

treatment ultrasound transducer 320. In one variation of the embodiment of FIG. 3, the at-least-one balloon portion (e.g., 330) is a fully-circumferential balloon portion. In a different variation, the at-least-one balloon portion (e.g., 332) is a blister balloon portion. In one example of the embodiment of FIG. 3, the at-least-one balloon portion 330 and 332 includes an outside surface 358 having a roughness average at least equal to 0.005-inch. In one variation, the outside surface includes ribs. Such surface roughness improves stabilization of the ultrasound end effector 326 with respect to patient tissue when the at-least-one balloon portion 330 and 332 is expanded against the patient tissue.

The embodiments, constructions, implementations, etc. of the embodiments of FIGS. 1-2 and 3 are equally applicable to the embodiment, constructions, implementations, etc. of the embodiment of FIG. 4. In one implementation of the embodiment of FIG. 3, the ultrasound medical system 310 also includes a controller, like the controller of the previously-illustrated and described arrangement of the embodiment of FIGS. 1-2, wherein the controller is operatively connected to the medical ultrasound transducer assembly, wherein the medical ultrasound transducer assembly is a medical-imaging-and-treatment ultrasound transducer assembly, and wherein the controller determines if the at-least-one balloon portion is acoustically coupled to, or acoustically decoupled from, patient tissue from ultrasonically imaging a balloon-tissue area using the medical-imaging-and-treatment ultrasound transducer assembly.

One method of the invention for ultrasonically treating a lesion in a patient is shown in block diagram form in FIG. 5, and an embodiment of an ultrasound medical system which can be used in performing the method is shown in FIG. 6. The method includes steps a) through e). Step a) is labeled as "Obtain Interstitial End Effector" in block 460 of FIG. 5. Step a) includes obtaining an interstitial end effector 426 including a distal end 462 and including a medical ultrasound transducer assembly 418 having at least one medical-treatment ultrasound transducer 420 and at least one end-effector-tissue-track ablation device 472, 474 and 476; It is noted that the distal end of an interstitial end effector is an end having a tissue-piercing tip. Step b) is labeled as "Insert End Effector Into Patient" in block 464 of FIG. 5. Step b) includes inserting the interstitial end effector 426 into the patient creating a tissue track which is surrounded by patient tissue and which ends at the distal end 462 of the inserted interstitial end effector 426. Step c) is labeled as "Ablate Lesion Using Ultrasound" in block 466 of FIG. 5. Step c) includes ultrasonically ablating the lesion using the at-least-one medical-treatment ultrasound transducer 420. Step d) is labeled as "Ablate Tissue Track Using End Effector" in block 468 of FIG. 5. Step d) includes using the at-least-one end-effector-tissue-track ablation device 472, 474 and 476 to ablate the patient tissue surrounding the tissue track along substantially the entire tissue track. Step e) is labeled as "Withdraw End Effector" in block 470 of FIG. 5. Step e) includes withdrawing the interstitial end effector 426 from the patient.

It is noted that creating a tissue track requires that the interstitial end effector 426 be interstitially inserted into patient tissue. It is also noted that the interstitial end effector 426 can be equipped with a retractable tip shield (not shown) for initial endoscopic or laparoscopic patient entry followed by interstitial insertion into patient tissue.

In one extension of the method of FIG. 5, there is included the step of using the at-least-one end-effector-tissue-track ablation device (e.g., 474) to ablate the patient tissue at the distal end 462 of the inserted interstitial end effector 426.

In one implementation of the method of FIG. 5, the at-least-one end-effector-tissue-track ablation device (e.g., 474) includes a non-ultrasound energy source, and step d) uses the

non-ultrasound energy source to ablate the patient tissue surrounding the tissue track. In one variation, the non-ultrasound energy source is chosen from the group consisting of a resistive heat energy source, a hot liquid energy source, a monopolar radio-frequency (RF) energy source, a bipolar radio-frequency (RF) energy source, a capacitive heat energy source, a microwave energy source, and combinations thereof.

In another implementation of the method, the at-least-one end-effector-tissue-track ablation device (e.g., 476) includes a tissue-ablating chemical agent, and step d) uses the tissue-ablating chemical agent to ablate the patient tissue surrounding the tissue track. In one variation, the tissue-ablating chemical agent is chosen from the group consisting of fibrin, alcohol, an acidic fluid, a chemotherapeutic agent, and combinations thereof.

In a further implementation of the method, step d) uses the medical ultrasound transducer assembly 418 to ultrasonically ablate the patient tissue surrounding the tissue track. In one variation, step d) ultrasonically ablates at a higher ultrasound frequency than does step c).

In the same or another extension of the method of FIG. 5, there is included the step of monitoring (such as for acoustic coupling and/or for tissue ablation) the patient tissue surrounding the tissue track during step d). In one variation, the monitoring is chosen from the group consisting of B-mode ultrasonic image monitoring, tissue temperature monitoring, tissue electric impedance, and combinations thereof.

In the same or another extension of the method of FIG. 5, there are included, after step b) and before step c), the step of stabilizing (such as by using a balloon, a tine and/or suction) the interstitial end effector 426 with respect to the patient tissue surrounding the tissue track and, after step c) and before step d), the step of releasing the stabilizing of the interstitial end effector 426 with respect to the patient tissue surrounding the tissue track.

In one application of the method of FIG. 5, step e) includes stepwise withdrawing the interstitial end effector 426 from the patient using a plurality of positional steps, and step d) includes ablating the patient tissue surrounding the tissue track for a predetermined time with the interstitial end effector at each positional step.

A fourth embodiment of the present invention, shown in FIG. 6, is an ultrasound medical system 410 comprising an interstitial end effector 426 which is interstitially insertable into patient tissue, which includes at least one medical-treatment ultrasound transducer 420, and which includes at least one end-effector-tissue-track ablation device 472, 474 and 476.

In one enablement of the embodiment of FIG. 6, the ultrasound medical system 410 includes a controller (such as the controller 142 illustrated in FIG. 1) which is operatively connected to the at-least-one medical-treatment ultrasound transducer 420 to ultrasonically ablate a lesion in patient tissue of the patient and which is operatively connected to the at-least-one end-effector-tissue-track ablation device 472, 474 and 476 to ablate patient tissue surrounding the interstitial end effector 426 during withdrawal of the interstitial end effector 426 from the patient.

In one application of the embodiment of FIG. 6, the at-least-one end-effector-tissue-track ablation device 472, 474, 476 includes a cylindrical ultrasound transducer 472. In the same or a different application, the at-least-one end-effector-tissue-track ablation device and the at-least-one medical-treatment ultrasound transducer are a single rotatable ultrasound transducer (such as ultrasound transducer 420 made rotatable such as in a previously illustrated and described implementation of the embodiment of FIGS. 1-2). Other

applications of an end-effector-tissue-track ablation device involving ultrasound are left to the artisan.

In another application of the embodiment of FIG. 6, the at-least-one end-effector-tissue-track ablation device 472, 474 and 476 includes a device 474 which uses a non-ultrasound energy source. In one variation, the non-ultrasound energy source is chosen from the group consisting of a resistive heat energy source, a hot liquid energy source, a monopolar radio-frequency (RF) energy source, a bipolar radio-frequency (RF) energy source, a capacitive heat energy source, a microwave energy source, and combinations thereof.

In a further application of the embodiment of FIG. 6, the at-least-one end-effector-tissue-track ablation device 472, 474 and 476 includes a device 476 which releases a tissue-ablating chemical agent. In one variation, the tissue-ablating chemical agent is chosen from the group consisting of fibrin, alcohol, an acidic fluid, a chemotherapeutic agent, and combinations thereof.

In one construction of the embodiment of FIG. 6, the interstitial end effector 426 has a length and an exterior surface 428 and includes position markings 478 on the exterior surface 428 along at least a portion of its length. Such position markings allow a user to withdraw the interstitial end effector 426 from patient tissue in positional steps while ablating patient tissue surrounding the end-effector tissue track for a predetermined dwell time at each positional step. In the same or a different construction, the interstitial end effector 426 has a longitudinal axis 424 and a distal end 462, and wherein the at-least-one end-effector-tissue-track ablation device 472, 474 and 476 includes an end-effector-tissue-track ablation device (such as 474) which is disposed proximate the distal end 462. It is noted that the distal end of an interstitial end effector is an end having a tissue-piercing tip. In the same or a different construction, the interstitial end effector 426 includes a tissue-ablating component (such as 474) adapted (such as by having a resistive heat energy source) to ablate (such as to thermally ablate) patient tissue longitudinally forward of the distal end 462.

In one variation, the ultrasound interstitial end effector includes a sheath 434 surrounding the medical-treatment ultrasound transducer 120 and having an acoustic window 480. In one modification, the entire sheath acts as an acoustic window. In another modification, the acoustic window is a thinner portion of the sheath. In a further modification, the acoustic window is a separate material(s) from the material(s) of the non-acoustic-window portion(s) of the sheath. Acoustic window component materials are known to those skilled in the art. Other modifications are left to the artisan.

It is noted that the embodiments, constructions, implementations, etc. of the embodiments of FIGS. 1-2, 3 and 4 are equally applicable to the embodiment, constructions, implementations, etc. of the embodiment of FIG. 6.

Several benefits and advantages are obtained from one or more of the embodiments and methods of the invention. In one example, having a non-ultrasound tissue-property-measuring sensor (such as a tissue temperature sensor and/or a tissue electric impedance sensor) allows ultrasound tissue ablation with feedback from the sensor used to evaluate the tissue ablation and/or modify the ultrasound treatment.

While the present invention has been illustrated by a description of several embodiments and methods, it is not the intention of the applicants to restrict or limit the spirit and scope of the appended claims to such detail. Numerous other variations, changes, and substitutions will occur to those skilled in the art without departing from the scope of the invention. For instance, the ultrasound medical system of the invention has application in robotic assisted surgery taking

into account the obvious modifications of such systems, components and methods to be compatible with such a robotic system. It will be understood that the foregoing description is provided by way of example, and that other modifications may occur to those skilled in the art without departing from the scope and spirit of the appended claims.

What is claimed is:

1. An ultrasound medical system comprising:

an ultrasound end effector, wherein the ultrasound end effector includes a sheath having an exterior surface, and wherein the ultrasound end effector is an ultrasound interstitial end effector which is interstitially insertable into patient tissue;

at least one non-ultrasound tissue-property-measuring sensor, wherein the at-least-one non-ultrasound tissue-property-measuring sensor is attached to the ultrasound interstitial end effector and is fixedly disposed substantially flush with the exterior surface; and

a medical ultrasound transducer assembly having at least one medical-treatment ultrasound transducer, wherein the medical ultrasound transducer assembly including the medical-treatment ultrasound transducer is surrounded by the sheath;

wherein the at-least-one non-ultrasound tissue-property-measuring sensor is supported by the ultrasound interstitial end effector and is disposable in contact with patient tissue; and

wherein the exterior surface includes at least one balloon portion which is expandable and contractible and which is expandable against patient tissue to provide at least some stabilization of the ultrasound interstitial end effector with respect to patient tissue, wherein a first balloon portion surrounds the medical ultrasound transducer assembly and acts as an acoustic window and longitudinally overlaps the medical-treatment ultrasound transducer, and wherein an acoustic coupling medium is disposable between the medical ultrasound transducer assembly and the first balloon portion.

2. The ultrasound medical system of claim 1, wherein the ultrasound interstitial end effector includes a longitudinal axis, wherein the at-least-one non-ultrasound tissue-property-measuring sensor includes a first non-ultrasound tissue-property-measuring sensor and a second non-ultrasound tissue-property-measuring sensor, and wherein the at-least-one medical-treatment ultrasound transducer is disposed longitudinally between the first and second non-ultrasound tissue-property-measuring sensors.

3. The ultrasound medical system of claim 1, wherein the at-least-one non-ultrasound tissue-property-measuring sensor measures tissue temperature.

4. The ultrasound medical system of claim 1, wherein the at-least-one non-ultrasound tissue-property-measuring sensor measures tissue electric impedance.

5. The ultrasound medical system of claim 1, wherein the exterior surface includes a second balloon portion longitudinally spaced apart from the medical ultrasound transducer assembly.

6. The ultrasound medical system of claim 1, also including a handpiece operatively connected to the ultrasound interstitial end effector, wherein the ultrasound interstitial end effector has a longitudinal axis and a shaft, wherein the medical

ultrasound transducer assembly is supported by the shaft, and wherein the shaft is rotatable with respect to the handpiece about the longitudinal axis.

7. An ultrasound medical system comprising:

an ultrasound interstitial end effector, wherein the ultrasound interstitial end effector includes a sheath having an exterior surface;

at least one non-ultrasound tissue-property-measuring sensor, wherein the at-least-one non-ultrasound tissue-property-measuring sensor is deployable to extend away from the exterior surface into patient tissue to provide at least some stabilization of the ultrasound interstitial end effector with respect to patient tissue and is retrievable to retract back toward the exterior surface; and

a medical ultrasound transducer assembly having at least one medical-treatment ultrasound transducer, wherein the medical ultrasound transducer assembly including the medical-treatment ultrasound transducer is surrounded by the sheath;

wherein the at-least-one non-ultrasound tissue-property-measuring sensor is supported by the ultrasound interstitial end effector and is disposable in contact with patient tissue; and

wherein the exterior surface includes at least one balloon portion which is expandable and contractible and which is expandable against patient tissue to provide at least some stabilization of the ultrasound interstitial end effector with respect to patient tissue, wherein a first balloon portion surrounds the medical ultrasound transducer assembly and acts as an acoustic window and longitudinally overlaps the medical-treatment ultrasound transducer, and wherein an acoustic coupling medium is disposable between the medical ultrasound transducer assembly and the first balloon portion.

8. The ultrasound medical system of claim 7, wherein the at-least-one non-ultrasound tissue-property-measuring sensor is storable inside the exterior surface.

9. The ultrasound medical system of claim 7, wherein the ultrasound interstitial end effector includes a longitudinal axis, wherein the at-least-one non-ultrasound tissue-property-measuring sensor includes a first non-ultrasound tissue-property-measuring sensor and a second non-ultrasound tissue-property-measuring sensor, and wherein the at-least-one medical-treatment ultrasound transducer is disposed longitudinally between the first and second non-ultrasound tissue-property-measuring sensors.

10. The ultrasound medical system of claim 7, wherein the at-least-one non-ultrasound tissue-property-measuring sensor measures tissue temperature.

11. The ultrasound medical system of claim 7, wherein the at-least-one non-ultrasound tissue-property-measuring sensor measures tissue electric impedance.

12. The ultrasound medical system of claim 7, wherein the exterior surface includes a second balloon portion longitudinally spaced apart from the medical ultrasound transducer assembly.

13. The ultrasound medical system of claim 7, also including a handpiece operatively connected to the ultrasound interstitial end effector, wherein the ultrasound end effector has a longitudinal axis and a shaft, wherein the medical ultrasound transducer assembly is supported by the shaft, and wherein the shaft is rotatable with respect to the handpiece about the longitudinal axis.

* * * * *

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摘要(译)

超声医疗系统包括超声末端执行器和至少一个非超声组织特性测量传感器。超声末端执行器包括具有至少一个医疗超声换能器的医疗超声换能器组件。至少一个非超声组织特性测量传感器由超声末端执行器支撑，并且可定位成与患者组织接触。

