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**Schulz et al.**

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(54) **PULSE OXIMETRY EAR SENSOR**

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21, 2002, provisional application No. 60/410,499,  
filed on Sep. 14, 2002.

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**A61B 5/00** (2006.01)

(52) **U.S. Cl.** ..... **600/309**; 600/344; 600/485;  
600/500

(58) **Field of Classification Search** ..... 600/300–301,  
600/309–312, 322–326, 340, 386–394; 381/FOR. 134  
See application file for complete search history.

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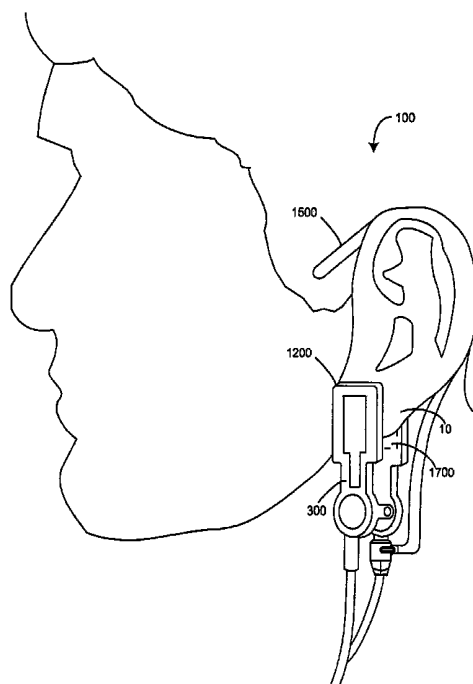
*Primary Examiner*—Robert L. Nasser

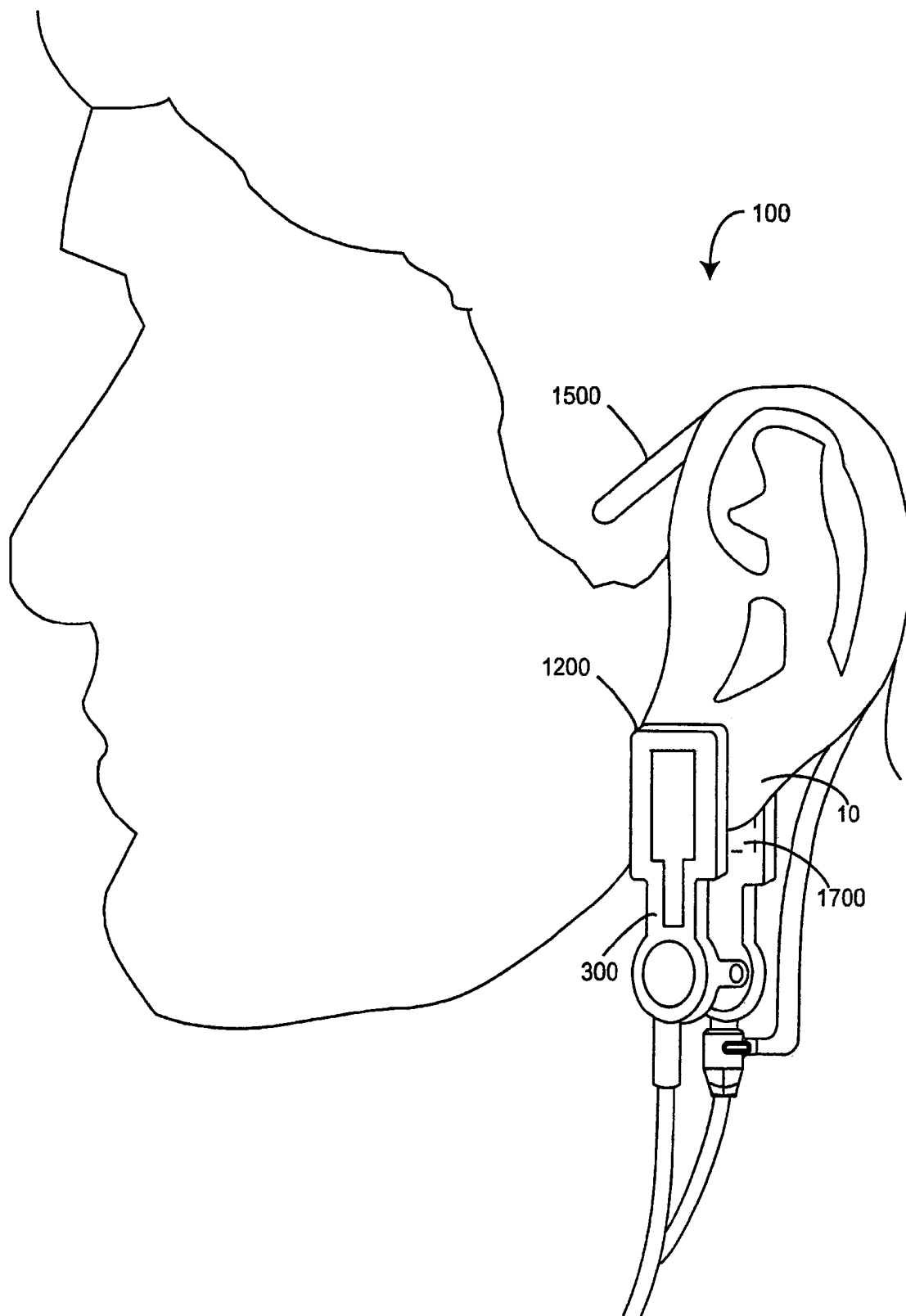
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(57) **ABSTRACT**

An embodiment of an ear sensor assembly comprises an emitter pad and a detector pad. A clip is configured to removably retain each of the pads. The clip has an open position for placement on an ear tissue site and a closed position for securing the pads to opposite sides of the site. The assembly includes a sensor connector adapted to electrically communicate with a host instrument. A sensor cable has a first end terminating at the pads and a second end terminating at the sensor connector and provides electrical communications between the pads and the connector. In one embodiment, one or more silicone lenses or removable adhesive tabs aid in relieving patient discomfort and pressure necrosis.

**17 Claims, 23 Drawing Sheets**



*FIG. 1*

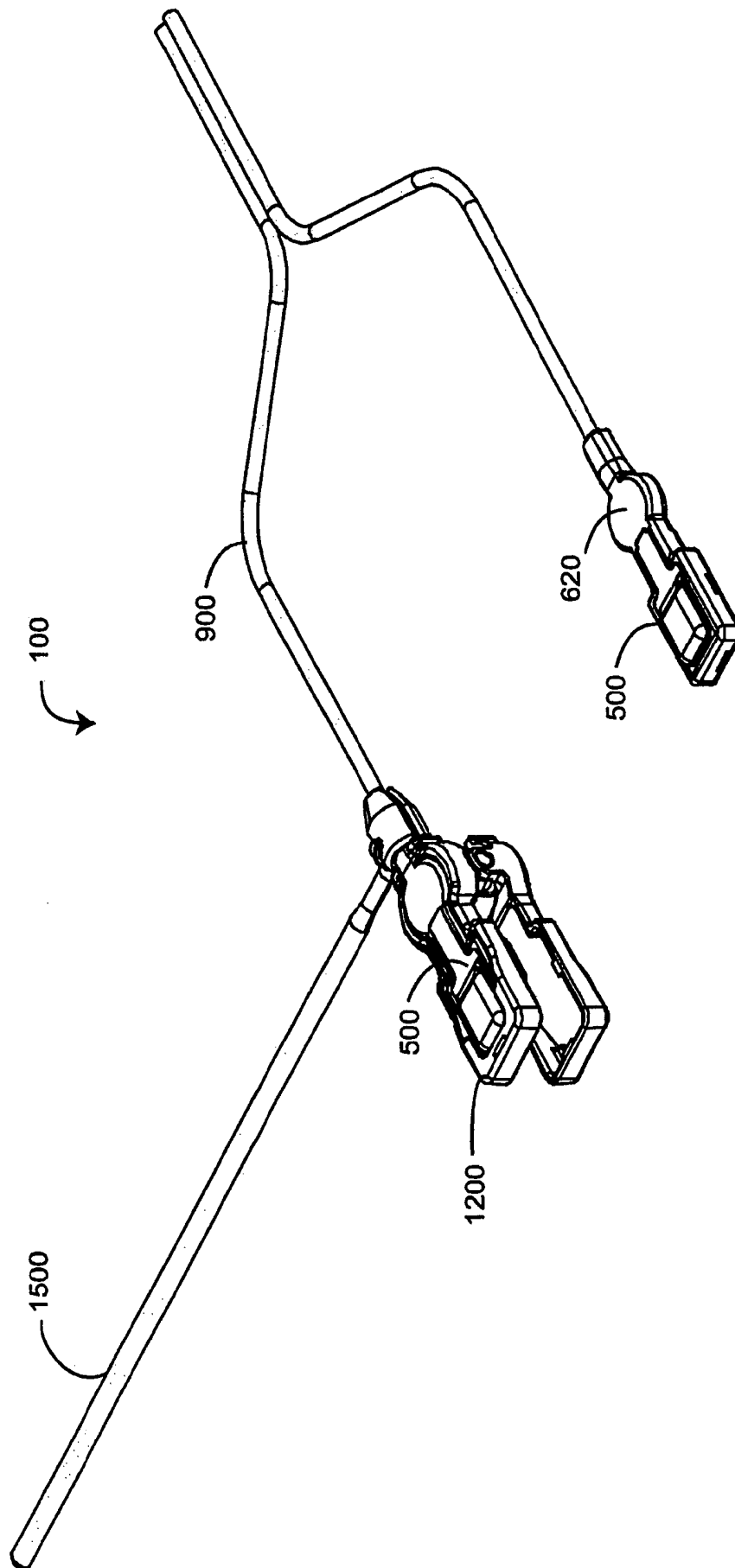


FIG. 2

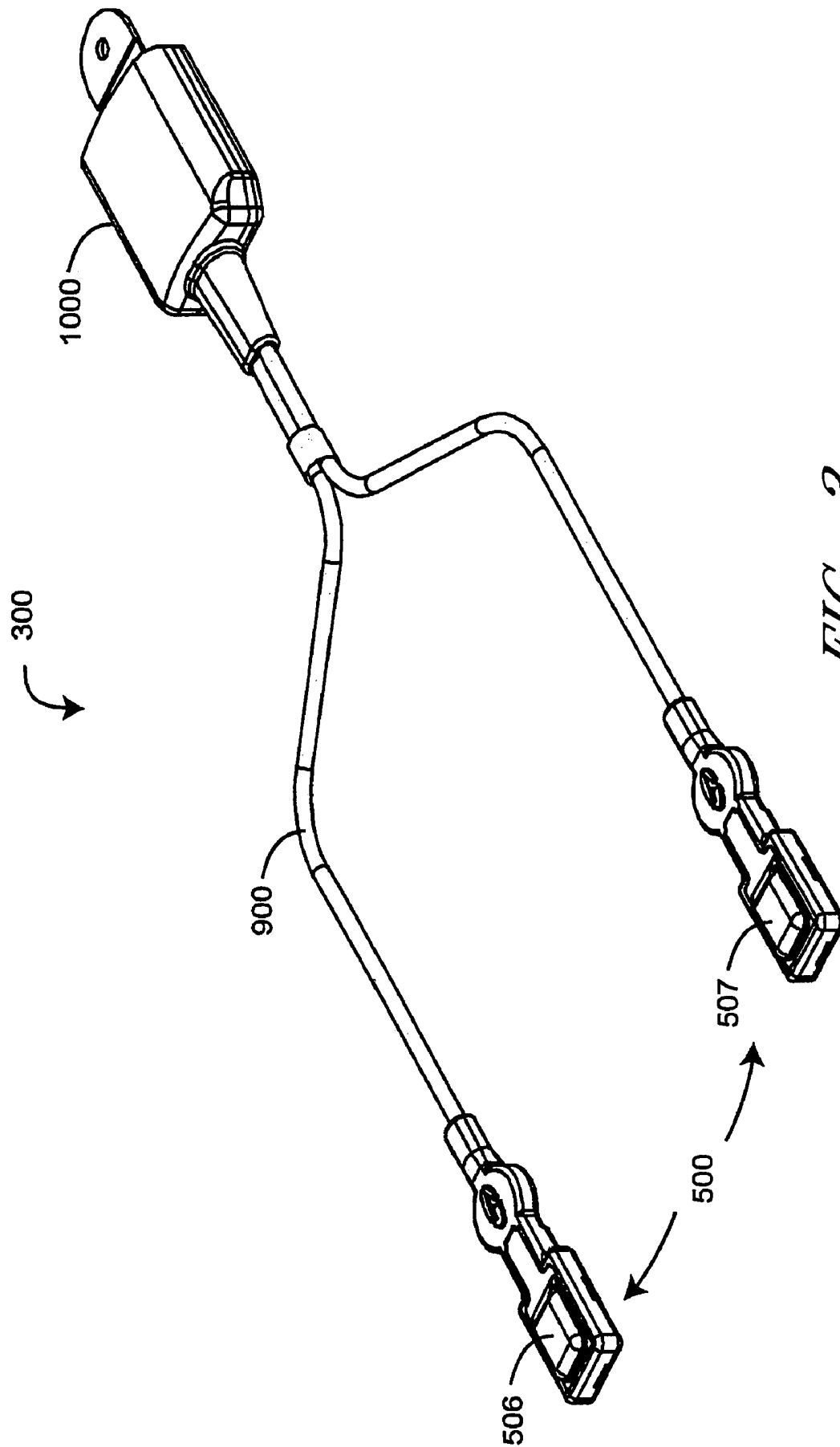
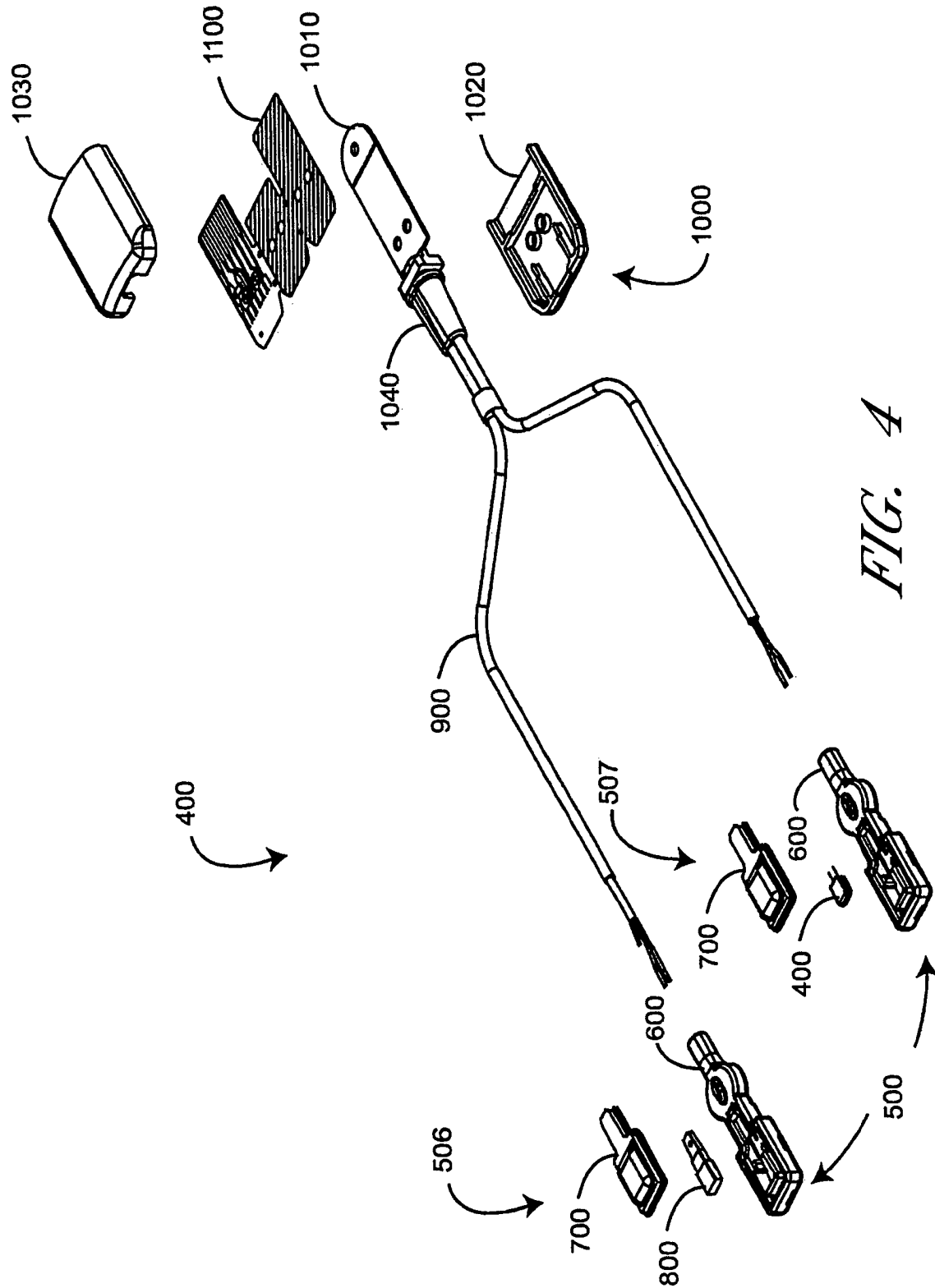
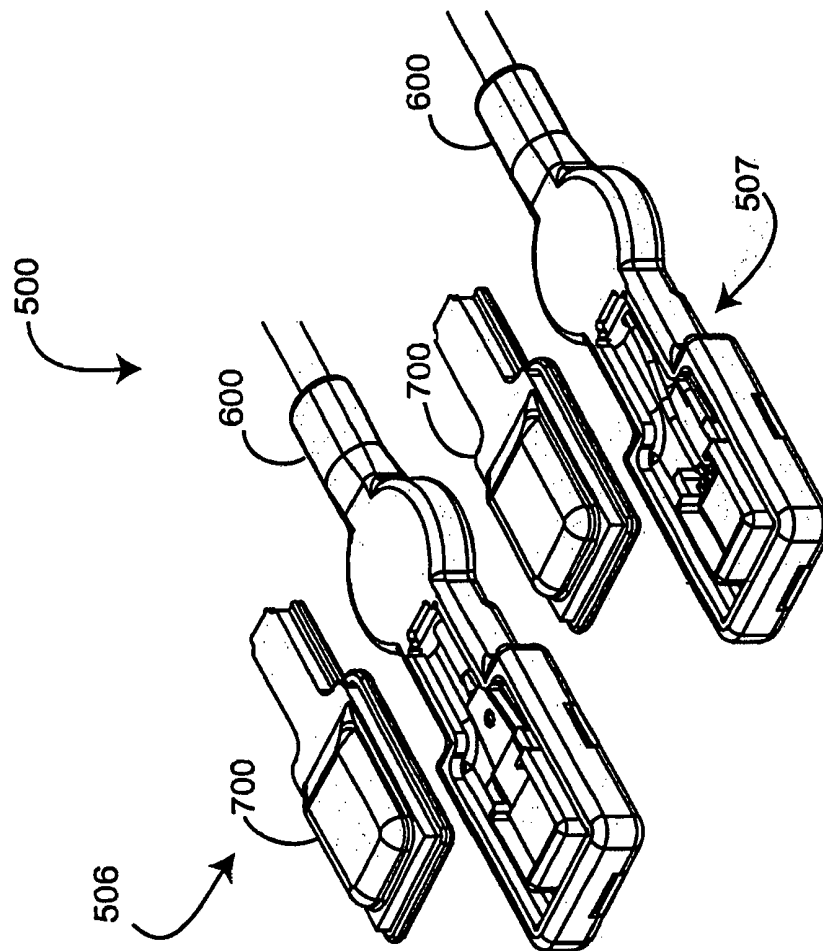
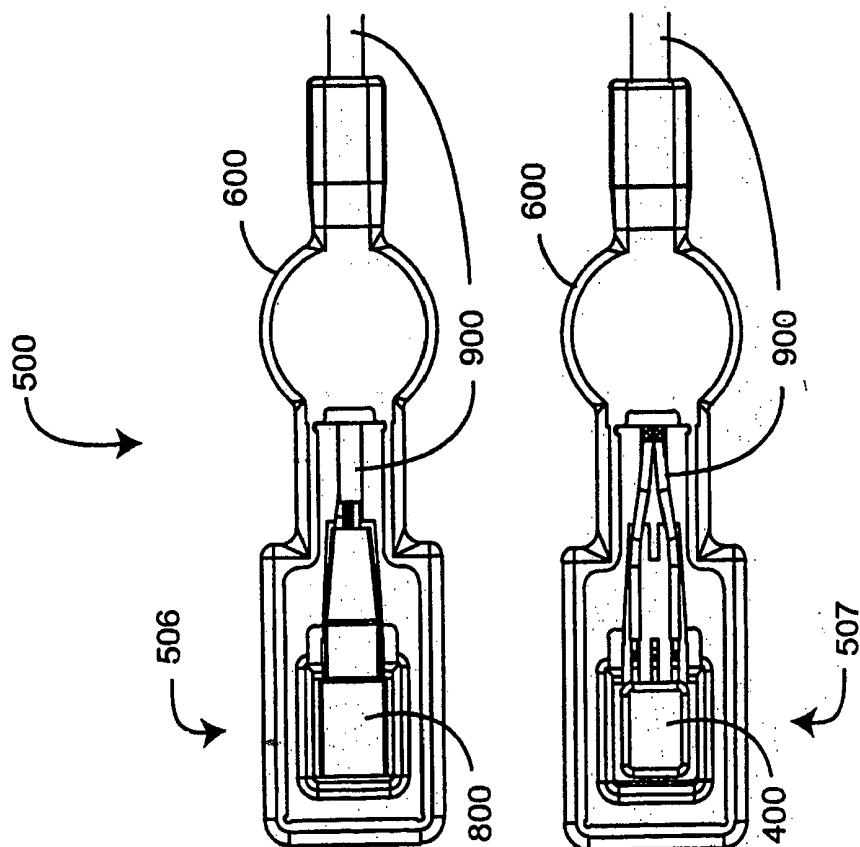


FIG. 3





*FIG. 5B*



**FIG. 5A**

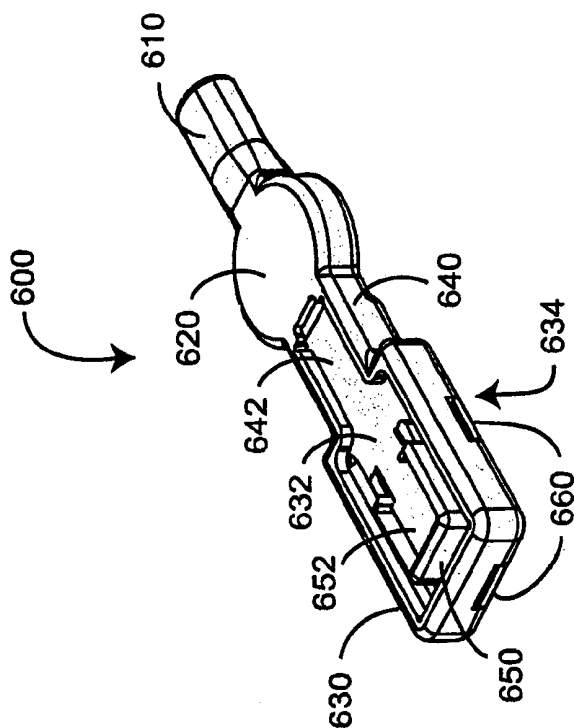


FIG. 6B

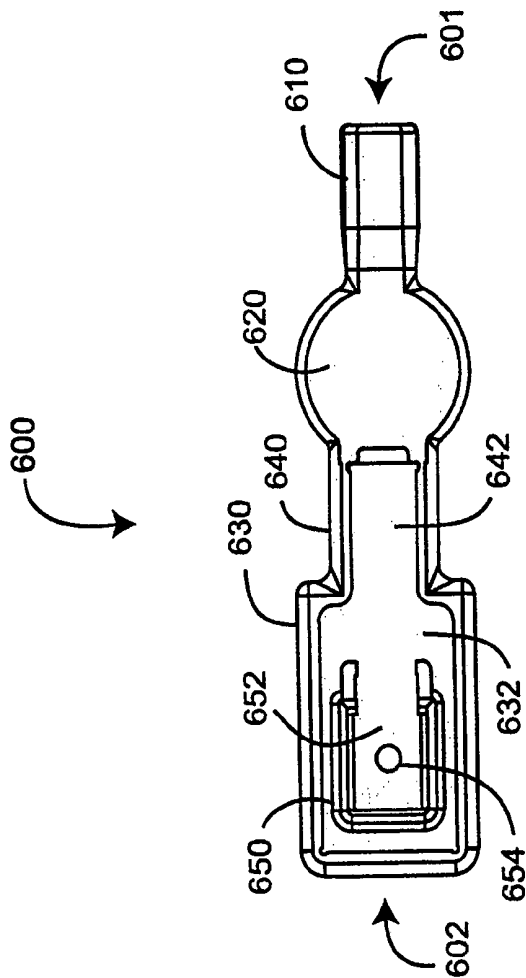
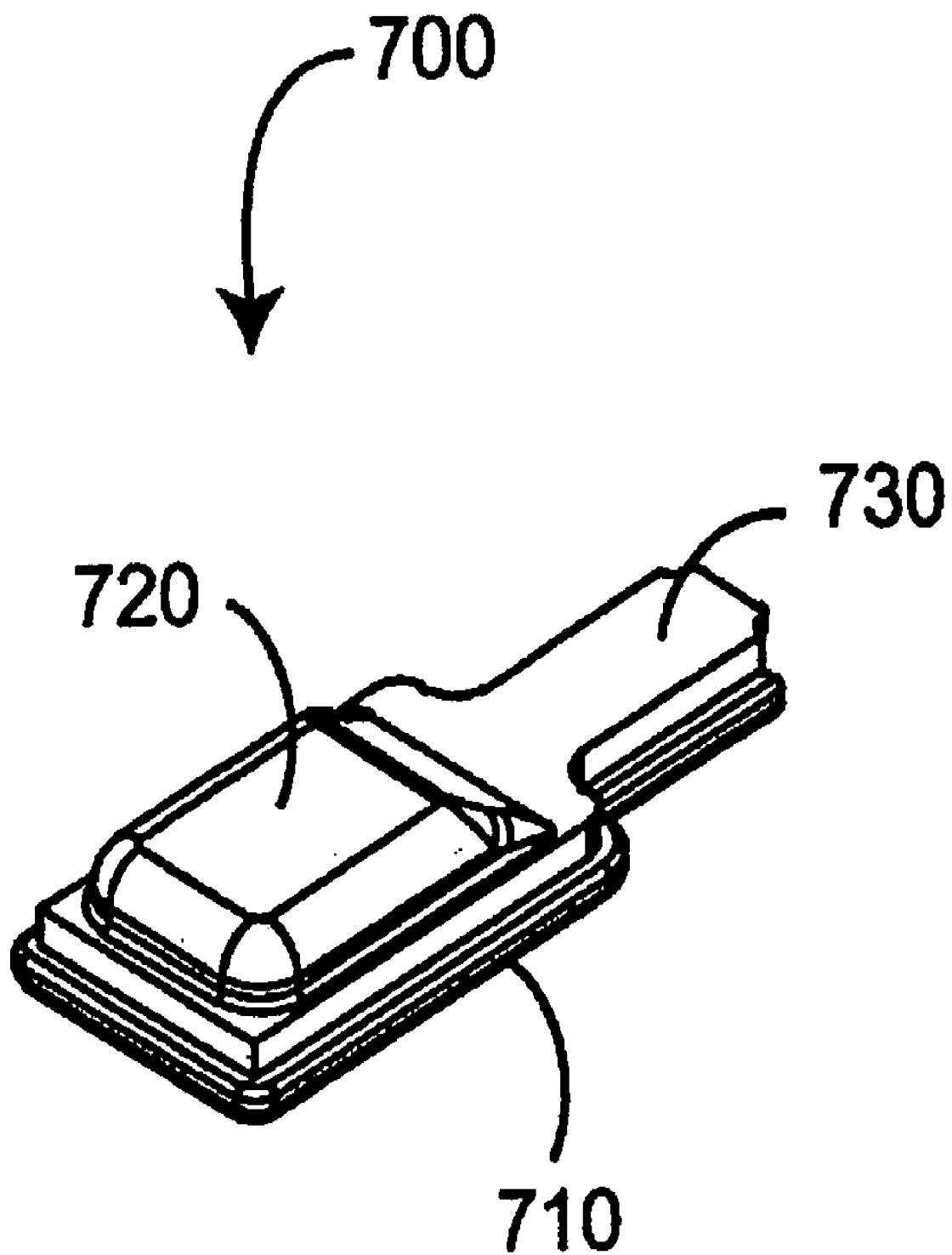


FIG. 6A



*FIG. 7*



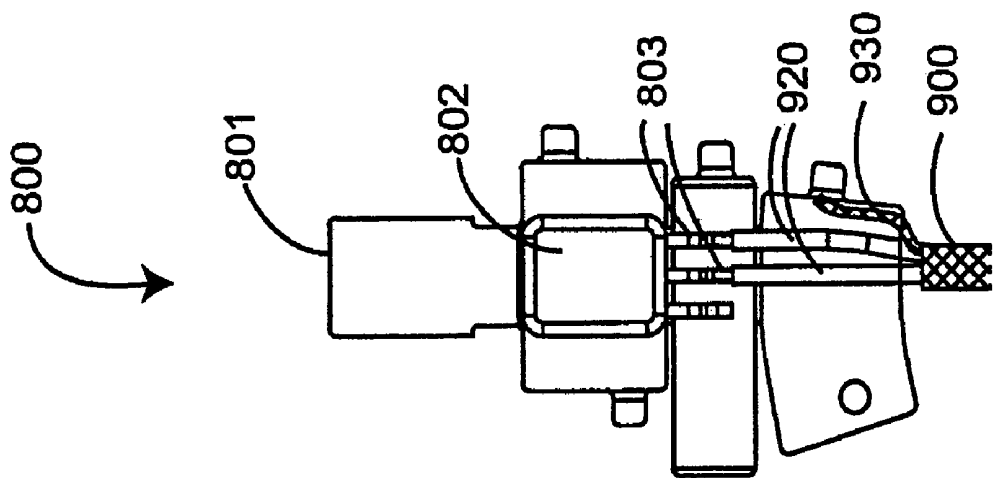


FIG. 8B

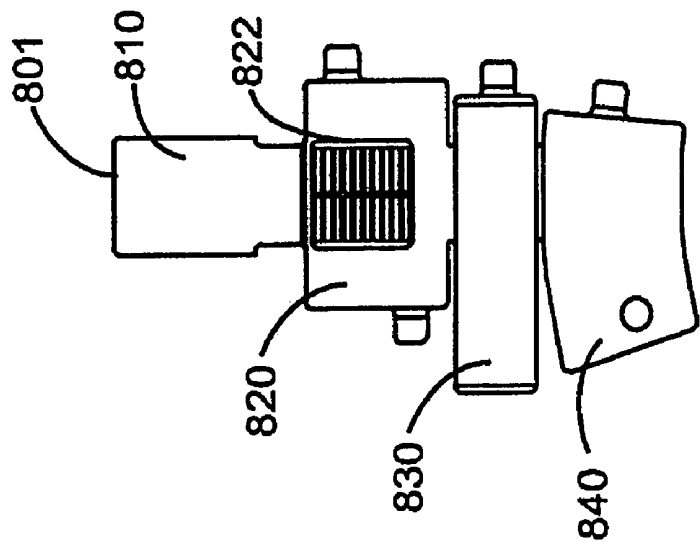


FIG. 8A

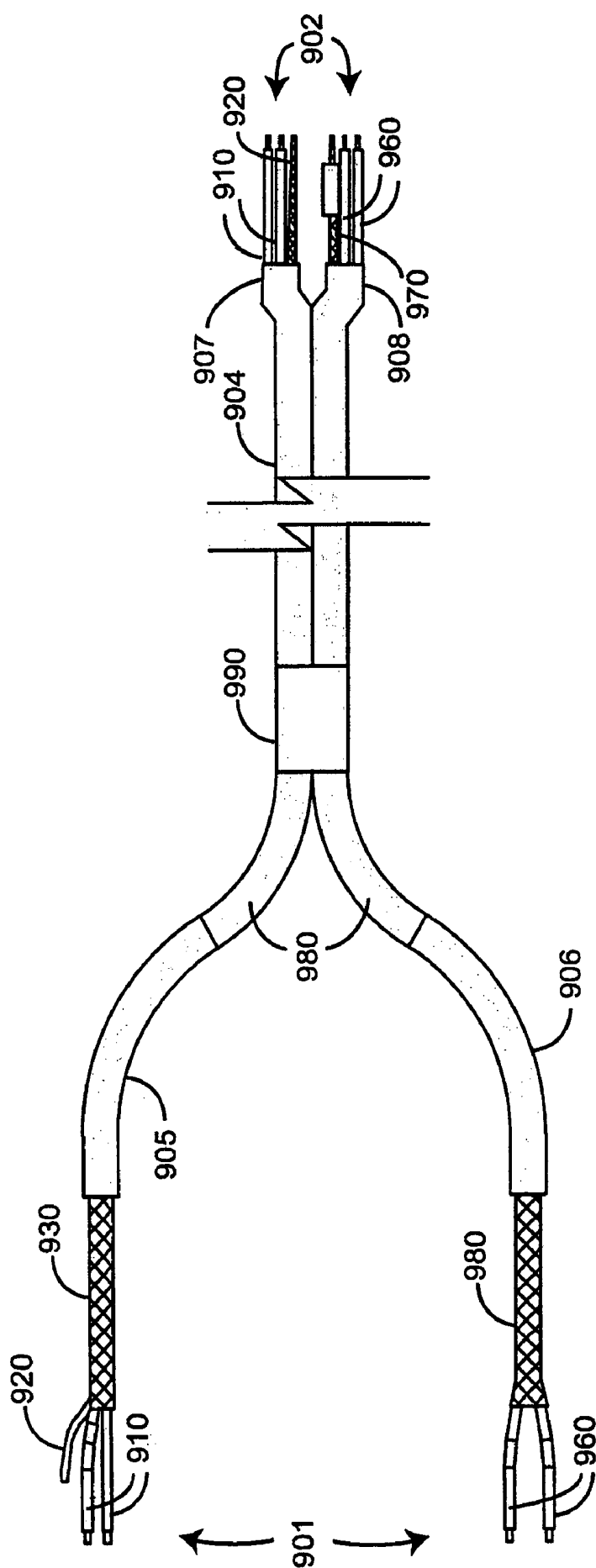


FIG. 9

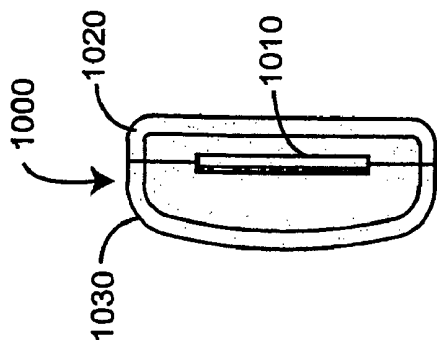


FIG. 10B

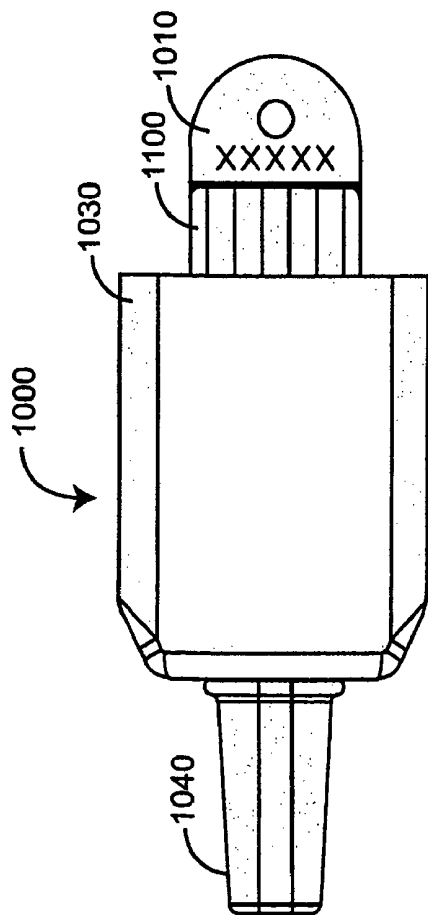


FIG. 10A

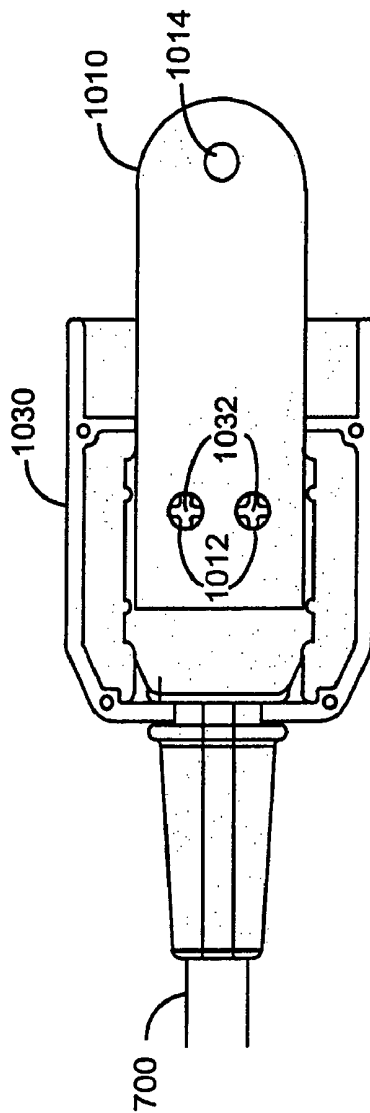


FIG. 10C

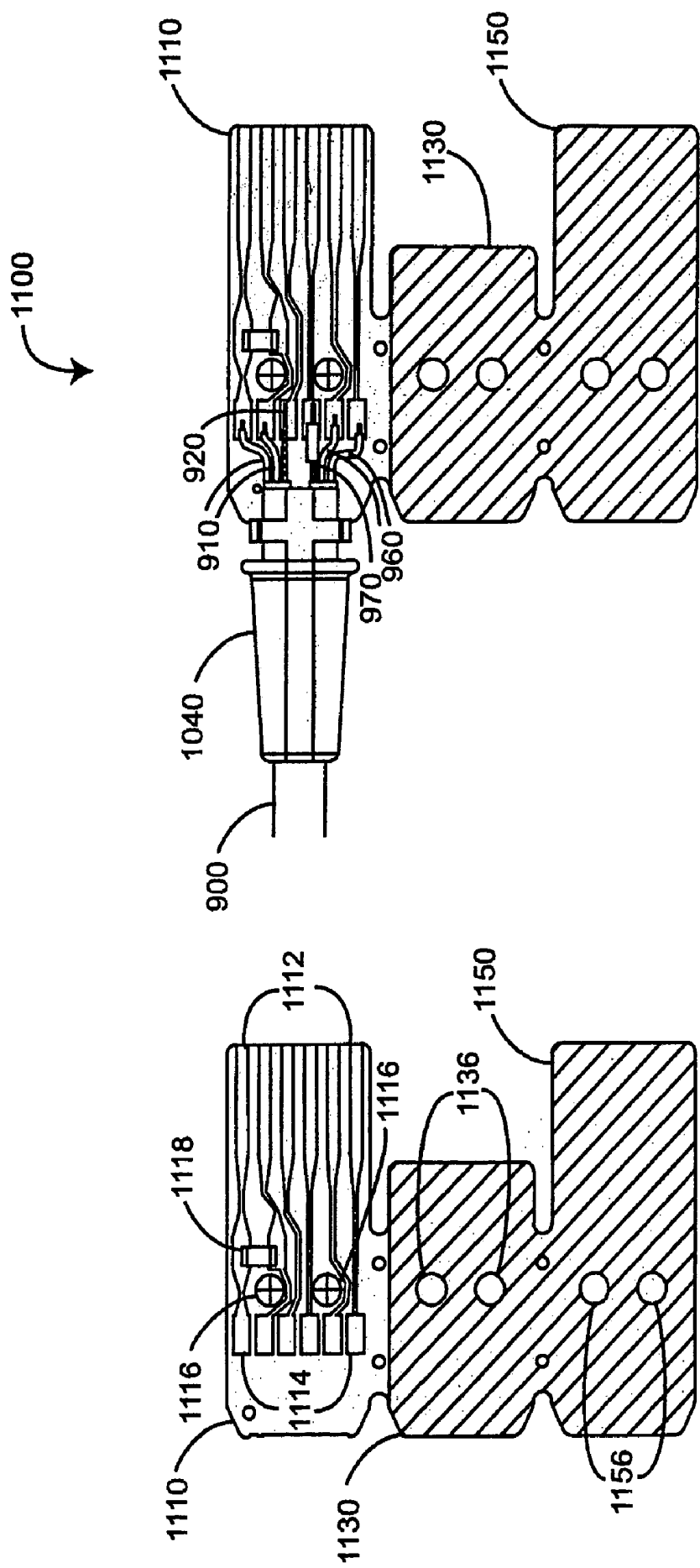
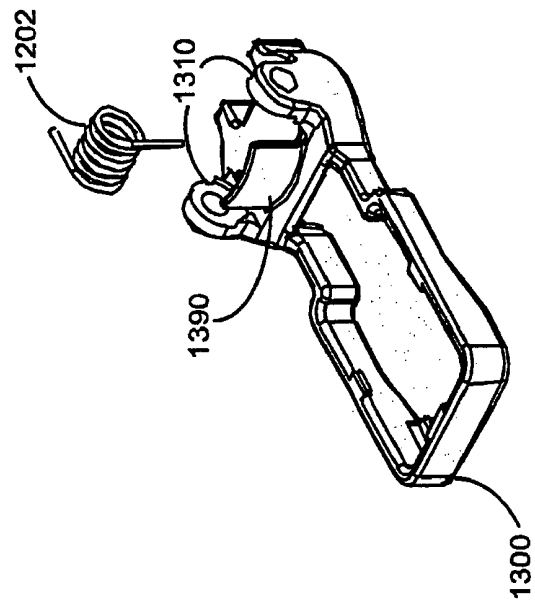
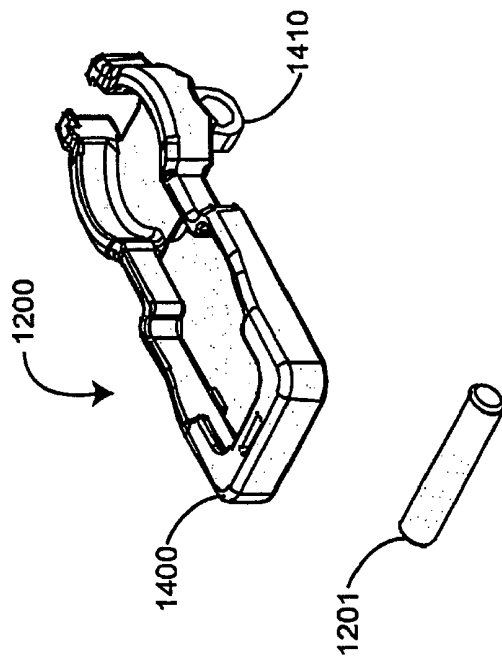
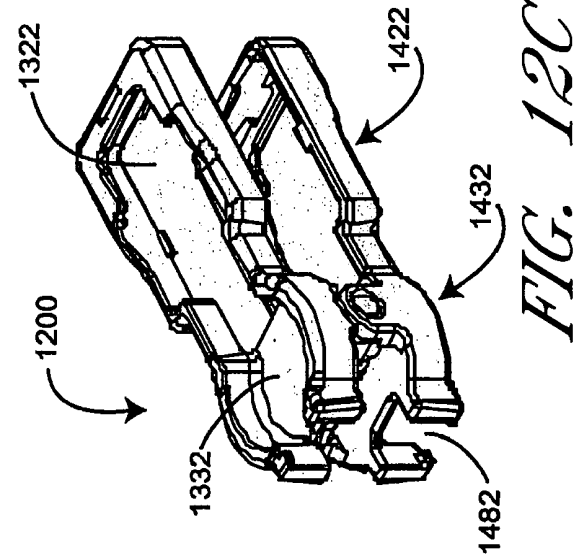
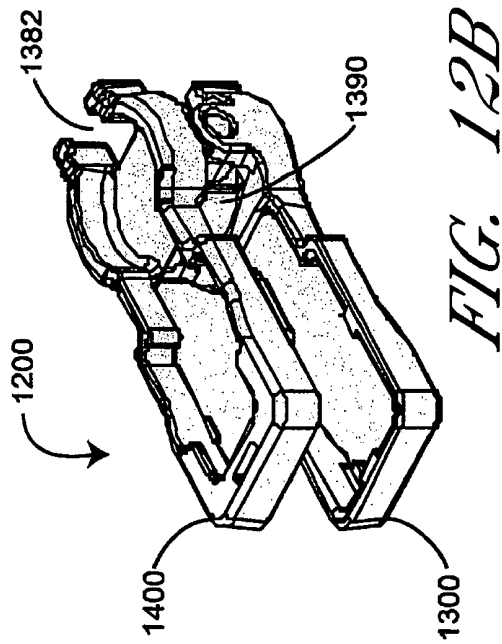


FIG. 11B

FIG. 11A



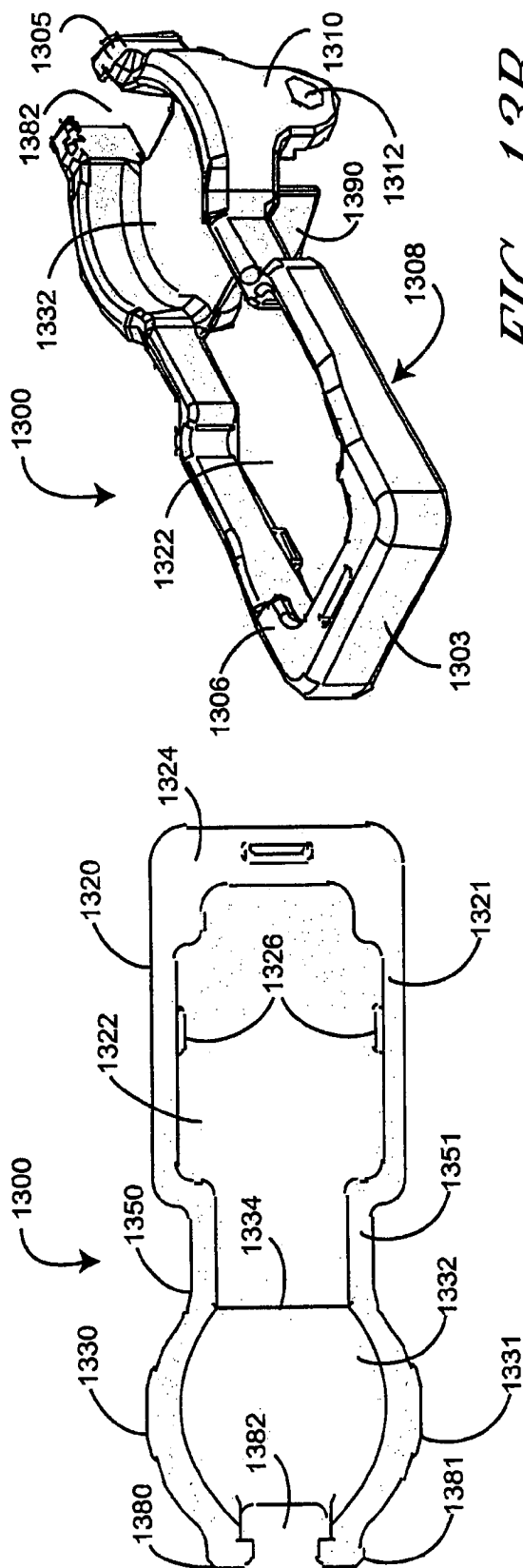


FIG. 13A

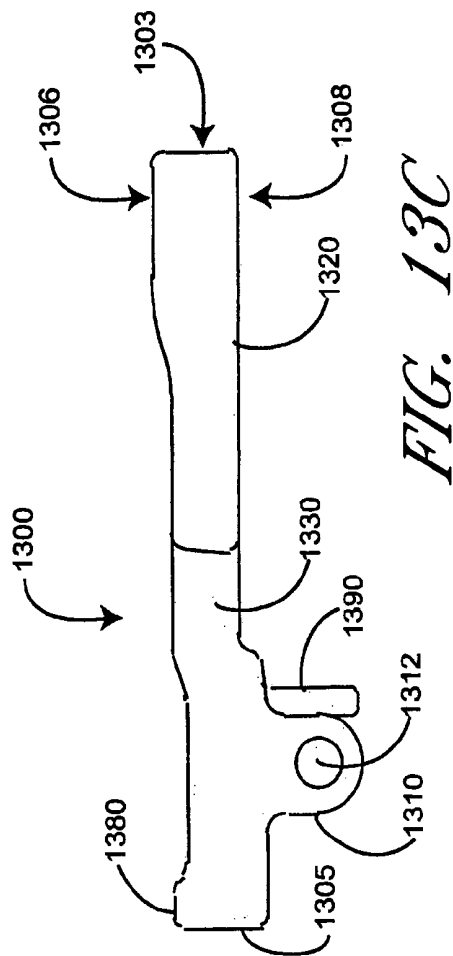


FIG. 13B

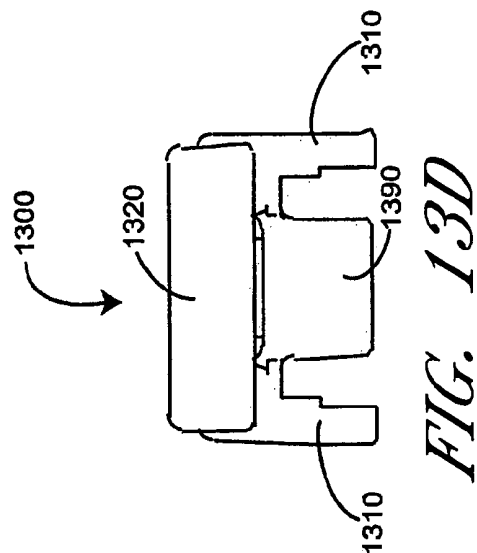
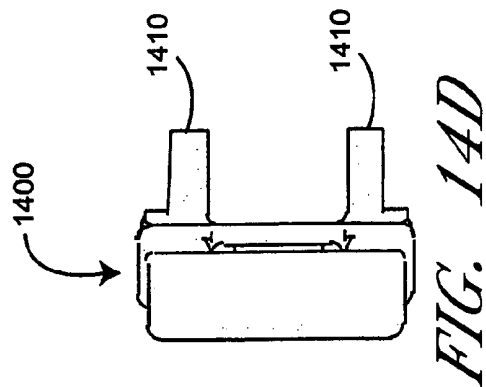
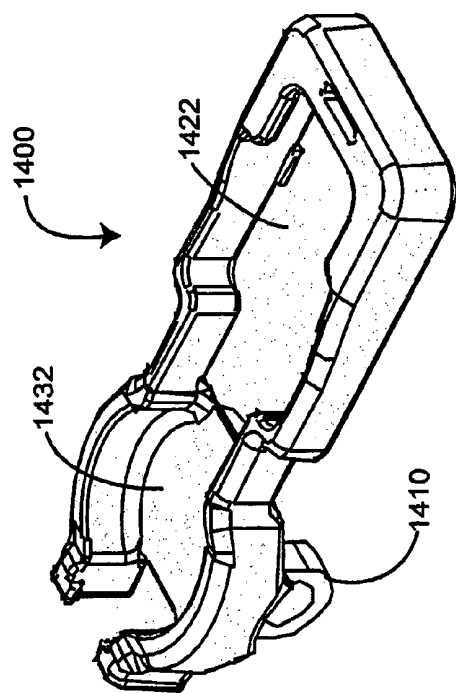
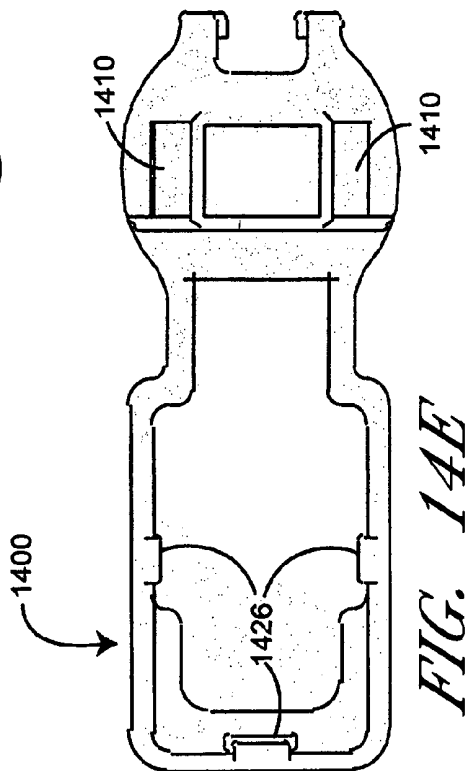
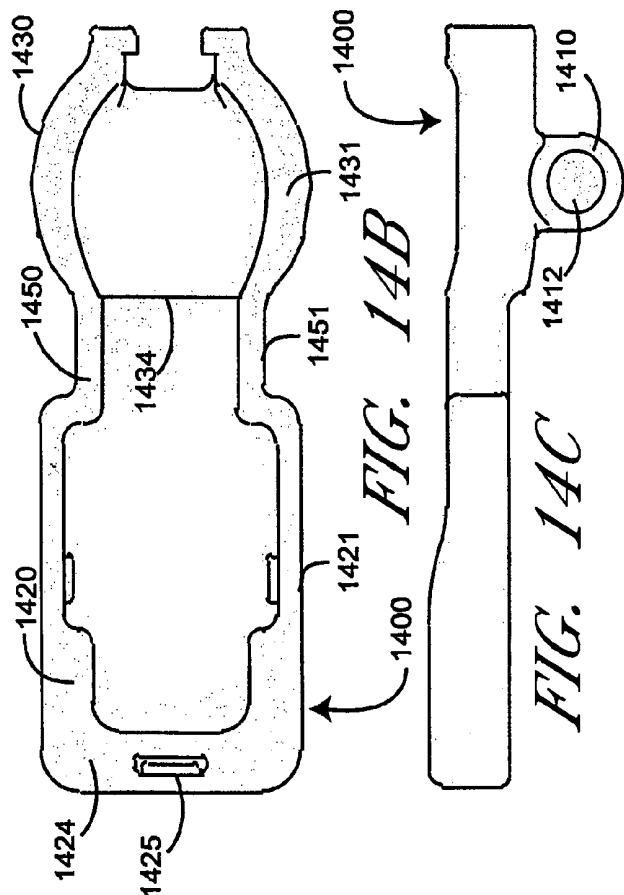
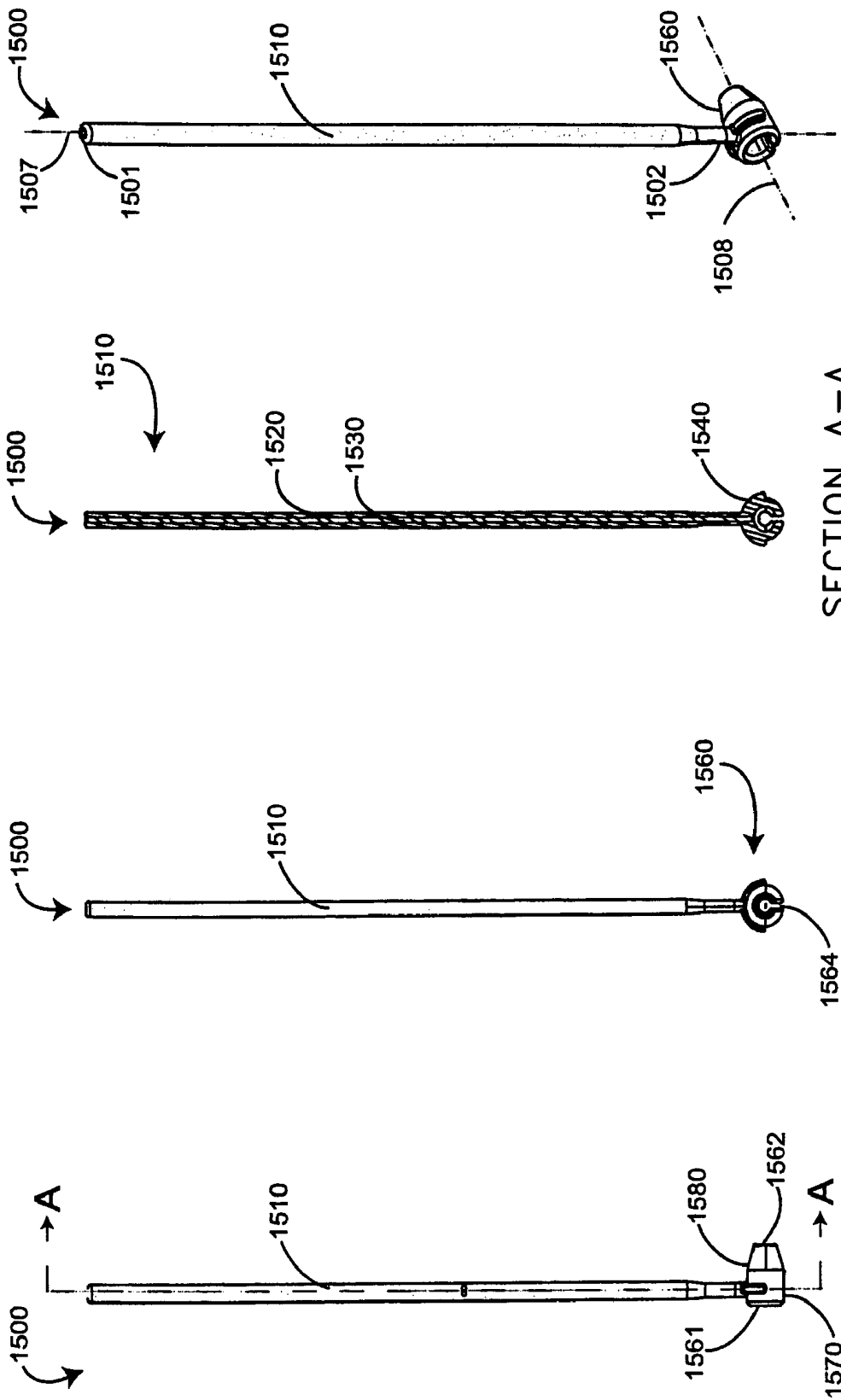


FIG. 13D

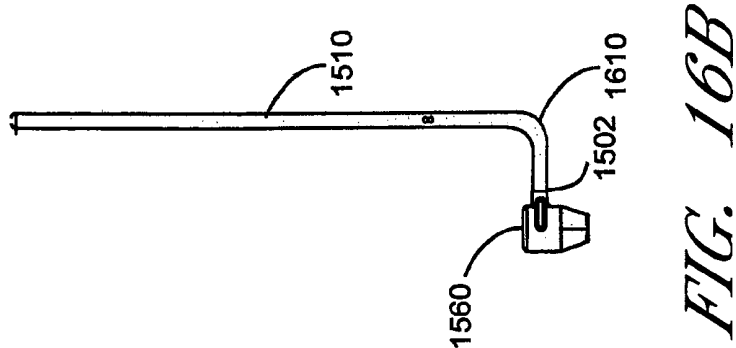
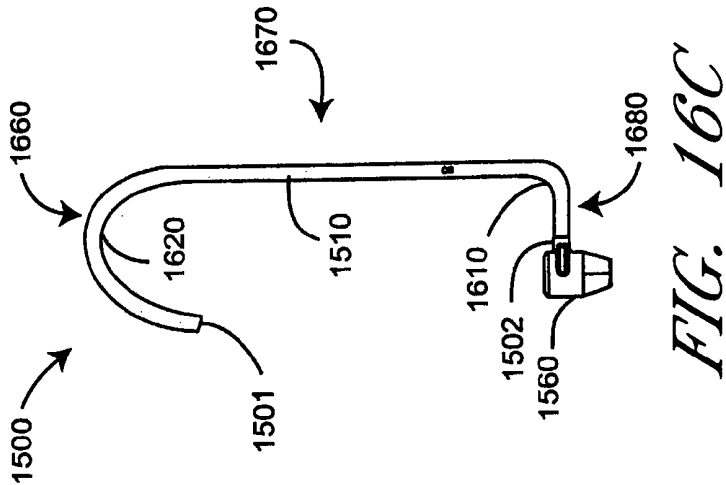
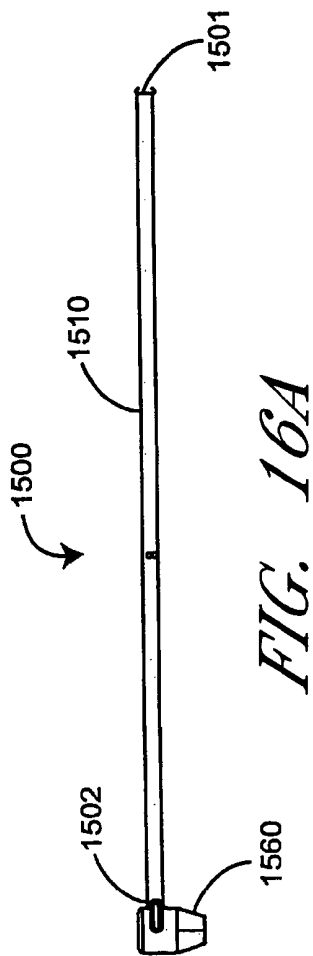




SECTION A-A

FIG. 15A      FIG. 15B      FIG. 15C      FIG. 15D





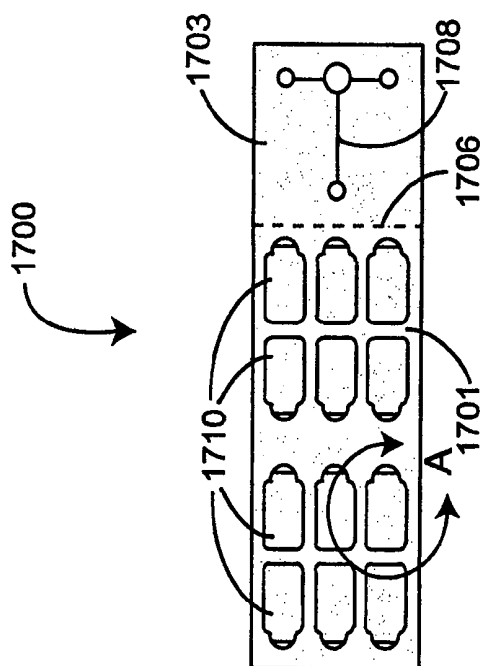
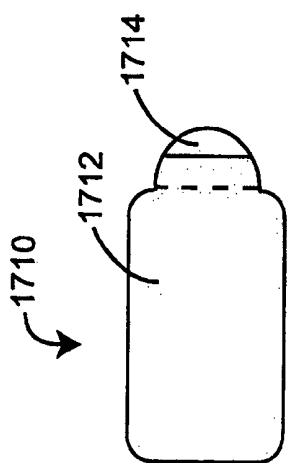


FIG. 17A



DETAIL A

FIG. 17C

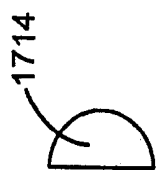


FIG. 17E

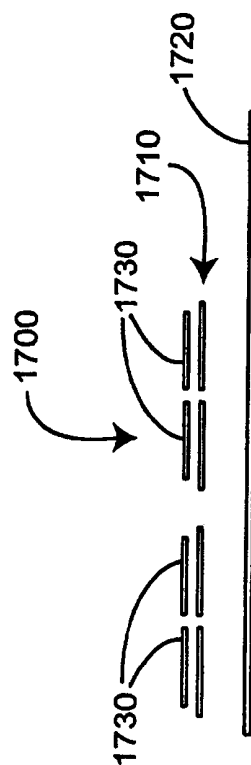


FIG. 17B

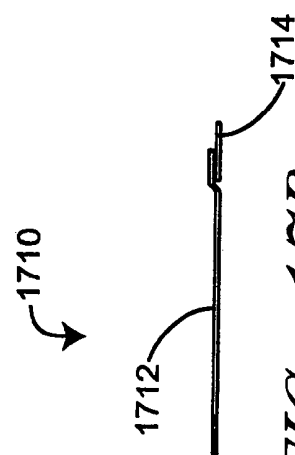


FIG. 17D

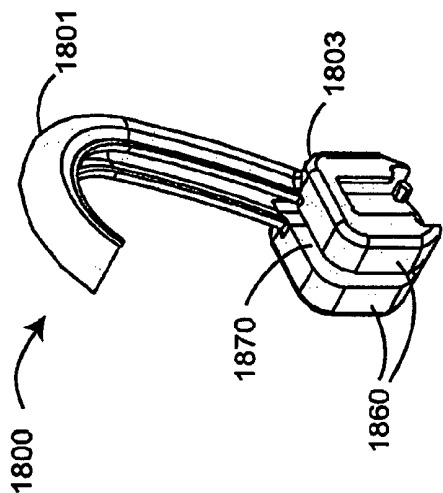


FIG. 18B

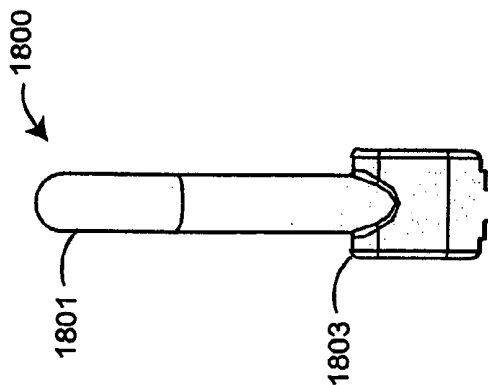


FIG. 18D

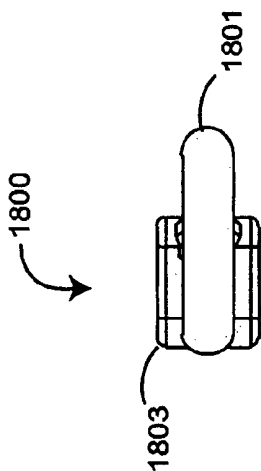


FIG. 18A

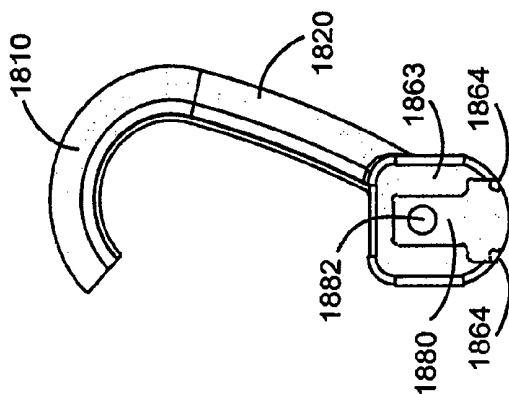


FIG. 18C

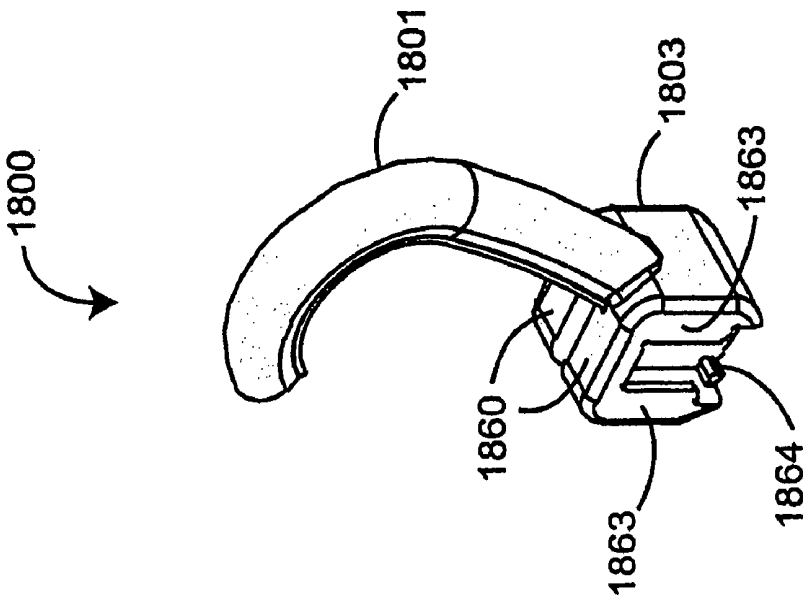


FIG. 18E

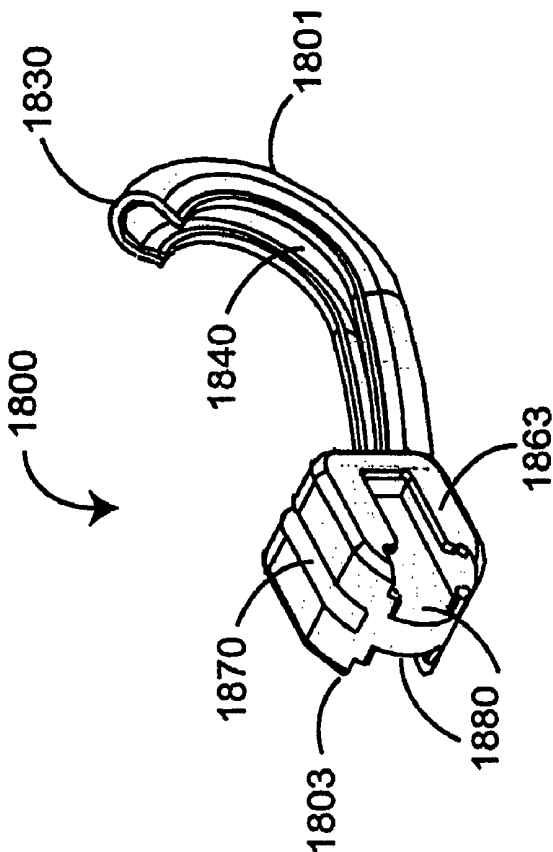


FIG. 18F

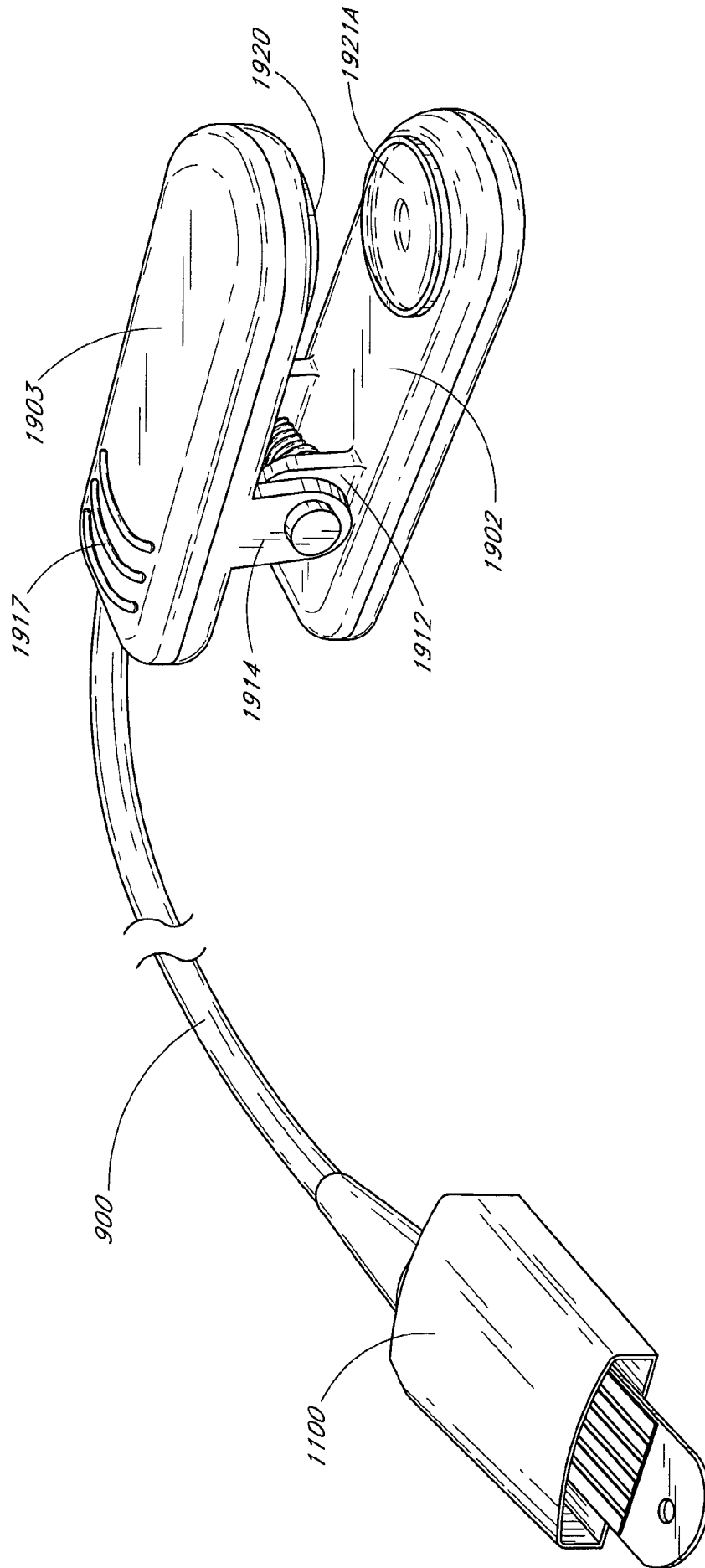
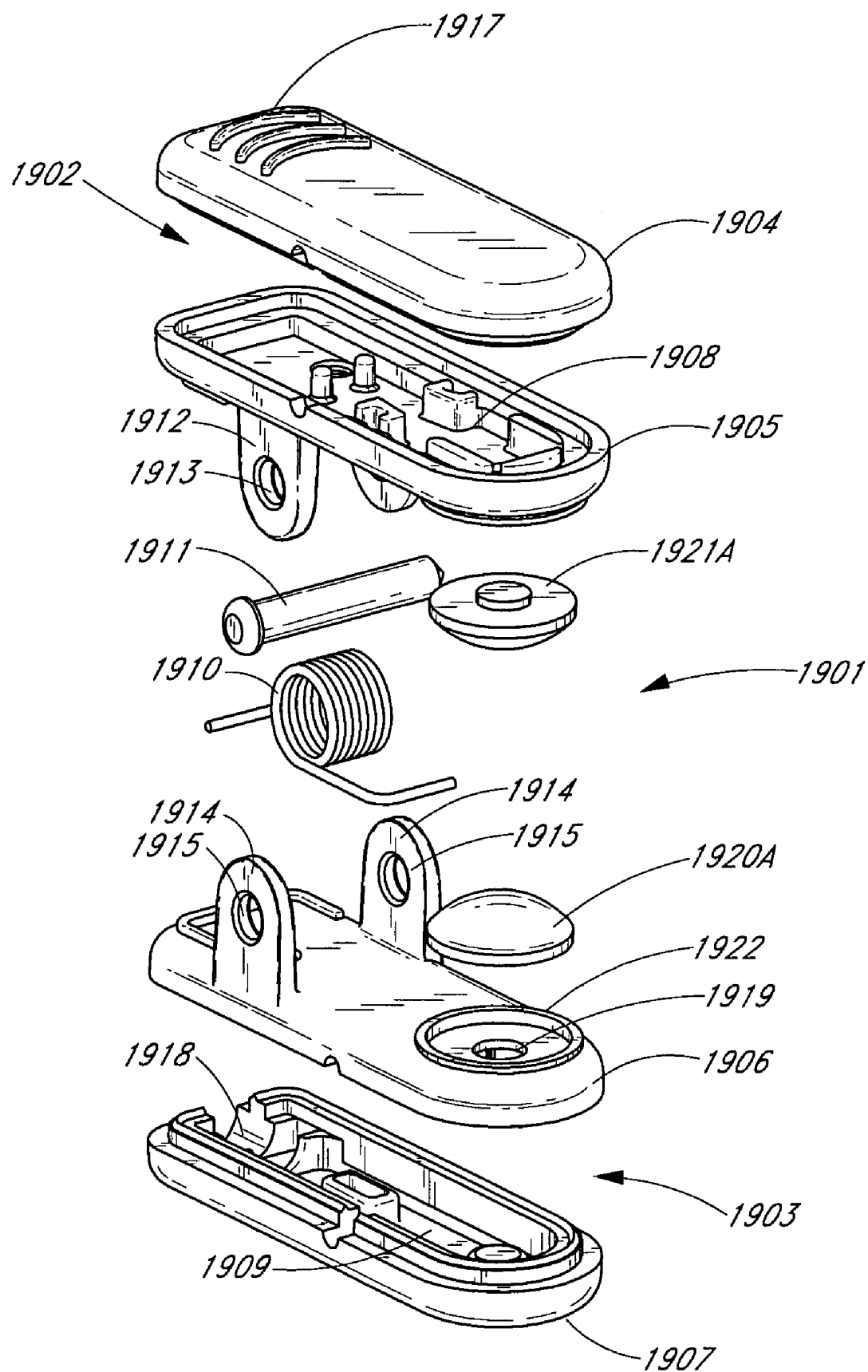
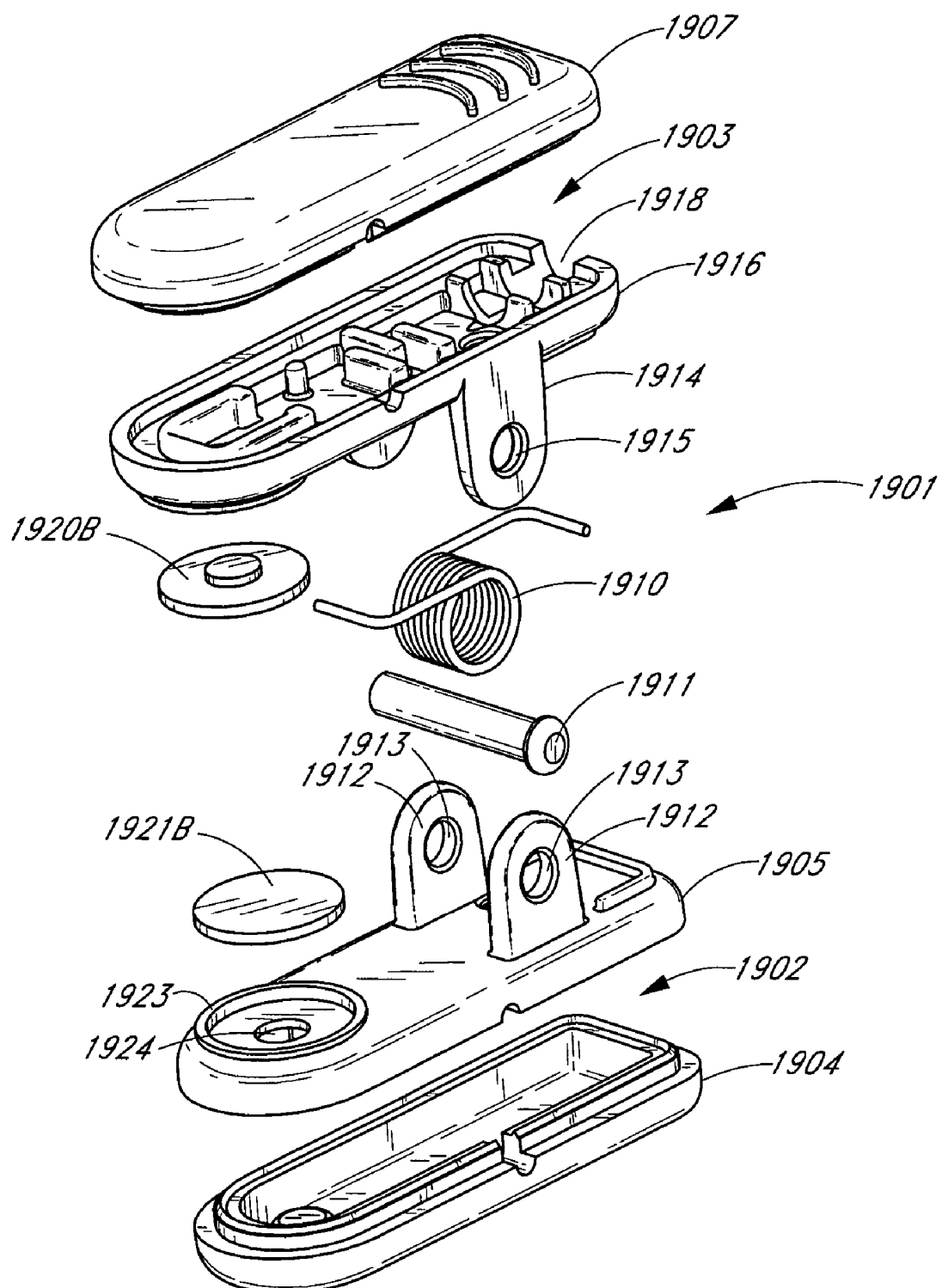
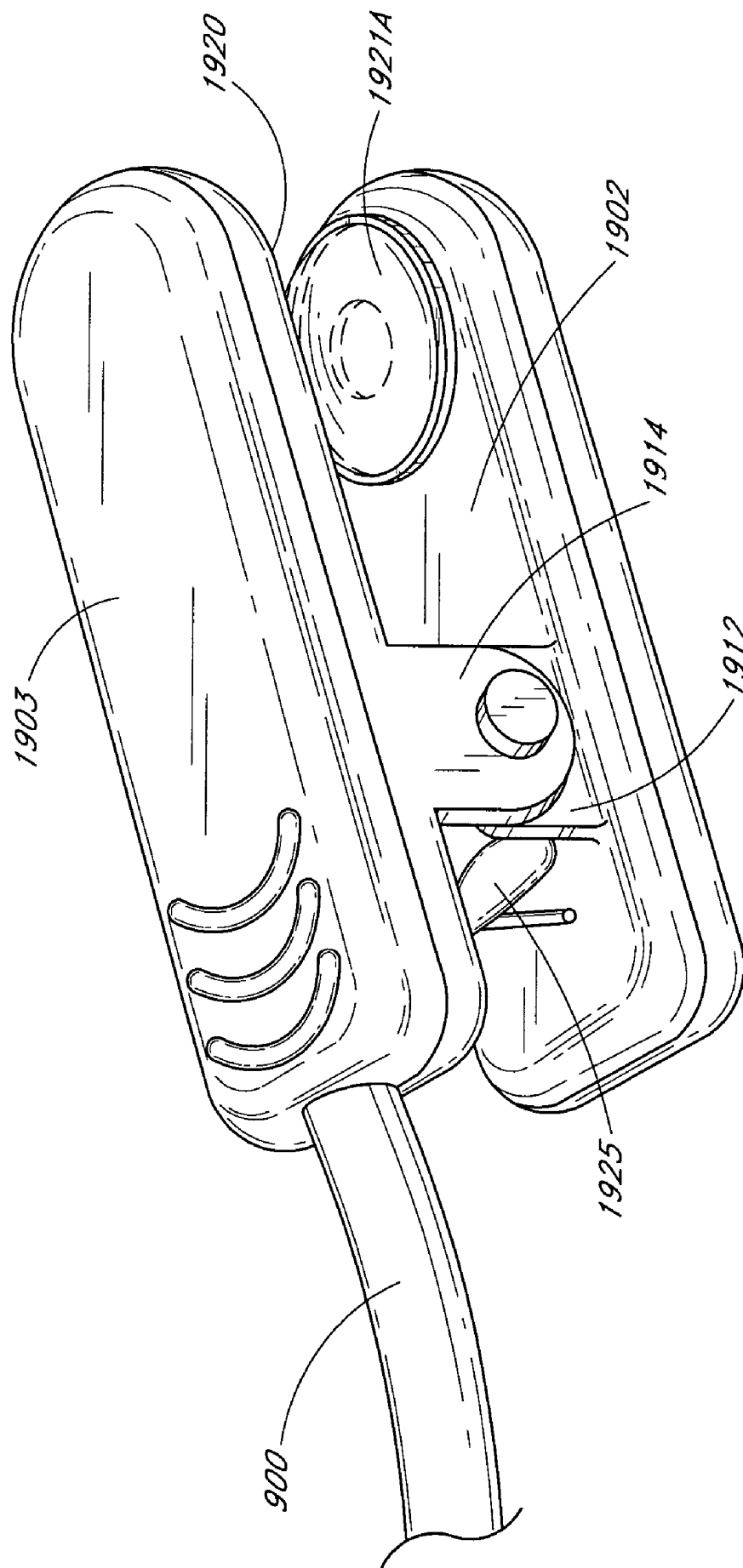


FIG. 19A

*FIG. 19B*

*FIG. 19C*



*FIG. 19D*



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**PULSE OXIMETRY EAR SENSOR**

## REFERENCE TO RELATED APPLICATIONS

The present application claims the benefit of U.S. Provisional Application Nos. 60/412,281, filed Sep. 21, 2002, entitled, "Pulse Oximetry Ear Sensor" and 60/410,499, filed Sep. 14, 2002, entitled, "Pulse Oximetry Ear Sensor," the disclosures of which are incorporated by reference herein.

## FIELD OF THE INVENTION

The present invention relates to the field of medical devices. More specifically, the invention relates to pulse oximetry sensors.

## BACKGROUND OF THE INVENTION

Pulse oximetry is a noninvasive procedure for measuring the oxygen saturation level of arterial blood, an important parameter in critical patient care applications. Pulse oximeters generally perform a spectral analysis of the pulsatile component of arterial blood in order to determine the relative concentration of oxygenated hemoglobin, the major oxygen carrying constituent of blood, to depleted hemoglobin. A pulse oximetry system includes of a sensor and a monitor. The sensor includes emitters generally having at least one red light emitting diode (LED) and at least one infrared LED that project light through blood vessels and capillaries underneath a tissue site, such as a fingernail bed. The sensor also has a detector typically consisting of a photodiode positioned opposite the LEDs so as to detect the emitted light as it emerges from the tissue site. Pulse oximeters have gained rapid acceptance in a wide variety of medical applications, including surgical wards, intensive care units, general wards and home care by providing early detection of decreases in the arterial oxygen supply and thereby, reducing the risk of accidental death and injury.

## SUMMARY OF THE INVENTION

A pulse oximetry sensor may be attached to a variety of tissue sites including a finger, a foot, an ear, a forehead, and the like. An ear site has the advantage of providing a fast response to central changes in oxygenation or lack thereof. Conventional ear sensors, however, have the disadvantage of constricting the ear site because such designs use the monitoring site to secure sensor attachment.

One aspect of a pulse oximetry ear sensor is an assembly configured to relieve patient discomfort and pressure necrosis. The assembly comprises an emitter pad and a detector pad, along with a clip configured to removably retain each of the pads. The clip has an open position for placement on an ear tissue site and a closed position for securing the pads to opposite sides of the site. The assembly includes a sensor connector adapted to electrically communicate with a host instrument. A sensor cable has a first end terminating at the pads and a second end terminating at the sensor connector and provides electrical communications between the pads and the connector. In one embodiment, the assembly includes an attachment supplement configured to assist the clip in securing the pads to the ear tissue site.

Another aspect of a pulse oximetry ear sensor are the steps of assembling a sensor with an attachment, positioning the sensor against an ear tissue site with the attachment and supplementing the attachment so as to reduce pressure on said site. A further aspect of a pulse oximetry ear sensor is

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a sensing means for transmitting and receiving an optical signal to and from a tissue site, an attachment means for securing the sensing means to the site and a supplemental means for assisting the attachment means in securing the sensing means to the site.

Yet another aspect of a pulse oximetry ear sensor is one or more silicone lenses that can be incorporated into a clip type oximetry sensor and can aid in relieving patient discomfort and pressure necrosis. In one embodiment, the lenses can provide grippy surfaces in contact with the patient's skin, which helps to keep the sensor from slipping off the patient's earlobe or other suitable tissue site. The silicone lenses can also provide pliable contact surfaces that accommodate the patient's skin shape and help to relieve the earlobe or other suitable tissue site from undue pressure. In one embodiment, the clip type sensor includes windows for the optical components of an oximetry sensor that allow for transmission of optical energy to or from a tissue site. The silicone lenses each comprise a translucent silicone material covering the foregoing windows.

For purposes of summarizing the invention, certain aspects, advantages and novel features of the invention have been described herein. Of course, it is to be understood that not necessarily all such aspects, advantages or features will be embodied in any particular embodiment of the invention.

## BRIEF DESCRIPTION OF THE DRAWINGS

A general architecture that implements the various features of the invention will now be described with reference to the drawings. The drawings and the associated descriptions are provided to illustrate embodiments of the invention and not to limit the scope of the invention. Throughout the drawings, reference numbers are re-used to indicate correspondence between referenced elements. In addition, the first digit of each reference number indicates the figure in which the element first appears.

FIG. 1 is a perspective view of a pulse oximetry ear sensor attached to a patient, according to an embodiment of the invention;

FIG. 2 is a perspective view of an ear sensor assembly;

FIG. 3 is a perspective view of an ear sensor;

FIG. 4 is an exploded perspective view of an ear sensor;

FIGS. 5A-B are top and perspective views, respectively, of ear sensor pad assemblies;

FIGS. 6A-B are top and perspective views, respectively of a pad base;

FIG. 7 is a perspective view of a pad cover;

FIGS. 8A-B are top views of a detector shield without and with a mounted detector, respectively;

FIG. 9 is a top view of an ear sensor cable;

FIGS. 10A-C are top enclosed, end enclosed, and bottom unenclosed views of a modular plug;

FIGS. 11A-B are top views of a connector flex circuit, with and without an attached sensor cable, respectively;

FIGS. 12A-C are exploded, front perspective and back perspective views, respectively, of a sensor clip;

FIGS. 13A-D are top, perspective, side and front-end views, respectively, of a clip outer jaw;

FIGS. 14A-E are perspective, top, side, bottom and front-end views, respectively, of a clip innerjaw;

FIGS. 15A-D are side, back, sectional and back perspective views, respectively, of an ear hanger;

FIGS. 16A-C are side views of an unformed, partially formed and fully formed ear hanger, respectively;

FIGS. 17A-E are views of an adhesive tab and an associated tab carrier;

FIGS. 17A-B are top and side views of a tab carrier;  
FIGS. 17C-D are top and side views of an adhesive tab;  
and

FIG. 17E is a top view of a tab handle; and

FIGS. 18A-F are top, front perspective, side, back, rear  
perspective and bottom perspective views, respectively, of  
an ear sensor boot.

FIGS. 19A-D are assembled front perspective, exploded  
bottom, exploded top, and rear perspective views, respec-  
tively, of an ear sensor clip with one or more silicone lenses.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

To facilitate a complete understanding of the invention,  
the remainder of the detailed description describes the  
invention with reference to the drawings, wherein like  
reference numbers are referenced with like numerals  
throughout.

FIG. 1 illustrates a pulse oximetry ear sensor assembly  
100 attached to an ear monitoring site 10. The ear sensor  
assembly 100 includes an ear sensor 300, a replaceable clip  
1200, an ear hanger 1500 and adhesive tabs 1710. The clip  
1200 advantageously has a relatively low spring tension and  
the area of the ear sensor 300 that contacts the ear is  
relatively large compared with conventional ear sensors,  
allowing longer monitoring on the ear by reducing patient  
discomfort and pressure necrosis. To provide secure sensor  
attachment to the ear site 10, the ear sensor assembly 100  
optionally utilizes an ear hanger 1500 and adhesive tabs  
1710, individually or in combination, to supplement the clip  
1200. The ear hanger 1500 goes around the ear, much like  
sports glasses, and supports the weight of the ear sensor  
assembly 100. The adhesive tabs 1710 may be added to the  
ear sensor 300 to provide adhesive attachment to the tissue  
site 10. Further, a clasp (not shown) may be added to a  
sensor cable 900 (FIG. 2) and attached to patient clothing,  
for example, to provide strain relief and reduce the risk that  
accidental cable snags might pull the ear sensor 300 off of  
the ear.

FIG. 2 further illustrates the ear sensor assembly 100. Ear  
sensor pads 500 removably press-fit into the clip 1200. The  
clip 1200 advantageously allows inexpensive replacement  
of a moving part upon wear or breakage. The ear hanger  
1500 removably clamps to an ear sensor cable 900. The ear  
hanger 1500 is advantageously constructed to be easily bent  
and shaped to comfortably fit various ear shapes and sizes,  
as described in further detail with respect to FIGS. 15-16,  
below. The ear hanger 1500 is provided to users either  
straight or preformed as shown in FIG. 16C. Additionally,  
FIG. 2 shows the ear sensor assembly including one or more  
integrated finger grips 620 as will be described in further  
detail with respect to FIG. 10 below.

FIG. 3 illustrates the ear sensor 300 including the sensor  
pads 500, the sensor cable 900 and a modular connector  
1000. The sensor pads 500 house the sensor optical com-  
ponents and include a detector pad 506 and an emitter pad  
507. The sensor cable 900 provides a signal path between the  
sensor pads 500 and the modular connector 1000. The  
modular connector 1000 provides pinouts for a patient cable  
(not shown), which is used to provide communication  
between the ear sensor 300 and a pulse oximeter (not  
shown).

FIG. 4 illustrates pieces of the ear sensor 300. The sensor  
pads 500 advantageously include a common base 600 and  
cover 700 for each of the detector pad 506 and the emitter  
pad 507. According to an embodiment used, the base 600

and cover 700 reduces or even minimizes the number of  
unique parts for the ear sensor 300. The detector pad 506  
houses a shielded detector assembly 800. The emitter pad  
507 houses an emitter 400. The modular connector 1000  
includes a connector flex circuit 1100 installed onto a tab  
1010 and enclosed between a bottom cover 1020 and a top  
cover 1030 that clasp a bend relief 1040.

FIGS. 5A-B further illustrate exemplary embodiments of  
the detector and emitter pads 500. As shown in FIG. 5A,  
both the detector (not visible) within the shielded detector  
assembly 800 and the emitter 400 are connected to the  
sensor cable 900 after the cable is inserted into the respective  
bases 600. As shown in FIG. 5B, the cover 700 is secured in  
place onto the base 600 so as to enclose, and in an embodi-  
ment, seal the shielded detector assembly 800 and emitter  
400 in their respective housings.

FIGS. 6A-B illustrate a base 600 having a bend relief 610,  
the integrated finger grip 620, a head 630 and a head  
extension 640. The base 600 has a cable end 601 and a head  
end 602. The bend relief 610 extends between the cable end  
601 and the finger grip 620 and is configured to accept one  
end of the sensor cable 900 (FIG. 9). The bend relief 610 is  
adapted to reduce bending stress on the sensor cable 900  
(FIG. 9). The finger grip 620 extends between the bend relief  
610 and the head extension 640 and provides a finger  
pressing surface so as to open the clip 1200 (FIGS. 12A-C).  
In one embodiment, the finger grip 620 provides a generally  
round, planar surface that may be comprised of a generally  
pliable material.

As shown in FIGS. 6A-B, the head 630 extends between  
the head end 602 and the head extension 640, opposite the  
head extension 640 from the finger grip 620. The head 630  
has an open face 632 and an opposite, generally planar pad  
face 634. The pad face 634 provides a generally planar  
contact surface for a tissue site. Advantageously, the pad  
face 634 has a relatively large area to minimize the force on  
a tissue site. In one embodiment, the area of the pad face 634  
is in the range of about 0.225 sq. in. to about 0.325 sq. in.  
In a particular embodiment, the pad face 634 is generally  
rectangular. In a specific embodiment, the pad face 634 has  
dimensions of about 0.69 in. by about 0.45 in. However, a  
skilled artisan will recognize from the disclosure herein that  
the pad face 634 may be sized to take into account a wide  
variety of parameters, including for example, tissue site size,  
component size, necrosis, patient comfort, combinations of  
the same or the like.

Also shown in FIGS. 6A-B, the open face 632 is config-  
ured to accept an optical component. In one embodiment,  
the open face 632 has a raised wall 650 defining a compo-  
nent cavity 652 configured to accept and retain either an  
emitter 400 (FIG. 4) or a detector assembly 800 (FIG. 4).  
The open face 632 also defines a window 654 that provides  
an aperture for transmission of optical energy to or from a  
tissue site. In one embodiment, the window 654 is filled with  
a translucent silicone material as will be further described  
with reference to FIG. 19. The extension 640 extends  
between the finger grip 620 and the head 630 and provides  
a channel 642 for the sensor cable 900 (FIG. 9). In one  
embodiment, the open face 632 is closed and sealed with the  
pad cover 700 (FIG. 7). The base 600 has slots 660 disposed  
along the base edges. The slots 660 are configured to mate  
with corresponding clip tabs 1326 (FIGS. 13A-D), 1426  
(FIGS. 14A-E) so as to retain the pads 500 (FIGS. 5A-B)  
within the clip 1200 (FIGS. 12A-C), as described with  
respect to FIGS. 12A-C, below.

FIG. 7 illustrates a pad cover 700 having a platform 710,  
a raised cap 720 and an extension 730. The cover 700 can be

configured to close and seal the base **600** (FIGS. 6A-B), as described with respect to FIG. 5B. In particular, the platform **710** corresponds to the open face **632** and covers an optical component. The raised cap **720** accommodates an optical component accordingly. The extension **730** corresponds to the channel **642** (FIGS. 6A-B) and covers the sensor cable leads. Both the base **600** (FIGS. 6A-B) and the cover **700** can be injection molded of a pliant material. In one embodiment, the material is a medical grade thermoplastic elastomer, such as AES Santoprene, #281-45. In a particular embodiment, the base **600** (FIGS. 6A-B) is constructed of a reflective material so as to advantageously reflect scattered light back into the tissue site, while the cover **700** is constructed of an absorbent material so as to block ambient light for noise reduction at the detector.

FIGS. 8A-B illustrate the shielded detector assembly **800**, having a shield **801** and a detector **802**. The shield **801** has a back shield **810**, a front shield **820** having a grid **822**, a detector lead shield **830** and a cable lead shield **840**. The detector **802** is placed on the shield **801** so that the front, light-receiving face (not visible) is proximate to and aligned with the grid **822**. The sensor cable **900** is attached to the detector **802** so that the detector cable leads **910** are electrically connected to the detector leads **803** and the detector cable shield lead **920** is electrically connected to the cable lead shield **840**. The shield **801** is then folded so that the back shield **810** is placed over the back face of the detector **802**, the sides of the front shield **820** are placed over the detector sides, the detector lead shield **830** is folded over the detector leads **803** and the cable lead shield **840** is folded over the cable leads **920**.

FIG. 9 illustrates a sensor cable **900** having a sensor end **901**, a connector end **902**, a cable midsection **904**, a detector cable **905** and an emitter cable **906**. Both the detector cable **905** and emitter cable **906** extend between the sensor end **901** and the connector end **902**. The detector cable **905** and emitter cable **906** are joined throughout the cable midsection **904**. The detector cable **905** and emitter cable **906** are separated at a Y-section **980** proximate the sensor end **901**. A binder **990**, such as a shrink-wrap insulator or an over mold section, binds the cable **900** between the Y-section **980** and the midsection **904** to prevent the Y-section **980** from extending into the midsection **904** by inadvertent separation of the detector cable **905** and emitter cable **906**. The detector cable **905** has detector cable leads **910** and a detector cable shield **930** that has a shield lead **920** formed from the shield **930** at both the sensor end **901** and the connector end **902**. The emitter cable **906** has emitter cable leads **960** and an emitter cable shield **980** that has a shield lead **970** formed from the shield **980** at the connector end **902**. An insulator **972** on the emitter cable shield lead **970** prevents electrical contact with the detector cable shield lead **920**.

FIGS. 10A-C illustrate the cable connector **1000** having a tab **1010**, a lower shell **1020**, an upper shell **1030** and a bend relief **1040**. As shown in FIG. 10A, the tab **1010** supports a flexible circuit assembly **1100**, which provides connector pinouts and connections to the sensor cable **900**, as described with respect to FIGS. 11A-B, below. The lower shell **1020** and upper shell **1030** are mating halves of the connector body, which provides a grip for connecting to a patient cable, protects the flexible circuit connections and retains the bend relief **1040**. The bend relief **1040** prevents the sensor cable **900** from bending a sharp angles at the boundary of the connector body **1020**, **1030**. As shown in FIG. 10C, the tab **1010** has a catch **1014** that provides a locking mechanism for a patient cable connector, such as described in U.S. Pat. No. 6,152,754 entitled "Circuit Board

Based Cable Connector," assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein. The tab **1010** also has apertures **1012** that accept corresponding posts **1032** of the upper shell **1030**. The posts **1032** fit into corresponding standoffs (not shown) of the lower shell **1020** so that the tab is held in position between the lower shell **1020** and upper shell **1030**.

FIGS. 11A-B illustrate a self-shielding flexible circuit assembly **1100** having a printed circuit **1110**, a top shield **1130** and a bottom shield **1150**. As shown in FIG. 11A, the printed circuit **1110** has pinouts **1112**, lead pads **1114**, apertures **1116** and an information element **1118**. The pinouts **1112** are electrically connected to corresponding ones of the lead pads **1114** and provide the connection to a mating patient cable connector. The apertures **1116** align with upper shell posts **1032** (FIG. 10C). The information element **1118** provides sensor information, such as sensor type, to a compatible pulse oximeter instrument connected to the ear sensor **300** (FIG. 3) via a patient cable (not shown). An information element is described in U.S. Pat. No. 6,011,986 entitled "Manual And Automatic Probe Calibration," assigned to Masimo Corporation, Irvine, Calif. and incorporated by referenced herein.

As shown in FIG. 1B, the sensor cable **900** is integrated with the flexible circuit assembly **1100** with the cable leads **910**, **920**, **960**, **970** attached and electrically connected to corresponding ones of the lead pads **1114**, such as with a soldered connection. After the sensor cable **900** is attached to the printed circuit **1110**, the top shield **1130** is folded over the printed circuit traces **1112**, **1114** and the bottom shield **1150** is wrapped around the printed circuit **1110** and folded over the bottom of the printed circuit **1110**. In this manner, the connections, in particular the detector leads **910**, are EMI shielded and physically protected. The top shield **1130** and bottom shield **1150** are folded so that top shield apertures **1136** and bottom shield apertures **1156** align with the printed circuit apertures **1116**. The folded flexible circuit assembly **1100** is attached to the tab **1010** (FIGS. 10A-C) with an adhesive, such as PSA, and mounted within the connector shells **1020**, **1030** (FIG. 10B), as described above.

FIGS. 12A-C illustrate a removable sensor clip **1200**. As shown in FIG. 12A, the removable clip **1200** has an outer jaw **1300**, an inner jaw **1400**, a hinge pin **1201**, and a hinge spring **1202**. The outer jaw **1300** has an outer hinge support **1310**, and the inner jaw **1400** has an inner hinge support **1410**. The clip **1200** is assembled with the hinge supports **1310**, **1410** aligned, the spring **1202** between the hinge supports **1310**, **1410**, and the pin **1201** inserted through the hinge supports **1310**, **1410** and the spring **1202** so as to rotatably attach the jaws **1300**, **1400** at their respective hinge supports **1310**, **1410**. The spring **1202** urges the jaws to a closed position in which the sensor pads **500** (FIGS. 5A-B) are held against an earlobe or other suitable tissue site.

The spring **1202** is advantageously designed so that the force the jaws **1300**, **1400** exert on a tissue site is relatively small. In an embodiment, the ear sensor assembly **300** (FIG. 3) utilizes various attachment mechanisms to supplement or supplant the jaw force in maintaining sensor attachment to the tissue site, including an ear hanger **1500** (FIGS. 15A-D), ear boot **1800** (FIGS. 18A-F), adhesive tabs **1710** (FIG. 17C), and/or silicone lenses (FIGS. 19A-D) described below. In a preferred embodiment, the force of the jaws **1300**, **1400** on a tissue site is in the range of about 90 gram force to about 140 gram force. In a more preferred embodiment, the jaw force is in the range of about 115 gram force to about 130 gram force. In a most preferred embodiment, the jaw force is about 116 gram force. However, an artisan

will recognize from the disclosure herein that a wide number of ranges can be implemented for the jaw force. For example a clip used on trauma or other potentially active patients or difficult tissue sites may use more or less force.

As shown in FIGS. 12B-C, the assembled clip 1200 has opposing head holders 1322, 1422 that removably retain the head portions 630 (FIGS. 6A-B) of the sensor pads 500 (FIGS. 5A-B). The assembled clip 1200 also has opposing grip holders 1332, 1432 that removably retain the finger grips 620 (FIGS. 6A-B). The finger grips 620 (FIGS. 6A-B) are squeezed so as to move the jaws 1300, 1400 to an open position in which the pads 500 (FIGS. 5A-B) are separated for positioning the ear sensor 300 (FIG. 3) on a tissue site or for removal of the ear sensor 300 (FIG. 3) from a tissue site. End slots 1382, 1482 removably retain the pad bend reliefs 610 (FIGS. 6A-B). A jaw stop 1390 advantageously prevents the jaws 1300, 1400 from closing to the extent that the pad faces 634 (FIGS. 6A-B) touch. In this manner, adhesive tabs 1710 (FIG. 17C) can be applied to the pad faces 634 (FIGS. 6A-B) to assist in holding the ear sensor 300 (FIG. 3) to an ear tissue site, without having the adhesive tabs 1710 (FIG. 17C) adhere to each other.

FIGS. 13A-D illustrate a clip outer jaw 1300 having a back end 1301, a front end 1303, a top side 1306 and a bottom side 1308. The outer jaw 1300 has a pair of hinge supports 1310, a head holder 1320 proximate the front end 1303, a grip holder 1330 extending from the back end 1301, a middle 1350 between and adjoining both the head holder 1320 and grip holder 1330, a bend relief holder 1380 at the back end 1301 and adjoining the grip holder 1330, and a jaw stop 1390. The hinge supports 1310 each extend from the bottom side 1308 at the grip holder 1330, generally perpendicular to the plane of the head holder 1320 and generally aligned with the grip holder walls 1331. The hinge supports 1310 each define a hinge aperture 1312 sized to accept and retain the hinge pin 1201 (FIG. 12A).

As shown in FIGS. 13A-D, the head holder 1320 has walls 1321 that extend from the top side 1306 to the bottom side 1308 around the periphery of the jaw 1300 so as to define a head holder interior 1322. A lip 1324 extends from the front end 1303 along the top side 1306 partially into the head holder interior 1322. Tabs 1326 extend from the walls 1321 partially into the interior 1322 of the head holder 1320. These tabs 1326 mate with corresponding base slots 660 (FIG. 6B). The head holder 1320 is configured to securely but removably retain a pad head 630 (FIGS. 6A-B). The grip holder 1330 has walls 1331 that extend from the top side 1306 to the bottom side 1308 around the periphery of the jaw 1300 so as to define a grip holder interior 1332. A shelf 1334 is disposed along the bottom side 1308 within the grip holder interior 1332. The grip holder 1330 is configured to securely but removably retain a finger grip 620 (FIGS. 6A-B).

Also shown in FIGS. 13A-D, the middle 1350 has walls 1351 that extend from the top side 1306 to the bottom side 1308 along the periphery of the jaw so as to connect the head holder walls 1321 and the grip holder walls 1331, the middle walls 1351 being closer together than the head holder walls 1321 or the grip holder walls 1331. The bend relief holder 1380 has walls 1381 that extend from the back end 1301 so as to define a bend relief slot 1382. The bend relief slot 1382 is configured to securely but removably retain the bend relief 610 (FIGS. 6A-B).

Further shown in FIGS. 13A-D, the jaw stop 1390 extends from the grip holder 1330 of the outer jaw 1300 along the bottom side 1308 proximate the middle 1350 generally normally from the jaw plane. The jaw stop 1390 is configured to contact a corresponding portion of the inner jaw

1400 so as to prevent the outer jaw 1300 and inner jaw 1400 from closing to the extent that installed sensor pads 500 (FIGS. 5A-B) would touch. In particular, the jaw stop 1390 advantageously prevents mutual contact and adhesion between adhesive pads 1710 (FIG. 17C) attached to the sensor pads 500 (FIGS. 5A-B).

FIGS. 14A-E illustrate a clip inner jaw 1400 having hinge supports 1410, a head holder 1420, a grip holder 1430, a middle 1450 and a bend relief holder 1480 as described with respect to FIGS. 13A-D, above. In one embodiment, the clip jaws 1300 (FIGS. 13A-D), 1400 are injection molded with an ABS/polycarbonate blend, such as GE Gycoloy #6200.

As shown in FIGS. 2, 6 and 12-14, sensor pads 500 are installed into a clip 1200 by inserting the heads 630 within the holder interiors 1322, 1422 underneath the lips 1324, 1424 and until the heads 630 are over the holder interiors 1322, 1422. The heads 630 are then pressed into the holder interiors 1322, 1422, the finger grips 620 are pressed into the grip holders 1330, 1430 and the bend reliefs 610 are pressed into the bend relief holders 1382, 1482. The pads 500 can be removed in a corresponding manner by lifting the bend reliefs 610 from the bend relief holders 1382, 1482 so that the bend relief 610, grip 620 and head 630 are released. The sensor pads 500 can then be pulled from underneath the lips 1324, 1424.

FIGS. 15A-D illustrate an ear hanger 1500. As shown in FIG. 15D, the ear hanger 1500 has a generally cylindrical stem 1510 extending from a first end 1501 to an opposite second end 1502 and a holder 1560 attached to the second end 1502, so that the stem axis 1507 is generally perpendicular to the holder axis 1508. As shown in FIGS. 15A-B, the holder 1560 has a generally cylindrical section 1570 at a first end 1561 that adjoins a generally conical section 1580 at a second end 1562. The cylindrical section 1570 has a relatively wide opening at the first end 1561, which tapers through the conical section 1580 to a relatively narrow opening at the second end 1562. A slit 1564 extends between the ends 1561, 1562 parallel to the holder axis 1508 distal the stem end 1502. The slit 1564 allows the insertion to and removal from the holder 1560 of either the detector cable 905 (FIG. 9) or the emitter cable 906 (FIG. 9) portion of the sensor cable 900 (FIG. 9). The wide opening at the first end 1561 is configured to accommodate a pad bend relief 610 (FIGS. 6A-B). The narrow opening at the second end 1562 is configured to accommodate the detector cable 905 (FIG. 9) or emitter cable 906 (FIG. 9).

As shown in FIG. 15C, the stem 1510 consists of a relatively stiff core 1520 surrounded by a relatively pliable outer layer 1530 so that the stem may be readily bent, yet will retain its shape. Advantageously, the stem 1510 can therefore be formed to accommodate a variety of ear shapes and sizes. The holder 1560 likewise consists of a pliable material 1540. In one embodiment, the core 1520 is a soft temper stainless steel such as #316 and the outer layer 1530 and holder material 1540 are a thermoplastic elastomer, such as AES Santoprene #281-87, which is molded over the core 1520 to form the hanger 1500.

FIGS. 16A-C illustrate a preformed shaping of an ear hanger 1500. FIG. 16A illustrates an unshaped ear hanger 1500, as described with respect to FIGS. 15A-D, above. As shown in FIG. 16B, a generally right angle bend 1610 is made in the stem 1510 proximate the second end 1502 and the holder 1560 and distal the first end 1501. As shown in FIG. 16C, a generally semi-circular bend 1620 is made in the stem 1510 proximate the first end 1501 and distal the second end 1502.

Also shown in FIG. 16C, the preformed ear hanger 1500 has a hook end 1660, a straight middle 1670 and a right angle end 1680. The hook end 1660 is configured to accommodate and comfortably fit the top and back portions of the ear. The right angle end 1680 is configured to position the wide opening at the first end 1561 (FIG. 15A) of the holder 1560 under an earlobe tissue site. The straight middle 1670 is configured to span the length of the ear sensor 300 (FIG. 1) and clip 1200 (FIG. 1) so as to accommodate the ear sensor 300 (FIG. 1) between the holder 1560 and the tissue site 10, as described above.

Although the ear hanger 1500 is described above as configured for the ear sensor 300 (FIG. 1) described herein, one of ordinary skill in the art will recognize that the ear hanger 1500 can be adapted as an attachment supplement for a variety of ear sensor configurations. In particular, the holder 1560 can be shaped, sized, oriented and/or attached along the stem 1510 or otherwise configured to accommodate various ear sensor cables, pads and clips.

FIGS. 17A-E illustrate adhesive tabs used to assist in holding the ear sensor 300 (FIG. 1) to a tissue site 10 (FIG. 1), as described above. As shown in FIG. 17A, a tab carrier 1700 is partitioned into a carrier side 1701 and a cable attachment side 1703. The carrier side 1701 holds multiple tabs 1710. The cable attachment side 1703 defines an opening 1708, which consists of a pattern of apertures and slits configured to accommodate the ear sensor 300 (FIG. 3) through the opening 1708 so that the tab carrier 1700 is slideably retained on the sensor cable 900 (FIG. 9). The carrier side 1701 and cable attachment side 1703 may be separated along a perforation 1706 so that the carrier side 1701 may be quickly and easily removed from the sensor cable 900 (FIG. 9). The remaining cable attachment side 1703 can be removed by sliding it over and off of the sensor cable 900 (FIG. 9). As shown in FIG. 17B, the tab carrier 1700 layers including individual tabs 1710 mounted between a single piece release liner 1720 and multiple piece release covers 1730. As shown in FIGS. 17C-E, an individual tab 1710 includes a double-sided adhesive layer 1712 and a non-adhesive handle 1714. Each tab 1710 is individually removed from the tab carrier 1700 by peeling the tab 1710 from the release liner 1720. Once removed, the tab 1710 can be applied to the ear sensor using the exposed adhesive side. After application, the release cover 1730 is peeled from the tab 1710 to expose the second adhesive side, which adheres to a tissue site 10 (FIG. 1).

FIGS. 18A-F illustrate another ear sensor assembly embodiment comprising an ear boot 1800. The ear boot 1800 is configured to attach an ear sensor 300 (FIG. 3) to a tissue site 10 (FIG. 1) in a manner similar to that described with respect to FIG. 1, above. The ear boot 1800, however, advantageously integrates the features of a clip 1200 (FIGS. 12A-C) and an ear hanger 1500 (FIGS. 15A-D). Specifically, the ear boot 1800 has an ear cover 1801 and a lobe cover 1803. The ear cover 1801 comprises a generally semi-tubular section 1830 defining a corresponding cavity 1840. The ear cover 1801 is configured as semi-circular bend 1810 and an extension 1820 adapted to accommodate the top and back of an ear. The lobe cover 1803 adjoins the ear cover 1801 proximate the extension 1820 and distal the bend 1810.

As shown in FIGS. 18A-F, the lobe cover 1803 has two opposing sensor holders 1860 defining an intervening lobe slot 1870, which is configured to comfortably accommodate an earlobe tissue site 10 (FIG. 1). On faces opposite the lobe slot 1870, each sensor holder 1860 defines a cavity 1880 and a corresponding aperture 1882. Each cavity 1880 is configured to accept and retain a corresponding ear sensor pad 500

(FIGS. 5A-B), either a detector pad 506 (FIGS. 5A-B) or an emitter pad 507 (FIGS. 5A-B). Each aperture 1882 is configured to generally align with each pad window 654 (FIGS. 6A-B) so that light is transmitted between the ear sensor optical components 400 (FIG. 4), 802 (FIG. 8B) through the apertures 1882 and through the tissue site 10.

Also shown in FIGS. 18A-F, each holder 1860 defines a lip 1863 disposed around the end of the cavity 1880 and a pair of catches 1864 located proximate the entrance to the cavity 1880. The ear sensor pads 500 (FIGS. 5A-B) are inserted, one each, into the cavities 1880 so that the holders 1860, and in particular, the lip 1863 and catches 1864 of each holder removably retain the sensor pads 500 (FIGS. 5A-B) on opposite sides of the lobe slot 1870. The ear cover 1801 is then fitted over the ear rim and the lobe slot 1870 is fitted over the earlobe. Alternatively, the ear boot 1800 may be attached to an ear initially and the ear sensor 300 (FIG. 3) installed in the ear boot 1800 afterwards. Although the ear sensor 300 (FIG. 1) is described above and shown in FIG. 1 as attachable to an earlobe, the ear sensor 300 (FIG. 1), ear hanger 1500 (FIGS. 15-16), adhesive tabs 1710 (FIG. 17C) and ear boot 1800 may be adapted for attachment to various other ear tissue sites such as the tragus or portions of the pinna.

FIGS. 19A-D illustrate another embodiment of an ear sensor clip 1900 comprising one or more silicone lenses. The embodiment of an ear sensor clip 1901 shown in FIG. 19 has oppositely positioned housings 1902 and 1903 that house one or more sensor optical components. Each housing 1902 and 1903 comprises an outward facing shell and an inward facing shell. Outward facing shell 1907 and inward facing shell 1906 are two mating halves of the body of housing 1903. Similarly outward facing shell 1904 and inward facing shell 1905 are two mating halves of the body of housing 1902. The two inward facing shells 1905 and 1906 face inward on either side of the patient's earlobe or other suitable tissue site when the oximetry sensor clip is attached to a patient.

In this embodiment the two housings 1903 and 1902 are hingedly connected through hinge supports 1912 and 1914. The holes 1913 and 1915 in the hinge supports 1912 and 1914 are aligned with the spring 1910. Hinge pin 1911 is inserted through the holes 1913 and 1915 and through the spring 1910 so as to rotatably attach the housings 1902 and 1903. The spring 1910 urges the housings to a closed position. The outward facing shells 1904 and 1907 may have ridges 1917 to allow a user to more easily grip the ends of housings 1902 and 1903 when opening the clip by pinching together the open ends of housings 1902 and 1903.

In an embodiment, the inward facing shells 1905 and 1906 further include windows 1919 and 1924 that provide an aperture for transmission of optical energy to or from a tissue site. Translucent silicone material covers windows 1919 and 1924 providing lenses 1920 and 1921. In an embodiment, circular rims 1922 and 1923 on the inward facing shells 1903 and 1902 define regions around windows 1919 and 1924, and lenses 1920 and 1921 formed of a translucent silicone material, substantially cover the regions defined by rims 1922 and 1923.

In an embodiment, the silicone lenses 1920 and 1921 can be formed using injection molding. In the preferred embodiment, the side of each lens that faces the tissue site when clipped onto a patient, has a slightly convex dome shape as shown in lenses 1920A and 1921A; however, the tissue facing side of a lens could alternatively be flat as shown in lenses 1920B and 1921B. Similarly, the side of each lens facing the window 1919 or 1924 can have a number of

different shapes such as concave, convex, or flat. The side of each lens facing the window **1919** or **1924** can also have a protrusion that extends into the window **1919** or **1924**. The protrusion extending into the window **1919** or **1924** can facilitate assembly of the sensor clip because it can facilitate centering and adhesion when attaching the lens to the inward facing shell **1905** or **1906**.

Although a lens in the preferred embodiment has a circular perimeter, in other embodiments, a lens can have a freeform perimeter or a perimeter of another shape such as a square, triangle, or polygon. The molded silicone lenses **1920** and **1921** can be secured to the inward facing shells **1905** and **1906** using silicone adhesive or another substance suitable for bonding silicone to the material used in constructing the inward facing shells **1905** and **1906**. Alternatively, the lenses **1920** and **1921** can be configured to fit securely within the rims **1922** or **1923** or to engage the windows **1919** and **1924** so that they can be removably attached to inward facing shells **1905** and **1906** without using adhesive.

In this embodiment, the surfaces of the sensor that have contact with the tissue site are primarily the lenses **1920** and **1921** over windows **1919** and **1924**. In an embodiment, the silicone lenses **1920** and **1921** can have a less smooth surface or a textured surface increasing the coefficient of friction between the lenses **1920** and **1921** and the tissue site. This grippy contact surface helps to prevent the sensor clip **1900** from sliding off the patient's earlobe or other suitable tissue site.

In an embodiment, the silicone material can be pliable so that it conforms somewhat to the surface of the tissue site allowing a greater portion of the surface area of the lenses **1920** and **1921** to have contact with the tissue site. In an embodiment, the lenses **1920** and **1921** can also have a larger perimeter to further increase the surface area in contact with the tissue site. The increased area of the contact surface increases the coefficient of friction between the lenses **1920** and **1921** and the tissue site. In addition, better conformity of the lens to the tissue site surface can help eliminate interference and can help to provide a more accurate reading.

Increasing the friction coefficient between contact surfaces of the oximetry sensor and the tissue site can advantageously reduce, for example, the spring tension desired to secure the sensor clip **1900** attached to the patient's earlobe or other suitable tissue site. As will be recognized from the disclosure herein, applying less pressure to the tissue site can advantageously reduce pressure necrosis, and can advantageously increase patient comfort.

In an embodiment, a thin sheet of opaque material can be placed inside either housing **1902** or **1903** between the optical components and the inward facing shell **1905** or **1906**. The thin sheet of opaque material is located beneath window **1919** or **1924**, and a window in the opaque material provides an aperture for transmission of optical energy to or from the tissue site. The opaque material blocks light, and the window in the opaque material can be sized as needed to block the proper amount of light from entering the aperture to, for example, avoid saturation of the light detector. In one embodiment, the opaque material is a thin sheet of metal.

Opening **1918** in shells **1906** and **1907** of housing **1903** provides space for the ear sensor cable **900** that electrically connects the optical components inside of housing **1903** with a sensor connector **1000**. Cable **1925** allows communication between the optical components in housings **1902** and **1903**.

A pulse oximetry ear sensor has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

Additionally, all publications, patents, and patent applications mentioned in this specification are herein incorporated by reference to the same extent as if each individual publication, patent, or patent application was specifically and individually indicated to be incorporated by reference.

What is claimed is:

1. An ear sensor for providing one or more intensity signals representative of at least one physiological parameter of pulsing blood, the ear sensor comprising:

an emitter which emits light of at least first and second wavelengths;

a light-sensitive detector which provides intensity signals resulting from detection of the at least first and second wavelengths of the light after the light is attenuated by body tissue carrying pulsing blood;

a clip housing including one or more windows through which the light or the attenuated light will pass, wherein the clip housing also houses the emitter and the detector in movable proximity to one another; and

a plurality of tissue contacting surfaces configured to be positioned between the emitter and the tissue and between the detector and the tissue when the clip housing is applied to a measurement site, wherein the tissue contacting surfaces comprise silicone lenses and wherein said silicone lenses comprise a substantially translucent textured surface that increases a coefficient of friction between the silicone lenses and a tissue site.

2. The ear sensor according to claim 1, wherein said silicone lenses are pliable thereby increasing a surface area contacting the skin.

3. The ear sensor according to claim 1, wherein at least one of said silicone lenses is sized to have a surface area greater than a surface area defined by at least one of the windows.

4. The ear sensor according to claim 1, wherein optical properties of said silicone lenses are substantially similar to optical properties of glass.

5. The ear sensor according to claim 1, wherein said silicone lenses are injection molded.

6. The ear sensor according to claim 1, wherein said silicone lenses are one of partially hemispherical and convex in shape.

7. The ear sensor according to claim 1, wherein said silicone lenses are disk shaped.

8. The ear sensor according to claim 1, wherein said silicone lenses are rectangular.

9. The ear sensor according to claim 1, wherein said clip housing comprises a disposable clip and said emitter and detector are removable from said disposable clip.

10. The ear sensor according to claim 1 further comprising an attachment supplement, wherein the attachment supplement comprises an ear hanger adapted to fit around an ear portion so as to support at least a portion of the ear sensor weight.

11. The ear sensor according to claim 1 further comprising an attachment supplement, wherein the attachment supplement comprises an ear hanger comprising:

a formable stem having a first end and having a second end;

a generally semi-circular bend proximate said first end;

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a generally right angle bend proximate said second end;  
and  
a holder attached to second end and configured to accom-  
modate a cable.

12. The ear sensor according to claim 1, wherein, in a 5  
closed position, said clip housing exerts a force on said  
tissue in the range of about 90 gram force to about 140 gram  
force.

13. The ear sensor according to claim 1, wherein, in a  
closed position, said clip housing exerts a force on a tissue 10  
site in the range of about 115 gram force to about 130 gram  
force.

14. An oximetry sensor comprising:

a plurality of opposing members each housing one of an  
emitter and a detector, and each including one or more 15  
windows covered by one or more silicone lenses,  
wherein said plurality of opposing members are con-

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figured to removably position said silicone lenses  
against the suitable tissue site and wherein said silicone  
lenses comprise a substantially translucent textured  
surface configured to aid in reducing movement of the  
sensor when the sensor is positioned against the tissue  
site.

15. The oximetry sensor of claim 14, wherein the plurality  
of opposing members is capable of removably positioning  
said silicone lenses against a patient's ear.

16. The oximetry sensor of claim 15, wherein opposing  
members further comprise a plurality of extended ridges  
adapted to assist in releasing said plurality of opposing  
members from said tissue site.

17. The ear sensor according to claim 14 further com-  
prising an attachment supplement.

\* \* \* \* \*

UNITED STATES PATENT AND TRADEMARK OFFICE  
**CERTIFICATE OF CORRECTION**

PATENT NO. : 7,341,559 B2  
APPLICATION NO. : 10/631882  
DATED : March 11, 2008  
INVENTOR(S) : Christian Schulz, Massi E. Kiani and Eugene Mason

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At Column 2, Line 61 Delete "innerjaw;" and insert -- inner jaw; --, therefor.

At Column 3, Line 3 After "tab;" delete "and"

At Column 3, Line 4 After "handle;" delete "and".

At Column 3, Line 7 Delete "boot." and insert -- boot; and --, therefor.

At Column 5, Line 34 Before "emitter" delete "a" and insert -- an --, therefor.

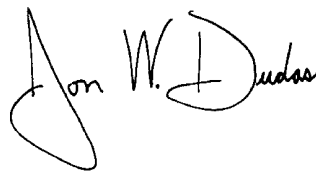
At Column 6, Line 24 Delete "1B," and insert -- 11B, --, therefor.

At Column 8, Line 12 Delete "Gycology#6200." and insert -- Cycology#6200. --, therefor.

At Column 10, Line 6 After "site" delete "10:" and insert -- 10. --, therefor.

Signed and Sealed this

Twenty-third Day of September, 2008

A handwritten signature in black ink, appearing to read "Jon W. Dudas". The signature is stylized with a large, looped initial "J" and a cursive "Dudas".

JON W. DUDAS  
*Director of the United States Patent and Trademark Office*



专利名称(译)	脉搏血氧仪耳朵传感器		
公开(公告)号	<a href="#">US7341559</a>	公开(公告)日	2008-03-11
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优先权	60/412281 2002-09-21 US 60/410499 2002-09-14 US		
其他公开文献	US20040054291A1		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

#### 摘要(译)

耳传感器组件的实施例包括发射器垫和检测器垫。夹子被配置为可移除地保持每个垫。夹子具有用于放置在耳组织部位上的打开位置和用于将垫固定到部位的相对侧的闭合位置。该组件包括适于与主机仪器电通信的传感器连接器。传感器电缆具有终止于焊盘的第一端和终止于传感器连接器的第二端，并提供焊盘和连接器之间的电通信。在一个实施例中，一个或多个硅树脂镜片或可移除的粘合剂片有助于缓解患者的不适和压力坏死。

