

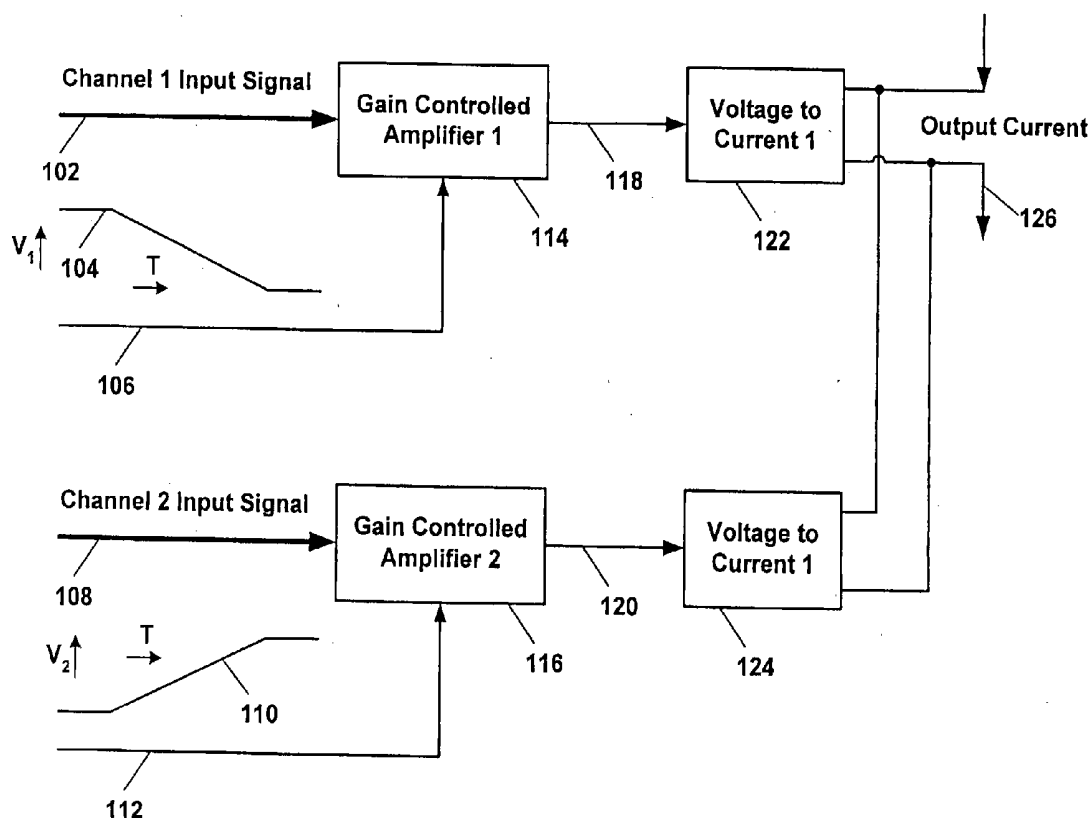


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(19) **United States**(12) **Patent Application Publication**
Boyce et al.(10) **Pub. No.: US 2008/0081970 A1**(43) **Pub. Date: Apr. 3, 2008**(54) **PULSE OXIMETRY SENSOR SWITCHOVER**(22) Filed: **Sep. 29, 2006**(75) Inventors: **Robin S. Boyce**, Pleasanton, CA
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A61B 5/00 (2006.01)(52) **U.S. Cl.** **600/323**(57) **ABSTRACT**

Switchover of a filtered and unfiltered pulse oximetry sensor is provided with gain controlled amplifiers controlled by separate gain control voltages that may change in opposite directions over a period of time. The outputs of the gain controlled amplifiers may be coupled to voltage-to-current converters whose outputs may be coupled in parallel. The parallel coupled outputs of the voltage-to-current converters may produce a current signal representative of the output of the gain controlled amplifier having the highest gain/signal.

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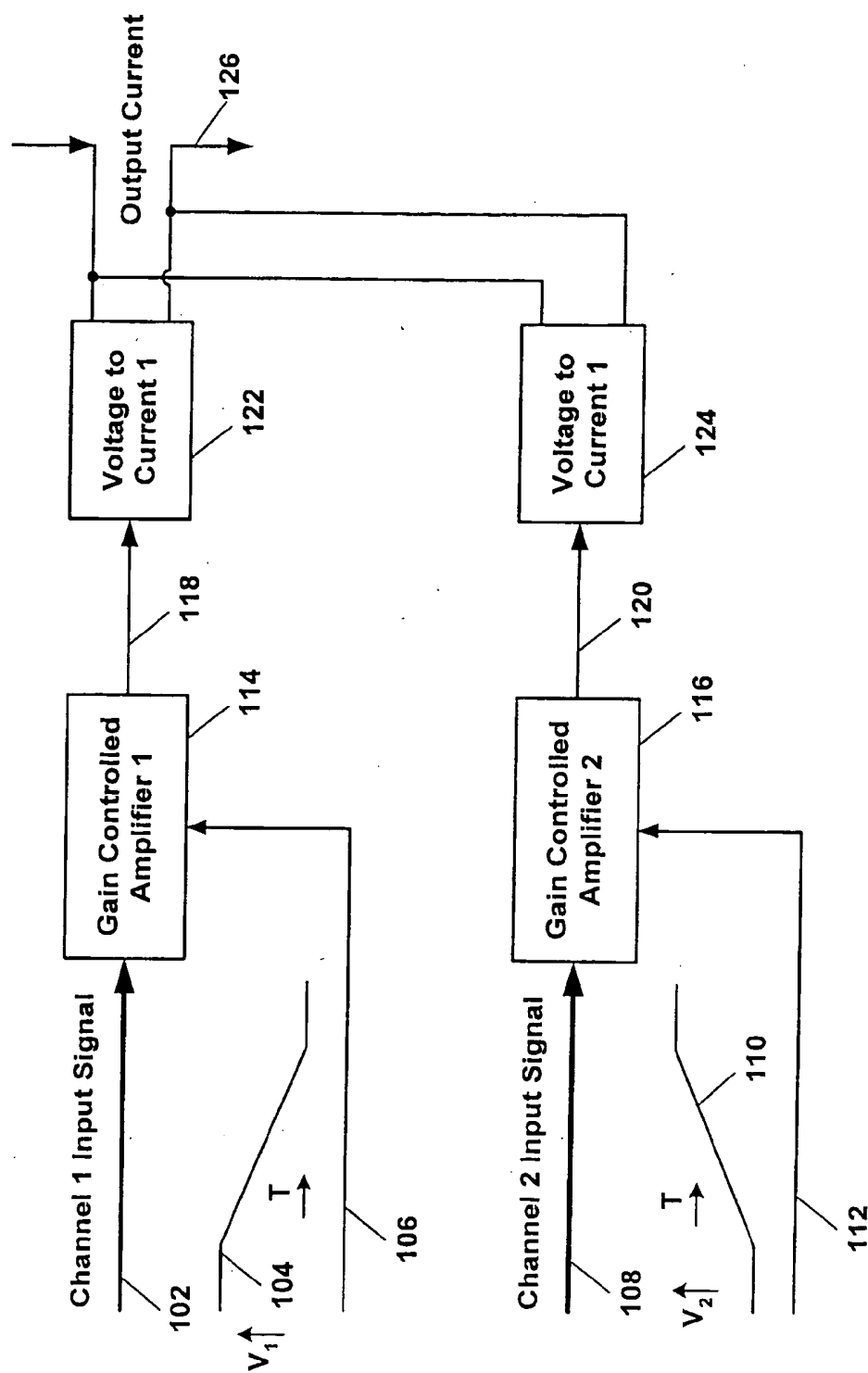


Figure 1

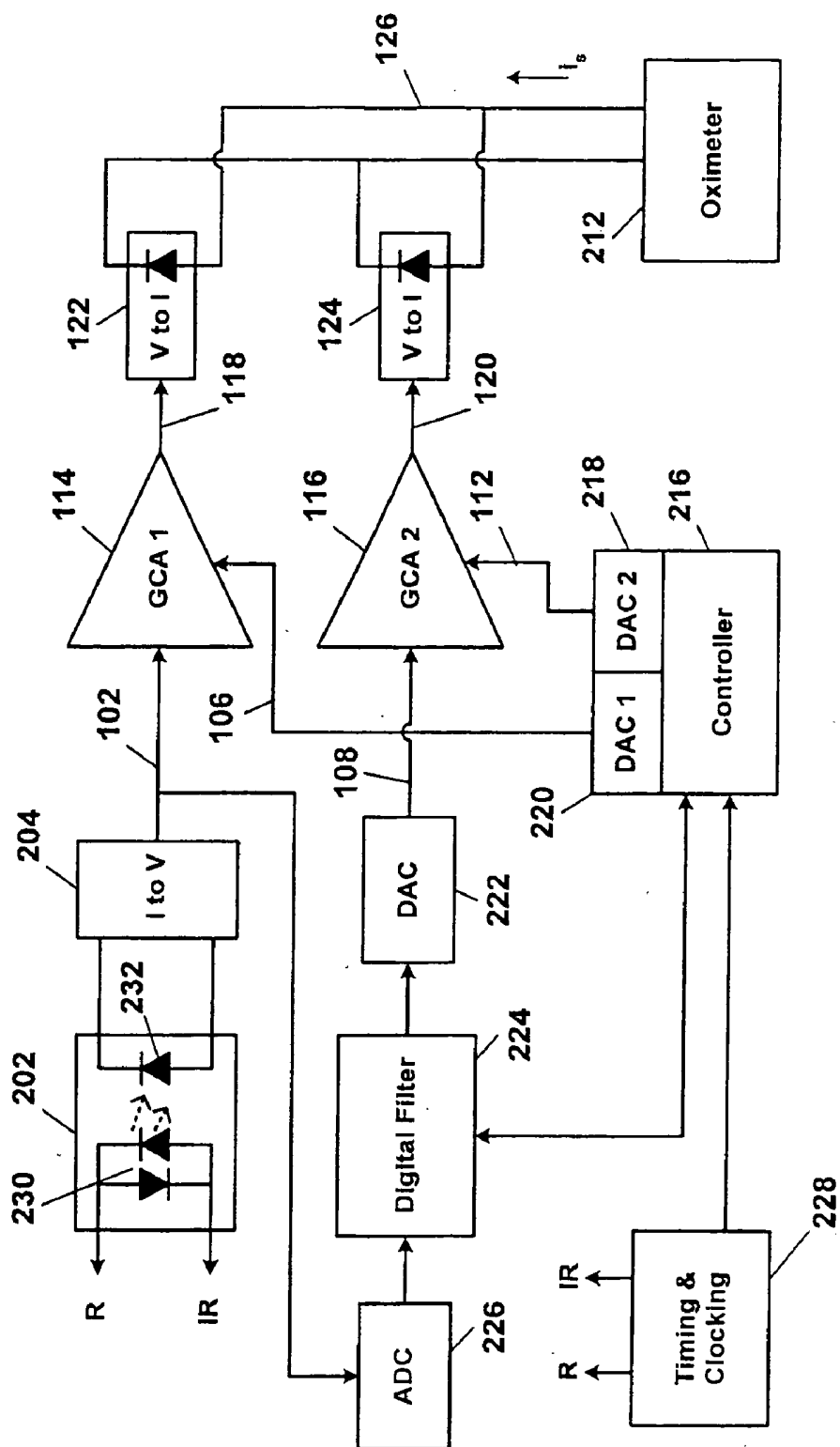


Figure 2

PULSE OXIMETRY SENSOR SWITCHOVER

TECHNICAL FIELD

[0001] The present disclosure relates generally to pulse oximetry and, more particularly to switching photodetector sensor output filtering in an oximeter.

BACKGROUND

[0002] This section is intended to introduce the reader to various aspects of art that may be related to various aspects of the present invention, which are described and/or claimed below. This discussion is believed to be helpful in providing the reader with background information to facilitate a better understanding of the various aspects of the present invention. Accordingly, it should be understood that these statements are to be read in this light, and not as admissions of prior art.

[0003] Pulse oximetry is a non-invasive method of monitoring the percentage of hemoglobin (hereinafter "Hb") that is saturated with oxygen. A pulse oximeter may include of a peripheral probe linked to a monitor that may be microprocessor controlled. The probe may be placed on a peripheral part of the body such as a digit (e.g., one finger or toe), ear lobe or nose. Within the probe, there are typically two light emitting diodes (LEDs), one in the visible red spectrum (e.g., 660 nm) and the other in the infrared spectrum (e.g., 940 nm). Using a transmission type sensor, these two beams of light pass through tissue to a photodetector. During passage through tissue, some light is absorbed by blood and soft tissue depending on the concentration of Hb. The amount of light absorption at each light wavelength depends on the degree of oxygenation of Hb within the tissue. By calculating the light absorption at the two wavelengths, the microprocessor of the monitor may compute the proportion of oxygenated Hb. A microprocessor of an oximeter may average oxygen saturation values over five to twenty seconds. The pulse rate may also be calculated from the number of LED cycles between successive pulsatile signals and averaged over a similar variable period of time, depending on the particular oximeter. A monitor may display the percentage of oxygen saturated Hb together with an audible signal for each pulse beat, a calculated heart rate, and in some monitors, a graphical display of the blood flow past the probe. User programmable audible alarms may also be provided.

[0004] From the proportions of light absorbed at each light wavelength, the microprocessor may calculate an estimation of the patient's SpO₂ level. The monitor may then display the oxygen saturation digitally as a percentage and/or audibly as a tone of varying pitch.

[0005] Reflection pulse oximetry uses reflected, rather than transmitted, light on a single-sided sensor. It can therefore be used proximally anatomically, e.g., on the forehead or bowel, although it may be difficult to secure. Other than using specific reflection spectra, the principles are generally the same as for transmission oximetry.

[0006] Oximeters may be calibrated during manufacture and may automatically check internal circuits when turned on. Oximeters may be accurate in the range of oxygen saturations of about 70% to 100% ($\pm 2\%$), but may be less accurate under 70%. The pitch of the audible pulse signal may fall in reducing values of saturation. The size of the pulse wave (related to flow) may be displayed graphically.

Some models automatically increase the gain of the display when the flow decreases, but in these models, the display may prove misleading. The alarms usually respond to a slow or fast pulse rate or an oxygen saturation below 90%. At this level, there may be a 30 marked fall in PaO₂ representing serious hypoxia.

SUMMARY

[0007] Certain aspects commensurate in scope with the originally claimed invention are set forth below. It should be understood that these aspects are presented merely to provide the reader with a brief summary of certain forms the invention might take and that these aspects are not intended to limit the scope of the invention. Indeed, the invention may encompass a variety of aspects that may not be set forth below.

[0008] According to a specific example embodiment of this disclosure, an apparatus for switchover of a pulse oximetry sensor may comprise: a pulse oximetry sensor; a first gain controlled amplifier having an input coupled to the pulse oximetry sensor; a digital filter having an analog input coupled to the pulse oximetry sensor; a second gain controlled amplifier having an input coupled to an analog output of the digital filter; a first voltage-to-current converter having a voltage input coupled to an output of the first gain controlled amplifier; a second voltage-to-current converter having a voltage input coupled to an output of the second gain controlled amplifier; the first and second voltage-to-current converters having outputs coupled together to produce a single current output; and a controller having a first gain control output coupled to the first gain controlled amplifier and a second gain control output coupled to the second gain controlled amplifier, wherein the controller may increase the gain of one of the gain controlled amplifiers over a period of time while decreasing the gain of the other gain controlled amplifier over the same period of time, so that the single current output from the first and second voltage-to-current converters represents the output of the gain controlled amplifier having the highest gain.

[0009] According to another specific example embodiment of this disclosure, a method of manufacturing a pulse oximeter may comprise providing a first gain controlled amplifier to which a pulse oximetry sensor may be coupled; coupling the pulse oximetry sensor to a digital filter; coupling the digital filter to a second gain controlled amplifier; coupling the first gain controlled amplifier to a first voltage-to-current converter; coupling the second gain controlled amplifier to a second voltage-to-current converter; and coupling the first and second voltage-to-current converter outputs together to produce a current output wherein the gain of one of the gain controlled amplifiers is adapted to increase over a period of time while the gain of the other gain controlled amplifier is adapted to decrease over the same period of time so that the current output from the first and second voltage-to-current converters represents the gain controlled amplifier having the highest gain.

[0010] According to yet another specific example embodiment of this disclosure, a pulse oximeter system having a switchover between unfiltered and filtered channels coupled to a pulse oximetry sensor may comprise: a pulse oximetry sensor; an unfiltered channel comprising a first gain controlled amplifier having an input coupled to the pulse oximetry sensor, and a first voltage-to-current converter having a voltage input coupled to an output of the first gain

controlled amplifier; a filtered channel comprising a digital filter having an analog input coupled to the pulse oximetry sensor, a second gain controlled amplifier having an input coupled to an analog output of the digital filter, and a second voltage-to-current converter having a voltage input coupled to an output of the second gain controlled amplifier; the first and second voltage-to-current converters having outputs coupled together to produce a single current output; and a controller having a first gain control output coupled to the first gain controlled amplifier and a second gain control output coupled to the second gain controlled amplifier, wherein when the unfiltered channel is selected the controller may increase the gain of the first gain controlled amplifier over a period of time while decreasing the gain of the second gain controlled amplifier over the same period of time so that the single current output from the first and second voltage-to-current converters represents an unfiltered and amplified signal from the pulse oximetry sensor; and when the filtered channel is selected the controller may increase the gain of the second gain controlled amplifier over a period of time while decreasing the gain of the first gain controlled amplifier over the same period of time so that the single current output from the first and second voltage-to-current converters represents a filtered and amplified signal from the pulse oximetry sensor.

BRIEF DESCRIPTION OF THE DRAWINGS

[0011] A more complete understanding of the present disclosure may be acquired by referring to the following description taken in conjunction with the accompanying drawings wherein:

[0012] FIG. 1 is a schematic block diagram of a switchover, two channel, gain controlled oximeter sensor amplifier having a current output, according to a specific example embodiment of the present disclosure; and

[0013] FIG. 2 is a detailed schematic block diagram of a switchover, two channel, gain controlled oximeter sensor amplifier having a current output, according to another specific example embodiment of the present disclosure.

[0014] While the present disclosure is susceptible to various modifications and alternative forms, specific example embodiments thereof have been shown in the drawings and are herein described in detail. It should be understood, however, that the description herein of specific example embodiments is not intended to limit the disclosure to the particular forms disclosed herein, but on the contrary, this disclosure is to cover all modifications and equivalents as defined by the appended claims.

DETAILED DESCRIPTION

[0015] During testing or use of oximeters, a need exists for an improved method to switch between photodetectors and/or different signal processing paths of a photodetector. Heretofore known switching between photo detectors and/or different signal processing paths of a photodetector has introduced undesirable signal transients that may set off oximeter monitor alarms and/or require longer periods of time for the transient to settle out of the normal five to twenty seconds averaging performed by a microprocessor of an oximeter monitor.

[0016] Accordingly, there is a need for improved methods, materials, and/or equipment to switch between photo detec-

tors and/or different signal processing paths of a photo detector, e.g., unfiltered and filtered channels of a pulse oximetry sensor.

[0017] Referring now to the drawings, the details of specific example embodiments are schematically illustrated. Like elements in the drawings are represented by like numbers, and similar elements are represented by like numbers with a different lower case letter suffix.

[0018] Referring to FIG. 1, depicted is a schematic block diagram of a switchover, two channel, gain controlled oximeter sensor amplifier having a current output, according to a specific example embodiment of the present disclosure. A channel 1 input signal 102 may be applied to a gain controlled amplifier 114, and a channel 2 input signal 108 may be applied to a gain controlled amplifier 116. Gains of the gain controlled amplifiers 114 and 116 may be controlled by gain control signal lines 106 and 112, respectively. The outputs 118 and 120 of the gain controlled amplifiers 114 and 116, respectively, are coupled to voltage-to-current converters 122 and 124, respectively. The current outputs of voltage-to-current converters 122 and 124 may be connected in parallel so as to generate a single switchover output current signal 126. Voltage-to-current converters 122 and 124 may be, for example, but not limited to, optical isolators each having a voltage controlled light emitting diode as an input and a photodetector as an output.

[0019] For example, at the beginning of a time period T, gain control signal line 106 has a control voltage 104 at a maximum V_1 thereby setting the gain of gain controlled amplifier 114 to a maximum. As the time period T proceeds, control voltage 104 decreases until it is at a minimum V_1 , thereby reducing the gain of gain controlled amplifier 114. In a similar, but opposite fashion, gain control signal line 112 has a control voltage 110 that starts at the beginning of the time period T at a minimum V_2 which may set the gain of gain controlled amplifier 116 to a minimum, and as the time period T proceeds, control voltage 110 increases until it is at a maximum V_2 , thereby, according to an embodiment, increasing the gain of gain controlled amplifier 116. Output current 126, according to an embodiment, represents the dominate gain controlled amplifier output signal 118 or 120, e.g., the one having the highest gain and signal input will block the other one. Thus, input signal transfer may switch from one of the input channels to the other without introducing a transient in the output current signal 126.

[0020] Referring to FIG. 2, depicted is a detailed schematic block diagram of a switchover, two channel, gain controlled oximeter sensor amplifier having a current output, according to another specific example embodiment of the present disclosure. A pulse oximetry peripheral probe 202 may comprise two light emitting diodes (LEDs), one in the visible red spectrum (e.g., 660 nm), and the other in the infrared spectrum (e.g., 940 nm). The sources of light from the two LEDs 230 pass through patient tissues to photodetector 232. Light wavelengths not absorbed by the tissues and blood supply are detected by photodetector 232. A current-to-voltage converter 204 receives the current source signal from detector 232 and produces a voltage on signal line 102 that represents the amplitudes of the detected light wavelengths. A signal line 102 is coupled to an input of the gain controlled amplifier 114 and an input of an analog-to-digital converter 226.

[0021] The output of analog-to-digital converter 226 may be coupled to a digital filter 224 that may be used to enhance

the signal information from the photo-detector **232**. A digital-to-analog converter **222** may be coupled to the output of a digital filter **224** so as to convert this output to an analog voltage that may be coupled to an input of gain controlled amplifier **116**. According to this specific example embodiment, the photodetector **232** may have an output that may be coupled directly (or indirectly) to the input of the gain controlled amplifier **114**. In addition, the output of the photodetector **232** may be coupled (e.g., indirectly) to the gain controlled amplifier **116** through the digital filter **224**. This particular embodiment is directed, in one aspect, to providing a switchover between signal line **102** having the unprocessed information from the photodetector **232** and the signal line **108** having the digitally filtered (enhanced) information from the photodetector **232**.

[0022] The controller **216**, e.g., a digital processor, a microprocessor, a microcontroller, a digital signal processor (DSP), an application specific integrated circuit (ASIC) and/or programmable logic array (PLA), in combination with digital-to-analog converters **218** and **220** may be used for controlling gains of the gain controlled amplifiers **114** and **116**. When a selection change, e.g., nurse or doctor initiated, is made between the unfiltered and filtered signal information from the photodetector **232**, the gain control signal line **106** may have a control signal from the digital-to-analog converter **220** that is at a maximum voltage at the beginning of a time period T, thereby, according to this embodiment, setting the gain of the gain controlled amplifier **114** to a maximum. As the time period T proceeds, the control signal on the gain control signal line **106** decreases until it is at a minimum, thereby, according to this embodiment, reducing the gain of gain controlled amplifier **114**. In a similar, but opposite fashion, the gain control signal line **112** may have a control signal that starts at the beginning of the time period T at a minimum voltage thereby, according to this embodiment, setting the gain of the gain controlled amplifier **116** to a minimum, and as the time period T proceeds, the control signal on the gain control signal line **112** increases until it is at a maximum voltage, thereby, according to this embodiment, increasing the gain of the gain controlled amplifier **116**.

[0023] Since the outputs of the voltage-to-current converters **122** and **124** may be in parallel, the output current **126** may represent the dominant gain controlled amplifier output signal **118** or **120**, e.g., the one having the highest gain and signal input will block the other one. Thus, according to this embodiment, input signals **102** and **108** may be switched without introducing a transient in the output current signal **126**. The output current signal **126** may be used to supply sensor information to an oximeter **212**, e.g., oximeter display monitor. The timing and clocking circuit **228** may be used for clock signals and timing signals for the light emitting diodes **230** and the controller **216**.

[0024] While embodiments of this disclosure have been depicted, described, and are defined by reference to example embodiments of the disclosure, such references do not imply a limitation on the disclosure, and no such limitation is to be inferred. The subject matter disclosed is capable of considerable modification, alteration, and equivalents in form and function, as will occur to those ordinarily skilled in the pertinent art and having the benefit of this disclosure. The depicted and described embodiments of this disclosure are examples only, and are not exhaustive of the scope of the disclosure.

What is claimed is:

1. A pulse oximetry switching system, the system comprising:
 - a pulse oximetry sensor;
 - a first gain controlled amplifier having an input coupled to the pulse oximetry sensor;
 - a digital filter having an analog input coupled to the pulse oximetry sensor;
 - a second gain controlled amplifier having an input coupled to an analog output of the digital filter;
 - a first voltage-to-current converter having a voltage input coupled to an output of the first gain controlled amplifier;
 - a second voltage-to-current converter having a voltage input coupled to an output of the second gain controlled amplifier, wherein the first and second voltage-to-current converters have outputs coupled together to produce a single current output; and
 - a controller having a first gain control output coupled to the first gain controlled amplifier and a second gain control output coupled to the second gain controlled amplifier, the controller adapted to control a gain increase of one of the gain controlled amplifiers over a period of time and a gain decrease of the other gain controlled amplifier over the same period of time, wherein the single current output from the first and second voltage-to-current converters represents the output of the gain controlled amplifier having the highest gain.
2. The apparatus according to claim 1, wherein a current output from the first and second voltage-to-current converters is coupled to an oximeter.
3. The apparatus according to claim 2, wherein the oximeter indicates percent oxygen saturation of blood.
4. The apparatus according to claim 2, wherein the oximeter indicates pulse rate.
5. The apparatus according to claim 3, wherein the pulse oximetry sensor is adapted to attach to a portion of a patient having blood flow therein and wherein the pulse oximetry sensor monitors oxygen saturation of the blood.
6. The apparatus according to claim 1, wherein the pulse oximetry sensor is coupled to the input of the first gain controlled amplifier and the input of the digital filter with a current-to-voltage converter.
7. The apparatus according to claim 1, wherein the pulse oximetry sensor is coupled to the digital filter with an analog-to-digital converter.
8. The apparatus according to claim 1, wherein the analog output of the digital filter is produced with a digital-to-analog converter.
9. The apparatus according to claim 1, wherein the controller comprises at least one of a digital processor, a microprocessor, a microcontroller, a digital signal processor, an application specific integrated circuit, or a programmable logic array, or any combination thereof.
10. The apparatus according to claim 9, wherein the first and second gain control outputs of the microprocessor are produced with first and second digital-to-analog converters, respectively.
11. The apparatus according to claim 1, wherein the current outputs of the first and second voltage-to-current converters are connected in parallel.

12. The apparatus according to claim 1, wherein the controller selects an operational channel for the pulse oximetry sensor by increasing the gain of the gain controlled amplifier associated with that operational channel.

13. A method of manufacturing a pulse oximeter, the method comprising:

- providing a first gain controlled amplifier to which a pulse oximetry sensor may be coupled;
- coupling the pulse oximetry sensor to a digital filter;
- coupling the digital filter to a second gain controlled amplifier;
- coupling the first gain controlled amplifier to a first voltage-to-current converter;
- coupling the second gain controlled amplifier to a second voltage-to-current converter; and
- coupling the first and second voltage-to-current converter outputs together to produce a current output, wherein the gain of one of the gain controlled amplifiers is adapted to increase over a period of time while the gain of the other gain controlled amplifier is adapted to decrease over the same period of time, wherein the current output from the first and second voltage-to-current converters represents the gain controlled amplifier having the highest gain.

14. The method according to claim 13, comprising coupling the current output of the first and second voltage-to-current converters to an oximeter.

15. The method according to claim 14, wherein the oximeter indicates percent oxygen saturation of blood.

16. The method according to claim 14, wherein the oximeter indicates pulse rate.

17. The method according to claim 13, wherein coupling the pulse oximetry sensor to the first gain controlled amplifier and the digital filter is via a current-to-voltage converter.

18. The method according to claim 13, wherein the pulse oximetry sensor is coupled to the digital filter with an analog-to-digital converter.

19. The method according to claim 13, wherein the controller comprises at least one of a digital processor, a microprocessor, a microcontroller, a digital signal processor, an application specific integrated circuit, or a programmable logic array, or any combination thereof.

20. A pulse oximeter channel switching system, the system comprising:

- a pulse oximetry sensor;
- an unfiltered channel comprising
 - a first gain controlled amplifier having an input coupled to the pulse oximetry sensor, and
 - a first voltage-to-current converter having a voltage input coupled to an output of the first gain controlled amplifier;
- a filtered channel comprising
 - a digital filter having an analog input coupled to the pulse oximetry sensor,
 - a second gain controlled amplifier having an input coupled to an analog output of the digital filter, and
 - a second voltage-to-current converter having a voltage input coupled to an output of the second gain controlled amplifier;
- the first and second voltage-to-current converters having outputs coupled together to produce a single current output; and
- a controller having a first gain control output coupled to the first gain controlled amplifier and a second gain control output coupled to the second gain controlled amplifier,

wherein the system is configured so that (i) upon selection of the unfiltered channel, the controller increases the gain of the first gain controlled amplifier over a period of time and decreases the gain of the second gain controlled amplifier over the same period of time so that the single current output from the first and second voltage-to-current converters represents an unfiltered and amplified signal from the pulse oximetry sensor; and

(ii) upon selection of the filtered channel, the controller increases the gain of the second gain controlled amplifier over a period of time and decreases the gain of the first gain controlled amplifier over the same period of time so that the single current output from the first and second voltage-to-current converters represents a filtered and amplified signal from the pulse oximetry sensor.

21. The system according to claim 20, wherein the controller comprises at least one of a digital processor, a microprocessor, a microcontroller, a digital signal processor, an application specific integrated circuit, or a programmable logic array, or any combination thereof.

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专利名称(译)	脉搏血氧饱和度传感器切换		
公开(公告)号	US20080081970A1	公开(公告)日	2008-04-03
申请号	US11/540248	申请日	2006-09-29
[标]申请(专利权)人(译)	内尔科尔普里坦贝内特公司		
申请(专利权)人(译)	NELLCOR PURITAN BENNETT INCORPORATED		
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IPC分类号	A61B5/00		
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其他公开文献	US8068890		
外部链接	Espacenet USPTO		

摘要(译)

滤波和未滤波的脉搏血氧饱和度传感器的切换提供有增益控制放大器，其由单独的增益控制电压控制，这些增益控制电压可以在一段时间内沿相反方向改变。增益控制放大器的输出可以耦合到电压 - 电流转换器，其输出可以并联耦合。电压 - 电流转换器的并联耦合输出可以产生表示具有最高增益/信号的增益控制放大器的输出的电流信号。

