



US 20080039701A1

(19) **United States**(12) **Patent Application Publication****Ali et al.**(10) **Pub. No.: US 2008/0039701 A1**(43) **Pub. Date: Feb. 14, 2008**(54) **DUAL-MODE PULSE OXIMETER****Related U.S. Application Data**

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(63) Continuation of application No. 10/911,391, filed on Aug. 3, 2004, which is a continuation of application No. 09/641,542, filed on Aug. 18, 2000, now Pat. No. 6,770,028, which is a continuation-in-part of application No. 09/491,175, filed on Jan. 25, 2000, now abandoned.

(60) Provisional application No. 60/117,097, filed on Jan. 25, 1999. Provisional application No. 60/161,565, filed on Oct. 26, 1999.

Publication Classification

(51) **Int. Cl.**
A61B 5/02 (2006.01)

(52) **U.S. Cl.** **600/301; 600/324**

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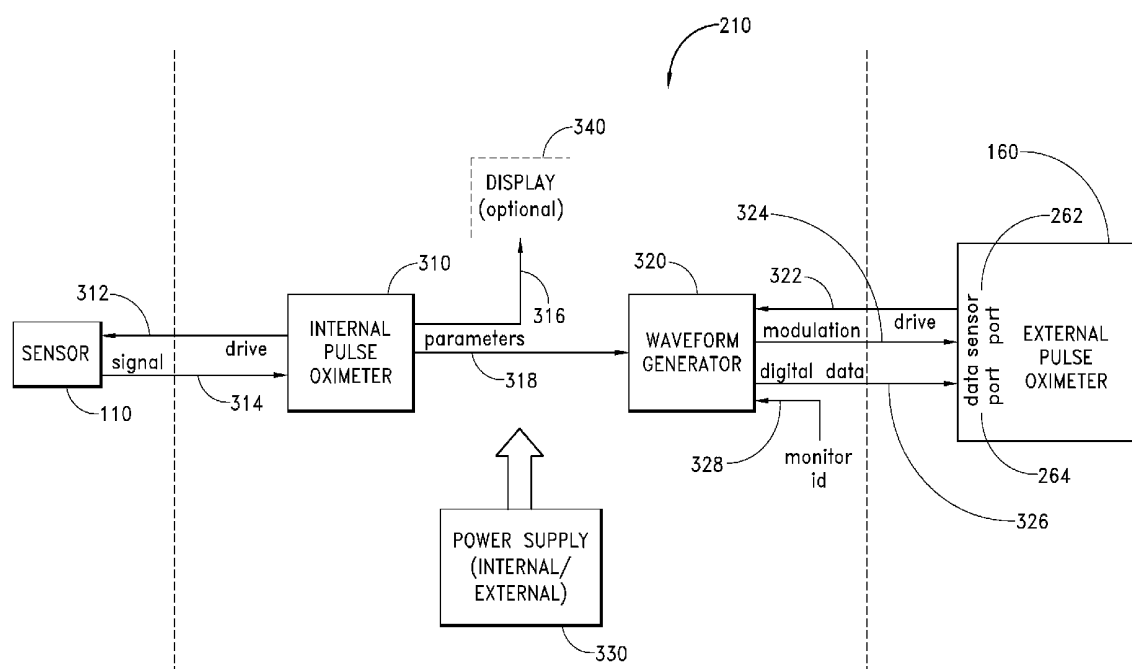
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(21) Appl. No.: **11/894,722**

(22) Filed: **Aug. 20, 2007**

(57) **ABSTRACT**

A portable stand alone patient monitor is dockable with a docking station attached to a patient bed. The portable monitor is configured to operate in a stand alone mode and a docked mode. The docking station can include a second local monitor.



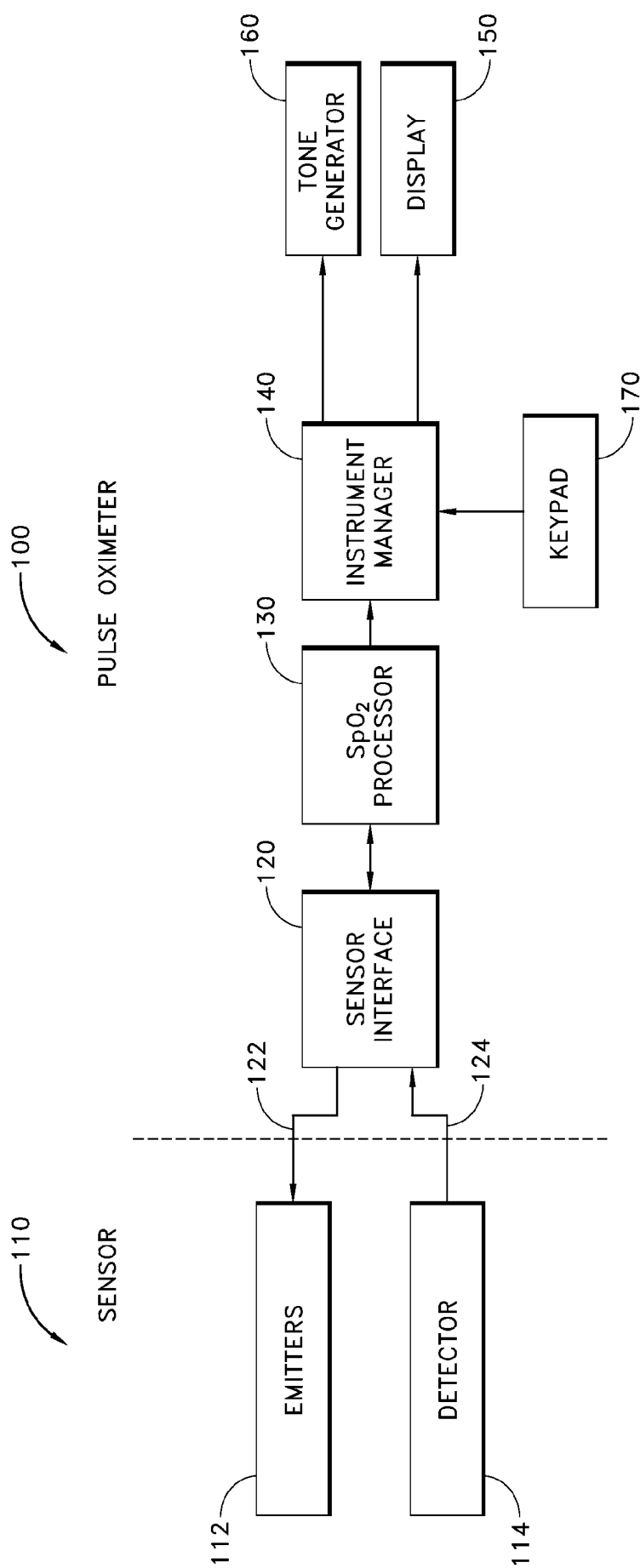


FIG. 1
(PRIOR ART)

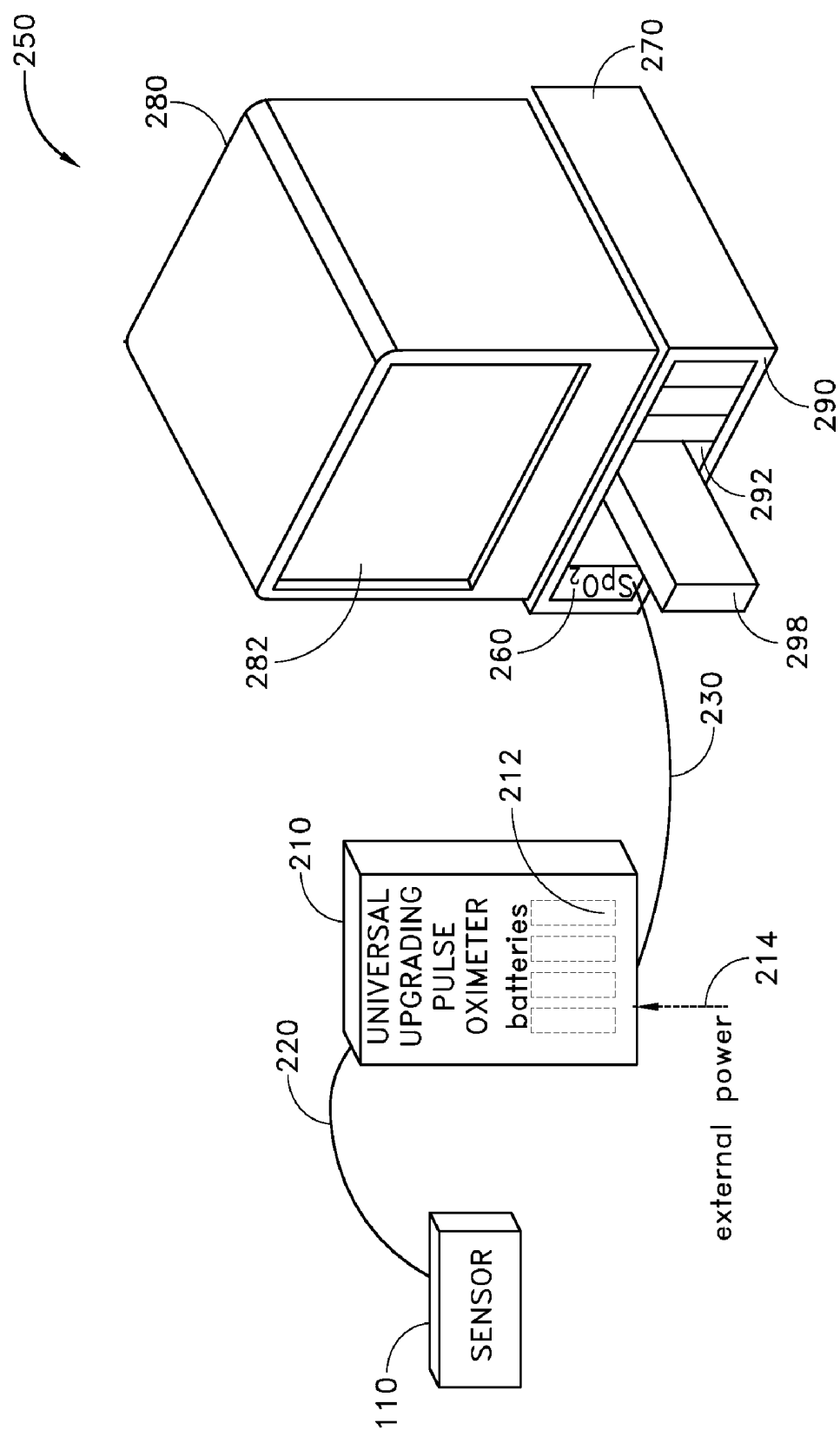


FIG. 2

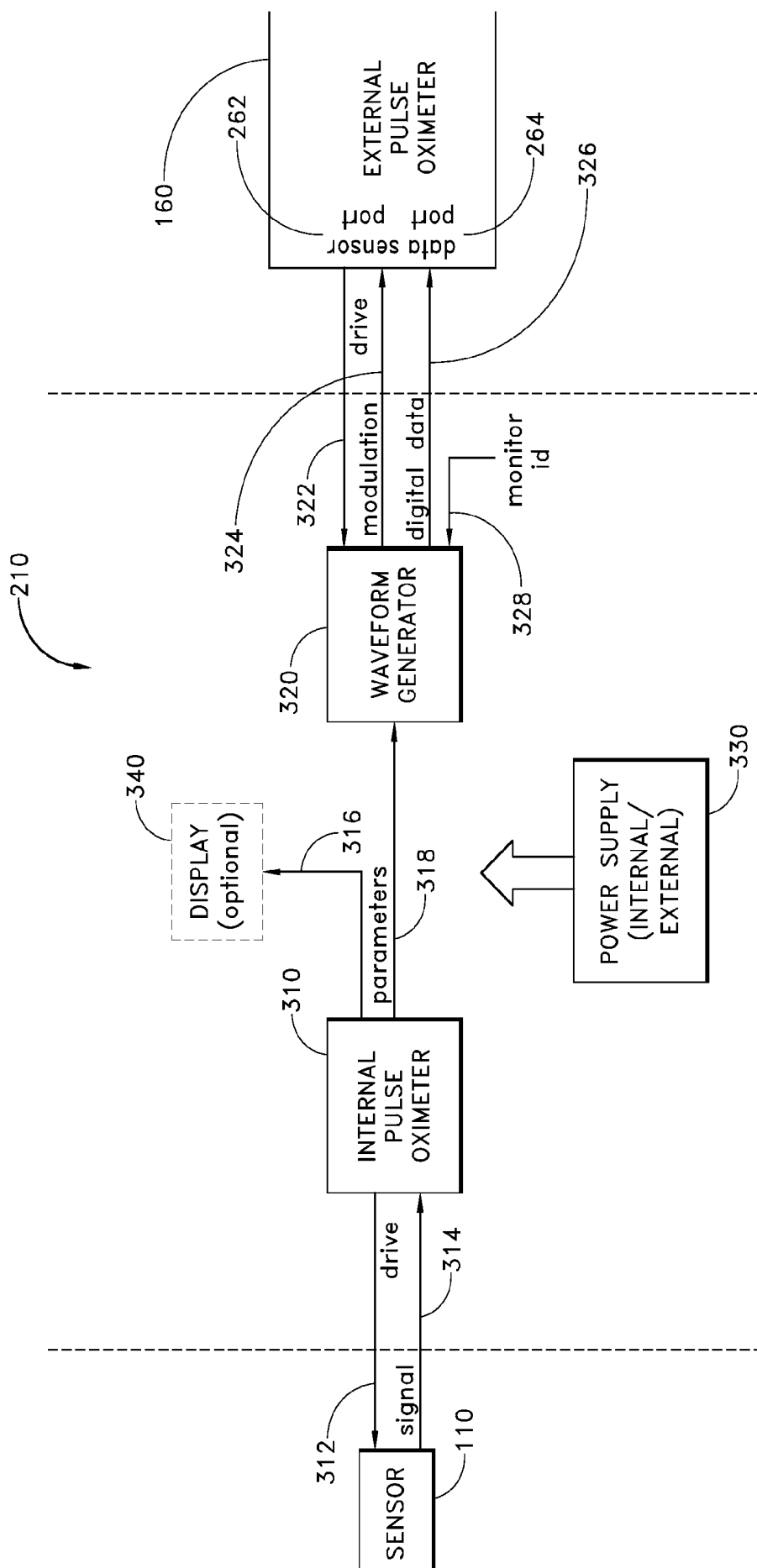
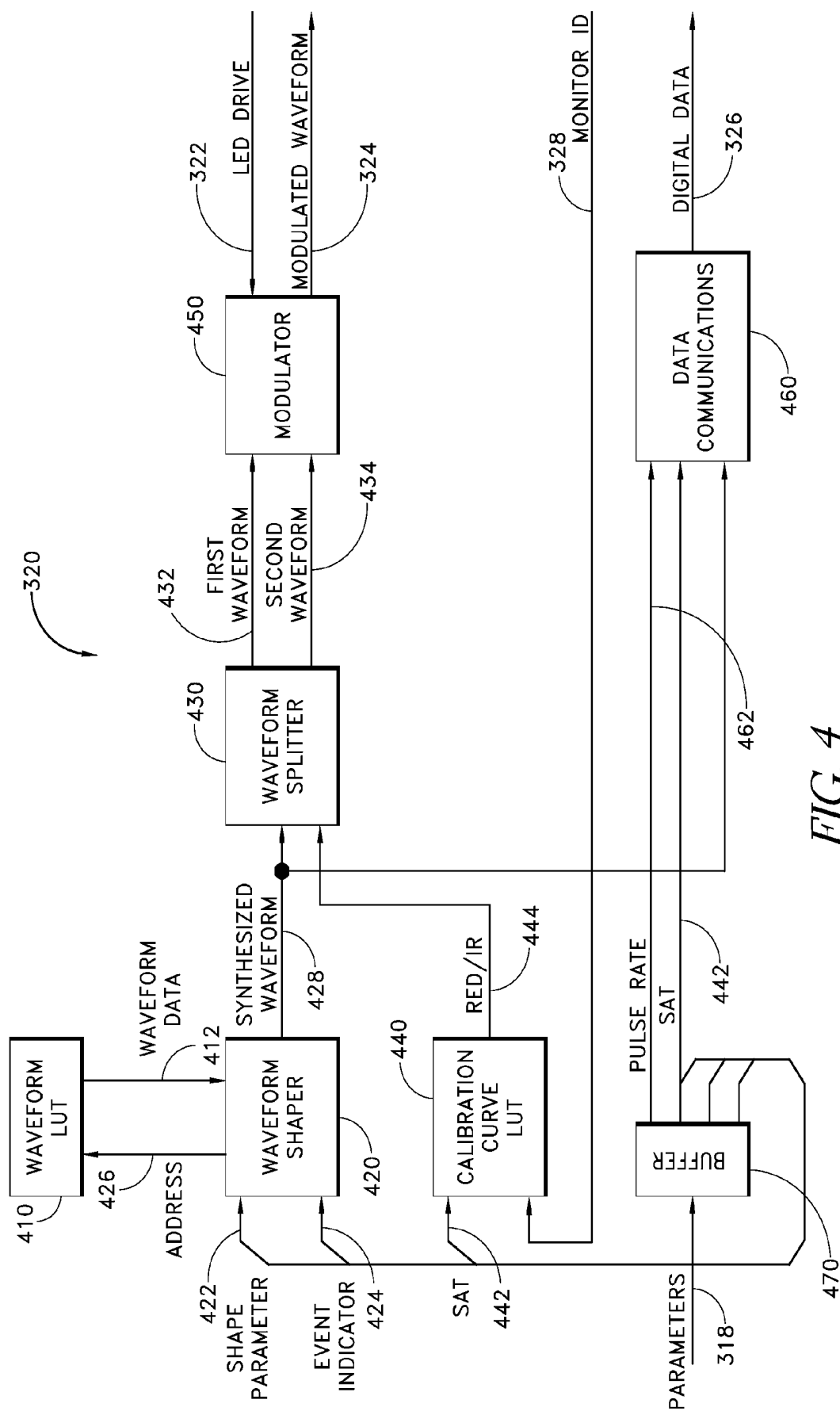


FIG. 3



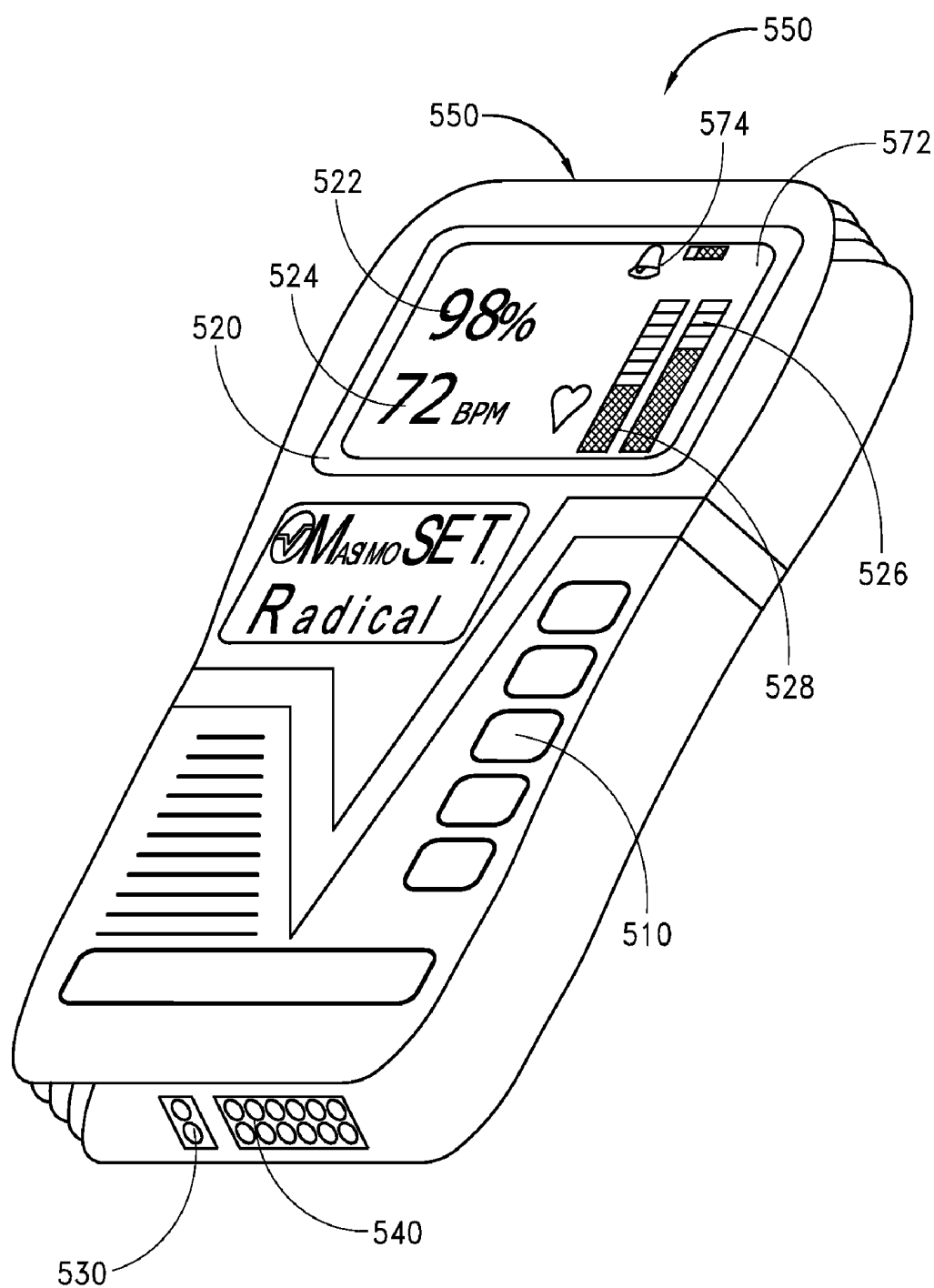


FIG. 5

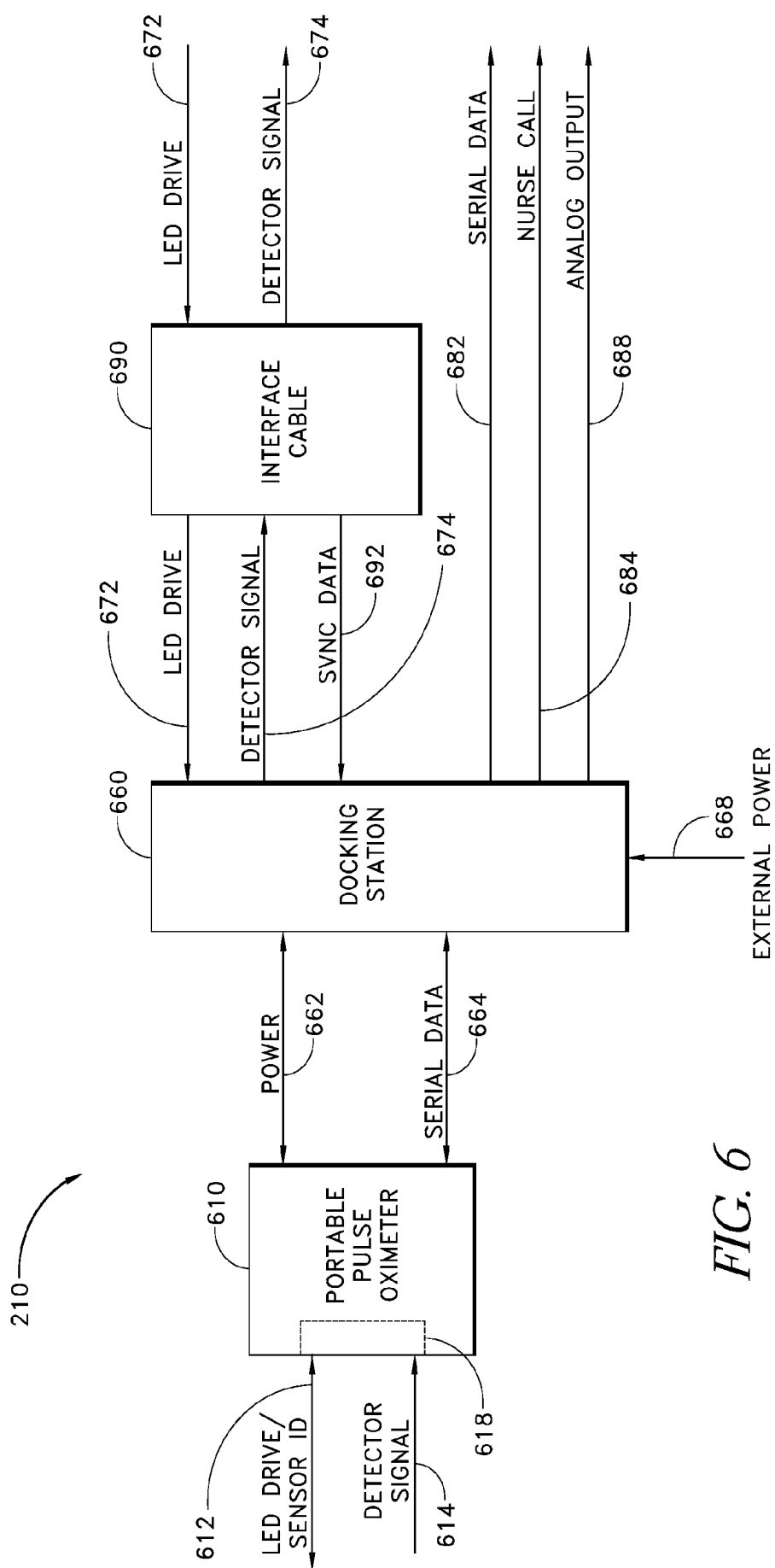
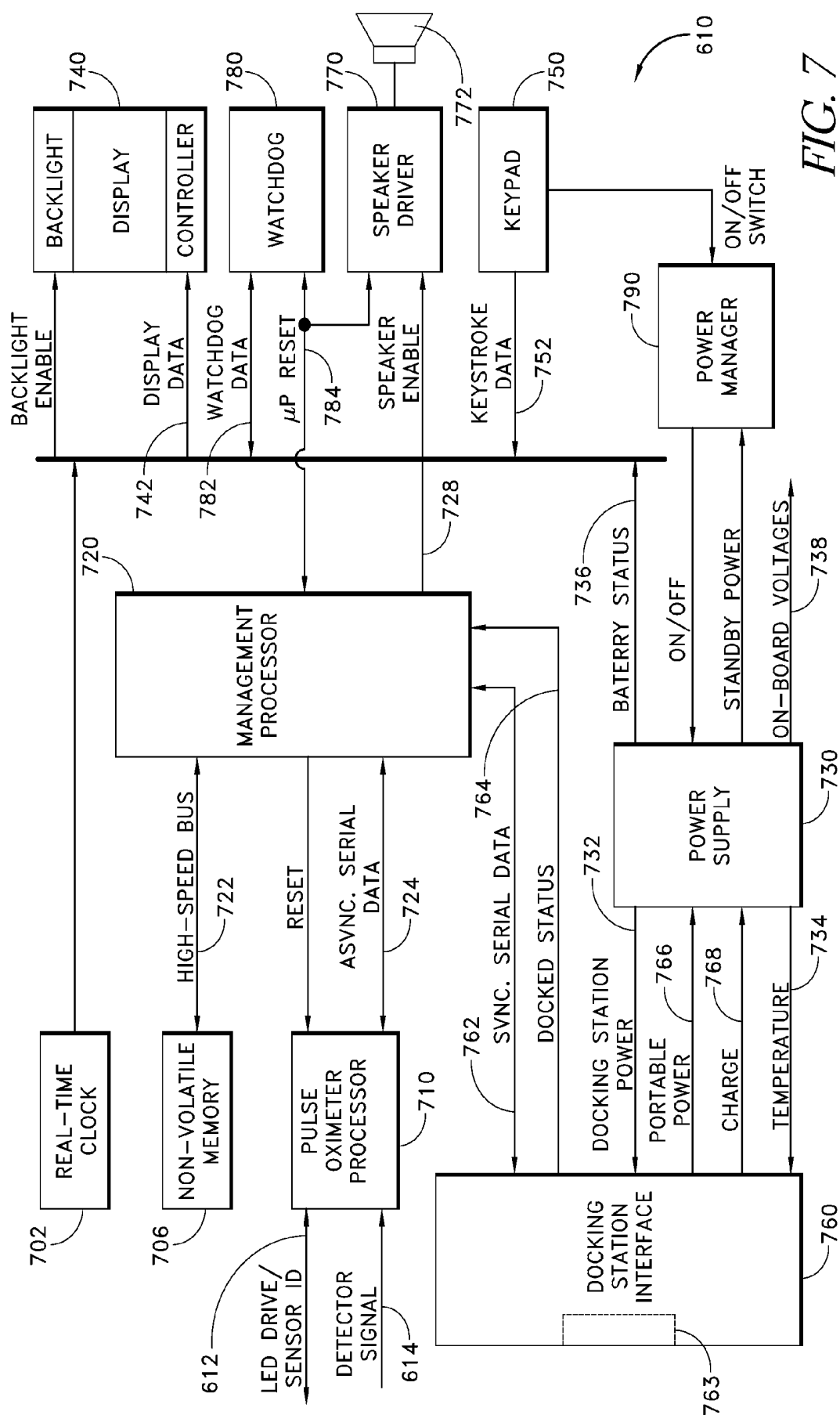


FIG. 6



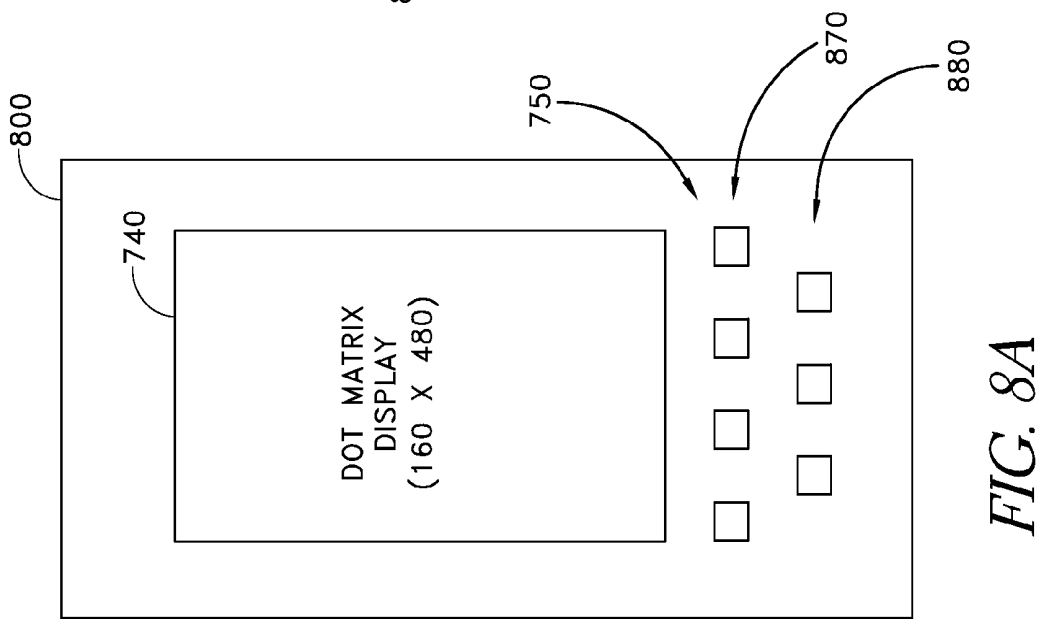


FIG. 8A

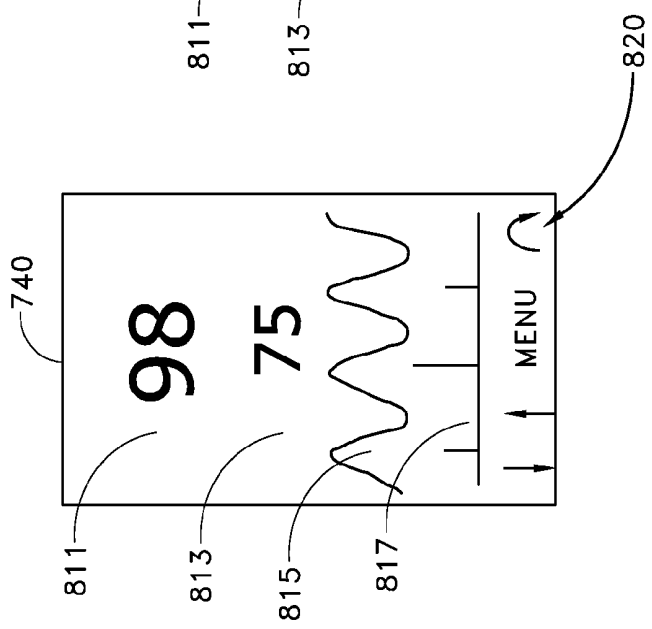


FIG. 8B

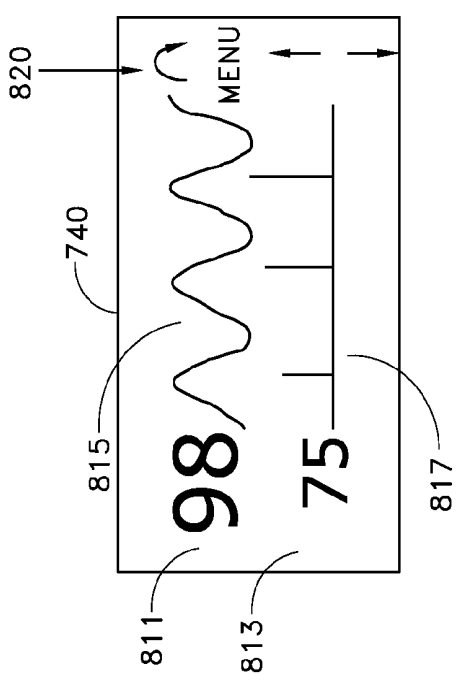


FIG. 8C

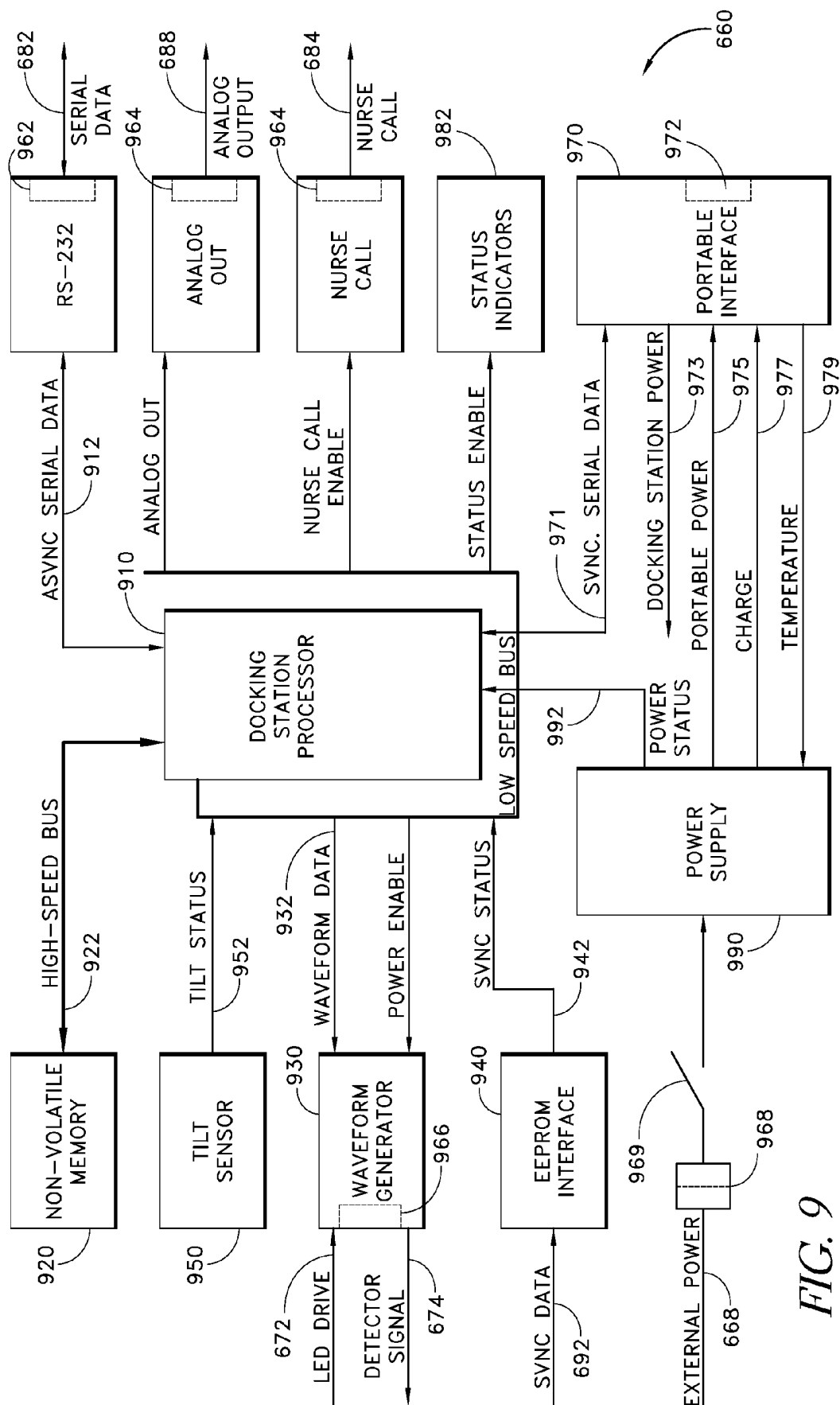


FIG. 9

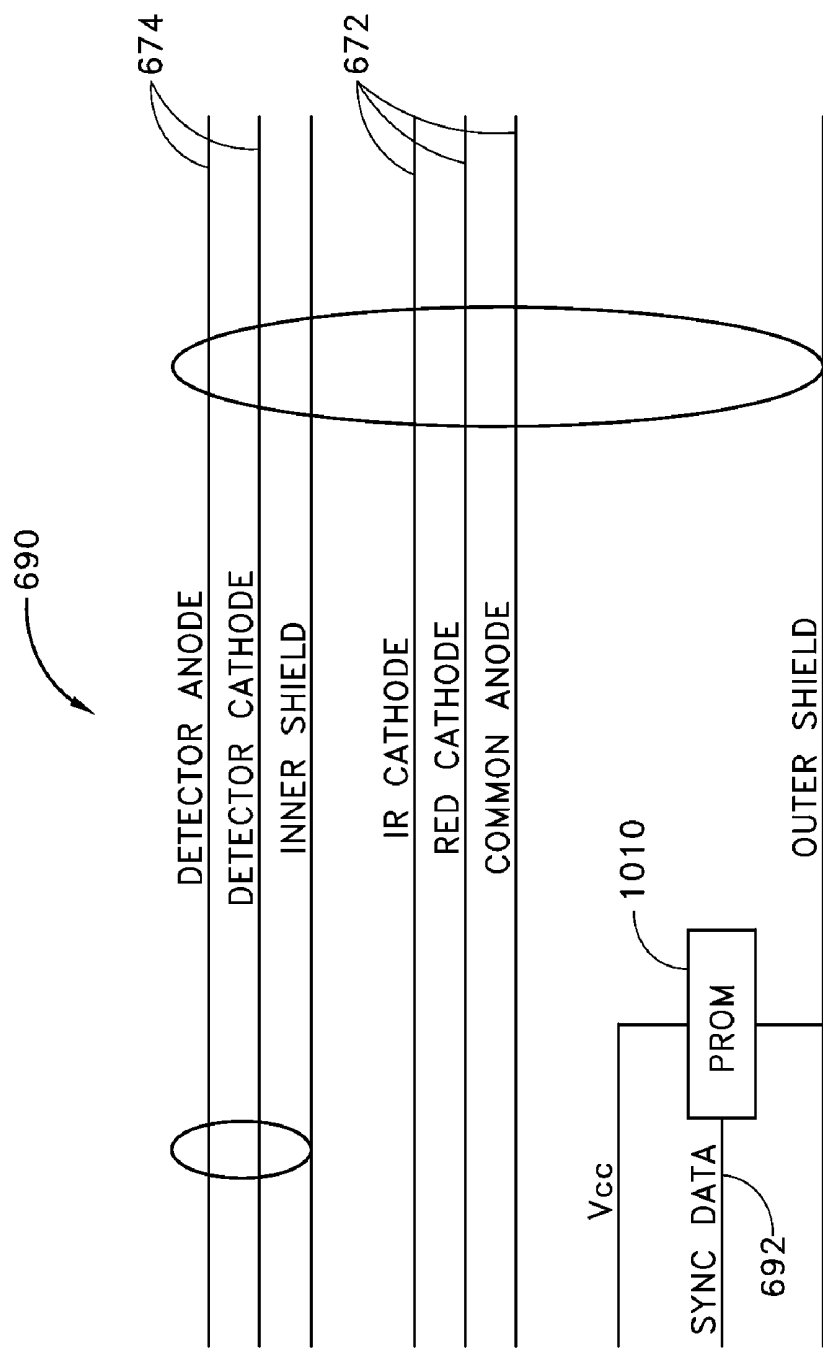


FIG. 10

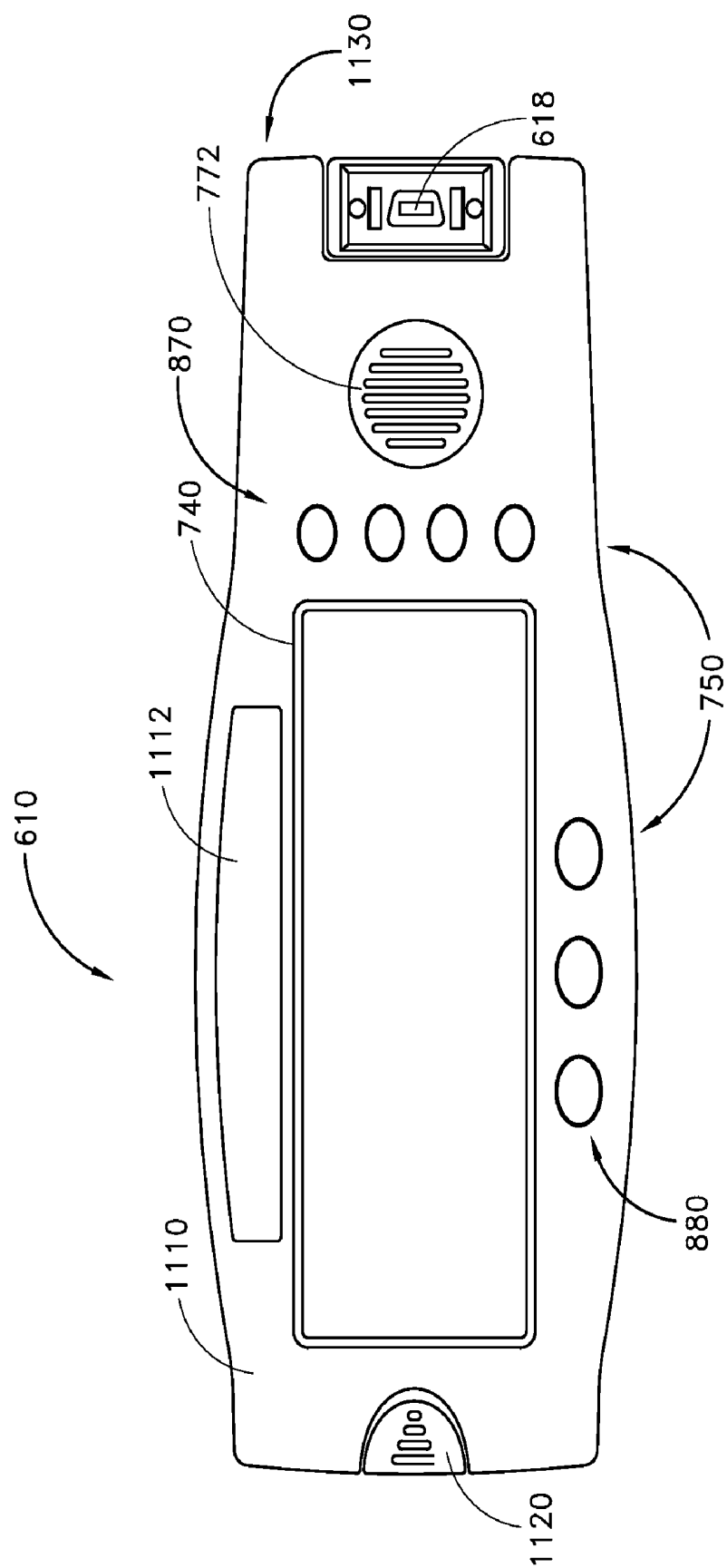


FIG. 11A

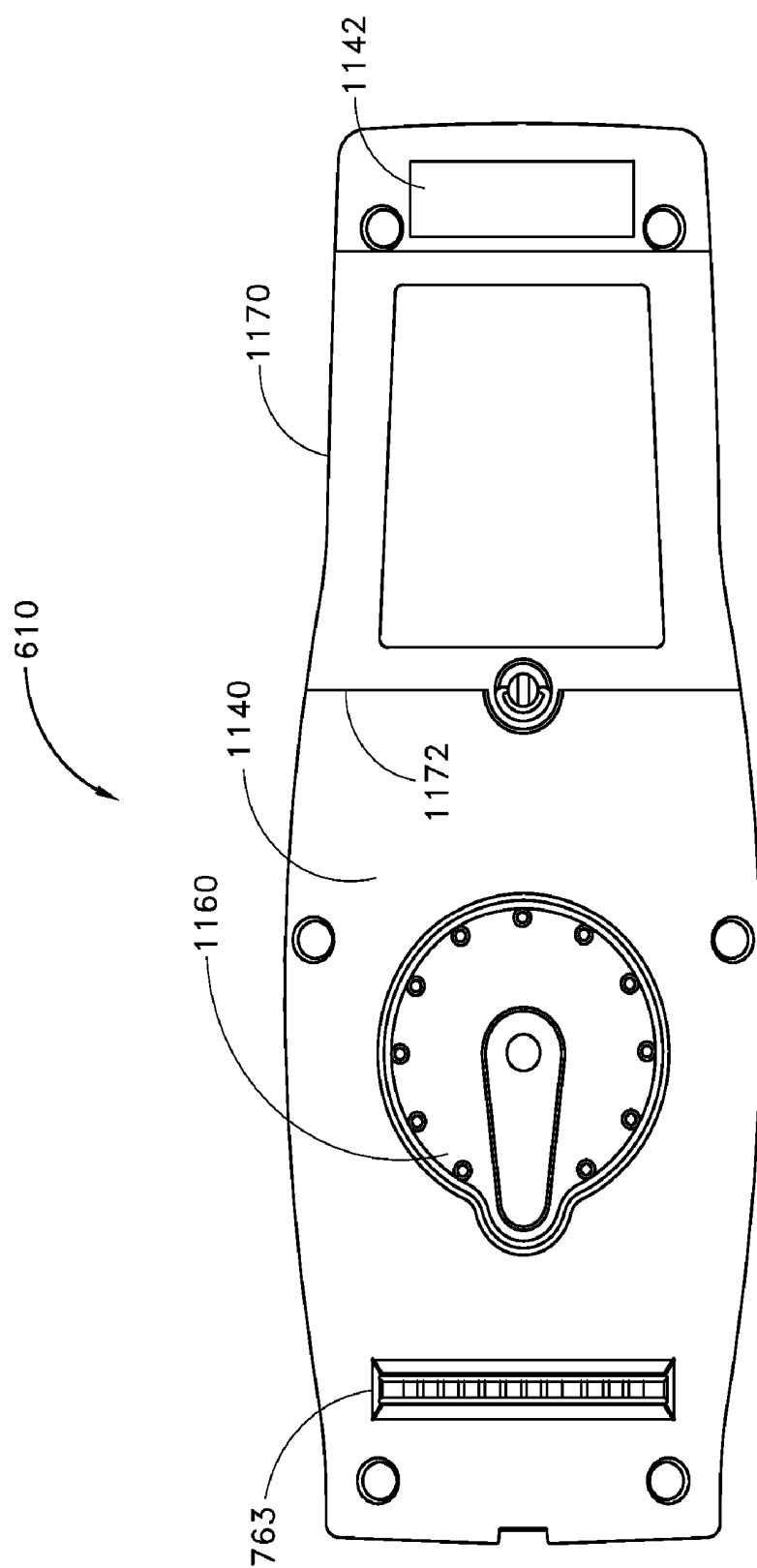


FIG. 11B

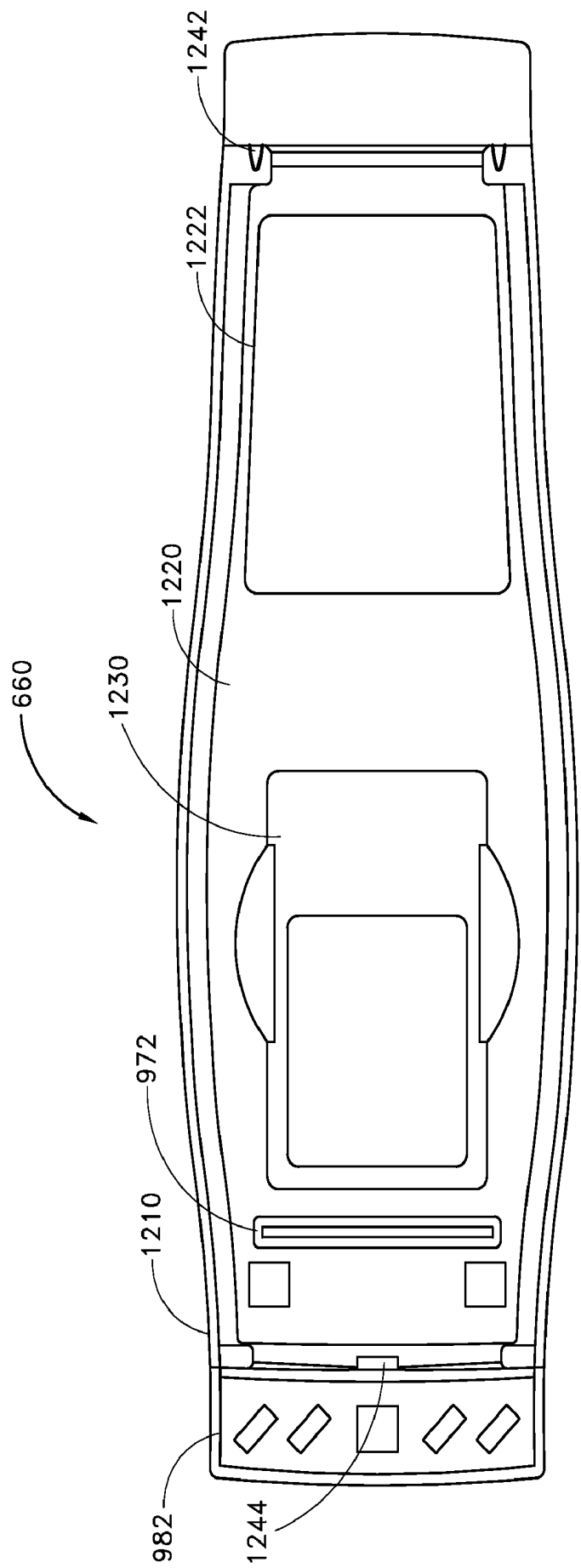


FIG. 12A

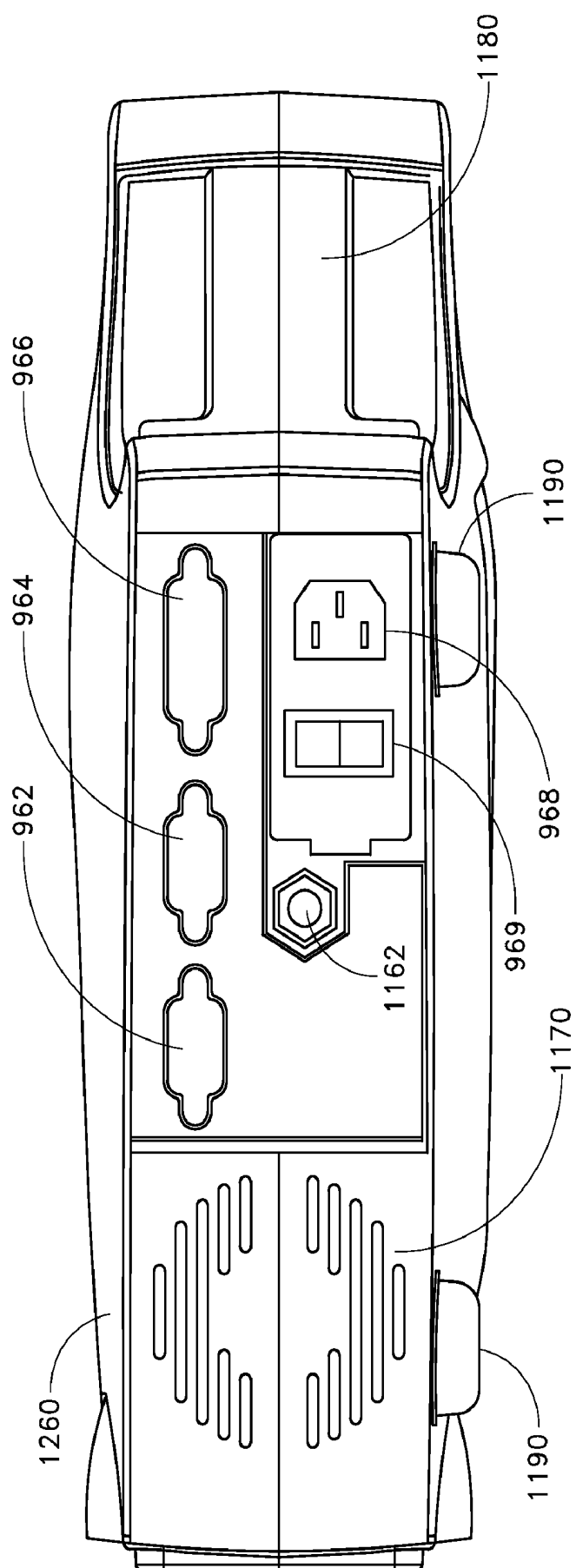


FIG. 12B

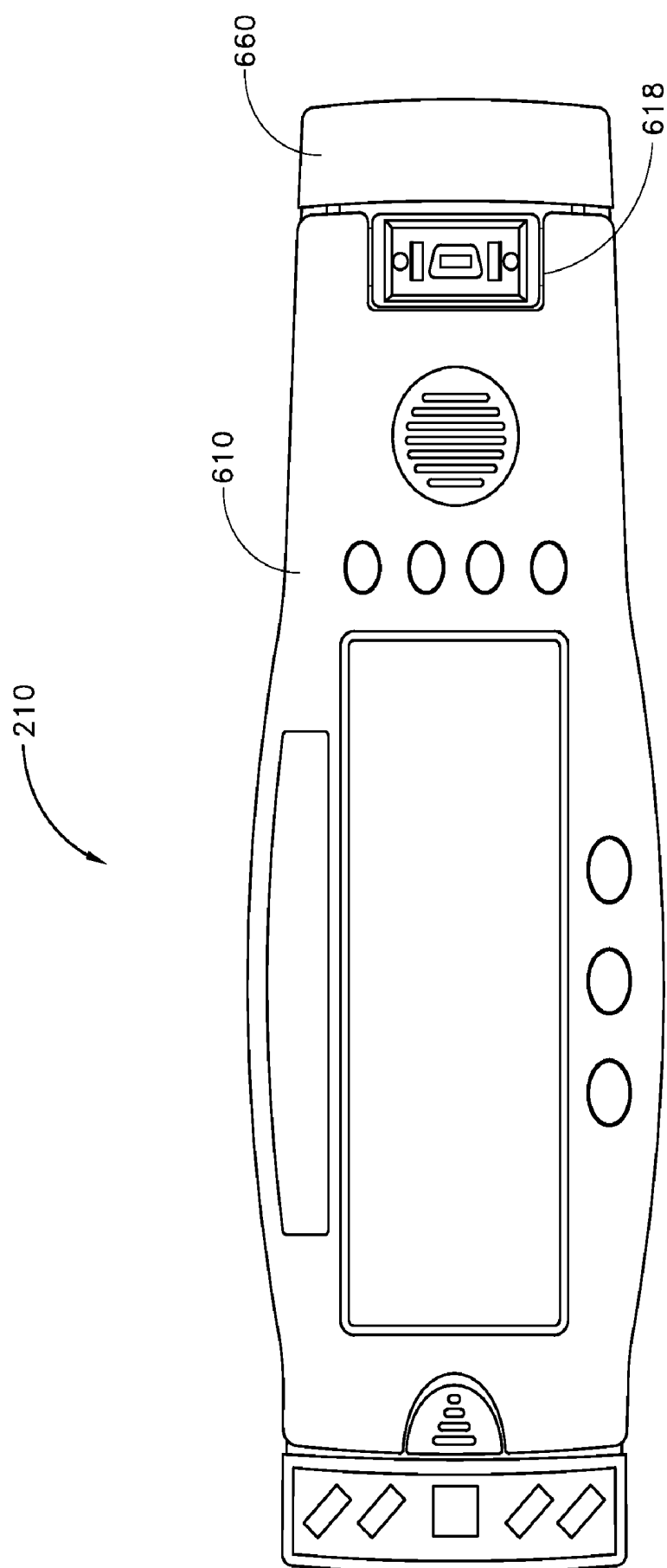


FIG. 13

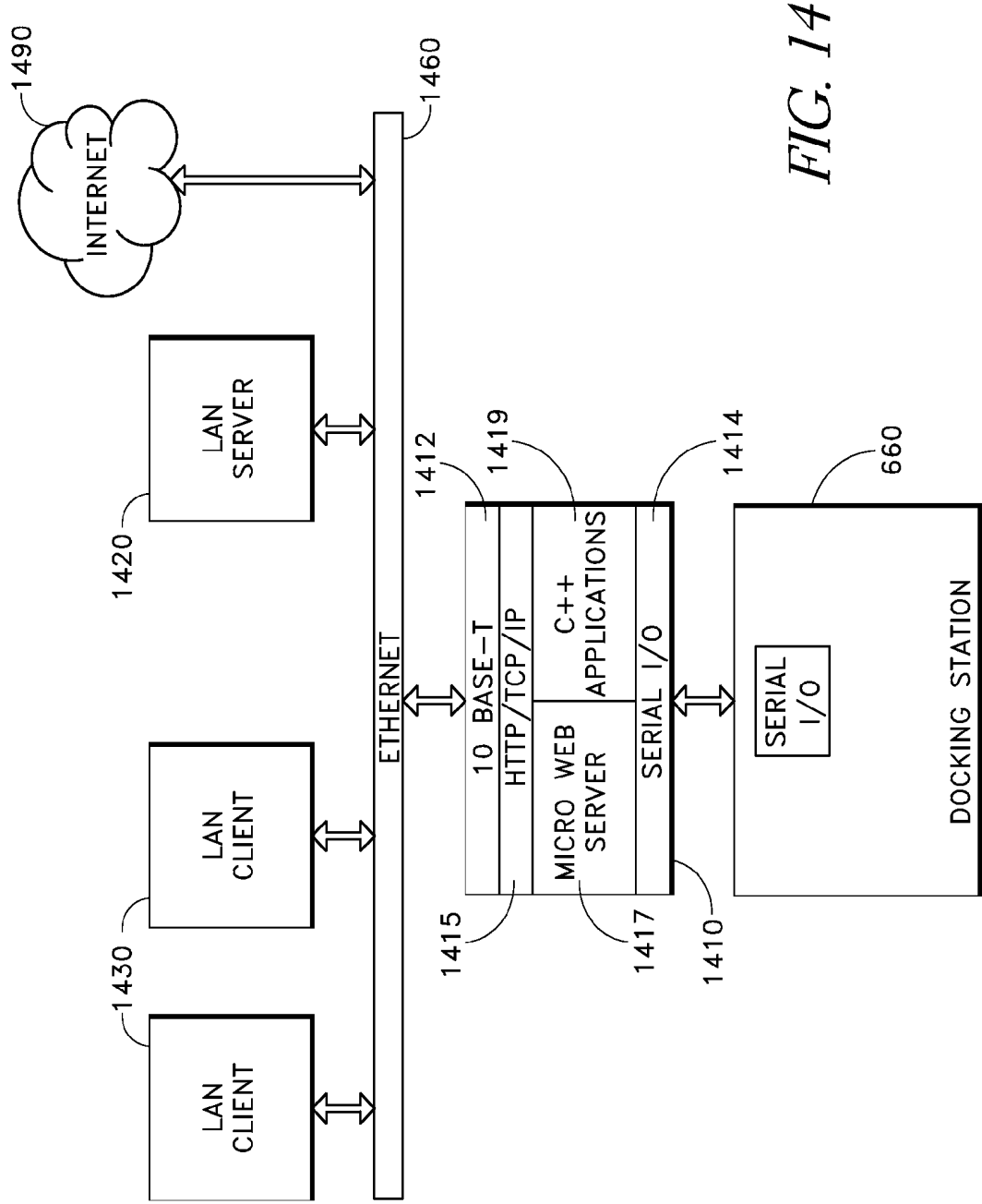


FIG. 14

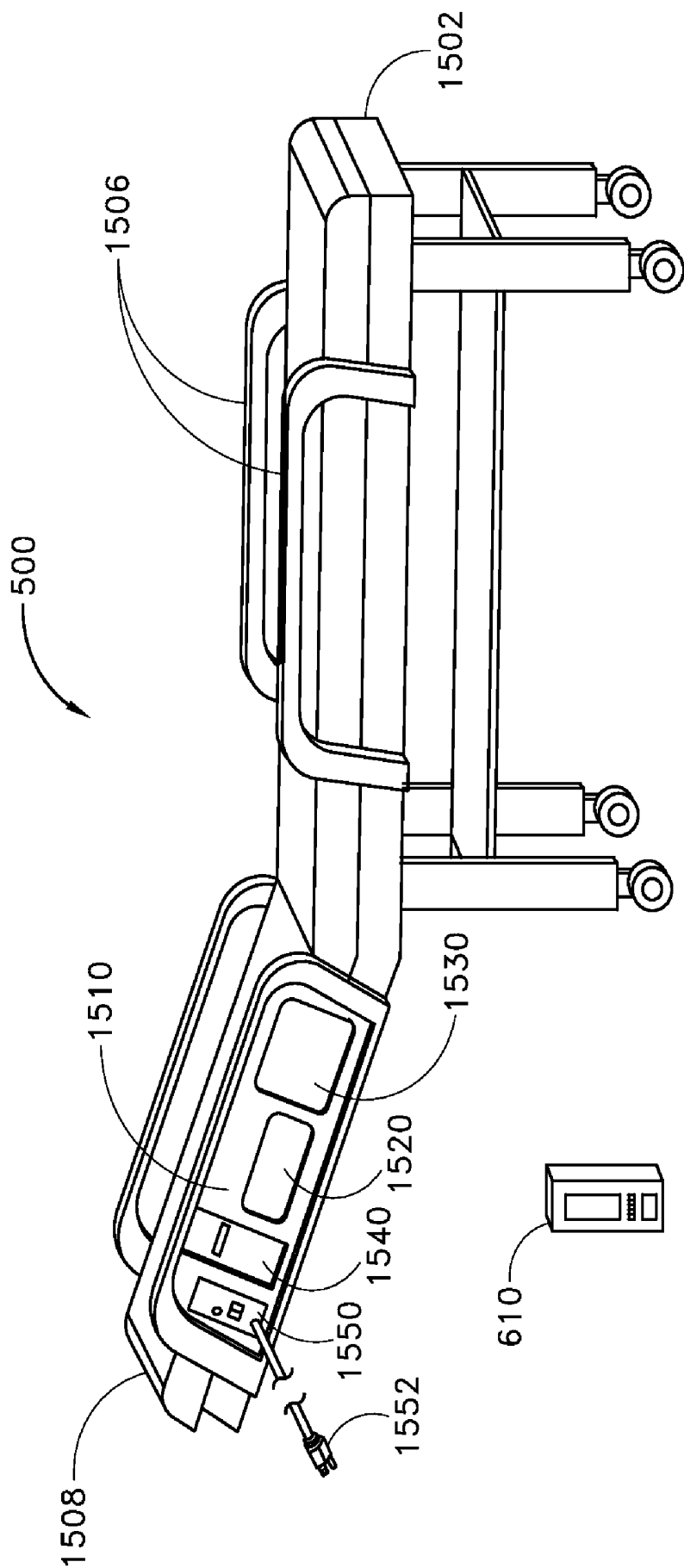


FIG. 15

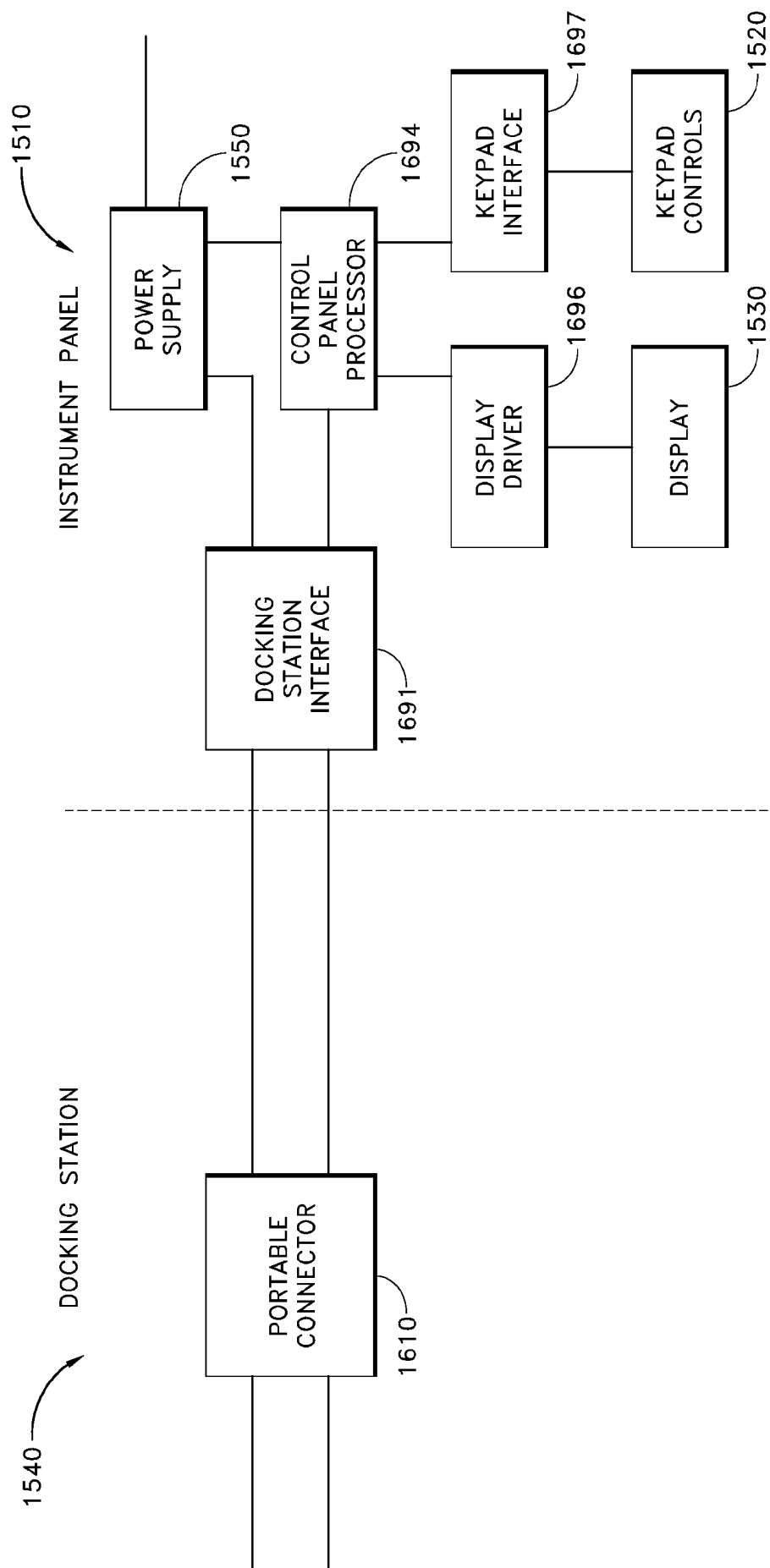


FIG. 16

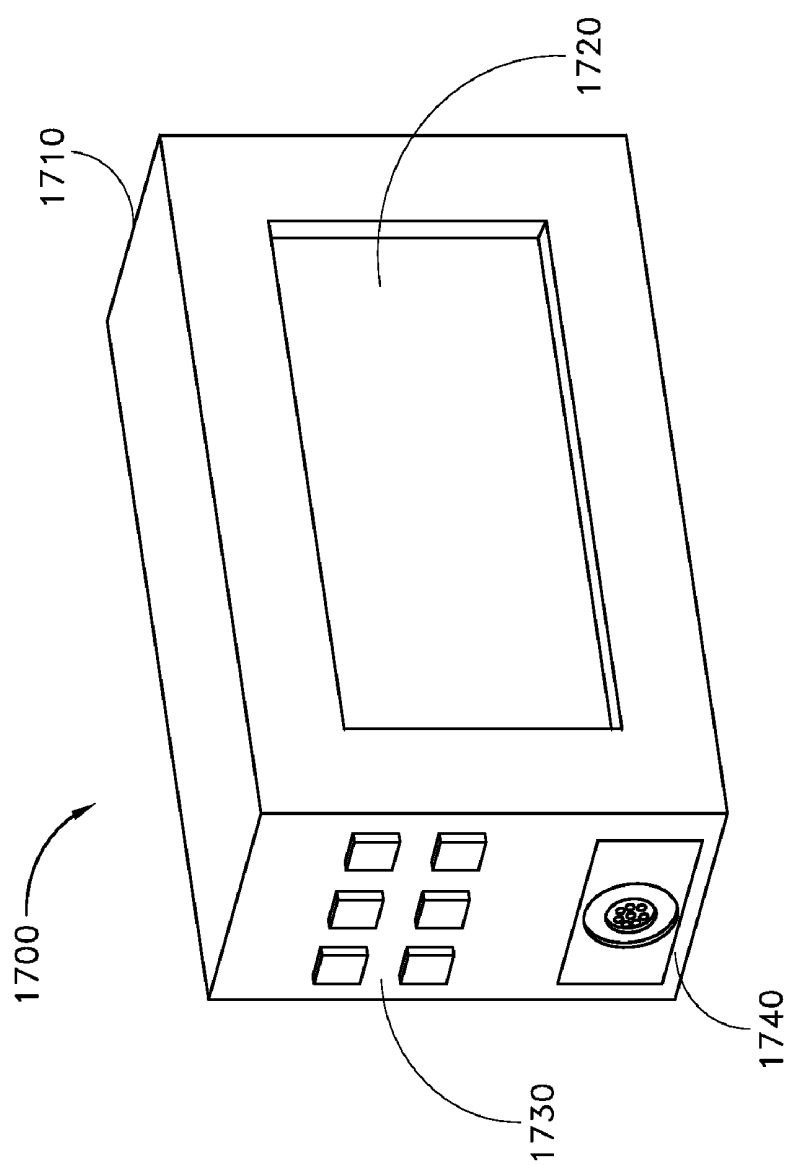


FIG. 17A

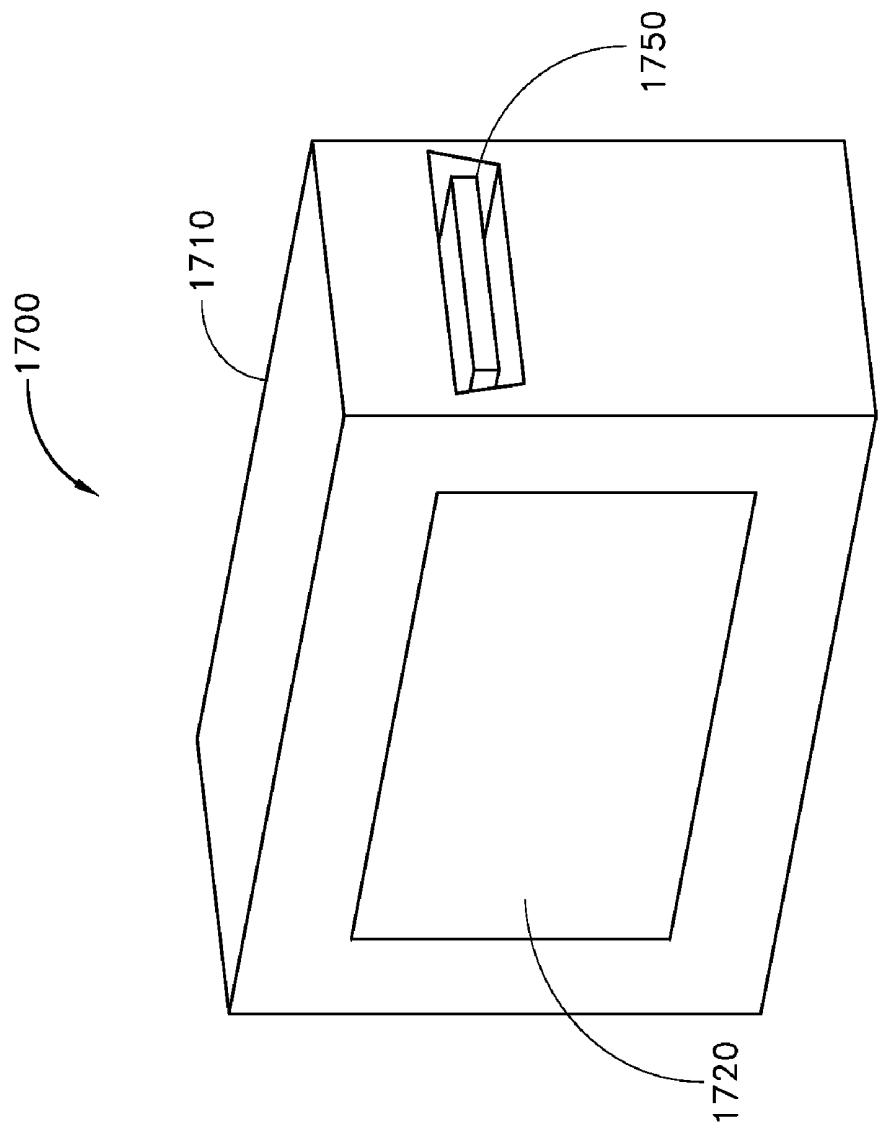


FIG. 17B

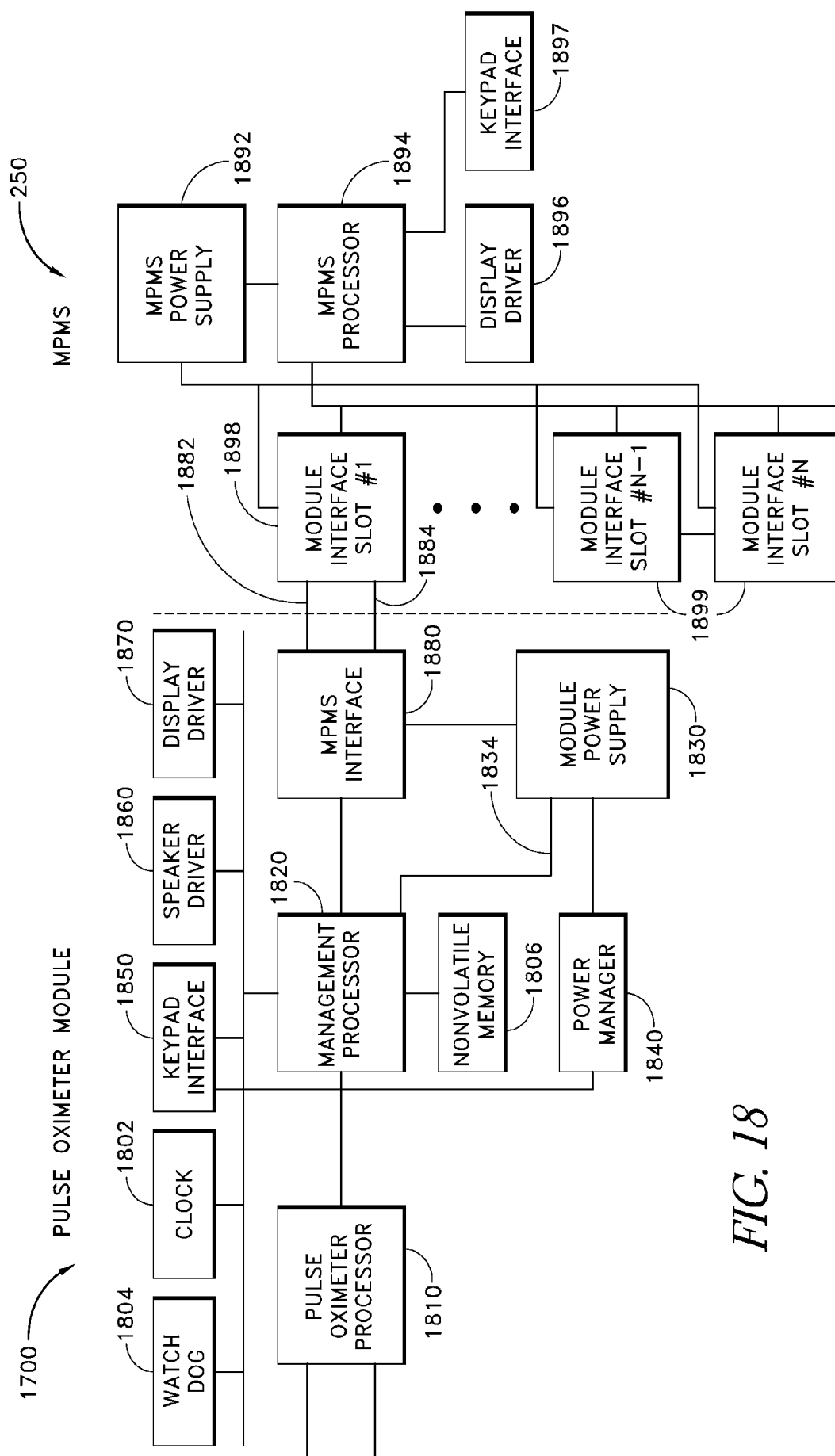
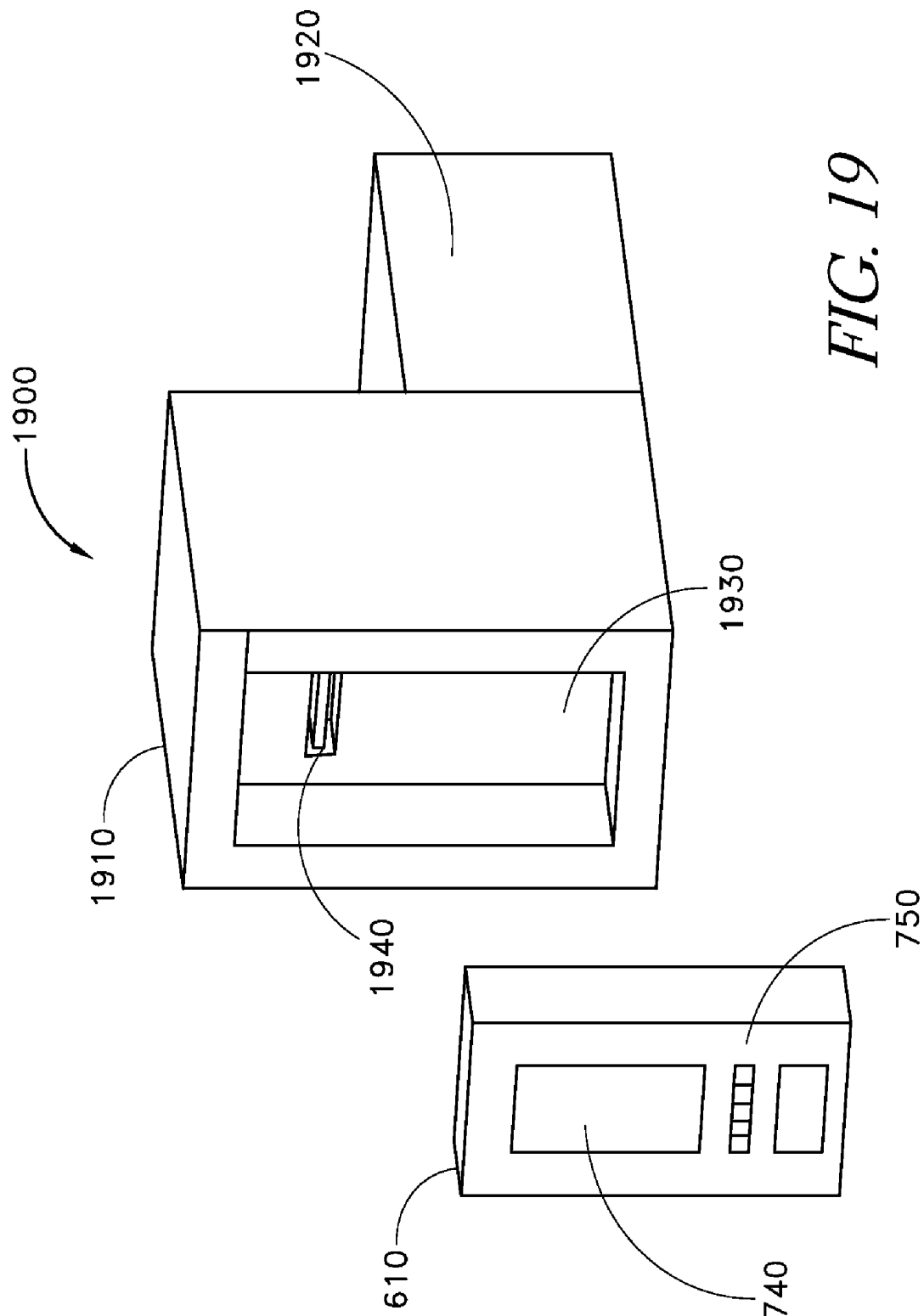


FIG. 18



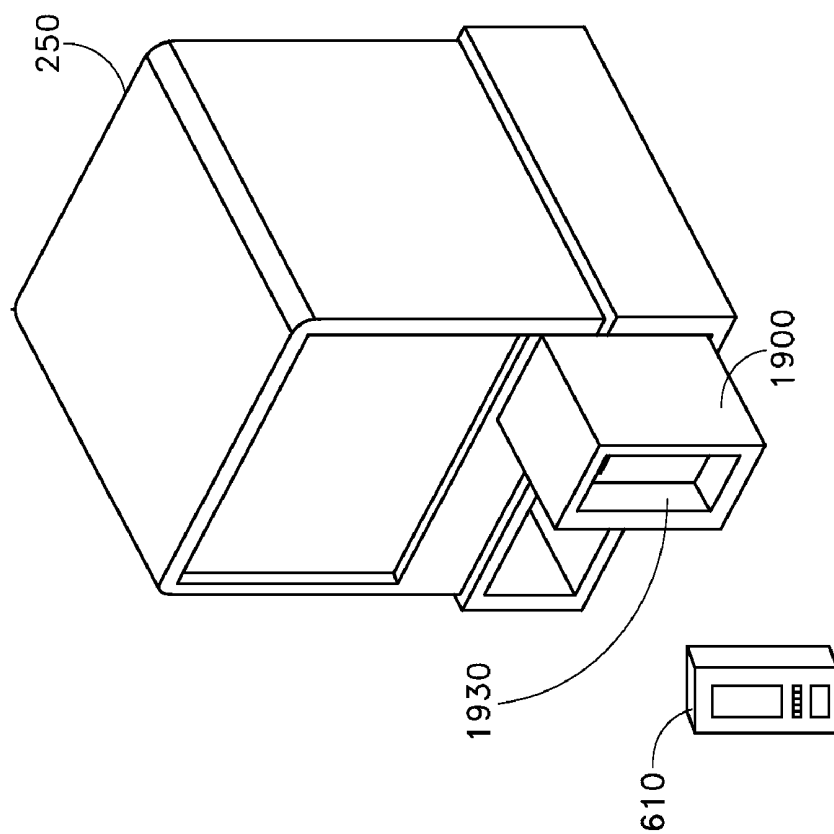


FIG. 20

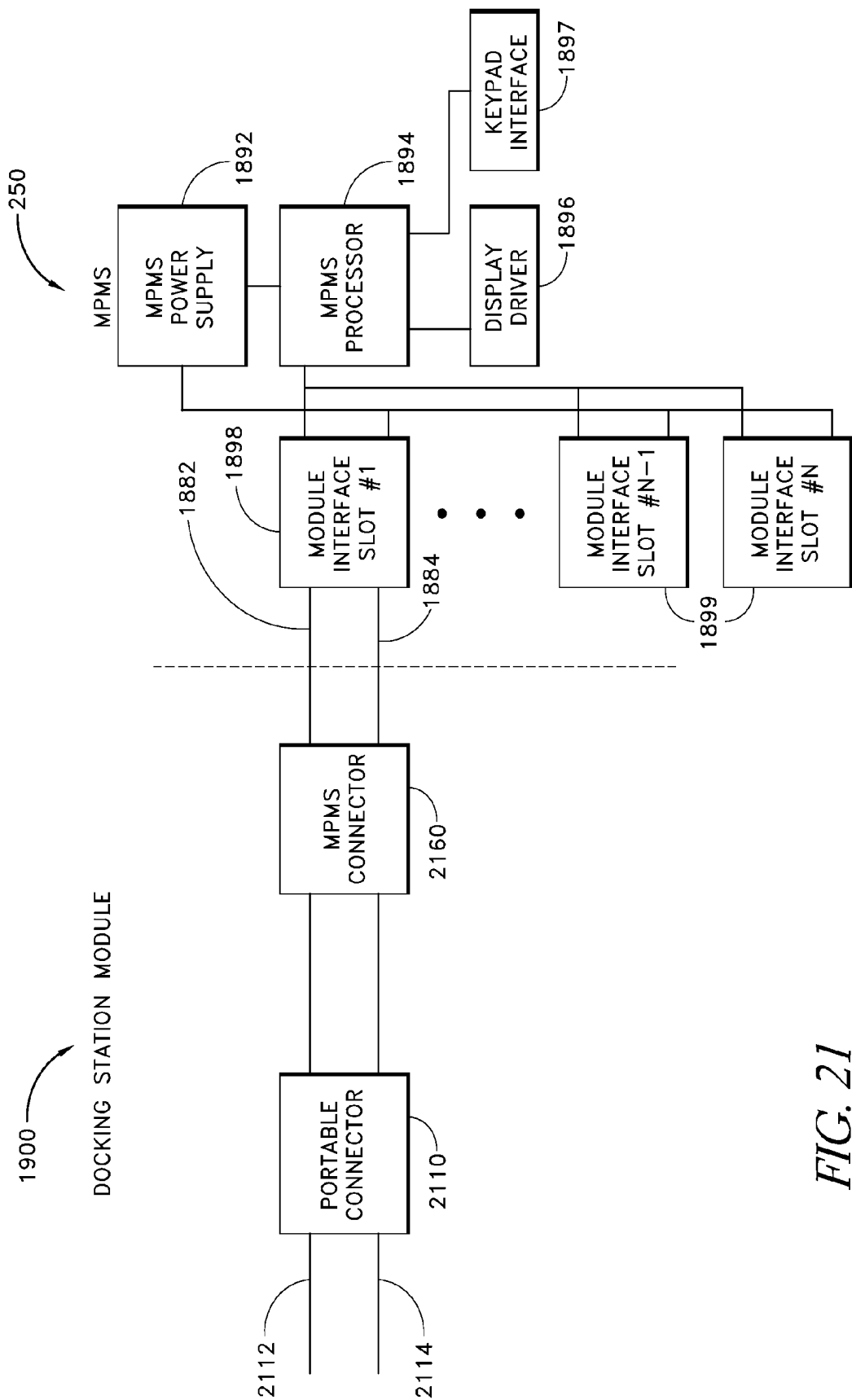


FIG. 21

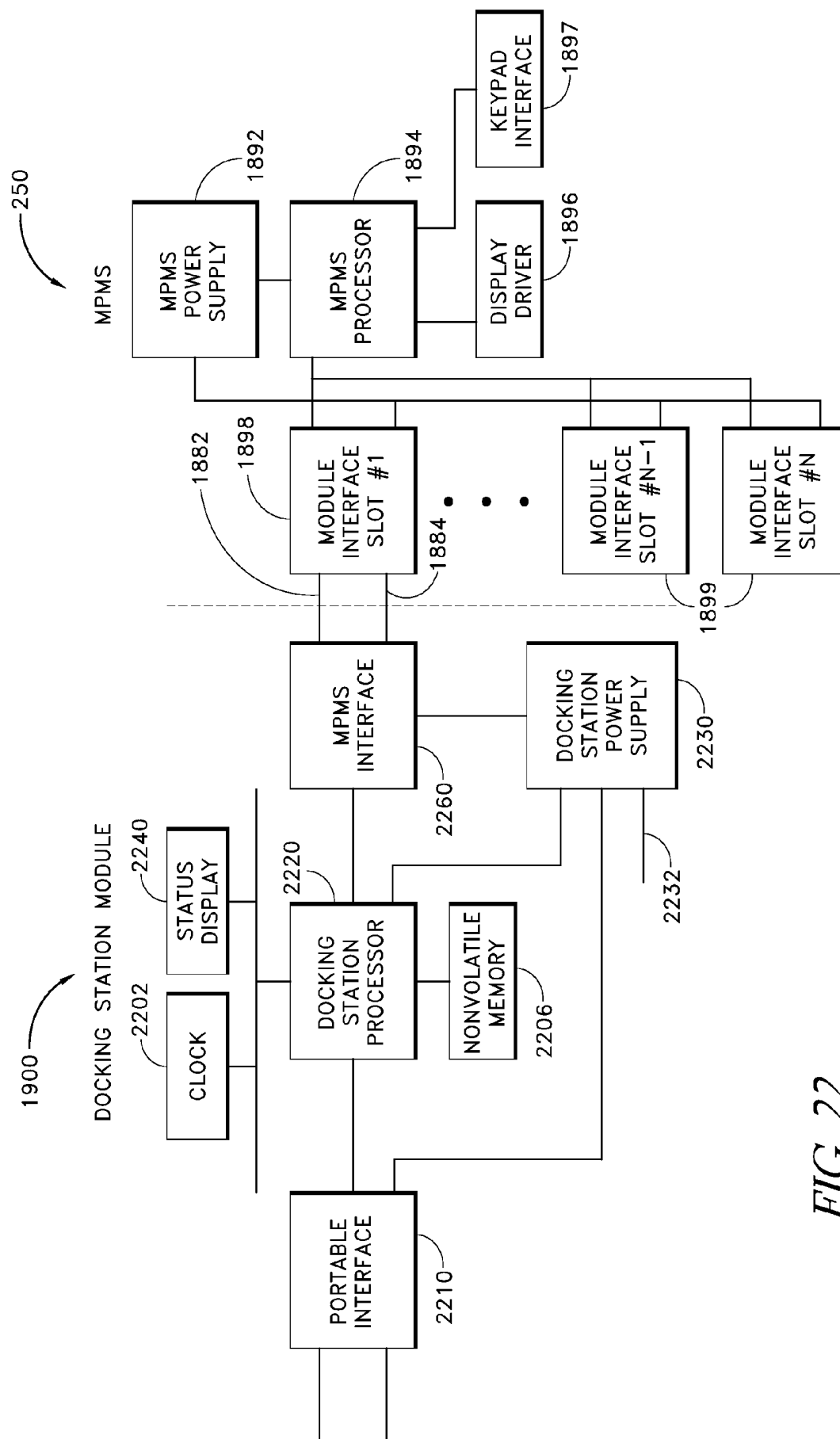


FIG. 22

DUAL-MODE PULSE OXIMETER

PRIORITY CLAIM

[0001] This application is a continuation of U.S. patent application Ser. No. 10/911,391, entitled "Dual-Mode Pulse Oximeter," filed Aug. 3, 2004, which is a continuation of U.S. patent application Ser. No. 09/641,542, entitled "Dual-Mode Pulse Oximeter," filed Aug. 18, 2000, which is a continuation-in-part of U.S. patent application Ser. No. 09/491,175 entitled "Universal/Upgrading Pulse Oximeter," filed Jan. 25, 2000, now abandoned, which claims a priority benefit under 35 U.S.C. §119(e) from U.S. Provisional Patent Application No. 60/161,565, filed Oct. 26, 1999, entitled "Improved Universal/Upgrading Pulse Oximeter," and 60/117,097, filed Jan. 25, 1999, entitled "Universal/Upgrading Pulse Oximeter." The present applications also incorporate the foregoing utility disclosure herein by reference.

BACKGROUND

[0002] Oximetry is the measurement of the oxygen level status of blood. Early detection of low blood oxygen level is critical in the medical field, for example in critical care and surgical applications, because an insufficient supply of oxygen can result in brain damage and death in a matter of minutes. Pulse oximetry is a widely accepted noninvasive procedure for measuring the oxygen saturation level of arterial blood, an indicator of oxygen supply. A pulse oximetry system generally consists of a sensor applied to a patient, a pulse oximeter, and a patient cable connecting the sensor and the pulse oximeter.

[0003] The pulse oximeter may be a standalone device or may be incorporated as a module or built-in portion of a multiparameter patient monitoring system, which also provides measurements such as blood pressure, respiratory rate and EKG. A pulse oximeter typically provides a numerical readout of the patient's oxygen saturation, a numerical readout of pulse rate, and an audible indicator or "beep" that occurs in response to each pulse. In addition, the pulse oximeter may display the patient's plethysmograph, which provides a visual display of the patient's pulse contour and pulse rate.

SUMMARY

[0004] FIG. 1 illustrates a prior art pulse oximeter 100 and associated sensor 110. Conventionally, a pulse oximetry sensor 110 has LED emitters 112, typically one at a red wavelength and one at an infrared wavelength, and a photodiode detector 114. The sensor 110 is typically attached to an adult patient's finger or an infant patient's foot. For a finger, the sensor 110 is configured so that the emitters 112 project light through the fingernail and through the blood vessels and capillaries underneath. The LED emitters 112 are activated by drive signals 122 from the pulse oximeter 100. The detector 114 is positioned at the fingertip opposite the fingernail so as to detect the LED emitted light as it emerges from the finger tissues. The photodiode generated signal 124 is relayed by a cable to the pulse oximeter 100.

[0005] The pulse oximeter 100 determines oxygen saturation (SpO_2) by computing the differential absorption by arterial blood of the two wavelengths emitted by the sensor 110. The pulse oximeter 100 contains a sensor interface 120,

an SpO_2 processor 130, an instrument manager 140, a display 150, an audible indicator (tone generator) 160 and a keypad 170. The sensor interface 120 provides LED drive current 122 which alternately activates the sensor red and IR LED emitters 112. The sensor interface 120 also has input circuitry for amplification and filtering of the signal 124 generated by the photodiode detector 114, which corresponds to the red and infrared light energy attenuated from transmission through the patient tissue site. The SpO_2 processor 130 calculates a ratio of detected red and infrared intensities, and an arterial oxygen saturation value is empirically determined based on that ratio. The instrument manager 140 provides hardware and software interfaces for managing the display 150, audible indicator 160 and keypad 170. The display 150 shows the computed oxygen status, as described above. The audible indicator 160 provides the pulse beep as well as alarms indicating desaturation events. The keypad 170 provides a user interface for such things as alarm thresholds, alarm enablement, and display options.

[0006] Computation of SpO_2 relies on the differential light absorption of oxygenated hemoglobin, HbO_2 , and deoxygenated hemoglobin, Hb, to determine their respective concentrations in the arterial blood. Specifically, pulse oximetry measurements are made at red and IR wavelengths chosen such that deoxygenated hemoglobin absorbs more red light than oxygenated hemoglobin, and, conversely, oxygenated hemoglobin absorbs more infrared light than deoxygenated hemoglobin, for example 660 nm (red) and 905 nm (IR).

[0007] To distinguish between tissue absorption at the two wavelengths, the red and IR emitters 112 are provided drive current 122 so that only one is emitting light at a given time. For example, the emitters 112 may be cycled on and off alternately, in sequence, with each only active for a quarter cycle and with a quarter cycle separating the active times. This allows for separation of red and infrared signals and removal of ambient light levels by downstream signal processing. Because only a single detector 114 is used, it responds to both the red and infrared emitted light and generates a time-division-multiplexed ("modulated") output signal 124. This modulated signal 124 is coupled to the input of the sensor interface 120.

[0008] In addition to the differential absorption of hemoglobin derivatives, pulse oximetry relies on the pulsatile nature of arterial blood to differentiate hemoglobin absorption from absorption of other constituents in the surrounding tissues. Light absorption between systole and diastole varies due to the blood volume change from the inflow and outflow of arterial blood at a peripheral tissue site. This tissue site might also comprise skin, muscle, bone, venous blood, fat, pigment, etc., each of which absorbs light. It is generally assumed that the background absorption due to these surrounding tissues is relatively invariant over short time periods and can be easily removed. Thus, blood oxygen saturation measurements are based upon a ratio of the time-varying or AC portion of the detected red and infrared signals with respect to the time-invariant or DC portion:

$$RD/IR = (\text{Red}_{AC}/\text{Red}_{DC}) / (\text{IR}_{AC}/\text{IR}_{DC})$$

The desired SpO_2 measurement is then computed from this ratio. The relationship between RD/IR and SpO_2 is most accurately determined by statistical regression of experimental measurements obtained from human volunteers and calibrated measurements of oxygen saturation. In a pulse

oximeter device, this empirical relationship can be stored as a "calibration curve" in a read-only memory (ROM) look-up table so that SpO_2 can be directly read-out of the memory in response to input RD/IR measurements.

[0009] Pulse oximetry is the standard-of-care in various hospital and emergency treatment environments. Demand has led to pulse oximeters and sensors produced by a variety of manufacturers. Unfortunately, there is no standard for either performance by, or compatibility between, pulse oximeters or sensors. As a result, sensors made by one manufacturer are unlikely to work with pulse oximeters made by another manufacturer. Further, while conventional pulse oximeters and sensors are incapable of taking measurements on patients with poor peripheral circulation and are partially or fully disabled by motion artifact, advanced pulse oximeters and sensors manufactured by the assignee of the present invention are functional under these conditions. This presents a dilemma to hospitals and other caregivers wishing to upgrade their patient oxygenation monitoring capabilities. They are faced with either replacing all of their conventional pulse oximeters, including multiparameter patient monitoring systems, or working with potentially incompatible sensors and inferior pulse oximeters manufactured by various vendors for the pulse oximetry equipment in use at the installation.

[0010] Hospitals and other caregivers are also plagued by the difficulty of monitoring patients as they are transported from one setting to another. For example, a patient transported by ambulance to a hospital emergency room will likely be unmonitored during the transition from ambulance to the ER and require the removal and replacement of incompatible sensors in the ER. A similar problem is faced within a hospital as a patient is moved between surgery, ICU and recovery settings. Incompatibility and transport problems are exacerbated by the prevalence of expensive and non-portable multi-parameter patient monitoring systems having pulse oximetry modules as one measurement parameter.

[0011] One aspect of the present invention is a dual-mode physiological measurement apparatus having a portable mode and an integrated mode. In the integrated mode, the measurement apparatus operates in conjunction with a multiparameter patient monitoring system (MPMS). In the portable mode, the measurement apparatus operates separately from the MPMS. The measurement apparatus has a physiological measurement processor, a display, a MPMS interface and a management processor. The physiological measurement processor has a sensor input and provides a physiological measurement output. In the portable mode, the display indicates a physiological parameter according to the physiological measurement output. In the integrated mode, the MPMS interface provides a communications link between the measurement apparatus and the MPMS. The management processor has as an input the physiological measurement output. The management processor controls the display in the portable mode and communicates the measurement output to the MPMS via the MPMS interface in the integrated mode.

[0012] In one embodiment, the measurement apparatus described in the previous paragraph further comprises a plug-in module. The plug-in module comprises the measurement processor and the MPMS interface and possibly

the display and management processor and is configured to be removably retained by and electrically connected to the MPMS in the integrated mode. The plug-in module may further comprise a patient cable connector providing the sensor input, a keypad accepting user inputs in the portable mode, and a module connector mating with a corresponding MPMS backplane connector in the integrated mode. In another embodiment, the measurement apparatus further comprises a docking station and a portable portion. The docking station has a docking portion, a plug-in portion and the MPMS interface. The plug-in portion is configured to be removably retained by and electrically connected to the MPMS. The portable portion comprises the measurement processor, the display and the management processor. In the integrated mode, the portable portion is configured to be removably retained by and electrically connected to the docking portion. In the portable mode, the portable portion is separated from the docking station and operated as a standalone patient monitoring apparatus. The portable portion may further comprise a patient cable connector providing the sensor input, a keypad accepting user inputs in the portable mode, and a portable connector mating with a corresponding docking station connector in the integrated mode.

[0013] Another aspect of the present invention is a patient monitoring method utilizing a standalone measurement apparatus and a multiparameter patient monitoring system (MPMS) comprising the steps of performing a first physiological measurement with the standalone apparatus physically and electrically isolated from the MPMS and presenting information related to the first measurement on a display portion of the standalone apparatus. Further steps include performing a second physiological measurement with the standalone apparatus interfaced to the MPMS, communicating the second physiological measurement to the MPMS, and presenting information related to the second measurement on a monitor portion of the MPMS.

[0014] One embodiment of the patient monitoring method described in the previous paragraph further comprises the step of plugging the measurement apparatus into a module slot portion of the MPMS so that the measurement apparatus is in electrical communications with the MPMS. Another embodiment further comprises the steps of plugging a docking station into a module slot portion of the MPMS so that the docking station is in electrical communications with the MPMS, and attaching the standalone apparatus to the docking station so that the standalone apparatus is in electrical communications with the docking station.

[0015] Yet another aspect of the present invention is a physiological measurement apparatus comprising a sensor responsive to a physiological state, a measurement processor means for calculating a physiological parameter based upon the physiological state, which presents the physiological parameter to a person, a packaging means for housing the measurement processor and the display and for providing a connection between the sensor and the measurement processor means, and an interface means for electrically connecting the packaging means to a multiparameter patient monitoring system (MPMS) in an integrated mode and for disconnecting the packaging means from the MPMS in a portable mode. In a particular embodiment, the packaging means comprises a module means for plugging into a slot portion of the MPMS. In another particular embodiment, the

physiological measurement apparatus further comprises a docking station means for plugging into a slot portion of the MPMS. In the integrated mode, the packaging means is configured to attach to the docking station.

BRIEF DESCRIPTION OF THE DRAWINGS

[0016] FIG. 1 is a block diagram of a prior art pulse oximeter;

[0017] FIG. 2 is a diagram illustrating a patient monitoring system incorporating a universal/upgrading pulse oximeter (UPO) according to the present invention;

[0018] FIG. 3 is top level block diagram of a UPO embodiment;

[0019] FIG. 4 is a detailed block diagram of the waveform generator portion of the UPO embodiment shown in FIG. 3;

[0020] FIG. 5 is an illustration of a handheld embodiment of the UPO;

[0021] FIG. 6 is a top level block diagram of another UPO embodiment incorporating a portable pulse oximeter and a docking station;

[0022] FIG. 7 is a detailed block diagram of the portable pulse oximeter portion of FIG. 6;

[0023] FIG. 8A is an illustration of the portable pulse oximeter user interface, including a keyboard and display;

[0024] FIGS. 8B-C are illustrations of the portable pulse oximeter display showing portrait and landscape modes, respectively;

[0025] FIG. 9 is a detailed block diagram of the docking station portion of FIG. 6;

[0026] FIG. 10 is a schematic of the interface cable portion of FIG. 6;

[0027] FIG. 11A is a front view of an embodiment of a portable pulse oximeter;

[0028] FIG. 11B is a back view of a portable pulse oximeter;

[0029] FIG. 12A is a front view of an embodiment of a docking station;

[0030] FIG. 12B is a back view of a docking station;

[0031] FIG. 13 is a front view of a portable docked to a docking station;

[0032] FIG. 14 is a block diagram of one embodiment of a local area network interface for a docking station;

[0033] FIG. 15 is a perspective view of a patient care bed incorporating a docking station;

[0034] FIG. 16 is a block diagram of a docking station integrated into a patient care bed;

[0035] FIGS. 17A-B are front and back perspective views of a dual-mode pulse oximeter module according to the present invention;

[0036] FIG. 18 is a block diagram of the dual-mode pulse oximeter module;

[0037] FIG. 19 is a perspective view of a docking station module according to the present invention;

[0038] FIG. 20 is a perspective view of the docking station module of FIG. 19 attached to a multiparameter patient monitoring system (MPMS);

[0039] FIG. 21 is a block diagram of a pass-through docking station module; and

[0040] FIG. 22 is a block diagram of a docking station module providing an MPMS interface.

DETAILED DESCRIPTION

[0041] FIG. 2 depicts the use of a Universal/Upgrading Pulse Oximeter ("UPO") 210 to perform patient monitoring. A pulse oximetry sensor 110 is attached to a patient (not illustrated) and provides the UPO 210 with a modulated red and IR photo-plethysmograph signal through a patient cable 220. It should be understood that while a pulse oximeter is illustrated, the present invention has applicability to other physiological parameter such as ECG, blood pressure, respiration, etc. The UPO 210 computes the patient's oxygen saturation and pulse rate from the sensor signal and, optionally, displays the patient's oxygen status. The UPO 210 may incorporate an internal power source 212, such as common alkaline batteries or a rechargeable power source. The UPO 210 may also utilize an external power source 214, such as standard 110V AC coupled with an external step-down transformer and an internal or external AC-to-DC converter.

[0042] In addition to providing pulse oximetry measurements, the UPO 210 also separately generates a signal, which is received by a pulse oximeter 260 external to the UPO 210. This signal is synthesized from the saturation calculated by the UPO 210 such that the external pulse oximeter 260 calculates the equivalent saturation and pulse rate as computed by the UPO 210. The external pulse oximeter receiving the UPO signal may be a multiparameter patient monitoring system (MPMS) 250 incorporating a pulse oximeter module 260, a standalone pulse oximeter instrument, or any other host instrument capable of measuring SpO₂.

[0043] As shown in FIG. 2, a MPMS 250 typically has a chassis 270, a multiparameter monitor 280, a processor 1894 (FIG. 18) and a power supply 1892 (FIG. 18), which derives power from a standard external AC power source. The monitor 280 typically incorporates a display 282. The chassis 270 typically has various slots 290 each configured to receive a plug-in module 298. A module connector, e.g. the connector 1750 (FIG. 17B) on the dual-mode pulse oximeter module described with respect to FIGS. 17A-B, below, mates and electrically connects with a corresponding back-plane connector (not shown) within the chassis 270. A variety of modules having various patient monitoring functions, such as blood pressure, EKG, respiratory gas and pulse oximetry 260 can be plugged into the slots 290 so that the associated patient parameters can be jointly monitored by the MPMS 250 and logged on the multiparameter display 282.

[0044] Also shown in FIG. 2, the UPO 210 is connected to an existing MPMS 250 with a cable 230, advantageously integrating the UPO oxygen status measurements with other MPMS measurements. This allows the UPO calculations to be shown on a unified display of important patient parameters, networked with other patient data, archived within electronic patient records and incorporated into alarm management, which are all MPMS functions convenient to the caregiver.

[0045] FIG. 3 depicts a block diagram of the major functions of the UPO 210, including an internal pulse oximeter 310, a waveform generator 320, a power supply 330 and an optional display 340. Attached to the UPO 210 is a sensor 110 and an external pulse oximeter 260. The internal pulse oximeter 310 provides the sensor 110 with a drive signal 312 that alternately activates the sensor's red and IR LEDs, as is known in the art. A corresponding detector signal 314 is received by the internal pulse oximeter 310. The internal pulse oximeter 310 computes oxygen saturation, pulse rate, and, in some embodiments, other physiological parameters such as pulse occurrence, plethysmograph features and measurement confidence. These parameters 318 are output to the waveform generator 320. A portion of these parameters may also be used to generate display drive signals 316 so that patient status may be read from, for example, an LED or LCD display module 340 on the UPO.

[0046] The internal pulse oximeter 310 may be a conventional pulse oximeter or, for upgrading an external pulse oximeter 260, it may be an advanced pulse oximeter capable of low perfusion and motion artifact performance not found in conventional pulse oximeters. An advanced pulse oximeter for use as an internal pulse oximeter 310 is described in U.S. Pat. No. 5,632,272 assigned to the assignee of the present invention and incorporated herein by reference. An advanced pulse oximetry sensor for use as the sensor 110 attached to the internal pulse oximeter 310 is described in U.S. Pat. No. 5,638,818 assigned to the assignee of the present invention and incorporated herein by reference. Further, a line of advanced Masimo SET® pulse oximeter OEM boards and sensors are available from the assignee of the present invention.

[0047] The waveform generator 320 synthesizes a waveform, such as a triangular waveform having a sawtooth or symmetric triangle shape, that is output as a modulated signal 324 in response to an input drive signal 322. The drive input 322 and modulation output 324 of the waveform generator 320 are connected to the sensor port 262 of the external pulse oximeter 260. The synthesized waveform is generated in a manner such that the external pulse oximeter 260 computes and displays a saturation and a pulse rate value that is equivalent to that measured by the internal pulse oximeter 310 and sensor 110. In the present embodiment, the waveforms for pulse oximetry are chosen to indicate to the external pulse oximeter 260 a perfusion level of 5%. The external pulse oximeter 260, therefore, always receives a strong signal. In an alternative embodiment, the perfusion level of the waveforms synthesized for the external pulse oximeter can be set to indicate a perfusion level at or close to the perfusion level of the patient being monitored by the internal pulse oximeter 310. As an alternative to the generated waveform, a digital data output 326, is connected to the data port 264 of the external pulse oximeter 260. In this manner, saturation and pulse rate measurements and also samples of the unmodulated, synthesized waveform can be communicated directly to the external pulse oximeter 260 for display, bypassing the external pulse oximeter's signal processing functions. The measured plethysmograph waveform samples output from the internal pulse oximeter 310 also may be communicated through the digital data output 326 to the external pulse oximeter 260.

[0048] It will be understood from the above discussion that the synthesized waveform is not physiological data from

the patient being monitored by the internal pulse oximeter 310, but is a waveform synthesized from predetermined stored waveform data to cause the external pulse oximeter 260 to calculate oxygen saturation and pulse rate equivalent to or generally equivalent (within clinical significance) to that calculated by the internal pulse oximeter 310. The actual physiological waveform from the patient received by the detector is not provided to the external pulse oximeter 260 in the present embodiment. Indeed, the waveform provided to the external pulse oximeter will usually not resemble the plethysmographic waveform of physiological data from the patient being monitored by the internal pulse oximeter 310.

[0049] The cable 230 (FIG. 2) attached between the waveform generator 320 and external pulse oximeter 260 provides a monitor ID 328 to the UPO, allowing identification of predetermined external pulse oximeter calibration curves. For example, this cable may incorporate an encoding device, such as a resistor, or a memory device, such as a PROM 1010 (FIG. 10) that is read by the waveform generator 320. The encoding device provides a value that uniquely identifies a particular type of external pulse oximeter 260 having known calibration curve, LED drive and modulation signal characteristics. Although the calibration curves of the external pulse oximeter 260 are taken into account, the wavelengths of the actual sensor 110 need not correspond to the particular calibration curve indicated by the monitor ID 328 or otherwise assumed for the external pulse oximeter 260. That is, the wavelength of the sensor 110 attached to the internal pulse oximeter 310 is not relevant or known to the external pulse oximeter 260.

[0050] FIG. 4 illustrates one embodiment of the waveform generator portion 320 of the UPO 210 (FIG. 3). Although this illustration may suggest a hardware implementation, the functions of the waveform generator may be implemented in software or firmware or a combination of hardware, software and firmware. The waveform generator 320 performs waveform synthesis with a waveform look-up table ("LUT") 410, a waveform shaper 420 and a waveform splitter 430. The waveform LUT 410 is advantageously a memory device, such as a ROM (read only memory) that contains samples of one or more waveform portions or segments containing a single waveform. These stored waveform segments may be as simple as a single period of a triangular waveform, having a sawtooth or symmetric triangle shape, or more complicated, such as a simulated plethysmographic pulse having various physiological features, for example rise time, fall time and dicrotic notch.

[0051] The waveform shaper 420 creates a continuous repeated waveform from the waveform segments provided by the waveform LUT 410. The waveform shaper 420 has a shape parameter input 422 and an event indicator input 424 that are buffered 470 from the parameters 318 output from the internal pulse oximeter 310 (FIG. 3). The shape parameter input 422 determines a particular waveform segment in the waveform LUT 410. The chosen waveform segment is specified by the first address transmitted to the waveform LUT 410 on the address lines 426. The selected waveform segment is sent to the waveform shaper 420 as a series of samples on the waveform data lines 412.

[0052] The event indicator input 424 specifies the occurrence of pulses in the plethysmograph waveform processed by the internal pulse oximeter 310 (FIG. 3). For example, the

event indicator may be a delta time from the occurrence of a previously detected falling pulse edge or this indicator could be a real time or near real time indicator or flag of the pulse occurrence. The waveform shaper 420 accesses the waveform LUT 410 to create a corresponding delta time between pulses in the synthesized waveform output 428. In one embodiment, the waveform shaper is clocked at a predetermined sample rate. From a known number of samples per stored waveform segment and the input delta time from the event indicator, the waveform shaper 420 determines the number of sequential addresses to skip between samples and accesses the waveform LUT 410 accordingly. This effectively “stretches” or “shrinks” the retrieved waveform segment so as to fit in the time between two consecutive pulses detected by the UPO.

[0053] The waveform splitter 430 creates a first waveform 432 corresponding to a first waveform (such a red wavelength) expected by the external pulse oximeter 260 (FIG. 3) and a second waveform (such as infrared) 434 expected by the external pulse oximeter 260. The relative amplitudes of the first waveform 432 and second waveform 434 are adjusted to correspond to the ratio output 444 from a calibration curve LUT 440. Thus, for every value of measured oxygen saturation at the sat input 442, the calibration curve LUT 440 provides a corresponding ratio output 444 that results in the first waveform 432 and the second waveform 434 having an amplitude ratio that will be computed by the external pulse oximeter 260 (FIG. 3) as equivalent to the oxygen saturation measured by the internal pulse oximeter 310 (FIG. 3).

[0054] As described above, one particularly advantageous aspect of the UPO is that the operating wavelengths of the sensor 110 (FIG. 3) are not relevant to the operating wavelengths required by the external pulse oximeter 260 (FIG. 3), i.e. the operating wavelengths that correspond to the calibration curve or curves utilized by the external pulse oximeter. The calibration curve LUT 440 simply permits generation of a synthesized waveform as expected by the external oximeter 260 (FIG. 3) based on the calibration curve used by the external pulse oximeter 260 (FIG. 3). The calibration curve LUT 440 contains data about the known calibration curve of the external pulse oximeter 260 (FIG. 3), as specified by the monitor ID input 328. In other words, the waveform actually synthesized is not a patient plethysmographic waveform. It is merely a stored waveform that will cause the external pulse oximeter to calculate the proper oxygen saturation and pulse rate values. Although this does not provide a patient plethysmograph on the external pulse oximeter for the clinician, the calculated saturation and pulse rate values, which is what is actually sought, will be accurate.

[0055] A modulator 450 responds to an LED drive input 322 from the external pulse oximeter to generate a modulated waveform output 324 derived from the first waveform 432 and second waveform 434. Also, a data communication interface 460 transmits as a digital data output 326 the data obtained from the sat 442, pulse rate 462 and synthesized waveform 428 inputs.

[0056] FIG. 5 depicts a handheld UPO 500 embodiment. The handheld UPO 500 has keypad inputs 510, an LCD display 520, an external power supply input 530, an output port 540 for connection to an external pulse oximeter and a

sensor input 550 at the top edge (not visible). The display 520 shows the measured oxygen saturation 522, the measured pulse rate 524, a pulsating bar 526 synchronized with pulse rate or pulse events, and a confidence bar 528 indicating confidence in the measured values of saturation and pulse rate. Also shown are low battery 572 and alarm enabled 574 status indicators.

[0057] The handheld embodiment described in connection with FIG. 5 may also advantageously function in conjunction with a docking station that mechanically accepts, and electrically connects to, the handheld unit. The docking station may be co-located with a patient monitoring system and connected to a corresponding SpO₂ module sensor port, external power supply, printer and telemetry device, to name a few options. In this configuration, the handheld UPO may be removed from a first docking station at one location to accompany and continuously monitor a patient during transport to a second location. The handheld UPO can then be conveniently placed into a second docking station upon arrival at the second location, where the UPO measurements are displayed on the patient monitoring system at that location.

[0058] FIG. 6 shows a block diagram of a UPO embodiment, where the functions of the UPO 210 are split between a portable pulse oximeter 610 and a docking station 660. The portable pulse oximeter 610 (“portable”) is a battery operated, fully functional, stand-alone pulse oximeter instrument. The portable 610 connects to a sensor 110 (FIG. 2) through a UPO patient cable 220 (FIG. 2) attached to a patient cable connector 618. The portable 610 provides the sensor 110 with a drive signal 612 that alternately activates the sensor’s red and IR LEDs, as is well-known in the art. The portable also receives a corresponding detector signal 614 from the sensor. The portable can also input a sensor ID on the drive signal line 612, as described in U.S. Pat. No. 5,758,644 entitled Manual and Automatic Probe Calibration, assigned to the assignee of the present invention and incorporated herein by reference.

[0059] The portable 610 can be installed into the docking station 660 to expand its functionality. When installed, the portable 610 can receive power 662 from the docking station 660 if the docking station 660 is connected to external power 668. Alternately, with no external power 668 to the docking station 660, the portable 610 can supply power 662 to the docking station 660. The portable 610 communicates to the docking station with a bidirectional serial data line 664. In particular, the portable 610 provides the docking station with SpO₂, pulse rate and related parameters computed from the sensor detector signal 614. When the portable 610 is installed, the docking station 660 may drive a host instrument 260 (FIG. 2) external to the portable 610. Alternatively, the portable 610 and docking station 660 combination may function as a standalone pulse oximeter instrument, as described below with respect to FIG. 13.

[0060] In one embodiment, the docking station 660 does not perform any action when the portable 610 is not docked. The user interface for the docking station 660, i.e. keypad and display, is on the portable 610 in the present embodiment. An indicator LED on the docking station 660 is lit when the portable is docked. The docking station 660 generates a detector signal output 674 to the host instrument 260 (FIG. 2) in response to LED drive signals 672 from the

host instrument and SpO₂ values and related parameters, received from the portable 610. The docking station 660 also provides a serial data output 682, a nurse call 684 and an analog output 688.

[0061] An interface cable 690 connects the docking station 660 to the host instrument. The LED drive signals 672 and detector signal output 674 are communicated between the docking station 660 and the host instrument 260 (FIG. 2) via the interface cable 690. The interface cable 690 provides a sync data output 692 to the docking station 660, communicating sensor, host instrument (e.g. monitor ID 328, FIG. 3) and calibration curve data. Advantageously, this data allows the docking station 660 to provide signals to a particular host instrument on which it can operate.

[0062] FIG. 7 provides further detail of the portable 610. The portable components has a pulse oximeter processor 710, a management processor 720, a power supply 730, a display 740 and a keypad 750. The pulse oximeter processor 710 functions as an internal pulse oximeter, interfacing the portable to a sensor 110 (FIG. 2) and deriving SpO₂, pulse rate, a plethysmograph and a pulse indicator. An advanced pulse oximeter for use as the pulse oximeter processor 710 is described in U.S. Pat. No. 5,632,272, referenced above. An advanced pulse oximetry sensor for use as the sensor 110 (FIG. 2) attached to the pulse oximeter processor 710 is described in U.S. Pat. No. 5,638,818, also referenced above. Further, a line of advanced Masimo SET® pulse oximeter OEM boards and sensors are available from the assignee of the present invention. In one embodiment, the pulse oximeter processor 710 is the Masimo SET® MS-3L board or a low power MS-5 board available from Masimo Corporation.

[0063] The management processor 720 controls the various functions of the portable 610, including asynchronous serial data communications 724 with the pulse oximeter processor 710 and synchronous serial communications 762 with the docking station 660 (FIG. 6). The physical and electrical connection to the docking station 660 (FIG. 6) is via a docking station connector 763 and the docking station interface 760, respectively. The processor 720 utilizes a real-time clock 702 to keep the current date and time, which includes time and date information that is stored along with SpO₂ parameters to create trend data. In one embodiment, the processor of the portable 610 and the docking station 660 (FIG. 6) can be from the same family of processors to share common routines and minimize code development time.

[0064] The processor 720 also controls the user interface 800 (FIG. 8A) by transferring display data 742 to the display 740, including display updates and visual alarms, and by interpreting keystroke data 752 from the keypad 750. The processor 720 generates various alarm signals, when required, via an enable signal 728, which controls a speaker driver 770. The speaker driver 770 actuates a speaker 772, which provides audible indications such as, for example, alarms and pulse beeps. The processor 720 also monitors system status, which includes battery status 736, indicating battery levels, and docked status 764, indicating whether the portable 610 is connected to the docking station 660 (FIG. 6). When the portable 610 is docked and is on, the processor 720 also decides when to turn on or off docking station power 732.

[0065] Advantageously, the caregiver can set (i.e. configure or program) the behavior of the portable display 740 and

alarms when the docked portable 610 senses that an interface cable 690 has connected the docking station 660 to an external pulse oximeter, such as a multiparameter patient monitoring system. In one user setting, for example, the portable display 740 stops showing the SpO₂ 811 (FIG. 8) and pulse rate 813 (FIG. 8) values when connected to an external pulse oximeter to avoid confusing the caregiver, who can read equivalent values on the patient monitoring system. The display 740, however, continues to show the plethysmograph 815 (FIG. 8) and visual pulse indicator 817 (FIG. 8) waveforms. For one such user setting, the portable alarms remain active.

[0066] Another task of the processor 720 includes maintenance of a watchdog function. The watchdog 780 monitors processor status on the watchdog data input 782 and asserts the μ P reset output 784 if a fault is detected. This resets the management processor 720, and the fault is indicated with audible and visual alarms.

[0067] The portable 610 gets its power from batteries in the power supply 730 or from power 766 supplied from the docking station 660 (FIG. 6) via the docking station interface 760. A power manager 790 monitors the on/off switch on the keypad 750 and turns-on the portable power accordingly. The power manager 790 turns off the portable on command by the processor 720. DC/DC converters within the power supply 730 generate the required voltages 738 for operation of the portable 610 and docking station power 732. The portable batteries are preferably rechargeable batteries or another renewable power source. The batteries of the power supply 730 supply docking station power 732 when the docking station 660 (FIG. 6) is without external power. A battery charger within the docking station power supply provides charging current 768 to rechargeable batteries within the power supply 730. The docking station power supply 990 (FIG. 9) monitors temperature 734 from a thermistor in the rechargeable battery pack, providing an indication of battery charge status.

[0068] A non-volatile memory 706 is connected to the management processor 720 via a high-speed bus 722. In the present embodiment, the memory 706 is an erasable and field re-programmable device used to store boot data, manufacturing serial numbers, diagnostic failure history, adult SpO₂ and pulse rate alarm limits, neonate SpO₂ and pulse rate alarm limits, SpO₂ and pulse rate trend data, and program data. Other types of non-volatile memory are well known. The SpO₂ and pulse rate alarm limits, as well as SpO₂ related algorithm parameters, may be automatically selected based on the type of sensor 110 (FIG. 2), adult or neonate, connected to the portable 610.

[0069] The LCD display 740 employs LEDs for a backlight to increase its contrast ratio and viewing distance when in a dark environment. The intensity of the backlight is determined by the power source for the portable 610. When the portable 610 is powered by either a battery pack within its power supply 730 or a battery pack in the docking station power supply 990 (FIG. 9), the backlight intensity is at a minimum level. When the portable 610 is powered by external power 668 (FIG. 6), the backlight is at a higher intensity to increase viewing distance and angle. In one embodiment, a button on the portable permits overriding these intensity settings, and provides adjustment of the intensity. The backlight is controlled in two ways. Whenever

any key is pressed, the backlight is illuminated for a fixed number of seconds and then turns off, except when the portable is docked and derives power from an external source. In that case, the backlight is normally on unless deactivated with a key on the portable 610.

[0070] FIG. 8A illustrates the portable user interface 800, which includes a display 740 and a keypad 750. In one embodiment, the display 740 is an LCD device having 160 pixels by 480 pixels. The display 740 can be shown in portrait mode, illustrated in FIG. 8B, or in landscape mode, illustrated in FIG. 8C. A tilt (orientation) sensor 950 (FIG. 9) in the docking station 660 (FIG. 6) or a display mode key on the portable 610 (FIG. 6) determines portrait or landscape mode. The tilt sensor 950 (FIG. 9) can be a gravity-activated switch or other device responsive to orientation and can be alternatively located in the portable 610 (FIG. 6). In a particular embodiment, the tilt sensor 950 (FIG. 9) is a non-mercury tilt switch, part number CW 1300-1, available from Comus International, Nutley, N.J. (www.comus-intl.com). The tilt sensor 950 (FIG. 9) could also be a mercury tilt switch.

[0071] Examples of how the display area can be used to display SpO₂ 811, pulse rate 813, a plethysmographic waveform 815, a visual pulse indicator 817 and soft key icons 820 in portrait and landscape mode are shown in FIGS. 8B and 8C, respectively. The software program of the management processor 720 (FIG. 7) can be easily changed to modify the category, layout and size of the display information shown in FIGS. 8B-C. Other advantageous information for display is SpO₂ limits, alarm limits, alarm disabled, exception messages and battery status.

[0072] The keypad 750 includes soft keys 870 and fixed keys 880. The fixed keys 880 each have a fixed function. The soft keys 870 each have a function that is programmable and indicated by one of the soft key icons 820 located next to the soft keys 870. That is, a particular one of the soft key icons 820 is in proximity to a particular one of the soft keys 870 and has a text or a shape that suggests the function of that particular one of the soft keys 870. In one embodiment, the button portion of each key of the keypad 750 is constructed of florescent material so that the keys 870, 880 are visible in the dark.

[0073] In one embodiment, the keypad 750 has one row of four soft keys 870 and one row of three fixed keys 880. Other configurations are, of course, available, and specific arrangement is not significant. In one embodiment, the functions of the three fixed keys 880 are power, alarm silence and light/contrast. The power function is an on/off toggle button. The alarm silence function and the light/contrast function have dual purposes depending on the duration of the key press. A momentary press of the key corresponding to the alarm silence function will disable the audible alarm for a fixed period of time. To disable the audible alarm indefinitely, the key corresponding to the alarm silence function is held down for a specified length of time. If the key corresponding to the alarm silence function is pressed while the audible alarm has been silenced, the audible alarm is reactivated. If the key corresponding to the light/contrast function is pressed momentarily, it is an on/off toggle button for the backlight. If the key corresponding to the light/contrast function is held down, the display contrast cycles through its possible values.

[0074] In the present embodiment, the default functions of the four soft keys 870 are pulse beep up volume, pulse beep down volume, menu select, and display mode. These functions are indicated on the display by the up arrow, down arrow, "menu" and curved arrow soft key icons 820, respectively. The up volume and down volume functions increase or decrease the audible sound or "beep" associated with each detected pulse. The display mode function rotates the display 740 through all four orthogonal orientations, including portrait mode (FIG. 8B) and landscape mode (FIG. 8C), with each press of the corresponding key. The menu select function allows the functionality of the soft keys 870 to change from the default functions described above. Examples of additional soft key functions that can be selected using this menu feature are set SpO₂ high/low limit, set pulse rate high/low limit, set alarm volume levels, set display to show trend data, print trend data, erase trend data, set averaging time, set sensitivity mode, perform synchronization, perform rechargeable battery maintenance (deep discharge/recharge to remove battery memory), and display product version number.

[0075] FIG. 9 provides further details of the docking station 660, which includes a docking station processor 910, a non-volatile memory 920, a waveform generator 930, a PROM interface 940, a tilt sensor 950, a portable interface 970 and associated connector 972, status indicators 982, a serial data port 682, a nurse call output 684, an analog output 688 and a power supply 990. In one embodiment, the docking station 660 is intended to be associated with a fixed (non-transportable) host instrument, such as a multiparameter patient monitoring instrument in a hospital emergency room. In a transportable embodiment, the docking station 660 is movable, and includes a battery pack within the power supply 990.

[0076] The docking station processor 910 orchestrates the activity on the docking station 660. The processor 910 provides the waveform generator 930 with parameters 932 as discussed above for FIGS. 3 and 4. The processor 910 also provides asynchronous serial data 912 for communications with external devices and synchronous serial data 971 for communications with the portable 610 (FIG. 6). In addition, the processor 910 determines system status including sync status 942, tilt status 952 and power status 992. The portable management processor 720 (FIG. 7) performs the watchdog function for the docking station processor 910. The docking station processor 910 sends watchdog messages to the portable processor 720 (FIG. 7) as part of the synchronous serial data 972 to ensure the correct operation of the docking station processor 910.

[0077] The docking station processor 910 can also perform resource downloading to the portable processor 720 (FIG. 7) as part of the synchronous serial data 971. That is, the docking station 660 can provide functionality not present in the portable 610 (FIG. 6), and, when docked, that added capability can be reflected by the portable user interface, i.e. the soft keys 870 (FIG. 8A) and the display 740 (FIG. 8A). For example, a portable 610 (FIG. 6) providing only pulse oximetry measurements can be docked to a docking station 660 having the added functionality of blood pressure measurements. The docking station 660 can download a blood pressure measurement menu and an associated user interface to the portable 610 (FIG. 6) upon docking, allowing the portable 610 (FIG. 6) to control and display this additional

docking station functionality. Docking station resource downloading would apply to other physiological measurements as well, such as respiration rate, EEG, ECG and EtCO₂ to name a few.

[0078] The docking station processor 910 accesses non-volatile memory 920 over a high-speed bus 922. The non-volatile memory 920 is re-programmable and contains program data for the processor 910 including instrument communication protocols, synchronization information, a boot image, manufacturing history and diagnostic failure history.

[0079] The waveform generator 930 generates a synthesized waveform that a conventional pulse oximeter can process to calculate SpO₂ and pulse rate values or exception messages, as described above with respect to FIG. 4. However, in the present embodiment, as explained above, the waveform generator output does not reflect a physiological waveform. It is merely a waveform constructed from stored memory data to cause the external pulse oximeter to calculate the correct saturation and pulse rate. In an alternative arrangement, physiological data could be scaled or otherwise mathematically converted and provided to the external pulse oximeter, but the external pulse oximeter would often not be able to calculate the proper saturation values, and the upgrading feature would be lost. This is particularly true due to the likely mismatch in the actual sensor wavelength and the calibration curves in the external pulse oximeter. The waveform generator 930 is enabled if an interface cable 690 (FIG. 6), described below with respect to FIG. 10, with valid synchronization information is connected. Otherwise, the power to the waveform generator 930 is disabled, thereby rendering the waveform generator inoperable.

[0080] The status indicators 982 are a set of LEDs on the front of the docking station 660 used to indicate various conditions including external power (AC), portable docked, portable battery charging, docking station battery charging and alarm. The serial data port 682 is used to interface with either a computer, a serial port of conventional pulse oximeters or serial printers via a standard RS-232 DB-9 connector 962. This port 682 can output trend memory, SpO₂ and pulse rate and support the system protocols of various manufacturers. The analog output 688 is used to interface with analog input chart recorders via a connector 964 and can output "real-time" or trend SpO₂ and pulse rate data. The nurse call output 684 from a connector 964 is activated when alarm limits are exceeded for a predetermined number of consecutive seconds. In another embodiment, data, including alarms, could be routed to any number of communications ports, and even over the Internet, to permit remote use of the upgrading pulse oximeter.

[0081] The PROM interface 940 accesses synchronization data 692 from the PROM 1010 (FIG. 10) in the interface cable 690 (FIGS. 6, 10) and provides synchronization status 942 to the docking station processor 910. The portable interface 970 provides the interconnection to the portable 610 (FIG. 6) through the docking station interface 760 (FIG. 7).

[0082] As shown in FIG. 9, external power 668 is provided to the docking station 660 through a standard AC connector 968 and on/off switch 969. When the docking station 660 has external power 668, the power supply 990 charges the battery in the portable power supply 730 (FIG.

7) and the battery, if any, in the docking station power supply 990. When the portable 610 (FIG. 6) is either removed or turned off, the docking station power 973 is removed and the docking station 660 is turned off, except for the battery charger portion of the power supply 990. The docking station power 973 and, hence, the docking station 660 powers on whenever a docked portable 610 (FIG. 6) is switched on. The portable 610 (FIG. 6) supplies power for an embodiment of the docking station 660 without a battery when external power 668 is removed or fails.

[0083] FIG. 10 provides further detail regarding the interface cable 690 used to connect between the docking station 660 (FIG. 6) and the host instrument 260 (FIG. 2). The interface cable 690 is configured to interface to a specific host instrument via the sensor input to the host instrument. A PROM 1010 built into the interface cable 690 contains information identifying a sensor type, a specific host instrument, and the calibration data (if necessary) of the specific host instrument. This PROM information can be read by the docking station 660 (FIG. 6) as synchronization data 692. Advantageously, the synchronization data 692 allows the docking station 660 (FIG. 6) to generate a waveform to the host instrument that causes the host instrument to display SpO₂ values equivalent to those calculated by the portable 610 (FIG. 6). The interface cable 690 includes an LED drive path 672. In the embodiment shown in FIG. 10, the LED drive path 672 is configured for common anode LEDs and includes IR cathode, red cathode and common anode signals. The interface cable 690 also includes a detector drive path 674, including detector anode and detector cathode signals.

[0084] A menu option on the portable 610 (FIG. 6) also allows synchronization information to be calculated in the field. With manual synchronization, the docking station 660 (FIG. 6) generates a waveform to the host instrument 260 (FIG. 2) and displays an expected SpO₂ value. The user enters into the portable the SpO₂ value displayed on the host instrument using the portable keypad 750 (FIG. 7). These steps are repeated until a predetermined number of data points are entered and the SpO₂ values displayed by the portable and the host instrument are consistent.

[0085] FIGS. 11A-B depict an embodiment of the portable 610, as described above with respect to FIG. 6. FIGS. 12A-B depict an embodiment of the docking station 660, as described above with respect to FIG. 6. FIG. 13 depicts an embodiment of the UPO 210 where the portable 610 is docked with the docking station 660, also as described above with respect to FIG. 6.

[0086] FIG. 11A depicts the portable front panel 1110. The portable 610 has a patient cable connector 618, as described above with respect to FIG. 6. Advantageously, the connector 618 is rotatably mounted so as to minimize stress on an attached patient cable (not shown). In one embodiment, the connector 618 can freely swivel between a plane parallel to the front panel 1110 and a plane parallel to the side panel 1130. In another embodiment, the connector 618 can swivel between, and be releasably retained in, three semi-locked positions. The connector 618 can be rotated from a semi-locked position with moderate force. A first locked position is as shown, where the connector is in a plane parallel to the front panel 1110. A second locked position is where the connector 618 is in a plane parallel to the side panel 1130.

The connector **618** also has an intermediate locked position 45° between the first and the second locked positions. The connector **618** is placed in the first locked position for attachment to the docking station **660**.

[0087] Shown in FIG. 11A, the portable front panel **1110** also has a speaker **772**, as described with respect to FIG. 7. Further, the front panel **1110** has a row of soft keys **870** and fixed keys **880**, as described above with respect to FIG. 8. In addition, the front panel **1110** has a finger actuated latch **1120** that locks onto a corresponding catch **1244** (FIG. 12A) in the docking station **660**, allowing the portable **610** to be releasably retained by the docking station **660**. An OEM label can be affixed to a recessed area **1112** on the front panel **1110**.

[0088] FIG. 11B depicts the portable back panel **1140**. The back panel **1140** has a socket **763**, a pole clamp mating surface **1160**, and a battery pack compartment **1170**. The socket **763** is configured to mate with a corresponding docking station plug **972** (FIG. 12A). The socket **763** and plug **972** (FIG. 12A) provide the electrical connection interface between the portable **610** and the docking station **660** (FIG. 12A). The socket **763** houses multiple spring contacts that compress against plated edge-connector portions of the docking station plug **972** (FIG. 12A). A conventional pole clamp (not shown) may be removably attached to the mating surface **1160**. This conveniently allows the portable **610** to be held to various patient-side or bedside mounts for hands-free pulse oximetry monitoring. The portable power supply **730** (FIG. 7) is contained within the battery pack compartment **1170**. The compartment **1170** has a removable cover **1172** for protection, insertion and removal of the portable battery pack. Product labels, such as a serial number identifying a particular portable, can be affixed with the back panel indent **1142**.

[0089] FIG. 12A depicts the front side **1210** of the docking station **660**. The front side **1210** has a docking compartment **1220**, a pole clamp recess **1230**, pivots **1242**, a catch **1244**, a plug connector **972** and LED status indicators **982**. The docking compartment **1220** accepts and retains the portable **610** (FIGS. 11A-B), as shown in FIG. 13. When the portable **610** (FIGS. 11A-B) is docked in the compartment **1220**, the pole clamp recess **1230** accommodates a pole clamp (not shown) attached to the portable's pole clamp mating surface **1160** (FIG. 11B), assuming the pole clamp is in its closed position. The portable **610** (FIGS. 11A-B) is retained in the compartment **1220** by pivots **1242** that fit into corresponding holes in the portable's side face **1130** and a catch **1244** that engages the portable's latch **1120** (FIG. 11A). Thus, the portable **610** (FIGS. 11A-B) is docked by first attaching it at one end to the pivots **1242**, then rotating it about the pivots **1242** into the compartment **1220**, where it is latched in place on the catch **1244**. The portable **610** (FIGS. 11A-B) is undocked in reverse order, by first pressing the latch **1120** (FIG. 11A), which releases the portable from the catch **1244**, rotating the portable **610** (FIGS. 11A-B) about the pivots **1242** out of the compartment **1220** and then removing it from the pivots **1242**. As the portable is rotated into the compartment, the docking station plug **972** inserts into the portable socket **763** (FIG. 1B), providing the electrical interface between the portable **610** and the docking station **660**. The status indicators **982** are as described above with respect to FIG. 9.

[0090] FIG. 12B depicts the back side **1260** of the docking station **660**. The back side **1260** has a serial (RS-232 or USB) connector **962**, an analog output and nurse call connector **964**, an upgrade port connector **966**, an AC power plug **968**, an on/off switch **969** and a ground lug **1162**. A handle **1180** is provided at one end and fan vents **1170** are provided at the opposite end. A pair of feet **1190** are visible near the back side **1260**. A corresponding pair of feet (not visible) are located near the front side **1210** (FIG. 12A). The feet near the front side **1210** extend so as to tilt the front side **1210** (FIG. 12A) upward, making the display **740** (FIG. 13) of a docked portable **610** (FIG. 13) easier to read.

[0091] FIG. 13 illustrates both the portable **610** and the docking station **660**. The portable **610** and docking station **660** constitute three distinct pulse oximetry instruments. First, the portable **610** by itself, as depicted in FIGS. 11A-B, is a handheld pulse oximeter applicable to various patient monitoring tasks requiring battery power or significant mobility, such as ambulance and ER situations. Second, the portable **610** docked in the docking station **660**, as depicted in FIG. 13, is a standalone pulse oximeter applicable to a wide-range of typical patient monitoring situations from hospital room to the operating room. Third, the portable **610** docked and the upgrade port **966** (FIG. 12B) connected with an interface cable to the sensor port of a conventional pulse oximeter module **260** (FIG. 2) within a multiparameter patient monitoring instrument **250** (FIG. 2) or other conventional pulse oximeter, is a universal/upgrading pulse oximeter (UPO) instrument **210**, as described herein. Thus, the portable **610** and docking station **660** configuration of the UPO **210** advantageously provides a three-in-one pulse oximetry instrument functionality.

[0092] Another embodiment of the docking station **660** incorporates an input port that connects to a blood pressure sensor and an output port that connects to the blood pressure sensor port of a multiparameter patient monitoring system (MPMS). The docking station **660** incorporates a signal processor that computes a blood pressure measurement based upon an input from the blood pressure sensor. The docking station **660** also incorporates a waveform generator connected to the output port that produces a synthesized waveform based upon the computed measurement. The waveform generator output is adjustable so that the blood pressure value displayed on the MPMS is equivalent to the computed blood pressure measurement. Further, when the portable **610** is docked in the docking station **660** and the blood pressure sensor is connected to the input port, the portable displays a blood pressure value according to the computed blood pressure measurement. Thus, in this embodiment, the docking station **660** provides universal/upgrading capability for both blood pressure and SpO_2 .

[0093] Likewise, the docking station **660** can function as an universal/upgrading instrument for other vital sign measurements, such as respiratory rate, EKG or EEG. For this embodiment, the docking station **660** incorporates related sensor connectors and associated sensor signal processors and upgrade connectors to an MPMS or standalone instrument. In this manner, a variety of vital sign measurements can be incorporated into the docking station **660**, either individually or in combination, with or without SpO_2 as a measurement parameter, and with or without the portable **610**. In yet another embodiment, the docking station **660** can be configured as a simple SpO_2 upgrade box, incorporating

a SpO₂ processor and patient cable connector for an SpO₂ sensor that functions with or without the portable 610.

[0094] Unlike a conventional standalone pulse oximeter, the standalone configuration shown in FIG. 13 has a rotatable display 740 that allows the instrument to be operated in either a vertical or horizontal orientation. A tilt sensor 950 (FIG. 9) indicates when the bottom face 1310 is placed along a horizontal surface or is otherwise horizontally-oriented. In this horizontal orientation, the display 740 appears in landscape mode (FIG. 8C). The tilt sensor 950 (FIG. 9) also indicates when the side face 1320 is placed along a horizontal surface or is otherwise horizontally oriented. In this vertical orientation, the display 740 appears in portrait mode (FIG. 8B). A soft key 870 on the portable 610 can override the tilt sensor, allowing the display to be presented at any 90° orientation, i.e. portrait, landscape, “upside-down” portrait or “upside-down” landscape orientations. The handheld configuration (FIG. 11A), can also present the display 740 at any 90° orientation using a soft key 870. In the particular embodiment described above, however, the portable 610 does not have a separate tilt sensor and, hence, relies on a soft key 870 to change the orientation of the display when not docked.

[0095] FIG. 14 illustrates the docking station 660 incorporated within a local area network (LAN). The LAN shown is Ethernet-based 1460, using a central LAN server 1420 to interconnect various LAN clients 1430 and other system resources such as printers and storage (not shown). In this embodiment, an Ethernet controller module 1410 is incorporated with the docking station 660. The controller module 1410 can be incorporated within the docking station 660 housing or constructed as an external unit. In this manner, the UPO, according to the present invention, can communicate with other devices on the LAN or over the Internet 1490.

[0096] The Ethernet controller module 1410 can be embedded with web server firmware, such as the Hewlett-Packard (HP) BFOOT-10501. The module 1410 has both a 10 Base-T Ethernet interface for connection to the Ethernet 1460 and a serial interface, such as RS-232 or USB, for connection to the docking station 660. The module firmware incorporates HTTP and TCP/IP protocols for standard communications over the World Wide Web. The firmware also incorporates a micro web server that allows custom web pages to be served to remote clients over the Internet, for example. Custom C++ programming allows expanded capabilities such as data reduction, event detection and dynamic web page configuration.

[0097] As shown in FIG. 14, there are many applications for the docking station 660 to Ethernet interface. Multiple UPOs can be connected to a hospital's LAN, and a computer on the LAN could be utilized to upload pulse rate and saturation data from the various UPOs, displaying the results. Thus, this Ethernet interface could be used to implement a central pulse oximetry monitoring station within a hospital. Further, multiple UPOs from anywhere in the world can be monitored from a central location via the Internet. Each UPO is addressable as an individual web site and downloads web pages viewable on a standard browser, the web pages displaying oxygen saturation, pulse rate and related physiological measurements from the UPO. This feature allows a caregiver to monitor a patient regardless of

where the patient or caregiver is located. For example a caregiver located at home in one city or at a particular hospital could download measurements from a patient located at home in a different city or at the same or a different hospital. Other applications include troubleshooting newly installed UPOs or uploading software patches or upgrades to UPOs via the Internet. In addition alarms could be forwarded to the URL of the clinician monitoring the patient.

[0098] The UPO may have other configurations besides the handheld unit described in connection with FIG. 5 or the portable 610 and docking station 660 combination described in connection with FIGS. 11-13. The UPO may be a module, with or without a display, that can be removably fastened to a patient via an arm strap, necklace or similar means. In a smaller embodiment, this UPO module may be integrated into a cable or connector used for attaching a sensor to a pulse oximeter. The UPO may also be a circuit card or module that can externally or internally plug into or mate with a standalone pulse oximeter or multiparameter patient monitoring system. Alternatively, the UPO may be configured as a simple standalone upgrade instrument.

[0099] FIG. 15 illustrates a UPO configuration utilizing a patient care bed 1500. The bed 1500 includes a bed frame and mattress 1502, lower rails 1506 and upper rails 1508. One of the upper rails 1508 incorporates an instrument panel 1510 and the docking station 1540 is incorporated into the instrument panel 1510 according to the present invention. The instrument panel 1510 typically has keypad controls 1520, a display 1530, and a power supply 1550. The power supply 1550 has a power cord 1552 that plugs into an AC power source. The docking station 1540 includes a docking station compartment that accepts and electrically connects to the portable 610. In this manner, UPO can monitor a patient as a portable 610 during transport and then dock at the patient's destination as an integral part of the bedside instrument panel 1510.

[0100] FIG. 16 is block diagram of the instrument panel 1510 and incorporated docking station 1540. The instrument panel 1510 has a processor 1694, which, in conjunction with a display driver 1696 and a keypad interface 1697, drives the display 1530 and receives commands from the keypad controls 1520. The processor 1694 also communicates with a docked portable 610 (FIG. 6) via the docking station interface 1691 and a portable connector 1610 within the docking station receptacle. In one embodiment, the docking station 1540 simply provides a communications path and a DC power path between the docked portable 610 (FIG. 6) and the instrument panel 1510 via the portable connector 1610 and the docking station interface 1690. In that embodiment, the portable management processor 720 (FIG. 7) is programmed with the communications protocol of the instrument panel processor 1694. In another embodiment, the docking station 1540 provides communications and upgrade capability in a manner similar to that shown in FIG. 9. In that embodiment, the bed-integrated UPO could also connect to and upgrade a MPMS pulse oximeter module 260 (FIG. 2) or other external pulse oximeter located near the patient bed 1500, in a manner as described with respect to FIG. 2, above.

[0101] Although a universal/upgrading apparatus and method have been mainly described in terms of a pulse

oximetry measurement embodiment, the present invention is equally applicable to other physiological measurement parameters such as blood pressure, respiration rate, EEG, ECG and EtCO₂ (capnography) to name a few. In addition, a universal/upgrading instrument having a single physiological measurement parameter or a multiple measurement parameter capability and configured as a handheld, standalone, portable, docking station, module, plug-in, circuit card, to name a few, is also within the scope of the present invention.

[0102] FIGS. 17A-B illustrate one embodiment of a dual-mode pulse oximeter module according to the present invention. As shown in FIG. 17A, a dual-mode pulse oximeter module 1700 is contained within a case 1710 having dimensions that conform to a multiparameter patient monitoring system (MPMS) slot 290 (FIG. 2). The dual-mode module 1700 has a display 1720, a keypad 1730, and a patient cable connector 1740. A module connector 1750 (FIG. 17B) mates and electrically connects with a corresponding backplane connector (not shown) within an MPMS slot 292 (FIG. 2).

[0103] In reference to FIGS. 17A-B, the dual-mode pulse oximeter module 1700 has a portable mode, separate from MPMS 250 (FIG. 2), and an integrated mode, plugged into an MPMS slot 292 (FIG. 2). In the portable mode, the pulse oximeter module 1700 functions as a handheld or standalone pulse oximeter, in a manner similar to that described with respect to FIG. 6, above. Specifically, the portable module 1700 is a battery-powered, pulse oximeter instrument. The portable module 1700 connects to a sensor through a patient cable attached to the patient cable connector 1740. The module 1700 provides the sensor with a drive signal that alternately activates the sensor's red and IR LEDs, as is well-known in the art. The pulse oximeter module 1700 also receives a corresponding photo-plethysmographic detector signal from the sensor, also well-known in the art. The portable module 1700 processes this sensor signal to derive oxygen saturation and pulse rate measurements. In the portable mode, this information is provided on the module display 1720, and a keypad 1730 provides a user interface for operational control of the portable module 1700.

[0104] Also in reference to FIGS. 17A-B, in the integrated mode, the pulse oximeter module 1700 is a plug-in module that functions in conjunction with the MPMS 250 (FIG. 2). When installed in a MPMS slot 290 (FIG. 2), the integrated module 1700 receives power from the MPMS 250 (FIG. 2), drives a sensor, receives a corresponding photo-plethysmographic sensor signal, and processes this sensor signal to derive oxygen saturation and pulse rate measurements, as described with respect to the portable mode, above. The integrated module 1700, however, communicates oxygen saturation, pulse rate and related measurements to the MPMS 250 (FIG. 2) via the module connector 1750. Typically, the integrated module display 1720 and keypad 1730 are disabled, and the MPMS monitor 280 (FIG. 2) displays the physiological measurements made by the integrated module 1700.

[0105] FIG. 18 is a block diagram of the dual-mode pulse oximeter module 1700. The pulse oximeter module 1700 includes a pulse oximeter processor 1810, management processor 1820, power supply 1830, power manager 1840, keypad interface 1850, speaker driver 1860, display driver 1870, clock 1802, watch dog timer 1804, and MPMS

interface 1880. These components function in a manner similar to that described with respect to FIG. 7, above. Specifically, the pulse oximeter processor 1810 functions as an internal pulse oximeter, interfacing the pulse oximeter module 1700 to a sensor and deriving oxygen saturation, pulse rate, a plethysmograph and a pulse indicator.

[0106] As shown in FIG. 18, the management processor 1820 controls the various functions of the pulse oximeter module 1700, including data communications with the pulse oximeter processor 1810 and communications with the MPMS 250 via the MPMS interface 1880. The physical connection to the MPMS 250 is via the module connector 1750 (FIG. 17B) and a corresponding MPMS backplane connector. The electrical connection is via a module interface 1898. The management processor 1820 utilizes a real-time clock 1802 to keep the current date and time, which includes time and date information that is stored in non-volatile memory 1806 along with oxygen saturation related parameters to create trend data. The management processor 1820 also controls a user interface by transferring data to a display driver 1870 and from a keypad interface 1850. The management processor 1820 generates various alarm signals, which control a speaker driver 1860. The management processor 1820 also monitors system status, which includes battery status, indicating battery levels, and plug-in status, indicating whether the pulse oximeter module 1700 is connected to the MPMS 250. Another task of the management processor 1820 includes maintenance of a watchdog function. A watchdog 1804 monitors processor status on the watchdog data input and asserts a management processor reset if a fault is detected, along with audible and visual alarms.

[0107] Also shown in FIG. 18, the pulse oximeter module 1700 gets its power from batteries in the power supply 1830 or from power supplied on line 1884 from the MPMS 250 via the MPMS interface 1880. A power manager 1840 monitors the keypad on/off switch via the keypad interface 1850 and turns-on module power 1830 accordingly. The power manager 1840 turns off module power 1830 on command by the management processor 1820. DC/DC converters within the power supply 1830 generate the required voltages for module operation. A battery charger within the module power supply 1830 provides charging current to recharge the internal batteries. A non-volatile memory 1806 is connected to the management processor 1820 and used to store boot data, alarm limits trend data and program data.

[0108] FIG. 19 illustrates another embodiment of a dual-mode pulse oximeter according to the present invention. A docking station module 1900 has a docking portion 1910 and a plug-in portion 1920. The docking portion 1910 has a docking compartment 1930 and a portable socket 1940. The docking compartment 1930 is configured to accept and retain a portable pulse oximeter 610, such as described with respect to FIGS. 6 and 11A-B, above. In particular, the portable 610 has a socket 763 (FIG. 11B) that mates with a corresponding plug 1940, providing an electrical connection between the portable pulse oximeter 610 and the docking station module 1900. The plug-in portion 1920 has dimensions that conform to an MPMS slot 290 (FIG. 2). A module connector similar to that of the pulse oximeter module connector 1750 (FIG. 17B) mates and electrically connects

with a corresponding backplane connector (not shown) within an MPMS slot 290 (FIG. 2).

[0109] In reference to FIG. 19, the docking station module 1900 allows the portable 610 to function as a dual-mode pulse oximeter. That is, the portable 610 has a portable mode separate from the MPMS 250 (FIG. 2) and an integrated mode connected to an MPMS slot 290 (FIG. 2) via the docking station module 1900. In this manner, the portable 610 functions much as the dual-mode module 1700 (FIGS. 17A-B) described with respect to FIGS. 17A-B, above. In the portable mode, the portable 610 functions as a handheld or standalone pulse oximeter as described with respect to FIG. 6, above. In the integrated mode, the portable 610 is docked to the docking station module 1900 and functions in conjunction with the MPMS 250 (FIG. 2). When installed in an MPMS slot 290 (FIG. 2), the portable receives power from a MPMS 250 (FIG. 2), drives a sensor, receives a corresponding photo-plethysmographic sensor signal, and processes this sensor signal to derive oxygen saturation and pulse rate measurements, as described with respect to FIG. 6, above. The integrated portable 610, however, communicates oxygen saturation, pulse rate and related measurements to the MPMS 250 (FIG. 2) via the docking station module 1900, as described below. Typically, the portable display 740 and keys 750 are disabled, and the MPMS monitor 280 (FIG. 2) controls and displays the physiological measurements made by the integrated portable 610.

[0110] Also in reference to FIG. 19, in an alternative embodiment, the docking compartment 1930 is configured to accept and retain a pulse oximeter module 1700 (FIGS. 17A-B). In that embodiment, the docking compartment 1930 has a docking connector (not shown) that mates with the module connector 1750 (FIG. 17B), providing an electrical connection between the pulse oximeter module 1700 (FIGS. 17A-B) and the docking station module 1900.

[0111] FIG. 20 illustrates the docking station module 1900 attached to the MPMS 250. The plug-in portion 1920 (FIG. 19) plugs into at least one of the MPMS slots 290 (FIG. 2) and electrically connects to the MPMS backplane as described with respect to FIG. 19, above. In the portable mode (shown), the portable pulse oximeter 610 functions in a manner similar to the portable module 1700 (FIGS. 17A-B), i.e. as handheld or standalone pulse oximeter. In the integrated mode, the portable 610 is installed into the docking compartment 1930, providing an electrical connection and communications interface between the MPMS 250 and the portable pulse oximeter 610. In the integrated mode, the combination of the portable pulse oximeter 610 and the docking station module 1900 functions in a manner similar to the integrated module 1700 (FIGS. 17A-B).

[0112] FIG. 21 is a block diagram of a pass-through embodiment of a docking station module 1900, which includes a portable connector 2110, an MPMS connector 2160 and a direct electrical path between the two connectors 2110, 2160. In this embodiment, the docking station module 1900 simply provides a physical interface between the portable 610 (FIG. 20) and the MPMS 250. A MPMS communications path 1882 is directly routed to the portable communications path 2112. MPMS power 1884 is also directly routed to the portable input power line 2114. The docking station module 1900, with various configurations of the plug-in portion 1920 (FIG. 19) and associated module

connector can be adapted to the slots 290 (FIG. 2) of various MPMS manufacturers. In this manner, the docking station module 1900 can function as a universal interface between the portable pulse oximeter 610 or, alternatively, the pulse oximeter module 1700 and various multiparameter patient monitoring systems.

[0113] FIG. 22 is a block diagram of another embodiment of a docking station module 1900a, which includes a portable interface 2210, docking station processor 2220, power supply 2230 and monitor interface 2260. These components function in a manner similar to that described with respect to FIG. 9, above. Specifically, the docking station processor 2220 orchestrates the activity of the docking station module 1900. The processor 2220 provides synchronous serial data for communications with the portable 610 (FIG. 6) and sends watchdog messages to the portable processor 720 (FIG. 7) as part of the synchronous serial data to ensure the correct operation of the docking station processor 2220. The docking station processor 2220 accesses non-volatile, re-programmable memory 2206 over a high-speed bus to obtain program data for the processor 2220. In one embodiment, the status display 2240 is a set of LEDs on the front of the docking station module 1900 used to indicate various conditions including portable docked, portable battery charging and alarm. The portable interface 2210 interconnects with the docking station interface 760 (FIG. 7) of the portable 610 (FIG. 6). External power 1884 is provided to the docking station module 1900a from the MPMS 250. The docking station power supply 2230 charges the battery in the portable power supply 730 (FIG. 7). When the portable 610 (FIG. 6) is either removed or turned off, the docking station power 2232 is removed and the docking station 1900 is turned off, except for the battery charger portion of the power supply 2230. The docking station power 2232 and, hence, the docking station 1900 turns on whenever a docked portable 610 (FIG. 6) is turned on.

[0114] Although the dual-mode physiological measuring apparatus and method of the present invention is described in detail with respect to pulse oximetry measurements, one of ordinary skill in the art will recognize that a dual-mode MPMS plug-in module or a portable apparatus that docks to a MPMS plug-in docking station module could incorporate physiological measurement capabilities other than or in addition to pulse oximetry, such as blood pressure, respiration rate, EEG, ECG and EtCO₂ (capnography) to name a few.

[0115] The dual-mode pulse oximeter has been disclosed in detail in connection with various embodiments of the present invention. These embodiments are disclosed by way of examples only and are not to limit the scope of the present invention, which is defined by the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications within the scope of this invention.

What is claimed is:

1. A physiological monitoring system including a portable physiological monitor and a docking station coupled to a patient bed, the physiological monitoring system comprising:

a portable physiological monitor including a first local display, the monitor capable of operating in a portable mode, said portable mode providing portable monitoring as a standalone patient monitor of one or more

physiological parameters of a patient through communication with one or more sensors, and capable of operating in a docked mode, said docked mode providing monitoring of one or more physiological parameters of a patient; and

a docking station including a second display, the docking station forming a patient monitoring system coupled to a patient bed, said docking station configured to mate with the portable physiological monitor when the monitor is operating in at least the docked mode, wherein the portable physiological measurement device is in communication with the docking station, and further wherein the docking station is in communication with the second local display.

2. The patient monitoring system of claim 1, wherein the one or more physiological parameters comprises blood oxygen saturation.

3. The patient monitoring system of claim 2, wherein the portable physiological monitor is capable of substantially accurately measuring blood oxygen saturation in the presence of motion induced noise.

4. The patient monitoring system of claim 1, wherein the docking station further comprises a management processor.

5. The patient monitoring system of claim 4, wherein the management processor generates an output usable by a second patient monitoring system in communication with the docking station to cause to be displayed at least one of the monitored one or more physiological parameters of the patient in an amount consistent with those displayed on the portable physiological monitor when the monitor is operating in at least the docked mode.

6. The patient monitoring system of claim 5, wherein the docking station communicates with the patient monitoring system by sending a sensor signal to the second patient monitoring system.

7. The patient monitoring system of claim 6, wherein the patient monitoring system communicates with a display device.

8. The patient monitoring system of claim 1, wherein the one or more physiological parameters comprises one or more of blood oxygen content, respiratory gas, blood pressure, ECG, and pulse rate.

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专利名称(译)	双模式脉搏血氧仪		
公开(公告)号	US20080039701A1	公开(公告)日	2008-02-14
申请号	US11/894722	申请日	2007-08-20
[标]申请(专利权)人(译)	梅西莫股份有限公司		
申请(专利权)人(译)	Masimo公司		
当前申请(专利权)人(译)	Masimo公司		
[标]发明人	ALI AMMAR AL CAROTHERS DON DALKE DAVID DIAB MOHAMED K GOLDMAN JULIAN KIANI MASSI E LEE MICHAEL NOVAK JEROME SMITH ROBERT VADEN VAL E		
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IPC分类号	A61B5/02 A61B5/00		
CPC分类号	A61B5/0002 A61B5/14551 A61B5/742 A61B2560/0271 A61B2560/0443 A61B5/7445 A61B5/0205 A61B5/021 A61B5/0402 A61B5/0476 A61B2560/0456		
优先权	60/117097 1999-01-25 US 60/161565 1999-10-26 US		
其他公开文献	US8532727		
外部链接	Espacenet USPTO		

摘要(译)

便携式独立式病人监护仪可与对接在病床上的对接站对接。便携式监视器被配置为在独立模式和对接模式下操作。扩展坞可包括第二本地监视器。

