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(54) CIRCUITS AND METHODS FOR ELECTROSURGICAL UNIT SIGNAL DETECTION

SCHALTUNGEN UND VERFAHREN ZUR DETEKTION VON SIGNALEN EINER ELEKTROCHIRURGISCHEN EINHEIT

CIRCUITS ET PROCÉDÉS DE DÉTECTION D'UN SIGNAL D'UNITÉ ÉLECTROCHIRURGICALE

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(56) References cited:
EP-A1- 2 674 125 US-A- 4 537 200
US-A1- 2009 018 429 US-B2- 6 985 833

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Description

TECHNICAL FIELD

[0001] The subject matter described herein relates generally to electric circuits, and, more specifically, to signal detection circuits.

BACKGROUND

[0002] Electrosurgical units (ESU) are routinely used in operating rooms and are known to interfere with the monitoring of patients' bio-potential signals (e.g. electrocardiogram signals, electroencephalography signals, blood pressure, etc.). An ESU applies a large amplitude (e.g., 100 V - 5 kV) and high frequency (>300 kHz) signal to a patient's body for operations. However, the ESU signal may also have energy at lower frequencies (e.g., from direct current to 100 Hz) because the high-frequency ESU signal amplitude is modulated due to cutting and subsequently rectified when a current passes through ESU electrodes. As a result, the lower frequency components of the ESU signal may generate noises in the pass band of bio-potential signals of interest. Such noise often produces false alarms (e.g., a high heart rate) in software algorithms that monitor the bio-potential signals.

[0003] US 2009/018429 discloses a method and apparatus that limits the effect of high frequency ("HF") interferences on acquired electro-physiological signals, such as the EEG and EMG. The method and apparatus comprise two separate electronic circuitries and steps or electronics for processing the signals. One circuit is used to block the transmission of HF interferences to the instrumentation amplifiers. The first circuit comprises a front-end active filter, a low frequency electromagnetic interference ("EMI") shield, and an isolation barrier interface which isolates the patient from earth ground. The second circuit measures the difference in potential between the two isolated sides of the isolation barrier. This "cross-barrier" voltage is directly representative of the interference level that the instrumentation amplifier is subjected to. The second circuit is used to confirm that the acquired signals are not corrupted by the interference.

[0004] US 4,537,200 discloses a technique of reducing the noise interference that is created by an electrosurgical instrument. The technique comprises utilizing a combination of adaptive noise cancelling and conventional signal processing. Some interference is eliminated by radio frequency shielding, passive and active lowpass filtering and optical isolation. A digital adaptive canceller using the least-mean-square algorithm is used to reduce the remainder of the interference.

SUMMARY

[0005] Circuits and methods are provided for detecting

an electrosurgical unit signal. An example circuit for detecting an electrosurgical unit signal includes: a filter configured to process a floating ground signal associated with measuring a bio-potential signal of a patient; and a detector configured to output a sensing signal based at least in part on the floating ground signal and an Earth ground for detecting an electrosurgical unit signal.

[0006] As an example, the filter includes: a capacitor; and a resistor including a first resistor terminal and a second resistor terminal, the first resistor terminal being electrically connected to the capacitor, the second resistor terminal being biased to the Earth ground. As another example, the capacitor includes a first capacitor terminal and a second capacitor terminal; the first capacitor terminal is configured to receive the floating ground signal; and the second capacitor terminal is electrically connected to the first resistor terminal.

[0007] For example, the detector includes: a diode including an anode terminal and a cathode terminal, the anode terminal being electrically connected to the filter; a capacitor including a first capacitor terminal and a second capacitor terminal, the first capacitor terminal being electrically connected to the cathode terminal, the second capacitor terminal being biased to the Earth ground; and a resistor including a first resistor terminal and a second resistor terminal, the first resistor terminal being electrically connected to the first capacitor terminal, the second resistor terminal being biased to the Earth ground.

[0008] In another example, the floating ground signal includes a high-frequency component and a low-frequency component; and the filter is configured to pass the high-frequency component and block the low-frequency component. In yet another example, the low-frequency component is associated with the bio-potential signal of the patient.

[0009] For example, the high-frequency component corresponds to a frequency value larger than a threshold; and the low-frequency component corresponds to a low frequency value smaller than the threshold. As another example, the detector is further configured to rectify the filtered floating ground signal to a direct current level.

[0010] In a specific example, the electrosurgical unit signal is detected when the direct current level is higher than a threshold. For example, a neutral drive amplifier is configured to receive the floating ground signal as an input. In one example, the detector includes a half-wave rectifier. In another example, the detector includes a full-wave rectifier. In yet another example, the detector includes a self-locked demodulator.

[0011] In a particular example, the circuit further includes: a signal processor configured to process the bio-potential signal according to an algorithm. As an example, the signal processor is further configured to change the algorithm based at least in part on the electrosurgical unit signal. In another example, the signal processor is further configured to change the algorithm linearly or non-linearly. For example, the bio-potential signal corresponds to an electrocardiogram signal. In another exam-

ple, the bio-potential signal corresponds to an electroencephalography signal. In a specific example, the filter and the detector are placed in an electrical isolation region where a monitor for the bio-potential signal is located.

[0012] An example method is provided for detecting an electrosurgical unit signal. The method includes: processing a floating ground signal associated with measuring a bio-potential signal of a patient; and outputting a sensing signal based at least in part on the floating grounding and the Earth ground for detecting an electrosurgical unit signal. For example, the method is implemented using the example circuit as described above.

[0013] The subject matter described herein provides many technical advantages. For example, the circuits described herein are inexpensive in that high-cost ADCs (analog to digital converters) for sampling MHz signals are not used. Also, the circuits described herein can be more reliable than software algorithms which often depend on complex nonlinear filtering at electrodes. Furthermore, voltages can be measured relative to a floating ground (not the Earth ground), and the circuitry described herein can be placed within the same electrical isolation region of a bio-potential monitoring circuitry, so as to greatly simplify circuit design.

[0014] The details of one or more variations of the subject matter described herein are set forth in the accompanying drawings and the description below. The invention is defined by appended claims 1-15.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015]

FIG. 1 depicts an example diagram for ESU signal detection.

FIG. 2 depicts an example diagram showing an ESU detection circuit.

FIG. 3 depicts an example diagram showing the ESU detection circuit for common mode sensing.

FIG. 4 depicts an example diagram showing the ESU detection circuit for differential sensing.

DETAILED DESCRIPTION

[0016] The interference of an ESU with bio-potential signal monitoring can be problematic. For example, false alarms may be produced when an ESU is in use, but alarm mechanisms may not be turned off to prevent such false alarms because the alarm mechanisms are still needed in between the use of the ESU. Software algorithms may be developed to detect an ESU in operation, but such algorithms may be inherently limited by the sampling rate of an ADC used for converting ESU signals to digital signals. Usually the sampling rate of the ADC is too low to detect high-frequency ESU signals which are often in the MHz range.

[0017] The systems and methods described herein can be configured to implement various mechanisms for

detecting whether an ESU is active. For example, the unique high frequency nature of ESU signals, usually separated from bio-potential signal related frequencies by more than two orders of magnitude, renders the high frequency ESU signals available for detection.

[0018] FIG. 1 depicts an example diagram for ESU signal detection. As shown in FIG. 1, a circuit 100 includes an ESU 102 and a bio-potential monitoring system 104. The circuit 100 can implement two ESU signal detection mechanisms: differential sensing and common mode sensing. For differential sensing, a sensing circuit (e.g., as shown in FIG. 2) can be connected between a bio-potential input terminal (e.g., point "A") and a floating ground 108 (e.g., point "B"), where the floating ground 108 corresponds to a floating ground signal and is used for measuring a bio-potential signal. For example, the floating ground 108 corresponds to a ground that is not electrically connected to the Earth ground 110, and the floating ground signal is a signal that is referenced to the floating ground 108. For common mode sensing, the sensing circuit can be connected between the floating ground 108 (e.g., point "C") and the Earth ground 110 (e.g., point "D").

[0019] Particularly, during the ESU operations, one or more ESU voltage components may be present on each bio-potential input signal (e.g., an electrocardiogram (ECG) signal), and the ESU voltage components may have some dynamic signal potential with respect to the floating ground 108. Thus, the ESU voltage components that indicate active ESU operations can be detected through differential sensing. Furthermore, during the ESU operations, the floating ground 108 can be floating at a common mode potential of the ESU 102, and may have a high level and a high frequency. The floating ground 108 can then be detected through common mode sensing.

[0020] Specifically, when the ESU 102 is activated, it has two output components: (1) a differential voltage 120 (e.g., V_{diff}) from a scalpel 122 to a return plate 132, and (2) a common mode voltage 124 (V_{cm}) on a patient body 126 with respect to the Earth ground 110. The differential voltage 120 (e.g., V_{diff}) represents the active "cutting" energy output for the ESU 102. For example, the differential voltage 120 is larger than $100 V_{p-p}$, and has a frequency value higher than 200 kHz. The common mode voltage 124 is a parasitic output that is generated (e.g., via a parasitic capacitance 128) because the ESU 102 is not perfectly isolated from the Earth.

[0021] The patient body 126 presents a differential load to the ESU 102. For example, the differential voltage 120 (e.g., V_{diff}) causes a current to flow through the body 126 which has internal resistance 134 (e.g., R_b). A right-leg electrode (RL) brings the body potential to the floating ground 108 through a neutral drive amplifier 106. The patient body 126 also presents a common mode impedance (e.g., 200 pF) to the Earth ground 110, which loads down the ESU common mode excitation. For example, the resulting common mode voltage 124 on the patient

is larger than $100 V_{p-p}$ at high frequencies.

[0022] An amplifier 136 for monitoring bio-potential signals is connected to the patient body 126 by placing electrodes at multiple physical locations. A voltage developed on any of the patient electrodes (e.g., left arm (LA), right arm (RA)) with respect to the floating ground 108 can be used to detect ESU operations. As shown in FIG. 1, the LA electrode is used as an example. For example, the voltage 112 on LA can be high-pass filtered and rectified to produce a direct-current (DC) output to indicate whether the ESU has been activated.

[0023] FIG. 2 depicts an example diagram showing an ESU detection circuit. As shown in FIG. 2, the ESU detection circuit 200 includes a high-pass filter for high-pass filtering a voltage signal 212 and a rectifying detector for rectifying the filtered signal to generate a DC output 214 (e.g., a sensing signal for detecting the ESU activities).

[0024] Specifically, the voltage signal 212 represents an ESU-related signal, e.g., the voltage 112 on LA, the floating ground 108, etc. The voltage signal 212 has a high level and a high frequency when the ESU 102 is activated. For example, the high-pass filter includes a capacitor 202 and a resistor 204, where a resistor terminal 220 of the resistor 204 is electrically connected to the capacitor 202. The rectifying detector includes a diode 206, a capacitor 208 and a resistor 210. As an example, a capacitor terminal 224 of the capacitor 208 is electrically connected to a resistor terminal 222 of the resistor 204. An anode terminal 226 of the diode 206 is electrically connected to the high-pass filter.

[0025] For example, the high-pass filter may pass signals that have a frequency value higher than 200 kHz, and blocks signals that have a frequency value lower than 2 kHz. The frequencies of the ESU signals are usually higher than 200 kHz, and the frequencies of the ECG signals are usually lower than 2 kHz. Thus, the high-pass filter can pass the ESU signals and block the ECG signals. It should be understood that the circuit 200 including the high pass filter and the rectifying detector as shown in FIG. 2 is merely an example, and can be varied in circuit design to meet other system requirements.

[0026] The DC output 214 can be monitored by subsequent circuitry (not shown). For example, if the ESU 102 is operating, the DC output 214 increases from 0 V to trigger action to modify bio-potential signal processing to reduce artifacts. Dynamic detection of the ESU operation can allow for implementation of automatic correction algorithms for bio-potential signals. As an example, the bio-potential monitoring system 104 includes a signal processor for processing the bio-potential signals using a signal processing algorithm. The signal processor may modify the signal processing algorithm according to the detection of the activities of the ESU 102 (e.g., an increase in the DC output 214). In one example, the signal processor changes the signal processing of the bio-potential signals linearly or non-linearly.

[0027] Other circuit designs may be implemented for the rectifying detector. For example, the rectifying detec-

tor can include a half-wave rectifier, a full-wave rectifier, and/or a self-clocked demodulator.

[0028] FIG. 3 depicts an example diagram showing the ESU detection circuit for common mode sensing. As shown in FIG. 3, the circuit 200 filters the floating ground 108 and rectifies the filtered signal to generate the DC output 214 for ESU detection, where the circuit 200 is biased to the Earth ground 110. During the ESU operations, the floating ground 108 has a high level (e.g., higher than a threshold) and a high frequency with respect to the Earth ground 110, and thus can be detected using the circuit 200.

[0029] FIG. 4 depicts an example diagram showing the ESU detection circuit for differential sensing. As shown in FIG. 4, the circuit 200 filters the voltage 112 on LA and rectifies the filtered signal to generate the DC output 214 for ESU detection, where the circuit 200 is biased to the floating ground 108. During the ESU operations, an ESU voltage component can be present on the voltage 112, and the ESU voltage component has a dynamic signal potential with respect to the floating ground 108. Thus, the ESU voltage component that indicates active ESU operations can be detected through differential sensing as shown in FIG. 4.

[0030] For example, the voltages described above can be measured relative to the floating ground 108 (not the Earth ground 110). The circuit 200 can be placed within a same electrical isolation region (e.g., a region electrically isolated from the Earth ground 110) as the bio-potential monitoring system 104, so as to greatly simplify circuit design.

[0031] One or more aspects or features of the subject matter described herein can be realized in digital electronic circuitry, integrated circuitry, specially designed application specific integrated circuits (ASICs), field programmable gate arrays (FPGAs) computer hardware, firmware, software, and/or combinations thereof. These various aspects or features can include implementation in one or more computer programs that are executable and/or interpretable on a programmable system including at least one programmable processor, which can be special or general purpose, coupled to receive data and instructions from, and to transmit data and instructions to, a storage system, at least one input device, and at least one output device.

[0032] In the descriptions above and in the claims, phrases such as "at least one of" or "one or more of" may occur followed by a conjunctive list of elements or features. The term "and/or" may also occur in a list of two or more elements or features. Unless otherwise implicitly or explicitly contradicted by the context in which it is used, such a phrase is intended to mean any of the listed elements or features individually or any of the recited elements or features in combination with any of the other recited elements or features. For example, the phrases "at least one of A and B;" "one or more of A and B;" and "A and/or B" are each intended to mean "A alone, B alone, or A and B together." A similar interpretation is also in-

tended for lists including three or more items. For example, the phrases "at least one of A, B, and C;" "one or more of A, B, and C;" and "A, B, and/or C" are each intended to mean "A alone, B alone, C alone, A and B together, A and C together, B and C together, or A and B and C together." In addition, use of the term "based on," above and in the claims is intended to mean, "based at least in part on," such that an unrecited feature or element is also permissible.

[0033] The subject matter described herein can be embodied in systems, apparatus, methods, and/or articles depending on the desired configuration. The implementations set forth in the foregoing description do not represent all implementations consistent with the subject matter described herein. Instead, they are merely some examples consistent with aspects related to the described subject matter. Although a few variations have been described in detail above, other modifications or additions are possible. The invention is defined by appended claims 1-15.

Claims

1. A circuit (100, 200) for detecting an electrosurgical unit signal, the circuit comprising:

a filter configured to process a floating ground signal associated with measuring a bio-potential signal of a patient (126); and
a detector configured to output a sensing signal (214) based at least in part on the floating ground signal and an Earth ground (110);

characterized in that:

the filter and the detector are placed in an electrical isolation region which is isolated from the Earth ground (110); and
a monitor for the electrosurgical unit signal is disposed within the electrical isolation region.

2. The circuit (100, 200) of claim 1, wherein the filter includes:

a capacitor (202); and
a resistor (204) including a first resistor terminal (220) and a second resistor terminal (222), the first resistor terminal (220) being electrically connected to the capacitor (202), the second resistor terminal (222) being biased to the Earth ground (110).

3. The circuit (100, 200) of claim 2, wherein:

the capacitor (202) includes a first capacitor terminal and a second capacitor terminal;
the first capacitor terminal is configured to re-

ceive the floating ground signal; and
the second capacitor terminal is electrically connected to the first resistor terminal (220).

4. The circuit (100, 200) as in any one of the preceding claims, wherein the detector includes:

a diode (206) including an anode terminal (226) and a cathode terminal, the anode terminal (226) being electrically connected to the filter;
a capacitor (208) including a first capacitor terminal and a second capacitor terminal (224), the first capacitor terminal being electrically connected to the cathode terminal, the second capacitor terminal (224) being biased to the Earth ground (110); and
a resistor (210) including a first resistor terminal and a second resistor terminal, the first resistor terminal being electrically connected to the first capacitor terminal, the second resistor terminal being biased to the Earth ground (110).

5. The circuit (100, 200) as in any one of the preceding claims, wherein:

the floating ground signal includes a high-frequency component and a low-frequency component; and
the filter is configured to pass the high-frequency component and block the low-frequency component.

6. The circuit (100, 200) as in claim 5, wherein the low-frequency component is associated with the bio-potential signal of the patient (126).

7. The circuit as in claim 5 or 6, wherein:

the high-frequency component corresponds to a frequency value larger than a threshold; and
the low-frequency component corresponds to a low frequency value smaller than the threshold.

8. The circuit (100, 200) as in any one of the preceding claims, wherein the detector is further configured to rectify the filtered floating ground signal to a direct current level, optionally wherein the electrosurgical unit signal is detected when the direct current level is higher than a threshold.

9. The circuit (100, 200) as in any one of the preceding claims, wherein a neutral drive amplifier is configured to receive the floating ground signal as an input.

10. The circuit (100, 200) as in any one of the preceding claims, wherein the detector includes a half-wave rectifier, a full-wave rectifier, and/or a self-clocked demodulator.

11. The circuit (100, 200) as in any one of the preceding claims, further comprising:
a signal processor configured to process the bio-potential signal according to an algorithm.
12. The circuit (100, 200) as in claim 11, wherein the signal processor is further configured to change the algorithm: a) based at least in part on the electrosurgical unit signal and/or b) linearly or non-linearly.
13. The circuit (100, 200) as in any one of the preceding claims, wherein the bio-potential signal corresponds to an electrocardiogram signal and/or an electroencephalography signal.
14. A method for detecting an electrosurgical unit signal, the method comprising:
- processing, with a filter, a floating ground signal associated with measuring a bio-potential signal of a patient (126);
and outputting, with a detector, a sensing signal (214) based at least in part on the floating grounding and the Earth ground (110)
characterized in that the filter and the detector are placed in an electrical isolation region which is isolated from the Earth ground (110); and
a monitor for the electrosurgical unit signal is disposed within the electrical isolation region.
15. The method of claim 14, wherein the method is implemented using a circuit (100, 200) as in any of claims 1-13.

Patentansprüche

1. Schaltung (100, 200) zum Detektieren eines Signals einer Elektrochirurgieeinheit, wobei die Schaltung Folgendes umfasst:
- ein Filter, das ausgelegt ist zum Verarbeiten eines Massesignals, das mit dem Messen eines Biopotentialsignals eines Patienten (126) verknüpft ist; und
einen Detektor, der ausgelegt ist zum Ausgeben eines Erfassungssignals (214), das zumindest teilweise auf dem Massesignal und einer Erde (110) basiert;
dadurch gekennzeichnet, dass:
- das Filter und der Detektor in einem elektrisch isolierten Bereich platziert sind, der gegenüber Erde (110) isoliert ist; und
ein Monitor für das Signal der Elektrochirurgieeinheit innerhalb des elektrisch isolierten Bereichs angeordnet ist.

2. Schaltung (100, 200) nach Anspruch 1, wobei das Filter Folgendes beinhaltet:
- einen Kondensator (202); und
einen Widerstand (204), der einen ersten Widerstandsanschluss (220) und einen zweiten Widerstandsanschluss (222) aufweist, wobei der erste Widerstandsanschluss (220) elektrisch mit dem Kondensator (202) verbunden ist, wobei der zweite Widerstandsanschluss (222) auf Erde (110) gelegt ist.
3. Schaltung (100, 200) nach Anspruch 2, wobei:
- der Kondensator (202) einen ersten Kondensatoranschluss und einen zweiten Kondensatoranschluss aufweist;
der erste Kondensatoranschluss ausgelegt ist zum Aufnehmen des Massesignals; und
der zweite Kondensatoranschluss elektrisch mit dem ersten Widerstandsanschluss (220) verbunden ist.
4. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei der Detektor Folgendes beinhaltet:
- eine Diode (206), die einen Anodenanschluss (226) und einen Kathodenanschluss aufweist, wobei der Anodenanschluss (226) elektrisch mit dem Filter verbunden ist;
einen Kondensator (208), der einen ersten Kondensatoranschluss und einen zweiten Kondensatoranschluss (224) aufweist, wobei der erste Kondensatoranschluss elektrisch mit dem Kathodenanschluss verbunden ist, wobei der zweite Kondensatoranschluss (224) mit Erde (110) verbunden ist; und
einen Widerstand (210), der einen ersten Widerstandsanschluss und einen zweiten Widerstandsanschluss aufweist, wobei der erste Widerstandsanschluss elektrisch mit dem ersten Kondensatoranschluss verbunden ist, wobei der zweite Widerstandsanschluss auf Erde (110) gelegt ist.
5. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei:
- das Massesignal eine Hochfrequenzkomponente und eine Niederfrequenzkomponente aufweist; und
das Filter ausgelegt ist zum Durchleiten der Hochfrequenzkomponente und zum Sperren der Niederfrequenzkomponente.
6. Schaltung (100, 200) nach Anspruch 5, wobei die Niederfrequenzkomponente mit dem Biopotential

des Patienten (126) verknüpft ist.

7. Schaltung nach Anspruch 5 oder 6, wobei:

die Hochfrequenzkomponente einem Frequenzwert entspricht, der größer als eine Schwelle ist; und

die Niederfrequenzkomponente einem Niederfrequenzwert entspricht, der kleiner als die Schwelle ist.

8. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei der Detektor ferner ausgelegt ist zum Gleichrichten des gefilterten Massesignals auf einen Gleichstrompegel, wobei optional das Signal der Elektrochirurgieeinheit detektiert wird, wenn der Gleichstrompegel höher als eine Schwelle liegt.

9. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei ein Neutralverstärker ausgelegt ist zum Empfangen des Massesignals als eine Eingabe.

10. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei der Detektor einen Halbwellengleichrichter, einen Vollwellengleichrichter und/oder einen selbstgetakteten Demodulator beinhaltet.

11. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, ferner umfassend: einen Signalprozessor, der ausgelegt ist zum Verarbeiten des Biopotentialsignals gemäß einem Algorithmus.

12. Schaltung (100, 200) nach Anspruch 11, wobei der Signalprozessor ferner ausgelegt ist zum Ändern des Algorithmus: a) zumindest teilweise basierend auf dem Signal der Elektrochirurgieeinheit und/oder b) linear oder nichtlinear.

13. Schaltung (100, 200) nach einem der vorhergehenden Ansprüche, wobei das Biopotentialsignal einem Elektrokardiogrammsignal und/oder einem Elektroenzephalographiesignal entspricht.

14. Verfahren zum Detektieren eines Signals einer Elektrochirurgieeinheit, wobei das Verfahren Folgendes umfasst:

Verarbeiten, mit einem Filter, eines Massesignals, das mit dem Messen eines Biopotentialsignals eines Patienten (126) verknüpft ist; und Ausgeben, mit einem Detektor, eines Erfassungssignals (214), das zumindest teilweise auf dem Massesignal und der Erde (110) basiert; **dadurch gekennzeichnet, dass:**

das Filter und der Detektor in einem elektrisch isolierten Bereich platziert sind, der gegenüber der Erde (110) isoliert ist; und ein Monitor für das Signal der Elektrochirurgieeinheit innerhalb des elektrisch isolierten Bereichs angeordnet ist.

15. Verfahren nach Anspruch 14, wobei das Verfahren unter Verwendung einer Schaltung (100, 200) nach einem der Ansprüche 1-13 implementiert wird.

Revendications

1. Circuit (100, 200) de détection d'un signal d'unité électrochirurgicale, le circuit comprenant :

un filtre configuré pour traiter un signal de masse flottante associé à la mesure d'un signal de potentiel biologique d'un patient (126) ; et un détecteur configuré pour émettre un signal de détection (214) sur la base au moins en partie du signal de masse flottante et d'une mise à la terre (110) ;

caractérisé en ce que :

le filtre et le détecteur sont placés dans une région d'isolation électrique qui est isolée par rapport à la mise à la terre (110) ; et un moniteur pour le signal d'unité électrochirurgicale est disposé à l'intérieur de la région d'isolation électrique.

2. Circuit (100, 200) selon la revendication 1, le filtre comprenant :

un condensateur (202) ; et une résistance (204) comprenant une première borne de résistance (220) et une seconde borne de résistance (222), la première borne de résistance (220) étant connectée électriquement au condensateur (202), la seconde borne de résistance (222) étant sollicitée vers la mise à la terre (110).

3. Circuit (100, 200) selon la revendication 2 :

le condensateur (202) comprenant une première borne de condensateur et une seconde borne de condensateur ; la première borne de condensateur étant configurée pour recevoir le signal de masse flottante ; et la seconde borne de condensateur étant connectée électriquement à la première borne de résistance (220).

4. Circuit (100, 200) selon l'une quelconque des reven-

- dications précédentes, le détecteur comprenant :
- une diode (206) comprenant une borne d'anode (226) et une borne de cathode, la borne d'anode (226) étant connectée électriquement au filtre ; un condensateur (208) comprenant une première borne de condensateur et une seconde borne de condensateur (224), la première borne de condensateur étant connectée électriquement à la borne de cathode, la seconde borne de condensateur (224) étant sollicitée vers la mise à la terre (110) ; et une résistance (210) comprenant une première borne de résistance et une seconde borne de résistance, la première borne de résistance étant connectée électriquement à la première borne de condensateur, la seconde borne de résistance étant sollicitée vers la mise à la terre (110).
5. Circuit (100, 200) selon l'une quelconque des revendications précédentes, le signal de masse flottante comprenant une composante haute fréquence et une composante basse fréquence ; et le filtre étant configuré pour laisser passer la composante haute fréquence et bloquer la composante basse fréquence.
 6. Circuit (100, 200) selon la revendication 5, la composante basse fréquence étant associée au signal de potentiel biologique du patient (126).
 7. Circuit selon la revendication 5 ou 6, la composante haute fréquence correspondant à une valeur de fréquence supérieure à un seuil ; et la composante basse fréquence correspondant à une valeur de basse fréquence inférieure au seuil.
 8. Circuit (100, 200) selon l'une quelconque des revendications précédentes, le détecteur étant en outre configuré pour redresser le signal de masse flottante filtré vers un niveau de courant continu, le signal d'unité électrochirurgicale étant éventuellement détecté lorsque le niveau de courant continu est supérieur à un seuil.
 9. Circuit (100, 200) selon l'une quelconque des revendications précédentes, un amplificateur de commande neutre étant configuré pour recevoir le signal de masse flottante en tant qu'entrée.
 10. Circuit (100, 200) selon l'une quelconque des revendications précédentes, le détecteur comprenant un redresseur demi-onde, un redresseur pleine onde, et/ou un démodulateur autosynchronisé.
 11. Circuit (100, 200) selon l'une quelconque des revendications précédentes, comprenant en outre : un processeur de signal configuré pour traiter le signal de potentiel biologique selon un algorithme.
 12. Circuit (100, 200) selon la revendication 11, le processeur de signal étant en outre configuré pour modifier l'algorithme : a) sur la base au moins en partie du signal d'unité électrochirurgicale et/ou b) de manière linéaire ou de manière non linéaire.
 13. Circuit (100, 200) selon l'une quelconque des revendications précédentes, le signal de potentiel biologique correspondant à un signal d'électrocardiogramme et/ou à un signal d'électroencéphalographie.
 14. Procédé de détection d'un signal d'unité électrochirurgicale, le procédé comprenant : le traitement, avec un filtre, d'un signal de masse flottante associé à la mesure d'un signal de potentiel biologique d'un patient (126) ; et l'émission, avec un détecteur, d'un signal de détection (214) sur la base au moins en partie de la masse flottante et de la mise à la terre (110) **caractérisé en ce que** le filtre et le détecteur sont placés dans une région d'isolation électrique qui est isolée par rapport à la mise à la terre (110), et un moniteur pour le signal d'unité électrochirurgicale est disposé à l'intérieur de la région d'isolation électrique.
 15. Procédé selon la revendication 14, le procédé étant mis en œuvre en utilisant un circuit (100, 200) selon l'une quelconque des revendications 1 à 13.

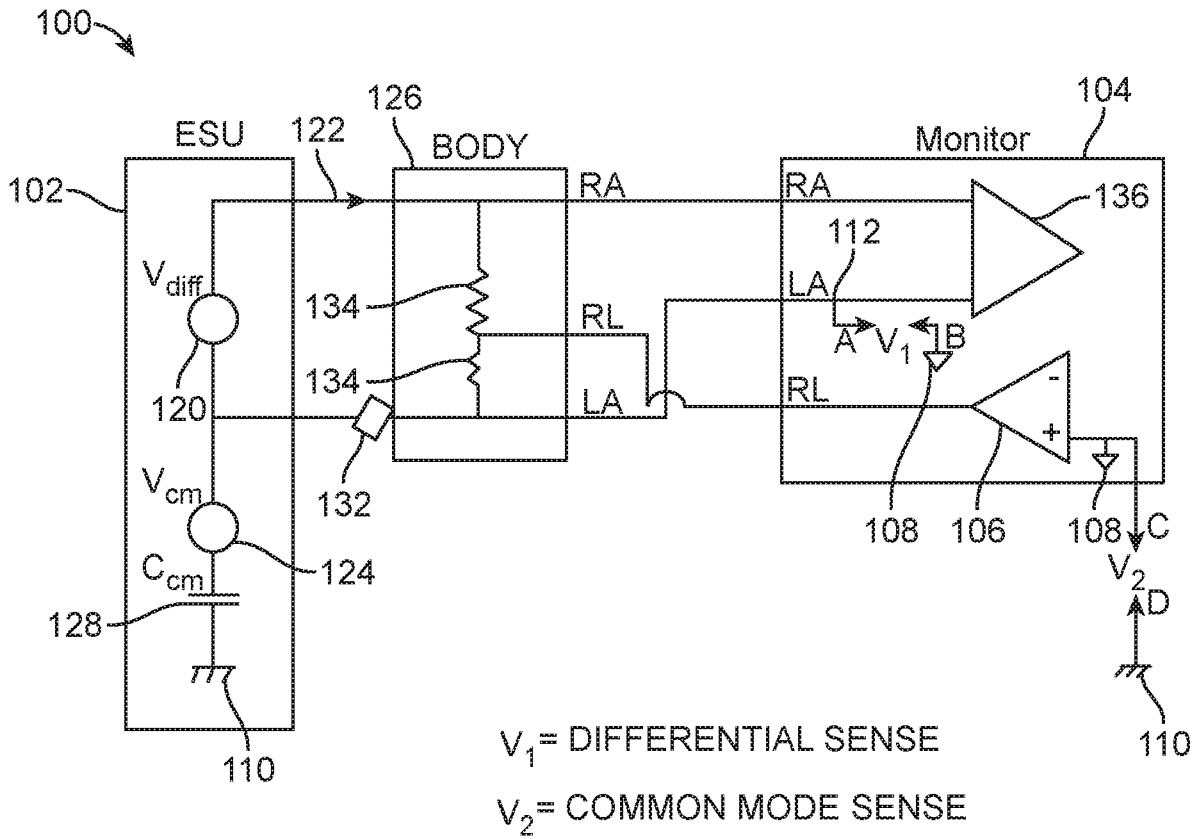


FIG. 1

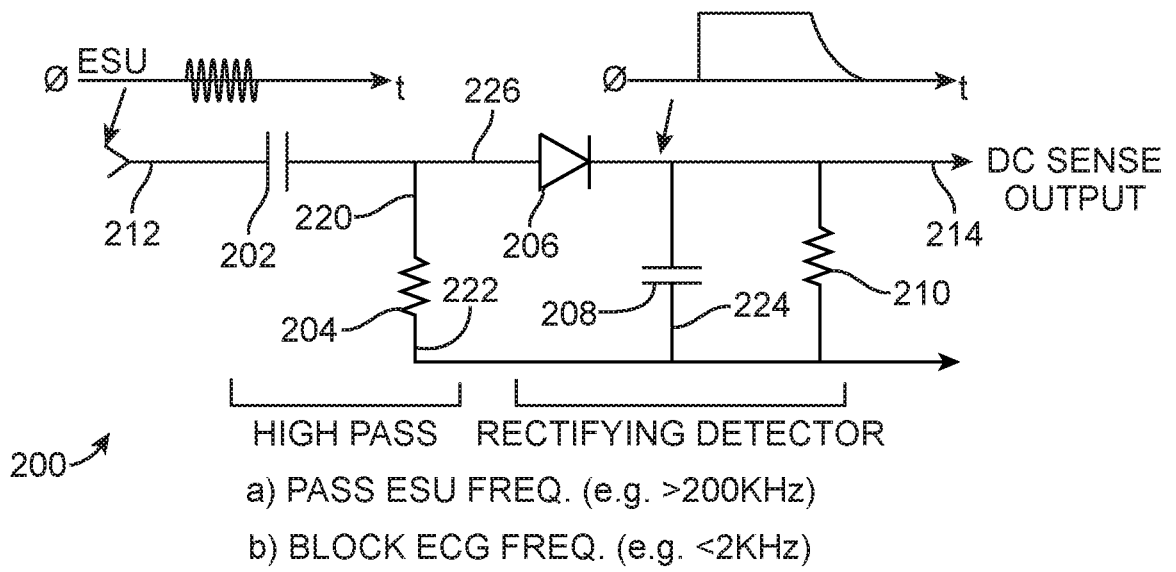


FIG. 2

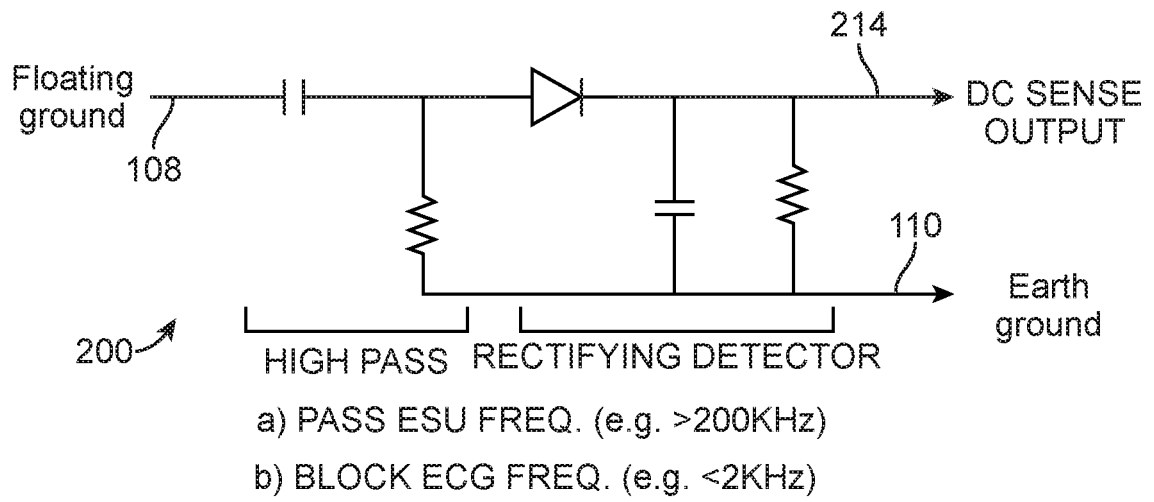


FIG. 3

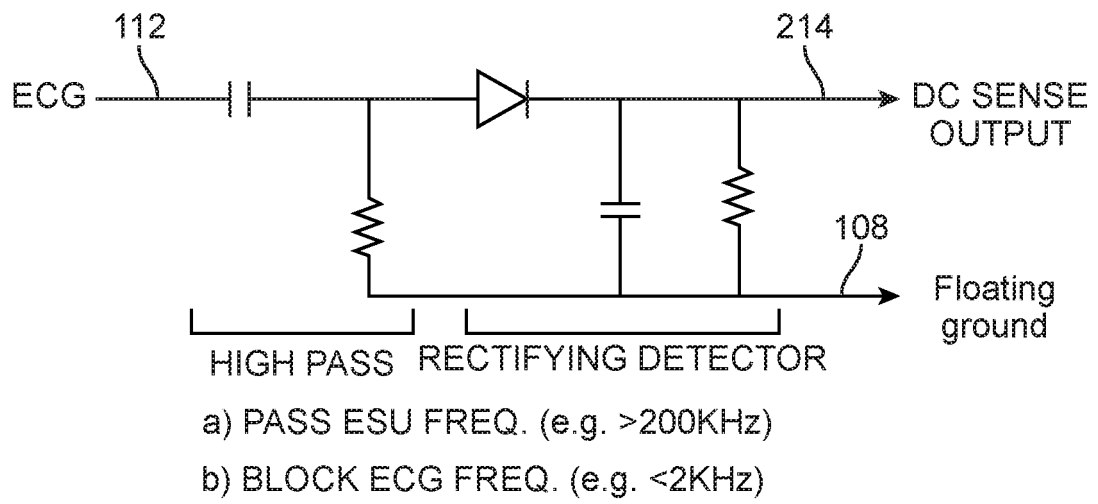


FIG. 4

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 2009018429 A [0003]
- US 4537200 A [0004]

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外部链接	Espacenet		

摘要(译)

提供了用于检测电外科单元信号的电路。 示例电路包括:滤波器,被配置为处理与测量患者的生物电势信号相关联的浮地信号;以及检测器,被配置为至少部分地基于浮地和地面来输出感测信号,以检测噪声。 电外科单元信号。