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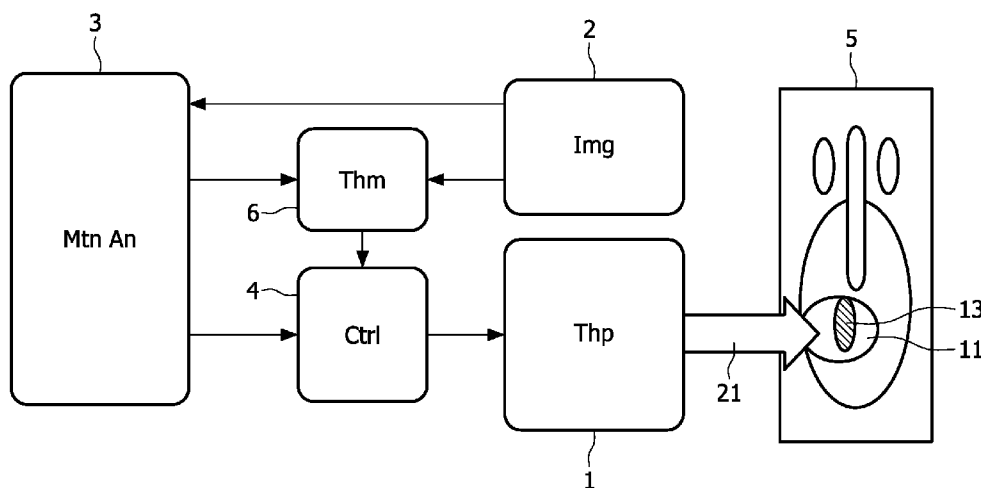


FIG. 1

(57) Abstract: A therapeutic system comprises a therapy module to direct a therapeutic action, e.g. focused ultrasound or RF energy to a target. An imaging module such as an magnetic resonance examination system generates image information of a therapy region that includes the target. By way of a motion analysis module a motion vector field is derived from the image information of the therapy region. A control module controls the therapy module on the basis of the motion vector field. Notably, on the basis of the motion vector field an accurate temperature distribution is derived from magnetic resonance signals and the motion vector field. Also magnetic resonance elastography data may be employed to improve the accuracy of the temperature distribution.

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Image guided therapy

FIELD OF THE INVENTION

The invention pertains to a therapeutic system comprising a therapy module to direct a therapeutic action to a target. The therapeutic system also comprises an imaging module to generate image information of a therapy region that includes the target and an area or volume around the actual target.

BACKGROUND OF THE INVENTION

Such a therapeutic system is known from the international application **WO98/52465**.

In the known therapeutic system the therapy module is an energy applicator such as a high intensity focused ultrasound unit. A magnetic resonance instrument has the function of the imaging module and is used to monitor hyperthermia treatments by the energy applicator. Further, the cited international application mentions that markers on the subject may be tracked so as to track and compensate for movement of the subject.

SUMMARY OF THE INVENTION

An object of the invention is to provide a therapeutic system which is able to take movements of the subject to be treated more accurately into account.

This object is achieved by a therapeutic system according to the invention comprising

- a motion analysis module to derive a motion vector field from the image information of the therapy region and
- a control module to control the therapy module on the basis of the motion vector field.

An insight on which the present invention is based, is that tracking of markers on the patient's skin only represents bulk movements of a therapy region that includes the target to be treated and consequently the control of the therapeutic action is not accurate. According to the invention a motion vector field represents local vector (magnitude and direction) movements of the therapeutic region at a predetermined spatial resolution. This

motion vector field is employed to control the therapeutic action. This allows the therapeutic action to be more accurately directed to the actual target. The therapeutic action may e.g. be a high intensity focused ultrasound beam which generates heat in the focus at which it is directed and thus causes therapeutic effects such as local hyperthermia in the tissue at the focus. In another example the therapeutic action is performed by high intensity radio-frequent electromagnetic radiation that is directed to the target and causes RF or laser ablation of the tissue in the target. Also a device for cryo-ablation is possible, in which the tissue is ablated by lowering the temperature. Further, the therapeutic action may concern local gene transfection or drug release e.g. by locally elevated temperature or drug release by cavitation of micro-bubbles containing drugs as an adjuvant therapy.

The target is usually a local lesion such as a (cancerous) tumour or (uterine) fibroids or an area of the myocardium having abnormal electrical conduction. The therapy region is an area or a volume onto which the therapeutic action is directed and that includes the actual target. Often the therapy region is a well delimited portion of the patient's anatomy such as an organ (e.g. liver, uterus or heart).

Further, the therapeutic action can be controlled to avoid (a) selected portion(s) of the treatment region outside of the actual target. This is achieved in that the control module has the function to distinguish (a) portion(s) of the therapy region to be avoided. This can be done on the basis of information provided by the user e.g. on the basis of image information from the imaging module or on the basis of pre-acquired images. Then the therapeutic action is adjusted to avoid these distinguished portion(s).

Selected portions to be avoided by the therapeutic action may be parts of the anatomy that are sensitive to the therapeutic action (ultrasound or RF energy) but should not be damaged. The accurate control provided on the basis of the motion vector field allows accurate direction to actual target, such as the lesion, while avoiding unintentional damage to healthy tissue around the lesion.

These and other aspects of the invention will be further elaborated with reference to the embodiments defined in the dependent Claims.

In one aspect of the invention the motion vector field represents displacements, orientation and deformations of the therapy region. That is, the motion vector field represents changes in shape and size as well as local deformations. Thus the control on the basis of the motion vector field enables that the therapeutic action accounts for complicated movements and deformations of the therapy region. According to this aspect of the invention, markers are placed in the therapy region. These markers in the therapy region

are imaged by the imaging module. For example the markers may be passive markers such as small spheres comprising a material having a short magnetisation decay time (T_1) which show up as signal voids in a magnetic resonance image, or as small spheres containing a material with another MR-observable nucleus, such as ^{19}F , which can be imaged at a different frequency and without background noise (since this nucleus does not naturally occur in human bodies). Active markers may be used e.g. in the form of micro coils that emit an RF signal that is picked up by the magnetic resonance examination system and are represented in the magnetic resonance image. Either active and/or passive markers or a combination of active and passive markers can be employed. In particular these passive or active markers may be disposed on an invasive instrument, such as a catheter, guidewire or needle.

In another aspect of the invention the imaging module is formed by a magnetic resonance examination system which is arranged to perform thermography. That is, the magnetic resonance examination system generates and acquires magnetic resonance signals from the patient and derives a temperature distribution of the therapy region from the magnetic resonance signals. The motion vector field is derived on the basis of the representation of the markers. The markers are e.g. represented by magnetic resonance signals from the markers when active markers are used or by effects in the magnetic resonance signals caused by the markers when passive markers are used. In this embodiment a temperature distribution calculation module is provided which makes use of the motion vector field to calculate an accurate temperature distribution from the MR signal, taking phase effects of motion into account. On the basis of the motion vector field phase contributions to the magnetic resonance signals due to motion are isolated from phase contributions due to temperature. Hence, an accurate temperature distribution in which errors due to motion are avoided or corrected for on the basis of the motion vector field is derived from the magnetic resonance signals by means of the motion vector field.

In a further aspect of the invention the imaging module has the function to perform magnetic resonance elastography (MRE). The technique of MRE is known per se from the papers '*Imaging anisotropic and viscous properties of breast tissue by magnetic resonance elastography*' in Magn.Reson.Med. **53**(2005)372-387 and '*Viscoelastic shear properties of in vivo breast lesions measured by MR elastography*' in Magn.Reson.Med. **23**(2005)159-165 by R. Sinkus et al. The MRE imaging module produces maps of elasticity and viscous properties of the tissue of the therapy region. On the basis of these elasticity and/or viscosity properties and the representations of the markers in the image (e.g. magnetic resonance image) a highly accurate motion vector field is derived. The elasticity and/or

viscosity properties allow to more accurately estimate the motion vector field at positions between the actually measured markers. For example, interpolation of the local movement, orientation and/or deformation at positions between the markers is interpolated on the basis of changes of positions of the markers where the interpolation is weighted on the basis of the elasticity and/or viscosity properties. Likewise, estimates of motion vectors can be obtained outside the region defined by the markers by extrapolation. Notably, as the tissue is more elastic, positions between the markers will follow the change of positions of the markers to a lesser extent and the tissue will be more deformed than displaced. The position of the passive or active markers are obtained by way of a conventional magnetic resonance imaging technique e.g. on the basis of magnetic resonance signals due to the markers. Further, the elasticity and/or viscosity properties acquired by MR elastography can be taken into account in the derivation of the temperature distribution of the therapy region. In this way deformation of the tissue is taken more accurately into account so that the temperature distribution is more accurate. Such highly accurate temperature distribution enables e.g. to trigger a genetic reaction or a drug release action in the target.

The invention further relates to a computer programme as defined in Claim 8. The computer programme of the invention can be provided on a data carrier such as a CD-ROM disk or a USB memory stick, or the computer programme of the invention can be downloaded from a data network such as the world-wide web. When installed in the computer included in therapeutic system e.g. including a magnetic resonance imaging system, the therapeutic system of the invention is enabled to operate according to the invention and achieve a more accurate performance of the therapeutic action.

The invention also relates to a method of monitoring a therapeutic action as defined in Claim 9. This method of monitoring a therapeutic action of the invention achieves a more accurate performance of the therapeutic action. The method of the invention merely provides monitoring information which forms a technical tool to support the physician in charge in carrying out the actual therapeutic action. Further, as only monitoring information is supplied concerning motion and/or deformation of the therapy region, the method of the invention in itself does not produce a diagnosis, or more in particular a diagnosis *in stricto sensu*, but rather produces an intermediate technical result of providing a technical aid to monitor the action of the therapy system.

BRIEF DESCRIPTION OF THE DRAWINGS

These and other aspects of the invention will be elucidated with reference to the embodiments described hereinafter and with reference to the accompanying drawing wherein

5 Figure 1 shows a diagrammatic representation of a therapeutic system according to the invention and

 Figure 2 shows a diagrammatic representation of the use of the motion vector field in a therapeutic system of the invention.

10 DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

 Figure 1 shows a diagrammatic representation of a therapeutic system according to the invention. The therapeutic system comprises a therapy module 1 which applies a therapeutic action 21 to a target 13 in a therapy region 1 of a patient 5. For example the therapy module is a high-intensity focused ultrasound apparatus which focuses a high-
15 intensity ultrasound beam onto the target 13 e.g. a uterine fibroid. Such a high-intensity ultrasound apparatus is known as such from the paper '*Local hyperthermia with MR-guided focused ultrasound: spiral trajectory for the focal point optimized for temperature uniformity in the target region*' by R.Salomir et al. in J. Magn. Res. Im. **12**(2000)571-583. Further, such a high-intensity ultrasound apparatus of which the ultrasound transducer can be easily
20 directed to the target is described in the European patent application EP06119781.0. The therapy module can also be formed by an RF or laser ablation apparatus which deposits electromagnetic energy at the target, e.g. at a lesion in the myocardium. RF ablation as such is discussed in the paper Am J Roentgenol. 1998 Apr;170(4):1023-8. The therapy module is controlled by a control module 4, notably the control module controls the position, direction
25 and/or focusing of the therapeutic action such as the focused ultrasound beam or the RF energy beam.

 The therapy system further comprises an imaging module 2, for example a magnetic resonance examination system. In particular the magnetic resonance examination system is enabled to perform magnetic resonance elastography. Alternatively, the imaging
30 module can be any medical diagnostic imaging modality such as x-ray imaging, computed tomography or ultrasound imaging. The imaging module acquires image information from the patient 5, notably of the therapy region 11 e.g. in the form of magnetic resonance signals from which a magnetic resonance image can be reconstructed. When magnetic resonance elastography is employed the magnetic resonance elastography image represents local visco-

elasticity properties of the therapy region. When in addition to a suitable magnetic resonance imaging protocol is employed for obtaining anatomical (morphological) information, the magnetic resonance signals may also represent the local temperature and thus the spatial temperature distribution of the therapy region can be derived. That is, the magnetic resonance examination system is also able to perform real-time thermography and – based on the measured temperature distribution - control the therapeutic action e.g. in the form of causing elevated local temperature in the tissue by means of suitably adjusting the therapy module. Further, the motion vector field derived on the basis of the local markers can be used to correct the local temperature for phase errors due to motion in the magnetic resonance signals. This is carried out in the temperature distribution module 6 that is arranged, notably in software, to compute the spatial temperature distribution in the therapy region on the basis of the magnetic resonance signals from the magnetic resonance examination system 2 and the motion vector field derived from the markers and/or visco-elastic properties.

Preferably, (shown in Figure 2), local markers 12 are provided in or near the therapy region. A motion analysis module 3 is provided in the form of an image processing unit that is programmed to derive information about motion and deformation of the therapy region from a time series of images from the imaging module. From the image information the motion analyses module 3 derives the magnitude and local motion in the form of the motion vector field in the therapy region. In particular, the motion vector field is derived from the changes in position of the local markers in combination with the visco-elastic properties obtained from the magnetic resonance elastography data or from an organ model represented by a software program. The motion vector field is applied to the control module 4 which then (re-) adjusts the therapy module to direct the therapeutic action to the target and in this the movement and deformation of the target and/or the therapy region around the actual target is taken into account.

Figure 2 shows a diagrammatic representation of the use of the motion vector field in a therapeutic system of the invention. In the therapy region 11 a target 13 is present. E.g. the therapy region is an organ such as the patient's heart or prostate or uterus to be treated and the target is a lesion, such as an electrical conduction fault in the patient's myocardium or a tumour or a uterine fibroid. From the change in position of the markers 12 and e.g. visco-elastic properties derived from magnetic resonance signals (or an organ model) the motion vector field 16 is computed. For example the motion vector field is computed by interpolation between measured displacements of the markers 12. In the interpolation the visco-elastic properties are taken into account in the interpolation coefficients. On the basis

of the motion vector field the displacement and deformation and/or compression of the target is computed as represented by the displaced and deformed target 14. Also gross changes in shape inside the target may occur as indicated by the dent 15. Accordingly the therapeutic action is accurately directed onto the deformed and displaced target. Additionally, due
5 account can be taken of healthy tissue delineated by the zone 15 that should be avoided by the therapeutic action 21.

CLAIMS:

1. A therapeutic system comprising
 - a therapy module (1) to direct a therapeutic action to a target
 - an imaging module (2) to generate image information of a therapy region that includes the target
 - 5 - a motion analysis module (3) to derive a motion vector field from the image information of the therapy region and
 - a control module (4) to control the therapy module on the basis of the motion vector field.
- 10 2. A therapeutic system as claimed in Claim 1, wherein the motion analysis module is arranged to derive the motion vector field from representations of markers, in particular disposed on a invasive instrument, in the therapy region.
- 15 3. A therapeutic system as claimed in Claim 1, wherein the motion vector field represents displacement and/or orientation and deformation of the therapy region.
4. A therapeutic system as claimed in Claim 1, wherein
 - the imaging module is formed by a magnetic resonance examination system to acquire magnetic resonance signals from the therapy region, derive the image information
 - 20 from the magnetic resonance signals and
 - the control module includes a thermography unit arranged to derive a temperature distribution of the therapy region from the magnetic resonance signals, taking the motion vector field into account.
- 25 5. A therapeutic system as claimed in Claim 1 wherein
 - the imaging module is formed by a magnetic resonance system able to perform MR elastography (MRE), in order to derive image information representing visco-elasticity properties of the tissue of the therapy region and

- the motion analysis module is arranged to derive the motion vector field also on the basis of the visco-elasticity properties.

6. A therapeutic system as claimed in Claim 1 wherein

- the control module is arranged to
- distinguish (a) portion(s) of the therapy region to be avoided
- in order to adjust the therapeutic action in such a manner taking the information about target motion and/or deformation into account that the therapeutic action remains locally restricted to the target and avoids to distinguished portion

7. A therapeutic system as claimed in Claim 4 wherein

- the imaging module is formed by a magnetic resonance system able to perform MR elastography, in order to derive image information representing visco-elasticity properties of the tissue of the therapy region and

- the thermography unit is arranged to taken the visco-elastic properties into account in the temperature distribution of the therapy region.

8. A computer programme comprising instructions to

- direct a therapeutic action to a target
- generate image information of a therapy region that includes the target
- derive a motion vector field from the image information of the therapy region

and

- control the therapy module on the basis of the motion vector field.

9. A method to monitor a therapeutic action including to

- generate image information of a therapy region that includes the target
- derive a motion vector field from the image information of the therapy region

and

- monitor therapeutic action on the basis of the motion vector field

- monitor therapeutic action on the basis of a temperature distribution which is calculated taking the motion vector field into account.

1/2

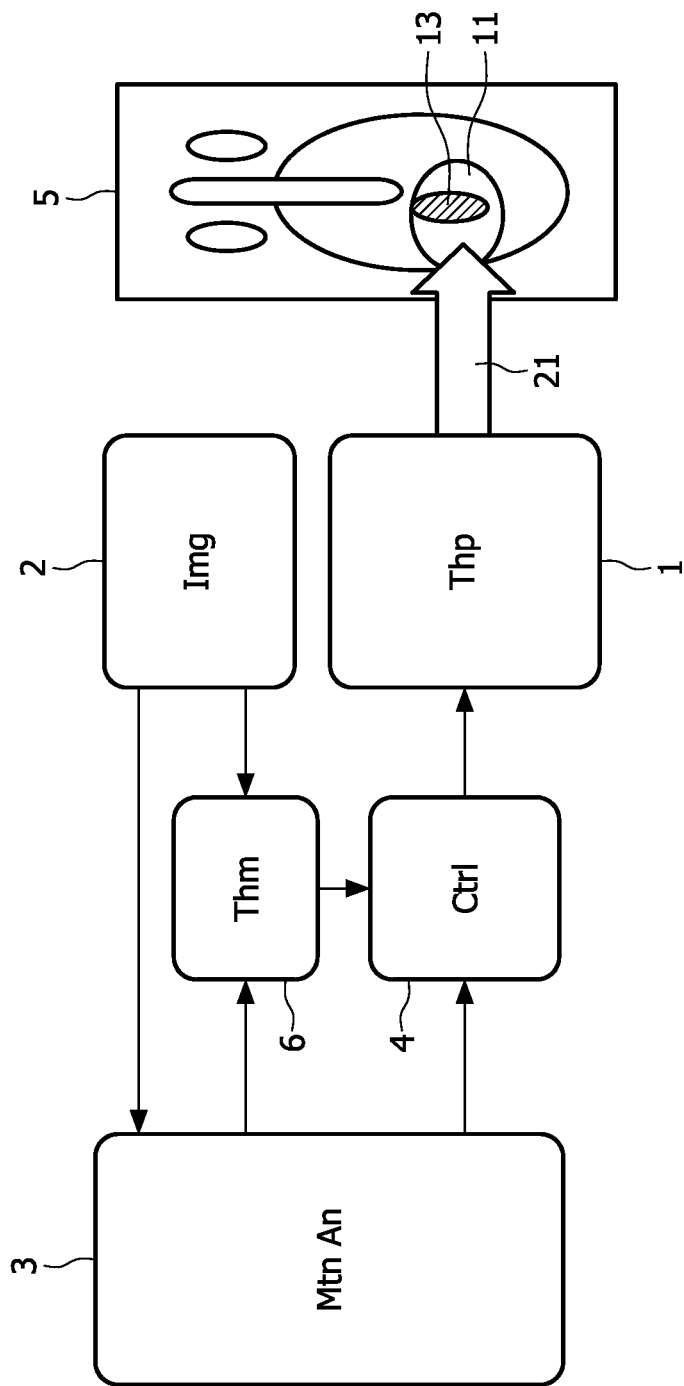


FIG. 1

2/2

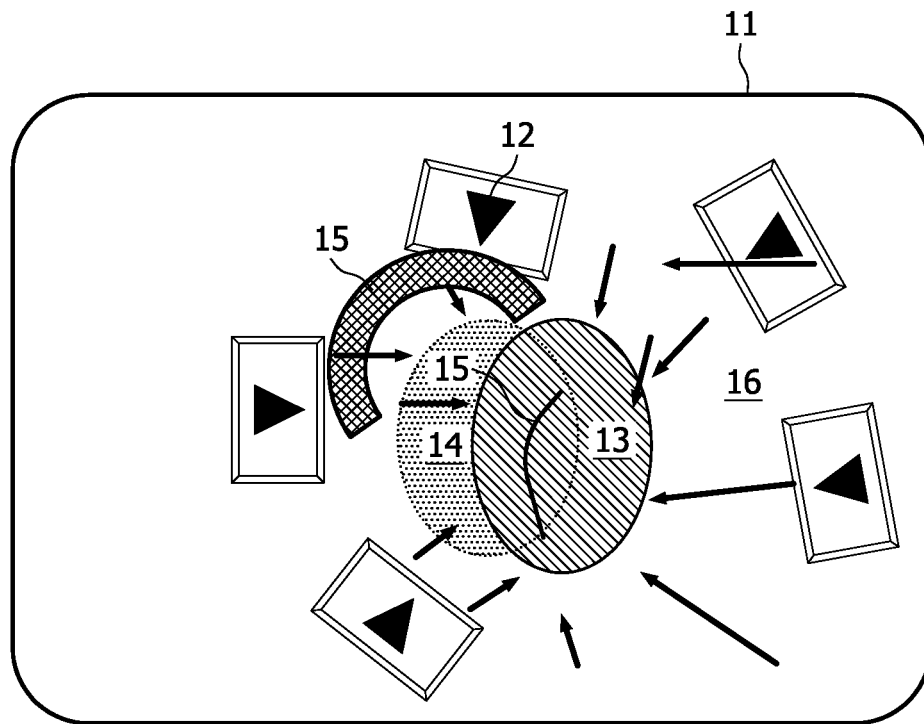


FIG. 2

专利名称(译)	图像引导治疗		
公开(公告)号	EP2158004A2	公开(公告)日	2010-03-03
申请号	EP2008763182	申请日	2008-06-04
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦电子N.V. 飞利浦知识产权及标准部GMBH		
当前申请(专利权)人(译)	皇家飞利浦N.V. 飞利浦知识产权及标准部GMBH		
[标]发明人	KUHN MICHAEL H COHEN JULIUS		
发明人	KUHN, MICHAEL, H. COHEN, JULIUS		
IPC分类号	A61N5/10 A61B5/00 A61B5/055 A61B19/00 A61N7/02 A61B5/01 A61B17/00 A61B18/14 A61B18/20 A61B34/20		
CPC分类号	A61N7/02 A61B5/015 A61B5/055 A61B18/14 A61B18/20 A61B34/20 A61B2017/00084 A61B2090/376 A61B2090/3904 A61B2090/3954		
优先权	2007110029 2007-06-12 EP		
其他公开文献	EP2158004B1		
外部链接	Espacenet		

摘要(译)

治疗系统包括治疗模块 (1) 以引导治疗作用 (21) , 例如治疗作用。聚焦超声或射频能量到目标 (13) 。诸如磁共振检查系统的成像模块 (2) 生成包括目标 (13) 的治疗区域 (11) 的图像信息。通过运动分析模块 (3) , 从治疗区域 (11) 的图像信息导出运动矢量场 (16) 。 '控制模块 (4) 基于运动矢量场控制治疗模块 (1) 。值得注意的是, 基于运动矢量场 (16) , 从磁共振信号和运动矢量场 (16) 导出精确的温度分布。还可以采用磁共振弹性成像数据来提高温度分布的精度。