

(19)



(11)

EP 2 068 706 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention
of the grant of the patent:
10.09.2014 Bulletin 2014/37

(51) Int Cl.:
A61B 5/00 (2006.01) **A61B 5/12** (2006.01)
A61B 5/0484 (2006.01)

(21) Application number: **07793316.6**

(86) International application number:
PCT/KR2007/003661

(22) Date of filing: **31.07.2007**

(87) International publication number:
WO 2008/035850 (27.03.2008 Gazette 2008/13)

(54) METHOD FOR OBJECTIVE AUTOMATED AUDIOMETRY

VERFAHREN FÜR DIE OBJEKTIVE AUTOMATISCHE AUDIOMETRIE

PROCÉDÉ D'AUDIOMÉTRIE AUTOMATISÉE OBJECTIVE

(84) Designated Contracting States:
**AT BE BG CH CY CZ DE DK EE ES FI FR GB GR
HU IE IS IT LI LT LU LV MC MT NL PL PT RO SE
SI SK TR**

(30) Priority: **20.09.2006 KR 20060091469**

(43) Date of publication of application:
17.06.2009 Bulletin 2009/25

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(56) References cited:
WO-A1-2006/122304 FR-A1- 2 299 004
US-A- 5 230 344 US-A- 5 697 379
US-A- 6 080 112 US-A1- 2003 073 920
US-B1- 6 196 977 US-B1- 6 200 273

- **ARNAUD JACQUIN ET AL: "Optimal Denoising of Brainstem Auditory Evoked Response (Baer) for Automatic Peak Identification and Brainstem Assessment", CONFERENCE PROCEEDINGS. ANNUAL INTERNATIONAL CONFERENCE OF THE IEEE ENGINEERING IN MEDICINE AND BIOLOGY SOCIETY (IEEE CAT. NO. 06CH37748); 30 AUG.-3 SEPT. 2006; NEW YORK, NY, USA, IEEE, PISCATAWAY, NJ, USA, 30 August 2006 (2006-08-30), pages 1723-1726, XP031235829, ISBN: 978-1-4244-0032-4**

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Description

Technical Field

[0001] The present invention relates to a method for automation of objective hearing test based on assessment of auditory evoked potential (AEP), for shortening testing time, and for minimization of inaccuracy and errors of hearing test that may be resulted from the automation and time shortening.

Background Art

[0002] The auditory brainstem response (ABR) audiometry is the most widely used method for objective hearing test.

[0003] For ABR audiometry, an electrode is placed on a subject's head and test stimulus is repetitively presented at least more than 1,500 times. After averaging the data, patient's audibility is determined by presence or absence of Wave V.

[0004] Although a click is commonly used for ABR audiometry, this stimulus is inappropriate for estimate of hearing thresholds on specific frequencies, such as 250Hz, 500Hz, 1000Hz, 2000Hz, 4000Hz, and 8000Hz. For this reason, tone-pip (or tone-burst) stimulus which has very short duration and can be presented as individual frequency, is used for estimate of the frequency-specific threshold. In this case, the term "tone-pip (or tone-burst) ABR audiometry" is currently used.

Disclosure of Invention

[0005] In the conventional tone-pip ABR audiometry, as each frequency-specific threshold should be estimated separately, it takes about 1.5-2 hours to test hearing thresholds. In addition, because user's determination of a subject's hearing threshold depends on visual discrimination of wave V peak in which amplitude decrease more and more when stimulus intensity gets closer to hearing threshold, it is difficult to avoid intervention of user's subjective judgment.

[0006] It is the most serious problem of the conventional ton-pip ABR audiometry that very long time is required for the hearing test. It takes long time to set manually the test stimulus presented separately according to frequency and intensity. In addition, each test stimulus should be presented more than 1,500 times to obtain a significant signal-to-noise ratio. Most of all, because the more stimulus intensity gets closer to hearing threshold, the more amplitude of wave V decreases, it takes long time for a user to determine the presence or absence of wave V peak.

[0007] In order to solve above-mentioned problems of the conventional method, the present invention provides a method for automation of tone-pip (or tone-burst) ABR audiometry, which can exclude both manual operation and user's subjective judgment. Another object of the

present invention is to provide a method for determining objective hearing threshold by computing the gap between wave V and SN10. Still another object of the present invention is to provide a method for obtaining excellent signal-to-noise ratio even after minimizing the number of averaging. Finally, a device for performing all above-mentioned objects is disclosed.

[0008] In order to achieve above-mentioned objects, there is provided a method for automation of tone-pip or tone-burst ABR audiometry comprising the steps of:

(a) setting test conditions, comprising the steps of: choosing the number of testing stimuli frequency; setting filtering frequency of notch filter to eliminate electrical background noise influxed from electrical source;

setting frequencies of high-pass band filter and low-pass band filter to eliminate low-frequency artifact from brain and high-frequency electrical harmonics, respectively;

setting the number of EEG data averaging; setting time range to randomize the time intervals between sequentially presented stimuli;

setting both time range and critical intensity value of potential change, which is needed to classify an abrupt potential change during the test as an artifact and to exclude the epoch with the abrupt potential change from averaging process;

setting a critical value which means a significant potential difference between section A containing positive peak of wave V and section B containing negative peak of SN10; and setting standards for both coordinates and graphic images which are visualized in a user interface; which is arbitrary done by a user before starting test.

(b) converting subject's spontaneous EEG, which is influxed from electrodes placed on a subject's head right before starting test, into a real-time graphic image;

(c) quantitative visualization of FFT analysis data on periodic artifacts among subject's spontaneous EEG;

(d) filtering distinctive periodic artifacts based on the FFT analysis data, which is arbitrarily done by a user;

(e) as a preliminary test, presenting standard test stimulus to a subject according to the test condition with random time interval fixed in step (a);

real-time counting and notifying the number of epochs included for averaging and the number of epochs excluded from averaging process according to the criteria of epoch fixed in step (a);

averaging the epochs where there seems to be no abrupt potential change; band-pass filtering of averaged data by applying the frequencies determined

In step (a) to eliminate low-frequency artifact from brain and high-frequency electrical harmonics; notch filtering of stimulus artifact generated in concert with the presented stimulus, by applying the same frequency as that of the test stimulus ; real-time imaging of the averaged EEG data on coordinates according to the number of averaging and coordinates standard fixed in step (a); and searching the positive peak of evoked wave V, and setting time section, which is the A and B section containing wave V positive peak and SN10 negative peak, respectively.

(f) setting initial intensity of the test stimulus for the main test, by gradually decreasing or increasing stimulus intensity, the minimal intensity, at which the potential difference between A and B section does not exceed the previously fixed critical value, is found out and set to Y, wherein the initial stimulus intensity of a main test is set to $Y + Z$ dB.; and

(g) as a main test, presenting test stimulus of each frequency, searching the minimal intensity where the potential difference between A and B section does not exceed the critical value fixed in advance in step (a), and determining objective hearing threshold of each frequency.

[0009] The step (a) is for setting test condition. This step comprises the steps of: choosing the number of testing frequency; setting filtering frequency of notch filter to eliminate electrical background noise influxed from electrical source; setting frequencies of high-pass band filter and low-pass band filter to eliminate low-frequency artifact from brain and high-frequency electrical harmonics, respectively; setting the number of averaging; setting time range to randomize the time intervals between sequentially presented stimuli; setting both time range and critical intensity value of potential change, which is needed to classify an abrupt potential change during the test as an artifact and to exclude the epoch with the abrupt potential change from averaging process; setting a critical value which means a significant potential difference between section A containing positive peak of wave V and section B containing negative peak of SN10; and setting specifications for both coordinates and graphic images which are visualized in a user interface.

[0010] The step (b) is the same as the conventional method for converting subject's spontaneous EEG, which is influxed from electrodes placed on a subject's head before starting test, into a real-time graphic image.

[0011] The step (c) is a quantitative visualization of FFT analysis data on periodic artifacts among subject's spontaneous EEG. In this step, a large number of notch filters are needed to completely eliminate minute artifacts influxed from electrical harmonics, because the minute artifacts cannot be completely eliminated by a small number of notch filters, which are generally used for elimination of electrical harmonics. For accurate filtering of minute artifacts influxed from electrical harmonics, real-

time frequency spectrum analysis for influxed potential is required, and it is desirable to use FFT analysis.

[0012] The step (d) is an arbitrary filtering by a user of distinctive periodic artifacts, which is based on the FFT analysis data of step (c). In this step, it is desirable to prudently use notch filters by considering the frequency and intensity of electrical harmonics, and the same frequency as that of the corresponding harmonics artifact is applied as the frequency of a notch filter.

[0013] The step (e) is a preliminary test. In this step, after searching the wave V peak, the A and B section, which comprises wave V peak and SN10 peak, respectively, is determined. In detail, the step (e) comprises the steps of: presenting standard test stimulus (e.g. 2KHz, 90dBHL, standard stimulus can be arbitrarily set by a user) to a subject according to the test condition with random time interval which is set in step (a); real-time counting and notifying the number of epochs included (accepted) for averaging and the number of epochs excluded (rejected) from averaging process according to the criteria of the epoch with the abrupt potential change fixed in step (a); averaging the accepted epochs where there seems to be no abrupt potential change; band-pass filtering of averaged data by applying the frequencies determined in step (a) to eliminate low-frequency artifact from brain and high-frequency electrical harmonics; notch filtering of stimulus artifact generated in concert with the presented stimulus, by applying the same frequency as that of the test stimulus; real-time imaging of the averaged EEG data on coordinates, according to the number of averaging and coordinates standard fixed in step (a); and after searching the positive peak of evoked wave V, setting time sections which are both A and B sections containing wave V positive peak and SN10 negative peak, respectively. An example of conditional sentences used to set the A and B section is as follows; "if the generation time of wave V peak, which is between 6 ms and 9 ms of averaged EEG section, is set to X, A section is $(X - 0.5) \text{ ms} \sim (X + 0.5) \text{ ms}$ and B section is $(X + 1.5) \text{ ms} \sim (X + 3.5) \text{ ms}$."

[0014] The step (f) is setting initial intensity of the test stimulus for main test. By gradually decreasing stimulus intensity (e.g. 90, 85, 80, 75 dBHL or dBnHL) in the preliminary test, minimal intensity, at which the potential difference between A and B section does not exceed the critical value fixed in advance in step (a), is found out and set to Y. The initial stimulus intensity of a main test is set to $Y + Z$ dB. (Z could be 5, 10, 15, 30, etc.)

[0015] Finally, the step (g) is a main test. After presenting test stimulus of each frequency to a subject and searching the minimal intensity of each frequency where the potential difference between A and B section does not exceed the critical value fixed in advance in step (a), the objective hearing threshold of each stimulus frequency is determined. Detail methods and processes applied to step (g) are the same as that of step (e).

Brief Description of the Drawings

[0016]

FIG. 1 is a configuration chart of a device for performing objective automated hearing test, not part of the present invention.

[32] FIG. 2 is a flow chart illustrating whole process of objective automated hearing test according to a preferred embodiment of the present invention.

Mode for the Invention

[0017] Hereinafter, the preferred embodiment of the present invention will be described with reference to the accompanying drawings.

[0018] The present invention provides with a method for automated tone-pip (or tone-burst) ABR test without both manual operation and user's subjective judgment, for determination of objective hearing thresholds based on the gap between wave V and SN10, and for acquisition of excellent signal-to-noise ratio by only minimal number of averaging.

[0019] The device for performing objective automated hearing test is firstly described and embodiments for performing automated tone-pip ABR test without both manual operation and user's subjective judgment, determination of objective hearing thresholds based on the gap between wave V and SN10, and obtaining excellent signal-to-noise ratio by only minimal number of averaging are described in this specification.

[0020] FIG. 1 is a configuration chart of a device for performing objective automated hearing test not being part of the present invention.

[0021] Referring to FIG. 1, the part for both EEG analysis and hearing threshold determination is firstly illustrated 100.

[0022] If evoked EEG analysis data indicates that hearing threshold is not determined, next stimulus is presented 102.

[0023] Concerning the method of stimulus presentation, unpredictable stimulus to both a user and a subject is presented in the present invention. This is accomplished by random processing of stimulus presenting part and is totally different from the conventional method. Generally used frequencies of tone-pip (or tone-burst) stimuli for objective hearing test are as follows; 250Hz, 500Hz, 1000Hz, 2000Hz, and 8000Hz. The number of tone-pip stimulus can be increased by applying subdivided frequency interval.

[0024] Wide range of stimulus intensity from maximum of 130dB SPL to minimum can be used for the test.

[0025] Test stimulus is presented to a subject's ear not directly through a speaker but after passing trigger part 104. The trigger part transmits synchronization signal (114) of stimulus onset time to the EEG analysis part 100, which is needed to define initial time for averaging, and at the same time presents the stimulus to a subject

through a speaker 106.

[0026] Concerning the location of electrodes placed to a subject, it is recommended to place an electrode on the upper part of subject's frontal lobe in the preferred embodiment of the present invention performing objective automated hearing test. The frontal lobe is a proper spot for minimizing difficulties accompanied by electrode placement. In addition, even when diverse methods suggested in the present invention for improving signal-to-noise ratio are applied to hearing test, evoked EEG with excellent signal-to-noise ratio can be drawn out from the frontal lobe without any deterioration.

[0027] EEG influxed from the subject's frontal lobe is transmitted to EEG sampling part 112 through electrode connecting part 110.

[0028] Both EEG data and synchronization signal of stimulus onset time, which are drawn out by EEG sampling part and inputted by trigger part, respectively, are simultaneously transmitted to EEG analysis & hearing threshold determination part 100. After real-time analyzing, the subject's final hearing threshold of each stimulus frequency is determined.

[0029] FIG. 2 is a flow chart illustrating whole process of objective automated hearing test according to a preferred embodiment of the present invention.

[0030] Referring to FIG. 2, in advance of performing objective automated hearing test, test condition is set 200.

[0031] Test condition setting comprises the steps of: choosing the number of testing frequency; setting filtering frequency of notch filter to eliminate electrical artifacts influxed from electrical source; setting frequencies of high-pass band filter and low-pass band filter to eliminate low-frequency artifact from brain and high-frequency electrical harmonics, respectively; setting the number of averaging; setting time range to randomize the time intervals between sequentially presented stimuli (i.e., inter-stimulus interval, ISI); setting both time range and critical intensity value of potential change, which is needed to classify an abrupt potential change during the test as an artifact and to exclude the epoch with the abrupt potential change from averaging process; setting a critical value which means a significant potential difference between section A containing positive peak of wave V and section B containing negative peak of SN10; and setting standards for both coordinates and graphic images which are visualized in a user interface.

[0032] After setting test condition, subject's spontaneous EEG, which is influxed from electrodes attached to the subject's head before testing, can be converted into a real-time graphic image. This step is the same as the conventional methods 202.

[0033] Next step 204 is a quantitative visualization of FFT analysis data on periodic artifacts among subject's spontaneous EEG. In this step, many number of notch filters are needed to completely eliminate minute artifacts influxed from electrical harmonics, because the minute artifacts cannot be completely eliminated by a small

number of notch filters, which are generally used for elimination of electrical harmonics. For accurate filtering of minute artifacts influxed from electrical harmonics, real-time frequency spectrum analysis of influx potential is required, and it is desirable to use FFT analysis.

[0034] Based on the FFT analysis data, distinctive periodic artifacts are arbitrarily filtered by a user 206. In this step, it is desirable to use notch filters considering the frequency and intensity of electrical harmonics, and the same frequency as that of the corresponding harmonics artifact is applied as the frequency of a notch filter.

[0035] The accuracy and reliability of hearing test can be increased by a preliminary test followed by a main test. In this step, once a user presses the start button, standard test stimulus is presented 208. Though 2KHz, 90dBHL (or 60dBnHL) tone-pip stimulus is usually used as a standard test stimulus, it can be arbitrarily set by a user. All the test stimulus containing standard test stimulus are presented to a subject with random time interval fixed in the step of test condition setting.

[0036] While standard test stimulus is presented to a subject, an abrupt potential change, which distorts the final data of averaging, can be generated together with evoked potential by tone-pip stimulus. During ensemble averaging process, it is desirable to completely eliminate the epochs, which are containing the abrupt potential change 210. The elimination of epochs is accomplished according to the criteria fixed in the step of test condition setting, which includes time section and critical intensity.

[0037] The epochs without abrupt potential change are averaged by the conventional method 212.

[0038] By band-pass filtering of averaged data, wave form is changed sharply or softly and low-frequency artifacts from brain and high-frequency electrical harmonics are eliminated 214.

[0039] As stimulus artifact, which is generated in concert with the presented stimulus, can be reflected to the final averaged data, notch filtering applying the same frequency as that of the test stimulus is included 216.

[0040] The peak of wave V is found out from the final averaged data 218.

[0041] After searching the wave V peak, both A and B sections, which contain the positive peak of wave V and negative peak of SN10 respectively, are set 220. An example of conditional sentences used to set the A and B sections is as follows; "if the generation time of wave V peak, which is between 6 ms and 9 ms of averaged EEG section, is set to X, A section is $(X - 0.5) \text{ ms} \sim (X + 0.5) \text{ ms}$ and B section is $(X + 1.5) \text{ ms} \sim (X + 3.5) \text{ ms}$."

[0042] By gradually decreasing (e.g. 90, 85, 80, 75 dBHL) or increasing (e.g. 95, 100, 105 dBHL) stimulus intensity, the minimal intensity, at which the potential difference between A and B section does not exceed the previously fixed critical value, is found out and set to Y. The initial stimulus intensity of a main test is set to $Y + Z$ dB 222.

[0043] In a main test 224 ~ 232, after presenting test stimulus of each frequency to a subject and searching

the minimal intensity of each frequency where the potential difference between A and B section does not exceed the previously fixed critical value, the objective hearing threshold of each stimulus frequency is determined. Detail methods and processes applied to the main test are the same as that of a preliminary test except diversity of test stimulus frequency.

Industrial Applicability

[0044] As described above, according to the preferred embodiment of the method for objective automated hearing test, users can shorten testing time by automatically performing tone-pip (or tone-burst) ABR test without both manual operation and user's subjective judgment. Further, according to the preferred embodiment of the present invention, in spite of minimization of the averaging number, reliable hearing test data with excellent signal-to-noise ratio is obtained by applying a decision method of objective hearing thresholds based on the gap between wave V and SN10.

Claims

1. A method for automation of tone-pip or tone-burst auditory brainstem response (ABR) audiometry comprising the steps of:

- (a) setting test conditions, comprising the steps of: choosing the number of testing stimuli frequency; setting filtering frequency of notch filter to eliminate electrical background noise influxed from electrical source; setting frequencies of high-pass band filter and low-pass band filter to eliminate low-frequency artifact from brain and high-frequency electrical harmonics, respectively; setting the number of EEG data averaging; setting time range to randomize the time intervals between sequentially presented stimuli; setting both time range and critical intensity value of potential change, which is needed to classify an abrupt potential change during the test as an artifact and to exclude the epoch with the abrupt potential change from averaging process; setting a critical value which means a significant potential difference between section A containing positive peak of wave V and section B containing negative peak of SN10; and setting standards for both coordinates and graphic images which are visualized in a user interface; which is arbitrarily done by a user before starting test.
- (b) converting subject's spontaneous EEG, which is influxed from electrodes placed on a

subject's head right before starting test, into a real-time graphic image;

(c) quantitative visualization of FFT analysis data on periodic artifacts among subject's spontaneous EEG;

(d) filtering distinctive periodic artifacts based on the FFT analysis data, which is arbitrarily done by a user;

(e) as a preliminary test, presenting standard test stimulus

to a subject according to the test condition with random time interval fixed in step (a);

real-time counting and notifying the number of epochs included for averaging and the number of epochs excluded from averaging process according to the criteria of epoch fixed in step (a); averaging the epochs where there seems to be no abrupt potential change; band-pass filtering of averaged data by applying the frequencies determined in step (a) to eliminate low-frequency artifact from brain and high-frequency electrical harmonics;

notch filtering of stimulus artifact generated in concert with the presented stimulus, by applying the same frequency as that of the test stimulus ; real-time imaging of the averaged EEG data on coordinates according to the number of averaging and coordinates standard fixed in step (a); and

searching the positive peak of evoked wave V, and setting time section, which is the A and B section containing wave V positive peak and SN10 negative peak, respectively.

(f) setting initial intensity of the test stimulus for the main test, by gradually decreasing or increasing (e.g. 95, 100, 105 dBHL) stimulus intensity, the minimal intensity, at which the potential difference between A and B section does not exceed the previously fixed critical value, is found out and set to Y, wherein the initial stimulus intensity of a main test is set to $Y + Z$ dB.; and

(g) as a main test, presenting test stimulus of each frequency, searching the minimal intensity where the potential difference between A and B section does not exceed the critical value fixed in advance in step (a), and determining objective hearing threshold of each frequency.

2. The method of claim 1, wherein at step (d) the filtering step is arbitrarily performed by applying the frequency of corresponding periodic artifact as the frequency of a notch filter.

3. The method of claim 1, wherein after presenting test stimulus of each frequency to a subject and searching the minimal intensity of each frequency where the potential difference between A and B section

does not exceed the previously fixed critical value, the objective hearing threshold of each stimulus frequency is determined in step (g).

Patentansprüche

1. Verfahren zum Automatisieren von Tone-Pip- oder Tone-Burst-Hirnstamm-Audiometrie (ABR), umfassend die Schritte:

(a) Einstellen von Testbedingungen, umfassend die Schritte:

Auswählen der Anzahl von Test-Reizfrequenzen;

Einstellen der Filterfrequenz des Notchfilters zum Entfernen von elektrischem Hintergrundrauschen, das von der elektrischen Quelle einströmt;

Einstellen der Frequenzen von Hochpass-Bandfilter und Tiefpass-Bandfilter zum Entfernen von niederfrequenten Artefakten aus dem Gehirn bzw. hochfrequenten elektrischen Oberschwingungen;

Einstellen der Zahl der EEG-Daten-Mittelwertbildung;

Einstellen des Zeitbereichs zum Randomisieren der Zeitintervalle zwischen sequenziell dargebotenen Reizen;

Einstellen des Zeitbereichs und des Werts der kritischen Intensität der Potentialänderung, die benötigt werden, um eine abrupte Potentialänderung während des Tests als Artefakt einzustufen und den Zeitraum mit der abrupten Potentialänderung aus dem Vorgang der Mittelwertbildung auszuschließen;

Einstellen eines kritischen Werts mit der Bedeutung eines signifikanten Potentialunterschieds zwischen Abschnitt A, der ein positives Maximum der Welle V enthält, und Abschnitt B, der ein negatives Maximum von SN10 enthält; und

Einstellen von Standardwerten sowohl für Koordinaten als auch für graphische Abbildungen, die in einer Benutzerschnittstelle visualisiert werden;

was von einem Benutzer vor dem Beginn des Tests frei wählbar durchgeführt wird;

(b) Umwandeln des spontanen EEG eines Subjekts, das von Elektroden einströmt, die unmittelbar vor dem Beginn des Tests an dem Kopf eines Subjekts platziert worden sind, in eine graphische Echtzeit-Abbildung;

(c) Quantitatives Visualisieren von FFT-Analy-

sedaten von periodischen Artefakten in dem spontanen EEG des Subjekts;

(d) Filtern von charakteristischen periodischen Artefakten auf der Grundlage der FFT-Analysedaten, was von einem Benutzer frei wählbar durchgeführt wird;

(e) als Vorversuch Darbieten eines Standard-Testreizes gemäß den Testbedingungen mit einem in Schritt (a) festgelegten beliebigen Zeitintervall an ein Subjekt;

Echtzeit-Zählen und Melden der Anzahl von Zeiträumen, die in der Mittelwertbildung enthalten sind, und der Anzahl von Zeiträumen, die gemäß den in Schritt (a) festgelegten Kriterien von der Mittelwertbildung ausgeschlossen sind; Mitteln der Zeiträume, bei denen keine abrupte Potentialänderung vorzuliegen scheint;

Bandpass-Filtern der gemittelten Daten durch Anwenden der in Schritt (a) festgelegten Frequenzen, um niederfrequente Artefakte von dem Gehirn und hochfrequente elektrische Oberschwingungen zu entfernen;

Notchfiltern des zugleich mit dem dargebotenen Reiz erzeugten Reizartefakts durch Anwenden der gleichen Frequenz wie jene des Testreizes; Echtzeit-Bildgebung der gemittelten EEG-Daten auf Koordinaten gemäß der Zahl der Mittelwertbildung und den in Schritt (a) festgelegten Standardkoordinaten; und

Ermitteln des positiven Maximums der evozierten Welle V und Einstellen des Zeitabschnitts, der der A- bzw. B-Abschnitt ist, der das positive Maximum der Welle V bzw. das negative Maximum von SN10 enthält;

(f) Einstellen der Anfangsintensität des Testreizes für den Haupttest durch allmähliches Verringern oder Erhöhen (beispielsweise 95, 100, 105 dBHL) der Reizintensität, wobei die Mindestintensität, bei der der Potentialunterschied zwischen dem A- und dem B-Abschnitt den zuvor festgelegten kritischen Wert nicht überschreitet, ermittelt wird und auf Y gesetzt wird, wobei die Anfangs-Reizintensität bei einem Haupttest auf Y + Z dB gesetzt wird; und

(g) als Haupttest Darbieten von Testreizen mit jeder Frequenz, Ermitteln der Mindestintensität, bei der der Potentialunterschied zwischen dem A- und dem B-Abschnitt den zuvor in Schritt (a) festgelegten kritischen Wert nicht überschreitet, und Bestimmen der objektiven Hörschwelle für jede Frequenz.

2. Verfahren gemäß Anspruch 1, wobei bei Schritt (d) der Filterschritt frei wählbar durch Anwenden der Frequenz des entsprechenden periodischen Artefakts als Frequenz eines Notchfilters durchgeführt wird.

3. Verfahren gemäß Anspruch 1, wobei nach dem Darbieten eines Testreizes mit jeder Frequenz an ein Subjekt und Ermitteln der Mindestintensität für jede Frequenz, bei der der Potentialunterschied zwischen dem A- und dem B-Abschnitt den zuvor festgelegten kritischen Wert nicht überschreitet, die objektive Hörschwelle für jede Reizfrequenz in Schritt (g) bestimmt wird.

Revendications

1. Procédé permettant d'automatiser une évaluation audiolologique des potentiels évoqués du tronc cérébral (ABR) comprenant les étapes suivantes :

(a) définir des conditions de test comprenant les étapes suivantes :

choisir le nombre de fréquences de stimulation de test ;

définir la fréquence de filtrage d'un filtre à élimination de bande pour éliminer le bruit de fond électrique provenant de la source électrique ;

définir des fréquences de filtre passe-bande haut et passe-bande bas pour éliminer respectivement les artéfacts basse fréquence du cerveau et les harmoniques électriques à haute fréquence ;

définir le nombre de données d'EEG moyennes ;

définir une plage de temps pour randomiser les intervalles de temps entre les stimuli présentés en séquence ;

définir à la fois une plage de temps et une valeur d'intensité critique de changement de potentiel, qui est nécessaire pour classer un changement de potentiel abrupt au cours du test comme étant un artéfact et pour exclure la durée contenant le changement de potentiel abrupt du processus de calcul de moyenne ;

définir une valeur critique qui signifie une différence de potentiel significative entre la section A contenant un pic positif d'onde V et la section B contenant un pic négatif SN10 ; et

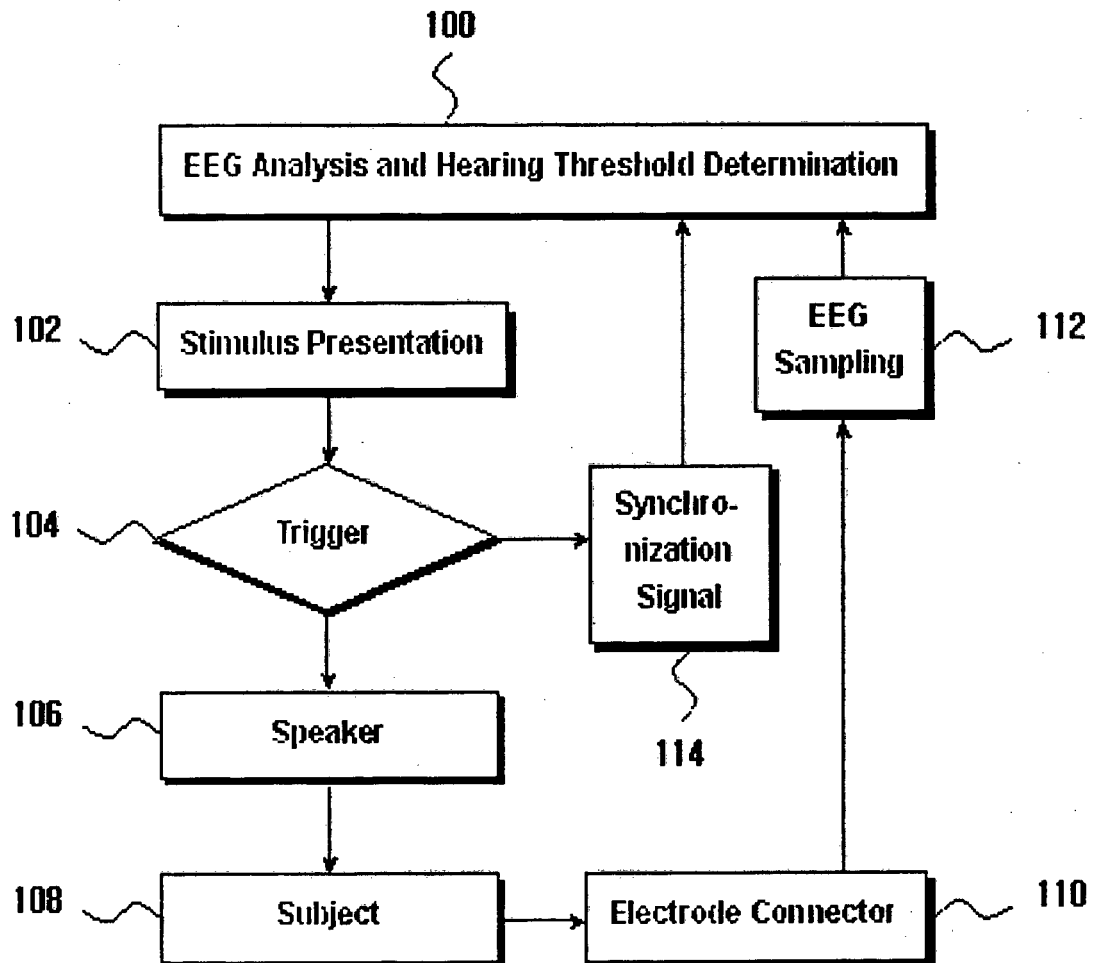
définir des standards pour à la fois les coordonnées et les images graphiques qui sont visualisées sur une interface utilisateur ; ce qui est effectué de manière arbitraire par un utilisateur avec de commencer le test ;

(b) convertir l'EEG spontané du patient, qui est relevé au moyen d'électrodes placées sur la tête d'un patient juste avant de commencer le test, en une image graphique en temps réel ;

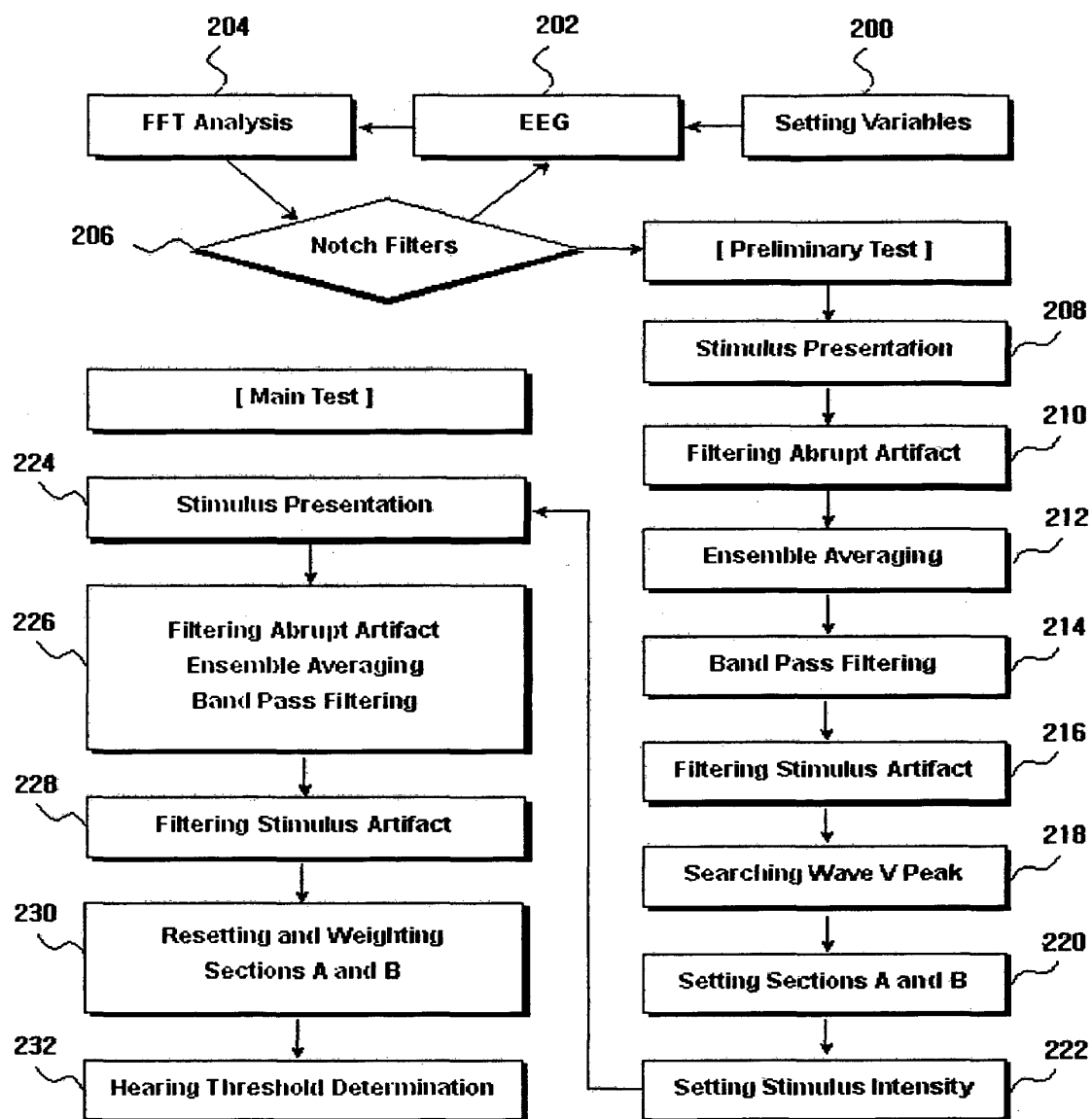
- (c) effectuer une visualisation quantitative des données d'analyse FFT sur des artéfacts périodiques d'EEG spontané d'un patient ;
- (d) filtrer des artéfacts périodiques distinctifs sur la base des données d'analyse FFT, ce qui est effectué de manière arbitraire par un utilisateur ;
- (e) comme test préliminaire, présenter un stimulus de test standard à un patient conformément à la condition de test avec un intervalle de temps aléatoire fixé à l'étape (a) ;
- compter en temps réel et notifier le nombre de durées incluses dans le calcul de moyenne et le nombre de durées exclues du processus de calcul de moyenne conformément aux critères de durée fixés à l'étape (a) ;
- moyenner les durées où il semble ne pas y avoir de changement de potentiel abrupt ;
- filtrer par un filtre passe-bande les données moyennées en appliquant les fréquences déterminées à l'étape (a) pour éliminer l'artéfact basse fréquence du cerveau et les harmoniques électriques à haute fréquence ;
- filtrer par un filtre à élimination de bande l'artéfact de stimulus généré de concert avec le stimulus présenté en appliquant la même fréquence que celle du stimulus de test ;
- imager en temps réel les données d'EEG moyennées sur des coordonnées conformément au nombre de standards de coordonnées et de moyennes fixés à l'étape (a) ; et
- rechercher le pic positif de l'onde V évoquée, et définir une section de temps, laquelle est la section A et la section B contenant respectivement un pic positif V et un pic négatif SN10 ;
- (f) définir une intensité initiale du stimulus de test pour le test principal, en diminuant ou en augmentant graduellement (par exemple, 95, 100, 105 dBHL) l'intensité du stimulus, l'intensité minimale, à laquelle la différence de potentiel entre la section A et la section B n'excède pas la valeur critique préalablement fixée, est trouvée et fixée à Y, où l'intensité initiale du stimulus d'un test principal est fixée à $Y + Z$ dB ; et
- (g) comme test principal, présenter un stimulus de test de chaque fréquence, rechercher l'intensité minimale où la différence de potentiel entre la section A et la section B n'excède pas la valeur critique fixée à l'avance à l'étape (a), et déterminer un seuil d'audition objectif pour chaque fréquence.
2. Procédé selon la revendication 1, dans lequel à l'étape (d), l'étape de filtrage est arbitrairement effectuée en appliquant la fréquence de l'artéfact périodique correspondant comme la fréquence d'un filtre à élimination de bande.
3. Procédé selon la revendication 1, dans lequel, après

avoir présenté un stimulus de test de chaque fréquence à un patient et avoir recherché l'intensité minimale de chaque fréquence où la différence de potentiel entre la section A et la section B n'excédait pas la valeur critique préalablement fixée, le seuil d'audition objectif de chaque fréquence de stimulus est déterminé à l'étape (g).

[Fig. 1]



[Fig. 2]



专利名称(译)	客观自动测听的方法		
公开(公告)号	EP2068706B1	公开(公告)日	2014-09-10
申请号	EP2007793316	申请日	2007-07-31
[标]申请(专利权)人(译)	KWAK SANGYEOP		
申请(专利权)人(译)	EARLOGIC KOREA INC. KWAK , SANGYEOP		
当前申请(专利权)人(译)	EARLOGIC KOREA INC. KWAK , SANGYEOP		
[标]发明人	KWAK SANGYEOP		
发明人	KWAK, SANGYEOP		
IPC分类号	A61B5/00 A61B5/12 A61B5/0484		
CPC分类号	A61B5/04845 A61B5/125 A61B5/725 A61B5/7257		
优先权	1020060091469 2006-09-20 KR		
其他公开文献	EP2068706A1 EP2068706A4		
外部链接	Espacenet		

摘要(译)

本发明涉及基于听觉诱发电位 (AEP) 评估的客观听力测试自动化方法，用于缩短测试时间，以及用于由此产生的不准确性和错误的最小化。自动缩短和缩短时间。该方法包括以下步骤：作为初步测试，向受试者提供标准测试刺激;搜索波V峰值和SN1 0峰值;并且作为测试，呈现每个频率的测试刺激，搜索最小强度并确定每个频率的客观听力阈值。

[Fig. 1]

