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**(54) Systems and methods for communicating with implantable devices**

Systeme und Verfahren zur Kommunikation mit implantierbaren Vorrichtungen

Systèmes et procédés de communication avec des dispositifs implantables

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<b>WO-A1-02/32502</b>	<b>US-A- 4 918 736</b>
<b>US-B1- 6 200 265</b>	

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**Description****FIELD OF THE INVENTION:**

**[0001]** The present invention relates generally to systems and methods for measuring physiological conditions and/or performing therapeutic functions within a patient's body, particularly to systems and methods for controlling and/or energizing devices that may be implanted within a body, and more particularly to implants that may be energized, activated, controlled, and/or otherwise communicate via acoustic energy.

**BACKGROUND OF THE INVENTION:**

**[0002]** Devices are known that may be implanted within a patient's body for monitoring one or more physiological conditions and/or to provide therapeutic functions. For example, sensors or transducers may be located deep within the body for monitoring a variety of properties, such as temperature, pressure, strain, fluid flow, chemical properties, electrical properties, magnetic properties, and the like. In addition, devices may be implanted that perform one or more therapeutic functions, such as drug delivery, defibrillation, electrical stimulation, and the like.

**[0003]** Often it is desirable to communicate with such devices once they are implanted within a patient by external command, for example, to obtain data, and/or to activate or otherwise control the implant. An implant may include wire leads from the implant to an exterior surface of the patient, thereby allowing an external controller or other device to be directly coupled to the implant. Alternatively, the implant may be remotely controlled, e.g., using an external induction device. For example, an external radio frequency (RF) transmitter may be used to communicate with the implant. RF energy, however, may only penetrate a few millimeters into a body, because of the body's dielectric nature, and therefore may not be able to communicate effectively with an implant that is located deep within the body. In addition, although an RF transmitter may be able to induce a current within an implant, the implant's receiving antenna, generally a low impedance coil, may generate a voltage that is too low to provide a reliable switching mechanism.

**[0004]** In a further alternative, electromagnetic energy may be used to control an implant, since a body generally does not attenuate magnetic fields. The presence of external magnetic fields encountered by the patient during normal activity, however, may expose the patient to the risk of false positives, i.e., accidental activation or deactivation of the implant. Furthermore, external electromagnetic systems may be cumbersome and may not be able to effectively transfer coded information to an implant.

**[0005]** PCT Publication WO01/074278 describes a battery powered cochlear implant that can be programmed in response to acoustic signals transmitted from an external acoustic remote control.

**[0006]** Accordingly, systems and methods for commu-

nicating with an implant that may be implanted within a patient's body, such as a pressure sensor, a drug delivery device, a pacemaker, or a nerve stimulator, would be considered useful.

**SUMMARY OF THE INVENTION:**

**[0007]** While the invention is defined in the independent claims, the present disclosure is generally directed to systems and methods for communicating with implants or other devices that are placed, e.g., using open surgical or minimally invasive techniques, within a mammalian body. The implant may include one or more sensors for monitoring pressure or other physiological parameters and/or may perform one or more therapeutic functions. More particularly, the present invention is directed to external systems for controlling, activating, energizing, and/or otherwise communicating with such implants using acoustic telemetry, and to methods for using such systems.

**[0008]** In accordance with one aspect of the present invention, a system is provided for communicating with an implant within a body that includes an external communications device, e.g., a controller, securable to an exterior surface of a patient's body. Preferably, the controller is sufficiently small and portable that it may remain secured to the patient, possibly for extended time periods. For example, the device may be attached to or within a patch that may be secured to a patient's skin.

**[0009]** In one embodiment, the device is an external controller that generally includes one or more acoustic transducers, including a first acoustic transducer, for transmitting one or more acoustic signals into the patient's body. The controller may also include an energy source for powering the one or more acoustic transducers, and/or a processor or other electrical circuit for controlling operation of the controller. In addition, one or more of the acoustic transducers, such as the first acoustic transducer, may be configured for receiving acoustic signals from an implant within the patient's body. The controller may include memory for storing data, and the processor may extract sensor data and/or other data from acoustic signals received from an implant, e.g., for storage in the memory. In addition, the controller may include

a connector, lead, transmitter, receiver, or other interface for communicating with a recorder or other electronic device, such as a computer, personal digital assistant, or a wireless device, such as a cellular phone. The controller may be coupled to such an electronic device for transferring sensor data or other data stored in the memory of the controller and/or for receiving instructions or commands from the electronic device. A system according to the invention includes an implant for placement within the patient's body. The implant includes an electrical circuit for performing one or more commands when the implant is activated, an energy storage device, and one or more acoustic transducers, e.g., a second acoustic transducer, coupled to the electrical circuit and/or the energy

storage device. The electrical circuit includes a switch coupled to the energy storage device and the second acoustic transducer. The second acoustic transducer may receive one or more acoustic signals from the first acoustic transducer of the external device. For example, the switch may be closed and/or opened in response to a first acoustic signal to begin or discontinue current flow from the energy storage device to the electrical circuit or other components of the implant.

**[0010]** In a preferred embodiment, the external controller's processor controls the first acoustic transducer to transmit a first acoustic signal/or and a second acoustic signal. The switch of the implant may be closed when the first acoustic signal is received by the second acoustic transducer, while the switch may be opened when the second acoustic signal is received by the second acoustic transducer. In addition or alternatively, the first acoustic transducer may transmit first and second acoustic signals separated by a delay. The switch may be closed and/or opened only when the second acoustic transducer receives the first and second acoustic signals separated by a predetermined delay, thereby minimizing the risk of accidental activation or deactivation of the implant.

**[0011]** In yet another alternative, the first acoustic transducer may transmit a first acoustic signal, e.g., an activation signal, followed by a second acoustic signal, e.g., including a set of commands. The second acoustic transducer may receive the first and second acoustic signals, and the electrical circuit of the implant may extract the set of commands from the second acoustic signal, and control operation of the implant as instructed by the set of commands. In a further alternative, the implant may run continuously or intermittently, and the external controller may control, monitor, energize, and/or program the implant using acoustic telemetry during operation of the implant. The implant includes a sensor coupled to the electrical circuit, and the one or more commands may include measuring a physiological parameter within the body using the sensor. The second acoustic transmitter may transmit one or more acoustic signals including sensor data indicating the physiological parameter to the controller. In an alternative embodiment, the implant may be coupled to a therapeutic device or may include an internal therapeutic device coupled to the electrical circuit. The electrical circuit may control the therapeutic device in response to a physiological parameter measured by the sensor or in response to acoustic signals received from the external controller. For example, the implant may include a pacemaker that may be implanted via a minimally invasive catheter-based procedure. Any programming and/or interrogation of the pacemaker may be accomplished using acoustic telemetry from the external controller. In yet another alternative embodiment, the implant may include an actuator coupled to the electrical circuit, and the one or more commands may include activating the actuator to control a therapeutic device coupled to the actuator, such as a nerve stimulator or a controlled delivery drug release system.

5 **[0012]** In addition, the energy storage device of the implant may include a rechargeable device, such as a capacitor or a battery. For this embodiment, the system may include an external charger that may include a probe configured for placement against an exterior of the patient's body. The charger may include a source of electrical energy, such as a radio frequency (RF) generator, that is coupled to the probe. The probe may include another acoustic transducer, e.g., a third acoustic transducer, for converting electrical energy from the source of electrical energy into acoustic energy. The third acoustic transducer may transmit acoustic signals including acoustic energy into the patient's body. One (RF) more acoustic transducers of the implant, e.g., the second acoustic transducer, may be configured for converting these acoustic signals into electrical energy for recharging the energy storage device and/or powering the implant.

10 **[0013]** Thus, a system in accordance with the present invention may include an external controller that has sufficient power to control its own operation and to communicate with the implant. Because of its limited energy requirements, however, the controller may be relatively small and portable, e.g., may be attached to the patient, 15 while still allowing the patient to engage in normal physical activity. The controller may be used to communicate with an implant, e.g., periodically activating or deactivating the implant, and/or recording data generated and transmitted by the implant. Because it is located outside 20 the patient's body, the controller may be more easily programmed or reprogrammed than the implant, and/or may be repaired or replaced if necessary without requiring an interventional procedure.

25 **[0014]** In addition, the system may include a separate external charger that includes a substantially more powerful energy source, enabling it to recharge the energy storage device of the implant. For this reason, unlike the external controller, the charger may be a relatively bulky device that may include a portable probe for contacting 30 the patient's skin, and a large energy generator or converter that is stationary or of limited mobility. In an alternative embodiment, the external controller and charger may be provided as a single device, e.g., including one or more acoustic transducers and/or one or more processors for performing the functions of both devices, as 35 described above. In this embodiment, however, portability of the system and convenience to the patient may be compromised.

40 **[0015]** Other objects and features of the present invention will become apparent from consideration of the following description taken in conjunction with the accompanying drawings.

#### BRIEF DESCRIPTION OF THE DRAWINGS:

45 **[0016]** The invention is herein described, by way of example only, with reference to the accompanying drawings, wherein:

FIGS. 1A-1C are schematic drawings, showing exemplary embodiments of an implant, in accordance with the present invention.

FIG. 2 is a schematic of an exemplary circuit for use as an acoustic switch, in accordance with the present invention.

FIG. 3 is a cross-sectional view of a patient's body, showing a system for communicating with an implant, in accordance with the present invention.

FIG. 4 is a schematic of an external controller for communicating with an implant, such as that shown in FIG. 3, in accordance with the present invention.

FIG. 5 is a schematic of another exemplary embodiment of an implant, in accordance with the present invention.

#### **DESCRIPTION OF THE PREFERRED EMBODIMENTS:**

**[0017]** Turning to the drawings, FIGS. 1A-1C schematically show several exemplary embodiments of an implant 110, 210, 310, in accordance with the present invention. Generally, the implant 110, 210, 310 includes an electrical circuit 112, 212, 312 configured for performing one or more functions or commands when the implant 110, 210, 310 is activated, as described further below. In addition, the implant 110, 210, 310 includes an energy storage device 114 and optionally may include a switch 116 coupled to the electrical circuit 112, 212, 312 and the energy storage device 114. The switch 116 may be activated upon acoustic excitation 100 from an external acoustic energy source (not shown) to allow current flow from the energy storage device 114 to the electrical circuit 112, 212, 312.

**[0018]** In a preferred embodiment, the switch 116 includes an acoustic transducer 118, such as that disclosed in PCT Publication No. WO 99/34,453, published July 8, 1999, or in U.S. application Serial No. 09/888,272, filed June 21, 2001. In addition, the switch 116 also includes a switch circuit 120, such as switch circuit 400 shown in FIG. 2, although alternatively other switches, such as a miniature electromechanical switch and the like (not shown) may be provided. In a further alternative, the acoustic transducer 118 may be coupled to the electrical circuit 112, 212, 312 and/or the energy storage device 114, and the switch circuit 120 may be eliminated.

**[0019]** The energy storage device 114 may be any of a variety of known devices, such as an energy exchanger, a battery and/or a capacitor (not shown). Preferably, the energy storage device 114 is capable of storing electrical energy substantially indefinitely for as long as the acoustic switch 116 remains open, i.e., when the implant 110, 210, 310 is in a "sleep" mode. In addition, the energy storage device 114 may be capable of being charged from an external source, e.g., inductively using acoustic telemetry, as will be appreciated by those skilled in the art. In a preferred embodiment, the energy storage device 114 includes both a capacitor and a primary, non-

rechargeable battery. Alternatively, the energy storage device 114 may include a secondary, rechargeable battery and/or capacitor that may be energized before activation or use of the implant 110, 210, 310.

**[0020]** The implant 110, 210, 310 may be surgically or minimally invasively inserted within a human body in order to carry out a variety of monitoring and/or therapeutic functions. For example, the electrical circuit 112, 212, 312 may include a control circuit 122, 222, 322, a biosensor 124, 224, an actuator 226, 326, and/or a transmitter 128, as explained in application Serial No. 09/690,015. The implant 210, 310 may be configured for providing one or more therapeutic functions, for example, to activate and/or control a therapeutic device implanted within a patient's body, such as an atrial defibrillator or pacemaker, a pain relief stimulator, a neuro-stimulator, a drug delivery device, and/or a light source used for photodynamic therapy. Alternatively, the implant may be used to monitor a radiation dose including ionizing, magnetic and/or acoustic radiation, to monitor flow in a bypass graft, to produce cell oxygenation and membrane electroporation, and the like. In addition or alternatively, the implant 110 may be used to measure one or more physiological parameters within the patient's body, such as pressure, temperature, electrical impedance, position, strain, pH, and the like.

**[0021]** The implant may operate in one of two modes, a "sleep" or "passive" mode when the implant remains dormant and not in use, i.e., when the acoustic switch 116 is open, and an "active" mode, when the acoustic switch 116 is closed, and electrical energy is delivered from the energy storage device 114 to the electrical circuit 112, 212, 312. Alternatively, the implant may operate continuously or intermittently. Because the acoustic switch 116 is open in the sleep mode, there is substantially no energy consumption from the energy storage device 114, and consequently, the implant may remain in the sleep mode virtually indefinitely, i.e., until activated. Thus, an implant in accordance with the present invention may be more energy efficient and, therefore, may require a relatively small energy storage device than implants that continuously draw at least a small amount of current in their "passive" mode.

**[0022]** Turning to FIG. 1A, a first preferred embodiment of an implant 110 is shown in which the electrical circuit 112 includes a control circuit 122, a biosensor 124 coupled to the controller 122, and a transmitter 128 coupled to the control circuit 122. The controller 122 may include circuitry for activating or controlling the biosensor 124, for receiving signals from the biosensor 124, and/or for processing the signals into data, for example, to be transmitted by the transmitter 128. Optionally, the electrical circuit 112 may include memory (not shown) for storing the data. The transmitter 128 may be any device capable of transmitting data from the control circuit 122 to a remote location outside the body, such as an acoustic transmitter, a radio frequency transmitter, and the like. Preferably, the control circuit 122 is coupled to the acous-

tic transducer 118 such that the acoustic transducer 118 may be used as a transmitter 128, as well as a receiver, instead of providing a separate transmitter.

**[0023]** The biosensor 124 may include one or more sensors capable of measuring physiological parameters, such as pressure, temperature, electrical impedance, position, strain, pH, fluid flow, electrochemical sensor, and the like. Thus, the biosensor 124 may generate a signal proportional to a physiological parameter that may be processed and/or relayed by the control circuit 122 to the transmitter 128, which, in turn, may generate a transmission signal to be received by a device outside the patient's body. Data regarding the physiological parameter(s) may be transmitted continuously or periodically until the acoustic switch 116 is deactivated, or for a fixed predetermined time, as will be appreciated by those skilled in the art.

**[0024]** Turning to FIG. 1B, a second preferred embodiment of an implant 210 is shown in which the electrical circuit 212 includes a control circuit 222 and an actuator 226. The actuator 226 may be coupled to a therapeutic device (not shown) provided in or otherwise coupled to the implant 210, such as a light source, a nerve stimulator, a defibrillator, an electrochemical oxidation/reduction electrode, or a valve communicating with an implanted drug reservoir (in the implant or otherwise implanted within in the body in association with the implant).

**[0025]** When the switch 120 is closed, the control circuit 222 may activate the actuator 226 using a pre-programmed protocol, e.g., to complete a predetermined therapeutic procedure, whereupon the switch 120 may automatically open, or the controller 222 may follow a continuous or looped protocol until the switch 120 is deactivated. Alternatively, the acoustic transducer 118 may be coupled to the control circuit 222 for communicating a new or unique set of commands to the control circuit 222. For example, a particular course of treatment for a patient having the implant 210 maybe determined, such as a flow rate and duration of drug delivery, drug activation, drug production, or an energy level and duration of electrical stimulation. Acoustic signals including commands specifying this course of treatment may be transmitted from an external controller (not shown), as described below, to the acoustic switch 116, e.g., along with or subsequent to the activation signal 100. The control circuit 222 may interpret these commands and control the actuator 226 accordingly to complete the course of treatment.

**[0026]** Turning to FIG. 1C, yet another preferred embodiment of an implant 310 is shown in which the electrical circuit 312 includes a control circuit 322, a biosensor 324, and an actuator 326, all of which may be coupled to one another. This embodiment may operate similarly to the embodiments described above, e.g., to obtain data regarding one or more physiological parameters and/or to control a therapeutic device. In addition, once activated, the control circuit 322 may control the actuator 326 in response to data obtained from the biosensor 324 to

control or adjust automatically a course of treatment being provided by a device connected to the actuator 326. For example, the actuator 326 may be coupled to an insulin pump (not shown), and the biosensor 324 may measure glucose levels within the patient's body. The control circuit 322 may control the actuator to open or close a valve on the insulin pump to adjust a rate of insulin delivery based upon glucose levels measured by the biosensor 324 in order to maintain the patient's glucose within a desired range.

**[0027]** Turning to FIG. 2, a preferred embodiment of a switch 400 is shown that may be incorporated into an implant in accordance with the present invention. The switch 400 includes a piezoelectric transducer, or other acoustic transducer (not shown, but generally connected to the switch 400 at locations piezo + and piezo -), a plurality of MOSFET transistors (Q1-Q4) and resistors (R1-R4), and switch S1. A "load" may be coupled to the switch 400, such as one of the electrical circuits described above. In the switch's "sleep" mode, all of the MOSFET transistors (Q1-Q4) are in an off state. To maintain the off state, the gates of the transistors are biased by pull-up and pull-down resistors. The gates of N-channel transistors (Q1, Q3 & Q4) are biased to ground and the gate of P-channel transistor Q2 is biased to +3V. During this quiescent stage, switch S1 is closed and no current flows through the circuit. Therefore, although an energy storage device (not shown, but coupled between the hot post, labeled with an exemplary voltage of +3V, and ground) is connected to the switch 400, no current is being drawn therefrom since all of the transistors are quiescent.

**[0028]** When the acoustic transducer of the implant detects an external acoustic signal, e.g., having a particular frequency, such as the transducer's resonant frequency, the voltage on the transistor Q1 will exceed the transistor threshold voltage of about one half of a volt. Transistor Q1 is thereby switched on and current flows through transistor Q1 and pull-up resistor R2. As a result of the current flow through transistor Q1, the voltage on the drain of transistor Q1 and the gate of transistor Q2 drops from +3V substantially to zero (ground). This drop in voltage switches on the P-channel transistor Q2, which begins to conduct current through transistor Q2 and pull-down resistor R3.

**[0029]** As a result of the current flowing through transistor Q2, the voltage on the drain of transistor Q2 and the gates of transistors Q3 and Q4 increases from substantially zero to +3V. The increase in voltage switches on transistors Q3 and Q4. As a result, transistor Q3 begins to conduct current through resistor R4 and main switching transistor Q4 begins to conduct current through the "load," thereby switching on the electrical circuit.

**[0030]** As a result of the current flowing through transistor Q3, the gate of transistor Q2 is connected to ground through transistor Q3, irrespective of whether or not transistor Q1 is conducting. At this stage, the transistors (Q2, Q3 & Q4) are latched to the conducting state, even if the piezoelectric voltage on transistor Q1 is subsequently

reduced to zero and transistor Q1 ceases to conduct. Thus, main switching transistor Q4 will remain on until switch S1 is opened.

**[0031]** In order to deactivate or open the switch 400, switch S1 must be opened, for example, while there is no acoustic excitation of the piezoelectric transducer. If this occurs, the gate of transistor Q2 increases to +3V due to pull-up resistor R2. Transistor Q2 then switches off, thereby, in turn, switching off transistors Q3 and Q4. At this stage, the switch 400 returns to its sleep mode, even if switch S1 is again closed. The switch 400 will only return to its active mode upon receiving a new acoustic activation signal from the piezoelectric transducer.

**[0032]** It should be apparent to one of ordinary skill in the art that the abode-mentioned electrical circuit is not the only possible implementation of a switch for use with the present invention. For example, the switching operation may be performed using a CMOS circuit, which may draw less current when switched on, an electromechanical switch, and the like.

**[0033]** Turning to FIGS. 3 and 4, a system 410 is shown for communicating with an implant 412, such as one of those described above. Generally, the system 410 includes an external communications device or controller 414, and may include a charger 416, one or more implants 412 (only one shown for simplicity), and an external recorder, computer, or other electronic device 434.

**[0034]** With particular reference to FIG. 4, the external controller 414 may include a processor or other electrical circuit 418 for controlling its operation, and an energy source 420, e.g., a nonrechargeable or a rechargeable battery, coupled to the processor 418 and/or other components of the controller 414, such as a power amplifier (RF) or oscillator (not shown). In addition, the controller 414 may include one or more acoustic transducers 422 that are configured for converting between electrical energy and acoustic energy, similar to those described above. As shown, a single acoustic transducer 422 is provided that may communicate using acoustic telemetry, i.e., capable both of converting electrical energy to acoustic energy to transmit acoustic signals, and converting acoustic energy to electrical energy to receive acoustic signals, as explained further below. Alternatively, separate and/or multiple acoustic transducers may be provided for transmitting and receiving acoustic signals.

**[0035]** In a preferred embodiment, the controller 414 also includes memory 424 coupled to the processor 418, e.g., for storing data provided to the controller 414, as explained further below. The memory 424 may be a temporary buffer that holds data before transfer to another device, or non-volatile memory capable of storing the data substantially indefinitely, e.g., until extracted by the processor 418 or other electronic device. For example, the memory 424 may be a memory card or an eprom (not shown) built into the controller 414 or otherwise coupled to the processor 418. The controller 414 may also include an interface 426, such as a lead or connector, or a transmitter and/or receiver, that may communicate with the

external electronic device, as explained further below.

**[0036]** Preferably, the controller 414 is carried by a patch 415 that may be secured to a patient, e.g., to the patient's skin 92. For example, the patch 415 may include one or more layers of substantially flexible material to which the controller 414 and/or its individual components are attached. The patch 415 may include a single flexible membrane (not shown) to which the controller 414 is bonded or otherwise attached, e.g., using a substantially permanent adhesive, which may facilitate the patch 415 conforming to a patient's anatomy. Alternatively, the controller 414 may be secured between layers of material, e.g., within a pouch or other compartment (not shown) within the patch 415. For example, the patch 415 may include a pair of membranes (not shown) defining the pouch or compartment. The space within which the controller 414 is disposed may be filled with material to acoustically couple the acoustic transducer(s) (formed, for example, from PZT, composite PZT, Quartz, PVDF, and/or other piezoelectric material) of the controller 414 to an outer surface of the patch 415. Alternatively, the acoustic transducer(s) may be exposed, e.g., in a window formed in a wall of the patch 415.

**[0037]** The patch 415 may be formed from a flexible piezoelectric material, such as PVDF or a PVDF copolymer. Such polymers may allow the patch 415 to produce ultrasonic waves, as well as allowing the controller 414 to be secured to the patient's skin 92. Thus, the wall of the patch 415 itself may provide an acoustic transducer for the controller 414, i.e., for transmitting acoustic energy to and/or receiving acoustic energy from the implant 412.

**[0038]** The patch 415 may then be secured to the patient's skin 92 using a material, such as a layer of adhesive (not shown), substantially permanently affixed or otherwise provided on a surface of the patch. The adhesive may be hydrogel, silicon, polyurethane, polyethylene, polypropylene, fluorocarbon polymer, and the like. Alternatively, a separate adhesive may be applied to the patch 415 and/or to the patient's skin 92 before applying the patch 415 in order to secure the controller 414 to the patient's skin 92. Such an adhesive may enhance acoustically coupling of the acoustic transducer(s) of the controller 414 to the patient's skin 92, and consequently to the implant 412 within the patient's body 94. Optionally, additional wetting material, including water, silicone oil, silicone gel, hydrogel, and the like, and/or other acoustically conductive material may be provided between the patch 415 or the acoustic transducer 422, and the patient's skin 92, e.g., to provide substantial continuity and minimize reflection or other losses and/or to secure the patch 415 to the patient.

**[0039]** Alternatively, the controller 414 may be carried by a belt (not shown) that may be secured around the patient, e.g., such that the acoustic transducer 422 is secured against the patient's skin. The belt may carry other components of the system 410, e.g., an external power supply for the controller 414. For example, a battery pack (not shown) may be carried by the belt that may

be coupled to the controller 414 for providing electrical energy for its operation.

**[0040]** The patch 415 may be relatively light and compact, for example, having a maximum surface dimension (e.g., width or height) not more than about ten to two hundred millimeters (10-200 mm), a thickness not more than about five to one hundred millimeters (5-100 mm), and a weight not more than about twenty to four hundred grams (20-400 g), such that the controller 414 may be inconspicuously attached to the patient. Thus, the patient may be able to resume normal physical activity, without substantial impairment from the controller. Yet, the internal energy source of the controller 414 may be sufficiently large to communicate with the implant 412 for an extended period of time, e.g., for hours or days, without requiring recharging or continuous coupling to a separate energy source.

**[0041]** The system 410 may be used to control, energize, and/or otherwise communicate with the implant 412. For example, the controller 414 may be used to activate the implant 412. One or more external acoustic energy waves or signals 430 may be transmitted from the controller 414 into the patient's body 94, e.g., generally towards the location of the implant 412 until the signal is received by the acoustic transducer (not shown in FIGS. 3 and 4) of the implant 412. Upon excitation by the acoustic wave(s) 430, the acoustic transducer produces an electrical output that is used to close, open, or otherwise activate the switch (also not shown in FIGS. 3 and 4) of the implant 412. Preferably, in order to achieve reliable switching, the acoustic transducer of the implant 412 is configured to generate a voltage of at least several tenths of a volt upon excitation that may be used as an activation signal to close the switch, as described above.

**[0042]** As a safety measure against false positives (e.g., erroneous activation for deactivation), the controller 414 may be configured to direct its acoustic transducer 422 to transmit an initiation signal followed by a confirmation signal. When the acoustic transducer of the implant 412 receives these signals, the electrical circuit may monitor the signals for a proper sequence of signals, thereby ensuring that the acoustic switch of the implant 412 only closes upon receiving the proper initiation and confirmation signals. For example, the acoustic switch may only acknowledge an activation signal that includes a first pulse followed by a second pulse separated by a predetermined delay. Use of a confirmation signal may be particularly important for certain applications, for example, to prevent unintentional release of drugs by a drug delivery implant.

**[0043]** In addition to an activation signal, the controller 414 may transmit a second acoustic signal that may be the same as or different than the acoustic wave(s) used to activate the acoustic switch of the implant 412. Thus, the switch may be opened when the acoustic transducer of the implant 412 receives this second acoustic signal, e.g., by the acoustic transducer generating a termination signal in response to the second acoustic signal, in order

to return the implant 412 to its sleep mode.

**[0044]** For example, once activated, the switch may remain closed indefinitely, e.g., until the energy storage device (not shown in FIGS. 3 and 4) of the implant 412 is completely depleted, falls below a predetermined threshold, or until a termination signal is received by the acoustic transducer of the implant 412 from the controller 414. Alternatively, the acoustic switch of the implant 412 may include a timer (not shown), such that the switch remains closed only for a predetermined time, whereupon the switch may automatically open, returning the implant 412 to its sleep mode.

**[0045]** FIG. 5 shows an alternative embodiment of an implant 510 that does not include an acoustic switch. Generally, the implant includes a sensor 512, one or more energy transducers 514, one or more energy storage devices 516, and a control circuit 518, similar to the embodiments described above. The sensor 512 is preferably a pressure sensor for measuring intra-body pressure, such as an absolute variable capacitance type pressure sensor. In alternative embodiments, one or more other sensors may be provided instead of or in addition to a pressure sensor 512. For example, the sensor 512 may include one or more biosensors capable of measuring physiological parameters, such as temperature, electrical impedance, position, strain, pH, fluid flow, and the like. An external controller (not shown), such as that described above, may also be used to communicate with this implant.

**[0046]** Returning to FIG. 3, an external controller 414 in accordance with the present invention preferably has only sufficient power to control its own operation and to communicate with the implant 412. Because of its limited energy requirements, the controller 414 may be relatively small and portable, e.g., may be attached to the patient, while still allowing the patient to engage in normal physical activity. The controller 414 may be used to communicate with the implant 412, e.g., periodically activating or deactivating the implant 412, and/or recording data generated and transmitted by the implant 412. Because it is located outside the patient's body, the controller 414 maybe more easily programmed or reprogrammed than the implant 412 itself, and/or may be repaired or replaced if necessary or desired.

**[0047]** In addition to the external controller 414, the system 410 may include one or more electronic devices 434 that may be coupled to the controller 414 via the interface 426, such as a recorder, a computer, a personal digital assistant, and/or a wireless device, such as a cellular telephone. The electronic device 434 may be directly coupled to the controller 414, by a connector or lead (not shown) extending from the patch 415 within which the controller 414 is provided. Alternatively, the controller 414 and/or patch 415 may include a wireless transmitter and/or receiver (not shown), e.g., a short-range RF transceiver, for communicating with the electronic device 434.

**[0048]** The electronic device 434 may be used to extract data from the memory 424 of the controller 414,

e.g., sensor data and the like, received from the implant 412. This data may be included in a patient database maintained by health care professionals monitoring the patient receiving the implant 412. In addition, the electronic device 434 may be used to program the controller 414, e.g., to program commands, timing sequences, and the like.

**[0049]** The system 410 may also include an external charger 418. For example, the implant 412 may include a rechargeable energy storage device (not shown in FIG. 3), preferably one or more capacitors, that are coupled to the acoustic transducer (also not shown in FIG. 3). The charger 416 may include a probe 428, including an acoustic transducer 430 for contacting a patient's skin 92. The charger 416 also includes a source of electrical energy 432, such as a radio frequency (RF) generator, that is coupled to the acoustic transducer 430. The charger 418 may also include electrical circuits for controlling its operation and buttons or other controls (not shown) for activating and/or deactivating the acoustic transducer 430.

**[0050]** The charger 418 may be used to charge or recharge the implant, e.g., periodically or before each activation. Because the charger 418 includes a substantially more powerful energy source than the controller 414, the charger 418 is generally a relatively bulky device compared to the controller 414, in particular due to the energy generator, which may be stationary or of limited mobility. In addition, the charger 418 may be used to recharge the controller 414 periodically, e.g., by a direct or wireless coupling. Alternatively, the controller 414 and patch 415 may be disposable, e.g., after its energy has been depleted, and replaced with another.

**[0051]** For purposes of comparison, an exemplary charger 416 may need to generate about ten kiloPascals (10 kPa) of acoustic energy for about twenty seconds (20 sec.) in order to fully charge the implant 412. In contrast, an exemplary controller 414 may be limited to outputting relatively smaller bursts of acoustic energy for communicating with, but not charging, the implant 412. Such acoustic signals may have a duration of as little as about one millisecond (1 ms), as opposed to the significantly longer charging signals generated by the charger 416.

**[0052]** The transducer 422 of the controller 414 may consume about one Watt (1 W) of power to produce a 1 kPa acoustic signal for about one millisecond. If the controller 414 communicates with the implant 412 on an hourly basis, the energy source 420 of the controller 418 may only need sufficient capacity to provide 0.024 Watt seconds per day (0.024 W.sec./day). Because of this low energy requirement, the energy source 420, and, consequently, the controller 418, may be relatively compact and portable, as compared to the charger 416. Thus, the energy source 420 may be self-contained within the controller 418, i.e., carried by the patch 415. Alternatively, a portable energy source, e.g., an external battery pack (not shown) may be provided for supplying electrical energy to the controller 418 that may be carried by the pa-

tient, e.g., on a belt (not shown).

**[0053]** In an alternative embodiment, the controller and charger may be provided as a single device (not shown), e.g., including one or more acoustic transducers and/or one or more processors for performing the functions of both devices, as described above. In this embodiment, the implant 412 may operate in a "half-duplex" mode, a quasi-continuous mode, or in a "full-duplex" mode, as described in the applications incorporated above.

**[0054]** It will be appreciated that the above descriptions are intended only to serve as examples, and that many other embodiments are possible within the scope of the present invention as defined by the claims. Aspects of the invention, inter alia, are:

1. A system for activating an implant within a body, comprising:

an external controller for contacting an exterior surface of a patient's body, the controller comprising a first acoustic transducer for transmitting a first acoustic signal into the patient's body, and an energy source for powering the first acoustic transducer; and

an implant for placement within the patient's body, the implant comprising an electrical circuit configured for performing one or more commands when the implant is activated, an energy storage device, a switch coupled to the electrical circuit and the energy storage device, and a second acoustic transducer coupled to the switch, the second acoustic transducer configured for receiving the first acoustic signal from the first acoustic transducer, the switch being closed in response to the first acoustic signal to allow current flow from the energy storage device to the electrical circuit.

2. The system of aspect 1, wherein the first acoustic transducer is configured for transmitting first and second acoustic signals separated by a predetermined delay, and wherein the switch is configured to close only when the second acoustic transducer receives the first and second acoustic signals separated by the predetermined delay.

3. The system of aspect 1, wherein the controller comprises a processor for controlling the first acoustic transducer to transmit one of a first acoustic signal and a second acoustic signal, and wherein the switch is closed when the first acoustic signal is received by the second acoustic transducer, and the switch being opened when the second acoustic signal is received by the second acoustic transducer for discontinuing current flow from the energy storage device to the electrical circuit.

4. The system of aspect 1, wherein the implant further comprises a sensor coupled to the electrical circuit, and wherein the one or more commands comprises measuring a physiological parameter within the body using the sensor. 5
5. The system of aspect 4, wherein the second acoustic transmitter is configured for transmitting a second acoustic signal comprising sensor data indicative of the physiological parameter to the controller, and the first acoustic transducer is configured for receiving the second acoustic signal from the implant. 10
6. The system of aspect 5, wherein the controller further comprises memory for storing the sensor data. 15
7. The system of aspect 5, wherein the controller comprises a processor for extracting the sensor data from the second acoustic signal. 20
8. The system of aspect 5, wherein the controller comprises an interface for transferring the sensor data to an external electronic device separate from the controller. 25
9. The system of aspect 1, further comprising a therapeutic device coupled to the electrical circuit, the electrical circuit being configured for controlling the therapeutic device in response to the physiological parameter measured by the sensor. 30
10. The system of aspect 1, wherein the energy storage device comprises a rechargeable device, and wherein the system further comprises an external charger configured for placement against an exterior surface of the patient's body, the charger comprising a source of electrical energy, and a third acoustic transducer for converting electrical energy from the source of electrical energy into acoustic energy and transmitting a second acoustic signal comprising the acoustic energy into the patient's body. 35
11. The system of aspect 10, wherein the second acoustic transducer is configured for converting the second acoustic signal into electrical energy for recharging the energy storage device. 40
12. The system of aspect 1, further comprising an adhesive for securing the controller to an exterior surface of a patient's body. 45
13. The system of aspect 1, wherein the controller is carried by a patch attachable to the patient's skin. 50
14. The system of aspect 1, wherein the implant further comprises an actuator coupled to the electrical circuit, and wherein the one or more commands comprises activating the actuator to control a therapeutic device coupled to the actuator. 55
15. An apparatus for communicating with an implant located within a patient's body, the implant including one or more acoustic transducers configured for communicating using acoustic telemetry, comprising:
- one or more acoustic transducers for converting between electrical energy and acoustic energy; a controller coupled to the one or more acoustic transducers such that the one or more acoustic transducers are configured for at least one of transmitting acoustic signals to and receiving acoustic signals from within the patient's body to communicate with the implant; an energy storage device for providing electrical energy to at least one of the controller and the one or more acoustic transducers; and means for securing the one or more acoustic transducers to an exterior surface of a patient's body.
16. The apparatus of aspect 15, wherein at least one of the acoustic transducers is configured for receiving acoustic signals from the implant within the patient's body.
17. The apparatus of aspect 16, wherein the one or more acoustic transducers comprise a single acoustic transducer configured for transmitting acoustic signals to and receiving acoustic signals from the implant.
18. The apparatus of aspect 16, wherein the controller comprises a processor for extracting data from acoustic signals received from the implant, and memory for storing the extracted data.
19. The apparatus of aspect 16, wherein the controller comprises an interface for transferring the extracted data to an external electronic device.
20. The apparatus of aspect 19, wherein the interface comprises at least one of a connector, a lead, and a wireless transmitter.
21. The apparatus of aspect 16, wherein the means for securing comprises a flexible membrane carrying the one or more transducers, the controller, and the energy storage device.
22. The apparatus of aspect 21, wherein the flexible membrane comprises a patch attachable to a patient's skin.

23. The apparatus of aspect 21, wherein the flexible membrane comprises a layer of adhesive thereon for securing the flexible membrane to a patient's skin.
24. The apparatus of aspect 16, wherein the means for securing comprises an adhesive. 5
25. The apparatus of aspect 24, wherein the adhesive comprises at least one of hydrogel, silicon, polyurethane, polyethylene, polypropylene, and fluorocarbon polymer. 10
26. The apparatus of aspect 16, further comprising an external charger configured for placement against an exterior surface of the patient's body, the charger comprising a source of electrical energy, and an acoustic transducer for converting electrical energy from the source of electrical energy into acoustic energy and transmitting the acoustic energy into the patient's body for energizing an energy storage device in the implant. 15
27. A method for communicating with an implant located within a patient's body, the implant comprising an acoustic transducer configured for communicating using acoustic telemetry, the method comprising: 20
- securing a portable communications device in contact with an exterior surface of the patient's body, the communications device comprising one or more acoustic transducers, and an energy storage device for providing electrical energy to operate the communications device; and communicating with the implant using the one or more acoustic transducers. 25
28. The method of aspect 27, wherein the communicating step comprises transmitting one or more acoustic signals from the communications device into the patient's body, the one or more acoustic signals comprising a command for controlling operation of the implant. 30
29. The method of aspect 28, wherein the command comprises measuring a physiological parameter within the body. 45
30. The method of aspect 28, wherein the command comprises controlling a therapeutic device coupled to the implant. 50
31. The method of aspect 27, wherein the communicating step comprises receiving one or more acoustic signals from the implant, the one or more acoustic signals comprising data indicative of a physiological parameter measured by the implant. 55
32. The method of aspect 31, further comprising extracting data from the one or more acoustic signals received from the implant.
33. The method of aspect 32, further comprising storing the extracted data in memory of the communications device.
34. The method of aspect 32, further comprising transferring the extracted data to an electronic device external to the patient's body.
35. The method of aspect 31, further comprising charging the energy storage device with an energy source located outside the patient's body.
36. The method of aspect 34, wherein the energy source comprises a charger that is separate from the communications device.
37. The method of aspect 27, wherein the communications device comprises a patch carrying the one or more acoustic transducers, and wherein the securing step comprises securing the patch to the exterior surface of the patient's body.
38. The method of aspect 37, wherein the one or more acoustic transducers are acoustically coupled to the patient's body when the patch is secured to the exterior surface of the patient's body.

## Claims

1. A system for activating an implant (110, 210, 310, 412) within a patient's body, comprising:

An external controller (414) including a first acoustic transducer (422) for transmitting acoustic signals into the patient's body; an implant (110, 210, 310, 412) for placement within the patient's body, the implant (110, 210, 310, 412) comprising a sensor, an electrical circuit (112, 212, 312) including a control circuit (122, 222, 322) configured for performing one or more commands when the implant is activated, an energy storage device (114), and a second acoustic transducer (118) configured for receiving acoustic signals from the first acoustic transducer (422); **characterised in that** the implant further includes a switch (120) coupled to the second transducer (118), the control circuit (122, 222, 322) and the energy storage device (114), the switch (120) actuatable from an open position to a closed position to allow current flow from the energy storage device (114) to the electrical circuit (112, 212, 312) and activate the implant in response to an acoustic activation command

- transmitted by the external controller (414), and wherein the external controller (414) is configured to acoustically transmit at least one command to the implant following the acoustic activation command.
2. The system of claim 1, wherein the activation command comprises a first acoustic signal followed by a second acoustic signal transmitted from the first acoustic transducer.
3. The system of claim 2, wherein the first and second acoustic signals transmitted from the first acoustic transducer (422) are separated by a predetermined delay, and wherein the switch (120) is configured to close only when the second acoustic transducer (118) receives the first and second acoustic signals separated by the predetermined delay.
4. The system of claim 2, wherein the first acoustic signal comprises an activation signal and wherein the second acoustic signal comprises a confirmation signal.
5. The system of claim 1, wherein the switch (120) is configured to open in response to a deactivation command received by the second acoustic transducer.
6. The system of claim 1, wherein the second acoustic transducer (118) is configured for transmitting an acoustic signal comprising implant data, and the first acoustic transducer (422) is configured for receiving the acoustic signal transmitted from the implant(110, 210, 310, 412).
7. The system of claim 6, wherein the external controller (414) comprises an interface for transferring the implant data to an external electronic device separate from the external controller (414).
8. The system of claim 1, further comprising a therapeutic device coupled to the control circuit (122, 222, 322), the control circuit (122, 222, 322) being configured for controlling the therapeutic device in response to a physiological parameter measured by the sensor.
9. The system of claim 1, wherein the energy storage (114) comprises a rechargeable device, and wherein the system further comprises an external charger configured for placement against an exterior surface of the patient's body, the charger comprising a source of electrical energy, and a third acoustic transducer for converting electrical energy from the source of electrical energy into acoustic energy and transmitting a second acoustic signal comprising the acoustic energy into the patient's body.
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10. The system of claim 1, wherein the second acoustic transducer(118) is configured for converting the second acoustic signal into electrical energy for recharging the energy storage device (114).
- 10
11. The system of claim 1, wherein the implant (110, 210, 310, 412)further comprises an actuator coupled to the control circuit , and wherein the one or more commands comprises activating the actuator to control a therapeutic device coupled to the actuator.
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12. The system of claim 1, wherein the implant (110, 210, 310, 412) consumes substantially no energy when the switch (120) is open.
13. A method for communicating with one or more implants (110, 210, 310, 412) located within a patient's body, at least one implant (110, 210, 310, 412) comprising an acoustic implant transducer configured for communicating using acoustic telemetry and a switch (120), said switch (120) being coupled to the acoustic implant transducer (118) and an energy storage device (114) of the at least one implant, wherein the switch (120) is configured to actuate the at least one implant between a sleep mode, in which current is limited from flowing from the energy storage device (114) of the at least one implant to an electrical circuit (112, 212, 312) of the implant including a control circuit (122, 222, 322), and an active mode, in which current flows from the energy storage device (114) of the at least one implant to the electrical circuit (112, 212, 312), the method comprising:
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- placing a portable external controller (414) adjacent to an exterior surface of the patient's body, the external controller (414) comprising one or more acoustic transducers (422), and an energy storage device for providing electrical energy to operate the external controller (414); transmitting an acoustic control signal into the patient's body and communicating with the at least one implant using the one or more acoustic transducers (422), the acoustic control signal adapted to activate said switch (120); and wherein communicating with the at least one implant includes transmitting one or more acoustic signals from the external controller (414) into the patient's body, the one or more acoustic signals including a command for controlling an operation of the at least one implant (110, 210, 310, 412).
14. The method of claim 13, wherein the one or more acoustic transducers (422) of the external controller (414) are configured for transmitting first and second acoustic control signals separated by a predetermined delay.

15. The method of claim 13, wherein upon receiving an acoustic control signal from the external controller (414), the acoustic implant transducer closes the switch (120) to allow electrical energy to flow from the energy storage device of the at least one implant to power the at least one implant (110, 210, 310, 412).

### Patentansprüche

1. System zum Aktivieren eines Implantats (110, 210, 310, 412) innerhalb des Körpers eines Patienten, welches aufweist:

eine externe Steuervorrichtung (414), die einen ersten akustischen Wandler (422) zum Senden akustischer Signale in den Körper des Patienten enthält;  
ein Implantat (110, 210, 310, 412) für die Anordnung innerhalb des Körpers des Patienten, welches Implantat (110, 210, 310, 412) einen Sensor, eine elektrische Schaltung (112, 212, 312) enthaltend eine Steuerschaltung (122, 222, 322), die zum Ausführen eines oder mehrerer Befehle, wenn das Implantat aktiviert ist, konfiguriert ist, eine Energiespeichervorrichtung (114) und einen zweiten akustischen Wandler (118), der zum Empfangen akustischer Signale von dem ersten akustischen Wandler (422) konfiguriert ist, aufweist,

**dadurch gekennzeichnet, dass**

das Implantat weiterhin einen Schalter (120) enthält, der mit dem zweiten Wandler (118), der Steuerschaltung (122, 222, 322) und der Energiespeichervorrichtung (114) gekoppelt ist, wobei der Schalter (120) aus einer geöffneten Position in eine geschlossene Position betätigbar ist, um zu ermöglichen, dass Strom von der Energiespeichervorrichtung (114) zu der elektrischen Schaltung (112, 212, 312) fließt, und das Implantat als Antwort auf einen akustischen Aktivierungsbefehl, der von der externen Steuervorrichtung (414) gesendet wurde, aktiviert, und wobei die externe Steuervorrichtung (414) konfiguriert ist zum akustischen Senden von zumindest einem Befehl zu dem Implantat folgend dem akustischen Aktivierungsbefehl.

2. System nach Anspruch 1, bei dem der Aktivierungsbefehl ein erstes akustisches Signal gefolgt von einem von dem ersten akustischen Wandler gesendeten zweiten akustischen Signal aufweist.
3. System nach Anspruch 2, bei dem das erste und das zweite akustische Signal, die von dem ersten akustischen Wandler (422) gesendet wurden, durch eine vorbestimmte Verzögerung getrennt sind, wobei der

5 Schalter (120) konfiguriert ist, nur dann zu schließen, wenn der zweite akustische Wandler (118) das erste und das zweite akustische Signal, die durch die vorbestimmte Verzögerung getrennt sind, empfängt.

4. System nach Anspruch 2, bei dem das erste akustische Signal ein Aktivierungssignal aufweist und das zweite akustische Signal ein Bestätigungssignal aufweist.
5. System nach Anspruch 1, bei dem der Schalter (120) konfiguriert ist, als Antwort auf einen von dem zweiten akustischen Wandler empfangenen Deaktivierungsbefehl zu öffnen.
6. System nach Anspruch 1, bei dem der zweite akustische Wandler (118) konfiguriert ist zum Senden eines Implantationsdaten aufweisenden akustischen Signals und der erste akustische Wandler (422) konfiguriert ist zum Empfangen des von dem Implantat (110, 210, 310, 412) gesendeten akustischen Signals.
7. System nach Anspruch 6, bei dem die externe Steuervorrichtung (414) eine Schnittstelle zum Übertragen der Implantatdaten zu einer externen elektronischen Vorrichtung, die von der externen Steuervorrichtung (414) getrennt ist, aufweist.
8. System nach Anspruch 1, weiterhin aufweisend eine therapeutische Vorrichtung, die mit der Steuerschaltung (122, 222, 322) gekoppelt ist, wobei die Steuerschaltung (122, 222, 322) konfiguriert ist, die therapeutische Vorrichtung als Antwort auf einen von dem Sensor gemessenen physiologischen Parameter zu steuern.
9. System nach Anspruch 1, bei dem der Energiespeicher (114) eine wiederaufladbare Vorrichtung aufweist, wobei das System weiterhin eine externe Ladevorrichtung, die zum Anordnen auf einer äußeren Oberfläche des Körpers des Patienten konfiguriert ist, welche Ladevorrichtung eine Quelle für elektrische Energie aufweist, und einen dritten akustischen Wandler zum Umwandeln von elektrischer Energie von der elektrischen Energiequelle in akustische Energie und zum Senden eines zweiten akustischen Signals, das die akustische Energie aufweist, in den Körper des Patienten aufweist.
10. System nach Anspruch 1, bei dem der zweite akustische Wandler (118) konfiguriert ist zum Umwandeln des zweiten akustischen Signals in elektrische Energie zum Wiederaufladen der Energiespeichervorrichtung (114).
11. System nach Anspruch 1, bei dem das Implantat (110, 210, 310, 412) weiterhin einen Aktuator auf-

weist, der mit der Steuerschaltung gekoppelt ist, wobei der eine oder die mehreren Befehle das Aktivieren des Aktuators zum Steuern einer mit dem Aktuator gekoppelten therapeutischen Vorrichtung aufweisen.

12. System nach Anspruch 1, bei dem das Implantat (110, 210, 310, 412) im Wesentlichen keine Energie verbraucht, wenn der Schalter (120) geöffnet ist.

13. Verfahren zum Kommunizieren mit einem oder mehreren Implantaten (110, 210, 310, 412), die sich innerhalb des Körpers eines Patienten befinden, wobei zumindest ein Implantat (110, 210, 310, 412) einen akustischen Implantatwandler, der konfiguriert ist zum Kommunizieren unter Verwendung von akustischer Telemetrie, und einen Schalter (120) aufweist, welcher Schalter (120) mit dem akustischen Implantatwandler (118) und einer Energiespeichervorrichtung (114) des zumindest einen Implantats gekoppelt ist, wobei der Schalter (120) konfiguriert ist zum Betätigen des zumindest einen Implantats zwischen einem Ruhemodus, in welchem von der Energiespeichervorrichtung (114) des zumindest einen Implantats zu einer elektrischen Schaltung (112, 212, 312) des Implantats enthaltend eine Steuerschaltung (122, 222, 322) fließender Strom begrenzt ist, und einem aktiven Modus, in welchem Strom von der Energiespeichervorrichtung (114) des zumindest einen Implantats zu der elektrischen Schaltung (112, 212, 312) fließt, welches Verfahren aufweist:

Anordnen einer tragbaren externen Steuervorrichtung (414) angrenzend an eine äußere Oberfläche des Körpers des Patienten, wobei die externe Steuervorrichtung (414) einen oder mehrere akustische Wandler (422) und eine Energiespeichervorrichtung zum Bereitstellen von elektrischer Energie zur Betätigung der externen Steuervorrichtung (414) aufweist; Senden eines akustischen Steuersignals in den Körper des Patienten und Kommunizieren mit dem zumindest einen Implantat unter Verwendung des einen oder der mehreren akustischen Wandler (422), wobei das akustische Steuersignal ausgestaltet ist zum Aktivieren des Schalters (120); und wobei das Kommunizieren mit dem zumindest einen Implantat das Senden von einem oder mehreren akustischen Signalen von der externen Steuervorrichtung (414) in den Körper des Patienten enthält und dass eine oder die mehreren akustischen Signale einen Befehl zum Steuern einer Operation des zumindest einen Implantats (110, 210, 310, 412) enthalten.

14. Verfahren nach Anspruch 13, bei dem der eine oder

die mehreren akustischen Wandler (422) der externen Steuervorrichtung (414) konfiguriert sind zum Senden eines ersten und eines zweiten akustischen Steuersignals, die durch eine vorbestimmte Verzögerung getrennt sind.

15. Verfahren nach Anspruch 13, bei dem bei Empfang eines akustischen Steuersignals von der externen Steuervorrichtung (414) der akustische Implantatwandler den Schalter (120) schließt, um zu ermöglichen, dass elektrische Energie von der Energiespeichervorrichtung des zumindest einen Implantats fließt, um das zumindest eine Implantat (110, 210, 310, 412) zu versorgen.

## Revendications

1. Système pour activer un implant (110, 210, 310, 412) à l'intérieur du corps d'un patient, comprenant :

un contrôleur externe (414) incluant un premier transducteur acoustique (422) pour transmettre des signaux acoustiques à l'intérieur du corps du patient ;

un implant (110, 210, 310, 412) destiné à être positionné à l'intérieur du corps du patient, l'implant (110, 210, 310, 412) comprenant un capteur, un circuit électrique (112, 212, 312) incluant un circuit de commande (122, 222, 322) configuré pour réaliser une ou plusieurs commande(s) lorsque l'implant est activé, un dispositif de stockage d'énergie (114) et un second transducteur acoustique (118) configuré pour recevoir des signaux acoustiques en provenance du premier transducteur acoustique (422), **caractérisé en ce que** l'implant inclut en outre un commutateur (120) couplé au second transducteur acoustique (118), au circuit de commande (122, 222, 322) et au dispositif de stockage d'énergie (114), le commutateur (120) pouvant être actionné depuis une position ouverte jusqu'à une position fermée pour permettre la circulation d'un courant depuis le dispositif de stockage d'énergie (114) jusqu'au circuit électrique (112, 212, 312) et pour activer l'implant en réponse à une commande d'activation acoustique transmise par le contrôleur externe (414), et dans lequel :

le contrôleur externe (414) est configuré de manière à transmettre au moins une commande à l'implant suite à la commande d'activation acoustique.

2. Système selon la revendication 1, dans lequel la commande d'activation comprend un premier signal acoustique suivi par un second signal acoustique

- transmis depuis le premier transducteur acoustique.
3. Système selon la revendication 2, dans lequel les premier et second signaux acoustiques transmis depuis le premier transducteur acoustique (422) sont séparés par un retard prédéterminé, et dans lequel le commutateur (120) est configuré de manière à être fermé seulement lorsque le second transducteur acoustique (118) reçoit les premier et second signaux acoustiques séparés par le retard prédéterminé. 10
4. Système selon la revendication 2, dans lequel le premier signal acoustique comprend un signal d'activation et dans lequel le second signal acoustique comprend un signal de confirmation. 15
5. Système selon la revendication 1, dans lequel le commutateur (120) est configuré de manière à être ouvert en réponse à une commande de désactivation reçue par le second transducteur acoustique. 20
6. Système selon la revendication 1, dans lequel le second transducteur acoustique (118) est configuré de manière à transmettre un signal acoustique comprenant des données d'implant, et le premier transducteur acoustique (422) est configuré de manière à recevoir le signal acoustique transmis depuis l'implant (110, 210, 310, 412). 25
7. Système selon la revendication 6, dans lequel le contrôleur externe (414) comprend une interface pour transférer les données d'implant à un dispositif électronique externe séparé du contrôleur externe (414). 30
8. Système selon la revendication 1, comprenant en outre un dispositif thérapeutique couplé au circuit de commande (122, 222, 322), le circuit de commande (122, 222, 322) étant configuré de manière à commander le dispositif thérapeutique en réponse à un paramètre physiologique mesuré par le capteur. 40
9. Système selon la revendication 1, dans lequel le dispositif de stockage d'énergie (114) comprend un dispositif rechargeable, et dans lequel le système comprend en outre un chargeur externe configuré de manière à pouvoir être positionné contre une surface extérieure du corps du patient, le chargeur comprenant une source d'énergie électrique, et un troisième transducteur électrique pour convertir l'énergie électrique en provenance de la source d'énergie électrique en une énergie acoustique et pour transmettre un second signal acoustique comprenant l'énergie acoustique à l'intérieur du corps du patient. 45
10. Système selon la revendication 1, dans lequel le second transducteur acoustique (118) est configuré de manière à convertir le second signal acoustique en 50
- énergie électrique pour recharger le dispositif de stockage d'énergie (114).
11. Système selon la revendication 1, dans lequel l'implant (110, 210, 310, 412) comprend en outre un actionneur couplé au circuit de commande, et dans lequel les une ou plusieurs commande(s) comprennent l'activation de l'actionneur afin de commander un dispositif thérapeutique couplé à l'actionneur. 55
12. Système selon la revendication 1, dans lequel l'implant (110, 210, 310, 412) ne consomme sensiblement pas d'énergie lorsque le commutateur (120) est ouvert.
13. Procédé pour communiquer avec un ou plusieurs implant(s) (110, 210, 310, 412) positionné(s) à l'intérieur du corps d'un patient, au moins un implant (110, 210, 310, 412) comprenant un transducteur d'implant acoustique configuré de manière à communiquer en utilisant une télémétrie acoustique et un commutateur (120), ledit commutateur (120) étant couplé au transducteur d'implant acoustique (118) et à un dispositif de stockage d'énergie (114) de l'au moins un implant, dans lequel le commutateur (120) est configuré de manière à actionner l'au moins un implant entre un mode sommeil, dans lequel le courant est limité en termes de circulation depuis le dispositif de stockage d'énergie (114) de l'au moins un implant jusqu'à un circuit électrique (112, 212, 312) de l'implant incluant un circuit de commande (122, 222, 322), et un mode actif dans lequel le courant circule depuis le dispositif de stockage d'énergie (114) de l'au moins un implant jusqu'au circuit électrique (112, 212, 312), le procédé comprenant :
- le positionnement d'un contrôleur externe portable (414) de telle sorte qu'il soit adjacent à une surface extérieure du corps du patient, le contrôleur externe (414) comprenant un ou plusieurs transducteur(s) acoustique(s) (422), et un dispositif de stockage d'énergie pour fournir de l'énergie électrique afin de faire fonctionner le contrôleur externe (414) ;
- la transmission d'un signal de commande acoustique à l'intérieur du corps du patient et la communication avec l'au moins un implant en utilisant les un ou plusieurs transducteur(s) acoustique(s) (422), le signal de commande acoustique étant adapté pour activer ledit commutateur (120) ; et dans lequel :
- la communication avec l'au moins un implant inclut la transmission d'un signal acoustique ou de plusieurs signaux acoustiques en provenance du contrôleur externe (414) à l'intérieur du corps du patient, les un ou plusieurs signaux acoustiques in-

cluant une commande pour commander un fonctionnement de l'au moins un implant (110, 210, 310, 412).

- 14.** Procédé selon la revendication 13, dans lequel les un ou plusieurs transducteurs acoustiques (422) du contrôleur externe (414) sont configurés de manière à transmettre des premier et second signaux de commande acoustiques séparés par un retard pré-déterminé. 5

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- 15.** Procédé selon la revendication 13, dans lequel, suite à la réception d'un signal de commande acoustique en provenance du contrôleur externe (414), le transducteur d'implant acoustique ferme le commutateur (120) pour permettre la circulation de l'énergie électrique depuis le dispositif de stockage d'énergie de l'au moins un implant pour alimenter l'au moins un implant (110, 210, 310, 412). 15

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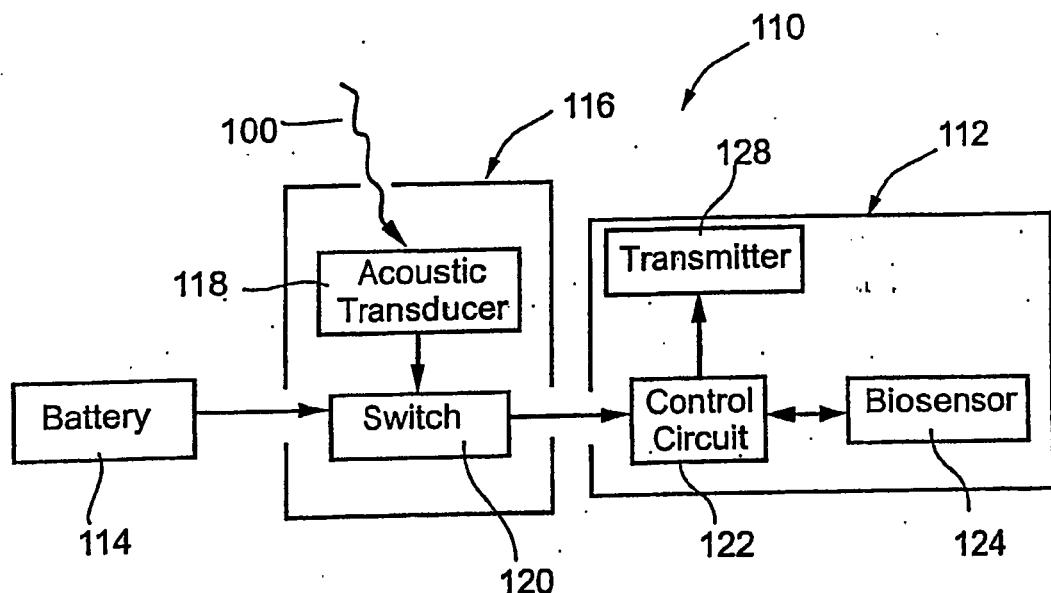


Fig. 1A

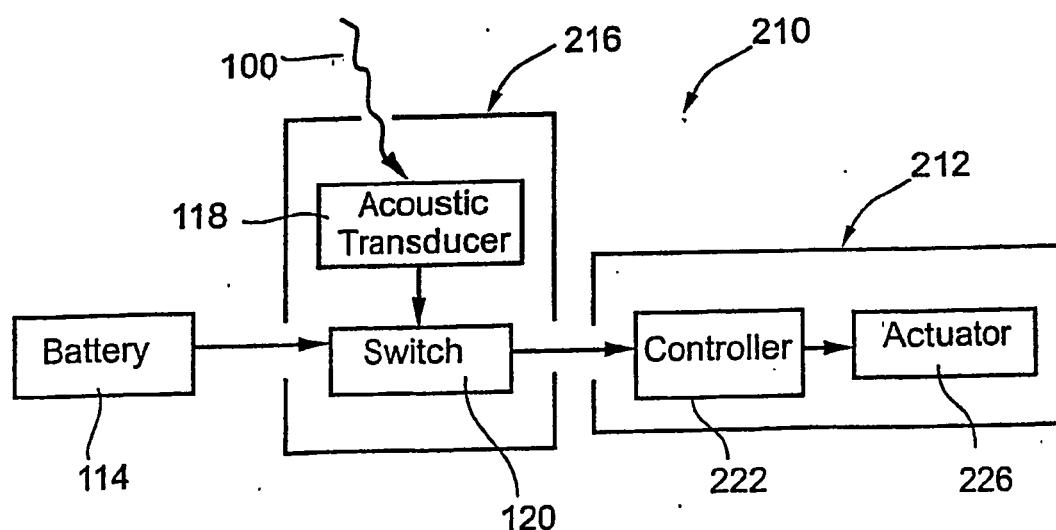


Fig. 1B

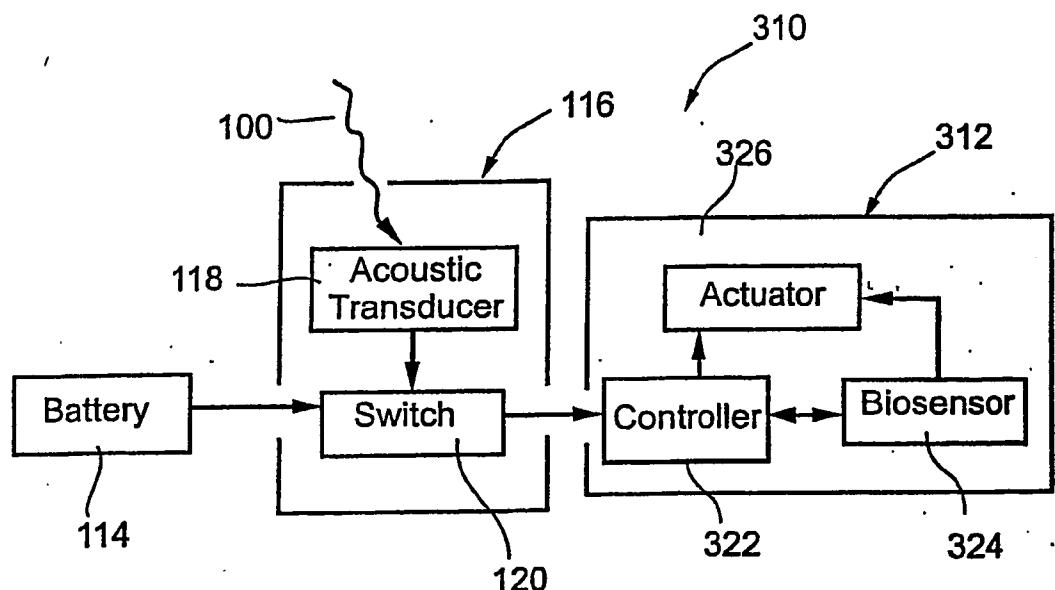


Fig. 1C

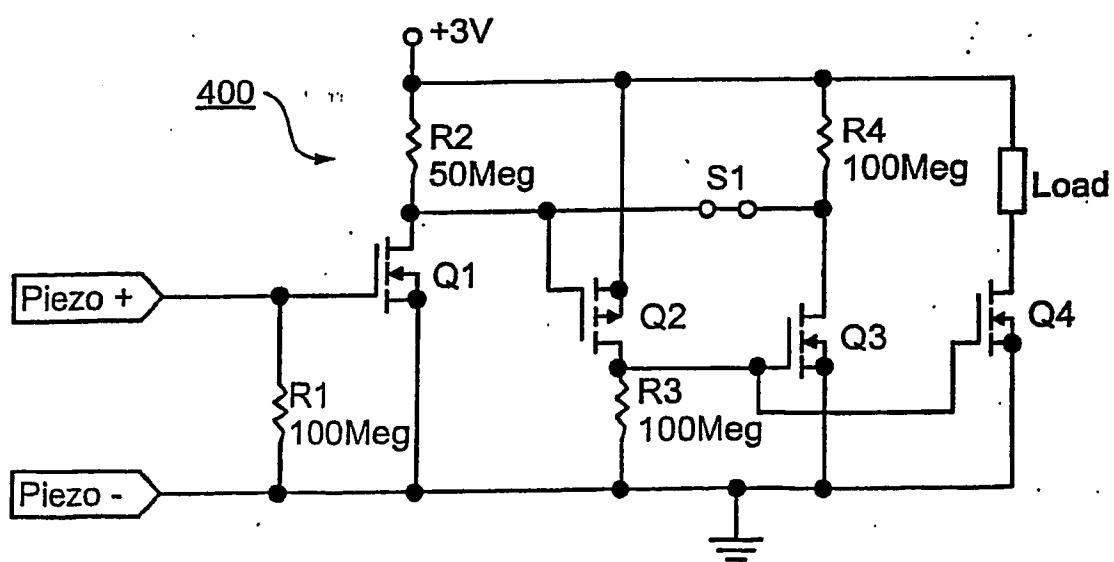
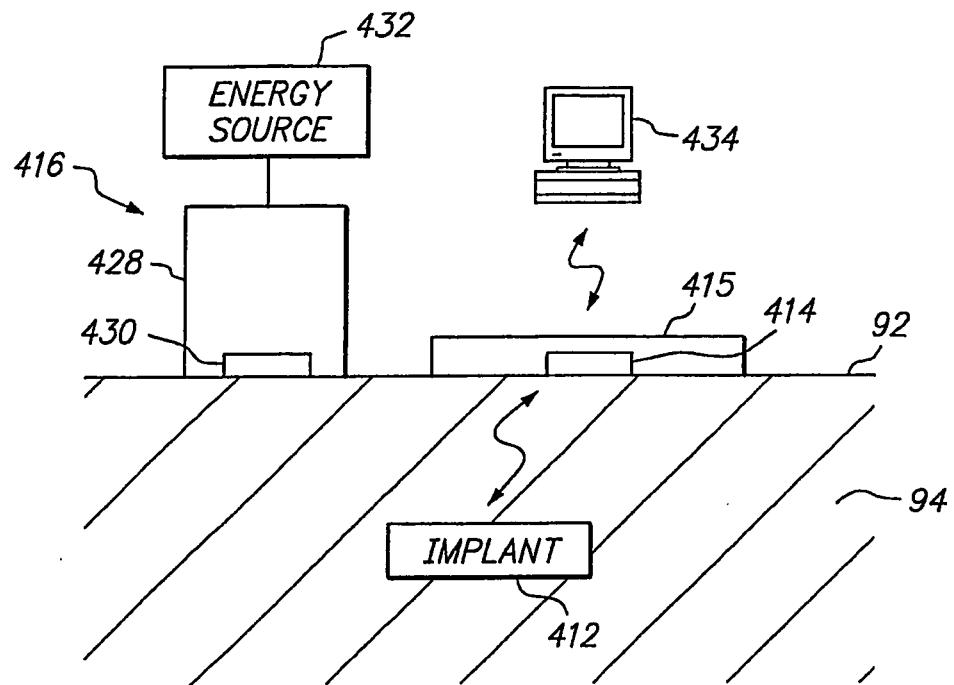
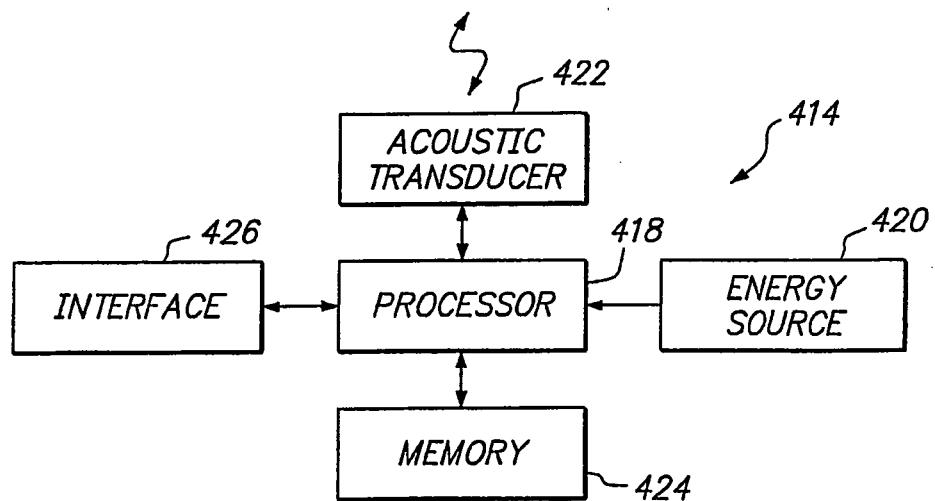


Fig. 2



**FIG. 3**



**FIG. 4**

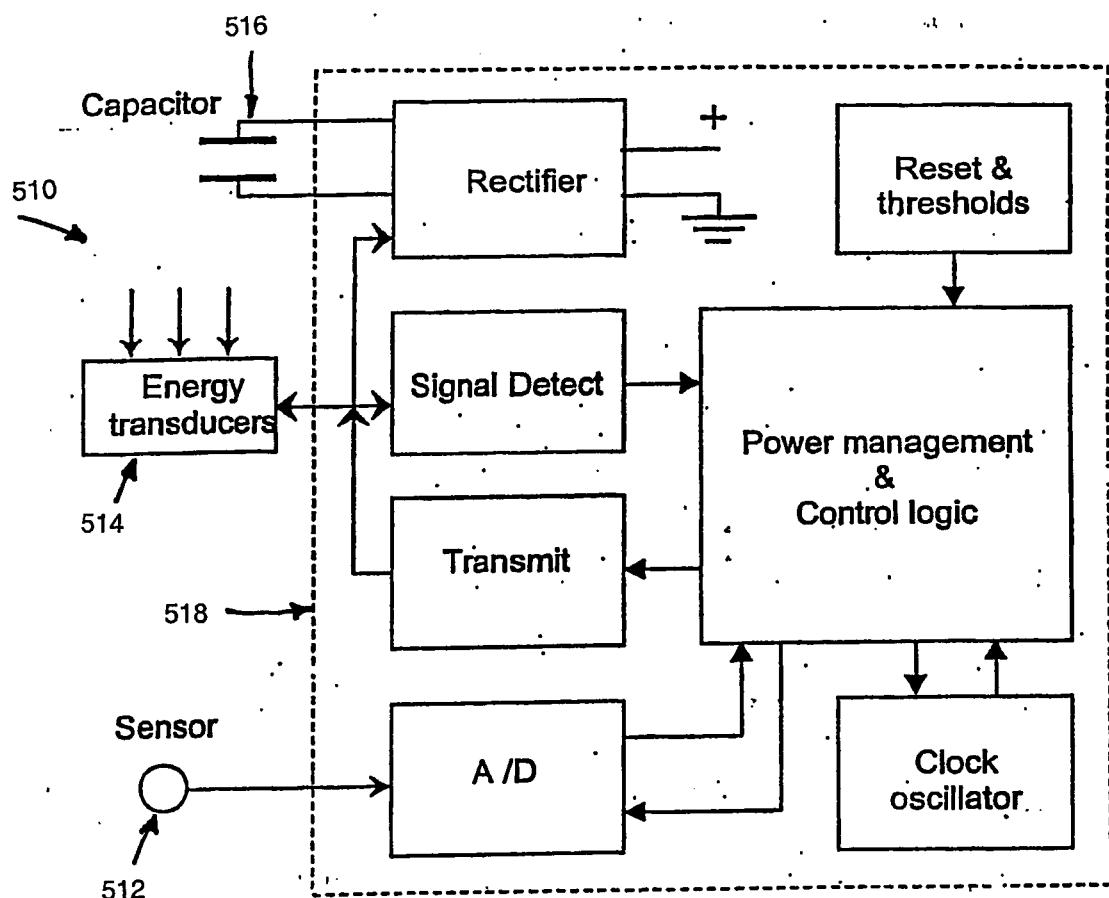


Fig. 5

**REFERENCES CITED IN THE DESCRIPTION**

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IPC分类号	A61N1/08 A61N1/378 A61B5/00 A61B5/02 A61B5/0215 A61B5/07 A61B5/11 A61B8/00 A61B5/145 A61N1/372 A61B5/103 A61M37/00 A61N1/34 A61N1/36		
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优先权	10/989912 2001-11-19 US		
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外部链接	<a href="#">Espacenet</a>		

### 摘要(译)

使用声学遥测技术与患者体内的植入物通信的系统和方法包括可附接到患者皮肤的外部通信设备。该装置包括声换能器，用于将声信号传输到患者体内和/或用于从植入物接收声信号。该装置包括用于提供电能以操作该装置的电池，用于从植入物接收的声信号中提取数据的处理器，以及用于存储数据的存储器。该装置可以包括用于与记录器或计算机通信的接口，例如，从植入物传输数据和/或接收用于控制植入物的指令。该装置固定到患者的皮肤上，用于控制，监测或以其他方式与植入物通信，同时允许患者保持活动。

