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(54) METHOD AND APPARATUS FOR DETERMINING CEREBRAL OXYGEN SATURATION

VERFAHREN UND GERÄT ZUR BESTIMMUNG DER ZEREBRALEN SAUERSTOFFSÄTTIGUNG

METHODE ET DISPOSITIF DESTINES A DETERMINER LA SATURATION EN OXYGENE
CEREBRAL

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Description**BACKGROUND OF THE INVENTION**

[0001] In the first above-identified previously filed patent application, a new concept is disclosed for determining the state of hemoglobin oxygen saturation in brain tissue, particularly fetal brain tissue, that is especially useful during the critical time of childbirth. Basically, this approach utilizes the concept of injecting a very short pulse of light at a selected wavelength in the near-infrared range (e.g. one nanosecond (ns) in length) into the head via a fiberoptic cable optically coupled to the head, detecting the corresponding photons emerging from the head into an adjacent detector and fiberoptic cable after a first very short period (e.g., one ns) and then detecting emerging photons once again after at least one more very brief period (on the order of 4 to 5ns).

[0002] The injected pulse of photons (sometimes referred to as a "bolus") spreads out from the injection site in the form of a rapidly expanding "glowball," due to the extensive amount of scatter which occurs in this medium (on average, photon direction becoming completely randomized after only 0.6mm of travel), and this translates into photon pathlength. Therefore, the detection of differing amounts of photons leaving the head at different relatively short intervals corresponding to photon travel over different effective pathlengths within the brain, which represents, and characterizes, differing depths of photon travel within the brain tissue. Thus, the quantities of photons detected at different intervals in effect sample different depths of travel, and hence different volumes of brain tissue. As a result, mathematical processing and correlation of these differential results will be directly indicative of differing amounts of photon absorption at different depths, including the amount of photon reduction which results (for example) from absorption by hemoglobin molecules. By using selected wavelengths of injected light, the amount of hemoglobin oxygenation can thus be determined, due to the difference in oxygen absorption as opposed to reduced or non-oxygenated hemoglobin, on a wavelength-specific basis.

[0003] The aforementioned U.S. Patent No. 6,381,480 discloses this technological concept in considerably greater detail, together with representative and then-contemplated preferred embodiments of apparatus and methodology for implementing the concept to create a useful fetal cerebral oximeter. As may be seen by further study of that patent, it will be seen that the disclosed apparatus basically includes a source of photons coupled to the head by a fiberoptic conductor which leads to an injection site (e.g., the forehead), plus a fiberoptic leading from a photon detection device that basically comprises at least two shuttered detectors which are gated open for a very brief period (on the order of 1ns) at specific time intervals after the instant of injection, preferably by using a trigger signal obtained from a fiberoptic conductor that transmits a small fraction of the photons emitted by the source to the shuttered detectors at different and specifically timed intervals.

[0004] US-A-5770454 discloses a device in which two different light paths lead to an optical switch.

SUMMARY OF THE INVENTION

[0005] The present invention comprises a new and improved method and apparatus for determining cerebral oxygenation based on the underlying concept of the aforementioned earlier patent, obtained by way of a novel implementation of such concept, and this forms the basis of the present patent, in which a disclosure is provided for a preferred embodiment of such implementation.

[0006] In one basic aspect, the present invention recognizes and provides a new processing methodology for oxygenation determination, in particular cerebral oxygenation as briefly noted above, based on the apprehension and discovery that time-based photon quantity determinations of the wavelength-specific light leaving the head of the patient may be significantly improved, and simplified, by determining the quantity of returning photons in at least one set of two different but closely spaced points in time following the instant of injection, and then taking the ratio of the determinations in each set, to thereby cancel and remove several important sources of error.

[0007] Furthermore, and in a more particular sense, the invention provides a novel and advantageous implementation of the methodology just described, by which the detection equipment is simplified and certain components shown in the implementation of U.S. Patent No. 6,381,480 eliminated, thereby providing substantial economies of manufacture, with related reduction of costs to users of the technology.

BRIEF DESCRIPTION OF THE DRAWINGS**[0008]**

Fig. 1 is a block diagram of the basic system and equipment disclosed in the aforementioned prior and related patent, corresponding to Fig. 3 thereof;

Fig. 2 is an enlarged representation of an image intensifier as shown in the aforementioned prior and related patent,

corresponding to Fig. 4 thereof;

Fig. 3 is a simplified system block diagram illustrating a detection system in accordance with the present invention;

Fig. 4 is an enlarged, simplified drawing showing the image intensifier portion of the shutter detector, as utilized in accordance with the invention;

Fig. 5 is a schematic block diagram showing a preferred and more detailed embodiment of the present invention; and

Fig. 6 is a pictorial view showing an exemplary visual display for use in operating the system.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0009] Inasmuch as an understanding of the present invention requires an understanding of the invention disclosed in the aforementioned prior related patent of the present inventors, Fig. 1 herein depicts the overall system of a preferred embodiment then contemplated, and an abbreviated commentary with respect thereto follows.

[0010] A very short (on the order of 1ns) pulse of photons at a selected wavelength in the near infrared range is provided by a source 10 and is conducted to the head ("HEAD") of the patient (fetus) by a fiberoptic cable 42 (photon travel designated "I" and shown with an arrow), and resulting photons exiting the head at brief intervals after that are detected at a point closely adjacent the point of entry at two (or more) closely spaced points in time (for example, on the order of 4ns and 5ns after injection). These detected photons are then coupled to a photon detection apparatus 20 that includes at least first and second shuttered detectors 22 and 24, via a receiving fiberoptic cable 44 (labeled "O"), after passing through a lens 28, partially reflecting mirrors 30 and 38, an auxiliary shutter 32, and a fluorescence-blocking filter 34. The total flow of photons exiting the head via cable 44 is monitored by a photodiode detector 26, to which a small fraction of such light is directed by partially reflecting mirror 38. Shuttered detectors 22 and 24 are gated open by a small amount of the light from source 12, via fiberoptic cables 46 and 48, which are accurately cut to precise lengths that will provide the desired time delay for sampling the exiting photon stream after the instant of injection.

[0011] Accordingly, the shuttered detectors 22 and 24 provide outputs which represent the amount of photons exiting the head at the corresponding points in time, and by choosing wavelengths which are selectively absorbed by oxygenated and reduced hemoglobin, a precise and accurate determination of cerebral oxygenation may be obtained. In this regard, the longer the time delay from the instant of insertion, the deeper the photons will travel within the brain due to the effects of scatter, as noted above. Therefore, the longer this duration (and deeper the extent of travel), the more absorption these photons will incur before they exit the brain and skull, *etc.* For these reasons, it may be advantageous to implement more than one of the longer periods of delay, and also to utilize an alternating wavelength set, since this enables the determination of oxygenation with attendant suppression of subject-dependent parameters and variations in skin contact.

[0012] The aforementioned shuttered detectors 22 and 24 must be very fast-acting, going from completely off to completely on in about 1ns, or less. Errors in turn-on relative to the instant of pulse injection cannot be tolerated even if amounting only to a few nanoseconds (*i.e.*, one or more). A satisfactory shutter and detector can be implemented by using a fast, linear, focused-dynode PMT; however, in a preferred first embodiment, an image-intensifier of the type widely used in night-vision devices was utilized with good results, and a schematic cross section of a typical proximity-focused such image intensifier, as utilized in the earlier patent, is illustrated in Fig. 2. Basically, this device consists of an entrance window "A" having a photocathode 60 which is very sensitive to the wavelength-specific near-infrared light pulses to be utilized. A few hundred microns from the photocathode is the input face of a microchannel plate electron multiplier (MCP) labeled "B." The electrons which emerge from the MCP are accelerated by appropriate bias voltages to impact a phosphor screen 62 deposited on the inside of an output window "C."

[0013] Such image intensifiers can be used as fast electronic imaging shutters by biasing the photocathode 60 by an appropriate positive electrical potential relative to the front of the MCP, and then applying a short negative pulse to momentarily turn the device "on." As used in accordance with both the previous patent and the present invention, the shuttered detectors 22, 24 also include a photodiode coupled to the image-intensifier outer window "C" so that an electrical signal is obtained that corresponds to the image intensity appearing on output window "C". As indicated previously, both of the shuttered detectors 22 and 24 (also designated "S1" and "S2," "S3") of the previous patent would, of course, each include its own image intensifier for independent switching.

[0014] The speed with which an image intensifier can be turned on and off is limited by a phenomenon called "irising," in which the peripheral image field appears first while the center of the field is still dark (off). The reason for this is that the photocathode material has a relatively high resistance per unit area and a distributed capacitance, principally to the front of the MCP, and an electrode ring 64 is used in such devices to apply the gating voltage. When a fast negative pulse is applied to the electrode ring 64, it takes a finite if short time to charge the photocathode center relative to its periphery. Typically, this delay will be on the order of at least several nanoseconds, before the intensifier is fully turned on. The effects of such irising are negated as used in accordance in the present invention, since the image intensifier is only being used for shuttered light detection rather than imagery. Thus, by limiting the fiber optics applying the input photons to only the edge of the photocathode, adjacent the ring electrode 64, the delay in fully turning on the center of the photocathode is made entirely irrelevant.

[0015] In accordance with the present invention, both the system (apparatus) and processing of the time-related detected photon signals are simplified and substantially improved. This is based on apprehension of the fact that a number of important sources of error may be cancelled by taking the ratio of the number or representative value of at least two bursts of mutually time-spaced returning photons, *i.e.*, those leaving the head of the patient and being coupled to the photon detection apparatus 20 on fiber optical cable 44, which are to be shutter-detected at points in time corresponding to two or more specifically designated time delays after introduction of the related wavelength-specific photons from source 10.

[0016] More particularly, the number of photons (N) received after a first time delay (t) may be expressed as:

$$N \propto TS e^{-\rho\sigma(\lambda,f)ct} \quad \text{Eq. 1}$$

where:

T= transmission at the fiberoptic-skin interface

S = sensitivity of the shuttered-detector

ρ = density of hemoglobin molecules (α) to blood density

σ = cross-section of a hemoglobin molecule at wavelength λ and fractional oxygen f

c = velocity of photons in tissue

t = time delay from injection

[0017] If, in the expression set forth above, ρ is in units of molecules per cubic centimeter and σ is in units of square centimeters, then $\rho\sigma$ is the familiar linear absorption coefficient " μ " in units of inverse centimeters. Likewise, if c is units of centimeters per second and t is units of seconds, then ct is the pathlength in units of centimeters.

[0018] Using the basic expression set forth above as Equation 1, the number of photons received at a second time delay t is expressed as follows:

$$N' \propto T'S' e^{-\rho\sigma(\lambda,f)c(t'-t)} \quad \text{Eq. 2}$$

[0019] By dividing Equation 2 by Equation 1, we get the following ratio:¹

$$\frac{N'}{N} = \left(\frac{T'}{T}\right)\left(\frac{S'}{S}\right) e^{-\rho\sigma(\lambda,f)c(t'-t)} \quad \text{Eq. 3}$$

¹ Note that the differential pathlength, $\Delta P = c(t'-t)$, is known exactly.

[0020] As can be seen from Equation 3 above, variations in the coupling of the fiber optics with the skin are cancelled, since with these very short times $T' = T$. Referring back to Fig. 1 and the accompanying discussion, it will of course be understood that each of the shuttered detectors 22, 24 will have its own characteristic sensitivity S, S'; however, in accordance with the invention, it is observed that if these two quantities could be made equal, they would also cancel, making the solution of the equation that much simpler. This novel and useful concept is accomplished in accordance with the present invention, and accomplished in a most effect way; *i.e.*, a single image detector is utilized to switch each of the time-delayed photon quantities exiting the head of the patient, that carry the oxygen-related hemoglobin absorption information which is desired.

[0021] As indicated above, the shuttered detectors 22, 24 utilized in the preferred embodiment include a proximity-focused image intensifier, the output light from which is measured by a photodetector (as referred to above, and as described in detail in the prior patent identified above. As disclosed in the prior patent, the termination of the fiber optic cable, (*i.e.* cable 44, as seen in Fig. 1) conducting the photons from the head is positioned at the edge of the image intensifier's photocathode to speed its response to the gating pulse by minimizing the distributed resistance and capacitance inherent in the thin photocathode, which causes the "irising" effect noted above. In accordance with the invention, a single image intensifier is utilized to provide two correlated but separate simultaneously acting shutters, by bringing a second fiberoptic cable (designated 144 in Figs. 3 and 4) from the head of the patient to the same image intensifier, but positioning its termination at the side of the photocathode opposite that where cable 44 is terminated (*i.e.*, 180° therefrom).

By using this arrangement, all that is required to make the device operate as a pair of separate or detectors is the presence of a second photodetector (66, 68) on the image intensifier's output side (Fig. 4). These two photodetectors must be arranged to separately view the images appearing on the ends of the two input fiber optic cables 44, 144, as they appear separately mapped on the image intensifier output screen 62. In this regard, it should be pointed out that by utilizing this inventive concept, the same image intensifier may be utilized to provide even more than two such shutters, or optical switches.²

² The only limitation is the angular spatial resolution of the image intensifier around the edge of the photocathode and the corresponding map on the output screen. An inexpensive "streak camera" device could be built using a large number of input fibers each with small, uniformly stepped delays.

[0022] Fig. 3 provides a schematic representation of such an improved, simplified system, and the image intensifier portion thereof, comparable to that shown in Fig. 4 of the referenced prior patent and Fig. 2 herein, is shown in Fig. 4 herein. As will be seen from Fig. 3 herein, the photon detection fiberoptic 44, 144 extending from the head of the patient to the shuttered detector 22, 24 may advantageously be implemented by use of a single bifurcated or branched fiberoptic cable, one branch forming cable 44 and the other forming cable 144. Also, as schematically illustrated in Fig. 4 herein, and as noted above, photon input cable 44 is directly aligned with an output location of the image intensifier that is coupled to its own photodetector, designated 66 herein, and photon delivery cable 144 is directly aligned with an image-intensifier output coupled to its own photodetector, designated here 68. Accordingly, the burst of photons to be detected at a first time interval following the instant of photon injection, t , is indicated by the arrow 100, and the other such burst, at time t' following injection, is indicated by the other such arrow, designated 200. As shown in this example, where two separate branches carrying differently timed photon bursts (or images) are being switched by a single image intensifier, the input and output cables or other such optical connectors are preferably disposed 180° from each other around the edge of the photocathode. Of course, if a greater number of photon bursts was being detected, a corresponding greater number of separate cable branches would be used and each would be correspondingly equally spaced from the others around the edge of the photocathode.

[0023] With further reference to the system of the aforementioned prior patent, and as noted above, the two (or more) shuttered detectors 22, 24 are gated by a small portion of the input photon burst from source 10 (laser 12), by using two different fiberoptic cables (there designated 46 and 48) having two different lengths, so that the shuttered detectors are gated on at different

points in time, thereby sampling or detecting the photons leaving the head at two different points in time, in effect taking "snapshots" at those points in time. In accordance with the present invention, the single shuttered detector 22, 24 is gated at a single point in time, utilizing a portion of the photons from the source directed toward the head. Although the single shuttered detector 22, 24 thus operates at a single and brief point in time, the different photon quantities which it detects at that single point in time actually emanate from the head of the patient at two closely spaced but different points in time, due to the precisely cut input cables 44 and 144. Thus, the outputs from the shuttered detectors which are applied to photodetectors 66 and 68 are specifically different, and comparatively unique, notwithstanding the fact that the shuttered detector is operated only a single time to switch photon inputs that occurred at different points in time.

[0024] As an example of such a system, assume that the source (laser) 12 produces the photon pulse at $t=0$ and the fiber optic conducting the light to the head (42) is 10ns long. Assume the fiberoptic receiving the photons 44, 144 from the head is split into two cables (bifurcated) going to opposite points on the edge of the image intensifier photocathode, as described above, but with one of the branches cut to be 6ns and the other branch 7ns long. If the gating fiber (47) between the laser 12 and the shuttered detector 22, 24 is 21ns long and cable branch 44 is 6ns long while branch 144 is 7ns long, the photons arriving over the 6ns fiber (44) will have left the head 5ns after injection while the photons arriving over the 7ns fiber (144) will have left the head 4ns after injection. Accordingly, with this system, the ratio of the two signals from the corresponding photodetectors 66, 68 will be independent of both time and amplitude ("jitter") in the shuttered detector gate, since $S' = S$.

[0025] Further improvements or enhancements in the system described in the previous patent are as follows. The first such feature, also comprising a part of the present invention, relates to the characteristics of the input and output fiberoptic cables, herein designated 42 and 44, 144 respectively. While it is obvious that the core material of these fibers should not scatter light, some such scattering is unavoidable. The very large injection pulse from the laser (12) initiates "reverberation" from scattering and reflection at the fiber ends that may persist long enough to interfere with the measurement of delayed light. Unlike the causes of this problem, its solution is not obvious; however, one measure which will or may help is to have the core material be deliberately partially absorbing. While the signal light passes through the fibers once, the reverberating light takes a longer path and will be discriminated against by such absorption.

[0026] The other item or feature has to do with insuring that the pulses used to gate the single shuttered (22, 24) detector on are of uniform amplitude. As indicated above, the photocathode of the image intensifier is biased off prior to the time of arrival of the laser-generated injection pulse (by a large positive voltage, which keeps the photoelectrons from getting to the microchannel plate), and it is only turned on (made negative) several nanoseconds later to measure the very small amount of delayed light from the head of the patient or test subject. However, the photocathode tends to

"remember" the large initial pulse and release some electrons to the microchannel plate when turned on, even if there is no delayed light. This phenomenon was referred to as "persistence" in the prior patent referred to above.

[0027] Two operating parameters appear to be most important in eliminating this 'persistence'. Firstly, the larger the "off" bias, the better. In the particular implementation described and illustrated, increasing the "off" bias from +170 to +190 volts appears to reduce the persistence by two orders of magnitude. Secondly, it is important to control the amplitude of the larger negative gate "on" pulse so that it does not take the photocathode more than 20v negative. Therefore, for a +190 volt "off" bias in this implementation, the gate "on" pulse peak amplitude should be very close to -210v. Since the gate pulse is derived directly from a photodiode which is driven by a fraction (delayed) of the laser pulse, its reproducibility depends on the laser pulse amplitude stability. Since the laser's stability is much less than the 2% needed to hold the on voltage to 20%, it is believed advantageous to use avalanche transistors to completely isolate the laser-generated photodiode gate pulse from the image intensifier photocathode. The photodiode will trigger an avalanche breakdown in a string of transistors that will then generate their own gate pulses with amplitudes that are independent of the laser output stability. Based on measurements taken of representative circuits, the avalanche transistor breakdown occurs in less than 1ns. (For a reference with respect to avalanche transistors, see Jinyuan L. Bing S. Zenghu C; "High voltage fast ramp pulse generation using avalanche transistor," Rev. Sci. Inst 69, 3066-67, 1998).

[0028] Fig. 5 is a schematic block diagram showing a preferred and more particular embodiment of the overall system of the invention shown in Fig. 3. The laser system 12 for the preferred embodiment shown in Fig. 5 consists of a flashlamp-excited Nd:YAG laser with its 5ns output pulses of infrared light (1064nm) closely coupled to a second harmonic generator ("SHG"), which converts the wavelength to green light (532nm) and width to 4ns.³ The pulse of light from the SHG is then closely coupled to an optical parametric oscillator (OPO) 13 where the wavelength is tuned to the range of 700 to 950nm depending on the angle of its internal prism with pulse widths of 3ns. The pulse of infrared photons from the OPO 13 (or laser) is divided into four parts⁴. Most such photons go to the head via the delivery fiber 42. Another part of them goes to a super diode 50 which triggers the avalanche gate 52, turning on the shuttered detector 22, 24. The third photon pickoff goes to another super diode 54, which signals the computer 56 to start a new data point sequence. A fourth photon part goes to the CCD spectrometer 58, which measures the wavelength of the photons in the pulse.

³ Another useful source is a Quantel Nd:YAG laser

⁴ Actually, more laser pulse pickoffs may also be used -- notably to drive a Pockels Cell used to quench the tail of the pulse.

[0029] With further reference to Fig. 5, light emerging from the head is carried to the shuttered detector inputs by two fibers 44, 144 that differ in length by 1ns. The two electrical equivalent outputs from the shuttered detector 22, 24 are sampled and digitized, and coupled to the computer 56 by appropriate components 70, 72, as labeled, under the control of the console computer and associated software.

[0030] Fig. 6 is a pictorial view showing an exemplary display-type user interface for use in operating a system in accordance with the invention. The system gathers data in a "list" mode. That is, for each laser (12) pulse the computer (56) saves the time, the signal and reference data for the two PMT's, the amplitude and wavelength of the pulse from the OPO, and several bits of "housekeeping" data. This data is binned (made into a histogram) on the fly to build up an absorption spectrum of the chromophores within the glowball and displayed on the computer monitor.

[0031] In the operator interface display shown in pictorial view Fig. 6, the box at top left ("VR6") sets the laser operating parameters. The middle box ("Status") displays the system status, and the box at the right ("Power Supplies") allows the operator to set the power supply voltages. The dynamic display on the lower left ("OPO") continuously shows the wavelength of each pulse and allows the wavelength range to be set. The display at lower right ("Data") continuously scrolls the outputs of the two channels.

[0032] As will now be readily apparent to those skilled in the art, a highly novel and advantageous improvement is provided herewith, both in connection with the particular fetal cerebral oximeter apparatus which forms the primary focus of this patent, and also, in a broader sense, in connection with the gating of such optical systems generally; *i.e.* the use of a single image intensifier that simultaneously sequentially gates a plurality of different optical circuits also has substantial potential advantage for various different applications. Consequently, both such aspects are to be considered part of this invention, as are the two other aspects set forth immediately above.

[0033] It is believed that those skilled in the art will readily recognize the novel and unobvious character of the inventions disclosed above, and also recognize the wide scope of applicability and high degree of advantage which they possess and provide. Of course, the above description is to be considered that of preferred embodiments only. Modifications and variations of this and other such embodiments may well occur to those skilled in the art and to those who make or use the invention after learning of it through access to such preferred embodiments. Accordingly, it is to be understood that the embodiment shown in the drawings and described above is merely for illustrative purposes and should not be used to limit the scope of the invention, which is to be interpreted according to the appended set of claims.

Claims

1. Apparatus for spectrophotometrically monitoring hemoglobin oxygenation in a test subject, comprising in combination:

5 a source (10) of photons having a desired wavelength;
 a probe coupled to said source to optically access a single location on the test subject by injecting photons into said subject from said source at said location and for receiving photons exiting said subject at said location after injection; and
 10 a photon-conducting device (44, 144) operatively associated with said probe to receive a stream of said exiting photons and to produce at least two differently timed streams of photons therefrom; **characterised by:**

15 a shuttered device coupled to said photon-conducting device to receive said at least two differently-timed photon streams and simultaneously switch each of said two streams on and off to create a pair of different photon bursts therefrom; and
 a detector (66, 68) coupled to said shutter device to receive said pair of separate photon bursts and provide corresponding output signals for processing.

2. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 1, wherein said photon-conducting device operatively associated with said probe comprises at least two fiberoptics (44, 144) having different effective light-conducting lengths to create said at least two differently-timed photon streams.

3. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 1, wherein said shutter device comprises an image intensifier.

4. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 3, wherein said photon-conducting device operatively coupled to said probe comprises at least two fiberoptics (44, 144) having different effective light-conducting lengths to create said at least two differently-timed photon streams.

5. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 4, wherein each of said at least two fiberoptics (44, 144) is coupled to said image intensifier to provide inputs which are switched simultaneously thereby.

6. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 5, wherein said image intensifier includes a generally annular photocathode and each of said at least two fiberoptics is terminated at said photocathode in a position spaced from the other, whereby said image intensifier produces at least two outputs and each such output is separately representative of a different one of said inputs.

7. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 6, wherein said image intensifier has an output element, and including at least two output conductors coupled to said output element to receive separate output signals therefrom, each of said separate output signals representative of a different one of said inputs.

8. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 7, wherein each of said at least two output conductors is coupled to said image intensifier output element in direct alignment with a different one of said at least two image intensifier inputs.

9. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 1, including a fiberoptic conductor (42) coupled between said source of photons and said probe for providing said photons for injection into said subject, wherein said fiberoptic conductor comprises a partially absorbing fiberoptic to discriminate against photon stream reverberation due to scatter and reflection effects.

10. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 3, including a coupling between a gating electrode of said image-intensifier and said photon source (10), whereby said image intensifier is gated on and off by operation of said source, said coupling including a device to convert photon from said source into a corresponding electrical signal.

11. The apparatus for monitoring hemoglobin oxygenation in a test subject according to claim 10, wherein said coupling

includes an avalanche transistor array.

12. A method of monitoring hemoglobin oxygenation in a test subject, comprising the steps of:

5 injecting a quantity of photons having a predetermined wavelength into said test subject at a predetermined time and location;
optically accessing said predetermined location on said test subject to receive photons exiting said test subject at at least two different timed intervals following said time of injecting; and
10 converting said received photons exiting said test subject at at least two different timed intervals into at least two corresponding concurrent signals for subsequent evaluative processing; **characterised in that** converting said received photons includes simultaneously switching at least two streams of said received photons on and off to create a pair of different photon bursts therefrom.

13. A method of claim 12, wherein said step of converting is carried out at least in part by applying said exiting photons to a common switching device as separate photon groupings.

14. The method of claim 12, wherein said step of converting said photons into corresponding concurrent signals includes the step of delaying a photon grouping received at a longer time interval after injection into said test subject at a first time with respect to a different grouping injected at a second and subsequent time.

15. The method of claim 14, wherein said step of converting is carried out at least in part by applying said photons to a common switching device as separate photon groupings.

16. The method of claim 12, wherein said evaluative processing includes determining the quantity of said received photons in the two different timed intervals following the instant of injection, and then taking the ratio of the determinations in each set.

Patentansprüche

1. Vorrichtung zum spektrophotometrischen Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson, welche in Kombination aufweist:

eine Quelle (10) von Photonen mit einer gewünschten Wellenlänge;
35 eine Sonde, die mit der Quelle verbunden ist, um optisch Zugang zu einer einzelnen Stelle an der Versuchsperson zu haben, indem Photonen von der Quelle an dieser Stelle in die Person injiziert werden, und um Photonen aufzunehmen, die nach der Injektion an dieser Stelle aus der Person austreten; und
eine photonenleitende Vorrichtung (44, 144), die betriebsbereit mit der Sonde verbunden ist, um einen Strom der austretenden Photonen aufzunehmen und wenigstens zwei unterschiedlich terminierte Photonenströme daraus zu erzeugen;
40 **gekennzeichnet durch:**

eine Blendenvorrichtung, die mit der photonenleitenden Vorrichtung verbunden ist, um die wenigstens zwei unterschiedlich terminierten Photonenströme aufzunehmen und jeden der beiden Ströme gleichzeitig ein- und auszuschalten, um daraus ein Paar unterschiedlicher Photonenbursts zu erzeugen; und
45 einen Detektor (66, 68), der mit der Blendenvorrichtung verbunden ist, um das Paar getrennter Photonenbursts aufzunehmen und entsprechende Ausgangssignale zur Verarbeitung zu liefern.

2. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 1, wobei die photonenleitende Vorrichtung, die betriebsbereit mit der Sonde verbunden ist, wenigstens zwei Glasfasern (44, 144) mit unterschiedlicher effektiver lichtleitender Länge aufweist, um die wenigstens zwei unterschiedlich terminierten Photonenströme zu erzeugen.

3. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 1, wobei die Blendenvorrichtung einen Bildverstärker aufweist.

4. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 3, wobei die photonenleitende Vorrichtung, die betriebsbereit mit der Sonde verbunden ist, wenigstens zwei Glasfasern (44,

144) mit unterschiedlicher effektiver lichtleitender Länge aufweist, um die wenigstens zwei unterschiedlich terminierten Photonenströme zu erzeugen.

5 5. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 4, wobei jede der wenigstens zwei Glasfasern (44, 144) mit dem Bildverstärker verbunden ist, um Eingänge zu liefern, die davon gleichzeitig geschaltet werden.

10 6. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 5, wobei der Bildverstärker eine im Allgemeinen ringförmige Photokathode aufweist und jede der wenigstens zwei Glasfasern an der Photokathode an einer Stelle endet, die von der anderen beabstandet ist, wobei der Bildverstärker wenigstens zwei Ausgänge erzeugt und jeder derartige Ausgang für sich für einen anderen der Eingänge repräsentativ ist.

15 7. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 6, wobei der Bildverstärker ein Ausgangselement hat und wenigstens zwei Ausgangsleiter aufweist, die mit dem Ausgangselement verbunden sind, um getrennte Ausgangssignale davon zu empfangen, wobei jedes der getrennten Ausgangssignale für einen anderen der Eingänge repräsentativ ist.

20 8. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 7, wobei jeder der wenigstens zwei Ausgangsleiter in direkter Ausrichtung mit einem anderen der wenigstens zwei Bildverstärker-Eingänge mit dem Bildverstärker-Ausgangselement verbunden ist.

25 9. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 1, die einen Glasfaserleiter (42) aufweist, der zwischen die Quelle von Photonen und die Sonde geschaltet ist, um die Photonen zur Injektion in die Person zu liefern, wobei der Glasfaserleiter eine teilweise absorbierende Glasfaser aufweist, um Photonenstromecho aufgrund von Streuungs- und Reflexionseffekten zu vermeiden.

30 10. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 3, die eine Verbindung zwischen einer Ansteuerungselektrode des Bildverstärkers und der Photonenquelle (10) aufweist, wobei der Bildverstärker durch Betrieb der Quelle angesteuert und ausgeblendet wird, wobei die Verbindung eine Vorrichtung aufweist, um Photonen von der Quelle in ein entsprechendes elektrisches Signal umzuwandeln.

11. Vorrichtung zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson gemäß Anspruch 10, wobei die Verbindung eine Lawinentransistoranordnung aufweist.

35 12. Verfahren zum Überwachen der Hämoglobin-Oxygenierung in einer Versuchsperson, das die folgenden Schritte umfasst:

Injizieren einer Menge von Photonen, die eine vorgegebene Wellenlänge haben, in die Versuchsperson zu einem vorgegebenen Zeitpunkt und an einer vorgegebenen Stelle;

40 optisches Zugreifen auf die vorgegebene Stelle an der Versuchsperson, um zu wenigstens zwei unterschiedlich terminierten Intervallen nach dem Zeitpunkt der Injektion Photonen aufzunehmen, die aus der Versuchsperson austreten;

45 Umwandeln der aufgenommenen Photonen, die aus der Versuchsperson zu wenigstens zwei unterschiedlich terminierten Intervallen ausgetreten sind, in wenigstens zwei entsprechende gleichzeitige Signale zur folgenden bewertenden Verarbeitung;

dadurch gekennzeichnet, dass

das Umwandeln der aufgenommenen Photonen das gleichzeitige Ein- und Ausschalten von wenigstens zwei Strömen der aufgenommenen Photonen umfasst, um ein Paar unterschiedlicher Photonenbursts daraus zu erzeugen.

50 13. Verfahren nach Anspruch 12, wobei der Schritt des Umwandelns wenigstens teilweise durch Anlegen der austretenden Photonen als getrennte Photonengruppen an eine gemeinsame Schaltvorrichtung durchgeführt wird.

55 14. Verfahren nach Anspruch 12, wobei der Schritt des Umwandelns der Photonen in entsprechende gleichzeitige Signale den Schritt des Verzögerens einer Photonengruppe, die in einem längeren Zeitintervall nach der Injektion in die Versuchsperson zu einem ersten Zeitpunkt aufgenommen worden ist, bezüglich einer anderen Gruppe, die zu einem zweiten und Folgezeitpunkt injiziert worden ist, umfasst.

15. Verfahren nach Anspruch 14, wobei der Schritt des Umwandelns wenigstens teilweise durch Anlegen der Photonen als separate Photonengruppen an eine gemeinsame Schaltvorrichtung durchgeführt wird.
16. Verfahren nach Anspruch 12, wobei das bewertende Verarbeiten das Ermitteln der Menge der aufgenommenen Photonen in den beiden unterschiedlich terminierten Intervallen nach der Injektion umfasst, und dann das Feststellen des Verhältnisses der Ermittlungen in jedem Set.

Revendications

1. Appareil pour contrôler par spectrophotométrie l'oxygénation de l'hémoglobine sur un sujet de test, comprenant en combinaison :

une source (10) de photons ayant une longueur d'onde souhaitée ;
 une sonde raccordée à ladite source pour accéder optiquement à un endroit unique sur le sujet de test, en injectant des photons dans ledit sujet à partir de ladite source audit endroit et pour recevoir des photons sortant dudit sujet audit endroit après l'injection ; et
 un dispositif conducteur de photons (44, 144) opérationnellement associé à ladite sonde pour recevoir un courant desdits photons en sortie et produire au moins deux courants de photons à des moments différents ;
caractérisé par :

un dispositif à obturateur raccordé audit dispositif conducteur de photon pour recevoir lesdits au moins deux courants de photons à des moments différents, et simultanément allumer et arrêter chacun desdits deux courants, afin de créer une paire de différentes salves de photons à partir de là ; et
 un détecteur (66, 68) raccordé audit dispositif d'obturateur pour recevoir lesdites paire de salves de photons séparées et fournir des signaux de sortie correspondants pour le traitement.

2. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 1, dans lequel ledit dispositif conducteur de photon opérationnellement raccordé à ladite sonde comprend au moins deux fibres optiques (44, 144) ayant des longueurs conductrices de lumières effectives différentes pour créer lesdits au moins deux courants de photons à des moments différents.
3. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 1, dans lequel ledit dispositif obturateur comprend un intensificateur d'image.
4. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 3, dans lequel ledit dispositif conducteur de photon opérationnellement raccordé à ladite sonde comprend au moins deux fibres optiques (44, 144) ayant différentes longueurs conductrices de lumière effectives différentes pour créer lesdits au moins deux courants de photons à des moments différents.
5. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 4, dans lequel chacune desdites au moins deux fibres optiques (44, 144) est raccordée audit intensificateur d'image afin de fournir des entrées qui sont alors simultanément commutées.
6. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 5, dans lequel ledit intensificateur d'image comprend une photocathode généralement annulaire et chacune desdites au moins deux fibres optiques se termine au niveau de ladite photocathode dans une position espacée de l'autre, moyennant quoi ledit intensificateur d'image produit au moins deux sorties et chacune de ces sorties est séparément représentative d'une entrée différente parmi lesdites entrées.
7. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 6, dans lequel ledit intensificateur d'image a un élément d'émission, et comprenant au moins deux conducteurs de sortie, raccordés audit élément de sortie pour recevoir des signaux de sortie séparés à partir de là, chacun desdits signaux de sortie séparés étant représentatif d'une entrée différente parmi lesdites entrées.
8. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 7, dans lequel chacun desdits au moins deux conducteurs de sortie est raccordé audit élément de sortie d'intensificateur d'image en alignement direct avec une entrée différente desdites au moins deux entrées d'intensificateur d'image.

- 5 9. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 1, comprenant un conducteur à fibres optiques (42) raccordé entre ladite source de photons et ladite sonde afin de fournir lesdits photons pour injection dans ledit sujet, dans lequel ledit conducteur à fibres optiques comprend une fibre optique à absorption partielle permettant de séparer la réverbération de courant de photon due aux effets de diffusion et de réflexion.
- 10 10. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 3, comprenant un raccordement entre une électrode de déclenchement dudit intensificateur d'image et ladite source de photon (10), moyennant quoi ledit intensificateur d'image est enclenché ou déclenché par le fonctionnement de ladite source, ledit couplage comprenant un dispositif pour convertir le photon de ladite source en un signal électrique correspondant.
- 15 11. Appareil pour contrôler l'oxygénation de l'hémoglobine sur un sujet de test selon la revendication 10, dans lequel ledit couplage comprend une matrice de transistors en avalanche.
- 20 12. Procédé de contrôle de l'oxygénation de l'hémoglobine sur un sujet de test, comprenant les étapes consistant à :
injecter une quantité de photons ayant une longueur d'onde prédéterminée sur ledit sujet de test à un moment et en un endroit prédéterminé ;
accéder optiquement audit endroit prédéterminé sur ledit sujet de test afin de recevoir des photons sortant dudit sujet de test à au moins deux intervalles de temps différents suivant ledit moment d'injection ; et
convertir lesdits photons reçus sortant dudit sujet de test à au moins deux intervalles de temps différent en au moins deux signaux simultanés correspondants pour un traitement d'évaluation successif ; **caractérisé en ce que** la conversion desdits photons reçus comprend simultanément l'allumage et l'extinction d'au moins deux courants desdits photons reçus, afin de créer une paire de différentes salves de photons à partir de là.
- 25 13. Procédé selon la revendication 12, dans lequel ladite étape de conversion est réalisée au moins en partie en appliquant lesdits photons en sortie à un dispositif de commutation commun sous forme de groupes de photons séparés.
- 30 14. Procédé selon la revendication 12, dans lequel ladite étape de conversion desdits photons en signaux simultanés correspondants comprend l'étape consistant à retarder un groupement de photon reçu à un intervalle de temps plus long après injection dans ledit sujet de test à un premier moment relativement à un groupement différent injecté à un second moment successif.
- 35 15. Procédé selon la revendication 14, dans lequel ladite étape de conversion est réalisée au moins en partie en appliquant lesdits photons à un dispositif de commutation commun, tel que des groupements de photons séparés.
- 40 16. Procédé selon la revendication 12, dans lequel ledit traitement d'évaluation comprend la détermination de la quantité desdits photons reçus aux deux intervalles à des moments différents suivant l'instant d'injection et ensuite en prenant le rapport des déterminations dans chaque ensemble.
- 45
- 50
- 55

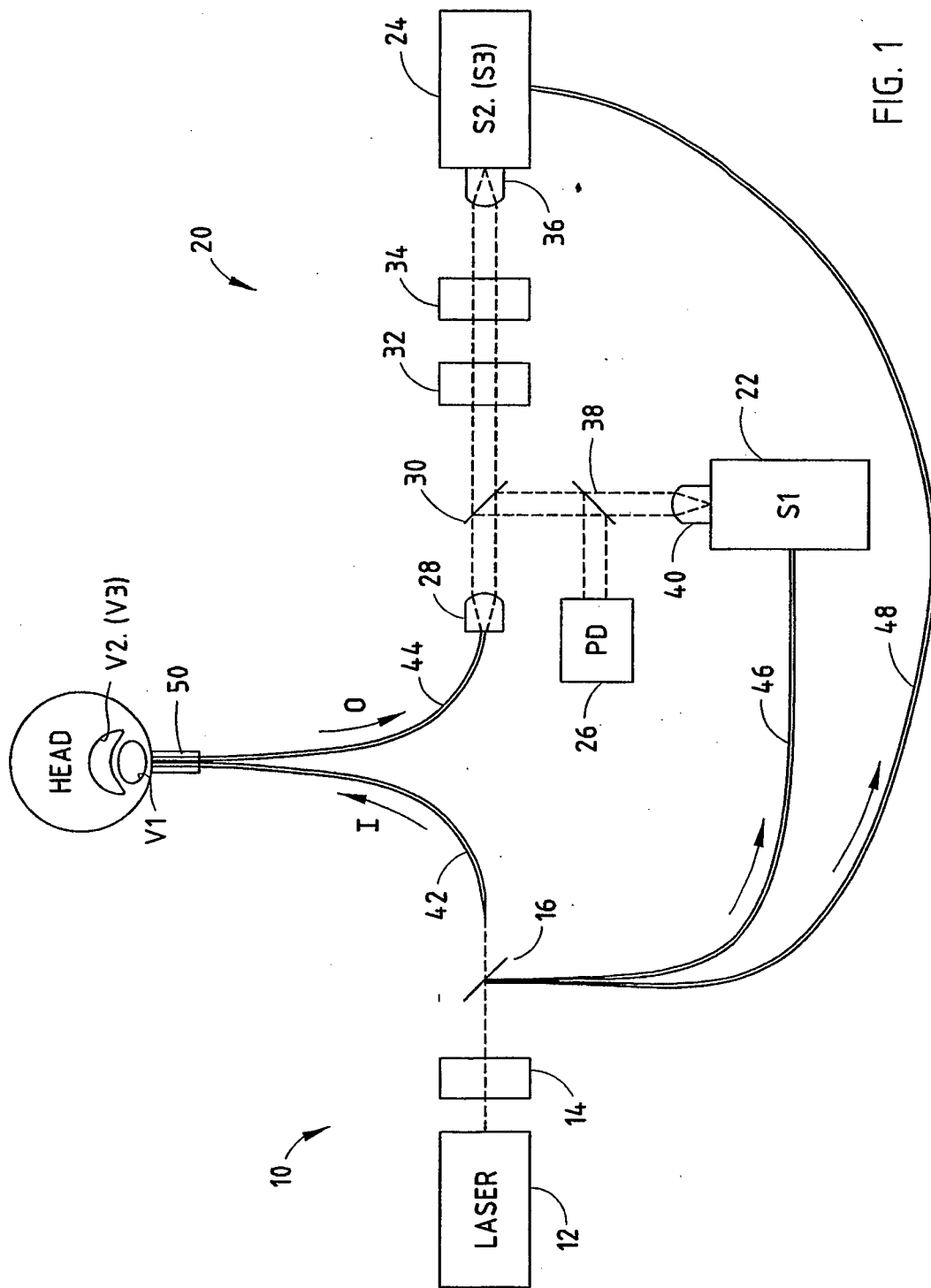


FIG. 1

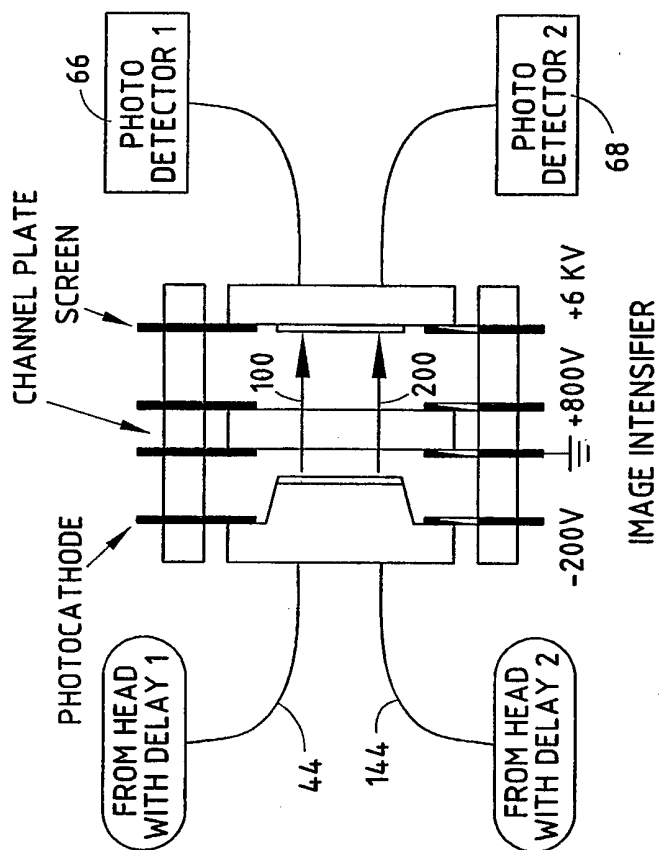


FIG. 4

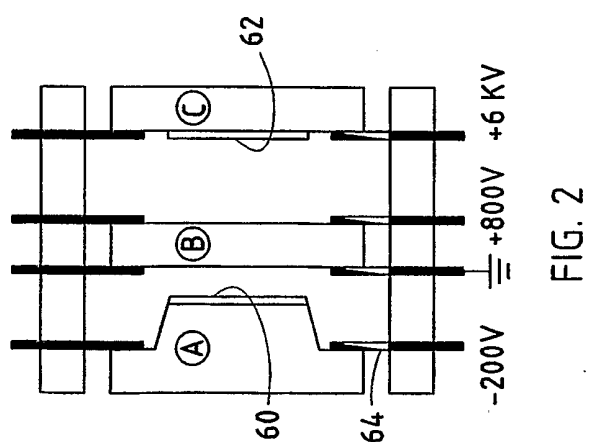


FIG. 2

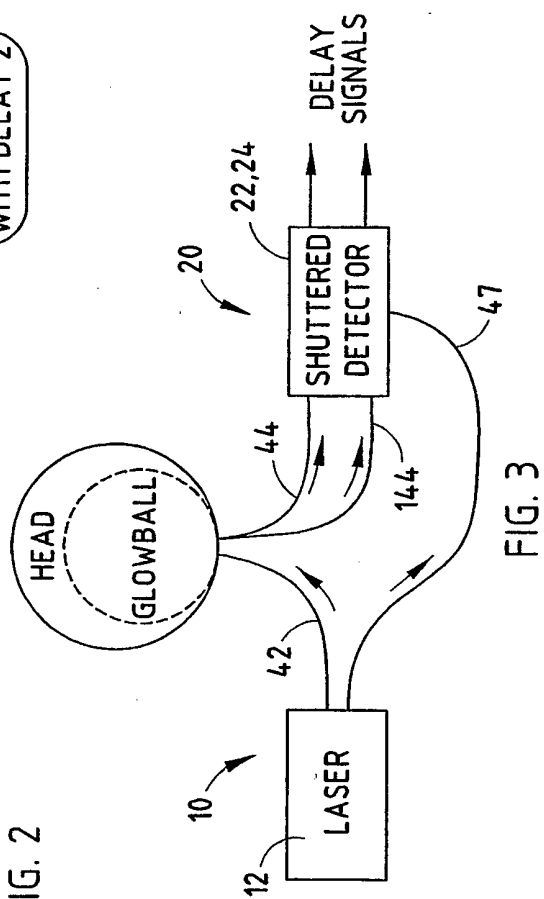
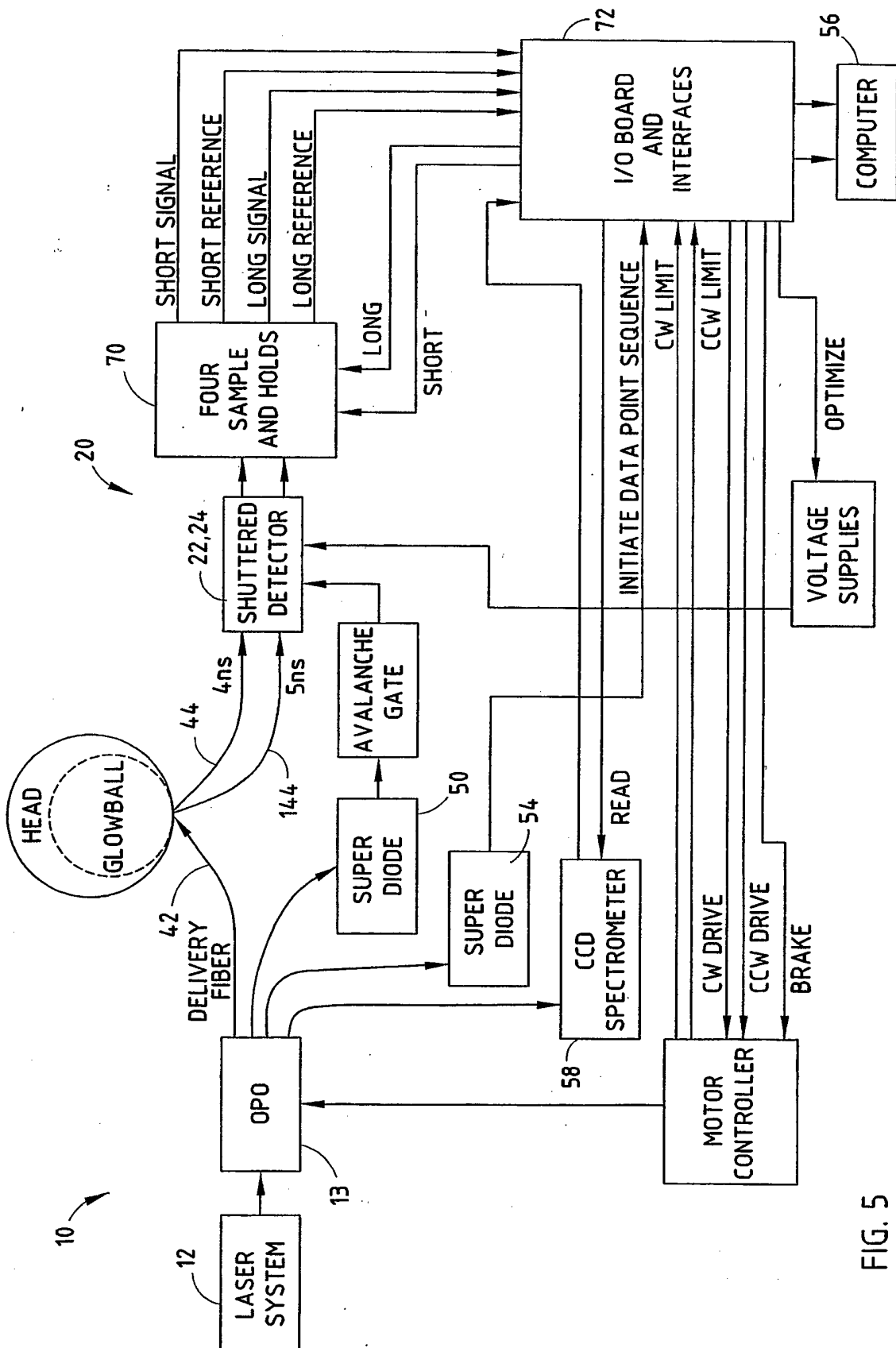


FIG. 3



FETAL MONITOR

YAG
STATUS

LASER OUTPUT

ENABLE

FLASHLAMP MODE

EXTERNAL

Q-SWITCH MODE

EXTERNAL

BURST:

DELAY:

INTERLOCKS

FLASHLAMP

REPLY

SAMPLING
SET...

DELAY 1

DELAY 2

POWER SUPPLIES
OFF

CATHODE

240

▼

MC PLATE

780

▼

PHOSPHOR

4.0K

▼

AVALANCHE

320

▼

SUPER DIODE

150

▼

PMT A

1000

▼

PMT B

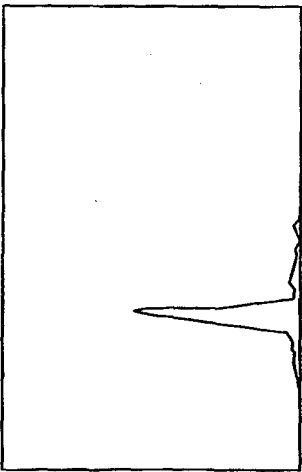
1000

▼

ACCEPT

REVERT

UPO

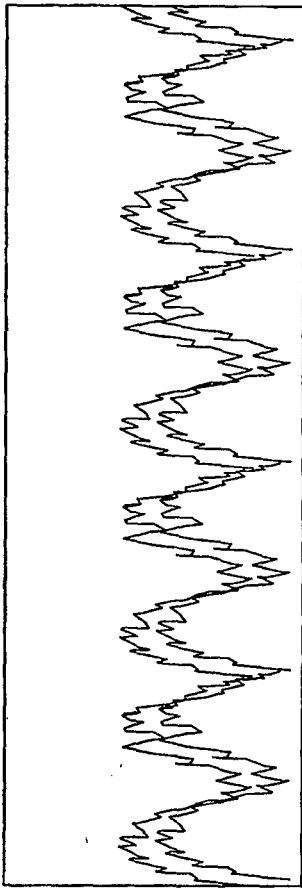


<<

SCAN

>>

DATA



CLEAR

GO

STOP

FIG. 6

15

REFERENCES CITED IN THE DESCRIPTION

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专利名称(译)	用于确定脑氧饱和度的方法和设备		
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外部链接	Espacenet		

摘要(译)

公开了一种用于确定脑氧合的新的和改进的方法和装置。在一个基本方面，来自激光器（12）的一小部分输入光子脉冲被注入头部。光子检测光纤（44,144）收集光子并将它们发送到快门检测器（22,24）。利用快门检测器（22,24），通过确定两个不同但紧密间隔的点中的至少一组中的返回光子的数量，可以显著改善和简化波长特定光的基于时间的光子量确定。在注射瞬间之后的时间，然后取每组中的测定的比率，从而取消并去除几个重要的误差源。

NaTSer

Eni

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