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(54) **FLEXIBLE BAND TINE ARRAY, PARTICULARLY FOR AN IMPLANTABLE CARDIAC PACEMAKER**

(57) The present invention relates to an anchoring device (1) for anchoring an implantable medical device (2) to tissue of a patient, wherein the anchoring device (1) comprises: an annular member (10), a plurality of elongated tines (20) connected to the annular member (10) and protruding from the annular member (10),

wherein the annular member (10) comprises at least one stretchable first section (100) that is stretchable along a peripheral direction (U) of the annular member (10). Further, the invention relates to an implantable medical device (e.g. an implantable cardiac pacemaker) comprising such an anchoring device.

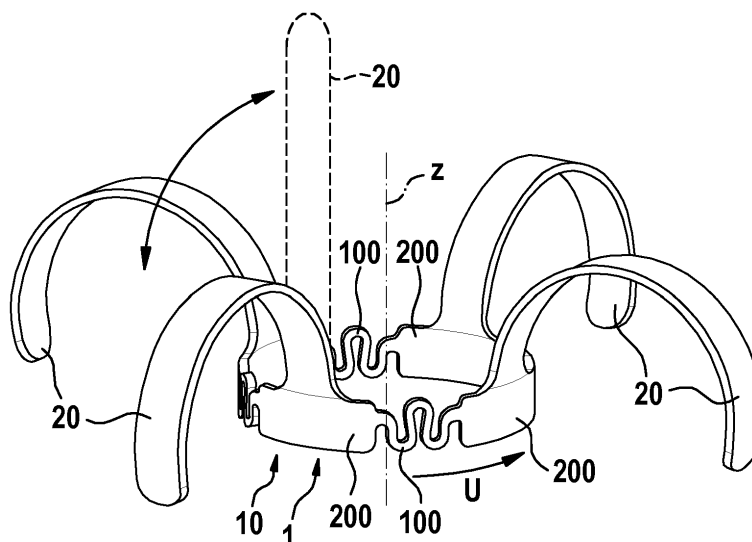


FIG. 1

Description

[0001] The invention relates to an anchoring device for an implantable medical device, particularly for an implantable cardiac pacemaker, particularly an intra-cardiac pacing systems (IPS) or an epicardiac pacing system (EPS).

[0002] Intra-cardiac pacing systems (IPS) are small active implants completely implanted within a heart. These IPS comprise leadless pacemaker devices, which are small pacemakers anchored in the heart with anchoring devices. Usually these leadless pacemakers are VVI pacemakers (see NASPE Code), which are implanted in the ventricle of the heart able to sense right ventricular signals only, and pace in the right ventricle only. In recent times so called VDD/DDD operations getting more and more important, which means that at least signals from the right atrium shall be considered for the therapy. These intra-cardiac VDD pacing systems may have atrial extensions.

For the purpose of the patent application the term "EPS" are associated with "epicardiac pacing systems", which define pacing systems, which can be attached to the outside of the heart tissue. Such an EPS may be particularly applicable to left ventricular pacing. These EPS comprise leadless epicardial pacemakers, which are small pacemakers anchored to the outside of the heart. Further, cardiac leads with an so called passive fixation is also included in the term IPS or EPS

[0003] Such an anchoring device usually comprises tines for anchoring the implantable medical device in the patient's tissue.

[0004] Individual tines have the flexibility of easy manufacturability (e.g. from flat ribbon Nitinol wire), and are relatively easy to configure to a number of tines (three, four or five) per IPS/EPS. However, they are more difficult to handle and assemble into an IPS/EPS header.

[0005] On the other hand, tine arrays with fixed annular member (e.g. annular band) are easier to handle and assemble into an IPS/EPS header. However, any design change on the IPS/EPS header (e.g., a wider diameter IPS/EPS) may require design change on the tine array and the shape setting tools, which renders the manufacturing of the IPS/EPS more complex and expensive. Furthermore, tines with fixed band as disclosed in US 2012/0172892 A1 may translate stress through the band from one tine to another. Eventually, this may lead to long term reliability issues.

[0006] Thus, based on the above, the problem to be solved by the present invention is to provide an improved anchoring device and implantable medical device.

[0007] This problem is solved by an anchoring device having the features of claim 1 as well as by an implantable medical device having the features of claim 11. Embodiments of these aspects of the present invention are stated in the corresponding sub claims and are described below.

[0008] According to claim 1, an anchoring device (also

denoted as tine array) for anchoring an implantable medical device to human or animal tissue is disclosed, comprising: an annular member, a plurality of elongated tines connected to the annular member and protruding from the annular member, wherein, according to the invention, the annular member comprises at least one stretchable first section that is stretchable along a peripheral direction of the annular member.

[0009] By providing at least one flexible first section on the connecting annular member, the above mentioned stresses are reduced. Further, one anchoring device may be used with a plurality of headers having different diameters. For example, one anchoring device with a certain (standard-diameter) annular member can be used for commonly known standard devices and additionally for example for IPS/EPS with high capacity batteries, which usually have larger diameters. Because of the stretchability of the first section of the annular member, the diameter of the annular member accommodates to larger diameters. This simplifies the supply during production.

[0010] The anchoring device according to the present invention may be fabricated from a drawn tube, e.g. a Nitinol tube that is laser cut to produce said tines protruding from an annular member. Particularly a cutting process as for example used in cutting vascular stents may be employed. Particularly, see also below, the present invention is adding narrow meandering structures on the connecting annular member. The meandering structures allow for the band to expand or contract radially, just like in stents. Doing so, the tine array/anchoring device can be cut from a stock tube with a diameter that is near the intended finish diameter. It does not have to be cut from tubes with the final diameter. The still malleable and already cut anchoring device may then be shape set and heat treated to form an e.g. super-elastic Nitinol structure using shape setting tool(s). The result is a tine array, which is long lasting due to an independent strut action of each tine, and comprises less induced cross-stressing as well as great design flexibility when mating with other components in the IPS/EPS header. Further, the final diameter of the anchoring device's annular member/band can be readily changed to a certain extend. Finally, the annular member allows an interference fit with one of the IPS's or EPS's components for easier handling, assembling and less play.

[0011] According to an embodiment of the present invention, the at least one stretchable first section is elastically or super-elastically stretchable, particularly in the peripheral direction of the annular member, so that the at least one first section can be prolonged in the peripheral direction leading to a corresponding larger diameter of the annular member.

[0012] Further, according to an embodiment of the present invention, the annular member is a circular annular member. Further, according to an embodiment, the annular member is an (e.g. circular) band that comprises an (e.g. flat) rectangular cross section in a plane extending perpendicular to the peripheral direction of the annu-

lar member.

[0013] Further, according to an embodiment of the present invention, the at least one stretchable first section is connected to a neighboring second section of the annular member.

[0014] Further, according to an embodiment of the present invention, the annular member comprises a plurality of stretchable first sections, wherein each two neighboring first sections are connected to each other via one second section. Particularly, the at least one of the plurality of first section comprises a first end and an opposing second end, wherein each end is in turn connected to a neighboring second section of the annular member.

[0015] Further, according to an embodiment of the present invention, the stretchable first section in both aforementioned embodiments comprises a smaller effective stiffness than the neighboring second sections regarding stretching in the peripheral direction of the annular member. Particularly, according to this application, "effective stiffness" is an overall resistance to deformation of a structure that consists of non homogenous members, material property or geometry wise, or combinations of both, under external loads.

[0016] Furthermore, according to a preferred embodiment of the present invention, the at least one stretchable first section in both aforementioned embodiments comprises a meandering shape. In an alternative embodiment, the stretchable section comprises a mesh, closed cell or helix structure, which is commonly known in the field of cardiac and peripheral stents, particularly self-expanding stents.

[0017] Particularly, the at least one stretchable first section in both aforementioned embodiments comprises a plurality of curved portions that are successively arranged along the peripheral direction and connected to one another so that the at least one first section extends along the peripheral direction from said first end to said second end as well as back and forth along an axial direction of the annular member, which axial direction particularly extends perpendicular to a radial direction of the annular member. Particularly, said axial direction coincides with a cylinder axis of the annular member.

[0018] Particularly, according to an embodiment, the tines are integrally connected to the annular member of the anchoring device. Particularly, the tines protrude from the same circumferential edge of the annular member.

[0019] Further, according to an embodiment of the present invention, the at least one first section is arranged along the peripheral direction between two sections of the annular member, wherein each of the plurality of tines protrudes from each of said two sections of the annular member.

Further, according to an embodiment of the present invention, each tine protrudes from an associated second section.

[0020] Particularly, in an embodiment, the first sections are equidistantly spaced along the peripheral direction.

Further, in an embodiment, the anchoring device comprises four first sections and four second sections as well as four tines, wherein each tine protrudes from an associated second section. Thus, in this embodiment, each tine is connected to its two neighboring tines via an (e.g. meandering) first section.

[0021] Further, according to an embodiment of the present invention, the tines are configured to move under the action of a restoring force from a first configuration in which the tines extend along said axial direction of the annular member to a second configuration in which each tine comprises a hook shape for engaging a patient's tissue.

[0022] In one embodiment, the restoring force of the stretched tine array locks the tine array onto one or more grooves, recesses, notches, or indentations on the implantable medical device and holds it there via a compression fit. In this embodiment, the stretchable section not only relieves stress in the tines, but also holds the tines in place, simplifying assembly.

[0023] Further, according to an embodiment of the present invention, the annular member and/or said tines are formed out of a metal, particularly a superelastic metal, particularly a superelastic Nickel-Titanium-Alloy, particularly Nitinol (see also above).

[0024] A further aspect of the present invention relates to an implantable medical device comprising an anchoring device according to the present invention.

[0025] According to an embodiment of the implantable medical device, the implantable medical device is an implantable cardiac pacemaker, particularly an intra-cardiac pacing system.

[0026] Particularly, in an embodiment, the implantable medical device (e.g. pacemaker, particularly IPS) is configured to be implanted into a chamber of the patient's heart, particularly into the right or left ventricle or right atrium, particularly via a catheter. Further, EPS devices are configured for accessing the epicardium, *i.e.* the outer heart wall accessed through the pericardial space external the heart, for addressing sensing and stimulating of left sided chambers. The implantable medical implant (e.g. pacemaker, particularly IPS/EPS) may comprise a hermetically sealed housing. The housing may enclose a pulse generator for generating pacing pulses to the heart of the patient, and a battery for supplying energy to the pulse generator. Particularly, the anchoring device is mounted to the implantable medical device (e.g. pacemaker, particularly IPS/EPS) such that the tines protrude out of an outer diameter of the housing at a face side of the housing for fastening the medical device (e.g. pacemaker, particularly IPS/EPS) to tissue of the chamber/ventricle (when the tines are in the second configuration). The medical device (e.g. pacemaker, particularly IPS/EPS) may comprise at least two pacing electrodes, wherein one pacing electrode is provided on the face side of the housing of the medical device (e.g. pacemaker, particularly IPS/EPS) between the tines for applying the electrical stimulation to the heart. At least one addi-

tional second electrode is situated at or near the opposite end of the housing. The latter one can be configured as a return electrode, for example in the shape of a ring electrode.

[0027] According to another embodiment of the implantable medical device, the implantable medical device is an intra-cardiac lead with anchoring tines.

[0028] Particularly, in an embodiment, the intra-cardiac lead is configured to be attached to a chamber of the patient's heart, particularly into the right or left ventricle or right atrium. The intra-cardiac lead may comprise a lead body comprising an electrically insulating material, in which electrical conductor wires are embedded. The lead body may enclose a longitudinally extending lumen for guiding means like guide wires or mandrins, in order to steer the lead into the ventricle or atrium of the heart. Particularly, the anchoring device is mounted to the distal tip of the intra-cardiac lead such that the tines protrude from the distal end of the lead body for fastening the intra-cardiac lead to tissue of the chamber (when the tines are in the second configuration).

[0029] Further features and embodiments of the present invention shall be described below with reference to the Figures, wherein

Fig. 1 shows a perspective view of an anchoring device according to the invention;

Fig. 2 shows a detail of Fig. 1;

Fig. 3 shows an implantable medical device in the form of an intra-cardiac pacing system (IPS) comprising an anchoring device according to the present invention;

[0030] Figures 1 and 2 show an embodiment of an anchoring device 1 according to the present invention for anchoring an implantable medical device 2 (depicted in Fig. 3) to tissue of a patient. The anchoring device 1, which is also denoted as tine array, comprises an annular member 10 and a plurality of elongated tines 20 connected to the annular member 10 and protruding from the annular member 10. According to the invention, the annular member 10 comprises at least one stretchable first section 100 that is stretchable along a peripheral direction U of the annular member 10.

[0031] Particularly, the annular member 10 is integrally connected to said tines 20, here to the same (e.g. upper edge 10a of the annular member 10. Particularly, the annular member 10 and the tines 20 are formed out of a superelastic alloy comprising nickel and titanium, particularly Nitinol.

[0032] As shown in Fig. 1, the annular member 10, which is particularly formed as a circular band having (at least in sections) a rectangular cross section, comprises a plurality of stretchable first sections 100, here four first sections 100, wherein each two neighboring first sections 100, i.e. first sections 100 that are neighbours in the pe-

ripheral direction U of the annular member 10, are connected to each other via a second section 200.

[0033] As shown in Figs. 1 and 2, the first sections 100 each comprise a meandering shape. Particularly, each first section 100 comprises a first end 101 and an opposing second end 102, wherein each end 101, 102 is connected to a neighboring second section 200 of the annular member 10. Further, particularly, the respective first section 100 comprises a plurality of curved portions 103 that are successively arranged along the peripheral direction U of the annular member and connected to one another so that the respective stretchable first section 100 extends along the peripheral direction U from its first end 101 to its second end 102 as well as back and forth along an axial direction z of the annular member 10. This allows stretching of the first sections 100 in the peripheral direction U, wherein the curvature of the curved portions 103 decreases leading to an elongation of the respective first section 100 in the peripheral direction U which in turn leads to an enlarged diameter of the annular member 10.

[0034] Further, each of the tines 20 protrudes from a second section 200 so that the individual tines are connected to each other via said meandering first sections 100.

[0035] Particularly, for the anchoring function, the tines 20 are configured to move under the action of a restoring force from a first configuration in which the tines 20 extend along an axial direction z of the annular member 10 (this first configuration is indicated for one tine 20 in Fig. 1 with a dashed line) to a second configuration in which each tine 20 comprises a hook shape for engaging a patient's tissue as shown in Fig. 1. Particularly, each hook-shaped tine 20 bends outwards so that the tines 20 form hooks in the second configuration that can be anchored in human or animal tissue at the implantation site (e.g. heart, particularly ventricle or atrium).

[0036] Further, Fig. 3 shows an implantable medical device 2 that comprises an anchoring device 1 according to the present invention. Here, as an example, said medical device 2 is an implantable cardiac pacemaker, particularly an intra-cardiac pacing system (IPS). However, in an alternative embodiment the anchoring device 1 can also be implemented or mounted to a face side of an EPS or to a distal tip of an intra-cardiac lead for attaching the distal end to tissue of the chamber/ventricle, for example the trabecular network.

[0037] Such an IPS 2 is configured to be implanted into a ventricle or atrium of the patient's heart, particularly into the right or left ventricle or right atrium, particularly via a catheter. The IPS 2 particularly comprise a hermetically sealed housing 3 which particularly encloses a pulse generator for generating pacing pulses that are to be applied to the patient's heart via at least one pacing electrode 4 of the IPS 2 and a battery for supplying energy to the pulse generator. Particularly, the anchoring device 1 is mounted such in the IPS 2 that the tines 20 protrude out of the housing 3 of the IPS 2 at a face side 3a of the housing 3 for fastening the IPS 2 to tissue of the cham-

ber/ventricle (when the tines 20 are in the second configuration), The pacing electrode 4 is particularly provided on the face side 4a of the housing 3 of the leadless pacemaker 2 between the tines 20 for applying said electrical stimulation to the heart of the patient. An additional second electrode, which works as a return electrode, is situated at or near the opposite end of the housing and can be configured as a ring electrode.

Claims

1. An anchoring device (1) for anchoring an implantable medical device (2) to tissue of a patient, the anchoring device (1) comprising:

- an annular member (10),
- a plurality of elongated tines (20) connected to the annular member (10) and
- protruding from the annular member (10),

wherein

the annular member (10) comprises at least one stretchable first section (100) that is stretchable along a peripheral direction (U) of the annular member (10).

2. The anchoring device according to claim 1, **wherein** the at least one stretchable first section (100) is connected to a neighboring second section (200) of the annular member (10).
3. The anchoring device according to claim 2, **wherein** the annular member (10) comprises a plurality of stretchable first sections (100), wherein each two neighboring first sections (100) are connected to each other via one second section (200).
4. The anchoring device according to one of the claims 2 or 3, **wherein** the at least one or the plurality of stretchable first sections (100) comprise a first end (101) and an opposing second end (102), wherein each end (101, 102) is connected to the neighboring second section (200) of the annular member (10).
5. The anchoring device according to one of the claims 2 to 4, **wherein** the at least one stretchable first section (100) comprises a smaller effective stiffness than the second sections (200).
6. The anchoring device according to one of the claims 2 to 5, **wherein** the at least one stretchable first section (100) comprises a meandering shape.
7. The anchoring device according to claim 6, **wherein** the at least one stretchable first section (100) comprises a plurality of curved portions (103) that are successively arranged along the peripheral direction

(U) and connected to one another so that the at least one stretchable first section (100) extends along the peripheral direction (U) from said first end (101) to said second end (102) as well as back and forth along an axial direction (z) of the annular member (10).

8. The anchoring device according to one of the claims 2 to 5, **wherein** each of the plurality of tines (20) protrudes from each of said second sections (200) of the annular member (10).
9. The anchoring device according to one of the claims 1 or 8, **wherein** the tines (20) are configured to move under the action of a restoring force from a first configuration in which the tines (20) extend along an axial direction (z) of the annular member (10) to a second configuration in which each tine (20) comprises a hook shape for engaging a patient's tissue.
10. The anchoring device according to one of the preceding claims, **wherein** the annular member (10) and/or said tines (20) are formed out of a metal, particularly a superelastic metal, particularly a superelastic alloy comprising nickel and titanium, particularly Nitinol.
11. Implantable medical device (2) comprising an anchoring device (1) according to one of the preceding claims.
12. Implantable medical device according to claim 11, wherein the implantable medical device (2) is an implantable cardiac pacemaker.
13. Implantable medical device according to claim 12, wherein the implantable medical device (2) is an intra-cardiac pacing system or epicardial pacing system.

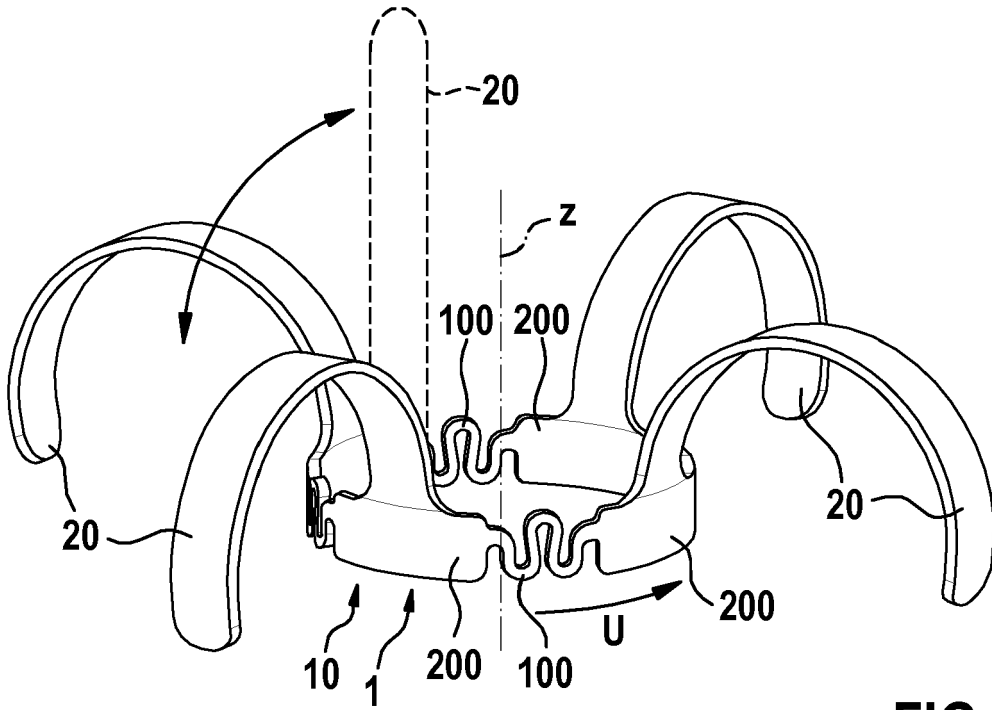


FIG. 1

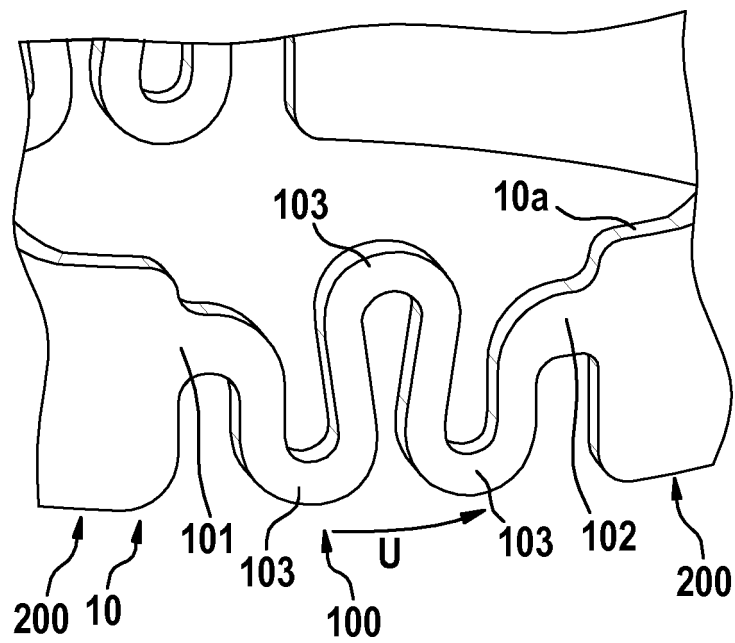


FIG. 2

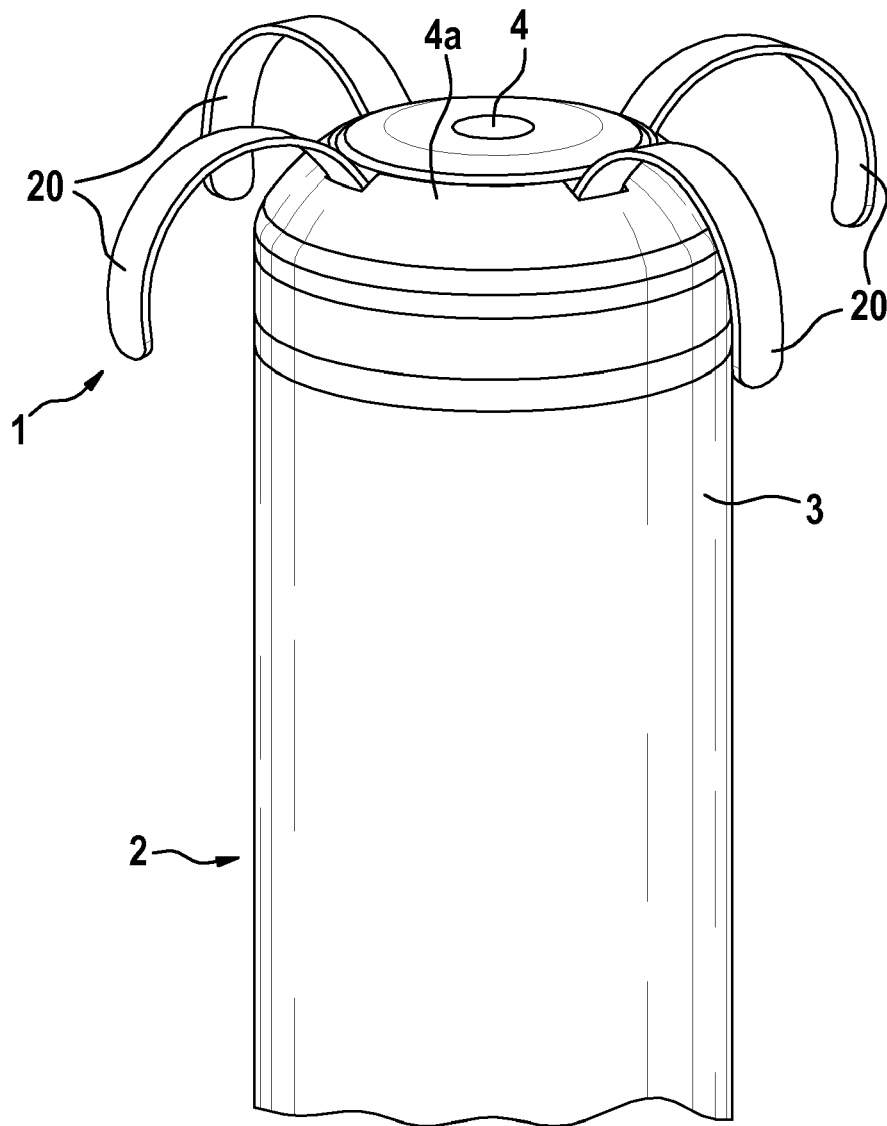


FIG. 3



EUROPEAN SEARCH REPORT

Application Number
EP 17 18 8073

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EPO FORM 1503 03.82 (P04C01)

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X,P	US 2017/209688 A1 (DRAKE RONALD A [US] ET AL) 27 July 2017 (2017-07-27) * paragraphs [0040] - [0048]; figures 1-4A *	1-13	INV. A61N1/375 A61N1/372
X	US 2011/270340 A1 (PELLEGRINI GIANFRANCO [US] ET AL) 3 November 2011 (2011-11-03) * paragraphs [0050] - [0054]; figures 19-27 *	1,11-13	ADD. A61N1/05 A61B5/00
X	US 2011/251660 A1 (GRISWOLD ERIK [US]) 13 October 2011 (2011-10-13) * paragraphs [0016] - [0023]; figures 1-3 *	1,9-13	
A	US 2012/172690 A1 (ANDERSON THOMAS A [US] ET AL) 5 July 2012 (2012-07-05) * paragraphs [0028] - [0031], [0047] - [0058], [0069] - [0075]; figures 1, 3A-6H *	1-13	
A	US 2016/059003 A1 (EGGEN MICHAEL D [US] ET AL) 3 March 2016 (2016-03-03) * abstract; figures 2A-3 *	1-13	TECHNICAL FIELDS SEARCHED (IPC) A61N A61B
A	US 2009/082828 A1 (OSTROFF ALAN [US]) 26 March 2009 (2009-03-26) * abstract; figures 4A-4D, 7A-7C, 20 *	1-13	
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 20 April 2018	Examiner Fischer, Olivier
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 17 18 8073

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This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
The members are as contained in the European Patent Office EDP file on
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Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2017209688 A1	27-07-2017	US 2017209688 A1	27-07-2017
		WO 2017127689 A1	27-07-2017
		WO 2017127695 A1	27-07-2017
US 2011270340 A1	03-11-2011	NONE	
US 2011251660 A1	13-10-2011	NONE	
US 2012172690 A1	05-07-2012	CN 103384546 A	06-11-2013
		CN 103561810 A	05-02-2014
		EP 2658599 A1	06-11-2013
		EP 2658600 A1	06-11-2013
		EP 3132824 A1	22-02-2017
		US 2012172690 A1	05-07-2012
		WO 2012092067 A1	05-07-2012
		WO 2012092074 A1	05-07-2012
US 2016059003 A1	03-03-2016	CN 106659898 A	10-05-2017
		EP 3185947 A1	05-07-2017
		US 2016059003 A1	03-03-2016
		WO 2016032716 A1	03-03-2016
US 2009082828 A1	26-03-2009	EP 2203216 A1	07-07-2010
		JP 2010540037 A	24-12-2010
		US 2009082828 A1	26-03-2009
		WO 2009039400 A1	26-03-2009

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 20120172892 A1 [0005]

专利名称(译)	灵活的带齿阵列，特别适用于植入式心脏起搏器		
公开(公告)号	EP3412337A1	公开(公告)日	2018-12-12
申请号	EP2017188073	申请日	2017-08-28
申请(专利权)人(译)	BIOTRONIK SE & CO.KG		
当前申请(专利权)人(译)	BIOTRONIK SE & CO.KG		
[标]发明人	MOMMA CARSTEN SUWITO WANTJINARJO VON ARX JEFFREY A FROTSCHER MATTHIAS BOSELMMANN MARCO		
发明人	MOMMA, CARSTEN SUWITO, WANTJINARJO VON ARX, JEFFREY A. FROTSCHER, MATTHIAS BOSELMMANN, MARCO		
IPC分类号	A61N1/375 A61N1/372 A61N1/05 A61B5/00		
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外部链接	Espacenet		

摘要(译)

锚固装置技术领域本发明涉及一种用于将可植入医疗装置（2）锚固到患者组织的锚固装置（1），其中锚固装置（1）包括：环形构件（10），多个细长尖齿（20）连接到环形构件（10）并从环形构件（10）突出，其中环形构件（10）包括至少一个可伸展的第一部分（100），其可沿环形构件的周向（U）伸展（10）。此外，本发明涉及包括这种锚固装置的可植入医疗装置（例如，可植入心脏起搏器）。

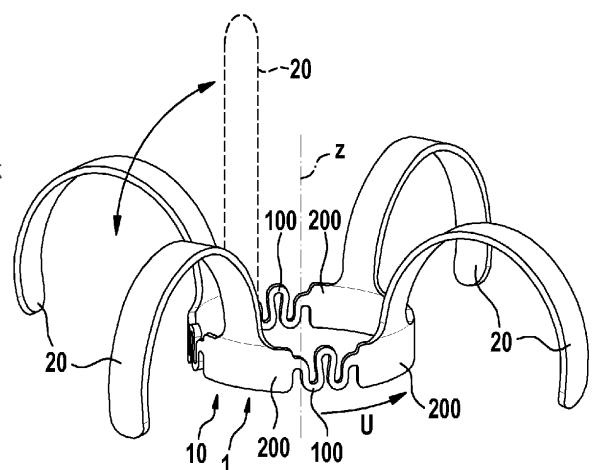


FIG. 1