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(54) **Apparatus and method for obtaining cardiac data**

(57) An apparatus and method for obtaining information, such as heart rate or the presence of atrial fibrillation, from electrodes (32, 34) applied to the feet of a subject. A scale (30) having electrodes (32, 34) may be used for this purpose. The signal obtained from the electrodes (32, 34) is digitized (46) and filtered (50) to obtain an electrocardiographic signal exhibiting periodic, sequen-

tial, discrete, magnitudinal variations associated with the heartbeats of the subject. The electrocardiographic signal is then analyzed (60) to identify discrete magnitudinal variations useful for obtaining the desired information. In determining the heart rate of the subject, an interval between variations having a desired magnitudinal characteristic may be employed. The absence of such variations is indicative of atrial fibrillation.

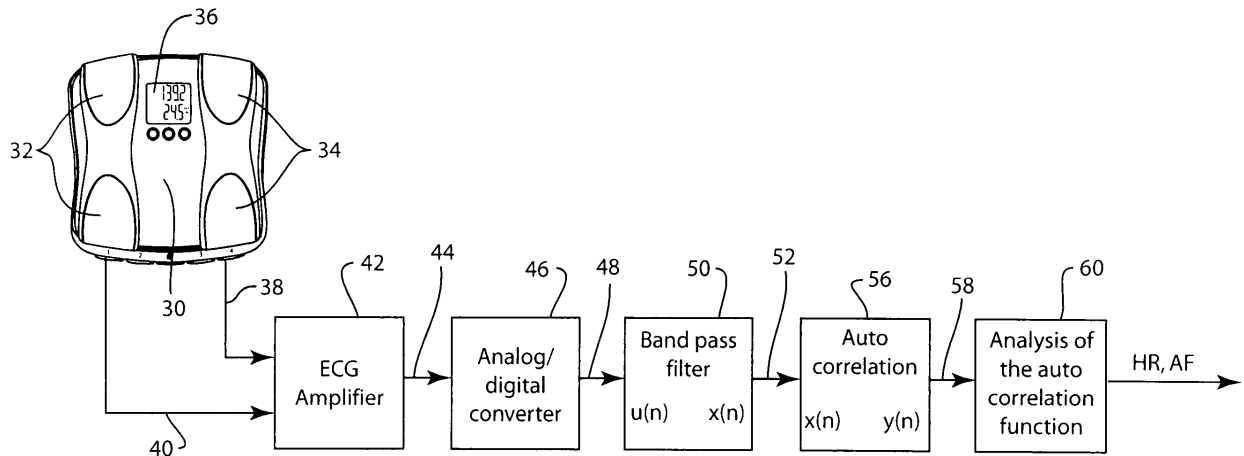


FIG. 3

**Description**

**[0001]** The present invention relates to an apparatus and method for obtaining cardiac data using conductive elements applied to the feet of a subject. While the invention is not so limited, the invention may be carried out using a body fat analysis scale.

**[0002]** Scales are conventionally used to measure body weight. For a commonly used type of scale, a person steps on footpads on the scale and the resulting compressive loading operates a mechanical or electrical apparatus to provide an indication of the person's weight.

**[0003]** Scales have been developed that can also be used to measure a person's body fat. The footpads on such a scale are made electrically conductive. A small electrical current is passed through the body of a person standing on the footpads. Fat tissue has different electrical properties than muscle tissue, due to differing amounts of water in the different tissues. The bioelectrical impedance that exists between the footpads is measured and used to determine body fat properties, typically the body fat percentage.

**[0004]** In an aspect of the invention, information about the heart, such as heart rate or the detection of arrhythmias, may be obtained from the feet of a person, as by using conductive footpads of a scale of the above type.

**[0005]** The heart rate of a person is an important physiological measurement. Increases in the heart rate are indicative of a variety of different diseases and conditions in the body, such as the presence of fever or the consumption of alcohol, caffeine, nicotine, or certain drugs. A permanently high heart rate is a risk predictor for overall mortality as noted in literature such as Wojciech Zaeba, Prognostic Significance of a Standard 12-Lead ECG after Myocardial Infarction, International Journal of Bioelectromagnetism, Vol. 5, No. 1, 2003. Hence, it may be desirable to frequently measure a person's heart rate. The convenience of obtaining a person's heart rate by simply stepping on a body fat analysis scale facilitates obtaining such information.

**[0006]** Arrhythmias can occur when the muscle fibers of the heart fail to contract synchronously. This has the potential to lessen the efficiency of the heart to pump blood. In fibrillation, the muscles of the heart quiver randomly and erratically. Ventricular fibrillation is fatal in the absence of immediate medical intervention. However, if the atrial portion of the heart is in fibrillation, the heart can still pump some blood so that the condition can exist until diagnosed and treated.

**[0007]** The detection of atrial fibrillation is important because of its serious nature, because of its frequent existence among the elderly, and because of the adverse prognosis attendant the presence of atrial fibrillation. See Nusser, Trieb, Weidner, *Differentialdiagnostik des EKG*, Schattauer Verlag. In some subjects atrial fibrillation is intermittent in that it is sometimes present and disappears at other times.

**[0008]** A way to check for the existence of atrial fibrillation that is convenient and lends itself to frequent use thus presents further significant health benefits.

**[0009]** To the foregoing ends, electrocardiographic (ECG) signal data is obtained from conductive footpads and processed to identify features, such as the reoccurring QRS complexes appearing in the electrocardiographic data. The timing between successive features is used to determine heart rate. Variations in the timing characteristics among successive heartbeats, or the absence of a heartbeat feature, are indicative of arrhythmias, such as those characterizing atrial fibrillation.

**[0010]** Various aspects and embodiments of the invention will now be described in connection with the accompanying drawings, in which:

Fig. 1 shows an electrocardiographic signal associated with a heartbeat;

Fig. 2 shows a typical electrical signal obtained from conductive element applied to the feet of a person;

Fig. 3 shows an embodiment of the present invention suitable for obtaining cardiac data from an electrical signal of the type shown in Fig. 2;

Fig. 4 shows an electrocardiographic signal provided at the output of a bandpass filter element of the apparatus of Fig. 3;

Fig. 5 shows an autocorrelation function of the electrocardiographic signal of Fig. 4 and the manner in which the function is used to obtain cardiac data such as a person's heart rate;

Fig. 6 shows an electrocardiographic signal exhibiting high variability in the heartbeats and indicative of the presence of atrial fibrillation;

Fig. 7 shows the autocorrelation function of the signal of Fig. 6; and

Fig. 8 shows a further embodiment of the apparatus of the present invention.

5 [0011] Fig. 1 shows the electrical phenomena or signal 10 associated with a heartbeat, along with the conventional designations for its various components. An initial feature in the morphology of the signal is the P wave resulting from the contraction of the atria of the heart to commence the heartbeat. The major feature of the graph, the QRS complex, is followed by the contraction of the ventricles, and in turn, by the T wave indicative of a refractory period for the heart muscle at the end of the heartbeat. An electrocardiographic signal 10 of the type shown in Fig. 1 is ordinarily obtained by electrodes applied to the chest and extremities of a person.

10 [0012] Fig. 2 shows a typical electrocardiographic signal 20 received from the feet of a person containing a small magnitude ECG signal and a considerable amount of electrical noise in the output from conductive footpads applied to the feet.

15 [0013] Fig. 3 shows apparatus for obtaining information about the heart from output signal 20 obtained from electrodes applied to the feet of a person. Scale 30 has pairs of conductive footpads 32 and 34 on which a subject stands to determine his/her body weight and body fat. While the invention is not so limited, the use of pairs of footpads increases the quality of data collected as one set of footpads may be used for data collection and the other set used for common mode rejection of noise. Scale 30 has display 36 for providing this information. Leads 38 and 40 extend from scale 30 to provide the output signal shown in Fig. 2.

20 [0014] Leads 38 and 40 are connected to input ECG amplifier 42 having appropriate characteristics of frequency response, gain, circuit protection, and the like. The ECG lead signal output from amplifier 42 is provided in conductor 44 to analog/digital converter 46. Analog/digital converter 46 samples the signal in conductor 44 at an appropriate rate and converts the analog signal in conductor 44 to a digital signal in conductor 48. The minimum sampling rate to collect data that will reproduce a signal accurately is two times the highest frequency component of the signal, as determined by Nyquist's theorem. Therefore a sampling rate of at least twice the line frequency is required to filter out the line frequency. In an embodiment of the invention, a sampling rate of 200 Hz is used when the line frequency is 50 Hz or 25 [0015] 240 Hz is used when the line frequency is 60 Hz.

30 [0015] The signal in conductor 48 is supplied to bandpass filter 50 that carries out high pass and low pass filtering of the signal to improve the signal to noise ratio over that found in the digital signal in conductor 48. In an embodiment of the invention, the bandpass filter 50 may have a low frequency cutoff at 2 Hz and a high frequency cutoff at 25 Hz. As a result of bandpassing only a selected portion of the total signal shown in Fig. 2, QRS complexes, P-waves, and T-waves found in the bandpassed signal are augmented and the noise in the signal is reduced. That is, the signal shown in Fig. 2 may contain noise frequency components in a range from 0 - 1,000 Hz whereas the signal in conductor 52 will contain only noise components between 2 - 25 Hz so that a substantial amount of the frequency content of the signal is removed by the bandpass filter. This results in leaving the predominant ECG signal while removing a substantial amount of the noise, as can be seen by comparing Figs. 2 and 4.

35 [0016] The high pass filter found in element 50 may comprise an infinite impulse response (IIR) filter. An IIR filter is suited for use as a high pass filter because a lower order and easier to calculate and implement filter of this type will provide a steeper cut-off frequency. An IIR filter also provides faster real-time signal processing also making it advantageous for use as a high-pass filter. The low pass filter found in element 50 may comprise a finite impulse response (FIR) filter. A FIR filter is appropriate for a low pass filter due to its stability and linear phase response and the ability to reject 60Hz or 50Hz line noise. It will be appreciated that other types of filters and sampling rates may be used in the apparatus shown in Fig. 3.

40 [0017] The output from bandpass filter 50 in conductor 52 is shown in Fig. 4 as the graph 54. It will be appreciated from an inspection of Fig. 4 that the features of the electrocardiographic data shown in Fig. 1 are augmented in the signal 54 in conductor 52 in the process of filtering signal 20 shown in Fig. 2. This includes the prominent QRS complex of the electrocardiographic signal shown in Fig. 1.

45 [0018] The signal 54 in conductor 52 is supplied to element 56 that performs an autocorrelation on the signal. An autocorrelation is carried out by comparing and correlating a signal with itself. An autocorrelation function measures the dependence of time series values at one time on the values of that time series at another time. A modified autocorrelation is calculated by equation (1):

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$$y(k) = \frac{\sum_{n=1}^{N-K} x(n)x(n+k)}{\sum_{n=1}^{N-K} x(n)^2} \quad (1)$$

Given the time series  $x(n)$ ,  $x(n+k)$ ,  $n=1, 2... N$ ,  $k=1, 2... K$

**[0019]** By definition, over a large time series, a stochastic or random process tends towards being a zero-mean time series, thus having an autocorrelation of zero. Therefore, the autocorrelation removes any random signal processes, leaving the desired underlying periodic signal, in this case the ECG signal. An autocorrelation function is most useful in extracting an underlying periodic signal out of random background noise including circumstances in which the underlying signal is masked by high amplitude and high frequency noise. This is the case in ECG signal processing. In element 56, the autocorrelation function pulls the ECG signal out of the underlying noise in the signal 54 in conductor 52 and provides the same to analysis element 60 in conductor 58.

**[0020]** The analysis of the autocorrelation function is carried out in the following manner as shown graphically in Fig. 5. The signal in conductor 58 is examined to locate a maximum spike amplitude 62 found in the autocorrelation function  $y(k)$ . A threshold value is then defined as a percentage of the maximum spike amplitude. For example, the threshold may be set at 60% of the spike amplitude. This permits information about the heart to be determined even in the presence of ventricular and supraventricular extrasystoles. Extrasystoles, or premature beats, are typically contractions of the ventricles that do not alter the fundamental rhythm of the heart or inject significant amounts of blood into the circulatory system.

**[0021]** Thereafter, the distance or timing from a first spike to a second spike that exceeds the threshold is determined. This is shown as the quantity  $K$  in Fig. 5.

**[0022]** When  $K$  is considered as a time quantity, such as 0.8 seconds between spikes, the formula for determining heart rate in beats per minute is

$$HR = 60/K \quad (2)$$

**[0023]** Due to the sampling carried out in analog/digital converter 46, it is often more convenient to express  $K$  as the number of samples between spikes. In this case, the formula would be

$$HR = (60 \times \text{sampling rate})/K \quad (3)$$

**[0024]** The heart rate of a person standing on scale 30 is thus determined from the feet of the person. Typically 10 seconds of data may be used to determine the heart rate. The heart rate so determined may be provided to display 36 of scale 30.

**[0025]** Fig. 6 shows an electrocardiographic signal 70 for a subject who is experiencing atrial fibrillation, as indicated by the high variability in the intervals between the QRS complexes in the ECG signal and the poor definition, or lack, of characteristics, such as the P wave.

**[0026]** Fig. 7 shows the autocorrelation function for the signal 70 of Fig. 6 in a manner corresponding to that of Fig. 5 showing a normal ECG signal. As can be seen from Fig. 7, the high variability, or conversely the low regularity, in the periodicity of the signal 70 shown in Fig. 6 results in low magnitude spikes in the autocorrelation function 72 of Fig. 7. As a result, none of the spikes will exceed the threshold established in analysis element 60 and this phenomenon may be used to provide an indication at output of element 60 that the subject from whom the data is obtained is experiencing atrial fibrillation.

**[0027]** While discrete components are shown for illustrative purposes in Fig. 3 and to facilitate an explanation of the

disclosed apparatus, it will be appreciated that many of the components may be formed by an appropriately programmed microprocessor or central processing unit (CPU), including that found in scale 30 for use in determining body weight and fat.

**[0028]** Fig. 8 shows another embodiment of apparatus suitable for carrying out the present invention. Apparatus 100 shown in Fig. 8 employs QRS trigger element 102. QRS trigger element 102 employs the magnitude or rate of change properties contained in the filtered signal 54 in conductor 52 to identify the QRS complexes in signal 54. For example, a digital equivalent of a Schmitt trigger may be used for this purpose. In such a circuit, a change in state of the output signal is "triggered" when the input signal crosses a predetermined threshold level. The output of QRS trigger element 102 is provided in conductor 104 to element 106 that includes timing or other circuitry to identify the interval between successive QRS complexes. For example, the interval between the feature in signal 54 corresponding to the R feature of the QRS complex in the ECG signal may be determined. The average of the duration of a series of intervals between R features, the average PR interval, for example from 10 seconds of ECG signal data is inserted in equation (4) to obtain the heart rate.

$$HR = 60/\text{average RR interval} \quad (4)$$

**[0029]** For the detection of atrial fibrillation, the irregularity in the intervals between QRS complexes may be used for this purpose. Or, an average or median heart beat characteristic comprising the PQRST-data for a given number of cycles, for example 10 cycles, may be determined from the signal in conductor 104. As noted above in atrial fibrillation, the P-wave is absent or ill-defined. The absence of at least a proper P-wave within the time of an average or median heart beat may be used to detect atrial fibrillation.

**[0030]** It will be appreciated that the present invention provides a convenient, simple way for a person to learn of an important health criteria from a small and noisy signal obtained from the feet. The information so obtained can be used along, or in connection, with other information, such as weight and body fat determined from a scale.

**[0031]** Various alternatives and other embodiments are contemplated as being within the scope of the present invention. For example, it is possible to provide the ability to enter age and gender information into the apparatus to personalize the data analysis carried out by analysis element 60 thus increasing the usefulness of the obtained cardiac data, for example, the accuracy of atrial fibrillation determination. Or, by using data storage capabilities, the analysis carried out by element 60 can be modified based on past data or over time, thus increasing the accuracy of data analysis. Data storage capability also allows for long-term analysis and trending of the collected physiological parameters. The data obtained by the apparatus may be communicated via RF, modem, or broadband technology to a related data collection site, such as a healthcare provider. Alternatively, the communication ability may comprise RF, infrared or serial connection to a data storage unit, a computer, or a printer.

PARTS LIST				
Part #	Part Name		Part #	Part Name
30	Scale		50	Bandpass
32	Conductive Footpads		52	Conductor
34	Conductive Footpads		56	Autocorrelation Element
36	Display		58	Conductor
38	Lead		60	Analysis Element
40	Lead		100	Invention Apparatus
42	ECG Amplifier		102	Trigger Element
44	Conductor		104	Conductor
46	A/D Converter		106	Timing Circuit
48	Conductor			

**Claims**

1. A method for obtaining cardiac information from a person, said method comprising the steps of:

5           applying electrodes (32, 34) to the feet of the person to obtain a bioelectrical signal (20) from the person including cardiac data;  
          filtering (50) the bioelectric signal to provide a filtered signal containing the cardiac data;  
          processing (56) the filtered signal to identify discrete magnitudinal variations in the signal useful for obtaining desired cardiac information;  
10          determining a characteristic of the discrete variations (60); and  
          using the determined characteristic to obtain the desired cardiac information from the person.

2. The method according to claim 1 further defined as determining an interval property between successive discrete variations.

15          3. The method according to claim 2 further defined as using the determined interval property to obtain the heart rate of the person.

20          4. The method of claim 2 or claim 3 further defined as using variation in the interval property between discrete magnitudinal variations to obtain information regarding atrial fibrillation in the person.

5. The method according to any preceding claim further defined as using the absence of a morphological feature of a heartbeat feature to obtain information regarding atrial fibrillation in the person.

25          6. The method according to any preceding claim wherein the step of applying the electrodes (32, 34) is further defined as the act of a person stepping on a scale having electrodes.

7. Apparatus for obtaining cardiac information from a person, said apparatus comprising:

30           electrodes (32, 34) applicable to the feet of the person to obtain a bioelectrical signal (20) from the person containing cardiac data;  
          a filter (50) receiving said bioelectrical signal and providing a filtered signal containing the cardiac data;  
          means for processing (56) the filtered signal to identify discrete magnitudinal variations in the signal useful for obtaining desired cardiac information;  
35          means for determining (60) a characteristic of the discrete variations; and  
          means for using the determined characteristic to obtain the desired cardiac information from the person.

8. The apparatus according to claim 7 wherein said means for using is further defined as using the determined interval property between successive discrete variations to obtain the heart rate of the person.

40          9. The apparatus according to claim 7 or claim 8 wherein said means for using is further defined as using variation in the interval property between discrete magnitudinal variations to obtain information regarding arterial fibrillation in the person.

45          10. The apparatus according to any one of claims 7 to 9 wherein said determining means is further defined as determining the absence of a morphological feature of a heartbeat to obtain information regarding arterial fibrillation in the person.

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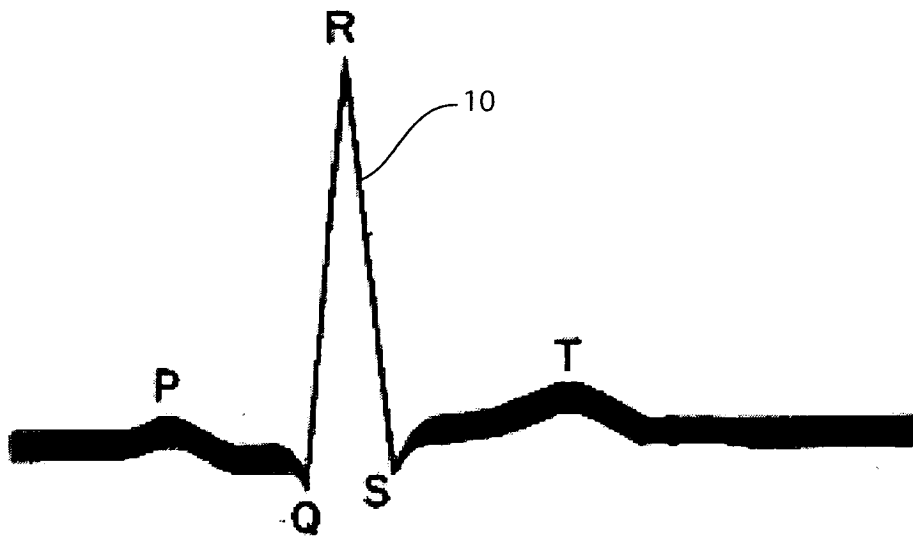


FIG. 1

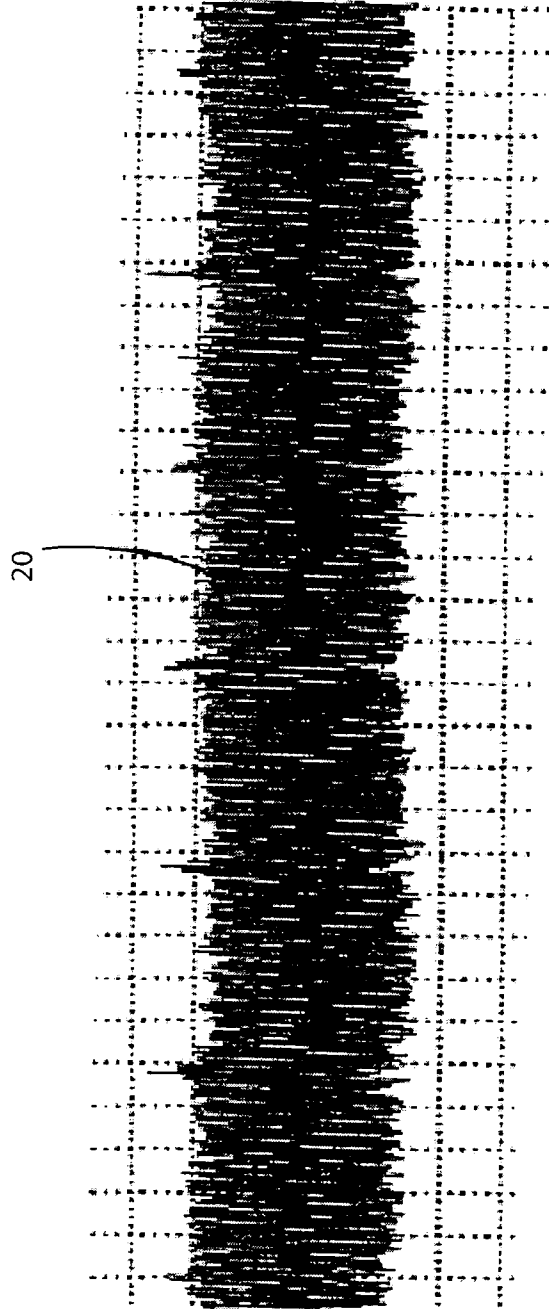


FIG. 2

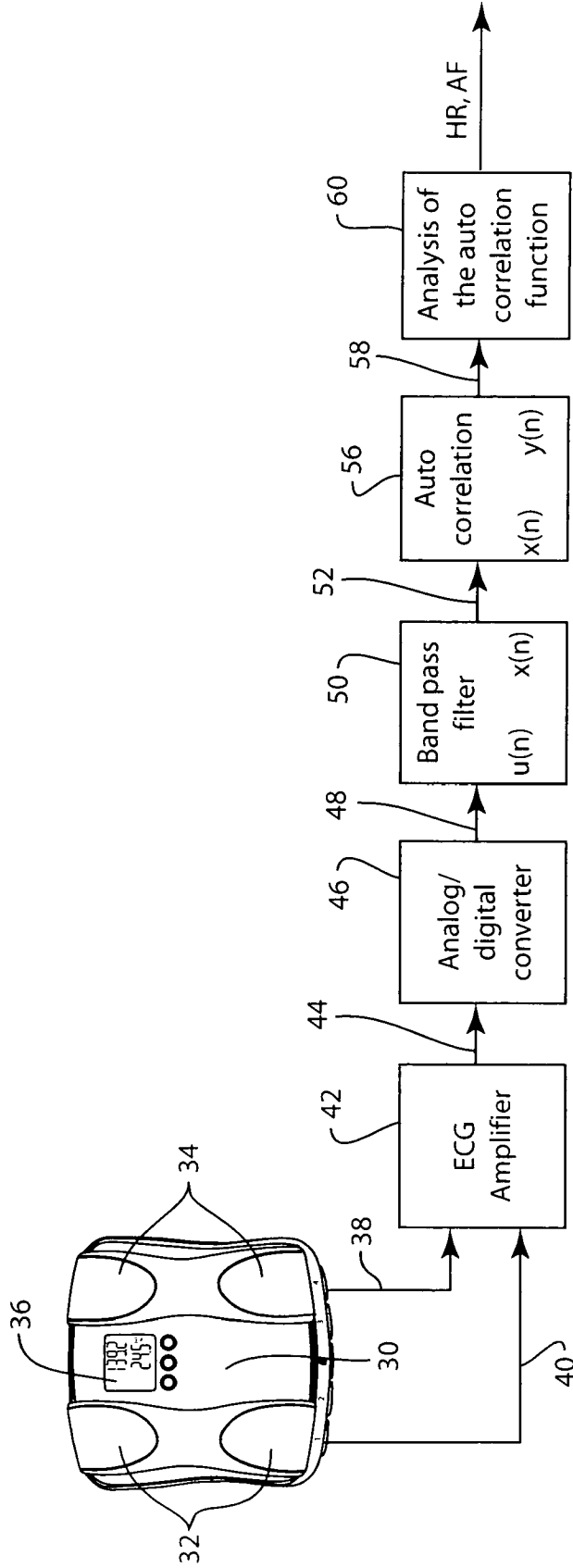


FIG. 3

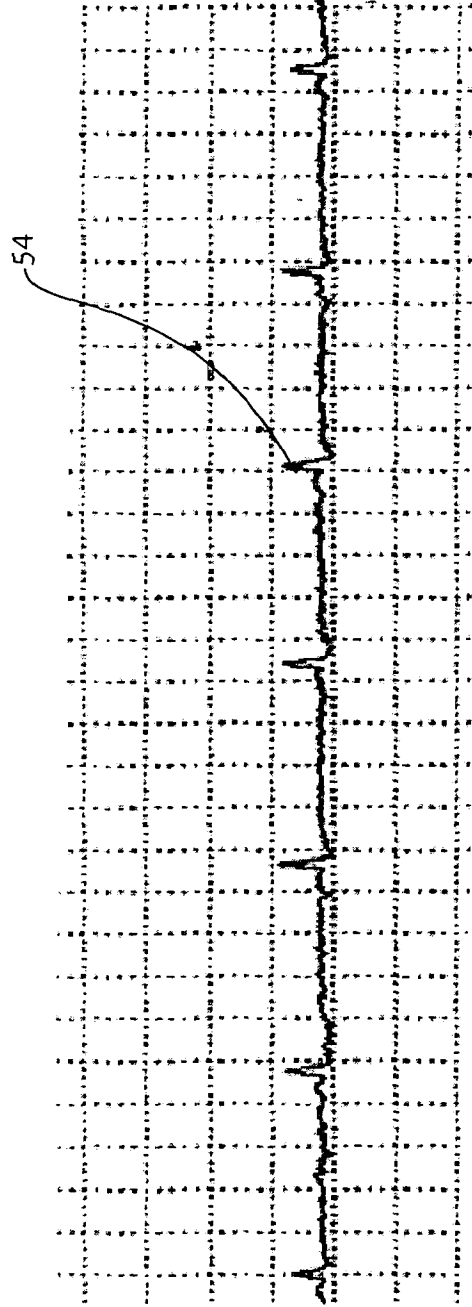


FIG. 4

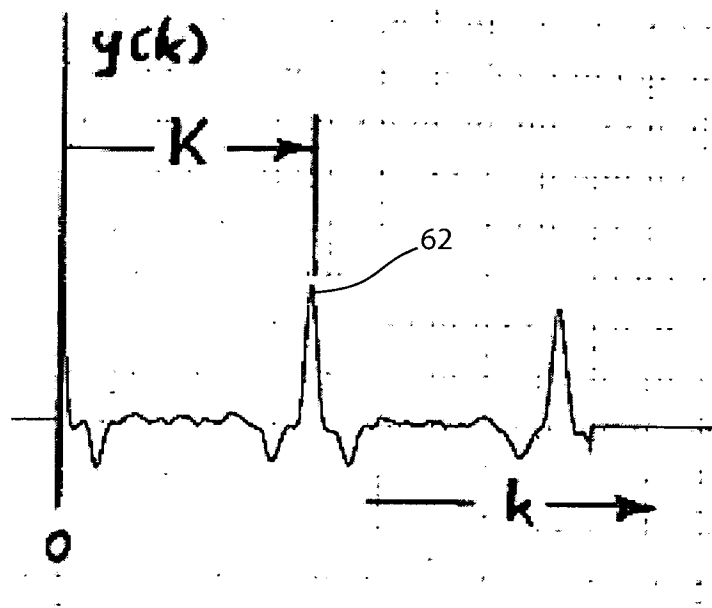


FIG.5

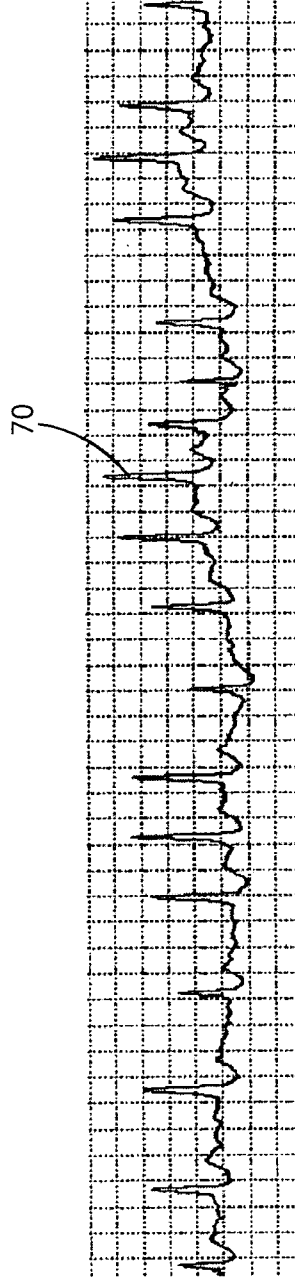


FIG.6

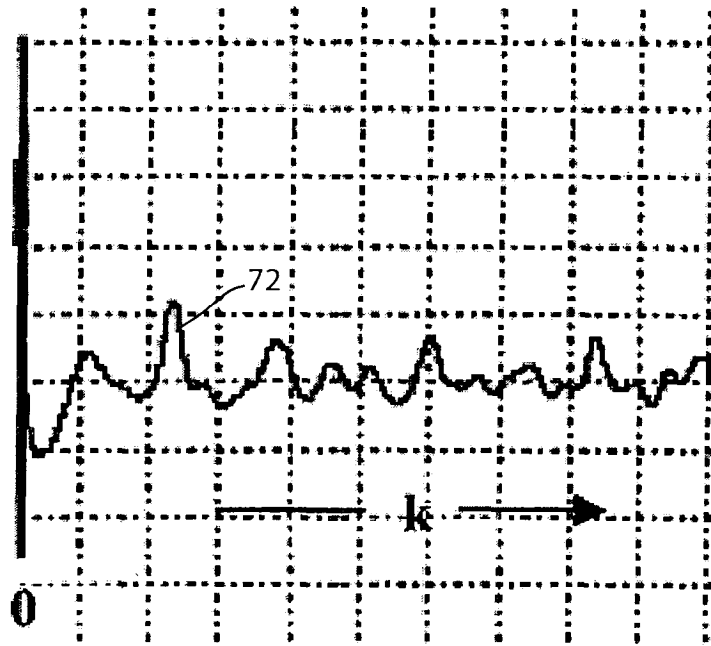


FIG. 7

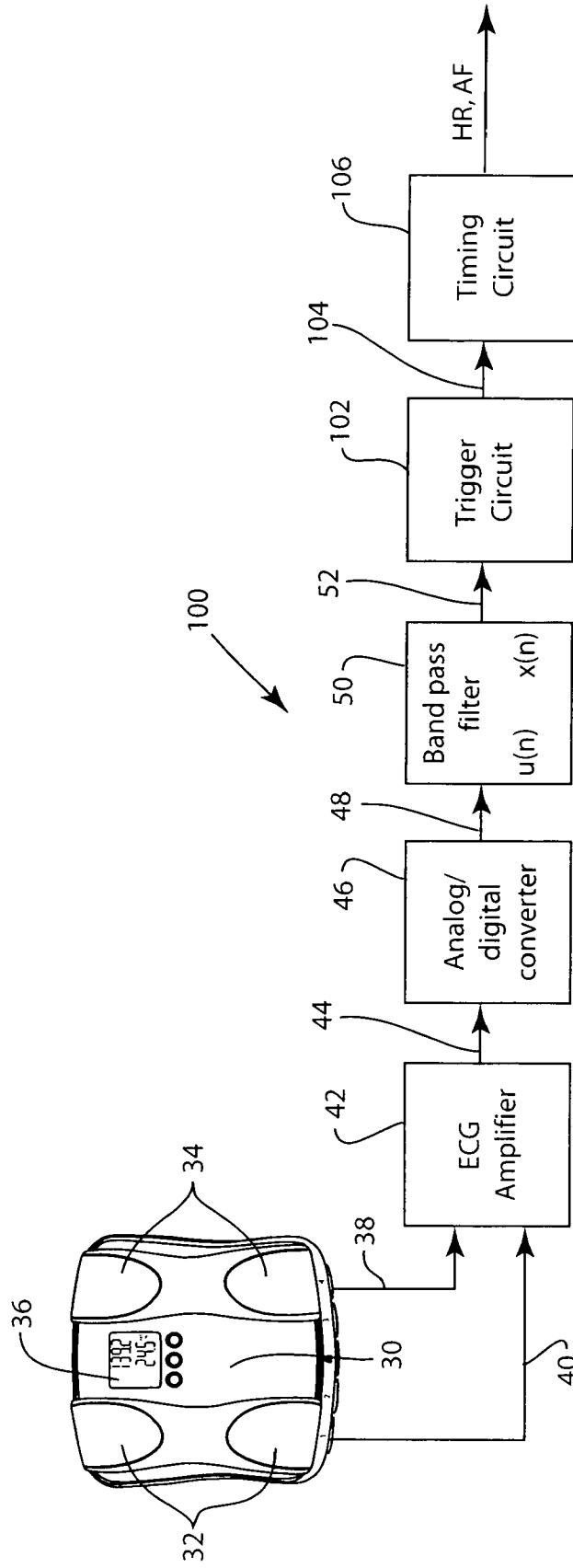


FIG.8



DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 2005/004483 A1 (LIN ABDADA) 6 January 2005 (2005-01-06) * abstract; figure 1 * * paragraphs [0010], [0021] *	1-3,7,8	INV. A61B5/00
Y	-----	4-6,9,10	
Y	US 6 519 490 B1 (WIESEL JOSEPH) 11 February 2003 (2003-02-11) * abstract; figure 1 * * column 1, lines 18-21 * * column 3, lines 12-19 * * column 4, line 34 - column 5, line 20 *	4,5,9,10	
Y	EP 1 147 740 A (TANITA CORPORATION) 24 October 2001 (2001-10-24) * the whole document *	6	
X,P	US 2006/116589 A1 (PARK WON-HEE) 1 June 2006 (2006-06-01) * abstract; figures 1,2 * * paragraphs [0002], [0006], [0013] *	1-3,6-8	
Y,P	-----	4,5,9,10	TECHNICAL FIELDS SEARCHED (IPC) A61B
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 6 October 2006	Examiner Pereda Cubián, David
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

13

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ANNEX TO THE EUROPEAN SEARCH REPORT  
ON EUROPEAN PATENT APPLICATION NO.

EP 06 25 3786

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report. The members are as contained in the European Patent Office EDP file on  
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06-10-2006

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**REFERENCES CITED IN THE DESCRIPTION**

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**Non-patent literature cited in the description**

- **WOJCIECH ZAEBA.** Prognostic Significance of a Standard 12-Lead ECG after Myocardial Infarction. *International Journal of Bioelectromagnetism*, 2003, vol. 5 (1 [0005])

专利名称(译)	用于获得心脏数据的设备和方法		
公开(公告)号	<a href="#">EP1745740A1</a>	公开(公告)日	2007-01-24
申请号	EP2006253786	申请日	2006-07-19
[标]申请(专利权)人(译)	通用电气公司		
申请(专利权)人(译)	通用电气公司		
当前申请(专利权)人(译)	通用电气公司		
[标]发明人	KAISER WILLI FINDEIS MARTIN		
发明人	KAISER, WILLI FINDEIS, MARTIN		
IPC分类号	A61B5/00 A61B5/024 A61B5/046		
CPC分类号	A61B5/046 A61B5/024 A61B5/6829		
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其他公开文献	EP1745740B1		
外部链接	<a href="#">Espacenet</a>		

摘要(译)

一种用于从施加到受试者的脚上的电极 ( 32,34 ) 获得信息 ( 例如心率或心房颤动的存在 ) 的装置和方法。具有电极 ( 32,34 ) 的标尺 ( 30 ) 可用于此目的。将从电极 ( 32,34 ) 获得的信号数字化 ( 46 ) 并过滤 ( 50 ) 以获得表现出与受试者心跳相关的周期性, 连续的, 离散的, 幅度变化的心电图信号。然后分析心电信号 ( 60 ) 以识别对获得所需信息有用的离散的幅度变化。在确定受试者的心率时, 可以采用具有期望的幅度特性的变化之间的间隔。没有这种变化表明心房颤动。

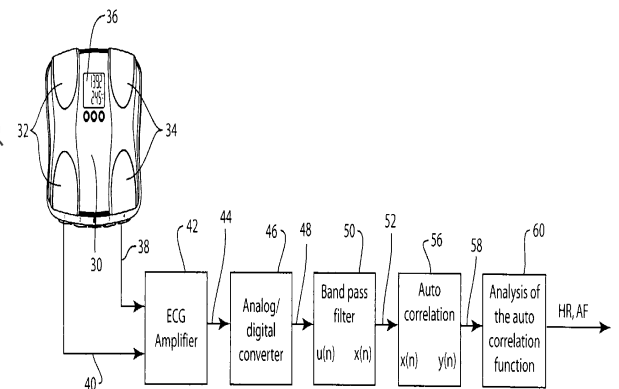


FIG.3